

# ELEC3104: Mini-Project – Cochlear Signal Processing

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**TLT – Level 3 (Credit Level):** Using the Level 2 IIR cochlear filter bank model, implement a spectral analysis system.

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Complete TLT-Level 2 first and ensure that you are on the right track before proceeding to TLT – Level 3

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# Short-time Spectrum Analyser

- ✓ You should use the IIR filter bank that you have designed in TLT-Level 2 to implement a short-time spectrum analyser. The bank of filters separates the frequency spectrum of interest (88 Hz to 7725 Hz) into  $N (=128)$  frequency bands.
- ✓ In this mini-project we will continue to use two spatial differentiations in order to sharpen the magnitude response of the filters.
- ✓ The spatially differentiated bandpass filter outputs are passed through a hair cell model (a rectifier followed by a first-order lowpass filter). The output of the hair cell model is a measure of energy ( $E$ ) of the signal in a particular frequency band.

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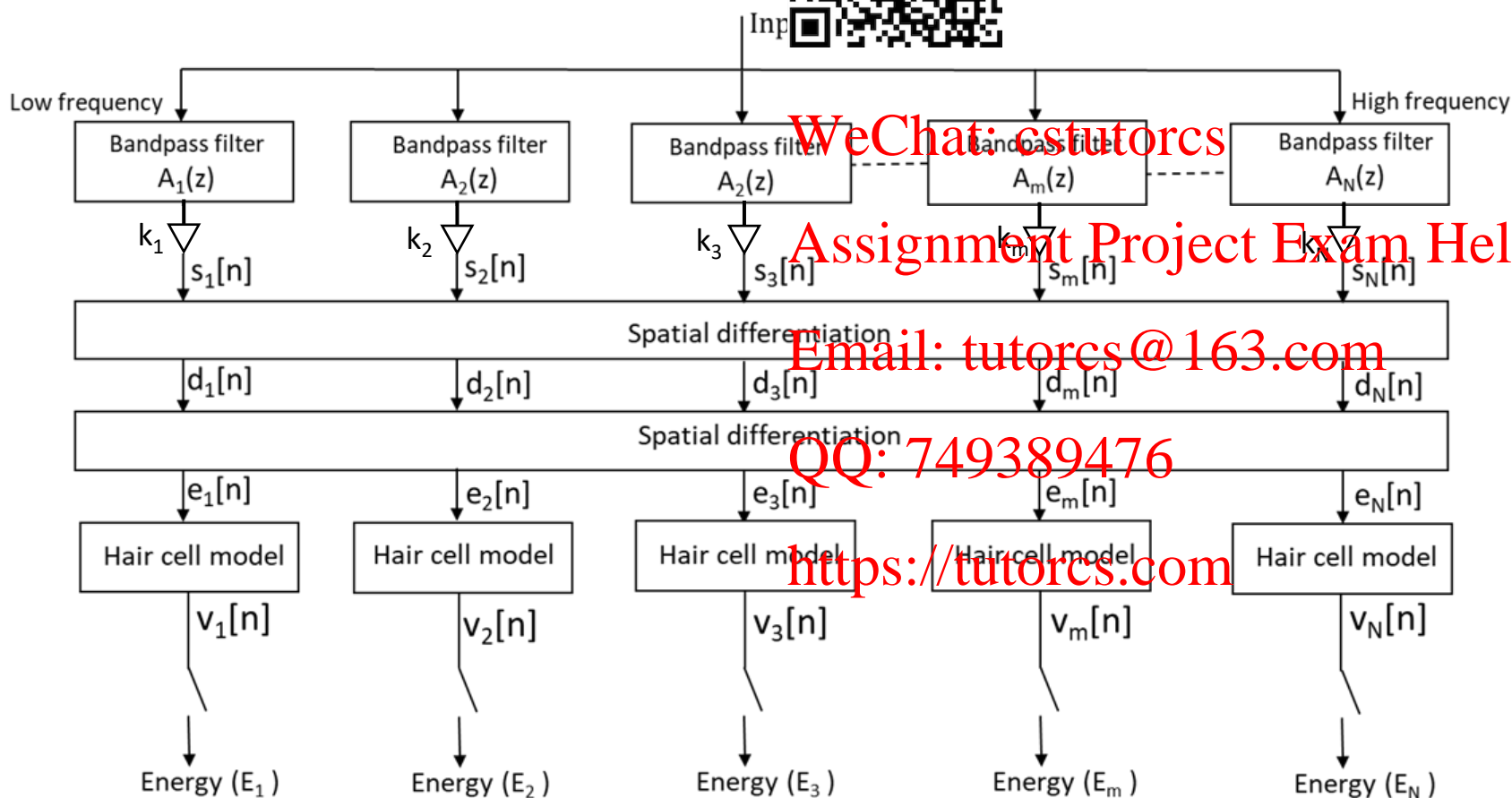
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**Note:**  $k_1 - k_N$  are the gain factors

Output Energy  $E_m$  is read (switch closed) once every 16 ms or so.

# Gain Factor Calculation ( $k_1$ to $k_N$ )

## Gain Factor Calculation for Filters $k_1$ to $k_N$

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- 1. Input Signal:** For each filter  $n$  (where  $n = 1, 2, \dots, N$ ) provide a sine wave of amplitude 1. The sine wave should have a centre frequency corresponding to the centre of the filter under consideration.
- 2. Filter Output:** Apply the sine wave to the filter and record the filter's output.
- 3. Maximum Value:** Measure the absolute maximum value of the filter's output, denoted as  $k_{max}^{(n)}$  for the  $n^{\text{th}}$  filter.
- 4. Gain Calculation:** The gain factor  $k_n$  for the  $n^{\text{th}}$  filter is calculated using the formula:  $k_n = \frac{1}{k_{max}^{(n)}}$
- 5. Repeat for All Filters:** Repeat steps 1 to 4 for all  $N$  filters to obtain the gain values  $k_1$  to  $k_N$ .

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# Spatial Differentiation and Inner hair cell model

## Spatial Differentiation

- ✓ Spatial differentiation of the membrane displacement represents coupling between the cilia of the inner hair cells, through the fluid in the subtectorial space.
- ✓ Spatial differentiation refers to taking the difference with respect to the position (along the basilar membrane). The discrete model is given by:

$$d_m[n] = s_m[n] - s_{m+1}[n] \quad \{e.g. d_1[n] = s_1[n] - s_2[n]\}$$

- ✓ The second spatial differentiation is given by:

$$e_m[n] = d_m[n] - d_{m+1}[n] \quad \{e.g. e_1[n] = d_1[n] - d_2[n]\}$$

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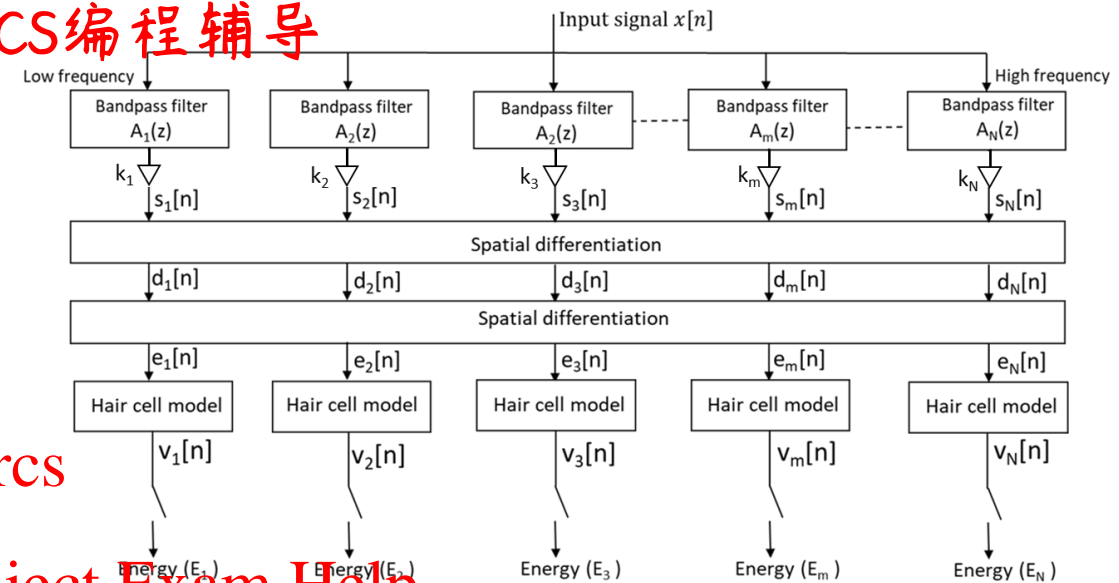
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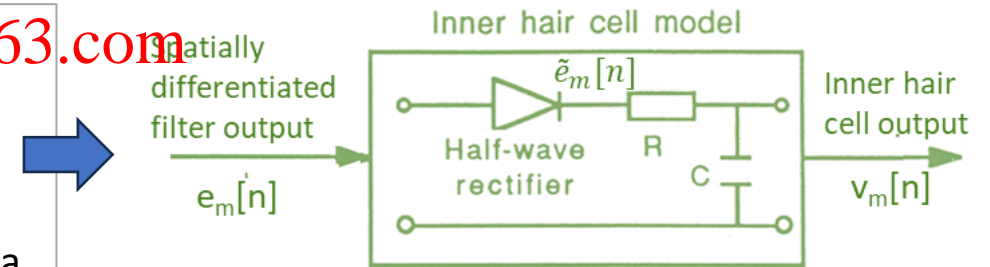


## Inner hair cell model

- ✓ The model of an inner hair cell is a capacitor model, in which the input voltage corresponds to the spatially differentiated membrane displacement output of the filter bank model.
- ✓ Bending the inner hair cell cilia (Half-wave rectification) is simulated by charging of the capacitor, and returning to the initial position of the cilia is equivalent to discharging the capacitor.
- ✓ This model is given by the following input-output relationship:

$$v_m[n] = (1 - c_0)\tilde{e}_m[n] + c_0 v_m[n - 1] \quad \text{where } c_0 = e^{-2\pi \frac{f_c}{f_s}}$$

Where,  $v(n)$  is the output electrical energy,



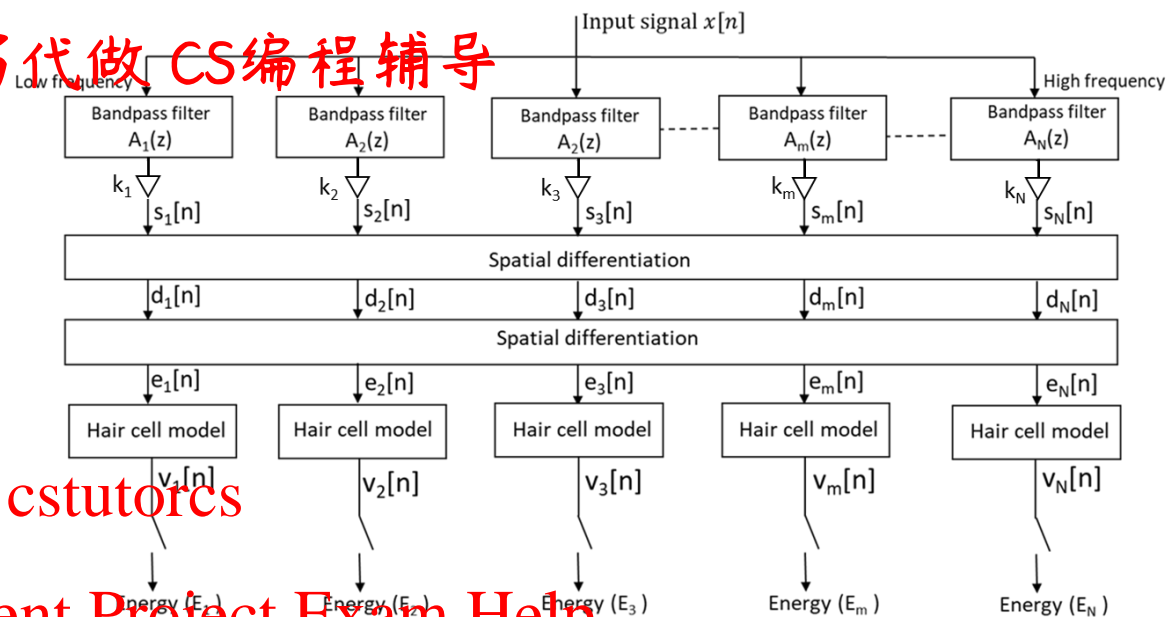
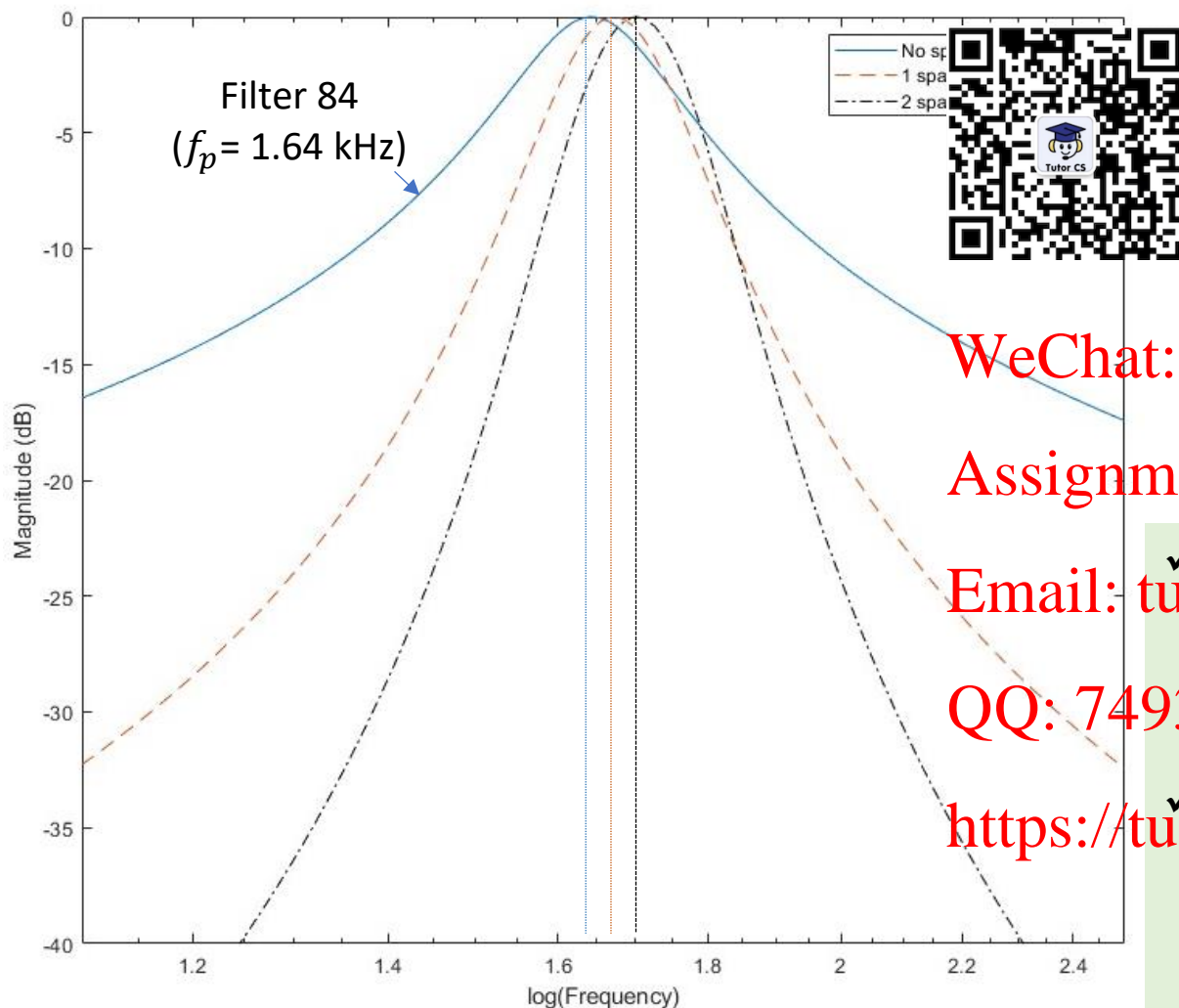
$\tilde{e}[n]$  is the spatially differentiated displacement after half-wave rectification.

Cut-off frequency ( $f_c$ ) of the hair cell model is based on the rate at which the switch is closed. (every 16 ms – 62.5 Hz). Therefore,  $f_c \leq 31.25$  Hz. Let's choose  $f_c = 30$  Hz; Sampling frequency ( $f_s$ ) = 16000 Hz.



# Are you on the right track?

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✓ If your implementation of the spatial differentiation is correct, you should get the magnitude response similar to the one shown in the diagram on the left, for the filter 84 with a centre frequency of 1640 Hz.

✓ You might notice that the centre frequency of each filter has shifted slightly with each spatial differentiation, and the filter shapes have become sharper, with a steeper slope. Why do you think this is the case?

# Are you on the right track?

- ✓ Apply a sum of two sinusoidal components (704.6 Hz [Filter no:60] and 2.88 kHz [Filter no: 100]) at the input  $x[n]$ .
- ✓ Plot the output  $\{s_1[n] \text{ to } s_N[n]\}$  of each filter against the filter number at a particular time instant .
- ✓ Repeat the above step for the output  $\{d_1[n] \text{ to } d_N[n]\}$  and  $\{e_1[n] \text{ to } e_N[n]\}$  at
- ✓ Do you notice any differences between these three plots?
- ✓ The inner hair cell output shows the spectral component

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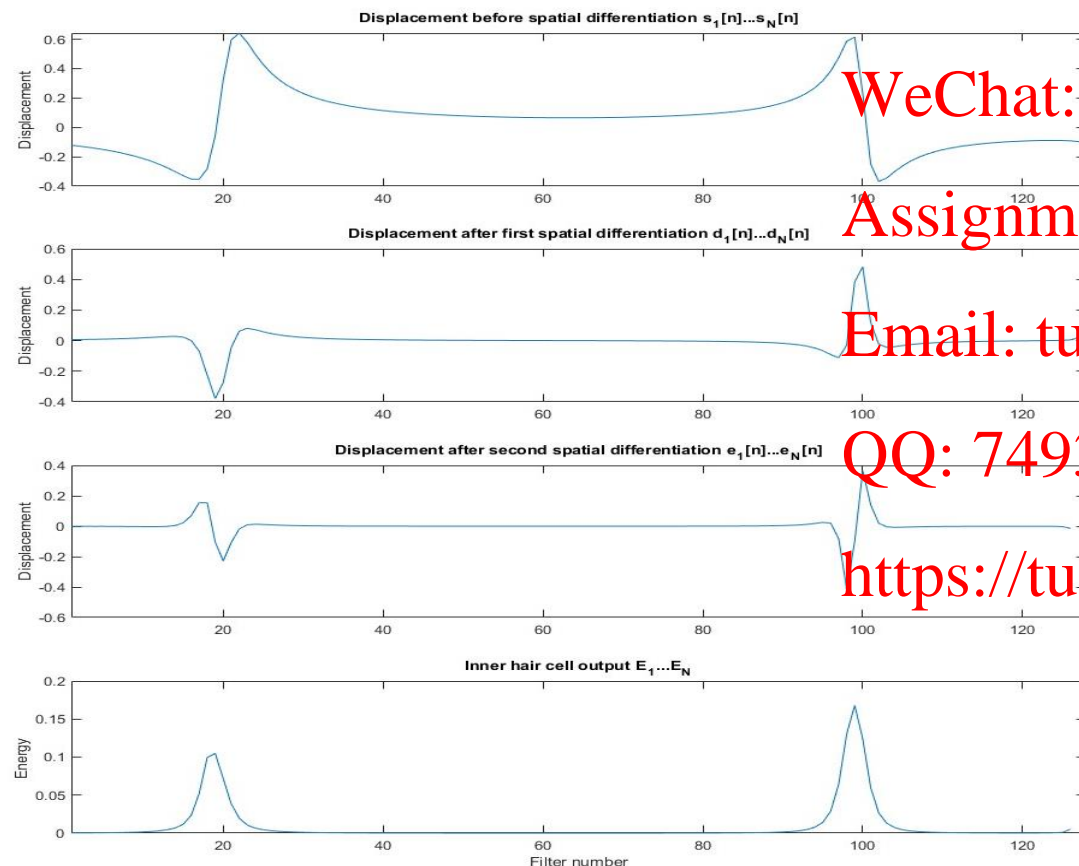
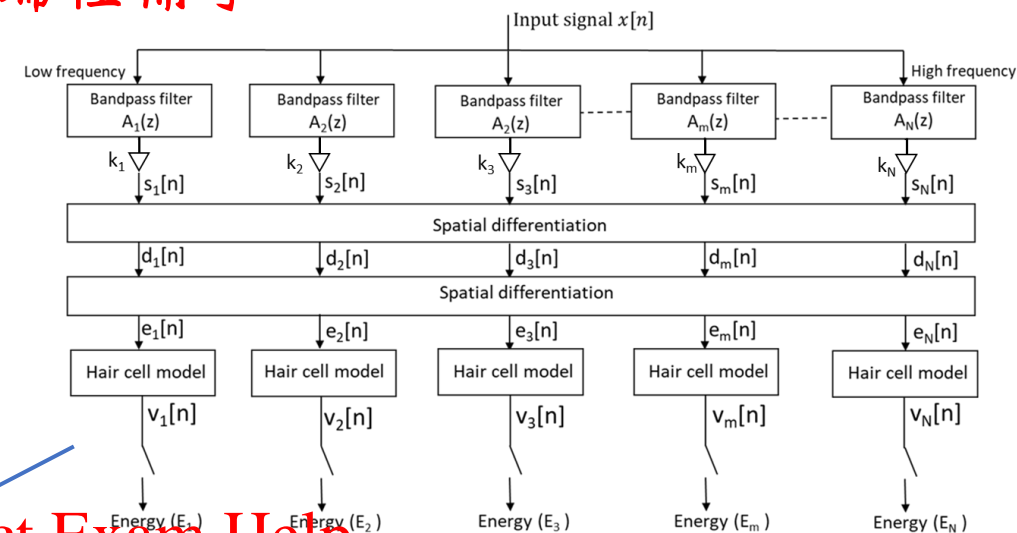
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- ✓ The figure on the left shows the spatially differentiated basilar membrane displacement ( $e_1[n] \text{ to } e_N[n]$ ) and the corresponding inner hair cell output in response to a sum of two sinusoidal components applied at the input (704.6 Hz [Filter no:60] and 2.88 kHz [Filter no: 100]).

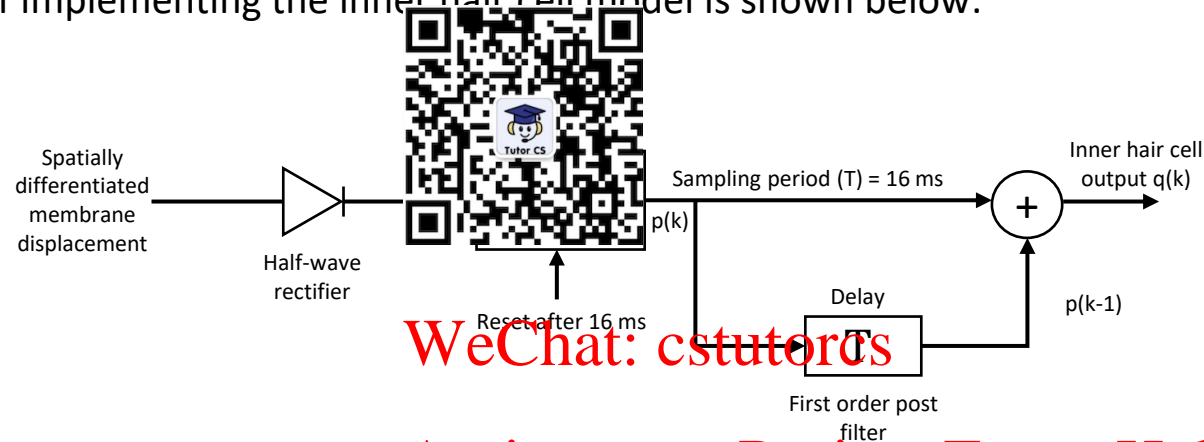
- ✓ If your implementation of the spatial differentiation is correct, you should get results that are very similar to the diagram on the left for a sum of two sinusoidal input.

# TLT-Level 3: An alternative inner hair cell model

## An alternative inner hair cell model

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- A second method of implementing the inner hair cell model is shown below:



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- In this model the positive cycle of the spatially differentiated (twice) membrane displacement is accumulated at each sampling instant and then the accumulated value is digitally filtered. (Post-filtering) at the end of each 16 ms frame. The accumulator is reset at the end of 16 ms frame.
- Replace the previous hair cell model with the above model.
- What is the main difference between the above hair cell model and the previous hair cell model in slide 4, TLT level 3? Discuss your understanding with your lab demonstrator.

# Are you on the right track?

## Final Implementation

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- Apply a signal which is a sum of six sinusoids, 1000-2000 samples, of equal amplitude and frequencies of your choice, to the input of the filter bank. Plot the output of the speaker (i.e the output of each filter in dB against the filter number) at a particular time instant.
- Plot the magnitude spectrum (using FFT) of the input signal and compare it with the filter bank output. Discuss the results that you get.
- Note that the sampling frequency of the input signal is 16 kHz and the output signal has a sampling interval of 16ms (62.5Hz). Explain why it is necessary to have a lower sampling rate at the output? What are the implications for the cut-off of the output LPF (see hair cell model) if we require a sampling of the output (close the switch) twice as often (125Hz)?
- Apply your own recorded voice at 16 kHz sampling frequency as an input and observe the hair cell output at a particular time instant. What do you notice? Discuss your observations with your lab demonstrator.

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