

# Implementation of the Density Evolution method with Fokker-Plank for L-NLIF Model in Python

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## 1 Introduction

This report contains a description of the work done by Valentin Haenel for a Lab Rotation within the Bernstein Center for Computational Neuroscience in Berlin. The rotation was done in the lab of Gabriel Curio under the supervision of Bartosz Telenczuck.

Throughout the project i have implemented a variant of the Leaky Integrate and Fire Neuron, and a method to fit the parameters of this neuron using a model of the input and extracellularly recorded spikes. This involved solving a partial differential equation and constructing a maximum likelihood objective function.

## 2 Model

The original model is a L-NLIF model, which consists of a Linear (L) Filter, followed by a probabilistic or Noisy (N) form of Leaky Integrate and Fire spike generation(LIF) (Paninski et al.[1]). For sake of completeness the model is briefly described here.

The evolution of the Voltage  $V$  is given by:

$$dV = (-g(V(t) - V_{leak}) + I_{stim}(t) + I_{hist}(t))dt + W_t \quad (1)$$

Where  $g$  is the leak conductance  $V_{leak}$  is the leak reversal potential  $I_{stim}$  is the convolution of linear filter with the input signal,  $I_{hist}$  is the spike current history and  $W_t$  is standard Gaussian white noise. More precisely:

$$I_{stim}(t) = \vec{k}x(t) \quad (2)$$

$$I_{hist}(t) = \sum_{j=0}^{i-1} h(t - t_j) \quad (3)$$

Where  $k$  is a linear filter and  $h$  is a fixed postspike current waveform.

## 3 Algorithms

This section describes the algorithms employed.

### 3.1 PDE Solver

#### 3.1.1 The Problem

If we define

$$P(V, t) \equiv P(V(t) \cap V(s) < V_{th} \forall s < t) \quad (4)$$

This refers to the probability of  $V(t)$ , the membrane potential, being less than  $V_{th}$  the firing threshold until time  $t$ .

As stated in [1] we need to solve the following Fokker-Planck drift diffusion equation numerically, and hence this method is called PDE Solver.

$$\frac{\partial P(V, t)}{\partial t} = \frac{\sigma^2}{2} \frac{\partial^2 P(V, t)}{\partial V^2} + g \frac{\partial [(V - V_{rest})P(V, t)]}{\partial V} \quad (5)$$

Given the boundary conditions:

$$P(V_{th}, t) = 0 \quad (6)$$

$$P(V, 0) = \delta(V - V_{reset}) \quad (7)$$

When solving numerically we also need a lower bound on the voltage  $V_{lb}$ , so this becomes an additional boundary condition:

$$P(V_{lb}, t) = 0 \quad (8)$$

Ideally  $V_{lb} = -\infty$  And the definition of  $V_{rest}$ .

$$V_{rest}(t) = V_{leak} + \frac{1}{g} (\vec{k} \cdot \vec{x}(t) \sum_{j=0}^{i-1} h(t - t_j)) \quad (9)$$

We can rewrite this as:

$$\frac{\sigma^2}{2} \frac{\partial^2 P(V, t)}{\partial V^2} + g(V - V_{rest}) \frac{\partial P(V, t)}{\partial V} + gP(V, t) - \frac{\partial P(V, t)}{\partial t} = 0 \quad (10)$$

Since we know that:

$$\frac{\partial [(V - V_{rest})P(V, t)]}{\partial V} = \frac{\partial (V - V_{rest})}{\partial V} \dot{P} + \frac{\partial P}{\partial V} (V - V_{rest}) \quad (11)$$

and

$$\frac{\partial (V - V_{rest})}{\partial V} = 1 \quad (12)$$

### 3.1.2 Finite Differencing

Next we discretize time and potential. We adopt the notation that Potential is discretized into  $W$  intervals of length  $w$  and indexed by  $\nu = 0, 1, \dots, W$ . Time is discretized into  $U$  intervals of length  $u$  and indexed by:  $\tau = 0, 1, \dots, U$ .  $P_{\nu,\tau} = P(\nu w, \tau u)$

Before we can write down the computationally stable Crank-Nicolson method [2] we must first write down our finite differencing scheme:

$$\hat{P} = P_{\nu,\tau} \quad (13)$$

$$\frac{\partial \hat{P}}{\partial t} = \frac{P_{\nu,\tau+1} - P_{\nu,\tau}}{u} \quad (14)$$

$$\frac{\partial \hat{P}}{\partial V} = \frac{P_{\nu+1,\tau} - P_{\nu-1,\tau}}{2w} \quad (15)$$

$$\frac{\partial^2 \hat{P}}{\partial V^2} = \frac{P_{\nu+1,\tau} - 2P_{\nu,\tau} + P_{\nu-1,\tau}}{w^2} \quad (16)$$

Using the Crank-Nicolson scheme we may now rewrite the derivatives using a new finite differencing scheme which is centered around  $t + u/2$ . Bearing in mind that this is only an approximation we get:

$$P_{CN} = \frac{P_{\nu,\tau} + P_{\nu,\tau+1}}{2} \quad (17)$$

$$\frac{\partial P_{CN}}{\partial t} = \frac{P_{\nu,\tau+1} - P_{\nu,\tau}}{u} \quad (18)$$

$$\frac{\partial P_{CN}}{\partial V} = \frac{P_{\nu+1,\tau} + P_{\nu+1,\tau+1} - P_{\nu-1,\tau} - P_{\nu-1,\tau+1}}{4w} \quad (19)$$

$$\frac{\partial^2 P_{CN}}{\partial V^2} = \frac{P_{\nu+1,\tau} - 2P_{\nu,\tau} + P_{\nu-1,\tau} + P_{\nu+1,\tau+1} - 2P_{\nu,\tau+1} + P_{\nu-1,\tau+1}}{2w^2} \quad (20)$$

### 3.1.3 Tridiagonal Equations

If we now let:

$$\begin{aligned} a &= \frac{\sigma^2}{2} \\ b &= g(V - V_{rest}) \\ c &= g \end{aligned}$$

and multiply throughout with  $4w^2u$  we may rearrange all the  $P_{*,\tau+1}$  terms on the left hand side:

$$\begin{aligned} \overbrace{-(2au + b w u)}^{A_\nu} P_{\nu+1,\tau+1} + \overbrace{(4au - 2cw^2u + 4w^2)}^{B_\nu} P_{\nu,\tau+1} - \overbrace{(2au - b w u)}^{C_\nu} P_{\nu-1,\tau+1} = \\ \underbrace{(2au + b w u)P_{\nu+1,\tau} + (-4au + 2cw^2u + 4w^2)P_{\nu,\tau} + (2au - b w u)P_{\nu-1,\tau}}_{D_\nu} \end{aligned} \quad (21)$$

For each  $\nu = 1, \dots, W - 1$

We note here that we have obtained  $W - 1$  simultaneous equations which we may now rewrite in the following tridiagonal matrix notation.

$$\underbrace{\begin{pmatrix} B_0 & A_0 & 0 & 0 & \cdots & 0 \\ C_1 & B_1 & A_1 & 0 & \cdots & 0 \\ 0 & C_2 & B_2 & A_2 & 0 & \\ \vdots & & \ddots & \ddots & \ddots & \vdots \\ 0 & \cdots & 0 & C_{W-1} & B_{W-1} & A_{W-1} \\ 0 & \cdots & 0 & 0 & C_W & B_W \end{pmatrix}}_{\Lambda} \underbrace{\begin{pmatrix} P_{0,\tau+1} \\ P_{1,\tau+1} \\ P_{2,\tau+1} \\ \vdots \\ P_{W-1,\tau+1} \\ P_{W,\tau+1} \end{pmatrix}}_{\chi} = \underbrace{\begin{pmatrix} D_0 \\ D_1 \\ D_2 \\ \vdots \\ D_{W-1} \\ D_W \end{pmatrix}}_{\beta} \quad (22)$$

However this matrix equation has  $W+1$  equations, so we must use the boundary conditions to specify the first and last rows of  $\Lambda$ . We can then use a tridiagonal matrix algorithm to solve  $\Lambda\chi = \beta$ .

This allows us to iteratively obtain the density evolution  $P(V, t)$  of the membrane potential for a given time interval.

### 3.2 First Passage Time

The maximum likelihood optimizer proposed in [1] however uses the first passage time density at a given time point which is defined as:

$$fpt(t) = -\frac{\partial}{\partial t} \int P(V, t) dV \quad (23)$$

and this can be easily computed from an  $P(V, t)$  matrix by summing across  $P$  and finding differences across  $t$ .

### 3.3 Maximum Likelihood Estimator

Putting together the PDE Solver and method for computing the First Passage Time The final likelihood is then simply

$$L_{\vec{x}, t_i} = \Pi_i fpt(t_i) \quad (24)$$

The pseudocode for the objective function can be described as follows:

for each spike interval do:

1. compute  $P(V, t)$  as matrix
2. compute  $fpt$  as vector

return the product of the last scalars in the  $fpt$  vectors.

This objective function could be presented to a standard numerical optimizer, for example the Nelder-Mead Downhill simplex [2], this needs no gradients and is fairly robust but slow.

### 3.4 Monte Carlo Method

To double check the results of the PDE Solver and the resulting First Passage Time , we additionally implemented some basic monte carlo simulations. This did not involve much more than simulating a few thousand single spike runs of our model, with noise. The resulting potential traces, and spike times were used to obtain both  $P(V, t)$  and  $fpt$ . The density evolution is compared qualitatively and the  $fpt$  is compared using a Kolmogorov-Smirnov (K-S) test[2].

## 4 Implementation

This section describes the concrete implementation

### 4.1 Availability and Design

The algorithm has been implemented in Python, and the full source code has been made available within a revision control system under a free software license at: <http://github.com/esc/molif/tree/master>. The name of the project is *Meaning Of LIF*, abbreviated to *molif* which is a reference to the Monty Python movie *Meaning of Life*. The name was chosen one the one hand because we think its funny, and secondly to underline one more time, that Python isn't about snakes.

The software is structured into a series of modules, one for the neuron model, one for the pde solver, one to minimize the negative likelihood, one for monte carlo simulation and a utility module.

The software uses the additional packages numpy, scipy for vector based and scientific computing, and pylab/matplotlib for plotting the results. We used the modules *scipy.sparse* and *scipy.linalg* for computing the solution to tridiagonal equations, and the method *optimize.fmin*, which implements the Nelder-Mead Downhill Simplex, for minimizing the negative likelihood.

### 4.2 Limitations and Future Work

The PDE solver uses sparse matrix algorithms to store and solve the tridiagonal matrix. Ideally we would like to use the routine *TRIDAG* described in [2], however an open source implementation in python was not available, although feasible. This improvement could possibly speed up the computation of  $P(V, t)$ .

There is a serious bug, whereby the value of sigma, must be within a specific range of  $0.1 - 0.05$ , otherwise strange oscillatory instabilities occur. Among the possible causes, are a numerical instability in the finite differencing scheme, a bug in our code, a bug in the solver for the linear equations or the discretization of  $P$  and  $t$  being too large.

Currently the gradient of the objective function isn't implemented, and any gradient based optimizer would need to compute their approximation from the function values.

We used a Kolmogorov-Smirnov (K-S) test to check that the first passage time computed by the pde-solver and the monte carlo method come from the same distribution. However the test currently returns a negative result, although at first glance the distributions look very similar.

Lastly we should mention that the objective function isn't fully operational yet. A simple test is executed as follows: first we generate some spikes with given parameters, and then we attempt to fit parameters to these spikes. If the code operates correctly the optimizer should not deviate away from the initial parameters vector. However currently this is not the case and the optimizer finds a minimum at a different position in parameter space.

### 4.3 Images

This section presents some plots.

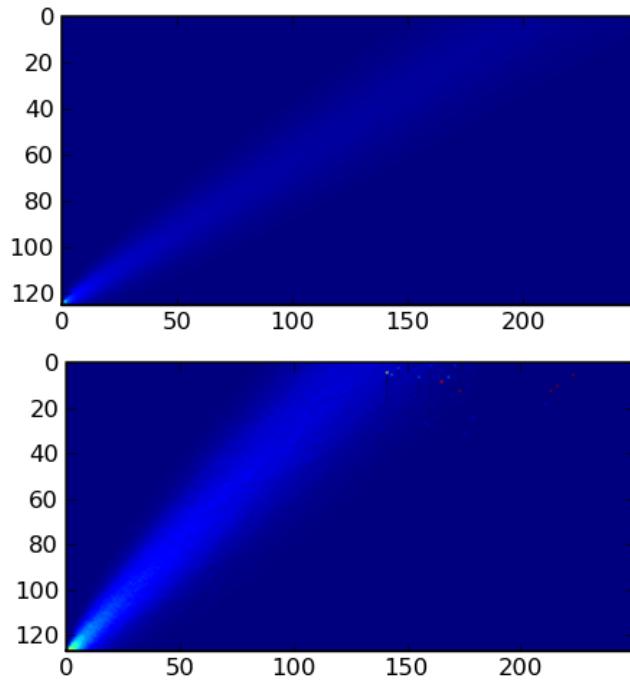


Figure 1: Density Evolution, Top = partial differential equation, Bottom = Monte Carlo method. X-Axis is time, Y-Axis is potential and should go from 0 to 1

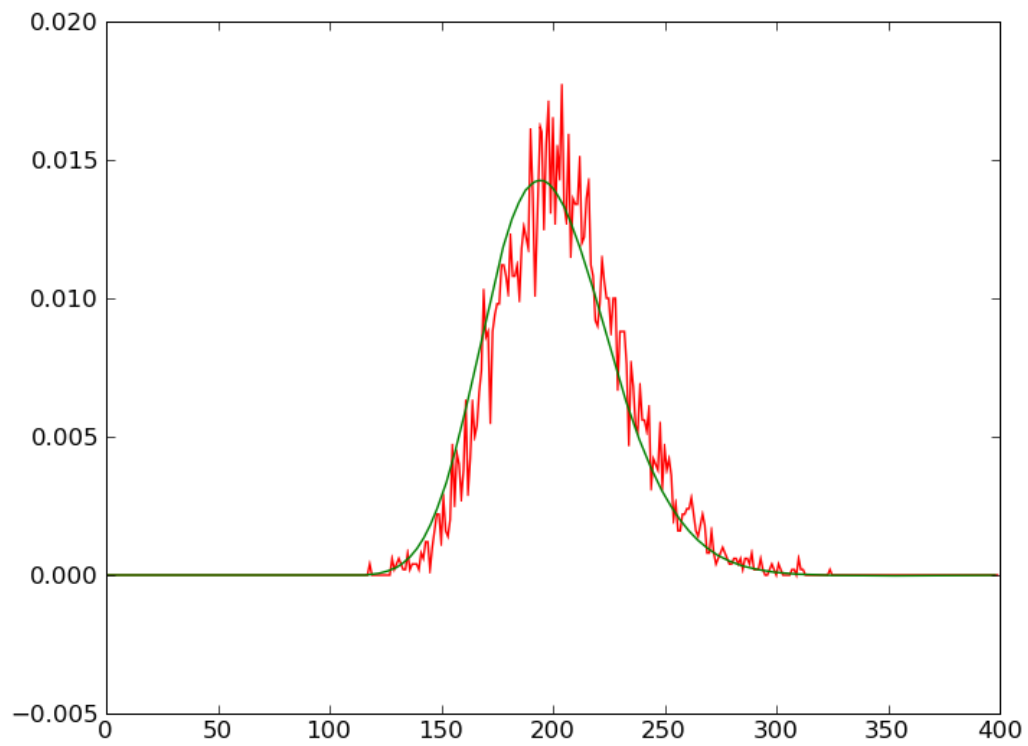


Figure 2: First Passage Time, Green = partial differential equation, red = monte carlo, x-axis is time, y axis is probability.

## 4.4 Conclusion

Not all of the initial Project Goals were reached to my full satisfaction. We did implement an Integrate and Fire neuron, and a method to fit the parameters, however we did not get as far as actually fitting real experimental data. None the less useful code has been produced and solid numerical techniques (Solving Partial Differential Equations) were learnt, and I consider the lab rotation to be successful.

## References

- [1] L. Paninski, J. W. Pillow, and E. P. Simoncelli. Maximum likelihood estimation of a stochastic integrate-and-fire neural encoding model. *Neural Comput*, 16(12):2533–2561, Dec 2004.
- [2] W. Press, S. Teukolsky, W. Vetterling, and B. Flannery. *Numerical Recipes in C*. Cambridge University Press, Cambridge, UK, 2nd edition, 1992.