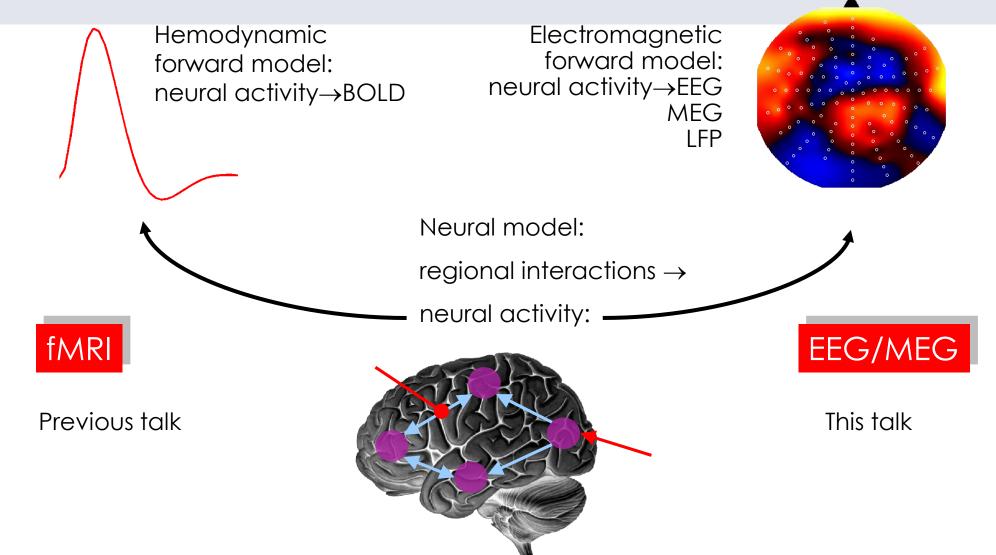
DCM for EEG

Dario Schoebi

University and ETH Zürich dschoebi@biomed.ee.ethz.ch



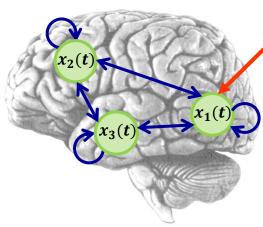
Recap: Dynamic Causal Modeling (DCM)



Recap: DCM approach to effective connectivity

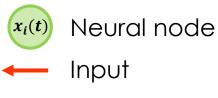
A simple model of a neural network

... described as a dynamical system ... causes the data (BOLD signal).



$$\dot{x} = f(x, u, \theta_x)$$

$$\dot{x} = f(x, u, \theta_x)$$
 $y = g(x, \theta_y) + \varepsilon$

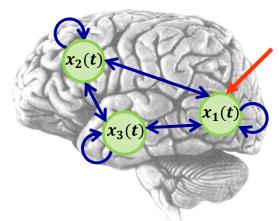


Connections

Let the system run with input (u) and parameters (θ_x, θ_y) , and you will get a BOLD signal time course y that you can compare to the measured data.

Recap: DCM approach to effective connectivity

A simple model of a neural network



... described as a dynamical system

EEG

... causes the data (BOLD signal).

EEG

$$\dot{x} = f(x, u, \theta_x)$$

$$\dot{x} = f(x, u, \theta_x)$$
 $y = g(x, \theta_y) + \varepsilon$



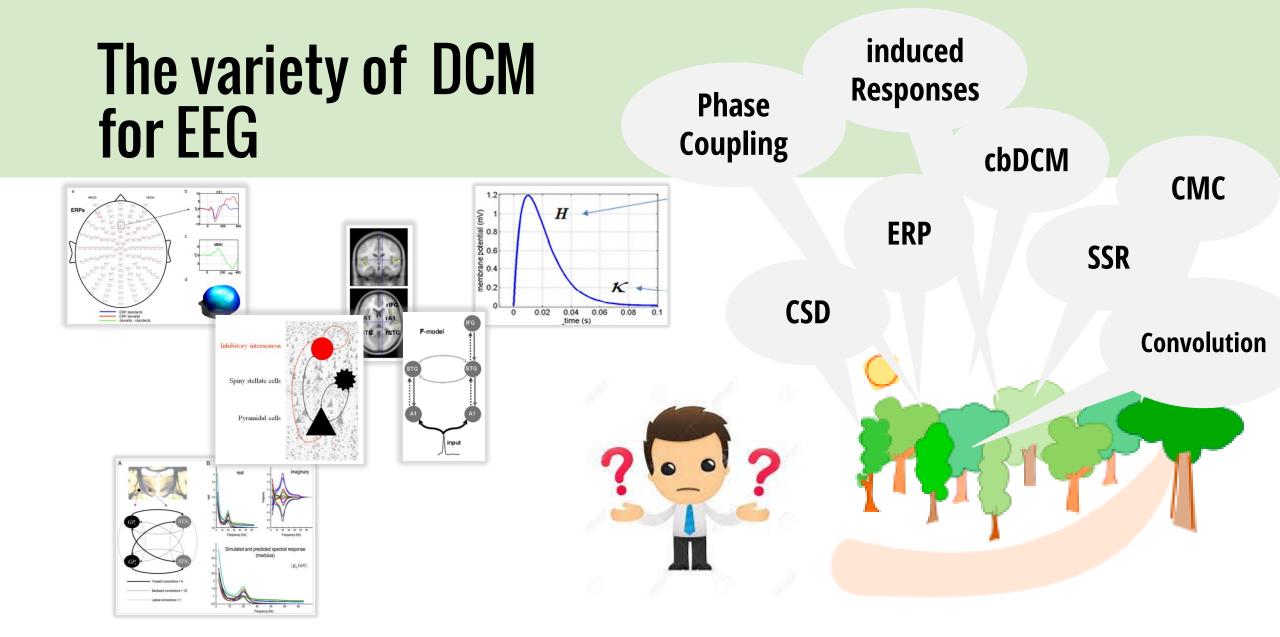


Input



Connections

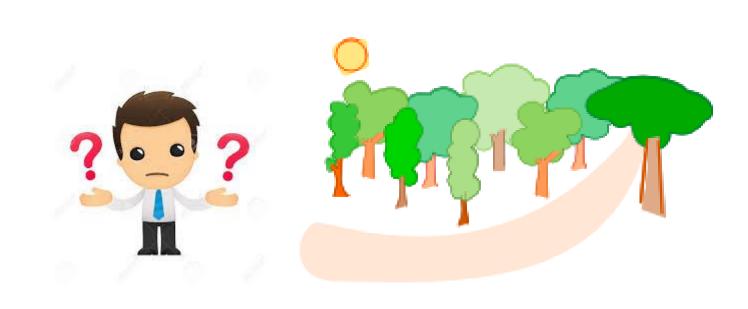
Let the system run with input (u) and parameters (θ_x, θ_y) , and you will get a **BOLD** signal time course y that you can compare to the measured data.



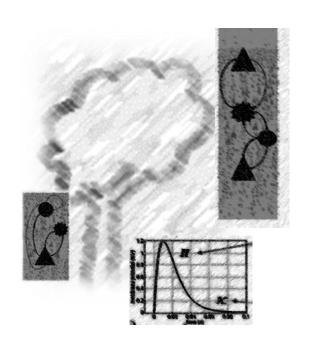
Garrido, Neuroimage, 2007; Moran, frontiers in Comp. Neuroscience, 2013; Friston, Neuroimage, 2012

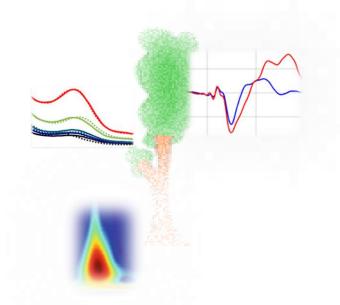
"... important distinction between different models and different data features ..."

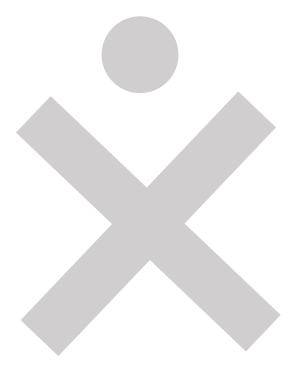
Moran, frontiers in Comp. Neuroscience, 2013







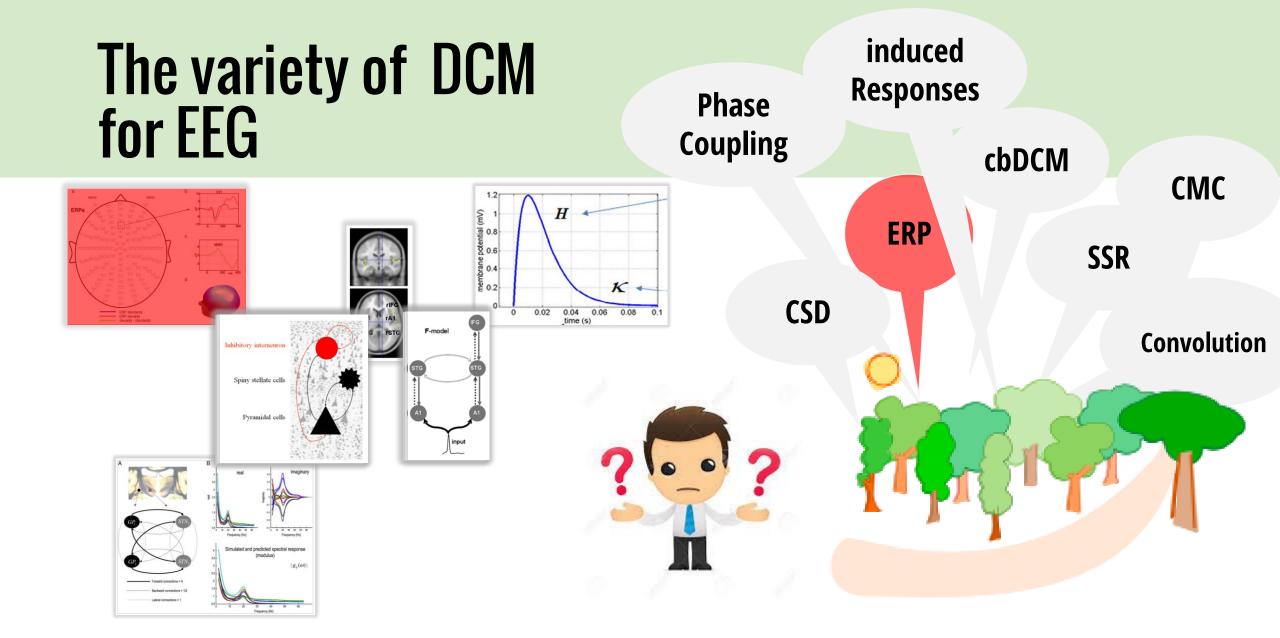






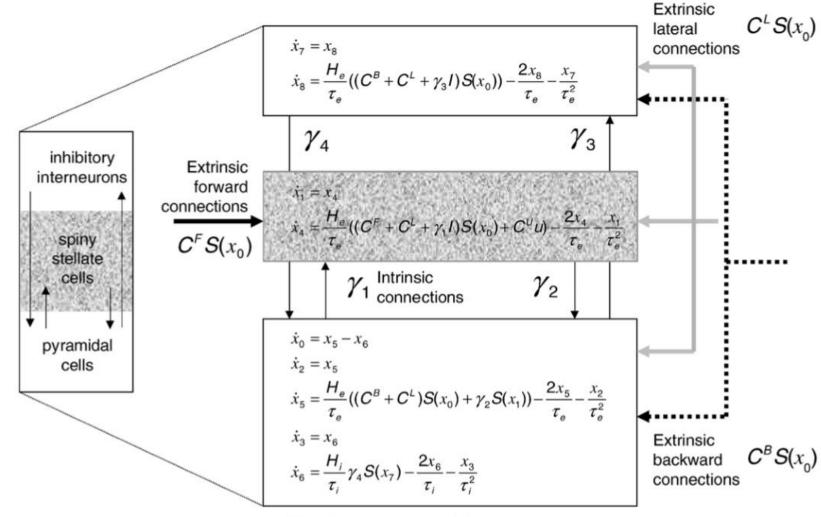
The naming refers to either data feature, within source connectivity, or dynamics.

There is usually not a unique model to model a data feature, but some might be more suited than others.



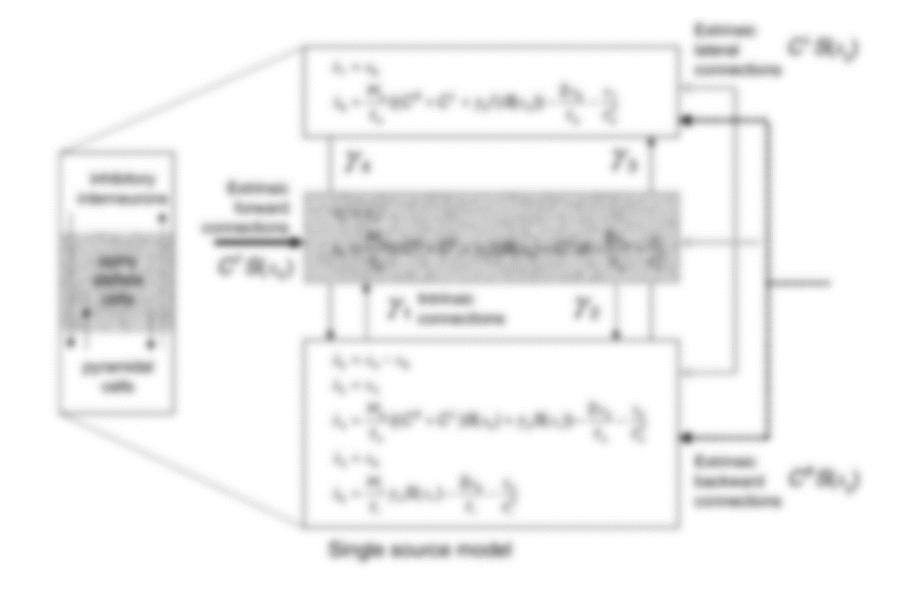
Garrido, Neuroimage, 2007; Moran, frontiers in Comp. Neuroscience, 2013; Friston, Neuroimage, 2012

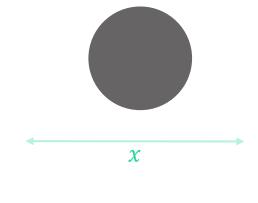
Models

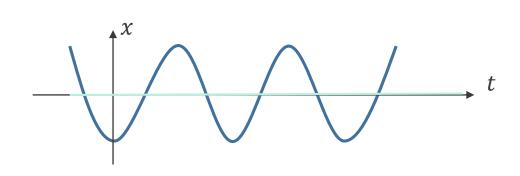


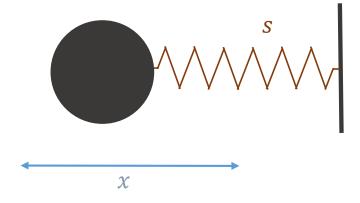
Single source model

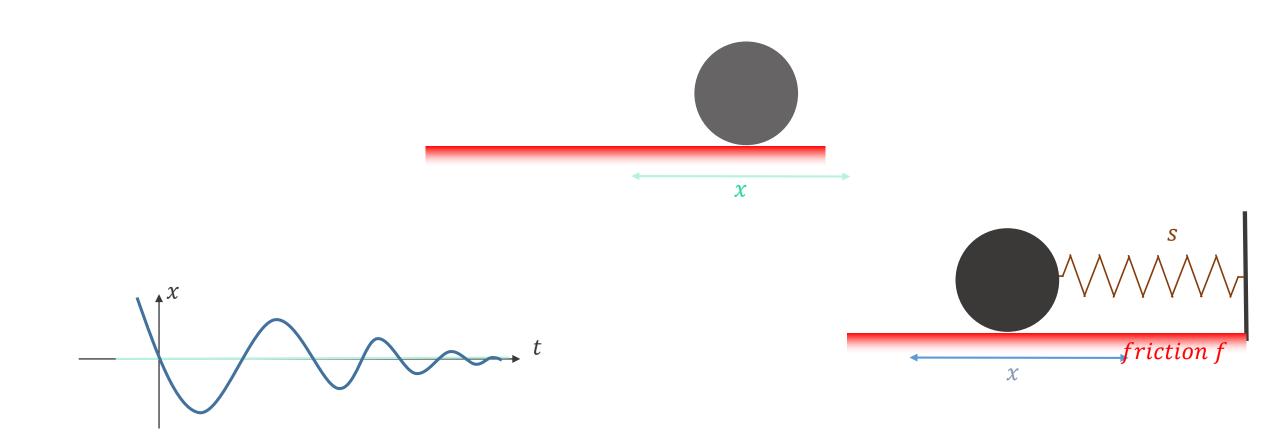
Models

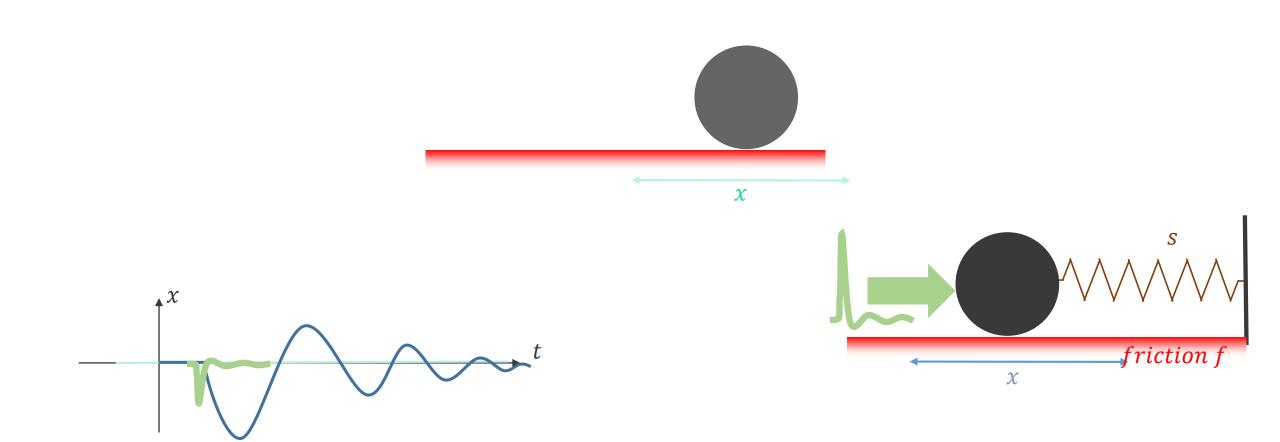


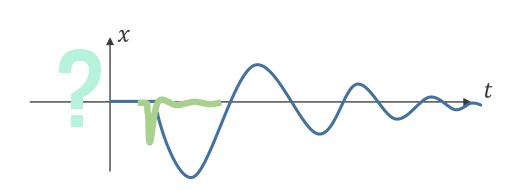


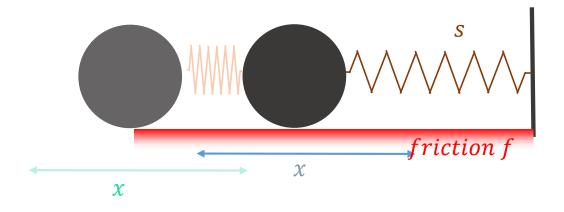




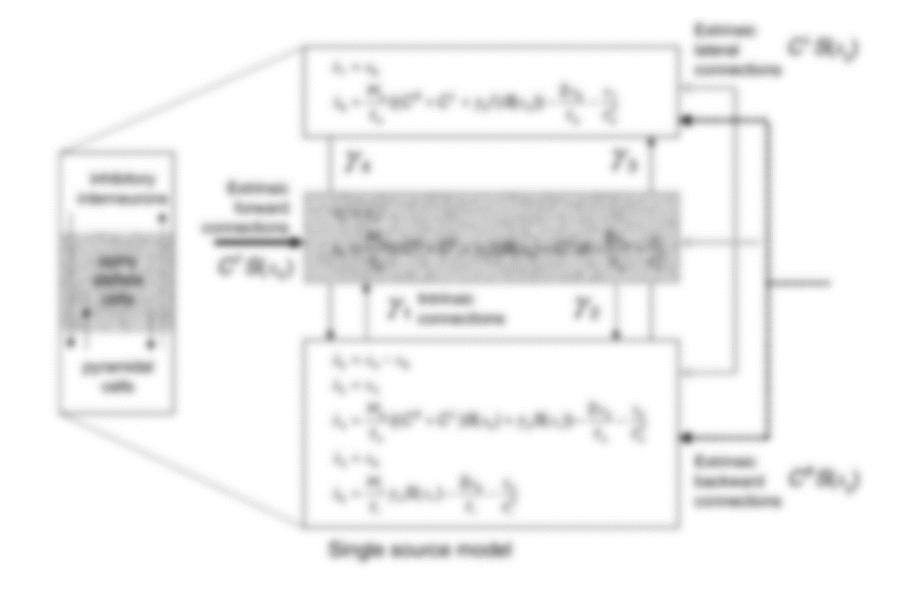




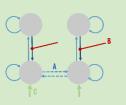




Models



Models



Between Source Connectivity



Within Source Connectivity



Dynamics



Forward Model

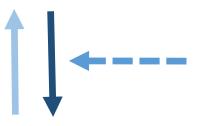
Between Source Connectivity

Sources / Regions



Three types of connections:

Forward, Backward, Lateral



Between condition effects



Input

SPM Variable

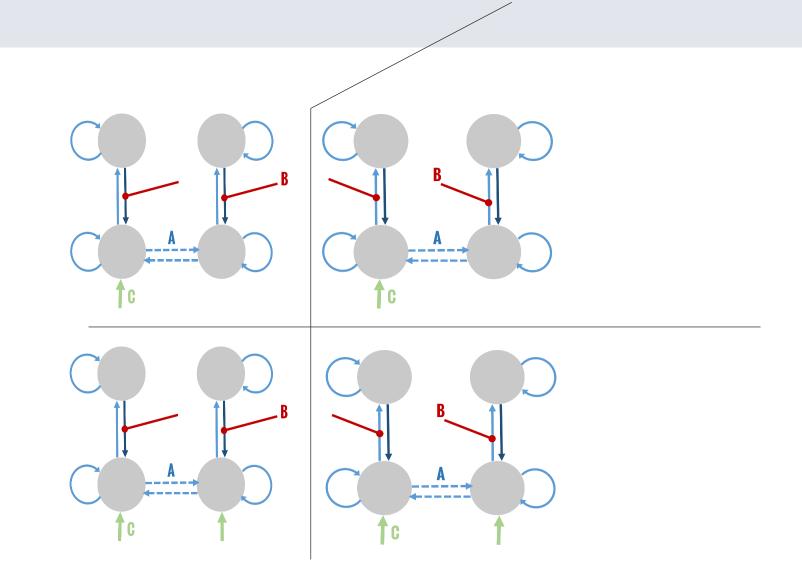
X

Α

F

Hypotheses should be based on classical finding.

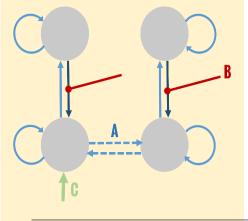
Once again, you try to explain a difference that is in the data.

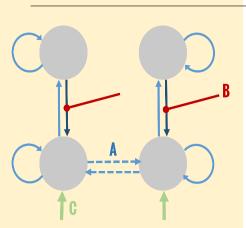


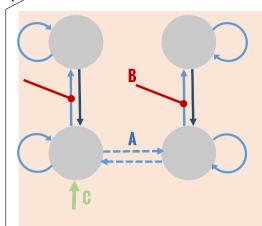
Hypotheses should be based on classical finding.

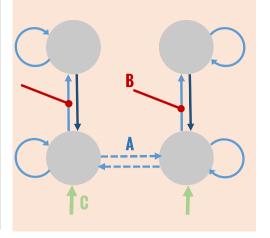
Once again, you try to explain a difference that is in the data.

Is there a condition specific forward modulation?



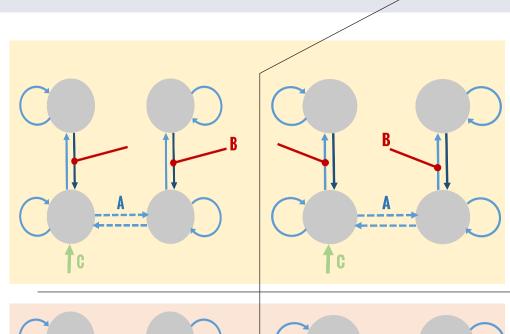




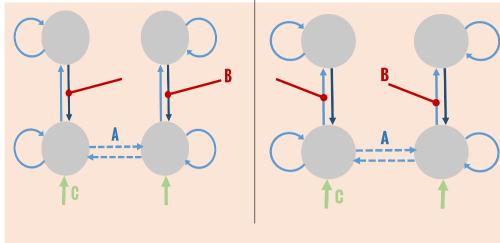


Hypotheses should be based on classical finding.

Once again, you try to explain a difference that is in the data.



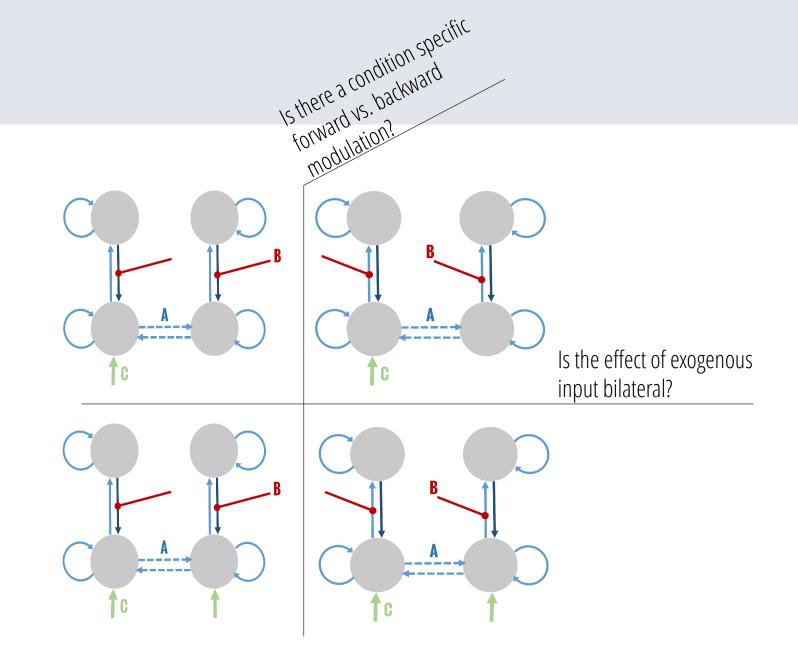
Is the effect of exogenous input bilateral?



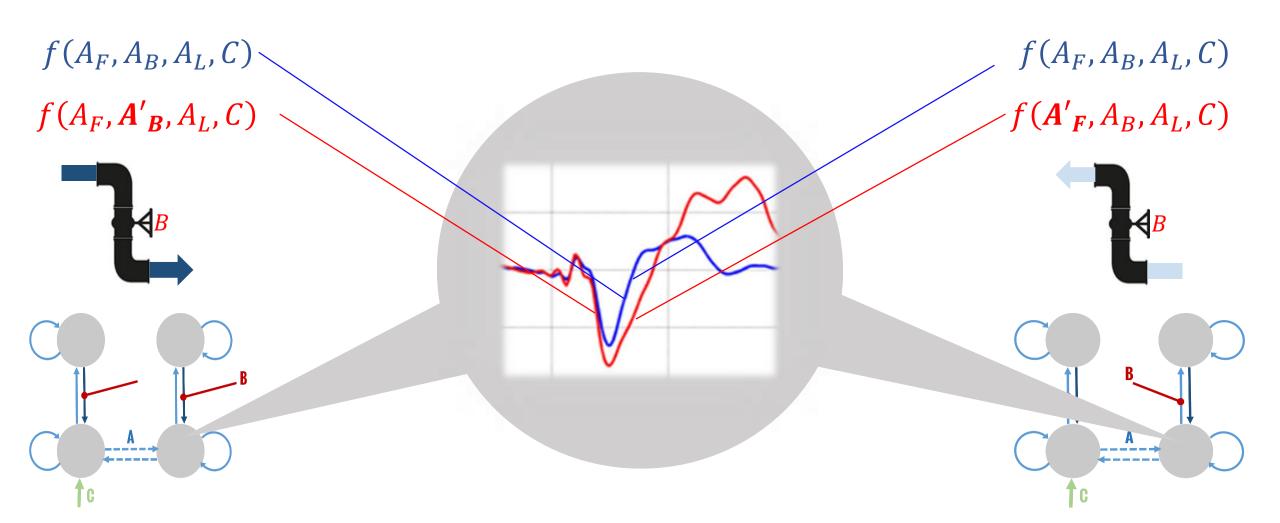
Computation of parameter estimates.

Model Comparisons

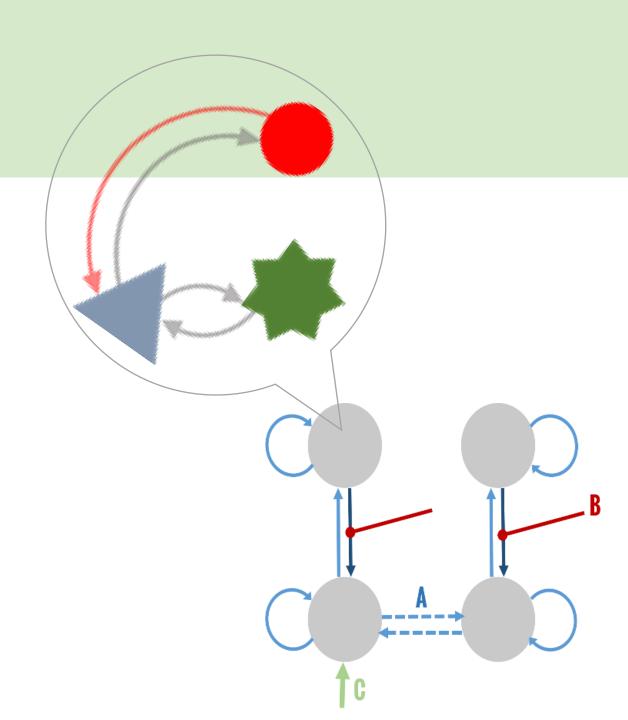
Which one of competing Hypotheses describes the data best.



What it means to have a condition specific effect

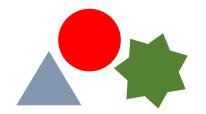


Within Source Connectivity



Within Source Connectivity

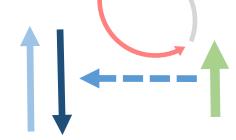
Three types of Cell Populations:



Pyramidal, Inhibitory, Stellate

Inhibitory / Excitatory effects on different populations

Dependence on Extrinsic Connectivity



SPM Variable

X

G

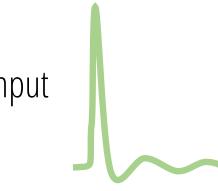
A, C

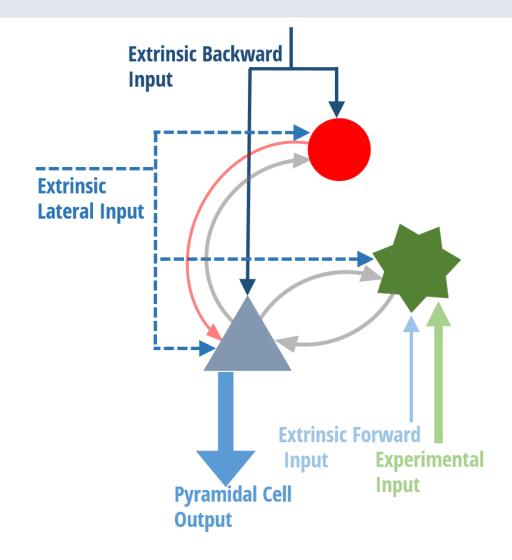
ERP Model

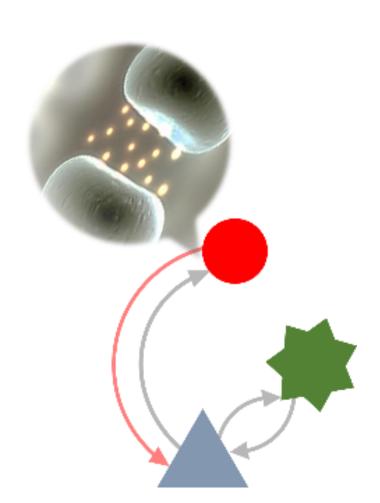
Name of a Between Source Connection refers to the cell population that is being targeted.

Output from the Pyramidal Cell

Experimental Input







Convolution Based Models

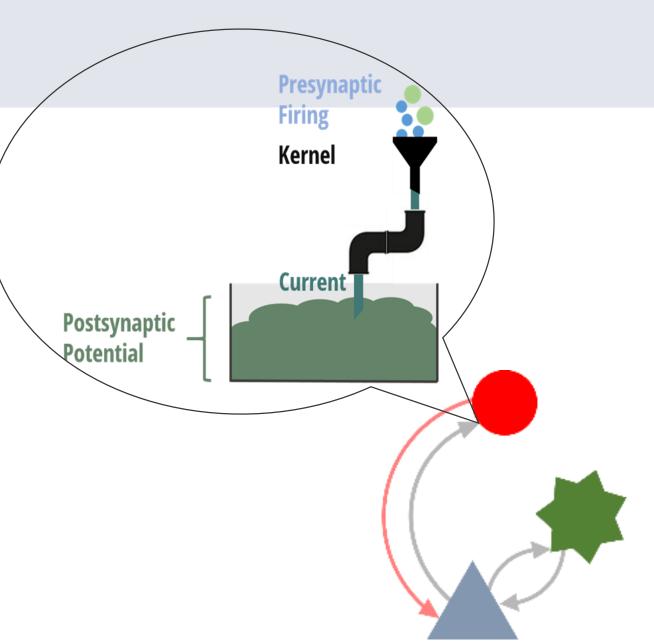
Jansen and Rit (1995)

The Kernel transforms the presynaptic firing rate into a postsynaptic potential.

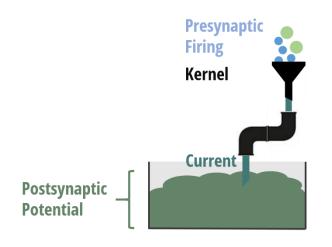
Transformation is a convolution.

Kernel is parameterized by two parameters.

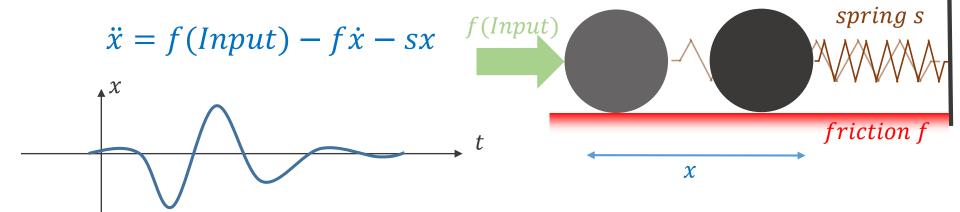
Voltage over time shows similarities with Harmonic Oscillator.



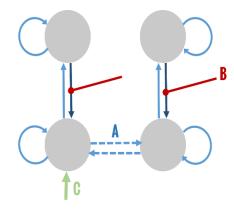
Convolution Based Models

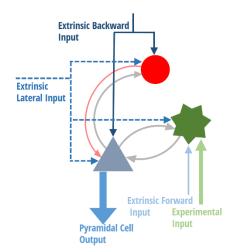


$$\ddot{v} = f(Input) - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$



$$\ddot{v} = f(Input) - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$











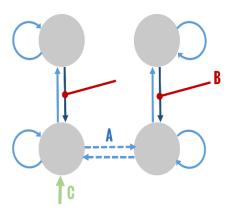
$$\ddot{v} = f(Input) - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$

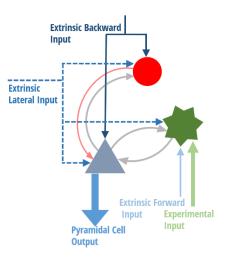












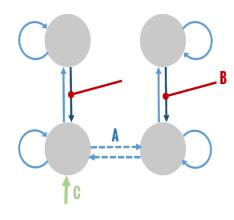
$$\ddot{v} = f(Input) - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$

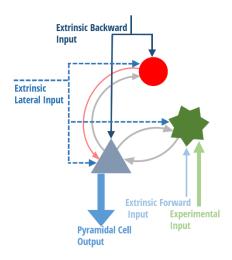












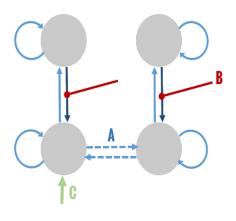
$$\ddot{v} = f(Input) - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$

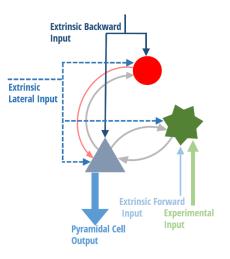












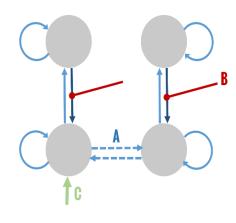
$$\ddot{v} = f(Input) - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$

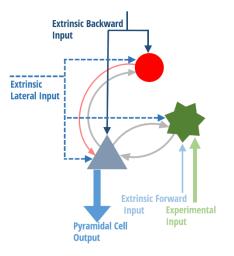










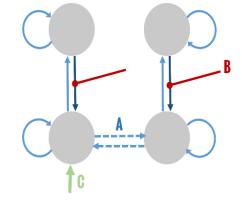


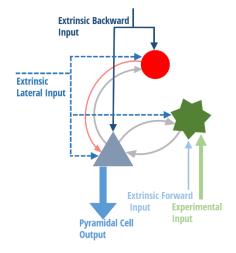
$$\ddot{v} = f(Input) - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$













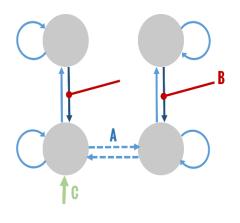
$$\ddot{v} = f(Input) - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$

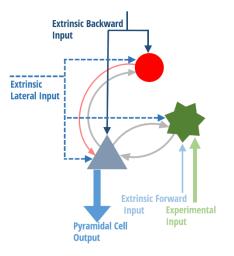












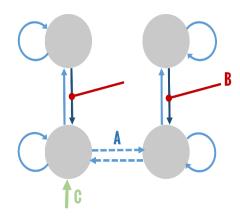
$$\ddot{v} = f(Input) - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$

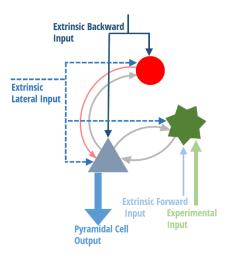
$$\ddot{v} = k_e((A_{back} + A_{lateral})) + G - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$

$$\ddot{v} = k_e((A_{Forward} + A_{lateral})) + G + C + C + \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$

$$\ddot{v} = k_e ((A_{back} + A_{lateral}) \triangle + G^* \bigcirc) - \frac{2}{\tau} \dot{v} - \frac{1}{\tau^2} v$$

$$\ddot{v} = k_i G - \frac{2}{\tau} \dot{v} - \frac{1}{\tau^2} v$$





$$\ddot{v} = f(Input) - \frac{2}{\tau}\dot{v} - \frac{1}{\tau^2}v$$

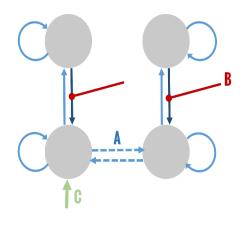
$$\ddot{v} = k_e \left((A_{back} + A_{lateral}) \triangle + G_{\bullet}^{\bullet} \triangle \right) - \frac{2}{\tau} \dot{v} - \frac{1}{\tau^2} v$$

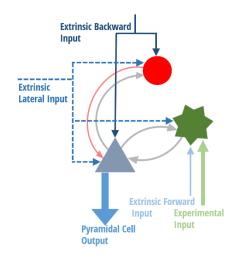
$$f(:,8) = (\text{He.*}((A\{2\} + A\{3\})*S(:,9) + G(:,3).*S(:,9)) - 2*x(:,8) - x(:,7)./Te)./Te;$$

$$\ddot{v} = k_e \left((A_{forward} + A_{lateral}) \triangle + G \triangle \right) + C - \frac{2}{\tau} \dot{v} - \frac{1}{\tau^2} v$$

$$\ddot{v} = k_e ((A_{back} + A_{lateral}) \triangle + G^* \bigcirc) -\frac{2}{\tau} \dot{v} - \frac{1}{\tau^2} v$$

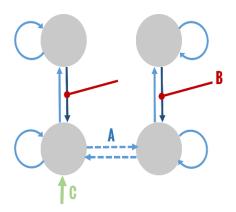
$$\ddot{v} = k_i G - \frac{2}{\tau} \dot{v} - \frac{1}{\tau^2} v$$

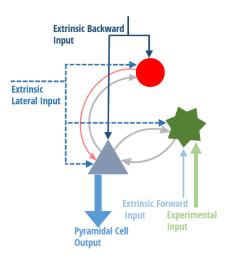




```
f(Input)
% Supragranular layer (inhibitory interneurons): Voltage & depolarizing current
f(:,7) = x(:,8);
f(:,8) = (He.*((A{2} + A{3})*S(:,9) + G(:,3).*S(:,9)) - 2*x(:,8) - x(:,7)./Te)./Te;
% Granular layer (spiny stellate cells): Voltage & depolarizing current
f(:,1) = x(:,4);
f(:,1) = x(:,4);

f(:,4) = (He.*((A{1} + A{3})*S(:,9) + G(:,1).*S(:,9) + U) - 2*x(:,4) - x(:,1)./Te)./Te;
% Infra-granular layer (pyramidal cells): depolarizing current
f(:,2) = x(:,5);
f(:,5) = (He.*((A{2} + A{3})*S(:,9) + G(:,2).*S(:,1)) - 2*x(:,5) - x(:,2)./Te)./Te;
% Infra-granular layer (pyramidal cells): hyperpolarizing current
f(:,3) = x(:,6);
f(:,6) = (Hi.*G(:,4).*S(:,7) - 2*x(:,6) - x(:,3)./Ti)./Ti;
% Infra-granular layer (pyramidal cells): Voltage
f(:,9) = x(:,5) - x(:,6);
```





Forward Model

Equivalent Current Dipoles
Leadfield matrix

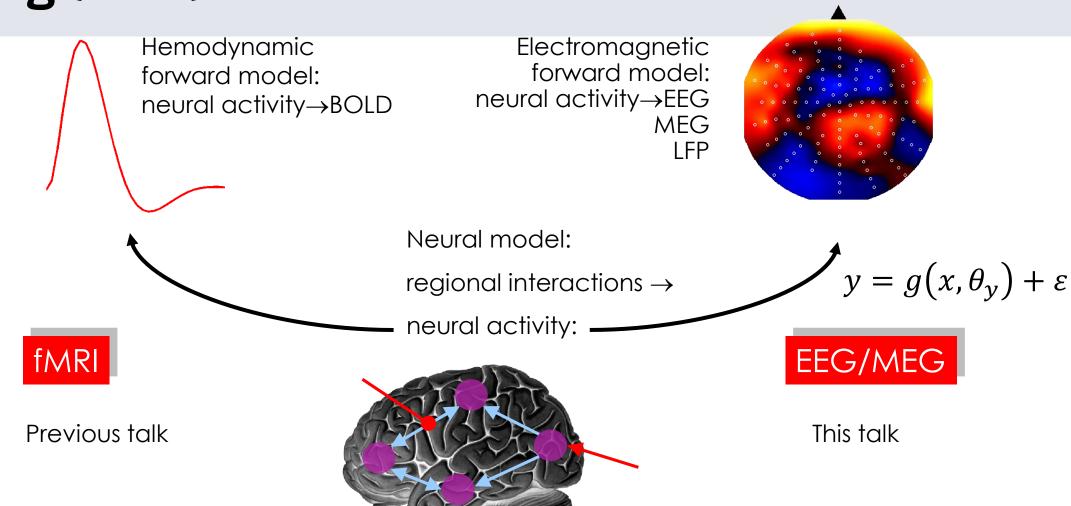
Measured Data

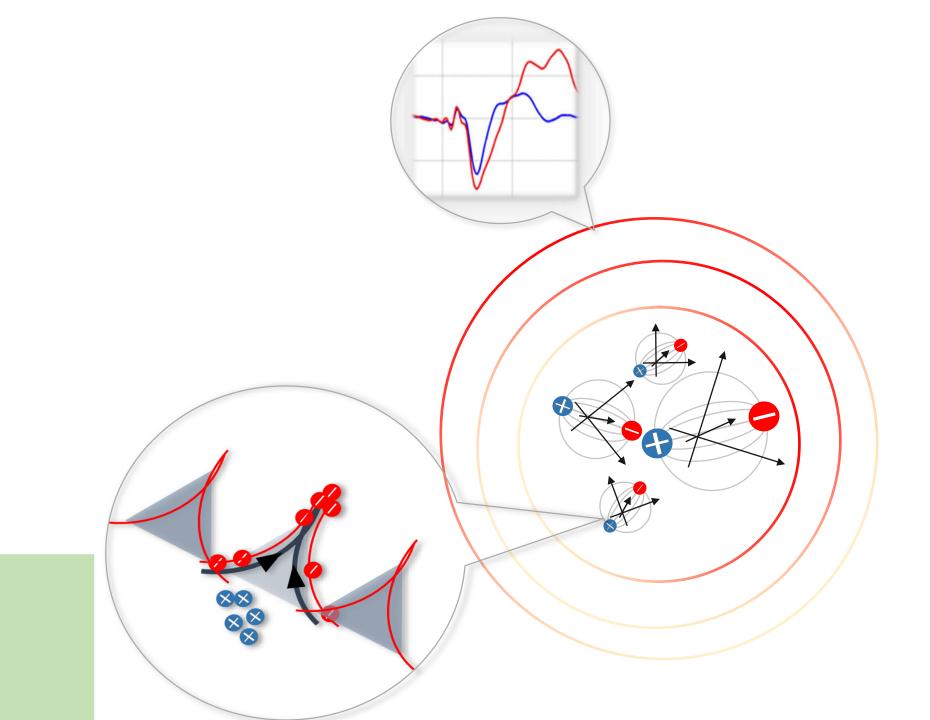
SPM Variable

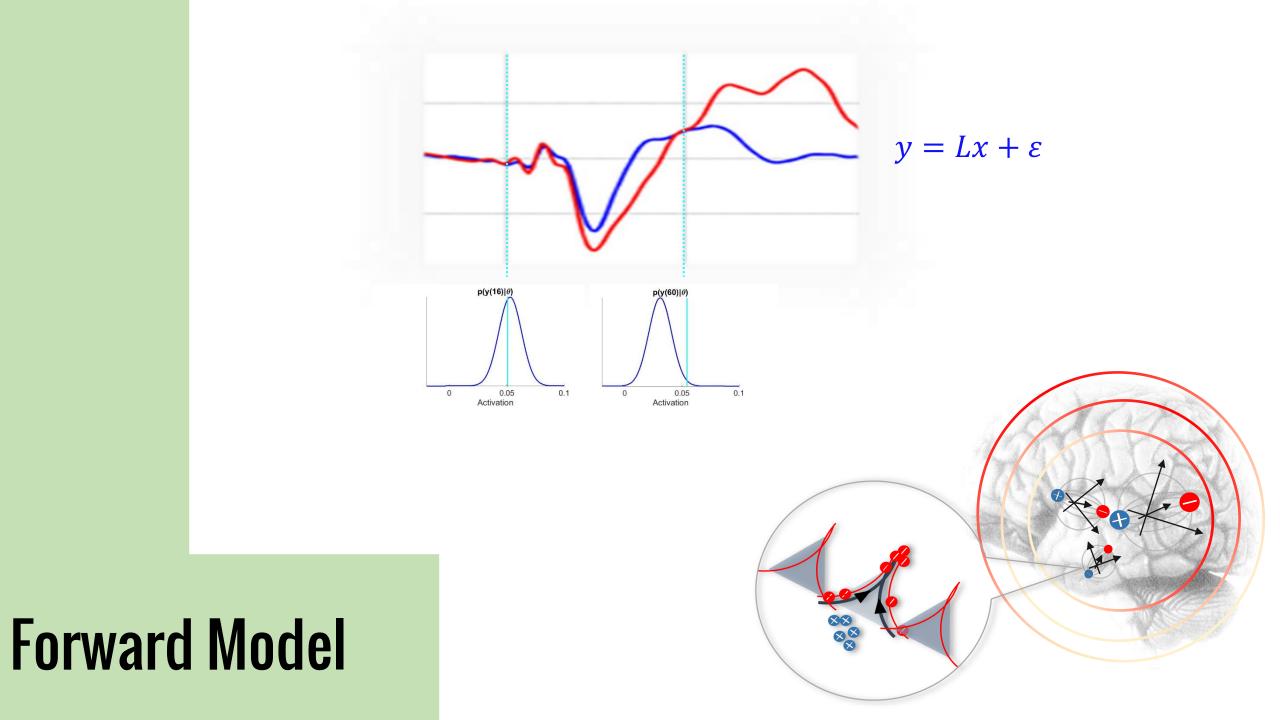
X

Y

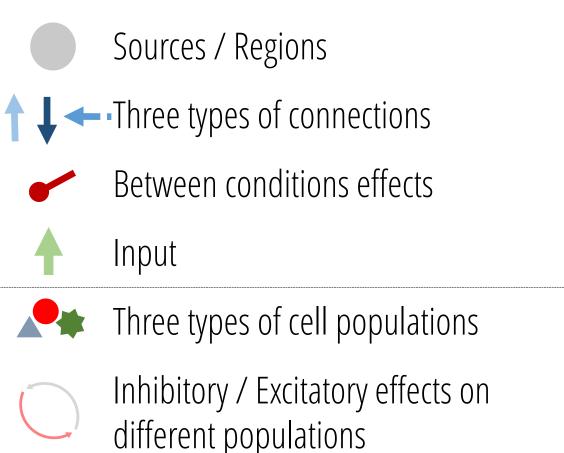
Recap: Dynamic Causal Modeling (DCM)

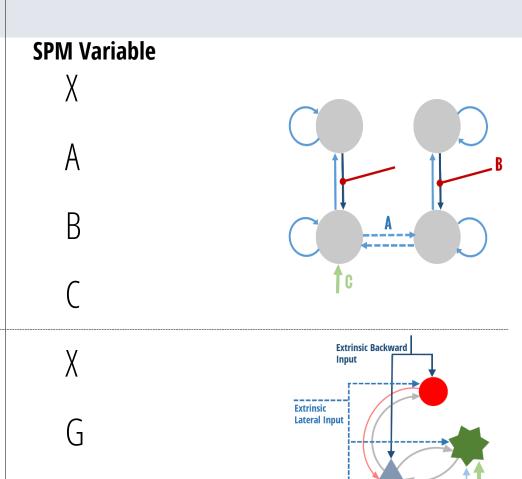


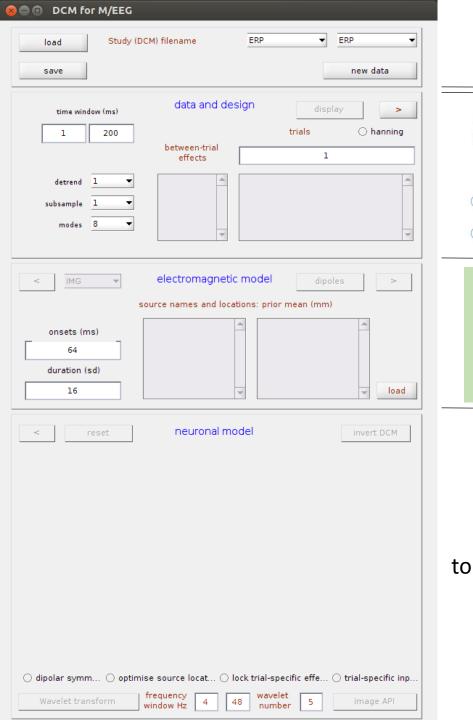




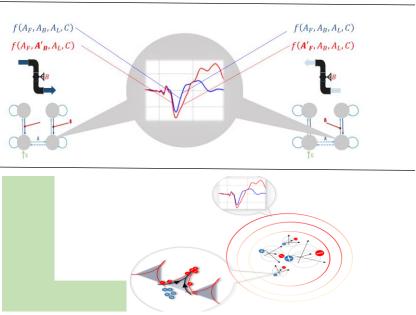
Reminder before SPM





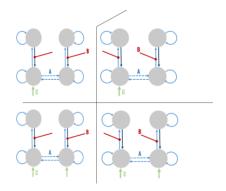






from

		IA1	rA1	ISTG	rSTG
	IA1				
)	rA1				
	ISTG				
	rSTG				·



Some weirdly unsorted appendix

Thank you

Dario Schoebi

University and ETH Zürich dschoebi@biomed.ee.ethz.ch

