

Quasi-steady-state (QUASS) Reconstruction-empowered T_1 Normalization in Apparent Exchange-dependent Relaxation (AREX) Analysis – Application to a Brain Tumor Patient at 3 Tesla

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INTRODUCTION: The apparent exchange-dependent relaxation (AREX) analysis has been proposed as an effective method for correcting T_1 contributions in CEST quantification (1). However, it has been recognized that AREX T_1 correction is challenging when CEST scans are not performed under equilibrium conditions (2). This study aimed to test whether quasi-steady-state (QUASS) reconstruction could enhance the accuracy of the AREX metric under common non-equilibrium scan conditions. We evaluated QUASS CEST and AREX MRI in both phantom studies and a brain tumor patient.

METHODS: We collected images from an 100mM l-carnosine phantom with different T_1 values and a brain tumor patient at 3T whole-body MAGNETOM Prisma scanner (Siemens Healthineers). The MRI parameters for the study were: $B_1 = 0.7$ uT, offset frequencies from -5 to 5 ppm with increments of 0.125 ppm, saturation duration and relaxation delays of 1.5/1.5 sec. For the brain tumor patient, imaging readout time = 547 ms, TE = 33 ms, FOV = 220 × 220 mm², in-plane matrix = 110 × 110, the number of slices = 8, interleaving slice ordering, slice thickness = 5 mm with 25% slice gap, with fat suppression, 1 average, readout bandwidth = 1976 Hz/pix, and total imaging time is 4 min 50 sec. The CESTR was calculated from the asymmetry analysis, as $CESTR^{app,QUASS} = \frac{I_0^{app,QUASS}(-3.5 \text{ ppm})}{I_0^{app,QUASS}} - \frac{I_0^{app,QUASS}(+3.5 \text{ ppm})}{I_0^{app,QUASS}}$, and AREX was calculated as $AREX^{app,QUASS} =$

$R_{1w} \cos^2 \theta \cdot \left(\frac{I_0^{app,QUASS}}{I_0^{app,QUASS}(+3.5 \text{ ppm})} - \frac{I_0^{app,QUASS}}{I_0^{app,QUASS}(-3.5 \text{ ppm})} \right)$. The QUASS CEST images were reconstructed as published previously (3).

RESULTS and DISCUSSION: In Fig 1, the measured T_1 were 2.80 ± 0.06 , 1.30 ± 0.02 , and 0.85 ± 0.04 sec for MnCl₂ concentration of 0, 15, and 30 μ M. Although $CESTR^{app}$, $CESTR^{QUASS}$, and $AREX^{app}$ showed dependence on manganese chloride concentrations, $AREX^{QUASS}$ had little dependence on T_1 variation. The effect of T_1 on CEST and AREX peaks was tested with the generalized linear regression model (Fig 2). Specifically, we have $CESTR^{app} = 1.97 + 0.38 \cdot T_1$, $CESTR^{QUASS} = 1.23 + 1.66 \cdot T_1$, and $AREX^{app} = 3.81 - 0.90 \cdot T_1$. In comparison, the solution form QUASS AREX had no significant correlation with T_1 , and we had $AREX^{QUASS} = 3.88 - 0.13 \cdot T_1$ ($P = 0.16$). In Fig 3, QUASS AREX showed (red contour) smaller estimated tumor size than the apparent CESTR (black contour). The T_1 value in the black contour area was 1.4 ± 0.1 sec.

CONCLUSION: We demonstrated that AREX analysis benefits from the equilibrium CEST effect reconstructed by QUASS, resulting in improved T_1 correction.

REFERENCES: [1] Zaiss M, *et al.* Neuroimage 2015;112:180-188. [2] Sun PZ. J Magn Reson 2021;329:107022. [3] Kim H, *et al.* Magn Reson Med 2022;87(2):810-819.

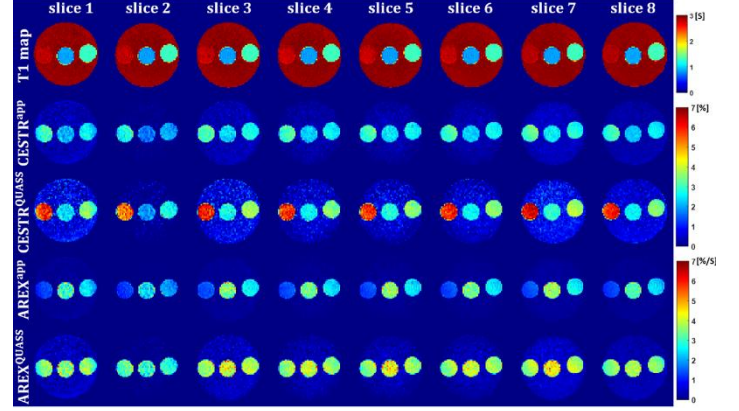


Fig 1. Experimental demonstration of T_1 map, apparent and QUASS CESTR maps, and apparent and QUASS AREX maps.

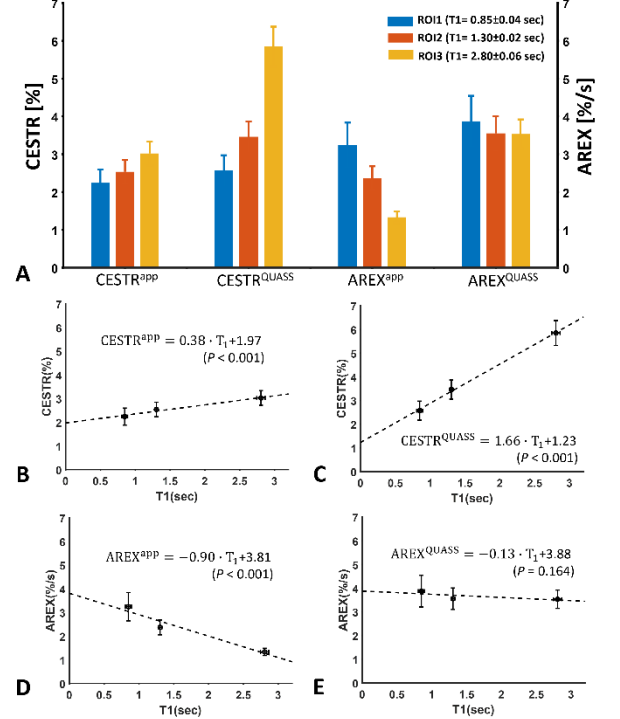


Fig 2. A. Comparison of apparent CESTR, QUASS CESTR, apparent AREX and QUASS AREX between different T_1 phantom. B-E. Correlation plots of CESTR and AREX (w/ and w/o QUASS) with T_1 values.

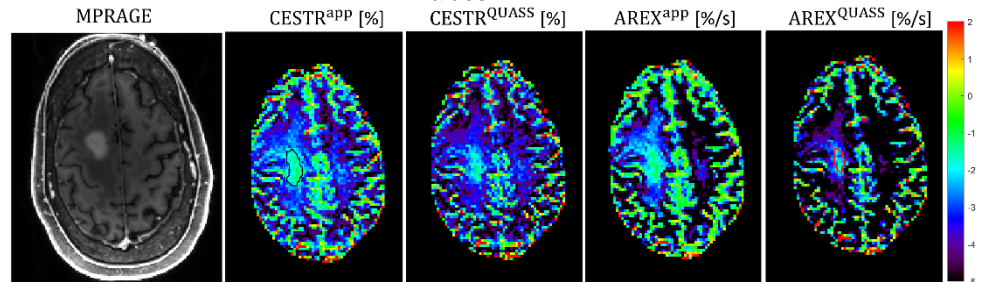


Fig 3. Comparison of CESTR and AREX (w/ and w/o QUASS) on a brain tumor patient.