

# **The influence of age on the ability to use Brain-Computer-Interfaces**

**Use-case: TV remote control**

**Masters Thesis**  
**To obtain the academic degree M.Sc.**

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## **Abstract**

In recent years, Brain Computer Interfaces - BCI in short - evolved to a level of maturity which allows for these devices to be produced cheaply and thus being available to consumers. The newest example with extensive media coverage was the video published by Elon Musks *Neuralink* where a monkey learned to play pong. The study in this thesis uses a device from a manufacturer called *Nextmind* to examine whether age has an effect on the ability to use such a device. A study was carried out with a number of **XXX** participants from different age groups. They were confronted with a task to use a Graphical User Interface to select elements by looking at them. **not finished**

# 1 Introduction

In recent years significant progress has been made on the development of interfaces which relies on direct interaction with the brain itself. The latest popular example is Elon Musks *Neuralink* with their monkey learning to play the game *Pong* only by using its brain ([Neuralink \(2021\)](#)). Apart from a solid scientific methodology, this study also presented a good media coverage including a showcase video which went viral. However there are more examples of a working interfacem, which will be discussed in section 1.4, since this vast area of resarch is an intersection between several areas of research: medical engineering, neuroscience, computer science and HCI<sup>1</sup>. These interfaces are generally called *Brain-Computer-Interface* or *BCI* in short. [Microsoft Research \(23/10/2020\)](#) has a very precise definition of the scope:

*Brain-Computer Interface (BCI) is a system that measures central nervous system (CNS) activity and converts it into artificial output that replaces, restores, enhances, supplements, or improves the natural CNS output and thereby changes the ongoing interactions between the CNS and its external or internal environment. BCI is direct communication pathway between an enhanced or wired brain and an external device.*

As of Q2 2021 there are already devices available for consumers to buy, which fall into this category. This opens up possibilities for a widespread application of these kind of interfaces. Nevertheless, new ways of interacting with computers require some degree of research to define useful and user-friendly ways to interact with such technology. This study aims to provide insight into one aspect of this process.

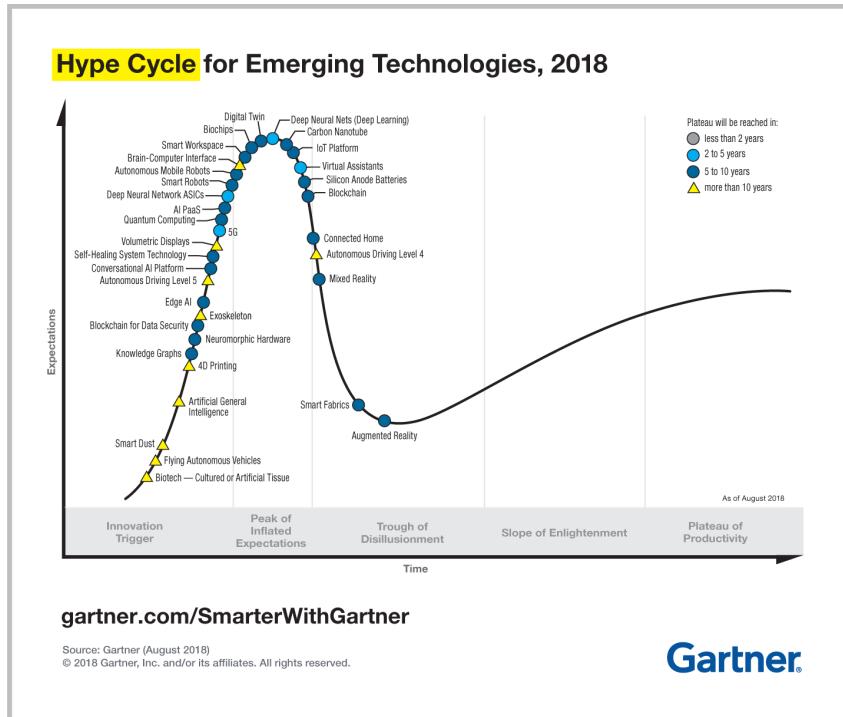
After a thorough disussion about the state of research in this field, the research hypothesis will be defined based on considerations about future use cases. Subsequently a user survey will be designed, carried out and conclusively evaluated to put the results into context.

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<sup>1</sup>Human Computer Interaction

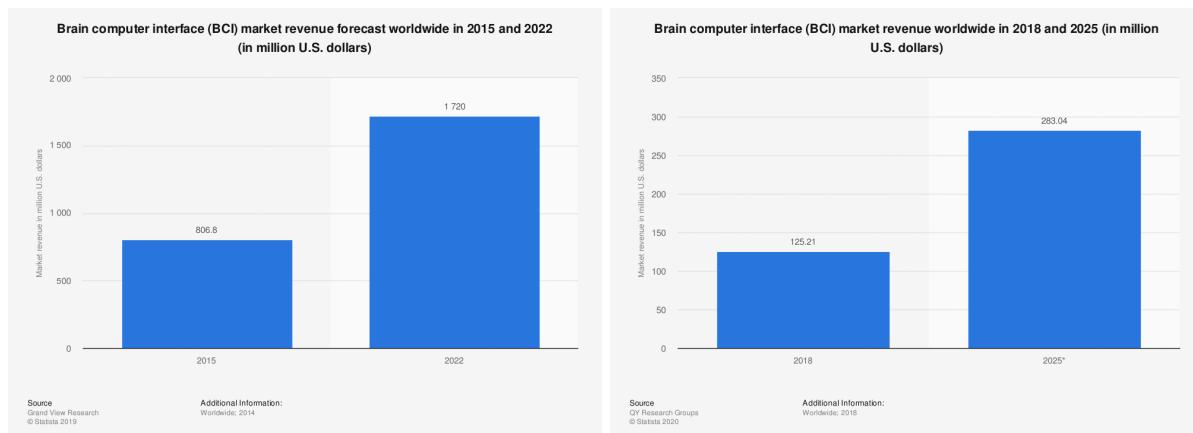
## 1.1 Management Summary

In the *2018 Gartner Hype Cycle* report ([Gartner \(24/05/2021\)](#)), which is shown in figure 1.1, BCIs are denoted as to be on the brink of the peak of inflated expectations:



**Figure 1.1:** Gartner report of emerging technologies 2018

It is important to note though that as of 2018, it'll still take more than 10 years to reach a plateau of productivity. Although there is no mention about this technology in subsequent reports in the following year, two market revenue forecasts from 2015 until 2022 and 2018 until 2022 show a similar pattern in figure 1.2.



**Figure 1.2:** Statista revenue forecast as of 2015 and 2018

Essentially the market revenue expectation has been very inflated from 2015 on so that it was corrected downwards in 2018. But although the absolute growth was projected to only a small fraction, the relative growth potential stayed about the same of doubling within the next seven

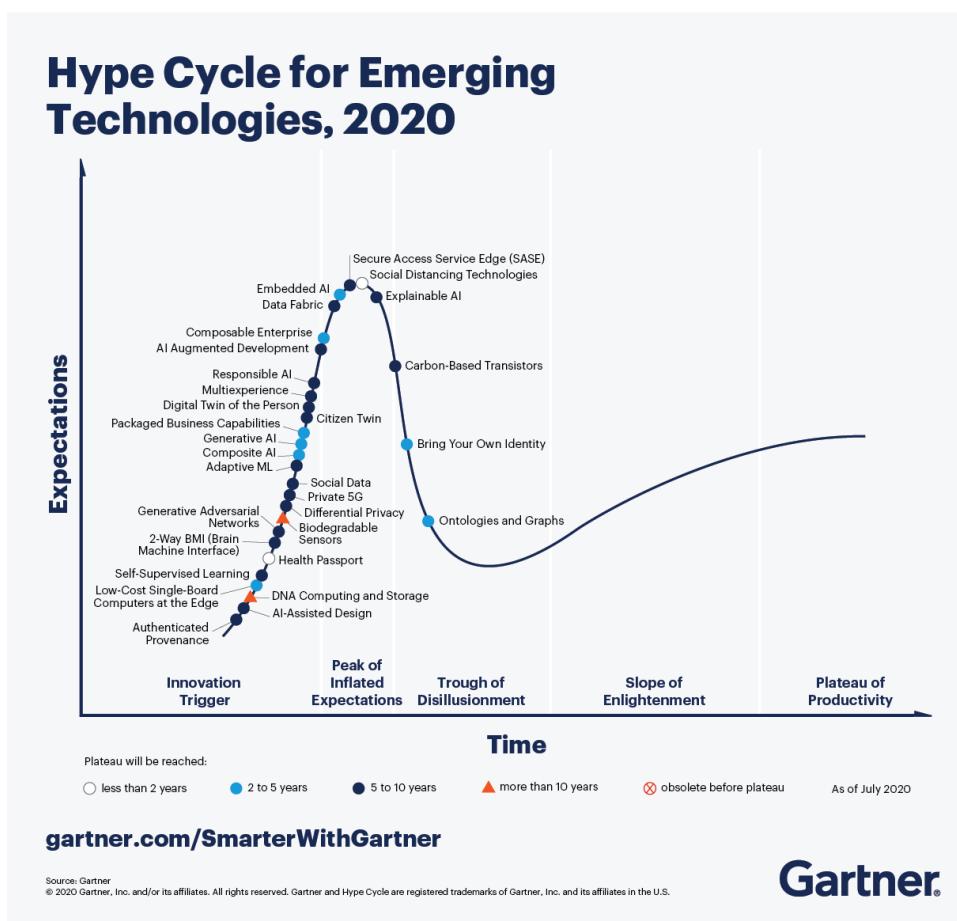
## 1 Introduction

years. This is very indicative for the technology being overhyped, as Gartner explains: ([Gartner \(24/05/2021\)](#))

*A wave of “buzz” builds and the expectations for this innovation rise above the current reality of its capabilities. In some cases, an investment bubble forms, as happened with the web and social media*

Nevertheless, what this technology sets apart from other featured technologies is the fact that it has been around for a few decades and has been continuously researched upon. A strong indicator is the amount of organizations and conferences held about this entire discipline, as can be seen in section 1.4. The fact that it has only been on the radar of early adopters and tech-enthusiasts in conjunction with market revenue projections is a strong indicator that this technology has reached a level of maturity which makes a widespread application outside of laboratories somewhat feasible.

The latest *2020 Gartner Hype Cycle* report shows already the enhanced version of bidirectional BCIs (titled "*2-Way Brain Machine Interface*") on the slope of innovation:



**Figure 1.3:** Gartner report of emerging technologies 2020

All in all, there are strong indicators that the technology gained traction over the last few years and could be considered a worthwhile investment if approached with care.

## 1.2 Brain-Computer-Interfaces

In this section a general overview of the working principle of these interfaces will be provided. Since this study is aimed at computer science and HCI<sup>2</sup>, the neuroscience and medical domain will be only covered very briefly.

First studies began by [Vidal \(1973\)](#), who investigated the possibility to use EEG<sup>3</sup> waves, which were first recorded by [Berger \(1929\)](#), as a way to create a direct interaction between a machine and a human brain.

There are three types of BCIs: invasive, partially invasive and non invasive. This depicts the degree of intrusion into the skull and brain tissue. *Invasive* BCIs are electrodes, which are implanted directly into or onto the grey matter of the brain. This can cause long term issues like scars and also degraded signal strength according to [Abdulkader et al. \(2015\)](#). Partially invasive BCI however are although located within the skull not in direct contact with the grey matter. Non-Invasive BCI are only placed on the head without intrusion of any tissue. Due to the direct contact, invasive BCI provide the best resolution of the measured signals. Non-invasive BCI in comparison suffer from signal degradation and deformation of the cranial bone tissue. Therefore partially invasive BCI are a compromise between good signal strength and the risk of medical conditions. Another potential advantage of non-invasive BCIs is that these Interfaces could be easier mass-produced and become affordable to consumers. Also they don't require specialized medical knowledge and equipment to operate.

The way these interfaces work is based on the same principle: A human brain emits electrical signals, which can be picked up. According to [Vidal \(1973\)](#), they can be described as follows:

*"Embedded in this sustained "spontaneous" or "ongoing" electrical activity, short, distinctive (0.5-2 sec) waveforms can be found that are evoked, for instance, when a brief sensory message (stimulus) such as a brief illumination of the visual field or a tap on the forearm is received by the subject."*

Based on the origin within the brain, these can be correlated to certain stimuli, mental and emotional states ([Jardim-Gonçalves \(2018\)](#)) and according to [Waldert \(2016\)](#) been used to drive *an external effector or affecting internal body parts and functions*. The external effector is the use case which is being examined in this study.

Without a BCI, interaction with a computer requires some physical interaction with devices such as keyboards, mouses or gestures on a touch screen. There are mainly two different reasons, why these devices are a constraint to speed and efficiency of HCI. The first reason is a limitation on interaction speed: Although there is no definitive consensus about the speed of thinking, alone being able to type along the spoken word is unattainable for non-professional typists. A professional typist has to be able to type at 180 - 220 WPM<sup>4</sup> according to [NCRA \(25/05/2021\)](#). [ScienceDaily \(25/05/2021\)](#) made a survey with 168.000 volunteers, where the fastest typists weren't even able to come close to this mark with 120 WPM. Therefore it is safe to assume that typing in the same speed as thinking is impossible except for rare individuals who devoted a significant time practicing. Secondly: in applications such as games, where reaction time and accuracy is the fundamental element for success or failure, an interaction based on motoric interaction with a physical pointing device has some significant drawbacks like limited accuracy, if the whole chain of wrist movement in conjunction with a mouse is under scrutiny.

If a BCI was to replace these types interaction, these constraints could potentially be alleviated and interaction based on physical interaction rendered obsolete.

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<sup>2</sup>Human Computer Interaction

<sup>3</sup>Electroencephalogram

<sup>4</sup>Words Per Minute

### 1.3 Working principle

Before any deeper considerations in regard to the general scope of this study can be made, it is important to understand the working principle of the BCI, which will be used. Although the vendor of the BCI in question does not disclose any details of the inner workings itself, it is safe to assume that the underlying technique used is the so called *Steady State Visually Evoked Potential* - SSVEP in short. [Sokol \(1976\)](#) provides detailed inside into the topic from a neuroscientific point of view. The general principle however is that any visual stimuli cause a certain pattern of waves within the visual cortex of the brain. These patterns can be used to evaluate if a certain pattern is being seen *and* in focus of the person.



**Figure 1.4:** How VEP works in principle [citation?](#)

This is being done by subsequently feeding the sensor data through a trained neural network. The objects, which are being seen by the person, have been labeled *neurotags* ([NextMind \(23/11/2020\)](#)) from the vendor of the BCI. These neurotags can provide two different readouts: If it is triggered (i.E. *seen*) and the confidence, which depicts the level of *focus* of the user on the neurotag ([NextMind \(18/11/2020\)](#)).

The physical layout of the sensor is shown at figure 1.5. It has 18 electrodes, which are arranged in pairs to cover the area, where the visual cortex is located at the back of the cranium. It is battery driven and communicates via the Bluetooth LowEnergy protocol.

### 1.4 Related work

As previously mentioned in section 1, research on BCIs is partitioned between four different domains: *medical engineering, neuroscience, computer science and HCI*. Apart from commercial entities such as *Microsoft* or *IBM* and scientific journals, the majority of the research community is clustered in three organizations:

- ICBCI (*International Conference of Brain Computer Interfaces*), which is a department of the WASET (*World Academy of Science Engineering and Technology*)
- EMBS (*Engineering in Medicine and Biology Society*), which is a department of the IEEE
- BCI Society, which is an entity of its own



**Figure 1.5:** Physical layout of the sensor

There are also research efforts in the east-asian region, according to corresponding tech-sites such as [Global Times \(20/04/2021\)](#) and [Techwire Asia \(24/05/2021\)](#) but due to a language barrier, these sources cannot be considered.

To narrow the scope, where this research paper is located at, the considerations from section 1.5 are taken into account. As already established in section 1.3, the sensor used in this study uses SSVEP and is non-invasive in nature. Therefore the general scope of this research is located in the realm of *non-invasive BCI based on SSVEP used for HCI*.

[Oralhan and Tokmakci \(2016\)](#) and [Resalat et al. \(2011\)](#) investigated the effects of different twinkle frequencies and duty cycles on the efficiency on precision of SSVEP BCI. They found that a certain combination of these parameters in fact could improve the ITR<sup>5</sup>. [Lee et al. \(2016\)](#) used a similar approach and found the ideal combination in conjunction with Korean characters. [S. M. Abdullah \(2014\)](#) used a consumer ready BCI by *EMOTIV* to create a *Matrix-Speller* in the Bengali-Language to allow people who have lost the ability to communicate to express themselves again. [Chen et al. \(2020\)](#) also used a SSVEP BCI to implement a BCI-speller and scrutinized the tradeoff between responsiveness and accuracy. [Chen et al. \(2020\)](#) designed an interface which is operated by a SSVEP BCI to control a robot arm, which could administer food to disabled people. [Soroush and Shamsollahi \(2018\)](#) developed a SSVEP BCI which overcomes the necessity for training the sensor to the user who wears it. The prototype reached a similar precision as *trained* interfaces. [Gergondet and Kheddar \(2015\)](#) investigated and selected certain visual stimuli which work best with certain use cases. [Meriño et al. \(2017\)](#) made a study, where participants controlled a UAV by using a SSVEP. [Peters et al. \(2018\)](#) used simulated impairments to examine if usage of a SSVEP is still possible with medical conditions which affects speech and ocular impairments.

Although not strictly within the SSVEP domain, the study by [Beveridge et al. \(2017\)](#) showed very promising results by not using visual stimuli but mechanical ones, where he had teenagers playing a racing videogame with the aid of mechanical stimuli.

There is a massive ongoing research effort to make the life of people who are suffering under ALS<sup>6</sup> better and improve their ability to communicate normally, by using SSVEP, a hybrid

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<sup>5</sup>Information Transfer Rate

<sup>6</sup>Amyotrophic lateral sclerosis

between an SSVEP and P300<sup>7</sup> or purely P300 based BCI. A significant number of relevant studies has been published in the BCI Society Journal: Sugata et al. (2016), Holz et al. (2015), Speier et al. (2017), Geronimo and Simmons (2017), Speier et al. (2018), Mowla et al. (2017), Huggins et al. (2016). All these studies aimed to provide a better understanding and performance of using BCI on people with medical conditions, which cause serious physical impairments.

### 1.5 Establishing a use-case

Establishing a use-case in the context of this study is a pivotal point hence this section will be split up into several sections:

1. General considerations
2. Deduction of the core points of this study
3. Evaluating the constraints of a participatory study
4. Deduction of use-case
5. Conclusion into hypothesis and use-case

#### 1.5.1 General considerations

The first step in conceiving any potential way of using such a device is to evaluate the way any user could interact with a BCI with a computer. According to (Buxton 2010: 4.13) the way users interact with a device require an agent of control i.e. a hand, what is being sensed by the device (position, motion or pressure) and the number of dimensions being sensed (1, 2, 3). This results in a different input taxonomy for any given device. However, a BCI does not have either of these parameters, since the interaction does not require physical interaction. Hence a classification by means of using a taxonomy cannot be achieved. Where the interactions of BCIs can be compared to those classified by taxonomies is by the way they function they apply in relation to a user interface.

The API<sup>8</sup> endpoints of the NextMind sensor offers two different modes of interaction. These are explained in the SDK<sup>9</sup> of the sensor in detail: NextMind (18/11/2020). They are depicted as *tracking results* with a *hit* property and a *confidence* metric. Where *hit* is a two state interaction: the neurotag is being seen by the user and subsequently recognized by the sensor and its backend or it is not. The *confidence* property depicts the attention which the user is paying to the *neurotag*. This is a continuous decimal value between 0 and 1. The fact that these types of interaction are based on neural activity raises the question if a pure mapping of continuous and discrete input modalities to established interfaces would be beneficial to the user experience. Under the reasonable assumption that without any training the metric *focus* can only be deliberately controlled on a very coarse level, the necessary sensitiveness required for modern GUIs<sup>10</sup> can not be achieved with this particular sensor. The remaining two state property, which can be utilized to select or deselect certain objects also only allows for limited interaction. However, these neurotags can be placed in arbitrary places. Although a *toggle*-like behavior is not mentioned explicitly, it might be possible to de-select any activated neurotag when the *focus* property falls under a certain value.

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<sup>7</sup>An Event Related Potential (ERP) BCI

<sup>8</sup>Application Programming Interface

<sup>9</sup>Software Development Kit

<sup>10</sup>Graphical User Interface

### 1.5.2 Corepoints of this study

Based on the previous reasoning, the following questions can be raised in regard to the feasibility of any interface which could potentially be conceived with this technology:

1. How fast is the perceived and measured reaction time of these neurotags?
2. What is the minimum size the neurotags have to have in order to be recognizable?
3. Is the interface usable for brains of all ages or do gerontological effects have an effect on usability?
4. Do certain medical conditions (i.e. attentiveness disorder) have an impact on the usability?
5. How fast can a user switch between neurotags?
6. Is a BCI controlled GUI intuitive to use?
7. Does a personal affinity to technology have an influence on the perceived difficulty of interaction?

These questions can be clustered into two groups: *neurological* and *interaction*. But all these considerations open up a vast space of potential cases, hence the priority is to examine whether these interfaces are generally usable by the majority of users and if these interfaces are intuitive to use. Out of this list only the points 1, 2, 3, 5, 6 and 7 can be applied to a general audience. Considered the possible interactions with the *Nextmind* sensor, a study which focusses on the neurological domain makes more sense in the context. **Revisit reasoning.** This leaves the points 3 and 5. Although these are two different topics, the setup of the experiment itself will show that in fact number 5 can be examined along the way as well, which will be discussed in section **Add ref + revisit argumentation.**

### 1.5.3 Constraints of a participatory study

Although this study won't use the *AttrakDiff* survey, which was designed by Hassenzahl (30/09/2020), it is still worth considering how a potential use-case might perform in the context of an *AttrakDiff*. The reasoning is that a survey, which is entirely constructed to serve the purpose of producing results in favour of the study, might be harder to grasp for the participants in the experiment. The reason being that an interaction purely for the sake of interacting with something does not provide an incentive for the user to do so. As a consequence, the results which are produced by the participants, might be skewed due to a lacking frame of reference.

Figure 1.6 shows two axes which depict the hedonistic quality of an interaction, which is a metric of pleasure and the pragmatic quality which depicts a metric of *ease of use* or *technical quality*. Even without any deeper knowledge it is safe to assume that it is preferential for the interaction to be located in the upper right corner, since this makes it "*desireable*" instead of "*unnecessary*". Given that, it is certain that any interaction needs a way to facilitate pleasure in the user.

### 1.5.4 Deduction of use-case

Concluding the two parameters *frame of reference* and *facilitation of pleasure* into a coherent picture, it can be inferred that the experiment has to be set up in a way that gives the participants a familiar use case which facilitates positive feedback.

As already established, this study will examine gerontological effects in the context of an interaction. Therefore the age of participants will very likely vary to a wide degree, what necessitates a use case which is common to all age groups alike. Because people above a certain



**Figure 1.6: MAKE ENGLISH AttrakDiff results for a given interaction model, Source: Hassenzahl (30/09/2020)**

age did not grow up with computers, an experiment which relies heavily on the usage of computer as main point of interaction is very likely not a good choice due to the difference in proficiency. One example where both these criteria are met is a remote control for a television. Although nowadays there are computers involved, the interaction hasn't really changed in the last decades on a general level.

Nevertheless the working principle of the BCI is a visible flashing pattern, as established in section 1.3. Therefore the representation of some kind of GUI on a display is still necessary. Since VR goggles provide better isolation from external visual stimuli, the representation within a VR application was chosen.

### 1.5.5 Concluding hypothesis and use-case

Section 1.5.2 established that age is the first parameter to examine in this context, therefore the fundamental research hypothesis can be defined as follows:

*"Age does not have a detrimental effect on the ability to use a non-invasive BCI based on VEP technology."*

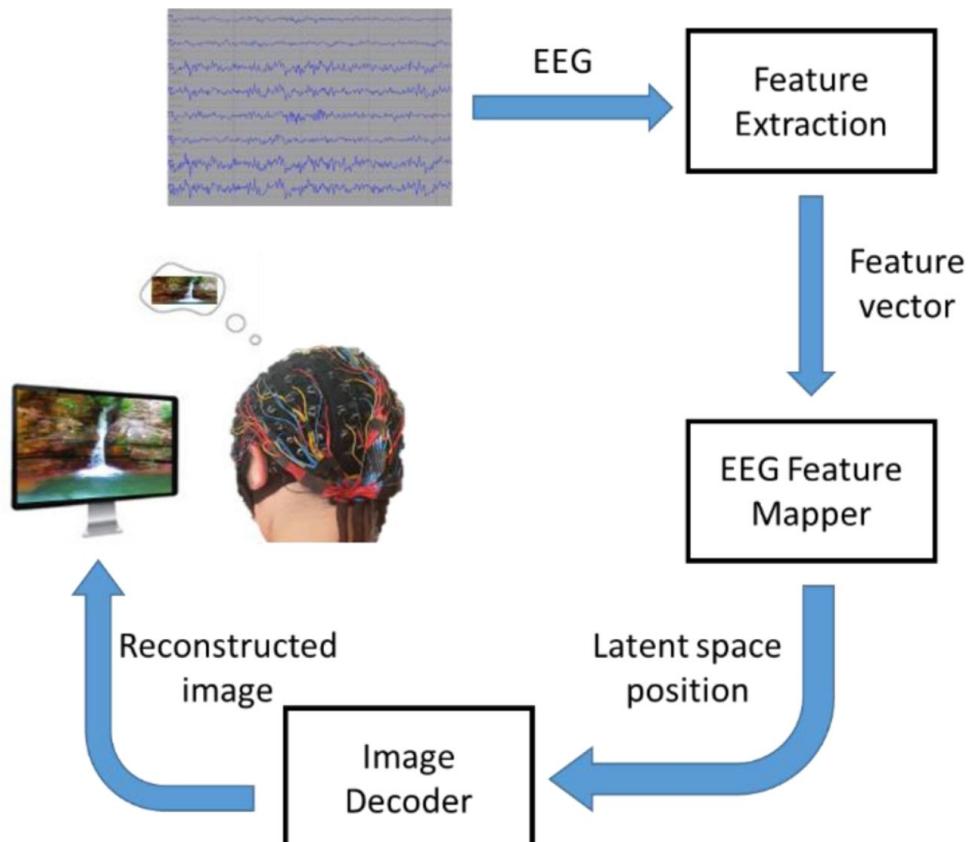
In Section 1.5.4 the fundamental reasoning behind the use case, which provides the necessary framework for this study was established:

*A GUI which represents a tv remote control will be presented to the participants within a VR environment.*

## 1.6 Beyond the scope

The case in this study is fairly limited in the realm of BCI. Section 1.4 already briefly mentioned that the general research on BCI has several fascinating topics to explore. This section aims to broaden the horizon on the realm of BCI technology.

**Picture synthesis** In 2019 [Rashkov et al. \(2019\)](#) published a paper which outlined the reconstruction of images seen by individuals by means of a BCI. They used a 128-channel EEG cap to record brainactivity in a 1...35Hz bandwidth while being shown videos of different subjects. The signals were treated with a PCA<sup>11</sup> to create a 20-dimensional feature vector which is feeded into a classification model, which yields the results:



**Figure 1.7:** General scheme of neurofeedback model, Source: [Rashkov et al. \(2019\)](#)

[O’Neill \(14/11/2019\)](#) wrote a good summarized article about the paper alongside results and a video which features a demonstration. On the other hand [Hernandez-Carmona and Penalosa \(2019\)](#) used a similar approach to enhance grasping of robotic arms by means of deciding on the correct technique to grasp based on image reconstruction from a BCI.

**Controlling vessels, aircraft and spacecraft** Since BCI like the P300 have been used as neuroprosthetics for physically impaired people, there are efforts made to study a broader application of BCI to control machines or vessels. ([Choi et al. 2018](#)) published a study, where invasive BCIs for direct control of machines were examined. They came to the conclusion that this is very much possible but requires several advancements to gain really high quality data for fine-motoric movements. This also requires that electrodes have to be implanted deep inside the brain in order to gain high resolution results.

<sup>11</sup>Principal Component Analysis

## 1 Introduction

(William Kucinski 2018) published an article on the SAE News homepage, describing a report published by the DARPA where an individual was able to control three warplanes in a simulator. The novelty in this research was also the feedback given to the individual, thereby posing a bidirectional BCI. As of Q2 2021, this article is no longer available on the DARPA homepage but several other news organizations wrote about this: ([Stockton 03/05/2015](#)), ([Blair 2018](#)) and ([Tucker 09/06/2018](#)). Since the DARPA is well known for being decades ahead with their research, it is very well feasible outlook to have BCIs in the future, which allows for control of not only aircraft but also ships and spacecraft.

**Improving human learning rate and augmenting system performance** In an article published by the Journal of neuroscience methods by ([Miranda et al. 2015](#)) the efforts by the DARPA<sup>12</sup>, which is a US federal agency to advance technology for defensive efforts, were outlined. These grouped into prosthetics and rehabilitation as well as efforts to improve human training and performance. The latter has fascinating research on Improving the learning rate of the human brain:

*The Narrative Networks (N2) program is developing new techniques to quantify the effect of narratives on human cognition and behavior, including initial development of a closed-loop BCI system that adapts a narrative in response to a listener's EEG signals. Such a system would have numerous applications to training and human performance domains.* ([Miranda et al. 2015](#))

Further applications were the integration of a *Human-in-the-loop*, scenario, where intelligence analysis and threat warning. A 10-fold improvement in analysis throughput was achieved in the former case. In the latter case of threat detection the incorporation of a BCI-enabled human increased the probability of threat detection to 91% compared to 53% detection rate solely relying on computer vision.

**Transferring thoughts over the internet** A paper published by ([Martins et al. 2019](#)) outlined the possibility of using nanotechnology to insert sensors to every single neuron and synapse in the human brain to have a real time stream from the within the human brain with a resolution down to a single neuron. This would allow for every human having a digital twin of himself in the cloud, having access to the whole repository of human knowledge without timedelay and even share experiences, thoughts and memories with other people.

A little less futuristic is a study published by ABC News: ([Lee et al. 2016](#)) and outlined in figure 1.8. In this case for the first time in human history, conscious communication from one brain to the other without the involvement of sensory or motoric stimuli was achieved. This is called a B2B or Brain-to-Brain communication. The according paper was written by ([Grau et al. 2014](#)). In this case two humans exchanged the greetings *Hola* and *Ciao* over the internet from India to France.

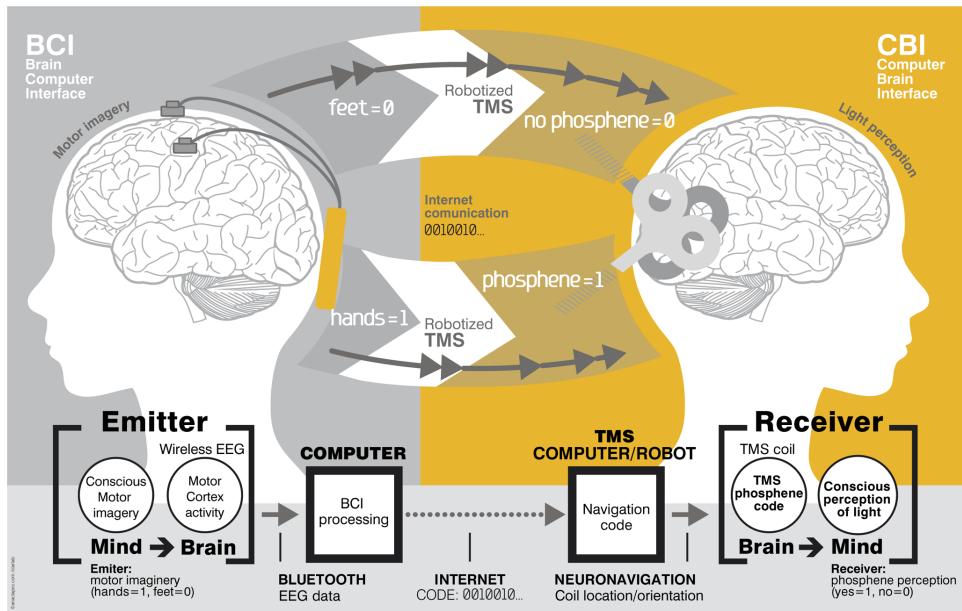
**Data privacy** With the latest innovation in the field of BCI and BMI a new concern arises along with them: privacy. ([Greenberg 2019](#)) published a paper, where she outlined the current status and outlook on data privacy in regard to brain data, where the jurisdictions of the EU, United States and Canada were compared with their different approaches:

*In relation to the governance of personal data in the private sector, the United States adopts a self-regulatory mechanism, while the European Union assumes a rights-based approach, with Canada's position being intermediate to the two extremes.*, [Greenberg \(2019\)](#)

She concludes that *As BMIs enter the marketplace, legal and ethical questions pertaining to brain data privacy are certain to arise* ([Greenberg 2019: 43](#)) and makes policy recommendations to be implemented in order to guarantee privacy. These recommendations outline a *privacy by*

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<sup>12</sup>Defense Advanced Research Projects Agency



**Figure 1.8:** B2B communication signal chain, Source: Grau et al. (2014)

design, improvement of transparency and general sharpening of existing policies to better suit the requirements of brain data applications.

## 1.7 EEG acquisition devices

Concluding section 1.2 and 1.6, it is reasonable to talk about some technical implications of BCIs and their limitations. In technical terms, these are EEG acquisition devices from the medical domain and only gather EEG brainwaves from certain regions of the brain. The placement of the electrodes on the skull determines which domain of brain activity will be recorded.

There is a great variety of these different EEG acquisition devices on the market. Ranging from consumer-grade cheaply and readily available sensors which cost a few hundred Euros up to medical grade devices. According to Zerafa et al. (2018) the difference in price and quality are mainly determined by the factors amplifiers, electrode type and count and transmission technique, which could be wired or wireless.

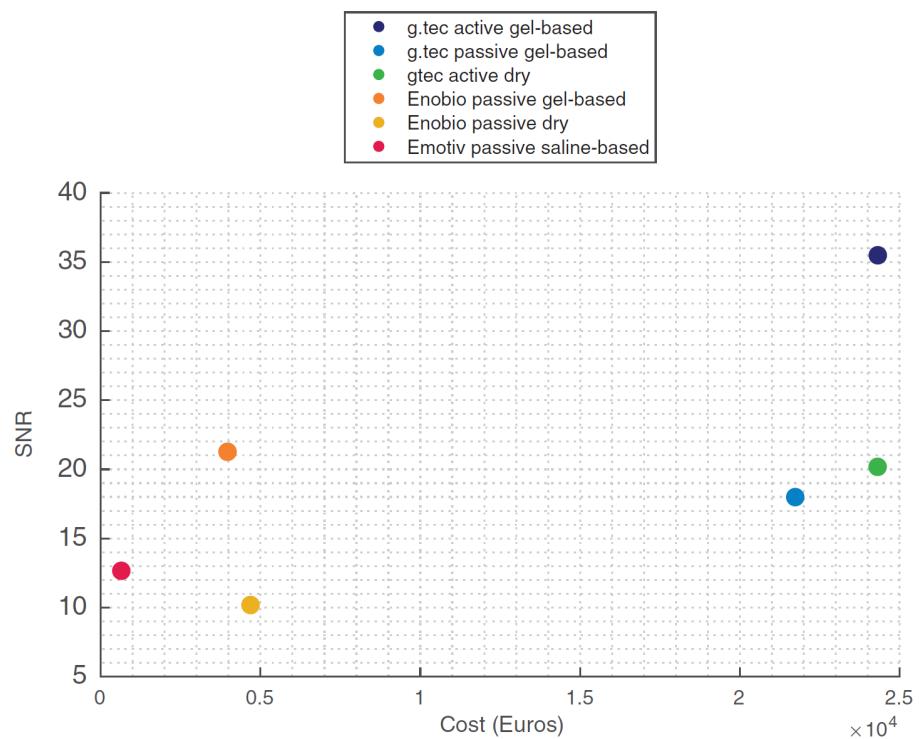
Since these sensors measure electrical potentials, the actual resolution of the electrodes and amplifiers is the single most influential parameter governing quality. Zerafa et al. (2018) used the SNR<sup>13</sup> of different sensors to compare them to one another, because quality in electrical measurements is best compared using the SNR value of each measurement:

Figure 1.9 shows the picture that *cheaper* sensors tend to have a worse SNR than more expensive ones with one exception which performed better. However, the cheaper sensors were perceived more comfortable and their set-up time was significantly less compared to fully fledged medical devices, which made them the better choice for experimenting and rapid prototyping. Also the expensive sensors required special treatment with gels and saline solutions, which wasn't necessary on the dry-electrode setup of the cheaper sensors. The conclusion of Zerafa et al. (2018) was that either of those two categories have their advantages in their own domain and there is no *best choice*.

Check if paper can be quoted like that.

<sup>13</sup>Signal to Noise Ratio

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**Figure 1.9:** SNR plotted against price, Source: [Zerafa et al. \(2018\)](#)

## 2 Survey Framework

Before any survey can be designed, certain considerations like sample size, population ... [ref to döring/bortz for details](#) have to be taken into account. Also depending on the desired outcome of the survey, the questionnaire has to be defined.

### 2.1 Considerations

The primary goal of the survey is to find empirical evidence that age does not affect the ability to use a BCI. In order to exclude certain parametres, which might cause an unwanted effect, potential disturbance parametres have to be identified and discussed:

- Age
- Gender
- Quality of the sensor readings
- Motion Sickness
- User wears glasses
- Cognitive impairments
- Medication or drugs known to affect EEG readings

Furthermore participants of the study should disclose if they had previous or ongoing conditions of seizures or epilepsy, especially in case of light or flashing related cases.

Apart from the demographic parametres of age and gender, the other factors have to be considered to prevent potential malformed data. Firstly, a condition which causes a detrimental effect on the ability to see and identify patterns might have a dampening effect for the visual cortex to create the required brain waves. However, the physical layout of the VR goggles used allow for prescription glasses to be worn. Hence this is not a concern in the context of this study. Secondly, when working with VR goggles, there is always the possibility of motion sickness involved. On the other side: this will unlikely have a negative effect since the experiments will be static. There won't be any movement from either the user itself within the environment nor the GUI involved, which removes the prevalent reason for motion sickness according to [Golding \(2006\)](#). Medical conditions or drug intake might also have a huge impact on the results. Diseases such as dementia or alzheimers or drug intake such als alcohol or caffeine have to be considered in the individual performance of each subject. [Kenemans and Lorist \(1995\)](#) showed that caffeine intake has an effect on brain wave activity, therefore this has to be taken into account. Lastly the readings of the sensor will very likely be different for each experiment. Since the sensor provides quality readings, these will be considered in the data evaluation. Nevertheless, there will be a questionnaire provided which will ask the user after experiment if he experienced any of these effects to have a possible explanation for potential outliers.

Under the assumption that gender has no effect on the study, because the brain of men and women is at least structurally identical. Therefore age is the only parameter which is the variable in this study. To put the results into context, the survey participants will be clustered by age into different groups.

## 2.2 Design of experiment

The solid proof that the hypothesis holds true or not can not be made based on looking at diagrams and educated guesses. Hence the need for design of experiment to provide a numerical framework which defines thresholds and quantities to make results reproducible. This section is based on the theoretical framework which is described in (Siebertz et al. 2017: 87ff) under the considerations in the previous section. There are two main parameters to consider, when it comes to the DoE<sup>1</sup>:

- How many samples are necessary to reliably prove that the hypothesis holds true?
- Where is the threshold which determines whether an effect is significant or not?

In the context of DoE the former is often depicted as  $\beta$  and the latter as  $\alpha$ .

**Parameter alpha -  $\alpha$ :** Alpha is the governing parameter, which decides how big the risk in a given sample size is that the hypothesis is wrong and therefore falsified. Since the hypothesis can be either true or false, the probability that it is wrong decreases with the number of samples taken in a binomial fashion (Siebertz et al. 2017: 103). That means in this case that the likelihood  $p$  of a participant to be above or below the threshold, which is discussed in section 4.7, is not determined by age. According to (Siebertz et al. 2017: 110) common values for alpha tend to be chosen such that the probability of a falsified hypothesis is at 1%, 5% and 10%. Where a smaller value means a more strict threshold. To account for the explorative character of this study the value of 5% is chosen. Therefore the susceptibility for unaccounted side-effects is reduced and the total number of participants is still not unfeasibly large.

**Parameter beta -  $\beta$ :** This parameter depicts how effective a potential effect is in a given sample size. The likelihood of a significant effect not being recognized decreases with an increasing number of samples, since it becomes increasingly unlikely that a systematic effect affects the samples always in a way which makes it undiscoverable. Table ref

Create table here

## 2.3 Information Transfer Rate

After establishing the necessary framework for the survey and how the results have to be interpreted in order to draw a meaningful conclusion, the underlying metric to examine and compare the performance of the individual subjects in the experiment has to be defined. The most widely adopted metric is the *Information Transfer Rate* or *ITR* in short, according to (Yuan et al. 2013: 1). This metric was conceived by Wolpow et al. (1998) and depicts the bits/symbol:

$$B = \log_2 N + P \log_2 P + (1 - P) \log_2 [(1 - P)/(N - 1)] \quad (2.1)$$

Where  $N$  is the total number of choices for a user to choose from and  $P$  is the probability that a desired or required choice in the experiment will be selected, therefore posing also a metric of accuracy. In the context of this study a symbol is equivalent to a single *choice* on the remote control (see Section 1.5.4). However, (Yuan et al. 2013: 4) summarized certain constraints which have to be met, in order to ensure the applicability of this formula:

1. BCI Systems are memory-less and stable discrete transmission channels.

---

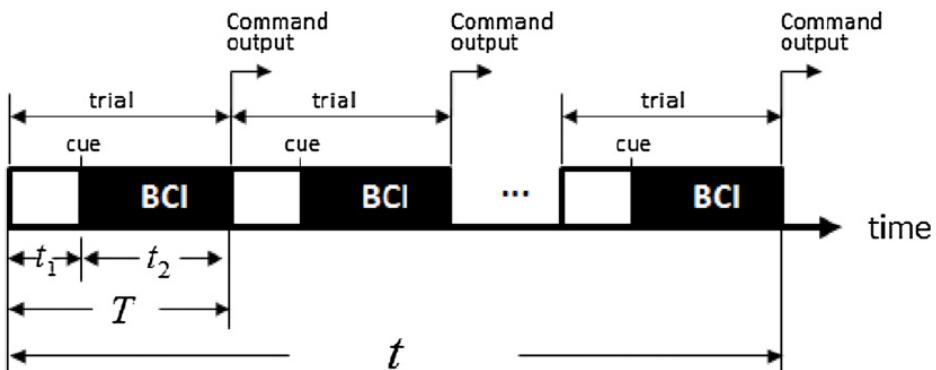
<sup>1</sup>Design of Experiment

2. All the output commands are equally likely to be selected ( $p(\omega_i) = 1/N$ )
3. The classification accuracy is the same for all the target symbols ( $p(y_i|x_i) = p(y_j|x_j)$ )
4. The classification error is equally distributed among all the remaining symbols ( $p(y_j|x_i)_{j \neq i} = (1 - p(y_i|x_i))/(N - 1)$ )

Where (1) is in the scope of this study solely determined by the choice of the interface and (2) solely on the implementation of the experiment. However (3) and (4) would be also considered solely depending on the implementation of the experiment. But since this might be influenced by the performance of the individual participant, there is a possibility of side effects like visual impairments resulting in varying performances when the target symbols are spatially distributed. Nevertheless in line with section 2.1, these considerations will be disregarded for the purpose of this study.

Going into detail regarding (1), it has to be elaborated, why the used sensor is within the set constraints. These are: synchronism, bijectivity regarding the mapping of available symbols and possible selections, no memory, lack of error correction and prediction and no goal directed behavior.

**Synchronism** A BCI works *synchronous*, when the time which passes from the presentation of a cue to the user until the symbol has been confirmed or erroneously chosen is solely determined by the system itself. A BCI might be considered *asynchronous* if there are measures in place to artificially increase the response time.



**Figure 2.1:** Timing of symbol recognition and activation / [create own graphic](#)

**Bijection** In regard to the equation in (3) this means a strict 1:1 relationship between the possible input symbols shown to the user and the resulting output symbols. Yuan et al. (2013) describes possible scenarios, where this rule applies as *idle-states* for example, where a user can deliberately choose to deactivate the interface.

**Memory** This regards to certain scenarios, where for example an ANN<sup>2</sup> which is used as a classifier to determine if a certain symbol is activated has an internal feedback loop. These ANNs therefore possess a *memory* of some sort, which would bias the result, since that is not *purely* relying on the user's EEG-data.

---

<sup>2</sup>Artificial Neural Net

**Lack of Error Correction** Modern smartphones for example have automated error correction upon text entry, which are based on an MLE *Maximum Likelihood Estimation* algorithm. This MLE in turn is derived for each specific language and determines if an entered character is valid or not. A similar behaviour for a BCI would violate the condition on bijectivity, since the strict 1:1 relationship would be lost in case of an error.

**Prediction** Similar to error correction a prediction would artificially increase the ITR, since there will be an output generated which is not relying on the user input, which also violates bijectivity.

**Goal directed behaviour** An application which aids the user navigating, violates the synchronism criteria and classification accuracy. The reason being that by leading the user to certain actions apart from the initial cue has an influence on these parametres which creates a bias on the resultung ITR.

In section 3 the design of the interface will be shown and it wil be proven that all these criteria will be met in this study. Section 4.7 will elaborate how this data will be used to evaluate the hypothesis from section 1.5.5.

# 3 Survey Contents

Chapter 2 established the theoretical framework of the survey. This chapter aims to define the experiment which will be used to gather the data. To do so, the following considerations have to be made:

1. What tools will be used?
2. How is the interface going to look like?
3. What data will be collected?
4. How are the age groups structured?
5. How is the data collected?
6. What are the questions in the questionnaire?

## 3.1 What tools will be used

**Oculus Quest2** The Oculus Quest2 is a state-of-the-art VR headset as of Q2 2021. This headset will be used to show the user the visual stimuli in the experimental *remote control interface*. Using a visually hermetic closed headset has the added benefit of blocking every external stimuli and therefore increasing the ability of the user to concentrate on the experiment. The expected result will be a reduced  $t_1$  time, shown in figure 2.1.

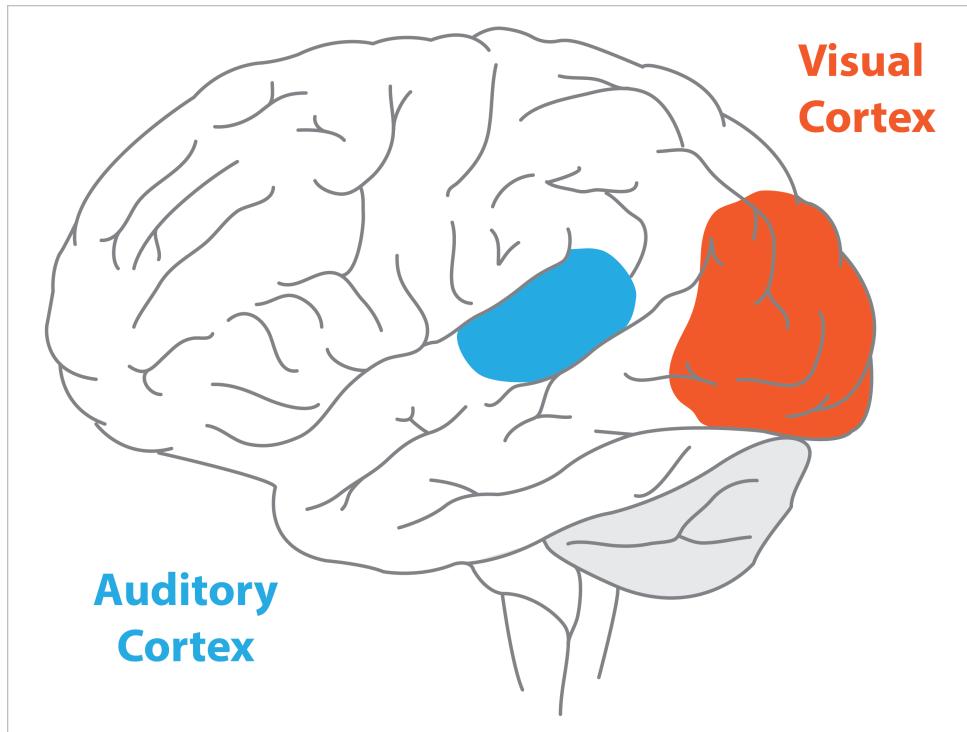
**Nextmind BCI** Shown in figure 1.5 is the Nextmind BCI, which will be used to gather the data from the VEP. The vendor provides a SDK which integrates really well in Unity and in consequence with the Quest2. During the experiments, this sensor will be located at the back of the participant's head, where the visual cortex is located at (figure 3.1.)

The Sensor will be strapped to the VR headset and thus these two devices will be easy to put on or off.

**Tablet for questions** A tablet will be used to collect anonymized demographic data from the participant. This is necessary for the evaluation of the results. See section 3.3 for details.

## 3.2 Remote control interface

Figure 3.2 shows the interface, which the user will see in the experiment. It resembles the number pad on a conventional TV remote control in structure. The rectangles with the numbers will be the neurotags, where the user has to look at. To measure the activation time, one neurotag will be visually cued - represented by the highlighted 6. As soon as this neurotag has been activated, a new visual cue will be given. The number of occurrences in total and of each neurotag will guarantee that the requirements for equation 2.1 will be met.



**Figure 3.1:** Position of the visual cortex. Left is front. Source: ?

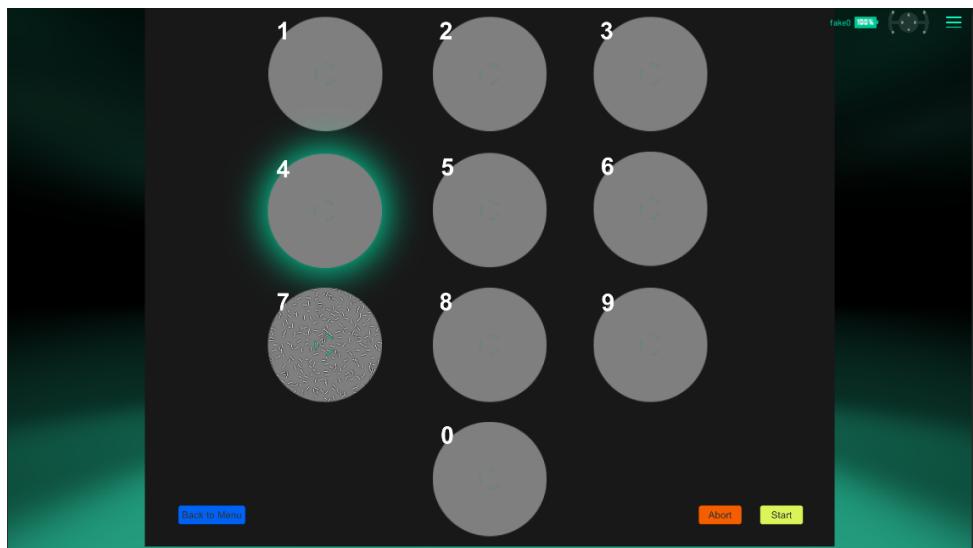
### 3.3 What data will be collected

The data collection will be structured in three blocks: Two questionnaires before and after the experiment which the participant had to answer and data collection during the experiment. The first questionnaire consisted of general questions regarding demographics and medical conditions:

- Demographics: Age and Sex
- If the participant wears glasses
- If the user felt motion sickness during the experiment
- Cognitive impairments
- Medication known to affect EEG readings
- Drug intake within the last 12hrs

The collected data during the experiment was collected on the VR headset ([application](#)) and stored in a file, which was available after the finished experiment. This data contained the following readings:

- Speed of each neurotag activation from the point where a cue was given. This is the start of  $t_1$  until the end of  $t_2$ , where the sensor is confident that a certain neurotag was looked at.
- Confidence score of each activated neurotag upon activation until another neurotag is activated.
- Quality readings from each single electrode to monitor the tracking quality of the sensor, in order to explain outliers in the collected data.



**Figure 3.2:** Interface of the remote control experiment. Ques are highlighted.

After the experiment the participant answered the second block of questions, which consisted of questions about the general experience of using the BCI:

- If the user felt motion sickness during the experiment (rated 1...5)
- comfort of wearing the sensor (rated 1...5)
- perceived time to setup the sensor (rated 1...5)
- ease of use (rated 1...5)

### 3.4 How are the age groups structured

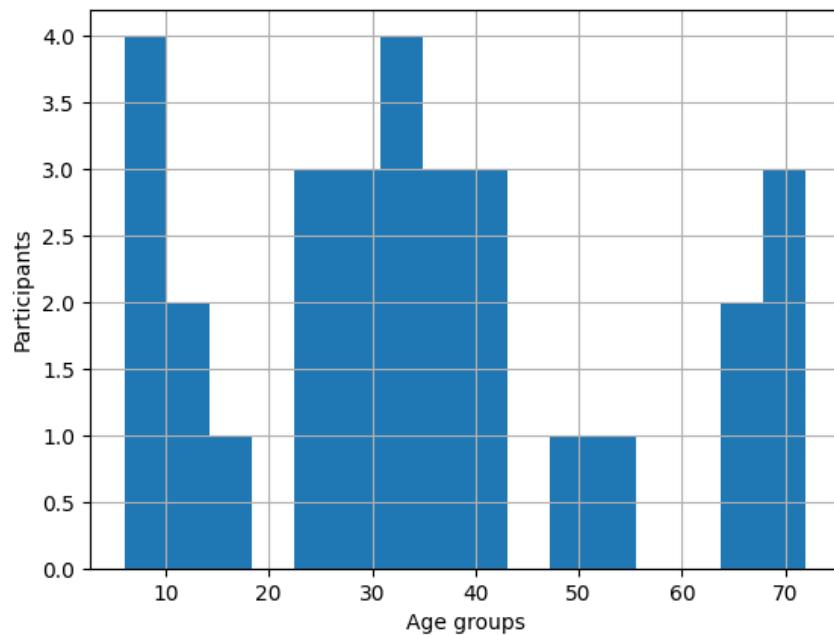
Write some elaborate text about the age distribution

### 3.5 Experimental Protocol

The data was collected in a single session lasting between 10-20mins for each participant. Each session started with the participant having to complete the first questionnaire A.1 and the form of consent A.1 for anonymized data processing. At this stage potential hazards, problems and dispositions as discussed in section 2.1 were identified. One individual could not participate as she had epilepsy, what might have gotten triggered by the experiment. Afterwards each participant was introduced into the experiment. The working principle of a SSVEP was explained and questions regarding data privacy were discussed. Subsequently the the GUI of the experiment was been shown to the participant with a short introduction about the nature of the task.

Then the participant was equipped with the BCI Sensor and placed in front of the screen as shown in figure 3.4. The distance to the screen was varying since each participant needed to adjust according to eyesight. The first step of the experiment was the calibration of the sensor to the participant. In case of non-optimal readings, the position of the sensor was adjusted accordingly until all electrodes showed at least *very good* contact (figure 3.5).

Then the experiment was started. The participant had to perform 50 neurotag activations. Each one consisted of a visual que (see figure 3.2) on which the participant had to focus on.



**Figure 3.3:** Age distribution of the participants

Upon a sucessful activation of the cued neurotag, the readings were saved to the logfile (see A.2) and the next cue was given in order to keep the  $t1$  timing as short as possible.

After completion of the experiment, each participant had to fill the second questionnaire A.1, which gathered information about the experiment such as wearing comfort, perceived difficulty and questions about the opinion towards the technology in general.

### 3 Survey Contents



**Figure 3.4:** Experimental setup

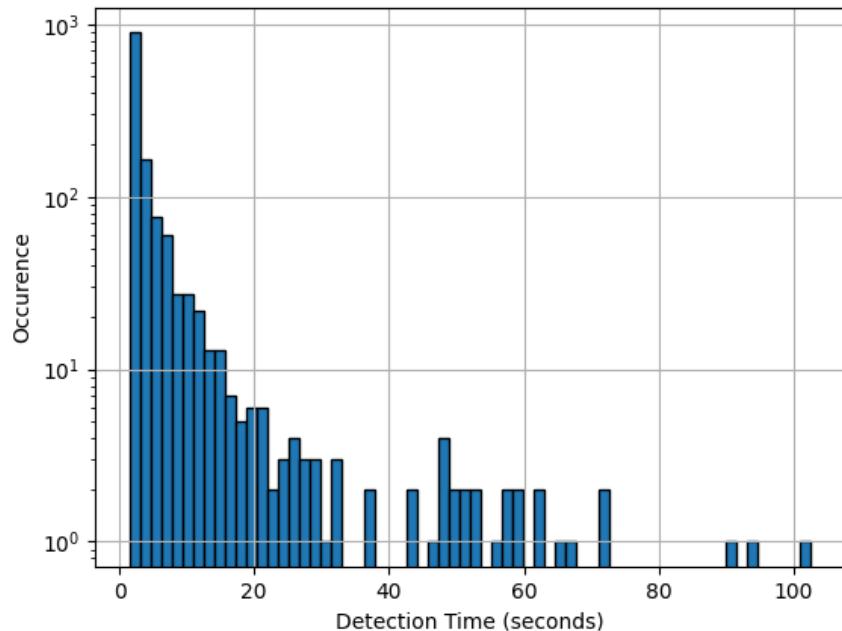


**Figure 3.5:** Quality readings of the sensor

# 4 Survey results

## 4.1 Raw results

The study gathered 1370 different target hits datapoints from 28 participants figure 4.1 shows a histogram of the achieved detection times. The y-axis is scaled logarithmically because approximately 870 out of all detections were made in under three seconds.



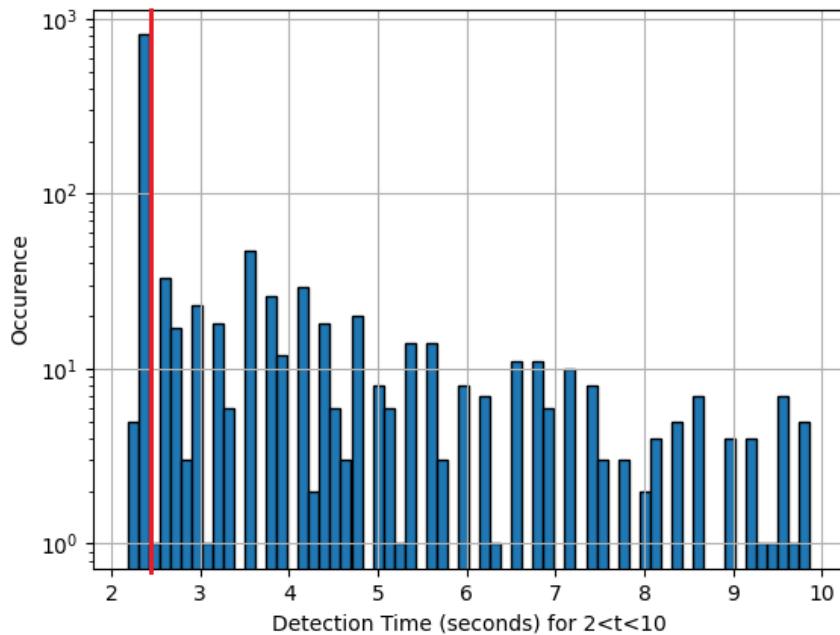
**Figure 4.1:** Histogram of achieved detection times

This is also shown very clearly in figure 4.2, where the time windows shows only the results between two and ten seconds, which also constitutes for the majority of data points (over 95%). The clustering of the detection right at the 2.3s mark, which is indicated by the red line with almost no other data points below that threshold might indicate, that this threshold is the minimum amount of time required to confidently identify a target. The logfiles show that a confidence score of  $>0.3$  qualifies for a successful identification. See Appendix A.2 for details. This score is not displayed for targets, which are identified under a certain amount of time, since there aren't enough samples supposedly.

## 4.2 Telemetry

The *NextMind* Engine provides telemetry readings on request. Figure 4.3 shows a boxplot of all quality readings prior to all successful conducted experiments. Each boxplot stands for one distinct electrode at the sensor.

Apart from some outliers, there are no significant systematic errors, which might lead to a significant error in the acquired data. There is a very small tendency in the outermost electrodes



**Figure 4.2:** Narrowed window of achieved detection times

to have slightly less quality over the course of the whole experiment what can be attributed to being to outer and bottom electrodes which might not have ideal contact on an individual basis if the skull shape is more elliptical than usual.

### 4.3 Demographic differences

To rule out potential side effects, the first questionnaire had more questions apart from age. Namely being gender, whether the participant wears glasses, neurological conditions, alcohol or drugs and colourblindness. However the latter four questions were answered negative entirely. The only exception was a neurological condition which prohibited conducting the experiment altogether. This leads the sex and if the participant wears glasses as the only major demographic parametres.

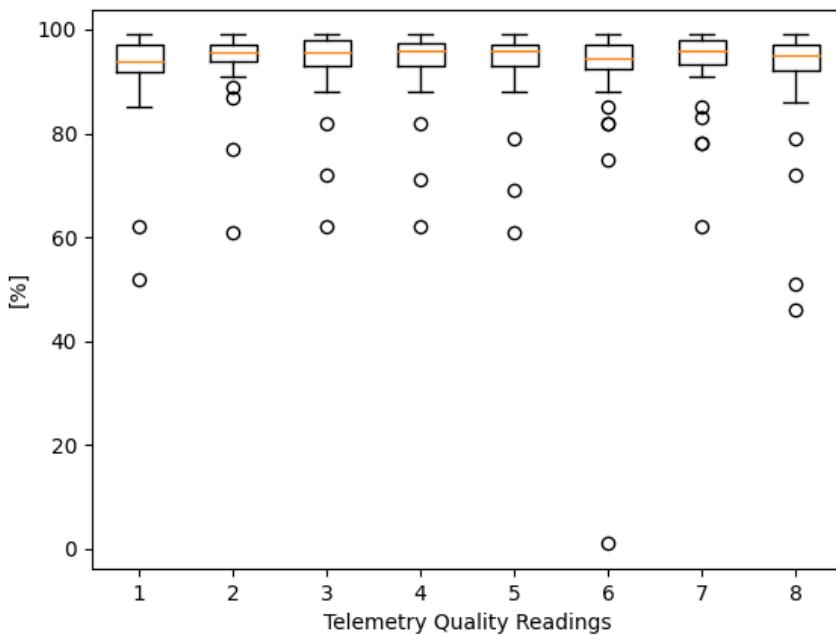
When the genders are compared side by side in figure 4.4, there is a tendency of women having a more consistent timing. The average value of both in approximately on the same level but the male results have a larger upper quartile and whisker therefore being less consistent in timing. As in figure 4.2, the window was narrowed down to 10s max, to cut large outliers. **Check if there is a skew in age/gender distribution.**

Figure 4.5 also shows the result that participants without glasses have a higher consistency in their target times. Although the average being at roughly the same level, the upper quartile and whisker is far more spread with the participants who are wearing glasses. **Check if theres a strong correlation with age!**

### 4.4 Detection time differences for each target

One effect observed during the experiment was, that some targets were generally faster detected than others. Figure 4.6 shows this phenomennon:

This effect comes presumably from the layout of the experiment itself, where the participant sat in front of a laptop and the interface was placed in a different angle. Therefore the targets,



**Figure 4.3:** Quality readings of the sensor prior to the experiments

which were arranged in rows and columns (see figure 3.2), were being seen in different angles. Since the test series of cues was the same for each experiment and close to evenly distributed in their occurrences, there is no systematic error in the experiment itself.

## 4.5 Conduction of the Survey

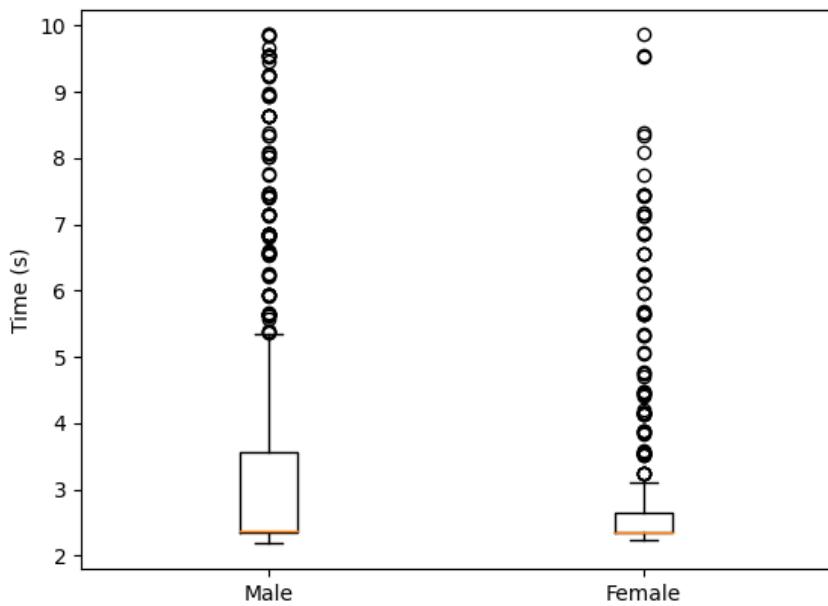
Two participants had not undergone the experiment itself due to an insufficient calibration score. One case was due to missing glasses for a clear view of the screen and another case had concentration problems. Both cases were in the above 60 age group. One participant also from the above 60 age group had to end the experiment prematurely due to concentration difficulties and eye strain.

Eye strain was reported from four participants. However there was no majority among any age group in this case which might indicate a correlation. Two participants wore contact lenses. One participant reported that focussing on the experiment made her forget about blinking her eyes.

Two participants reported that they felt the SSVEP physically inside their brain with a pulsating or tickling sensation. However, this was not reported to be painful.

In many cases the calibration wasn't successful at first try. Usually a sufficient score was reached after 3-5 attempts. Also for some participants the optimal sensor position was in a different place on the back of the skull than recommended by *NextMind*. In these cases the results were perfect instantly after a relocation of the sensor to a different position.

One participant inadvertently altered the position of the sensor which did not have a significant effect on the detection time. Also with this same participant the calibration score was comparatively low. Although not explicitly tested in this survey, this might indicate that the *NextMind* sensor has a resilient design to a shifting position.



**Figure 4.4:** Detection times between Male and Female participants

## 4.6 Questionnaire Results

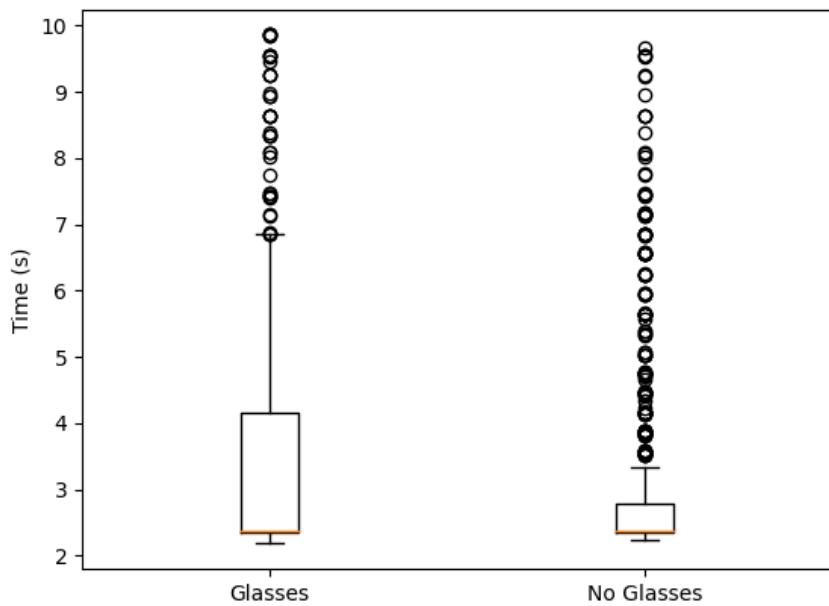
While the first survey had the primary goal to evaluate the Demographic data for the experiment and whether the subject was even able to conduct the experiment from a medical standpoint, the second survey A.1 asked questions about the parameters of the experiment itself.

These were:

- Wellbeing: How the participant felt that way, which might impact the ability to concentrate
- Dizziness: If the participant felt dizzy after the experiment
- Focus: How easy it was for the participant to focus on the task
- Comfort: The comfort of wearing the headset.
- Time: How the participant perceived the procedure of calibrating the sensor
- Difficulty: If the task of targeting Neurotags felt difficult.

Figure 4.7 shows the results from the survey on a 1...5 scale. The **Wellbeing** on the day of the experiment of most participants was generally good. Only one participant had back pain, which however didn't impair the ability to concentrate. Almost no participant felt **dizziness** after the experiment. **Focus**, **Difficulty** and **Time** didn't show any noteworthy results. Interestingly there was no real tendency to the **Comfort** of wearing this sensor. The opinions about the device are very evenly distributed, which is interesting because some participants apparently found it very comfortable to wear whereas others found it really uncomfortable.

In terms of opinion about the technology, which is not part of this study per se but interesting to gauge a general opinion nevertheless. Only 3 out of 25 participants are sceptical towards this technology. Three persons abstained from giving an opinion and two persons didn't fill the second questionnaire. 15 out of 30 participants would use the technology themselves with the remaining



**Figure 4.5:** Detection times between participants with and without glasses

15 answers consisting of two abstentions, two not filled questionnaires and the remaining 11 being negative answers. However, 24 participants think that this technology provides a benefit in the right domain. Again two persons didn't fill the questionnaire and four refrained from answering the question.

### evaluate the following topics:

- average speed per age group (boxplot?)

use results to construct an argument about statistical significance (DOE)

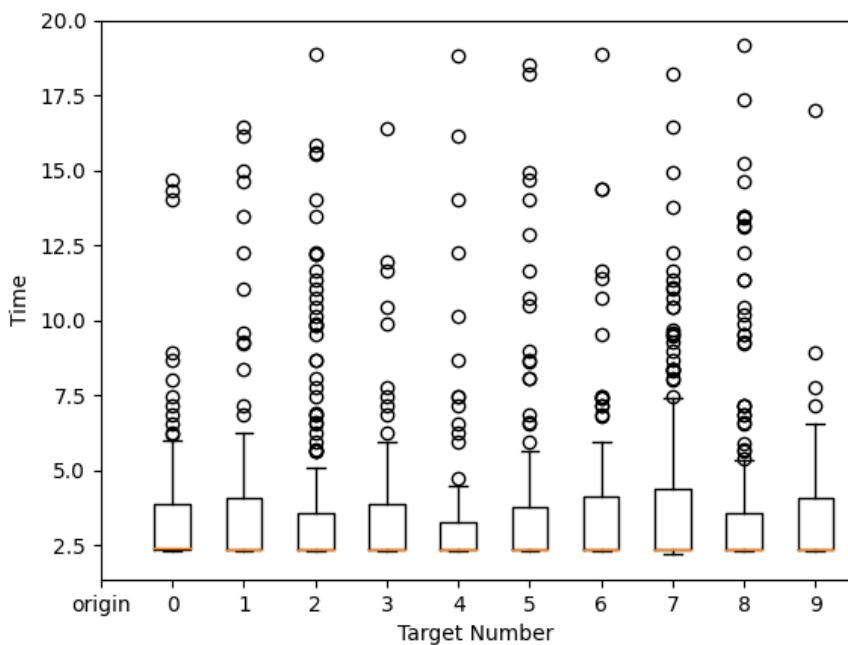
## 4.7 Interpretation of the collected data

Chapter 2.2 provided the necessary framework to decide whether the hypothesis holds true or not and Chapter 2.3 explains how BCI performance has to be interpreted in a given context. This section focusses the contextualization of these metrics in regard to the hypothesis and DOE.

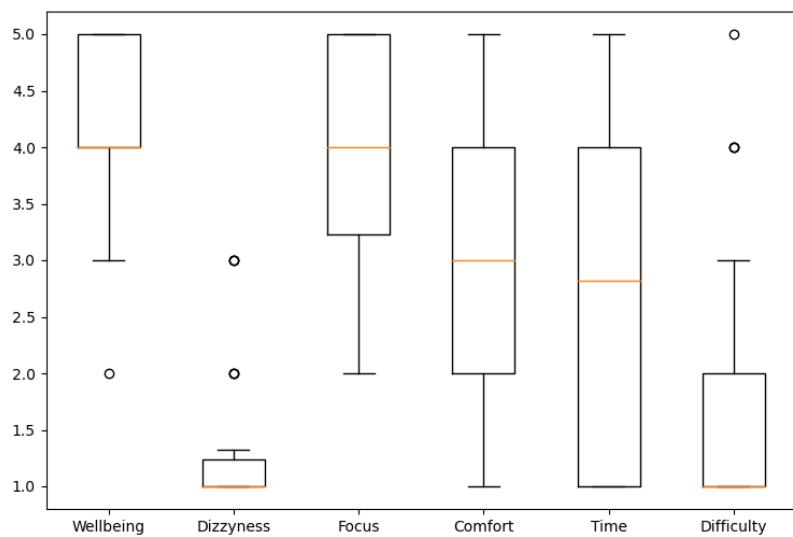
create coherent argument about ITR and DOE.

In regard to figure 2, 3, 4 in Yuan et al. (2013): use t1, t2, T and deltaB as argument for performance in experiment.

Once the study has been structured and carried out, I can write down the results.



**Figure 4.6:** Detection times for the different targets Correct X-axis



**Figure 4.7:** Results of post experiment user survey

## **5 Findings**

This section also depends on the outcomes in context to the research question.

# **6 Conclusion**

## **6.1 Results**

Summarizing the results and findings of the study briefly.

## **6.2 Future Work**

Based on the findings and new devices on the horizon, this should give a brief outlook on how to continue this research.

## **7 Acknowledgements**

I want to thank Prof. Dr. Roland Greule and Dipl. Inf. Rüdiger Höfert to examine this study and always set the right impulses to guide the outcome of this thesis. Rüdiger Höfert in particular helped me out with the procurement of necessary equipment to conduct the study. I also want to express my gratitude to the Hamburg University of Applied Sciences to provide the necessary framework to obtain my degree and aid with the procurement of necessary equipment. I also want to express my appreciation for every single participant who took part in my experiments despite certain constraints due to the Covid19 pandemic. A special thanks goes to B.Sc. Moritz Bednorz, who helped me sharpen and clarify my knowledge in the field of medical engineering and design of experiment, which gave this thesis a coherent perspective on all domains. I will be eternally grateful to my father Dr. Thomas Neudecker to set the right impulses which made pursue an academic degree. He may rest in piece. My biggest thanks is dedicated to my girlfriend B.A. Alexandra Michels for her emotional support and creative input to some of the figures in this thesis.

# A Material

## A.1 Survey forms

The following forms were used during the experiment. They are written in the german language since every participant was native german.

*Every document is in its original layout, hence the difference in terms of layout to the rest of this document.*

# Informationsbogen vor dem Experiment

## Informationsblatt

In diesem Experiment wird ein sogenanntes *Brain-Computer-Interface* (BCI) verwendet, dieses misst ähnlich einem EKG (Elektrokardiogramm) die Gehirnströme. Dafür werden sogenannte *Visuell Evozierte Potenziale* (VEP) mittels spezieller visueller Stimuli erzeugt. Die Messergebnisse werden anschließend maschinell mit Hilfe eines mathematischen Modells verarbeitet und Steuerbefehle für einen Computer daraus generiert.

Das Experiment verursacht **keine** Schmerzen oder sonstige ungewohnte oder unangenehme Empfindungen.

Das Experiment verursacht **keinerlei** gesundheitliche Schäden durch Strahlenexposition oder das Einbringen von Fremdkörpern in den Körper.

Es können **keine** Gedanken gelesen und **keine** Daten gesammelt werden, die später einem Individuum und seinen politischen oder persönlichen Ansichten persönlichen Ansichten zuordenbar sind.

Es werden **keine** Daten gesammelt, die an eine dritte Partei über das Internet oder sonstwie übertragen werden.

Es findet **keinerlei** Beeinflussung des Gehirns durch den Sensor statt. Zu jedem Zeitpunkt des Versuchs ist das Datenfluss strikt unidirektional in Richtung des Computers.

Es wird **keine** Manipulation des Gehirns durchgeführt, die in irgendeiner Weise unmittelbar oder zukünftig eine der obengenannten Szenarien ermöglicht.

Alle Daten werden strikt anonym anhand der Teilnehmernummer verarbeitet und zu keiner Zeit werden anhand der Daten Rückschlüsse auf den Teilnehmer möglich sein.

Die gesammelten Daten belaufen sich auf zwei Fragebögen und eine maschinell generierte Log-Datei mit dem folgenden exemplarischen Inhalt:

## Einverständniserklärung

Ich bin über den Inhalt des Experiments und die Verarbeitung der gesammelten Daten belehrt worden und stimme der Teilnahme und der anonymen Verarbeitung der gesammelten Daten zu.

Datum und Unterschrift: \_\_\_\_\_

# Fragebogen vor dem Experiment

## Einleitung

Dieser Fragebogen hat zum Ziel demografische und medizinische Daten zu sammeln, die im weiteren Verlauf der Studie zur Auswertung herangezogen werden können. Sämtliche Daten werden anonymisiert verarbeitet.

Teilnehmernummer: \_\_\_\_\_ (*Wird Ihnen mitgeteilt.*)

## Fragebogen

1. Alter: \_\_\_\_\_
2. Biologisches Geschlecht:    W     M     keine Angabe
3. Tragen Sie eine Brille?    Ja     Nein
4. Leiden Sie unter neurologischen Erkrankungen?    Ja     Nein
5. Nehmen Sie Medikamente zu sich, die sich auf das Gehirn auswirken?    Ja     Nein
6. Haben Sie in den letzten 12h Alkohol zu sich genommen?    Ja     Nein
7. Haben Sie eine Farbsehschwäche?    Ja     Nein

**Bitte beantworten Sie die folgenden Fragen auf einer Skala von 1 (schlecht) bis 5 (gut):**

- 8a. Wie fühlen Sie sich? 1 ———— 5

# Fragebogen nach dem Experiment

## Einleitung

Dieser Fragebogen hat zum Ziel Daten zur Versuchsdurchführung zu sammeln, die im weiteren Verlauf der Studie zur Auswertung herangezogen werden können. Die von Ihnen angegeben Daten in diesem Fragebogen werden für die spätere Auswertung der Studie herangezogen. Sämtliche Daten werden anonymisiert und vertraulich behandelt.

Teilnehmernummer: \_\_\_\_\_ (*Wird Ihnen mitgeteilt.*)

## Fragebogen

**Bitte beantworten Sie die folgenden Fragen auf einer Skala von 1 = wenig/angenehm bis 5 = viel/unangenehm:**

- 1a. Haben Sie während des Versuchs Schwindel verspürt? 1  2  3  4  5
- 1b. Wie gut konnten Sie sich auf das Experiment konzentrieren? 1  2  3  4  5
- 1c. Beurteilen Sie den Tragekomfort des Sensors? 1  2  3  4  5
- 1d. Beurteilen Sie die wahrgenommene Zeit zum Einrichten des Sensors 1  2  3  4  5
- 1e. Beurteilen Sie wie schwer Ihnen diese Übung fiel: 1  2  3  4  5

## Fragen zur Technologie

2. Stehen Sie dieser Technologie skeptisch gegenüber? Ja  Nein  keine Angabe
3. Würden Sie ein BCI selbst verwenden? Ja  Nein  keine Angabe
4. Sehen Sie einen Mehrwert in dieser Technologie? Ja  Nein  keine Angabe

## A.2 Example logfile

This is an excerpt of a genuine logfile and shows all the relevant data which was gathered during a trial.

*Since the data is anonymized, there is no way to identify a certain individual from this excerpt.*

---

```

1626361044463;Model.NeuroTagMarkedAsTargetLogEntry;7
1626361044468;Model.SensorTelemetryLogEntry;94;95;94;93;93;85;97;94;C
1626361044468;Model.ExperimentEventLogEntry;started
1626361044559;Model.NeuroTagConfidenceLogEntry;7;0.03284512
1626361044858;Model.NeuroTagConfidenceLogEntry;7;0.02825086
1626361045158;Model.NeuroTagConfidenceLogEntry;7;0.04584821
1626361045458;Model.NeuroTagConfidenceLogEntry;7;0.0324579
1626361045758;Model.NeuroTagConfidenceLogEntry;7;0.1790879
1626361046075;Model.NeuroTagConfidenceLogEntry;7;0.2322663
1626361046374;Model.NeuroTagConfidenceLogEntry;7;0.2289219
1626361046658;Model.NeuroTagConfidenceLogEntry;7;0.2858692
1626361046958;Model.NeuroTagConfidenceLogEntry;7;0.2982492
1626361047258;Model.NeuroTagMarkedAsTargetLogEntry;2
1626361047259;Model.NeuroTagHitLogEntry;7
1626361049623;Model.NeuroTagMarkedAsTargetLogEntry;9
1626361049623;Model.NeuroTagHitLogEntry;2
1626361051955;Model.NeuroTagMarkedAsTargetLogEntry;8
1626361051955;Model.NeuroTagHitLogEntry;9
1626361054287;Model.NeuroTagMarkedAsTargetLogEntry;7
1626361054287;Model.NeuroTagHitLogEntry;8
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1626361056636;Model.NeuroTagMarkedAsTargetLogEntry;1
1626361056636;Model.NeuroTagHitLogEntry;7
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1626361058986;Model.NeuroTagHitLogEntry;1
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1626361061335;Model.NeuroTagHitLogEntry;2
1626361061335;Model.NeuroTagConfidenceLogEntry;7;0
1626361063699;Model.NeuroTagMarkedAsTargetLogEntry;0
1626361063700;Model.NeuroTagHitLogEntry;7
1626361066049;Model.NeuroTagMarkedAsTargetLogEntry;8
1626361066049;Model.NeuroTagHitLogEntry;0
1626361066049;Model.NeuroTagConfidenceLogEntry;8;0.1005409
1626361068381;Model.NeuroTagMarkedAsTargetLogEntry;7
1626361068381;Model.NeuroTagHitLogEntry;8
1626361070729;Model.NeuroTagMarkedAsTargetLogEntry;6
1626361070729;Model.NeuroTagHitLogEntry;7
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1626361073396;Model.NeuroTagConfidenceLogEntry;6;0.2086784
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1626361075495;Model.NeuroTagConfidenceLogEntry;6;0.2939416
1626361075795;Model.NeuroTagMarkedAsTargetLogEntry;2

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