Reproducibility Project for CS598 DL4H in Spring 2023

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1 Introduction

It is a central task in hospital operation and resources planning to reliably predict the length of stay for hospitalized patients, especially for those critically ill patients staying in the Intensive Care Unit (ICU). Our selected paper aims to build a novel and reliable deep-learning predictive model for the length of stay in the ICU(Rocheteau et al., 2021).

Historically, the two most popular models used for the length of stay prediction are LSTMs and Transformers due to the centrality of time series in the EHR (Sheikhalishahi et al., 2019; Song et al., 2018). More recently Temporal Convolutional Networks (TCN) were developed as a variation of CNN to handle sequential data (Bai et al., 2018). Our selected paper described a novel Temporal Pointwise Convolution (TPC) model, which is based on the combination of temporal convolution networks and pointwise (1x1) convolution to predict ICU length of stay. The TPC model is specifically designed to handle common challenges with EHR, such as skewness, irregular sampling, and missing data. In the paper, the TPC model significantly outperforms the commonly used LSTM and Transformer models for ICU length of stay prediction.

2 Scope of reproducibility

We aim to reproduce the finding that the novel TPC model based on temporal convolution networks combining with pointwise convolution will have lower mean absolute deviation (MAD) and mean absolute percentage error (MAPE) in predicting ICU length of stay than LSTM and transformer models trained on eICU database.

2.1 Addressed claims from the original paper

- The TPC model significantly outperforms the commonly used LSTM and Transformer models for ICU length of stay prediction by margins of 18-68%.

- The use of mean-squared logarithmic error (MSLE) loss function instead of commonly used mean squared error (MSE) loss will lead to better model performance, as the former handles positively-skewed labels more naturally.

- The data processing pipeline developed by the authors for the eICU and MIMIC-IV databases could mitigate the common problems of sparsity and missing data in the EHR and the approach is generalizable to other EHR databases.

3 Methodology

3.1 Model descriptions

Initially, for every timepoint *t*, there are two channels per time series feature: F feature values $x_t^{'} \in \mathbb{R}^{F\times 1}$ and their corresponding decay indicators $x_t^{''} \in \mathbb{R}^{F\times 1}$. The decay indicators tell the model how recently the observation $x_t^{'}$ was recorded. As we pass through the layers of model, we repeatedly extract trends and inter-feature relationships.

Author used stacked TCNs to extract temporal trends in the data. TCNs are a subclass of CNN that evolve over the time dimension (Figure 2a). They operate on two key principles: the output is the same length as the input, and there can be no leakage of data from the future(Bai et al., 2018). The paper made a unique adjustment to not allow weights sharing across features, thus weight sharing is only across time. The philosophy is that the features from EHR differ sufficiently in their temporal characteristics to warrant specialized processing.

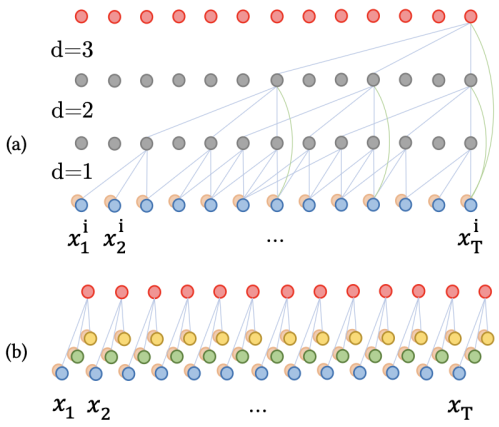

Figure 2: (a) Temporal convolution with skip connections (green lines). Each time series, i (blue dots) and their decay indicators (pale orange dots) are processed with independent parameters. (b) Pointwise convolution. There is no information sharing across time, only across features (blue, green, yellow dots).

Pointwise convolution is traditionally used to reduce the channel dimension when processing images. It can be conceptualised as a fully connected layer, applied separately to each timepoint (Figure 2b). Contrary to TCNs, in the paper weights are shared across features in pointwise convolution to obtain interaction features, while there is no information transfer across time.

Finally, the TPC model combines TCNs and pointwise convolution in parallel (figure 3). In a TPC layer the temporal output is combined with the skip connections first, then concatenated with the pointwise output after latter has been broadcasted. The full model has N TPC layers stacked sequentially. After N layers, the output h_t^N is combined with static features $s \in \mathbb{R}^{S\times 1}$, and a diagnosis embedding $d^* \in \mathbb{R}^{D\times 1}$. Two pointwise layers are then applied to obtain the final predictions. The model also enables flexible selection of temporal receptive field sizes (independently for each feature) because of the skip connections. Batch normalisation and dropout are used throughout to regularize the model.

Of interest, the author selected mean squared log error (MSLE) as the loss function in training instead of the commonly-used mean squared error (MSE) loss. This choice aims to address the positive skew in LOS.

3.2 Data descriptions

The paper used the eICU Collaborative Research Database v2.0 and MIMIC-IV v0.4 Database, both available through PhysioNet. We selelcted eICU

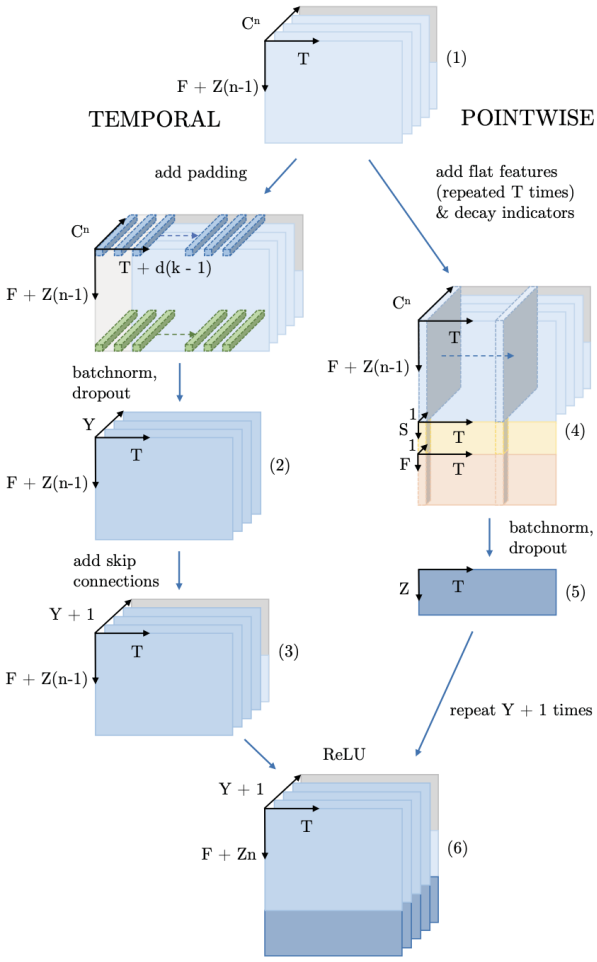

Figure 3: The n_{th} TPC layer. Left-sided padding (off-white) is added to the temporal side before each feature is processed independently. On the pointwise side, flat features (yellow) and decay indicators (orange) are added before each convolution.

data for the purpose of replication, and statistic overview of the eICU data is listed in table 1.

eICU data are first downloaded and build into postgreSQL database following steps in: https://github.com/MIT-LCP/eicu-code/tree/master/build-db/postgres. A customized SQL file provided by the paper is subsequently run to generate all input files. Of note, due to limitation of computation resources, we only selected eICU database and utilized 50% of hospital stays in the training of model. We find this compromise to be acceptable as the performance superiority of TPC model is already evident when using 50% training set as demonstrated in table 12 of original paper.

3.3 Hyperparameters

The paper already performed comprehensive hyperparameters searches by running total 75 trials to fine tune total 11 hyperparameters (eg., batch size,

Table 1: eICU Cohort Summaries

	eICU
Number of patients	118,535
Train	82,973
Validation	17,781
Test	17,781
Number of stays	146,671
Train	102,749
Validation	22,033
Test	21,889
Gender (% male)	54.1%
Age (mean)	63.1
LoS (mean)	3.01
LoS (median)	1.82
Number of input features	104
Time series	87
Static	17

learning rate). We used the best hyperparameters values of each model provided by the author (Table 2).

Table 2: Summary of model hyperparameters

Model	Layers	Batches	Epochs
TPC	9	32	15
CW-LSTM	2	512	25
LSTM	2	512	6
Transformer	6	32	14
Point. Only	9	32	15
Temp. Only	9	32	15

3.4 Implementation

We reused the existing codes by the author and tailored it to be run on Google Colab (https://github.com/EmmaRocheteau/TPC-LoS-prediction). We made several adjustment to fix bugs due to package and version incompatibility. We also write codes for the models to be run on 50% of training data set. We write new codes for the new experiments not designed in the paper.

3.5 Computational requirements

The eICU database preprocessing was performed on a M1 MacBook pro but unfortunately had to be done under a x86 architecture due to package compatibility issue, therefore significantly limited CPU performance. The whole data preprocessing step took 14 hours. All experiments are run on Goolge ColabPro+, which has the advantage of background execution and premium GPU support comparing to its free version. The TPC, transformer and traditional LSTM models typically require up to 3GB of CPU RAM and up to 3GB of GPU, while cw-LSTM model requires up to 30GB of GPU. All experiments combined consumed about 400+ compute units on ColabPro+, of which the two CW-LSTM models used 100 compute units each. All experiments are run on Tesla T4 GPU (standard GPU acceleration in ColabPro+), with the exception of the two CW-LSTM which are run on NAVIDA A100 GPU (premium GPU acceleration in ColabPro+) due to it's much heavier consumption of computing resource. A summary of computing times of different models are listed in Table 3.

Table 3: Computational times for different models

Model	Hours
TPC	3
LSTM	0.75
CW-LSTM	4.8
Transformer	2.2
Point. Only	1.8
Temp. Only	2
TPC(no skip)	2
TPC (no diag)	3
TPC(MSE)	3
Transformer(MSE)	2.2
LSTM(MSE)	0.75
CW-LSTM(MSE)	4.8

4 Results

Overall, we are able to replicate the main findings in the original paper and demonstrate the superior performance of TPC model in the task of ICU LOS prediction.

4.1 Model performance benchmark and ablation studies

Detailed results are listed in Table 4. All models are trained on 50% of training set. All evaluation metrics are calculated on testing set. Our results are largely consistent with those from paper, with TPC model outperforms the channelwise-LSTM (CW-LSTM), LSTM and Transformer models for ICU length of stay prediction by margins of 35%. Consistent with the paper, other than TCP the best performing model is Transformer.

Results from ablation studies are shown in Table 5. The temporal-only model is superior to the pointwise-only model, but neither reaches the performance of the TPC model. Removing the skip connections reduces performance by 7%. Interestingly and surprisingly, we found that the exclusion

Table 4: Comparison with results from paper. MAD: mean absolute deviation; MAPE: mean absolute percentage error; MSE: mean squared error; MSLE: mean squared logarithmic error;

Source	Model	MAD	MAPE	MSE	MSLE	R^2	Kappa
Paper	TPC	1.95±0.02	72.0±3.1	23.8±0.4	0.87±0.03	0.19±0.01	0.51±0.01
	CW-LSTM	2.40±0.01	123.4±0.7	26.5±0.1	1.48±0.01	0.1±0.0	0.31±0.00
	LSTM	2.41±0.01	129.9±1.9	26.2±0.2	1.52±0.00	0.11±0.1	0.31±0.01
	Transformer	2.39±0.00	120.1±0.6	26.5±0.1	1.48±0.00	0.10±0.0	0.31±0.00
Replication	TPC	1.74	41.86	22.02	0.47	0.37	0.67
	CW-LSTM	2.68	123.54	32.25	1.49	0.08	0.30
	LSTM	2.67	133.17	31.46	1.54	0.10	0.32
	Transformer	2.65	117.45	32.19	1.47	0.08	0.30

Table 5: Ablation studies results

Model	MAD	MAPE	MSE	MSLE	R^2	Kappa
TPC	1.74	41.86	22.02	0.47	0.37	0.67
Point. Only	2.77	30.98	142.71	1.53	0.12	0.40
Temp. Only	1.85	53.97	23.30	0.62	0.34	0.64
TPC(no skip)	1.87	59.69	22.63	0.68	0.36	0.63
TPC(no diag)	1.66	43.15	21.05	0.45	0.40	0.70

of diagnoses does not seem to harm the mode. All above findings are described in the original paper.

4.2 Model performance when trained with MSLE vs MSE

Results are listed in Table 6. Consistent with findings from the paper, we can see that using the MSLE (rather than MSE) loss function leads to significant improvements in all models, with large performance gains in MAD, MAPE, MSLE and Kappa.

4.3 eICU data preprocessing pipeline analysis

The data processing pipeline developed for eICU database in the paper involves several steps:

- **Data Cleaning:** A series of data cleaning methods such as imputing missing values, removing outliers, and normalizing the data are used to resolve the missing values, outliers, and inconsistencies issues in raw data.
- **Feature Engineering:** This step extracts static and temporal features from the data, such as demographics, vital signs, and lab test results. And also create new features, such as the difference between consecutive measurements, to capture the temporal dynamics of the data.
- **Temporal Alignment:** This step align the data in a consistent manner using fixed-length non-overlapping windows (e.g., 4-hour windows). This allows the model to analyze the data within a consistent time frame and capture temporal patterns.
- **Data Transformation:** This step transforms the data to make it suitable for the TPCN model. It uses one-hot encoding for categorical variables and normalize the continuous variables to have zero mean and unit variance.
- **Data Splitting:** The dataset is split into training, validation, and test sets. This allows us to train the model on one set of data, tune the hyperparameters using the validation set, and evaluate the model's performance on the test set.

4.4 Additional results not present in the original paper

Intrigued by the surprising finding that the exclusion of diagnosis codes as input features actually improves TPC performance, we performed similar analysis to the rest of models without diagnosis codes as input (Table 7). After skip diagnosis, rest of input variables include vital signs, nurse observations, machine logged variables among other time series data. In consistent with TPC model, we observed that exclusion of diagnosis does not seem to harm any models. In fact, there is minor performance improvements (about 1%) in all models but less than that seen in TPC model (7% improvement in MAD).

Table 6: Comparision when using MSLE vs MSE

Loss function	Model	MAD	MAPE	MSE	MSLE	R^2	Kappa
MSLE	TPC	1.74	41.86	22.02	0.47	0.37	0.67
	CW-LSTM	2.68	123.54	32.25	1.49	0.08	0.30
	LSTM	2.67	133.17	31.46	1.54	0.10	0.32
	Transformer	2.65	117.45	32.19	1.47	0.08	0.30
MSE	TPC	2.21	111.13	22.13	1.90	0.37	0.55
	CW-LSTM	2.83	211.11	30.72	1.87	0.12	0.28
	LSTM	2.93	249.57	30.73	2.06	0.12	0.25
	Transformer	2.89	241.17	30.36	2.00	0.13	0.26

5 Discussion

5.1 TPC Outperforms LSTM and Transformer Model

The experimental results obtained in our study support the hypothesis that the TPC model significantly outperforms the commonly used LSTM and Transformer models for ICU length of stay prediction. Our findings align with the original paper, demonstrating that the TPC model outperforms other models, such as the channelwise-LSTM (CW-LSTM), LSTM, and Transformer models, by a margin of 35%. The Transformer model was found to be the second-best performing model, consistent with the paper's claims. Additionally, our ablation studies revealed similar trends to the original paper, with the temporal-only model outperforming the pointwise-only model, but neither reaching the performance of the TPC model. Removing skip connections led to a 7% reduction in performance, and interestingly, excluding diagnoses did not negatively impact the model's performance. These findings indicate that the original paper is largely reproducible, and our study corroborates the paper's claims regarding the effectiveness of the TPC model for predicting ICU length of stay.

5.2 MSLE Loss Function Outperforms MSE

The experimental results from our study strongly support the second hypothesis that using the MLSE loss function instead of the commonly used MSE loss function leads to better model performance. As presented in Table 6, the application of the MSLE loss function resulted in significant improvements in all models across various performance metrics, including MAD, MAPE, MSLE, and Kappa. This finding is consistent with the original paper's claims and demonstrates the ability of the MSLE loss function to better handle positively-skewed labels. Our results suggest that the original paper is reproducible, validating the advantages of using the MSLE loss function over the traditional MSE loss function in predicting ICU length of stay. The consistency between our study and the original paper supports the robustness of the conclusions and indicates that there are no factors impeding the reproducibility of the paper's results.

5.3 Generalizability of Data Processing Pipeline

The data processing pipelines designed for eICU and MIMIC-IV effectively address the common challenges of sparsity and missing data in EHRs, supporting the hypothesis that this approach is generalizable to other EHR databases. The reasons for this generalizability are as follows:

- **Common Data Types:** Most EHR databases contain similar types of data, including patient demographics, vital signs, laboratory results, medications, diagnoses, and other clinical variables. The extraction and preprocessing steps in both pipelines address these data types, making them applicable to other databases containing similar information.

- **Data Preprocessing Techniques:** The data preprocessing methods employed, such as imputing missing values, standardizing units of measurement, and converting categorical variables to numerical representations, are widely applicable across various EHR databases.

- **Feature Engineering:** The process of creating meaningful features from raw data is a critical aspect of any machine learning project. The feature engineering steps in both pipelines can be adapted to different databases, as long as the necessary clinical knowledge is available to guide the transformation of raw data into relevant features.

Table 7: Comparison when exclude diagnosis code for all models

Contain diagnosis	Model	MAD	MAPE	MSE	MSLE	R^2	Kappa
Yes	TPC	1.74	41.86	22.02	0.47	0.37	0.67
	CW-LSTM	2.68	123.54	32.25	1.49	0.08	0.30
	LSTM	2.67	133.17	31.46	1.54	0.10	0.32
	Transformer	2.65	117.45	32.19	1.47	0.08	0.30
No	TPC	1.66	43.15	21.05	0.45	0.40	0.70
	CW-LSTM	2.65	128.53	32.20	1.48	0.08	0.30
	LSTM	2.69	134.13	32.17	1.57	0.08	0.29
	Transformer	2.63	121.56	31.73	1.47	0.096	0.31

- **Temporal Alignment:** Handling the temporal nature of EHR data is a common challenge across different databases. The alignment and interpolation techniques used in both pipelines can be applied to other EHR databases that also contain irregularly sampled time series data.
- **Data Normalization:** Normalizing the data to ensure that features have the same scale is a standard step in many machine learning projects. The normalization techniques used in both pipelines can be easily applied to other EHR databases.
- **Data Splitting:** The practice of dividing data into training, validation, and testing sets is a standard procedure in machine learning projects and can be easily applied to other EHR databases.

5.4 Additional results not present in the original paper

When diagnosis info were excluded in the input data, we observed an universal improvements in performance across all models. This could be because the relevant diagnoses for predicting LoS e.g. Acute Heart Failure Exacerbation, are discernible from other information in time series alone e.g. BNP, Troponin, Lasix etc.

5.5 Reflection of the original paper

Our project re-demonstrated the potential advantage of TPC model in the task of ICU LOS prediction. We feel the claims from the paper are well supported. Of note giving the constrain on budget, we had to compromise on using 50% of training set though find it to be a reasonable compromise.

5.6 What was easy

The original codes are well written and documented, along with a complimentary video presentation that make things easier to re-implement. It took some effort and time to process eICU data into PostgreSQL database then into input files, but overall it's not bad. The computing resource and running time is manageable using the paid Google ColabPro+, though did cost us 50 USD.

5.7 What was difficult

It took us quite some time to debug several minor issues in the existing codes (e.g., one bug is related to dropping the last batch in testing set when the size is 1). Decent amount of efforts are made to ensure software package compatibility among different python versions, default packages in Colabs and required higher Version of CUDA toolkit for using NAVIDA A100. The total running times of all experiments are quite long, especially wiht the two CW-LSTM models which consumed 40% of total computing units combined. In addition, the challenge in installing all required packages on a M1 MacBook Pro proven to be more challanging then one would think, and can only be done in a virtual environment using x86 architecture at the significant expense of performance.

5.8 Recommendations for reproducibility

Several commonly encountered questions were raised in the clsoed issues under original github repo.

6 Communication with original authors

We submitted tickets in github repo (https://github.com/EmmaRocheteau/TPC-LoS-prediction/issues/10).

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