**Cortical efficient coding shapes behavioral performance.**

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**Abstract**

The efficient coding hypothesis postulates that neurons shape their response properties to match their dynamic range to the statistics of incoming signals. However, whether and how such efficient neuronal codes inform behavior has not been previously shown directly. Here, we trained mice to detect a target presented in noise shortly after a change in the noise contrast. The observed changes in behavior followed the predictions of a normative model of efficient cortical sound processing. Target detection and sensitivity improved in low contrast relative to high contrast noise. Furthermore, the time course of target detectability varied depending on contrast, decreasing rapidly after a transition to high contrast, and increasing at a slower rate after a transition to low contrast. The auditory cortex was required for detection of targets in noise and cortical neuronal responses exhibited the predicted patterns of target detectability. The magnitude of gain modulation in cortical neurons predicted individual differences in behavioral performance. Combined, our results demonstrate that efficient neural codes in auditory cortex directly influence perceptual behavior.

**Introduction**

As we navigate the world around us, the statistics of the environment can change dramatically. The efficient coding hypothesis postulates that neurons match their limited dynamic range to the statistics of incoming sensory signals[1]. Thus, through adaptation of their response properties, neurons can preserve their ability to encode information within many types of environments[2–4]. Such neuronal adaptation to the statistics of the environment has been found throughout different sensory modalities and brain regions[5–13]. In the auditory system, neurons exhibit contrast gain control, adapting the gain of their response function to match the contrast (variance) of the incoming sounds[14–18]. Yet it remains unknown whether and how contrast gain control in the auditory system informs behavior, as a direct link between neuronal adaptation and behavior has not been previously established.

The efficient coding hypothesis has been formally implemented through normative models of brain function[3,19–22]. These models allow us to simulate how neural function constrains behavior and to assess whether and how neuronal adaptation shapes sensory representations. There has been previous work demonstrating that efficient codes can explain psychophysical biases[23] and shape the rate of information transmission when stimulus statistics change dynamically [19,21,22]. These studies, which are either theoretical in nature or based in human psychophysics, rely on assumptions of neuronal mechanisms of efficient coding that were not simultaneously measured. As such, there are no studies combining behavioral psychophysics with recordings of brain activity to simultaneously test the neural assumptions and behavioral predictions of these models.

Psychophysical studies suggest that the auditory system exhibits adaptation to acoustic contrast. In humans, target volume discriminability is greater in low contrast than in high, an effect consistent with gain control observed in primary auditory cortex[24]. Similar effects have also been shown in ferrets performing an acoustic localization task, where it was demonstrated that neural responses in the inferior colliculus of anesthetized ferrets changed in a manner consistent with observed perceptual shifts[10]. However, it remains unclear whether the observed behavioral effects are indeed due to changes in gain in auditory neurons, as previous behavioral studies were not performed with simultaneous neural recordings, so a direct relationship between neural gain and perceptual performance has yet to be assessed.

Our goal for the study was to first build a formal framework based on efficient coding to predict behavioral detection of targets given changes in background sound contrast. Next, to directly test the role of efficient coding in auditory behavior, we trained mice to detect targets in variable contrast backgrounds. Mouse behavior followed the model predictions. Simultaneous chronic neural recordings show that the neural code in auditory cortex is not only predictive of individual differences in behavior, but also that variability in neural contrast adaptation is predictive of task performance in a contrast-dependent manner and on a trial-by-trial basis. Combined, our results identify a novel relationship between efficient neuronal coding and acoustic behavior, and provide a normative framework that can be used to predict behavioral performance across other behaviors and sensory modalities.

**Diagram

Description automatically generatedFigure 1.**

1. Experimental setup. Head-fixed mice are presented with sounds from an ultrasonic speaker. During behavior, mice receive water rewards through a lick spout. In a subset of mice, tetrodes were implanted in ACtx to record spiking activity.
2. GO/NO-GO task design. *Left:* example NO-GO trials. From top to bottom: spectrogram of an example low-to-high contrast trial (colorbar indicates volume in dB SPL); waveform for sample spectrogram; example spectrogram for a high-to-low contrast trial; waveform for example spectrogram; temporally jittered response window to estimate false alarms over time; schematic lick responses during in the window; timeout delivered after the first lick for 7 seconds. Vertical red dashed line indicates the contrast switch after 3 seconds. Black horizontal scale bar indicates 1s. *Right:* example GO trials. From top to bottom: same as in left panel, except the response window immediately follows target presentation and licks within the target window trigger a ~5uL water reward.
3. Target manipulation example waveforms. *Top:* overlaid trials where target volume differed. Volume is indicated by the amplitude and colorbar, with low volume targets shaded in cyan, and high volume targets shaded in magenta. *Bottom:* overlaid trials where target timing differed. Target timing is indicated in the colorbar, with light magenta targets occurring shortly after the contrast switch, and darker targets occurring at increasing delays. The red vertical dashed line indicates the contrast switch.
4. Normative model of the task. Left inset shows volume distributions for backgrounds (light lines) and targets (dark lines) in low and high contrast. (1) Spike generation process: a 1-dimensional sensory stimulus consisting of a background that transitions between low and high contrast (light lines) with superimposed targets (solid dots) feeds into a model neuron. The response of the model neuron is governed by a sigmoidal function which then generates stochastic spikes through a Poisson process. (2) Based on the observed spiking, a variance estimator integrates spike counts to estimate the current variance of the stimulus. (3) This estimate is then used to adjust the gain of the model neuron to optimize the estimate of stimulus variance at each time step. (4) The average change in gain of the model after each contrast transition. Dashed lines and dots indicate the time taken to reach half of the range of gain values in each contrast.
5. Model psychometric functions. Discriminability between model spike rates in response to the background and targets as a function of contrast and target volume. Arrow indicates target mean of 1.50 which is the volume used to assess time courses in c).
6. Model target discrimination as a function of time and contrast. Dashed vertical line indicates the time where the background contrast changes.

**Results**

*A novel target-in-noise detection task and normative model for task predictions.*

To assess how perceptual performance is impacted by stimulus contrast, we devised a GO/NO-GO task in which head-fixed mice were trained to detect targets embedded in different contrast backgrounds. During each trial, the mouse was first presented with 3s of dynamic random chords (DRCs) of one contrast, after which a switch occurred, either to a higher or lower contrast background. At variable delays after the switch, broad-band target chords were superimposed on the background chords, and mice were trained to lick for a water reward upon hearing the target. Target trials were interleaved with noise-only trials, during which the mouse was trained to withhold licking, but would receive a 7s timeout if licking after the contrast switch (Figure 1a,b). To assess behavioral sensitivity to targets, we parametrically varied target volume in each contrast (Figure 1c, top panel) and to assess behavioral adaptation, we parametrically varied target timing (Figure 1c, bottom panel). This stimulus design allowed us to quantitatively test whether and how adaptation to background contrast manifested in behavior.

To build an intuition for the effects of contrast gain control on target detectability, we simulated a neuron designed to estimate the contrast of the recent stimulus by adjusting the gain of its nonlinearity. A detailed description of the model is provided in the methods, but briefly: 1) at each timestep, a stimulus which varied in contrast over time generated stochastic spikes in the model neuron, 2) based on this spiking activity, the variance of the stimulus in a brief window before the current timestep is estimated, 3) the variance estimate error is then fed back to the model neuron and the neuron updates its gain to improve the estimate (Figure 1d, panels 1-3). We find that the timescale of gain control in this model has a few key features: 1) gain decreases after a switch from low-to-high contrast and vice-versa from high-to-low contrast, and, 2) gain adaptation times are asymmetric, adapting faster for high contrast than low contrast, as indicated by the time taken to reach half of the range of each curve (Figure 1d, panel 4).

Using this framework for efficient coding of stimulus contrast, we simulated how well the model can detect targets added to this fluctuating background. By varying the target mean in each contrast, we observed that in low contrast, the model is more sensitive to changes in volume, as indicated by the steeper slope, and has lower detection thresholds compared to high contrast (Figure 1e). Additionally, when holding target volume fixed and varying target time relative to the switch, we see target detection adaptation in line with model gain adaptation (as mentioned in Figure 1d, panel 4). Specifically, after a low-to-high contrast switch, targets are readily discriminable from noise, and this discriminability decreases as gain decreases, while after a high-to-low contrast switch, we see the opposite trend (Figure 1f). Next, we tested these two predictions, 1) increased performance in low contrast, and, 2), differential timing for the change in target detection performance in each contrast in behaving mice.

*Mouse behavioral detection is modulated by background contrast.*

Mice learned this task reliably, typically reaching criterion performance of 80% correct within 2-3 weeks in either contrast and performed this task for many weeks (Figure 2a). In all of the mice we tested, we found that targets were easier to detect in low contrast, observing significantly lower detection thresholds in low contrast (*M* = 7.29, *SD =* 1.44) compared to high contrast (*M =* 12.89, *SD =* 1.80; paired t-test: *t(40)* = -11.13, *p* = 8.14e-14, Figure 2b,c).

Using psychometric testing, we found significantly lower target thresholds in low contrast (*M* = 5.33, *SD =* 2.46) compared to high contrast (*M =* 12.28, *SD =* 1.31; paired t-test: *t(5)* = -4.38, *p* = 0.007; Figure 2e) and significantly higher psychometric slopes in low contrast (*M* = 0.054 *SD =* 0.007) compared to high contrast (*M =* 0.038, *SD =* 0.002; paired t-test: *t(5)* = 3.86, *p* = 0.012; Figure 2f).

To assess behavioral adaptation to the background contrast, we presented targets at threshold volume at variable delays following the contrast transition. We observed behavioral time-courses consistent with our model: in high contrast, mice initially were able to detect targets with high accuracy which fell off over time, while in low contrast we observed increasing detection rates over time (Figure 2g). By fitting each mouse’s adaptation time-course with an exponential function and comparing time constants for each contrast, we also found that behavioral adaptation is significantly faster in high contrast (*Mdn* = 0.013) compared to low contrast (*Mdn =* 0.128; Wilcoxon rank-sum test: *T*  = 475, *z* = 2.76, *p* = 0.006; Figure 2h).

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**Figure 2.**

1. Behavioral performance. Percent correct performance relative to the first session of task exposure. Dots indicate a session, while the traces indicate a running average using a 7 day window. Blue dots and traces indicate sessions in which mice detected targets in low contrast (ie. after high-to-low contrast transitions), while red dots and traces indicate sessions in which mice detected targets in high contrast (ie. after low-to-high contrast transitions).
2. Psychometric functions averaged for n=21 mice in low and high contrast. Error bars indicate SEM over mice at individual target SNRs, while the solid lines are logistic function fits to the average performance per contrast. Colors as in d).
3. Psychometric thresholds per contrast. Each dot represents a mouse, lines connect individual mouse performance on low and high contrast sessions. Bars indicate the average threshold over mice, while error bars in black indicate threshold SEM over mice. Bar colors as in d).
4. Behavioral psychometric functions. Dots with error bars indicate average performance +- SEM over mice as a function of contrast and target volume. Overlaid dark colored lines indicate psychometric fits to the averages, with the black dot indicating the average threshold. Light colored lines indicate the psychometric curves of individual mice. Black horizontal line indicates chance (0.5) performance.
5. Psychometric thresholds per contrast. Each dot represents a mouse, lines indicate where a mice participated in both low and high contrast sessions. Bars indicate the average threshold over mice, while error bars in black indicate threshold SEM over mice.
6. Psychometric slopes per contrast. Presentation as in **e**.
7. Behavioral performance as a function of contrast and target time relative to the switch in contrast. Dots with error bars indicate average performance +- SEM over mice. Solid colored lines indicate exponential function fits to the average over mice. Black, dashed vertical line indicates the contrast switch.
8. Average time constant of exponential fits in low and high contrast. Presented as in **h**. In all plots, blue indicates when targets were presented in low contrast and red indicates high contrast.

*Auditory cortex is necessary for detection in noise.*

**Previous studies have shown that gain control can occur at multiple areas in the autiory pathway… etc why do we choose cortex here?** We next tested whether adaptation in auditory cortex shapes performance in this behavioral task. To test this prediction, we inactivated auditory cortex using the GABA agonist muscimol to assess whether it is necessary for task performance. We first validated that muscimol disrupts cortical coding of target sounds by applying muscimol topically to the cortical surface of awake, untrained mice while recording neuronal responses during passive playback of the behavioral stimuli (Supplementary Figure 1a). We first recorded baseline responses to all stimuli, then topically applied muscimol or saline, waited 30 minutes, and recorded stimulus responses again. After muscimol application, there was a marked decrease in neural responses to targets compared to the baseline recordings (Supplementary Figure 1b, top). Notably, in our saline control, we observed little to no change in neural responses after saline application (Supplementary Figure 1b, bottom). We used a 3-way ANOVA to compare the effects of muscimol, contrast, and target volume on target responses in the saline and muscimol recording sessions. We found a significant main effect of muscimol (*F*(1) = 322.65, *p* = 4.88e-67) and volume (*F*(6) = 15.48, *p* = 1.98e-17), but no main effect of contrast (*F*(1) = 0.39, *p* = 0.53), indicating nearly complete suppression of responses to both targets and noise in high and low contrast (Supplementary Figure 1c). These results confirmed that muscimol effectively disrupts the cortical coding of our behavioral stimuli.

To test whether this cortical activity disruption by muscimol perturbs behavioral performance, we repeated the same experiments in behaving mice, administering muscimol or saline bilaterally through chronically implanted cannulae (Figure 3a). As observed in cortical activity, there was a profound decrease in the rate of responding to both targets (hits) and noise (false alarms) in both contrasts (Figure 3b). We quantified these effects on the psychometric curve, and observed significant decreases in the response rate at the highest volume, false alarm rate, and slope of the psychometric functions (Figure 3c, **STATS TABLE**). The only parameter that was unaffected by muscimol was the behavioral threshold (Figure 3c, bottom left panel).

A potential alternative effect of muscimol is a general loss of function that is not specific to hearing target sounds. To control for this, we devised another task where instead of detecting targets in noise (Figure 3d), mice detected targets in silence (Figure 3e). To ensure equivalency between the two tasks, we took the highest volume trial of the target in noise task (25dB SNR in high contrast; Figure 3d, left panel), and removed the background noise during the target detection period (Figure 3e, left panel). As such, mice detected the exact same targets as in the previous task, but without the flanking noise, allowing us to test whether auditory cortex is specifically required for detection in the presence of noise.

To assess psychometric performance in this new task, we modulated detection difficulty by attenuating the volume of each target. As observed previously, inactivation of auditory cortex hindered detection in high contrast noise (Figure 3d, right panel). However, cortical inactivation had little effect on psychometric performance in silence (Figure 3e, right panel). We quantified these effects in the two tasks as previously described, and found that the effect of muscimol was greatest during the target in noise task, significantly affecting the max response rate (STATS), threshold and moderately affecting slope (**STATS TABLE**). On the other hand, during the detection in silence task, muscimol only significantly increased detection thresholds (**STATS TABLE**), while all other metrics were unaffected. These results demonstrate that cortex is specifically necessary for detection in the presence of noise.

An additional alternative effect of muscimol is a general loss of the ability to lick. To assess this, we monitored the lick probability of the mice throughout the trial duration, and found that muscimol specifically reduced licking responses during the period where targets were presented (Wilcoxon rank-sum test: *T* = 337, *z* = -4.23, *p* = 2.34e-5; Supplemental Figure 1d, right panel of Supplemental Figure 1e). Mice also tended to lick immediately after the trial onset (Supplemental Figure 1e, left panel), but we found that the lick rates under muscimol and saline conditions were identical during this period (Wilcoxon rank-sum test: *T* = 528, *z* = 0.23, *p* = 0.81). These results suggest that muscimol does not impair the mouse’s ability to lick in general, but results in a specific deficit in licking in response to targets.

Combined, our results demonstrate that the auditory cortex is required for detection of tones in noise after contrast transitions. Our next goal was to test the relationship between neuronal activity in AC and behavioral performance.

*Population responses to targets track individual behavioral performance.*

To better understand how representations in auditory cortex could give rise to behavior, we chronically recorded from populations of neurons in auditory cortex while mice performed the behavioral task (Figure 4a). In the psychometric task where we varied target volume, many cortical neurons monotonically increased their firing rate with increased target volume (example neuron, Figure 4b; simultaneously recorded populations from two example sessions, Figure 4c).

To leverage our ability to simultaneously record from multiple neurons, we adapted a population vector approach[25] to generate metrics of target from noise discriminability from population activity. To do this, we estimated the coding direction in the high dimensional space of simultaneously recorded neurons by subtracting population vector responses to noise alone from population vector responses

Diagram

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**Figure 3.**

1. Setup schematic for chronic muscimol application in behaving mice.
2. Behavioral psychometric functions during muscimol or saline application for n=4 mice. Dark solid lines and filled circles indicate average performance after saline injection. Dark dashed lines and open circles indicate average performance after muscimol injection. Light solid and dashed lines are psychometric curves from individual sessions. Error bars indicate S.E.M. across sessions.
3. Behavioral performance metrics as a function of contrast and pharmacological intervention. Open circles indicate performance in individual sessions. Colored bars indicate average performance across sessions. Bars with low transparency and solid outlines are averages after saline application, while high transparency bars with dashed outlines are averages after muscimol application. Clockwise from the upper left, are plots of the max response rate, false alarm rate, psychometric threshold, and the maximum slope of the psychometric curve.
4. *Left:* Example stimulus spectrogram for the target-in-noise detection task with the corresponding waveform below. The scale line indicates 1 second, and the colorbar indicates the volume for each time-frequency bin. *Right:* psychometric performance for n=2 mice in the target-in-noise task, with target volume on the abscissa and probability of responding on the ordinate. Filled circles and dark solid lines indicate average performance after saline injection and psychometric fits to the average. Red open circles and dark dashed lines indicate average performance after muscimol injection and psychometric fits to the average. Light red solid and dashed lines are psychometric curves from individual sessions. Errorbars indicate S.E.M. across sessions.
5. *Left:* Example stimulus spectrogram for the target-in-silence detection task with the corresponding waveform below. Time scale and volume scale as in **d)**. *Right:* psychometric performance for n=2 mice (same mice as in **d)**) in the target-in-silence task, with target attenuation relative to the highest volume target from the target-in-noise task on the abscissa and probability of responding on the ordinate. Black filled circles and dark solid lines indicate average performance after saline injection and psychometric fits to the average. Open circles and dark dashed lines indicate average performance after muscimol injection and psychometric fits to the average. Light grey solid and dashed lines are psychometric curves from individual sessions. Errorbars indicate S.E.M. across sessions.
6. Behavioral performance metrics as a function of task type (detection in noise or detection in silence) and pharmacological intervention. Formatting and metrics as in **c)**. Dark and light red bars indicate performance in the detection-in-noise task, with application of saline or muscimol. Dark and light grey bars indicate performance in the detection-in-silence task, with application of saline or muscimol.

to targets. The resulting coding direction vector is the direction in high dimensional space between the average response to noise and targets (Figure 4d, left panel). This vector was trained on all but one trial, and the remaining trials’ population response was projected along this coding direction to generate a single projection value along this coding direction. This was repeated for all trials, and the projection values were averaged for every trial within a 40ms window after target onset. We then grouped these values into trial distributions for each target volume, and compared them to noise trial distributions by estimating a criterion projection value that best predicted whether each was a target or noise trial[26] (example projection value distributions from the recording session in Figure 4C, left panel is shown in Figure 4d, right panel).

Using this criterion, we then computed the accuracy of the neural population in discriminating targets from noise at each volume and at each contrast. This allowed us to estimate neurometric functions for direct comparison to the corresponding psychometric functions of each mouse (Figure 4e). On average, neurometric and psychometric functions were qualitatively similar, with neurometric functions exhibiting slightly lower thresholds, and shallower slopes (Figure 4f). We found that behavioral thresholds were highly predictive of the observed neural thresholds across both contrasts (single linear regression: *F*(1,17) = 23.7, *p* < 0.001, *R2* = 0.58; Figure 4g). We also observed a significant relationship between behavioral and neural thresholds in low contrast alone (single linear regression: *F*(1,9) = 6.24, *p* = 0.034, *R2* = 0.34), suggesting that the observed correlation across contrasts is not just due to contrast, but that cortical neurons track behavioral thresholds independently of contrast (Figure 4g). We tested whether neurometric and psychometric thresholds were similarly affected by background contrast using a two-way ANOVA, with thresholds as the dependent variable and threshold measure (psychometric or neurometric) and contrast as independent variables. We found a main effect of contrast (*F*(1) = 29.30, *p* = 5.00e-6), but no main effect of threshold measure (*F*(1) = 0.02, *p* = 0.89) or interaction between measure and contrast (*F*(1) = 0.04, *p* = 0,85), which demonstrates that behavioral and neural thresholds were similarly affected by background contrast. Additionally, we find that across both contrasts there is a significant relationship between neurometric and psychometric slopes (single linear regression: *F*(1,17) = 20.4, *p* < 0.001, *R2* = 0.52, Figure 4h), with a significant relationship within high contrast (*F*(1,9) = 7.07, *p* = 0.038, *R2* = 0.46), and a marginally significant relationship in low contrast (single linear regression: *F*(1,9) = 3.93, *p* = 0.079, *R2* = 0.23). We examined whether neurometric and psychometric slopes using a two-way ANOVA, as described above, and found a significant main effect of slope measure (*F*(1) = 5.88, *p* = 0.021) and contrast (*F*(1) = 8.31, *p* = 0.007). Post-hoc testing revealed that psychometric slopes were significantly steeper than neurometric slopes (**DO POST HOC TESTING**).

*Cortical gain tracks individual behavioral performance.*

Our behavioral results and model provide strong evidence that gain control in the auditory system shapes patterns of behavioral performance. To more directly assess the role of gain control in auditory cortex in shaping

behavior, we leveraged the design of our background sounds to estimate the gain of cortical neurons using a generalized-linear-nonlinear model (gLN). Briefly, we estimated the spectrotemporal receptive fields (STRFs) of individual cortical neurons using generalized linear regression and convolved them with the stimulus spectrogram to generate linear predictions of cortical activity (Figure 5a, panels 1-3). We could then compare the linear prediction to the observed firing rate elicited by the background to estimate the nonlinearity of each neuron in high and low contrast (Figure 5a, panel 4). This modeling strategy allowed us to estimate cortical gain during different periods in the task, and assess how gain is related to behavioral performance.

During the task, we used DRC backgrounds with fixed patterns, allowing us to quantify reliability of the responses to the background by taking the ratio of noise power of the responses to the signal power, a value known as the noise ratio[27] (see Methods) (Figure 5b, spike raster). The estimated STRF for this example unit is shown in Figure 5c, along with the nonlinearities estimated for low and high contrast in Figure 5d. By fitting nonlinearities separately to high and low contrast portions of each trial, we were able to estimate neural gain for all of the recorded units during the task. After pooling all of the neurons recorded across all mice and sessions, and including only neurons with high reliability in both contrasts (noise ratio < 100 in low and high contrast), we observed substantial gain control during the task (**STATS**) confirming previous findings in ferret and mouse auditory cortex[14,17].

We then assessed whether gain in auditory cortex reliably predicts how well a mouse is able to hear targets in these different backgrounds. To do so, we averaged the gain of target-selective neurons during the target period of the task for each mouse and then compared the target period gain for each mouse to the behavioral thresholds and slopes collected in the psychometric task. We found a significant negative relationship between cortical gain and behavioral threshold across contrasts (single linear regression: *F*(1,12) = 24.2, *p* < 0.001, *R2* = 0.67), suggesting that increased gain yielded greater sensitivity to lower target volumes. However, we didn’t observe this relationship when only including low contrast sessions (*F*(1,7) = 1.42, *p* = 0.27, *R2* = 0.17) or high contrast (*F*(1,3) = 2.02, *p* = 0.25, *R2* = 0.40), so we cannot definitely conclude that contrast-independent fluctuations in gain predict behavioral thresholds (Figure 5f). We conducted the same analysis between gain and psychometric slopes, and found significant positive relationships across contrasts (single linear regression: *F*(1,12) = 12.0, *p* = 0.005, *R2* = 0.50) and within low contrast (*F*(1,7) = 6.96, *p* = 0.034, *R2* = 0.50), suggesting that individual differences in cortical gain influence behavioral sensitivity to changes in volume, independently of contrast gain control.

Diagram

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1. Experimental setup for chronic ACtx recordings from behaving mice.
2. Example spiking responses to targets and noise in low contrast during behavior. The top portion of the plot is a spike raster ordered by target identity. Colored bars indicate the target volume, grey bars indicate noise only trials. The bottom portion of the plot contains spike rates for each target condition, averaged over trials and smoothed with a 2ms standard deviation Gaussian kernel. *Inset:* Grey solid line indicates the behavioral percent correct for this session. Closed circles and the solid blue line indicate the performance of an ideal observer in discriminating between noise responses and target responses at each volume. Circle colors indicate the presented volume. The dashed horizontal line indicates chance performance (0.5). Error bars are the 95% confidence interval of ideal observer performance as assessed through a bootstrap procedure.
3. Neurograms of populations of simultaneously recorded neurons during a low contrast and high contrast session from the same mouse. Neurons are plotted along the ordinate, while target volume is plotted along the abscissa. Within each plot, shade indicates the neural response to each target, with the average response to noise alone subtracted. White indicates no change in firing rate, blue/red indicate increases in firing rate relative to the noise response, and cyan indicates suppression below the noise response. Asterix indicates the responses of the neuron in panel b).
4. Discriminating targets from noise using population responses. *Left:* schematic of coding direction analysis. In high dimensional neural space, noise trials are represented as a gray point cloud, while target responses are represented by a blue point cloud. The coding direction (CD) is the vector defining the average difference between these two point clouds as indicated by the arrow. *Right:* trial distributions of projections along the coding direction for one session (session CA118-200707, as plotted in c). The blue distribution is the average projection value in a 40ms window after presentation of 20 dB SNR targets. The gray distribution is the average projection value in the same window during noise only trials. The vertical red line is the criterion which yielded the highest performance in predicting target presence across all trials.
5. Example neurometric and psychometric curves. *Left:* Low contrast curves. Light blue circles and solid lines indicate psychometric performance and a logistic fit, respectively. Dark blue circles and solid lines indicate neurometric performance from the session plotted in **c)**. The horizontal dashed line indicates chance performance (0.5). The arrow indicates the neural performance computed from the distributions and criterion plotted in **d)**. *Right:* High contrast curves from the same mouse for the session plotted in **c)** (plot appearance as in left).
6. Average psychometric and neurometric functions across mice. Light circles indicate average behavioral performance, dark red and blue circles indicate average neural performance. Light solid curves indicate logistic fits to average behavioral performance, while vertical lines indicate the fit thresholds. Dark solid lines indicate fits and thresholds for the neural data. The dashed vertical line indicates chance performance. Shades of blue and red indicate averages over low and high contrast respectively.
7. Relationship between behavioral and neural thresholds. Each circle represents the average behavioral and neural threshold for each mouse for each contrast (as indicated by the circle fill color). Grey lines and shaded areas indicate the linear regression fit across contrasts, +- the 95% confidence interval. The solid black line indicates unity. Inset text indicates the significance of linear fits between all data points (black), low contrast data points only (blue), or high contrast data points only (red).
8. Relationship between behavioral and neural slopes. Appearance as in g).
9. Population decoder performance while varying contrast transition, and target timing relative to the transition (indicated by the dashed vertical black line at 0s). Ticks on the abscissa indicate average target time from the transition in milliseconds. Solid lines and circles indicate the percent correct performance of a target decoder after a switch low contrast (blue) or high contrast (red). Errorbars indicate S.E.M. over sessions. Horizontal lines significant changes in performance between the first target presentation time and subsequent target presentation times, as assessed by Wilcoxon Sign-rank tests with false discovery rate correction for multiple comparisons. The span of the lines indicates the target times being compared, while the color of the lines indicates whether the test was performed within high contrast (red) or low contrast (blue).
10. Adaptation time constants of exponentials fitted to the average neural decoder performance for each mouse in each contrast. Blue and red circles indicate the adaptation time constants from neural populations for each mouse in low and high contrast respectively. Solid black lines indicate time constants from the same mouse.

**Discussion**

On daily basis, we navigate through many auditory environments, each defined by different statistical properties. The dynamic range, or contrast, of acoustic inputs poses a challenge to the auditory system, which is composed of neurons with limited dynamic range in their response. The efficient coding hypothesis predicts that as acoustic contrast shifts, neurons throughout the auditory pathway adjust their sensitivity, so as to match the dynamic range of their response to that of the stimulus distribution. This process allows auditory neurons to encode volume information within each contrast, despite changes in the dynamic range. Multiple studies have demonstrated that indeed, neurons throughout the auditory pathway exhibit contrast adaptation[14,16,17,28]. However, whether contrast adaptation plays a role in auditory behavior has not been previously examined directly, while recent work has demonstrated a link between cortical codes and human psychophysical performance [24]. In this study, we directly linked neuronal contrast gain control to auditory behavior through the use of a theoretical model of efficient coding, behavioral psychophysics, and simultaneous manipulation and recordings of cortical activity.

To tackle this complex question, we first developed a normative framework[22] that allowed us to make specific predictions for behavioral performance as expected by contrast gain control. The model predicted that (1) The detection threshold of a target in noise under low contrast should be lower than under high contrast; (2) Upon a shift in the background noise contrast, detection improves upon transition from high to low contrast, but is impaired upon transition from low to high contrast; and (3) The time constant for this change in detection performance is slower for transitions from high to low contrast than from low to high contrast (Figure 1). To test these predictions, we trained mice to detect a target in noise background, as noise contrast shifted from low to high or from high to low. As predicted by the normative model, mice exhibited a lower threshold for detecting targets in low as compared to high background. Over time, we observed a decrease in tone detection after a switch to high contrast, and in increase in tone detection after a switch to low contrast. Behavioral adaptation was faster in high contrast, as compared to low contrast backgrounds, in agreement with our model and previous theoretical models[19] (Figure 2). We furthermore found that AC is necessary specifically for this detection-in-noise task, and that AC population activity reflected the behavioral shifts. Combined, our results provide evidence for the relevance of efficient coding in auditory behavior.

Neurons throughout the auditory system adapt to the statistics of the acoustic environment, including distribution of stimuli over time[29,30] and more complex sound patterns[31]. In this study, we focused on contrast gain control as a fundamental statistical adaptation that relates to efficient coding. Contrast gain control is present at multiple stages in the auditory system, increasing in magnitude from the auditory nerve to inferior colliculus, auditory thalamus and auditory cortex[24,28] with slower adaptation speeds in auditory cortex[24]. As such, we focused on the auditory cortex, and found that its inactivation selectively impaired the detection of target in noise background. Importantly, cortical inactivation did not impair detection of targets without background (Figure 3), therefore confirming that cortex plays a specific role in extracting targets from noise. Our findings are consistent with multiple previous studies, which found that the auditory cortex is not required for performance in simple tasks but is required for more complex behavioral tasks[32–37]. In fact, whether AC is required for a specific auditory behavior depends not simply on the stimulus selection, but how differentiable stimuli are from each other at the level of population cortical activity[38–40].

Whereas previous work largely studied the behavioral or psychophysical performance separately from the neuronal activity, which was recorded in anesthetized or passive subjects, we were able to record neuronal responses from behaving mice. Not only is this important to control for the level of arousal and attention, which can dramatically alter responses in AC[41–46], but also allowed us to test for a statistical relationship between the effects of contrast on neuronal encoding and behavioral performance across subjects. Leveraging individual differences in behavioral performance, we showed that population representations in cortex were highly predictive of behavioral performance metrics (Figure 4). Additionally, a recent study examining thousands of simultaneously recorded neurons in V1 showed that neural acuity far outperformed mouse visual acuity, and was not correlated with task performance[53]. In the current study, we found that individual differences in behavioral performance were correlated with individual differences in neurometric performance in the auditory cortex.

Inspired by previous studies[43,54–57], we intentionally designed our task stimuli using unbiased white-noise backgrounds, which allowed us to leverage our behavioral stimuli to map spectro-temporal receptive fields and estimate neuronal gain using linear-nonlinear modelling tools. This approach allowed us to assay the relationship between cortical gain and behavioral performance (Figure 5), but also permits exploration of other behavioral outcomes, such as choice, and whether they impact receptive fields or cortical gain on a trial-by-trial basis. The selection of background sound should therefore be carefully considered in experimental designs in order to leverage the power of encoding models fit to neuronal responses[58–61].

While this study demonstrates the necessity of auditory cortex for detection in varying-contrast noise, the neuronal mechanisms driving adaptation to contrast remain sparsely explored. Additionally, while we observed theoretically optimal asymmetric adaptation to changes in contrast, the neural circuits driving these temporal asymmetries are unknown. In the current study, we have likely recorded from a mixed population of excitatory and inhibitory neurons. Different inhibitory neuronal subtypes exhibit specific roles in adaptation[62–65]. It is also thought that specific inhibitory neuronal subtypes facilitate divisive (gain) or subtractive control of excitatory responses in visual[66,67] and auditory cortex[18,68,69], whereas others contribute to target detection and behavioral choice(**CITE**). Through the use of modelling techniques, behavior, and cell-specific neuronal manipulation and recording methods, these unresolved questions provide many future avenues to study the relationship between neural circuits and behavior.

A picture containing diagram

Description automatically generated

**Figure 5.**

1. Schematic of the generalized-linear-nonlinear model. 1) Schematic of a spectrotemporal response function. 2) Example stimulus spectrogram of low and high contrast. 3) The gray trace is the filter response when convolving the STRF with the spectrogram. The black trace is the observed spike rate during the same stimulus period. 4) Schematized nonlinearities fit separately to low and high contrast periods.
2. Example background-locked responses from a well-tuned cortical unit across the trial duration. The top portion of the plot is a spike raster sorted by the frozen noise pattern (FN1-5) of the background. The bottom portion of the plot is a PSTH of the observed spiking, binned every 25ms (black trace). The colored traces are the model predictions in each contrast (red trace uses the red nonlinearity in d), blue trace uses the blue nonlinearity in d)).
3. STRF for this example neuron. STRF values are indicated by the colorbar.
4. Estimated nonlinearities for this example neuron. Points indicate the mean observed firing rate (ordinate), binned according to observed filter prediction values (abscissa). Solid lines indicate exponential function fits to the underlying points. Each line is a fit to the test set in a cross-validation run (see Methods).
5. Gain control in auditory cortex during the task. Each histogram is the distribution of gain values in high and low contrast across all cells recorded during behavior. Dashed vertical lines indicate the median of each distributions.
6. Relationship between gain and behavioral threshold. Each circle represents the gain and behavioral threshold for each mouse for each contrast (as indicated by the circle fill color). Grey lines and shaded areas indicate the linear regression fit across contrasts, +- the 95% confidence interval.
7. Relationship between gain and behavioral slope. Appearance as in f).

**Methods**

*Animals*. All experiments were performed in adult male (n = **xxx**) and female (n = **xxx**) mice (The Jackson Laboratory; age 12-15 weeks; weight 20-30g; STRAINS, etc.), housed with, at most, five mice per cage, at 28°C on a 12-h light:dark cycle with food provided ad libitum, and a restricted water schedule (see *Water Restriction*). All experiments were performed during the animals’ dark cycle. All experimental procedures were in accordance with NIH guidelines and approved by the Institutional Animal Care and Use Committee at the University of Pennsylvania.

*Surgery*. Mice were anesthetized under isoflurane (1-3%, vol/vol). Prior to implantation, all mice were administered subcutaneous doses of buprenorphine (Buprenex, **DOSE**) for analgesia, dexamethasone (DOSE) to reduce brain swelling, and bupivicane (**DOSE**) for local anesthesia. In mice undergoing electrophysiological experiments, two ground screws attached to ground wires were implanted in the left frontal lobe and right cerebellum, with an additional skull screw implanted over the left cerebellum to provide additional support. A small craniotomy was performed over the target stereotactic coordinates relative to bregma, -2.6mm anterior, -4.3mm lateral. Either custom 16-channel microdrives, 32-, or 64-channel shuttle drives (cite) holding tetrode bundles of polyimide-coated nichrome wires were chronically implanted over auditory cortex, and tetrodes were lowered 800um below the pial surface. The exposed base of the tetrodes were covered with GelFoam (**CITE**) or sterile silicone lubricant (**CITE**) and sealed with QuikCast (**CITE**). The plastic body of the microdrive and a custom titanium headplate were secured to the skull using dental cement (C&B Metabond) and acrylic (Lang Dental). Mice undergoing only behavioral experiments were implanted with two skull screws in the cerebellum, and a custom titanium headplate was mounted on the skull as previously described. An antibiotic (Baytril, **DOSE**) and analgesic (Meloxicam, **DOSE**) were administered daily (for 3 days) during recovery.

*Water Restriction*. Following surgical recovery (3 d postop), each mouse’s weight was monitored for three days to establish a baseline weight. Over the next seven days, mice were water deprived, beginning with a daily ration of 120uL/g and gradually decreasing their ration to 40-50uL/g. During the task, if mice did not receive their full ration, the remainder of their ration was provided in their home cage. Mouse weight relative to baseline was monitored during all stages of water restriction. Additional health signs were used to determine a health score and subsequent treatment plan if a mouse lost more than 20% of baseline weight, as described by previously published methods[70] and approved by the Institutional Animal Care and Use Committee at the University of Pennsylvania.

*Behavioral Apparatus*. During the Go/NoGo task, the mouse was head-fixed in a custom-built, acoustically isolated chamber. A capacitive touch sensor (AT42QT1010, SparkFun) soldered to a lick spout monitored lick activity. Water rewards were dispensed from a gravity fed reservoir, controlled by a solenoid valve (161T011, Neptune Research) calibrated to deliver approximately 4-5uL of water per reward[71]. Low level task logic, such as lick detection, reward and timeout delivery, and task timing intervals, was directly controlled by an Arduino Uno microprocessor running custom, low-latency software routines. High level task logic, such as trial randomization, stimulus buffering and presentation, and online data collection and analysis were controlled by custom MATLAB (Mathworks) software communicating with the Arduino over a serial port. Digital waveforms were converted to analog signals via a soundcard (Lynx E44, Lynx Studio Technology, Inc.) or a National Instruments card (NI PCIe-6353) and delivered through an ultrasonic transducer (MCPCT-G5100-4139, Multicomp). The transducer was calibrated to have a flat frequency response between 3 kHz and 80 kHz using a 1/4-inch condenser microphone (Brüel & Kjær) positioned at the expected location of the mouse’s ear, as described previously[72,73]. During electrophysiological recording sessions, licks were detected using an optical interrupt sensor (EE-SX771, Omron Automation), to prevent lick-related electrical artifacts introduced by contact with the capacitive sensor.

*Behavioral Timeline*. Each mouse underwent four stages in the behavioral task: 1) water restriction and habituation, 2) behavioral training, 3) psychometric testing, and, 4) offset testing. During the induction of water restriction, mice were simultaneously habituated to head-fixation in the behavioral chambers and receiving water through the lick spout, by providing a water reward for any licks separated by more than 2 s. After the mouse began to receive its entire ration by licking in the booth, behavioral training was initiated (typically 1 week). Each mouse was initially trained and tested in one contrast condition (see *Stimuli*), with the initial training condition counterbalanced across mice. Behavioral performance was monitored during training, and mice were considered trained after completing at least three consecutive sessions with over 80% percent correct (~2-3 weeks). After completing training, behavioral thresholds were measured during at least three sessions in which psychometric stimuli were presented (see *Stimuli*). After estimating the behavioral threshold for each mouse, offset stimulus sets were generated using threshold-level targets. After completion of at least three sessions in the offset task, each mouse was then retrained on the remaining contrast condition. Upon reaching the training criterion of 80% in the new contrast condition, mice were then tested in the psychometric and offset tasks as previously described. For mice in electrophysiological experiments, this sequence of training and testing was continued until the recording site yielded less than three units, or until the mouse stopped performing in the task.

*Stimuli*. All stimuli were created in MATLAB and sampled at 192 kHz or 200 kHz and 32-bit resolution. A set of dynamic random chords (DRCs) were created with different contrasts, similarly to those described in previous studies[14,17,24]. This stimulus was used 1) to measure the spectrotemporal receptive fields of neurons by fitting a linear-nonlinear model, and 2) to modulate the gain of auditory neurons by manipulating stimulus contrast. To construct a DRC, amplitude modulated pure tones were generated at multiple frequencies and then superimposed to create a chord. In some experiments, 34 frequencies were sampled between 4 and ~40kHz in 1/10 octave steps, in the remaining experiments, 33 frequencies were sampled between 4 and 64kHz in 1/8 octave steps. The amplitude envelope of each tone was generated as follows: every 25 ms, amplitudes for each frequency were sampled from a uniform distribution with a mean of 50 dB and a width of ±5 dB in low contrast or ±15 dB in high contrast. Between each 20 ms chord, the amplitude envelope of each frequency band was linearly ramped over 5 ms to the amplitude value for the next chord, such that the total duration of each chord and its ramp was 25 ms. To synthesize the stimuli, amplitude envelopes were multiplied by a sine wave of their respective frequencies, and summed to produce the final waveform.

In all stages of behavioral training and testing, stimuli created for each trial consisted of a DRC background containing a change in contrast, and the presence or lack of a target at a delay after the change in contrast. Each trial was initialized with 3 seconds of DRC noise of one contrast, followed by a switch to the other contrast. Targets consisted of a fixed chord composed of 17 frequencies pseudo-randomly sampled from the frequencies contained in the DRC background, such that the target frequencies were uniformly distributed across the frequency range of the background. To add targets to the background noise, the target amplitude at each target frequency was simply added to a single chord in the amplitude envelope of the background, and ramped as described previously; this procedure ensured that target timing was perfectly aligned to changes in the background noise, removing asynchronous timing cues that could be used by the animal to detect the target. Target amplitudes are described in values of signal-to-noise ratio (SNR) relative to the average level of the background noise (ie. a 50 dB target embedded in 50 dB noise would have an SNR of 0 dB). We note that because the targets only contained power in half of the frequency bands used to construct the noise background, target SNRs were typically above 0 dB. \*\*\*\* INSERT TABLE DESCRIBING ALL DIFFERENT EXPERIMENTAL CONDITIONS \*\*\*\* In all trials, targets were embedded after a change in the background contrast, with a delay and volume dependent on the current training or testing stage (see Behavioral Task).

*Behavioral Task*. We employed a Go/NoGo task to measure mouses’ perceptual ability to detect targets in noise. In this task, each trial consisted of a noise background with a contrast shift, along with the presence or absence of a target after the change in contrast. Mice were trained to lick when they detect a target (hit), or to withhold licking in the absence of a target (correct reject). This behavior was reinforced by providing a 4-5uL water reward when the mouse performed a hit, and by initiating a 7-10s timeout when the mouse licked in the absence of a target (false alarm). Any licks detected during the timeout period resulted in the timeout timer being reset. In a subset of mice, we introduced an additional trial abort period coincident with the first part of the contrast background, before the contrast switch. Any licks detected in this abort period resulted in the trial being reset after a 7-10s timeout, until the mouse withheld from licking during this period. In this task, misses and correct rejects were not rewarded or punished. Trials were separated by a minimum 1.5s inter-trial-interval (ITI). To discourage spontaneous licking, licks were monitored during this period, and if any licks occurred the ITI timer would be reset.

Several of our behavioral tasks varied the timing of the target relative to the contrast shift, which required a method for estimating hit rates and false alarm rates at different times during each trial, and to reward and punish the animal during these times in an unbiased manner. To approach this issue, we considered licks as responses only during a 1 s response window after a target presentation in the trial (eg. if a target was presented 500 ms post-contrast-switch, the response window persisted from 500 to 1500 ms post-contrast-switch). To apply this method to noise-only trials, in which no targets were presented, we considered noise trials as target trials containing infinitely small target amplitudes. For each noise trial, we assigned a response window with equiprobable delay matched to the target conditions, and considered only licks within those “target” response windows. Thus, over the course of a session, we randomly sampled lick probabilities in noise trials during the same temporal windows as those licks considered during target trials. Using this scheme, we treated target and noise trials identically, and estimated hit rates and false alarm rates over time in an unbiased manner.

Each mouse performed three stages in the behavioral task: training, psychometric testing, and offset testing. During the training task, trials consisted of two types, noise trials or target trials presented with equal probability. To facilitate learning, we selected target SNRs at the highest end of the range described previously: in low contrast training sessions, targets were 16 dB SNR, and in high contrast training sessions, targets were 20 dB SNR. To prevent response bias as a function of target timing, we randomly varied the target delay between 250, 500, 750 and 1000ms after the contrast change in each trial. During the psychometric testing task, there 7 trial types consisting of noise trials and target trials spanning six different SNRs (\*\*\* TABLE\*\*\*). Based on behavioral piloting, we presented high SNR trials with a greater probability, to prevent mice from giving up during the task. In low and high contrast psychometric sessions, the probability of a noise trial was 0.4, the probability of the four lowest target SNRs was 0.05 each, and the probability of the two highest target SNRs was 0.2 each. As in training, target timing was varied randomly between 250, 500, 750 and 1000ms after the contrast change in each trial. After completing at least three sessions of the psychometric task, stimuli were generated for the offset testing task. This task consisted of 15 unique trial types: 3 target volumes (noise trials, threshold target trials, and high SNR target trials), and 5 target delays relative to the contrast change (25, 75, 225, 475, 975 ms delay). Threshold target amplitudes were determined individually for each mouse by estimating target detection thresholds in each contrast condition during psychometric testing sessions, and varied between ~2-12 in low contrast and ~8-16 dB SNR in high contrast. Based on behavioral piloting, noise trials, threshold target trials, and high SNR target trials were presented with probabilities of 0.4, 0.2, and 0.4, respectively. Target delay on each trial was selected with equal probability. In all behavioral stages, trial order was pseudorandomly generated, such that there were no more than three target or noise trials in a row.

***Normative Model***

*Electrophysiological Recordings*. Neural signals were acquired from awake, behaving mice as they performed the psychometric and offset testing tasks described previously. Chronically implanted, 16-, 32-, or 64-channel microdrives[74,75] were connected to one or two 32 channel Intan amplifier headstages. Amplified signals were recorded at 30 kHz using an openEphys acquisition board via an SPI cable, where the signals were digitized. Prior to spike analysis, broadband signals were filtered between 500 and 6000 Hz, offset corrected, and re-referenced to the median across all active channels. The preprocessed data was then sorted using KiloSort[76] or KiloSort2 and the resulting clustering was manually corrected in phy2 according to community-developed guidelines. The resulting units were labelled as single units if they exhibited a clear refractory period and did not need to be split. Splitting assessments were made through manual examination of principle component features for the two best channels of a cluster. If two noticeable clusters in feature space were evident in a unit, the unit was either manually split, or classified as a multiunit.

*Behavioral and Neural Detection Performance.* To calculate performance in target-in-noise detection task we adopted commonly used signal detection theory methods[50,77] to estimate the ability of an ideal observer to discriminate between two sensory distributions: in our case, a distribution for target trials and a distribution for noise trials. When analyzing behavior, we computed the percent correct performance of an ideal observer[78] as a function of the probability of hits and false alarms:

where is the inverse z-transform of a standard normal distribution (normcdf in MATLAB), is the inverse of the normal distribution (norminv in MATLAB), is the hit rate, and is the false alarm rate. For psychophysical performance, hit rates and false alarm rates near 0 and 1 were adjusted using the log-linear rule[79], to reduce biases in performance estimation caused by low numbers of trials.

To calculate neural performance in the same reference frame as the behavior, we employed similar ideal observer techniques. First, neuronal responses (either spike rates or single units, or population projection values), were averaged in a 100ms window post target onset (for noise trials, this window was randomly chosen on each trial to coincide with target presentation times on target trials). Then, using the distributions of responses during target and noise trials, we computed receiver-operating-characteristic curves and took the area under the curve (AUC) as the percent correct of an ideal observer discriminating between the target and noise distributions. To determine whether the AUC value for a given set of trial distributions was significantly different from chance, we performed a bootstrap procedure where we sampled from all the trials with replacement 500 times and recomputed AUC for each sample. If the 95% confidence intervals for this bootstrapped distribution did not include chance (.5), we defined that AUC value as significant. For population analyses which generated single-trial predictions, neural hit and false alarm rates were transformed to percent correct as described above.

To characterize performance, psychometric curves were fit with a logistic function:

where is the x-offset of the function, determined the slope, or sensitivity of the function, determined the guess rate (lower bound), determined the lapse rate (upper bound) and was performance. determined the threshold of this function, defined as the x-value corresponding to the steepest part of the curve. This function was fit to behavioral or neural performance using constrained gradient descent (fmincon in MATLAB) initialized with a 10x10 grid-search of parameters and .

To characterize adaptation time constants, adaptation curves were fit with an exponential function:

where determined the y-offset of the function, was a multiplicative scaling factor, and was the time constant of the exponential in units of . This function was fit to behavioral or neural responses using constrained gradient descent, initialized with a 10x10x10 grid search across all three parameters.

*Population Response Metrics.* On sessions where three or more neurons were simultaneously recorded, we used a coding direction technique[25] to estimate the ability of neural populations to discriminate targets from noise. First, target and noise spike rates for each neuron were averaged in a 100ms window post-target onset. Then, using a leave-one-out procedure, we computed a trial averaged population vector for target trials, , and a separate average population vector for noise trials, . We then estimated the coding direction in high dimensional neural space that best separated the target and noise responses: The held out trial was then projected along this dimension, by taking the population response vector on that trial and projecting it along the estimated coding direction: . This procedure was repeated holding out each trial, and estimating the coding direction from the remaining trials. For psychometric testing sessions, the target responses from the two loudest target volumes were used to estimate coding direction, and in offset testing sessions the target responses from the high SNR target trials were used. After computing projections for every trial, the resulting matrix was normalized between 0 and 1.

*Criterion Classifier*. Based on previously described methods[26], we used a criterion-based decision rule to estimate how a down-stream neuron may read out neural activity during the task. As before, trial distributions of neural responses to targets and noise were created from the average activity in a 100ms window post-target. Then, we sampled 100 criterion values between the minimum and maximum response, and for each criterion estimated the proportion of correct trials under two decision rules: 1) report target present if the response is greater than the criterion, or, 2) report target present if the response is less than the criterion. By assessing these two decision rules, responses that may be suppressed by target presence were treated equally to those in which target presence enhanced the neural response. Finally, we chose the criterion and decision rule that yielded the highest proportion of correct trials, and computed neural hit rates and false alarm rates for each target level, and noise-only. These hit rates and false alarm rates were then transformed to percent correct according the formula above, to ensure equivalency with the behavioral metrics.

*Linear-nonlinear Model*. First, we selected only neurons in the dataset which had reliable stimulus responses (noise ratio < 100). The linear nonlinear model was then composed of two main parts, a spectrotemporal receptive field (STRF) and a set of rectifying nonlinearities. The STRF was fit using gaussian generalized linear regression (glmnet package in MATLAB), with a history window of 300ms (13 stimulus bins) and frequency bins corresponding to the frequencies composing the dynamic random chords (see *Stimuli*). Before fitting the full model, we cross-validated glmnet’s elastic net mixing parameter (cvglmnet in MATLAB) using matched time windows of low and high contrast responses from every trial. Then, using that parameter, we fit the full model using 10-fold cross-validation in the following manner.

For each fold, we selected 90% of the trials for training, leaving the remaining 10% to be held out for testing. Within each trial, we excluded neuronal responses around transitions from silence, or transitions in contrast, to prevent the model from overfitting strong transients in the neural response. Additionally, we excluded neural responses within a 50ms window after target presentations, to prevent overfitting to target responses. Given these exclusion criteria, we calculated the duration of stimulus sampled in the shorter target period for each trial, and, for that trial, sampled the same duration of stimulus within the adaptation period. This procedure ensured that the model was fit to the same amount of high and low contrast stimulation, to avoid overfitting to one condition. Then, a stimulus design matrix was made using these stimulus periods, and the STRF was fit to the neuronal data using lasso-regularized generalized linear regression (glmnet in MATLAB). Based on prior pilot analyses, we found that in reliably responsive neurons, STRFs estimated separately in high and low contrast were nearly identical, so for this analysis we estimated STRFs using both high and low contrast periods (**SUPPLEMENT?**). Using the STRF fit to the training data, we generated a linear prediction of the stimulus by convolving the STRF with the spectrogram of the training stimulus. We then separated the linear predictions into low and high contrast periods. For each contrast period, we generated a histogram of the linear prediction values (50 bins), and for each bin, computed the mean spike rate of the neuron when the linear prediction fell within those bin edges (Figure 5d, scatter points). The resulting set of linear prediction values and average spike rates were fit with an exponential function:

where determined the minimum firing rate, was a multiplicative scaling factor, determined the gain of the exponent, and determined the x-offset, or firing threshold of the neuron. This function was fit to each cell using contstrained gradient descent, using a 10x10 grid search for parameters and . These fits were determined for each contrast, and the gain for each contrast for each neuron was estimated using . This entire process was repeated for each cross-validation fold, and the final parameter estimates for the STRF and nonlinearities were taken as the average over the 10 runs.

To determine the relationship between neuronal gain and behavioral performance, we examined our dataset of neurons collected during the psychometric task. First, we selected all of the neurons with significant AUC values to at least two of the six targets to ensure that we were sampling from neurons with information about target volume. Then, across all of these neurons for each mouse, we computed the average neural gain for each contrast. We then compared neural gain for each mouse to corresponding average psychometric thresholds and slopes to assess the relationship between neural gain and behavioral performance.

Diagram

Description automatically generated

**Supplemental Figure 1.**

1. Setup schematic for acute muscimol recordings in ACtx.
2. Example spike rasters pre- and post-muscimol or saline application. On top of the raster is the timeline for each recording. A baseline recording of all stimuli was performed prior to muscimol application, then all stimuli were recorded again 30 minutes after application. Rasters are sorted by contrast and target volume, with color indicating low or high contrast backgrounds, color shade indicating target volume, and grey indicating noise only trials (-Inf). *Top left panel:* raster of target and noise responses of a representative neuron recorded prior to muscimol application. *Top right panel:* raster of the same neuron 30 minutes after muscimol application. *Insets:* Mean firing rate for each condition. Shade indicates target volume and the scale bar indicates a firing rate of 50Hz. Error bars indicate S.E.M. across trials. *Bottom panels:* Example neuron before and after application of saline. Formatting as in top panels.
3. Firing rate averaged across neurons after drug application in muscimol and saline recording sessions. Filled circles and solid lines are responses after saline was applied while open circles and dashed lines are responses after muscimol was applied. Light shaded open and closed circles that are unconnected by lines are the responses to noise alone. Error bars indicate S.E.M. across neurons.
4. Lick probability over time during muscimol or saline sessions. Dashed vertical lines indicate trial onset (0 s) and the contrast switch (3 s). Green traces are muscimol sessions and black traces are saline sessions. The shading around each trace indicates S.E.M. across sessions.
5. *Left:* comparison of lick probability during the adaptation period. *Right:* comparison of lick probability during the target period. Each circle indicates a session and color is as in **d)**.
6. Cumulative probability of licking throughout the trial, normalized within muscimol or saline conditions to sum to 1. Colors as in **d)**, **e)**. Shading indicates S.E.M. across sessions.

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