

Conformable Heart Sensors using Graphene-infused Silly Putty™

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Limitations

Trade off between sensor stiffness & resistivity

Relaxation makes it difficult to obtain long term

processing (DSP)

special equipment

measurements without additional digital signal

Response behavior depends heavily on morphology,

and sensor preparation (i.e. graphene loading factor)

Conclusion

Successfully resolved pressures as low as 40 mmHg

Sensing performance extremely sensitive to loading

factor making it versatile but also potentially imprecise

Sensor was flexible, conformable, and sensitive

• Graphene preparation (72 hr exfoliation) requires

Relatively low cost to create functional sensor

significant time investment, prone to overheating

• Using this putty as a heart sensor would require some

Motivation

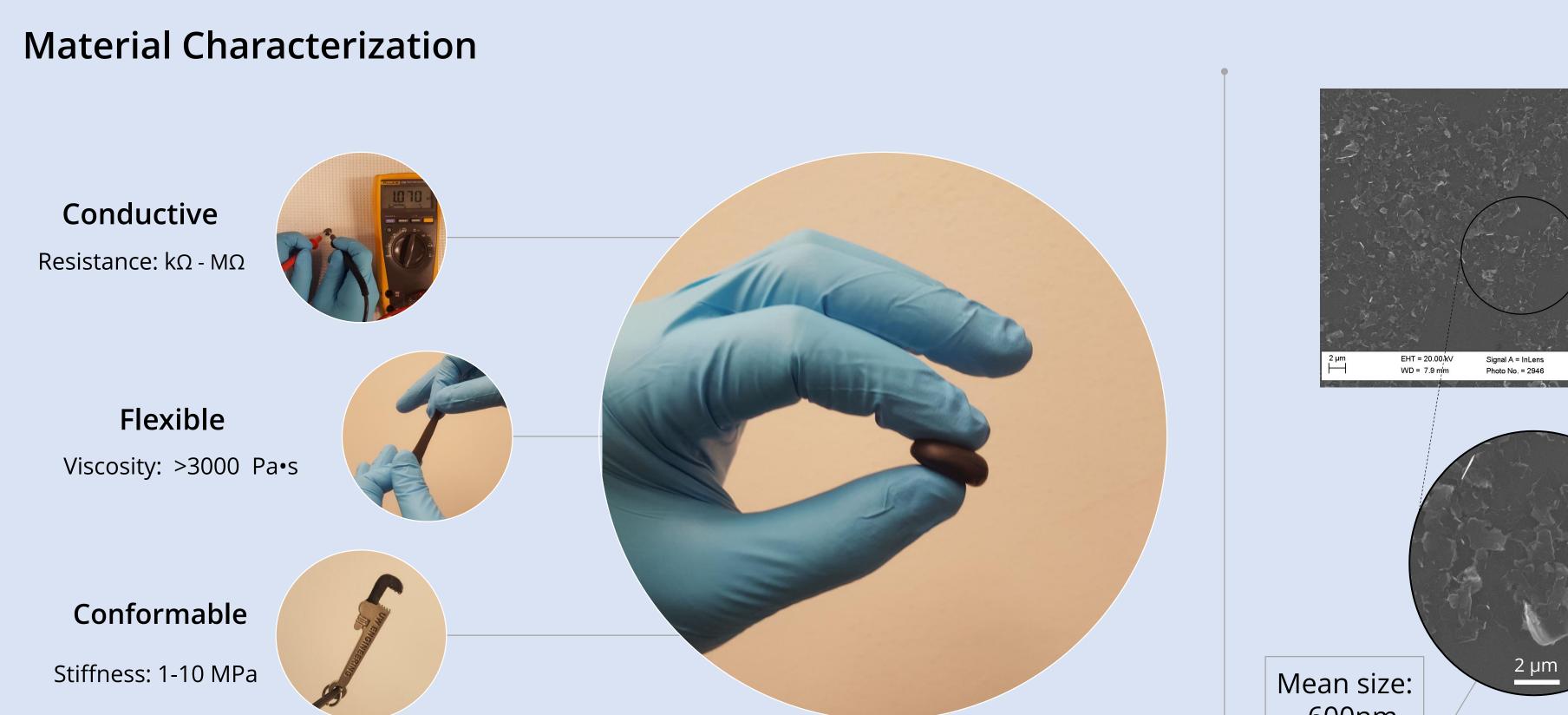
 Touchscreens & other modern sensors offer sensitivity at the expense of flexibility and **cost**

 A composite sensor made from graphene offers unparalleled flexibility & conductivity to accurately resolve skin w/out sacrificing sensitivity

 The demand for robust wearable sensors calls for sensors that are more conformable and **sensitive**

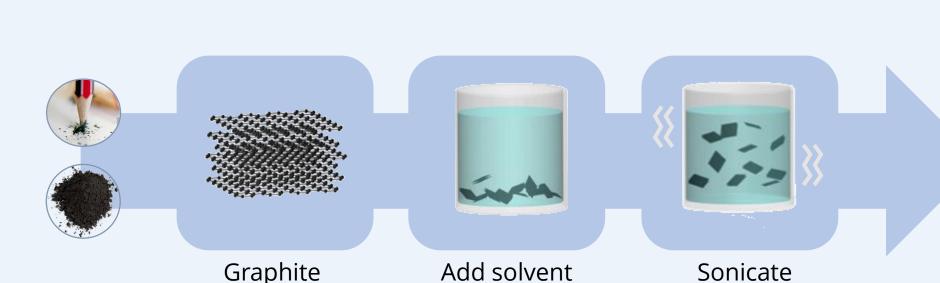
pressures of ~40 mmHg

Results



Methods

Graphene Preparation



- An organic solvent (NMP) stabilizes the exfoliation of the graphite sheets by means of tip sonication for 72 hrs
- Re-dispersing graphene in chloroform allows for easy evaporation after mixing

Sylgard 184 silicone oil (PDMS) is mixed

Stirring under high heat causes thermal

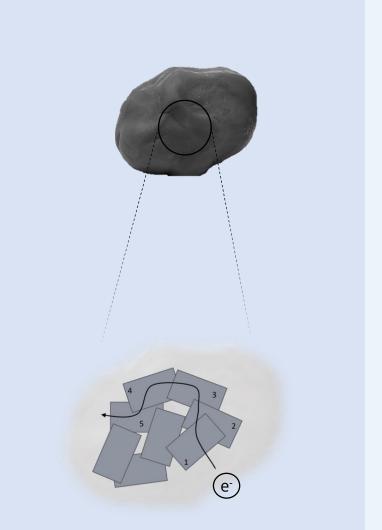
with finely ground boric acid

cleavage of siloxane bonds

Mechanism

 Impact can cause graphene network deformation resulting in an **increase** in overall resistance then relaxation as network is repaired

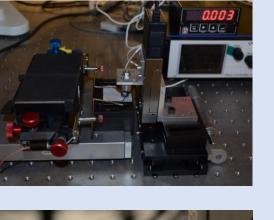
 However, for very thin sheets network is compressed and resistance decreases



5.E-09

Measurement Setup

- Piezoelectric load tester applies uniform normal force to active surface of sensors; precision power supply/DMM measures current for a fixed voltage
- Hardware interfaced with LabVIEW software for automatic data acquisition



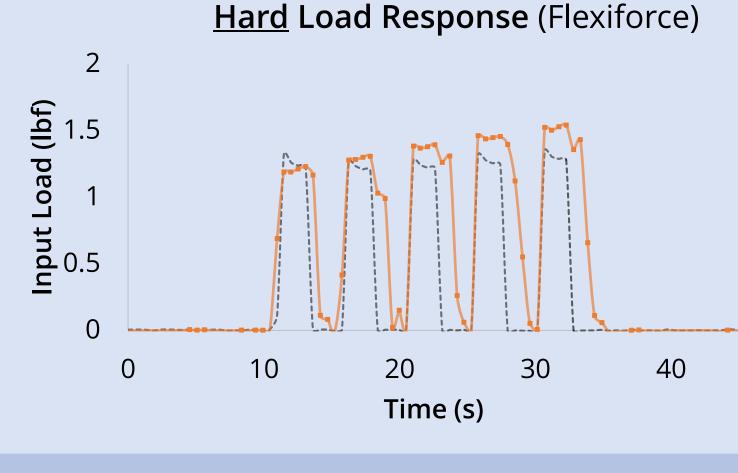


DSP Reconstructed **Original Signal** Signal fft (no drift) peak detection

extra data processing, careful consideration, and

 Reconstructed signal compatible with machine learning classifiers for use in short-term arrhythmia diagnoses

Sensor Characteristics







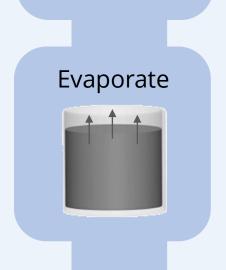


PDMS Putty

Graphene -

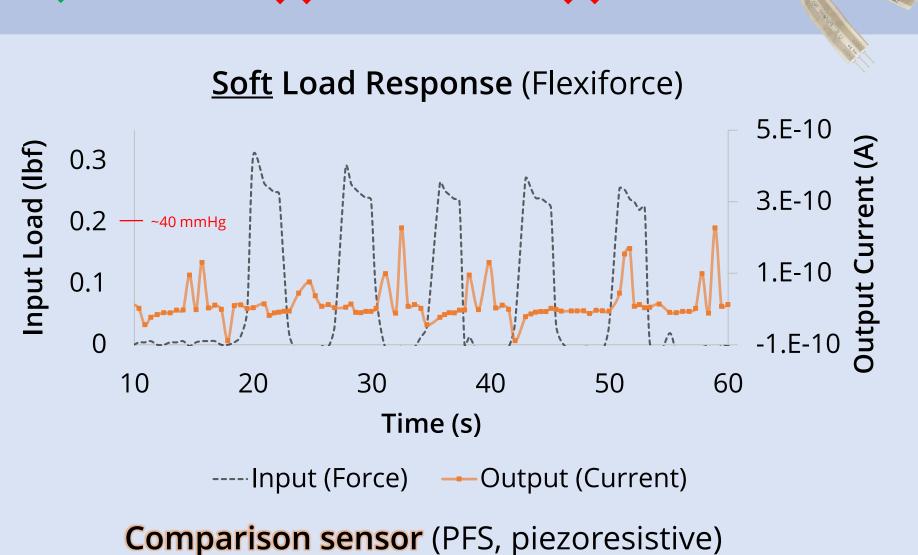
Graphene +

chloroform

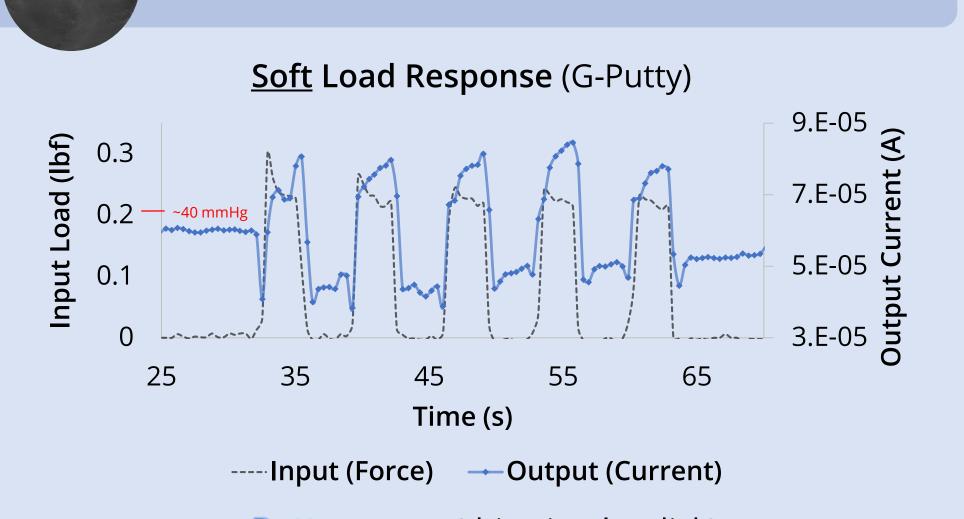




4.E-09 3.E-09 2.E-09 1.E-09 🕏 0.E+00 **X** Conformable **X** Sensitive **Soft Load Response** (Flexiforce)



Hard Load Response (G-Putty) 9.E-05 8.E-05 **₹** 7.E-05 5 6.E-05 5.E-05 🕇 4.E-05 0 Time (s) **Soft Load Response (G-Putty)**



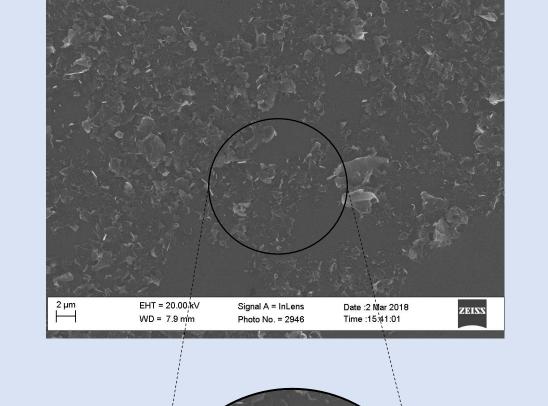
Acknowledgments

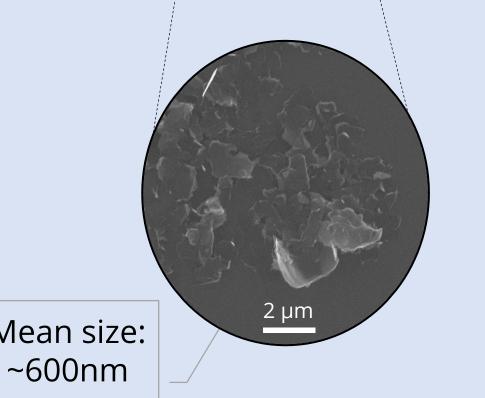
- Professor Vivek Maheshwari for lending his expertise and offering us his lab space and equipment for tests
- Velocity for allowing us to use their equipment
- Dr. Coleman and his team at Trinity College Dublin for being the first to demonstrate the potential for this material and providing help when needed

References

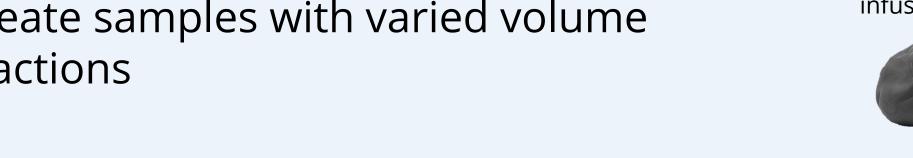
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 To detect blood pressure & heart rate with a singular sensor it must be able





Putty sensor (thin circular disk)



Boric acid forms reversible crosslinks with terminated bonds forming pristine viscoelastic white putty

Putty preparation

- Putty (~2 g) dissolved in 50 -100 mL of chloroform + graphene solution (~10 mg/mL) then mixed & sonicated
- Chloroform allowed to evaporate leaving a black conductive putty with variable resistance
- Stock putty mixed with pristine putty to create samples with varied volume fractions