

# Mitigating Blurring Artifacts in 3D Snapshot CEST MRI through Tailored Flip Angle Train Optimization

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**INTRODUCTION** In Chemical Exchange Saturation Transfer (CEST) MRI measurements, one challenge is to measure prepared longitudinal magnetization fast and precisely. However, the readout itself alters the prepared magnetization during acquisition, leading to blurring effects. In the spiral-centric-reordered 3D GRE snapshot [1], the prepared magnetization decays towards the steady state with the T1-Look-Locker-decay rate leading to blurring that affects image intensity, quality and contrast. To reduce this effect, we optimized a sequence with variable flip angle (vFA) using the MR-zero framework [2] with a fully differentiable Phase Distribution Graph [3] simulation to achieve a better estimation of the prepared magnetization.

**METHODS** To simplify the optimization problem, an inversion recovery sequence (TI=3s) was used as CEST surrogate during the training. The image loss was calculated based on the magnitude of the normalized magnetization prepared image. The GRE Snapshot sequence parameters are the following: matrix: 96x96x4, FOV: 200x200x20 mm<sup>3</sup>, TE: 3.2ms, TR: 5.1ms, spiral elongation factor: 0.5, bandwidth: 500Hz/pixel. For comparison of the vFA sequence, a constant flip angle of 5° (cFA 5°) was used for 384 repetitions. The target of the optimization process is a fully segmented image, where every k-space line is prepared individually. For measurement close to ideal state, an 8-shot sequence was used due to measured time vs. sharpness compromise.

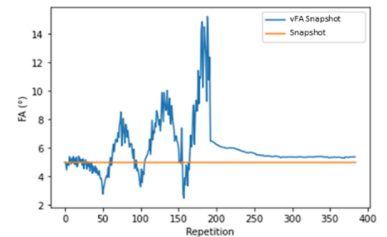
The tailored vFA train was subsequently combined with the low power multi-pool CEST protocol [4,5], with saturation at B<sub>1rms</sub>=0.9  $\mu$ T at 56 different frequency offsets. Signal simulations and optimization were performed using the Phase Distribution Graph algorithm [2,3], using brain data generated from the BrainWeb [6] database. Two healthy subjects were scanned after written informed consent and under approval of the local ethics committee, at a MAGNETOM Prisma 3T scanner (Siemens Healthcare GmbH, Erlangen, Germany).

**RESULTS** The vFA pattern is shown in Figure 1. With varying the flip angles the measurement of a prepared magnetization can be improved as shown exemplary for one slice in Figure 2. Sharper images, a lower RMSE and higher SSIM can be achieved using vFA. The difference images to the measured 8-shot sequence show a clear reduction of relaxation effects. This also translates to the CEST measurement where better contrast is achieved and finer structures are resolved (red arrows, Figure 3). The profile plot in Figure 3g reveals especially sharper and darker minima, an indication for reduced image blurring.

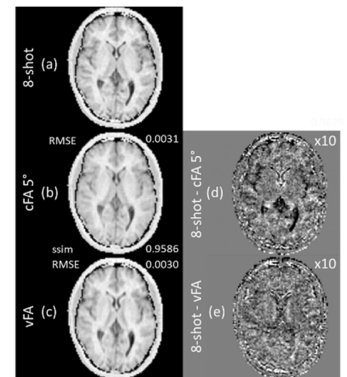
**DISCUSSION & CONCLUSION** Here, we demonstrated the removal of T1 Look-Locker-blurring by a flip angle optimization for a 3D GRE snapshot sequence as commonly used for CEST MRI. Compared to previous published flip angle shapes [7], we found new k-space-reordering-tailored patterns reducing image blurring. This potentially allows us to further increase flip angle and number of slices for higher signal and more coverage within one snapshot CEST readout. An improved visibility of CEST features is especially important for fast high-resolution CEST in pathologies.

## REFERENCES

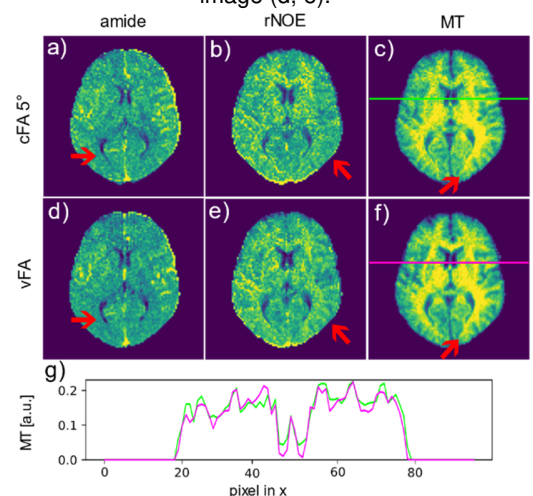
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**Fig. 1:** Constant and tailored flip angle train. Structures emerge due to LL-decay and 3D reordering.



**Fig. 2:** (a) 8-shot snapshot; (b) snapshot with constant FA of 5°; (c) vFA snapshot, difference image (d, e).



**Fig. 3:** Amide (a,d), rNOE (b,e) and MT (c,f) CEST maps for cFA 5° and vFA. Profile plot (g) of MT image intensity along lines defined in c) and f)