

Characterization study of the human skin

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Abstract— In this paper, a system, consisting a sensor mounted on a rotating axe around a stepper motor in order to calculate a polar diffusion diagram of skin sample which is based on its reflectance rate, is presented. Moreover, a spectrophotometer is used to gather the data of the tissue as a spectrum in visible wavelengths. Once, signal-to-noise ratio computation is performed, its data feed a processing system to characterize each sample and then, a cross-validated recognition task, achieving 100% accuracy and legitimizing the biometric application of this method, is executed.

I. INTRODUCTION

Skin is the largest organ of the body and the most discriminative part of the recognition task of different human beings. Its inner characteristics of humidity determines the quality of the skin pores [1], and the skin chromophores constitutes the main element of interaction with light [2]–[4]. The melanin rate is used to make a barrier to avoid harmful exposure of electromagnetic radiations in the environment [5], and the oxy-hemoglobin which can be found in veins can inform suffocation or breath irregularities of the human being [6]. Moreover, the blood flow can be analyzed in order to determine the heartbeat of the body, among other uses [7]. The skin has very specific properties studied in different fields as in cosmetics (how to make more efficient products that penetrate or protect the skin [8]), computer graphics (in order to emulate realistic tissues [9]), and medicine to evaluate skin irregularities, and human health [10].

Optical analysis of human skin is a non-invasive way to observe skin physiology, morphology and composition. For instance, white light can be used to obtain a spectrum which is useful to analyze the skin and also all the quantitative variations related to skin components. Reflective properties are used to identify and recognize humans by presenting a part of their skins, as in biometrics, and to detect spatially distributed irregularities such as veins or abnormally vascularized regions, melanomas or malign tumors. In fact, different skin tissues have distinct or unique reflectance pattern which helps to differentiate different skin conditions [2], [11], [12]. Hence, the idea behind the diffuse reflectance is that light reflected from a target tissue provides information on the quantity of melanin pigment and its chemical structure, oxygenated and deoxygenated hemoglobin, carotene, and also the chemicals [13], [14]. This information, based on biochemical composition and the structure of the tissue, does not only indicate the presence and location of a pathology, but also indicates where it has originated, also contributes to find

the most appropriate treatment to cure it by observing the characteristics of the tissue if it is needed [11], [12].

Those characteristics, and the recent developments in analytical techniques of the skin, made us think about what kind of system should be envisaged to identify individuals in terms of biometrics. Thus, analyzing diffusion diagram of the skin, and the spectrum of skin diffusion by using certain wavelength is proposed.

In the next section, different physical aspects of the interaction of light with skin are introduced. Then the measurement system is described and characterized. In the second section, samples, measurement protocol and results are presented. In the last section before conclusion, the obtained results are analyzed and discussed in terms of efficiency for biometric applications.

II. DEVELOPMENT

A. Physical aspects, skin-light interaction

Spectroscopy is a non-invasive method which allows to capture physiological and biochemical data of the tissue [15], [16]. Photons beam directed to the skin by a light source can be scattered, absorbed, reflected or transmitted. Skin contains various chromophores and rough surface [17]. Thus, light directed to a part of skin tissue is affected by all above mentioned phenomena.

Each person has a different structure of skin, its thickness, distribution and capacity of various chromophores [3]. Therefore, input light directed on the skin is transformed in different ways for each person. Chromophores present in the skin, which have a major contribution to the light transformation, are hemoglobin, melanin, and others [11]. Each of them causes distinctive effects, which varies depending on the wavelength. The chromophores mainly absorb or scatter the incident light, while for water, lipids, and proteins, especially collagen, absorption is low and scattering is high [18]. Melanin, which accumulates in basal layer of epidermis, is produced by melanocytes and is the only pigment which affects the transmittance of human epidermis [5]. Melanin absorbs waves in spectrum between 250 and 1200 nm. The absorption intensity heightens towards shorter wavelengths and it is irregular. Consequently, most of short wavelengths are absorbed or retransmitted in epidermis and do not reach deeper skin layers, contrary to long wavelengths [5]. Dermis optic features differ more from of epidermis. The

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optics properties are determined by blood-borne chromophores, mainly hemoglobin. It transports oxygen from lungs to the remaining tissues through blood vessels and returns carbon dioxide to lungs. The absorption of hemoglobin is present in the spectral range from 390 nm to 1000 nm and has few peaks depending whether the oxygen is transported. There are two peaks for hemoglobin without oxygen with maxima at 550 nm and 760 nm, and two with oxygen with maxima are at 548 nm and 576 nm [19].

Pathways of the incident light in skin are illustrated in Fig.1 and absorption coefficient of different chromophores is represented as a function of wavelength in Fig.2. Such a complex process of reflecting, scattering and absorbing of the electromagnetic radiations delivered by a light source, should affect the individual features of the skin spectra.

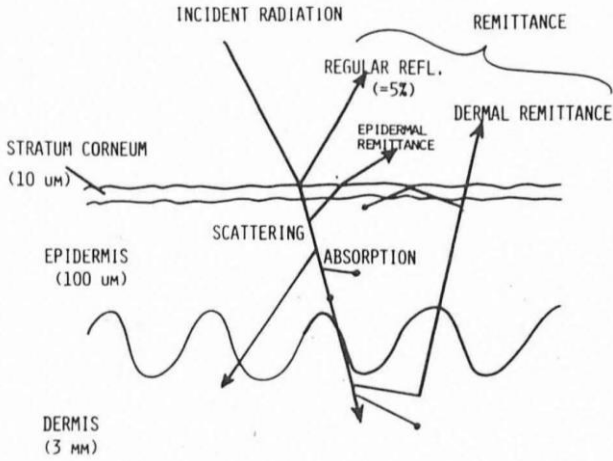


Fig.1 : Schematic diagram of optical pathways in human skin [11].

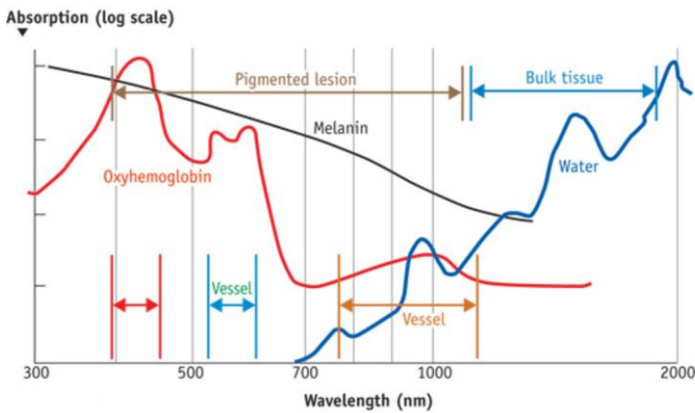


Fig.2: Absorption coefficients of different chromophores as a function of wavelengths [20]

Scattering relies upon coefficient a , depth of the scattering centers, incident wavelength λ , and illumination angle θ . In the Rayleigh model, the effective section for each solid angle is proportional to $a^6(1 + \cos^2 \theta)/\lambda^4$. For bigger particles, a more relevant theory based on Mie's work gives intensity

meters which are no longer isotropic, and the scattering takes places further as bigger the particle size rise [21].

The objective is to estimate the phase function $f(\cos\theta)$, or angular distribution of intensity of light that skin scatters. This phase function is a probability density, related to g , the anisotropic factor defined as $g = \int f(\cos\theta)\cos\theta d(\cos\theta)$, with $\theta = \hat{s} \cdot \hat{s}'$, the angle between the incident direction of the wave, and direction of the scattered wave [21]. This anisotropic factor g quantifies anisotropic scattering, i.e. its inclination to be scattered in definite directions. Figure 3. summarizes those scattering theories (Rayleigh and Mie).

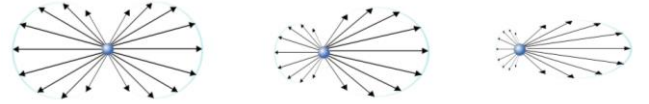


Fig.3: Radiation indicators for different kinds of scattering on a spheric particle, beam coming from left. Left, Rayleigh scattering; center, intermediate scattering (Rayleigh-Mie); right, Mie scattering, mostly forwards [22], [23].

For instance, $g = 0$ if scattering is perfectly isotropic, $g = 1$ if scattering is completely forwards (propagating without scattering). As a biological tissue, scattering goes forward in a general manner, with $0.8 < g < 0.98$, but a certain amount scatter backward. The study consisted of variations of energetic parameters, function of the angle of view, as represented in Figure 4.

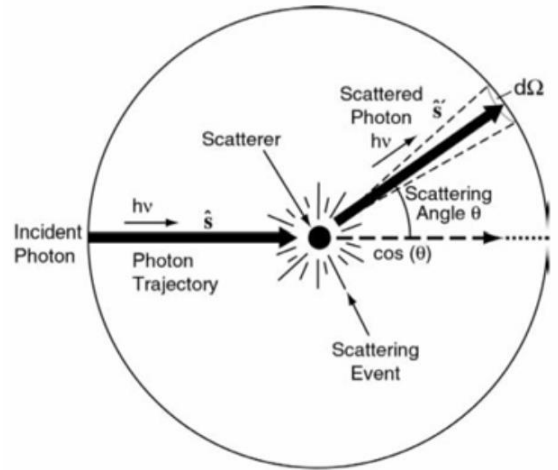


Fig.4: Definition of the incident direction \hat{s} , scattering trajectory \hat{s}' and scattering angle. Credits: Tuan Vo-Dinh [23]

Thus, a sensible surface of a photodiode is placed perpendicular to the incident wave (approximately spherical) also in order to conserve invariant of solid angle for each measurement. For instance, if the captured luminance is measured, the same solid angle is obtained for each measurement while the photodiode surface is placed in a same way, tangentially at the front of spherical wave. The captured flux shows up with the same solid angle, therefore, coherent

measurement is obtained with simple and fast calculations. The luminance in $W.m^{-2}.sr^{-1}$, which is pertinent and common parameter for our study, can be obtained, since the sensible surface of the sensor and solid angle are constant for each angle.

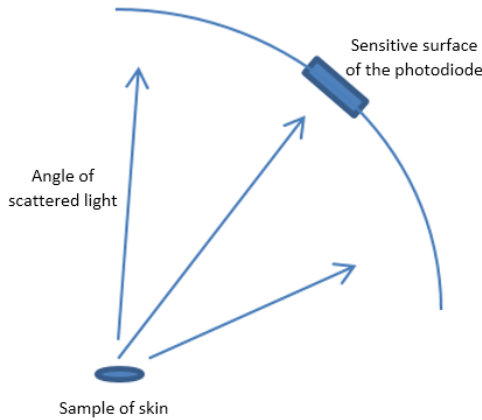


Fig. 5: Position of the photodiode

The choice of fixing the photodiode one extremity of mobile arm while the other extremity is relied on stepper motor. Fig. 5 shows the sweeping mechanism which is able to rotate at several angles, measures the diffusion for each different angle. Then the signal is transmitted into the acquisition chain.

B. Instrumental aspects

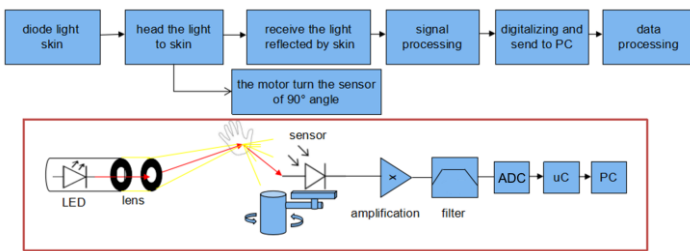


Fig.6: Descriptive diagram and schematic of the system, consisting of the photodiode mounted on stepper motor fixed in a box, in order to rotate the photodiode.

As it is seen in Fig. 6, the device is placed inside of a box in order to isolate the external light which can disturb the measurement. Light beam, emitted by LED and converging by lens in order to be focused on a skin sample. Photons stream, namely light beam, directed on the skin by a light source can be scattered, absorbed, reflected or transmitted.

REPRISE TRADUCTION

Reflected light is captured by the sensor, converted into electrical current and amplified. The sensors are attached to a mechanical arm rotated by a stepper motor. This robotic arm is provides rotational movement at several angles during the measurement. The signal, acquired by the photodiode, is sampled by the microcontroller (METTRE LES VARIABLES

QU'ON PEUT MODIF), and is sent through a serial port to a computer. Saved and processed data are used as training examples of a learning algorithm in order to implement a recognition tool.

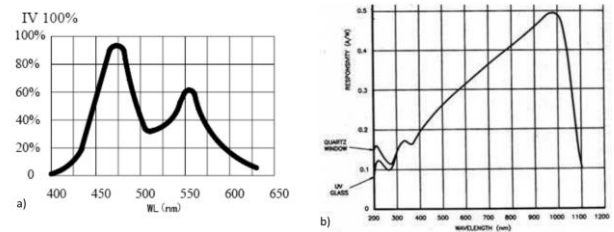


Fig.7: Spectral response of the emitting (a, 5050 LED) and receiving (b, OSD 35-7X CQ) components used for the experimentation.

A photodiode consists of an active p-n junction which is operated in reverse bias. When light falls on the junction, a reverse current flows which is proportional to the illuminance [25]. The linear response to light makes it a useful element in photodetectors for this application. In Fig. 7, spectral response of photodiode is shown. Spectral response is a ratio by the generated photocurrent to incident light power, expressed in $A.W^{-1}$ when used in photoconductive mode (DEFINIR). The wavelength dependence may also be expressed as a quantum efficiency, or the ratio of the number of photon-generated carriers to incident photons [26].

Incident light emitted by the LED has a certain range of wavelengths. The aim is to obtain the spectrum of light scattering as the output of the system. Incident light emitted by the LED, has a certain spectrum. The skin absorbs some more or less parts of the spectrum, which means the scattering, and reflect another part of the light. The reflected light is measured by a photodiode. Due to the characteristic of the photodiode, it is possible to capture certain band of wavelengths. In our case, a photodiode sensible to the near infra-red wavelengths [27], with closed environment in order to minimize as much as possible spurious light sources, is used. In fact, the signal produced by the photodiode is current, and it is needed to be converted into voltage, thanks to a [transimpedance] in order to make the data compatible with the microcontroller. This obtained voltage is directly correlated with the number of photons reaching the photodiode over its sensitive spectrum, in correspondence and sensing spectrum.

C. Recognition system characteristics



Fig. 8: Illustration of the skin sample area (inside the red circle) used for each subject, as input of the acquisition system.

Through the system described before, the photodiode sends a current for each step of the motor (ANGLE IS A STEP, A DEFINIR), and this current is converted into a digital number proportionally to its magnitude by an analog to digital converter (ADC). For each scanned backhand of each subject, a dataset entry is created while the scan process is performed, and stored in order to use as an input of k-nearest neighbor based recognition system [28]. Those data are associated to spectrums acquired with an GretagMacbeth Eye-One spectrophotometer, which is already calibrated with white object, as described in Fig. 9.

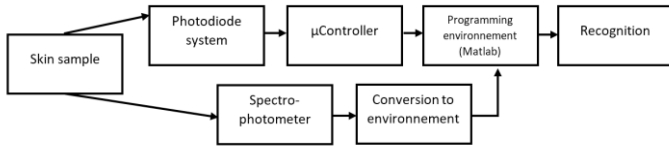


Fig. 9: Block-diagram of the recognition system. The skin sample is scanned at different time intervals in the system, and in the spectrophotometer.

When the dataset entry is created, several acquisitions are applied/ARE REALIZED for the same angle, which is related to a given angular position of stepper motor. (((Each measurement exhibit an offset which is removed by acquiring with turned-off emitter.))) ENSUITE ON PUET DIRE QU'ON FAIT LA SOUSTRACTION DES DEUX calibrated with an offset, and calculated with turned off emitter, in the system as well as for the multiple entries of each wavelength spectrum with the spectrophotometer. This process permits to measure the average and the standard deviation for different acquisitions, which provides a model representing multiple presentations of the subject, through the statistical (kppv) machine learning algorithm. It is important to emphasize that two processes are differentiated, respectively learning phase, consisting of data acquisition and storage as a function of polar scattering diagram and the light scattering, and the recognition phase, consisting of the acquisition of new data entry and finding the k nearest neighbors of this data entry, also determining the class of this vector in a supervised way (préciser le mode supervision et description, définir les distances). In order to validate this biometric application, the

recognition is validated with a cross-validated recognition task, and the results will be discussed in section IV.

III. EXPERIMENTATION

The device is tested on seven different subjects with different skin color, ((on a database composed on seven differents subject either Caucasian or African, remarkably discriminative colors (ajouter un tableau avec les gens et leur couleur de peau)) with apparent melanin concentration discrimination, as they are Caucasian to African, for the validation of the scattering spectrums. Via this protocol, the spectrums are obtained in Fig. 10, each point (lines) on these spectrums corresponds to the characteristic vectors used as the training examples feeding a pattern recognition tool (CoUPER PHRASE EN DEUX) containing k-nearest neighbors (k-NN) statistical approach for classification and regression in learning algorithm. This learning algorithm contributes to the individual identification, namely recognition, from acquired data.

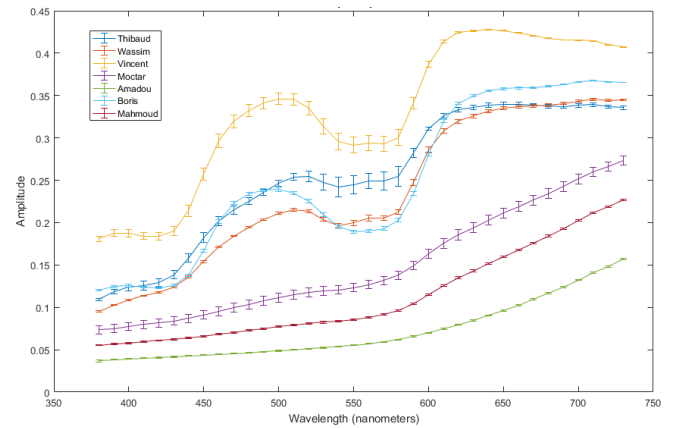


Fig. 10. Spectrum of skin samples acquired from back of right hand for the seven subjects

Besides, in order to observe variation of the spectrum due to the tissue humidity, measurement of dry and wet skin, among the seven people, we choose (either dry or humidify, ///) subjects is effectuated, using our system, as we can see in Fig. 11. (PELLICULE DE PEAU) The skin has been humidified by applying water on the back of the hand, resulting in a thin layer.

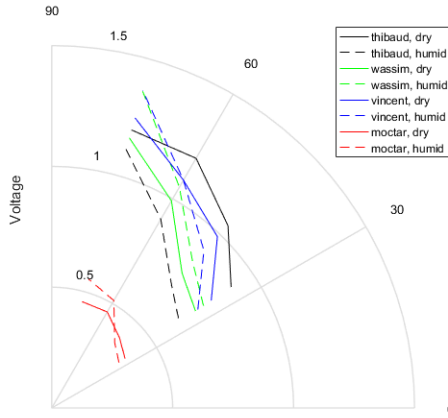


Fig. 11: Polar scattering diagram of subjects, continuous line represents dry skin measurements, dashed line represents humidified skin measurements.

Once [truc ont été faits], data was process by recognition system, computing a cross-validated task, achieving up to 100% accuracy [mot plus precis pour designer la reocnnaissance] as we can see in the Fig. 12.

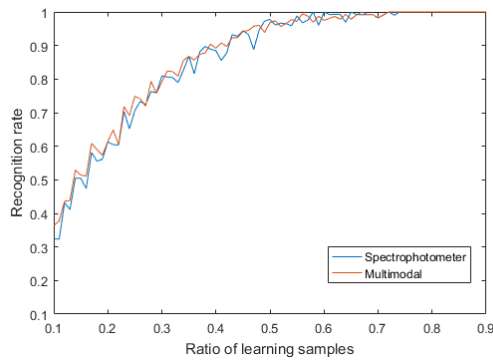


Fig. 12: Recognition rate for the two modalities of the recognition task. In blue, the recognition task was done with the spectrophotometer data, in red, all the data (with our system) was used. Only one angle is used in the algorithm.(is performed with spectrometer data, FAIRE GAFFE MULTIMODAL=VALISE)

IV. DISCUSSION

Although the scattering through the skin is discriminative for all the wavelengths measured with spectrometer, Fig. 10 show the difference deviation between the seven hands/people/subject.

The standard deviation of the values for each subject, is minor as the measurements are consistent from each other. The influence of noise. Indeed, errorbars in fig. 10 shows that each sample can be easily separated.

This permits an almost perfect recognition in the classification system, achieving a recognition rate of 100%. These results is obtained because there is a sufficient amount of data in learning set and the seven subjects presents very different skin properties (chromophores)

when sufficient amount of data is used in the learning set, and because of the seven test subjects whose chromophores are adequately distinctive.

Including sensor system data in the recognition process leads to an increased performance in classification process. However, the gain is not remarkably significant (A MODERER) as shown in Fig. 10, due to lack of samples test subjects. (HOWEVER, PAS TRES SIGNIFICATIF MAIS]The recognition system was made with data of (ONLY) one particular angle, corresponding to the specular angle. Scalar-extracted feature causes a lack of dimensionality as it confirmed by recognition rates in Fig. 12. (expliquer la phrase pour décrire le phénomène qued'un cote il y a de spetites données et d'un autres des données plus grand)

The system is constraint to multiple limitations, as the (mettre au passif) absorption spectrum of the skin, $\int S_E * S_S * S_R d\lambda$ where S_E, S_S , and S_R are respectively the spectrum of emission, diffusion and reception, conditioned by the spectrums of LED emission and photodiode reception. Thus, the quantity of the complex molecules (mainly oxyhemoglobin, melanin and water) are mixed. (a consequence portion of the skin is illuminated) Despite, we present a consequent portion of the skin (around 7cm²), averaging the oxyhemoglobin amount in the measurement, amplifying the measurement of melanin. (this is the common task used by humans,) which humans used in order to discriminate the skin, in the visible spectrum.

However, the accuracy of the method is efficient on the proposed protocol to identify the subjects, validating the biometric application of this methodology.

V. CONCLUSION (CLAIMS)

Skin recognition system is presented using a spectrophotometer in order to obtain input data as scattering diagrams due to the skin components (un peu trop long, couper, dire que la peau présente un certain nombre de proprietes)

, for learning algorithm which provides individual detection, reaching 100% accuracy with seven test subjects. The improvements in skin recognition may be used in medicine as a pathology detector instead of biopsy procedure, in cosmetology in order to observe reaction of chemical components on the skin, in computer graphics for animation, photorealistic rendering as well as in biometrics in order to individual detection.

VI. PERSPECTIVES

Our perspective contains improvements for the optical system, acquisition, and augmented accuracy in algorithm with higher accuracy which requires higher number of training examples also a better clustering.

Training samples implies the accuracy of the learning algorithm. In this case, the training samples are acquired from a system containing a LED (phrase sans verbe) as the emitter. (A ENLEVER CAR C'EST PAS DES PESPECTIES) A monochromator could be used in order to generate a narrow

spectrum, the input data for recognition tool would have greater dimensionality, providing better individual clustering with more training data. The monochromator can sweep its functional wavelength in order to make a spectrum of multiple wavelengths.

As described in the last paragraph, we could have a spectrum for each angle of measurement. This can be done also with a diffraction grating, that we could set up near the optics of camera filming the scene, in order to collect diffraction of the light by the skin.

The system is using a photodiode as the sensor, leading to different kind of noises, as the direct current noise of the power supply, or the electronic noise of the sensor. The noise could be filtered and amplified in a fashionable way to maximize the signal-to-noise ratio of the filtered signal, minimizing the standard deviation of multiple measurements.

In order to compensate the lack of dimensionality in the recognition system, the diffusion diagram would be used as input as well as in Fig. 11. This will be presented during the project valorization process, as the team is preparing a demonstrative system instead of the prototype used to gather the data presented in this article.

Another improvement for the recognition tool would be provided by coupling the system with a camera, which increase the quality of input data (binning methods) for a better clustering, and could be used to analyze the veins as the spatial arrangement of local distribution of the oxy-hemoglobin. Thus, it would be adequately distinctive to characterize a person, like in wide range of biometric solution.

Another perspective related to the training example is the determination of the study field. For instance, in order to adapt this device into medical field, the pathological samples would be needed as input of learning algorithm in order to make a pathological recognition tool. Another constraint comes from medical regulation which evaluate the device as well as its software as a medical device. Hence, in order to make a medical device to detect skin pathologies, this non-invasive device would be a class I medical device due to CE regulation and its software would reach certain accuracy for certain number of tests.

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