

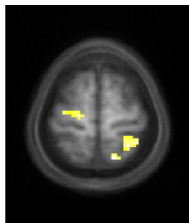
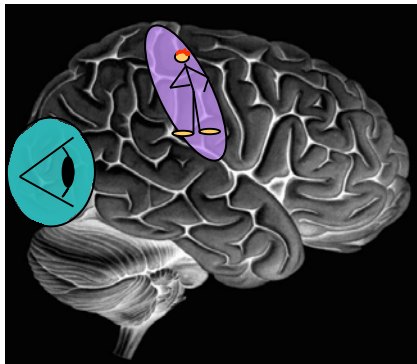
Dynamic causal modelling for fMRI

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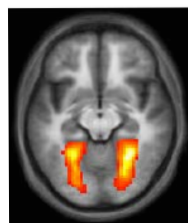
CPC 2018, Zürich, Switzerland

Specialisation vs. Integration

Functional Specialisation



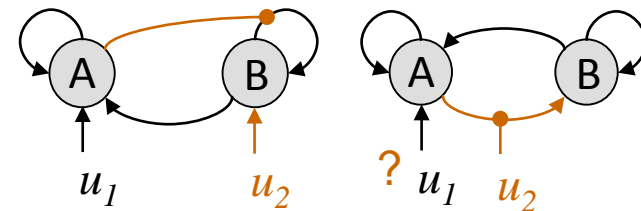
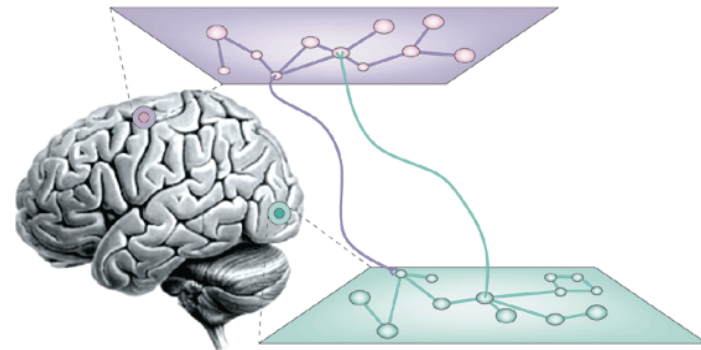
u_1



$u_1 \times u_2$

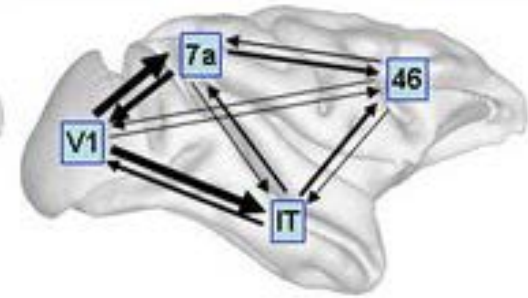
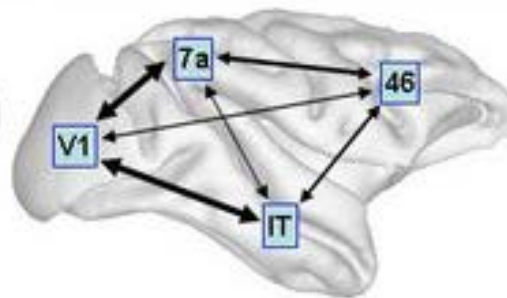
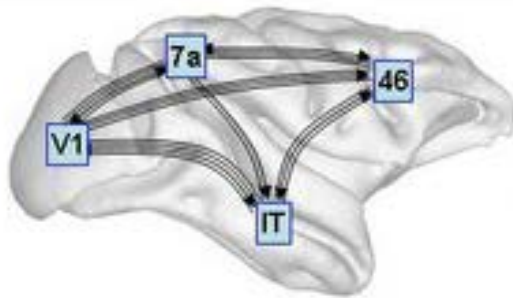
«**Where**, in the brain, did my experimental manipulation have **an effect**?»

Functional Integration



«**How** did my experimental manipulation **propagate through the network**?»

Structural, functional & effective connectivity



Sporns 2007, *Scholarpedia*

anatomical/structural

- presence of physical connections

→ *DWI, tractography, tracer studies (animals)*

functional

- statistical dependency between regional time series

→ *correlations, ICA*

effective

- direct influences between neuronal populations

→ *DCM*

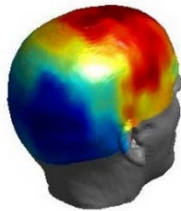
Context-independent

Mechanism - free

Mechanistic

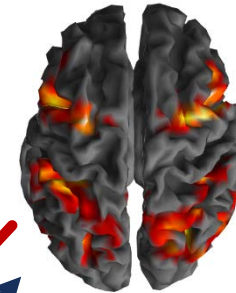
Dynamic causal modelling

EEG,
MEG



Model inversion:
Estimating
neuronal
mechanisms

fMRI



Forward model:
Predicting
measured activity

$$y = g(x, \theta) + \varepsilon$$



$$\frac{dx}{dt} = f(x, u, \theta) + \omega$$

State equation:
Describing neuronal
dynamics (and
hemodynamics)

DCM for EEG
→ Next lecture
→ Dario Schöbi



Dynamic causal modelling



ACADEMIC
PRESS

Available online at www.sciencedirect.com



NeuroImage 19 (2003) 1273–1302

NeuroImage

www.elsevier.com/locate/ynimg

Dynamic causal modelling

K.J. Friston,* L. Harrison, and W. Penny

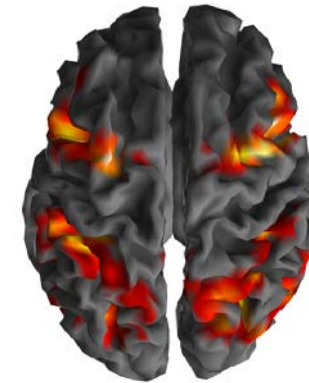
The Wellcome Department of Imaging Neuroscience, Institute of Neurology, Queen Square, London WC1N 3BG, UK

Received 18 October 2002; revised 7 March 2003; accepted 2 April 2003

DCM for fMRI - Overview

Model inversion:

Estimating
neuronal
mechanisms

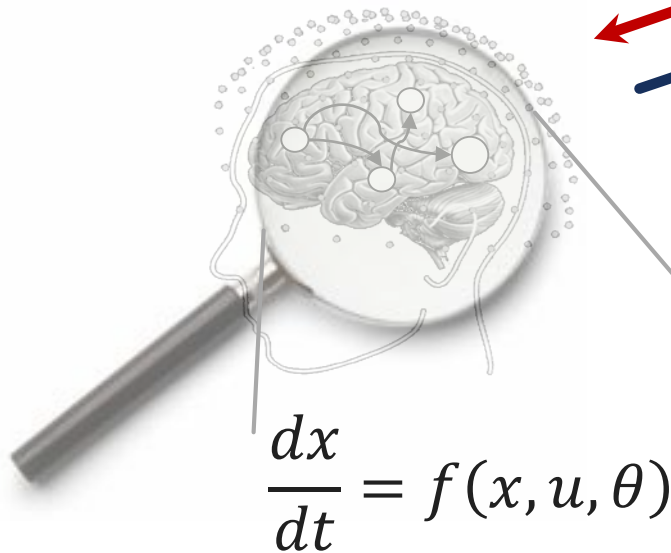


fMRI

Forward model:

Predicting
measured activity

$$y = g(x, \theta) + \varepsilon$$



Neural state equation:

Describing neuronal
dynamics

DCM for fMRI - Overview

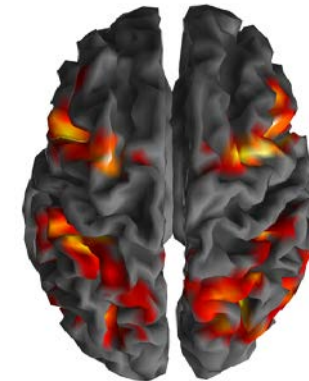
Model inversion:
Estimating
neuronal
mechanisms

Forward model:
Predicting
measured activity

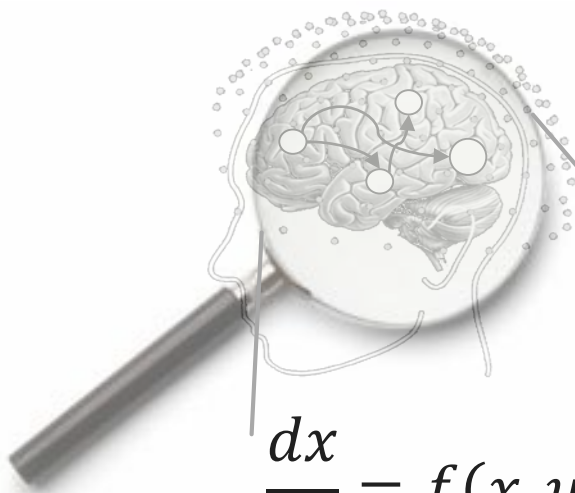
$$y = g(x, \theta) + \varepsilon$$

Neural state equation:
Describing neuronal
dynamics

$$\frac{dx}{dt} = f(x, u, \theta)$$



fMRI





Neuronal state equations

$$\frac{dx}{dt} = f(x, u)$$

Neuronal state equations

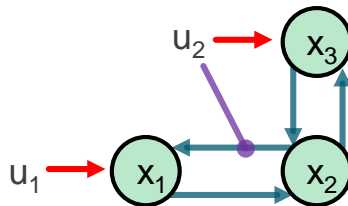
$$\frac{dx}{dt} = f(x, u) \approx f(x_0, 0) + \frac{\partial f}{\partial x} x + \frac{\partial f}{\partial u} u + \frac{\partial^2 f}{\partial x \partial u} ux + \frac{\partial^2 f}{\partial x^2} \frac{x^2}{2} + \dots$$

bilinear model

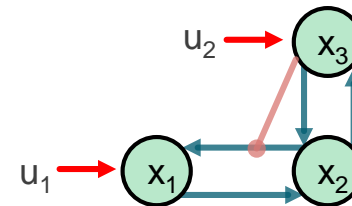
Neuronal state equations

$$\frac{dx}{dt} = f(x, u) \approx f(x_0, 0) + \overset{A}{\frac{\partial f}{\partial x}} x + \overset{C}{\frac{\partial f}{\partial u}} u + \overset{B}{\frac{\partial^2 f}{\partial x \partial u}} ux + \overset{D}{\frac{\partial^2 f}{\partial x^2} \frac{x^2}{2}} + \dots$$

bilinear model

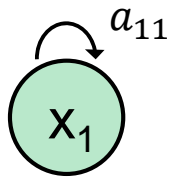


nonlinear model



Neuronal state equations

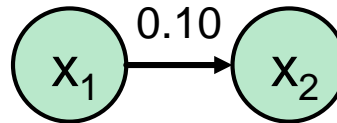
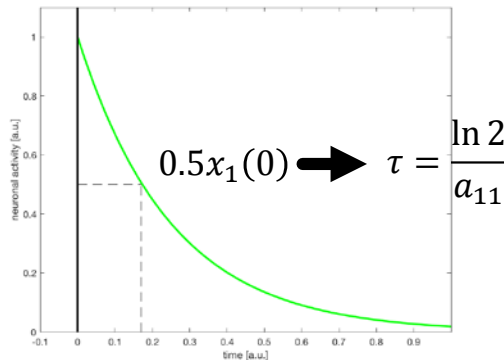
DCM effective connectivity parameters are rate constants



$$\frac{dx_1}{dt} = a_{11}x_1$$



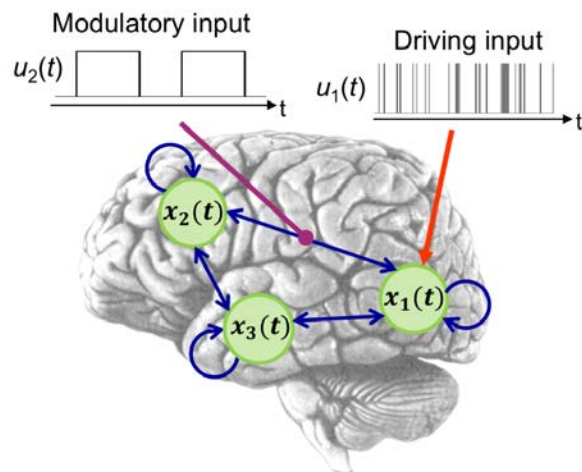
$$x_1(t) = x_1(0) \cdot \exp(a_{11}t)$$



If $\text{region}_1 \rightarrow \text{region}_2$ is 0.10s^{-1} , this means that, per unit time, the increase in activity in region_2 corresponds to 10% of the current activity in region_1

Neuronal state equations

Interim summary: bilinear neuronal state equation



State change

External inputs

Current state

$$\frac{dx}{dt} = \underbrace{\left(A + \sum_{j=1}^m u_j B^{(j)} \right)}_{\text{connectivity}} x + C u$$

$$\theta = \{ A, B^{(1)}, \dots, B^{(m)}, C \}$$

Endogenous connectivity

Modulatory connectivity

Driving inputs

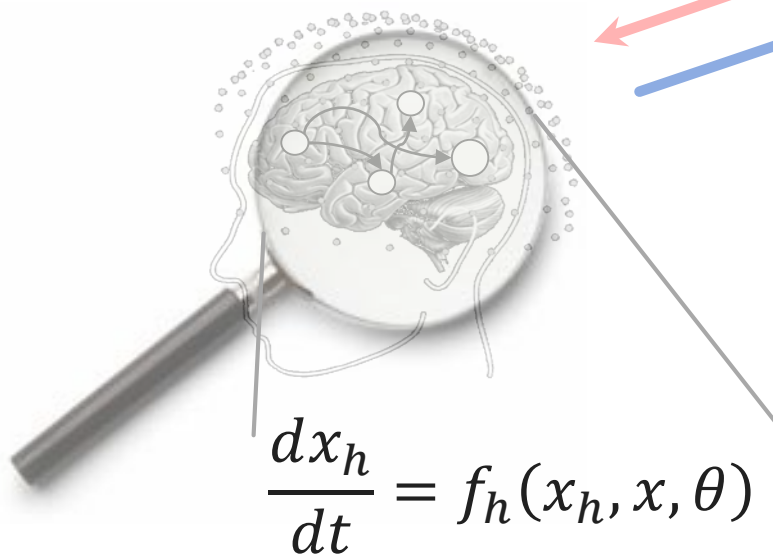
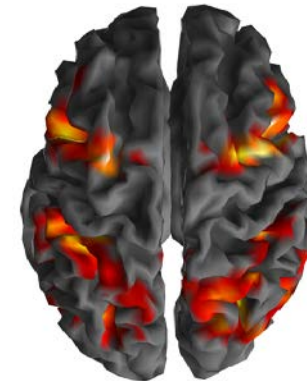
DCM for fMRI - Overview

Model inversion:
Estimating
neuronal
mechanisms

Forward model:
Predicting
measured activity

$$y = g(x, \theta) + \varepsilon$$

fMRI

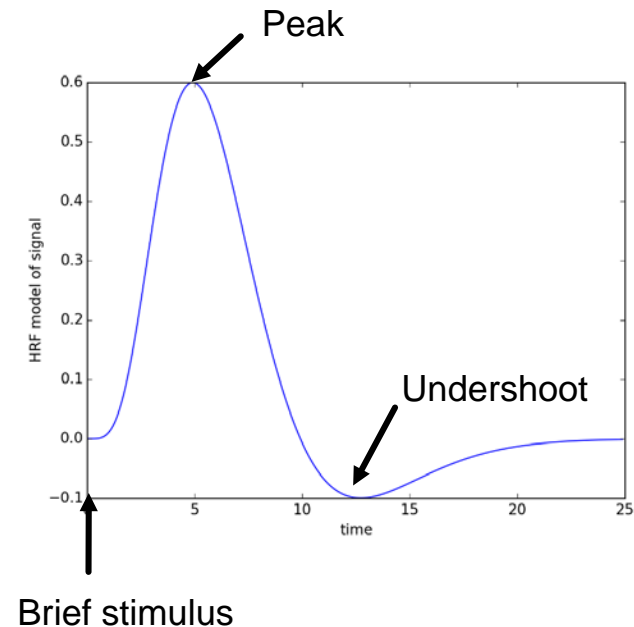
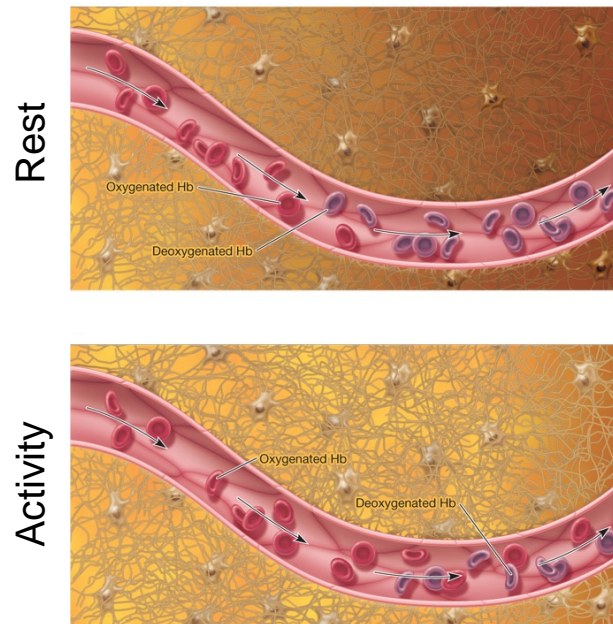


Hemodynamic state equation:
Describing hemodynamics

The hemodynamic response

Neuronal dynamics only indirectly observable via hemodynamic response

↑ neuronal activity
 ↑ blood flow
 ↑ oxygenated Hb
 ↑ $T2^*$
 ↑ fMRI signal



The hemodynamic model

6 parameters:

$$\theta^h = \{\kappa, \gamma, \tau, \alpha, \rho, \varepsilon\}$$

Important for model fitting,
but typically of no interest
for statistical inference.

Region specific HRF

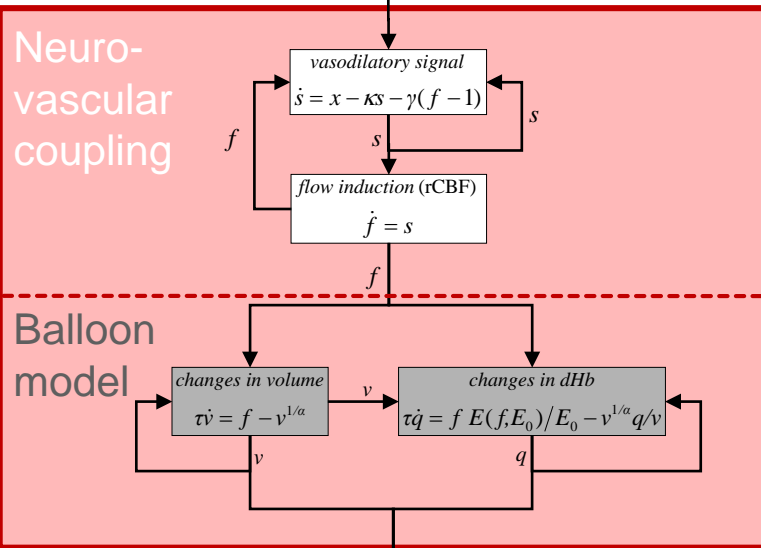
→ Parameters computed
separately for each region

State equation

neural

Inputs u

$$\frac{dx}{dt} = \left(A + \sum_{j=1}^m u_j B^{(j)} \right) x + Cu$$



hemodynamic

$$\lambda(q, v) = \frac{\Delta S}{S_0} \approx V_0 \left[k_1(1 - q) + k_2 \left(1 - \frac{q}{v} \right) + k_3(1 - v) \right]$$

$$k_1 = 4.3 \vartheta_0 E_0 TE$$

$$k_2 = \varepsilon r_0 E_0 TE$$

$$k_3 = 1 - \varepsilon$$

**BOLD signal
change equation**

DCM for fMRI - Overview

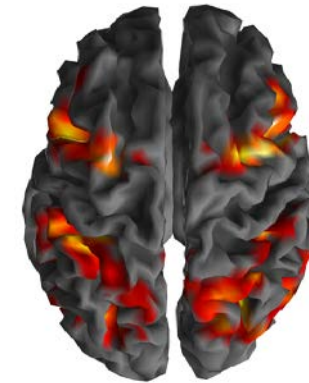
Model inversion:
Estimating
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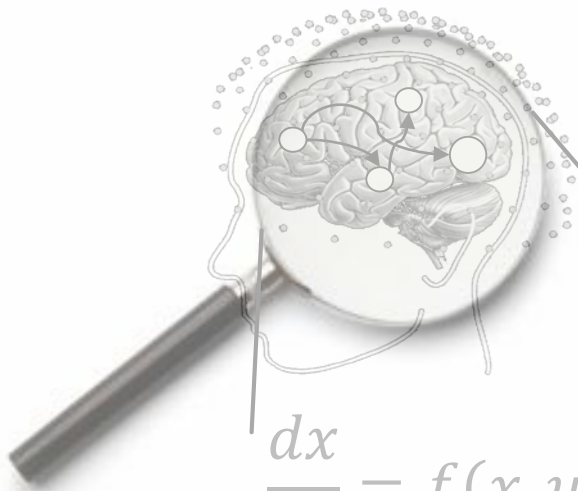
$$y = g(x, \theta) + \varepsilon$$

Neural state equation:
Describing neuronal
dynamics

$$\frac{dx}{dt} = f(x, u, \theta) + \omega$$



fMRI



The BOLD signal equation

Resting blood
volume

Deoxyhemoglobin
content

Blood
volume

$$\lambda(q, v) = \frac{\Delta S}{S_0} \approx V_0 \left[k_1(1 - q) + k_2 \left(1 - \frac{q}{v} \right) + k_3(1 - v) \right]$$

BOLD-Signal Parameters:

$$k_1 = 4.3 \vartheta_0 E_0 TE$$

$$k_2 = \varepsilon r_0 E_0 TE$$

$$k_3 = 1 - \varepsilon$$

$$V_0 = 0.04 \quad E_0 = 0.32 - 0.4$$

At 1.5 Tesla

At 3 Tesla

At 7 Tesla

$$\vartheta_0 \approx 40.3 \text{ s}^{-1}$$

$$\vartheta_0 \approx 80.6 \text{ s}^{-1}$$

$$\vartheta_0 \approx 188 \text{ s}^{-1}$$

$$r_0 \approx 25 \text{ s}^{-1}$$

$$r_0 \approx 110 \text{ s}^{-1}$$

$$r_0 \approx 340 \text{ s}^{-1}$$

$$TE \approx 0.04 \text{ s}$$

$$TE \approx 0.035 \text{ s}$$

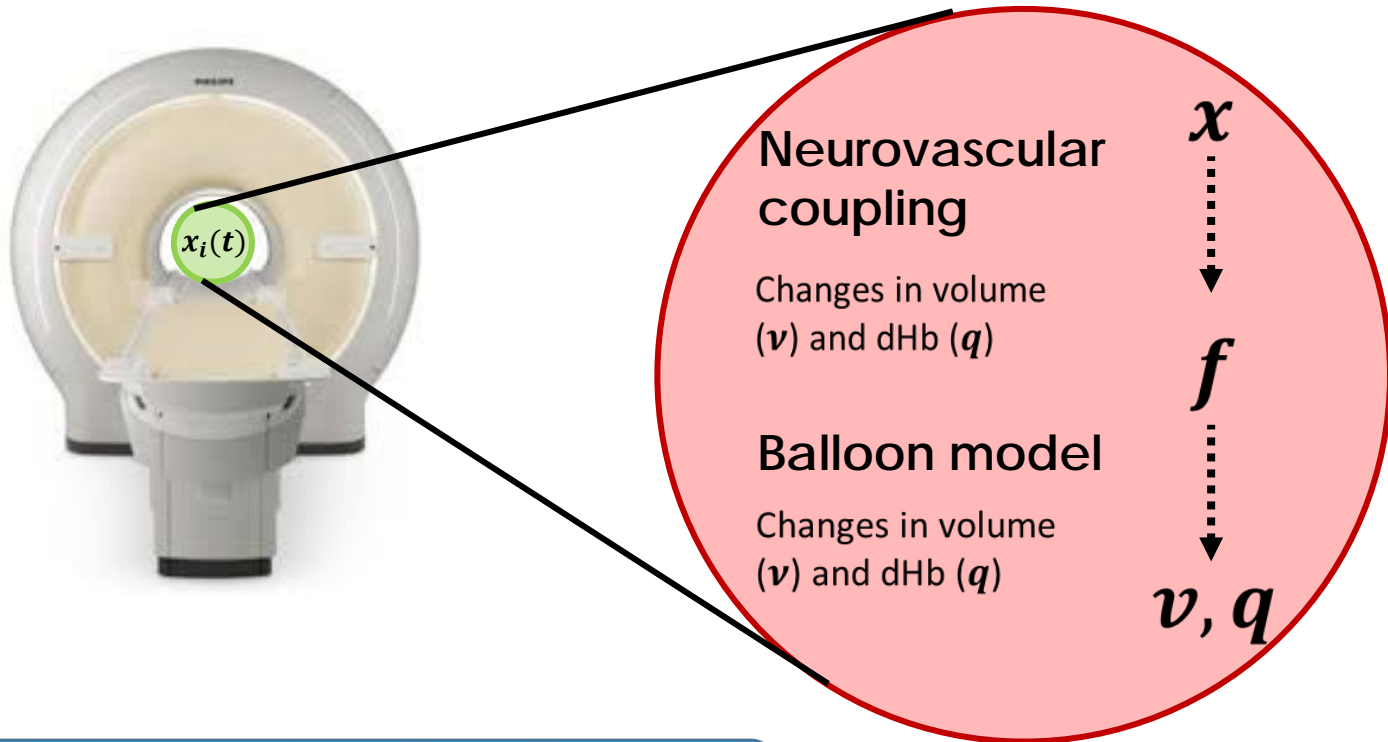
$$TE \approx 0.025 \text{ s}$$

$$\varepsilon \approx 1.28$$

$$\varepsilon \approx 0.47$$

$$\varepsilon \approx 0.026$$

From neural activity to the BOLD signal: Summary

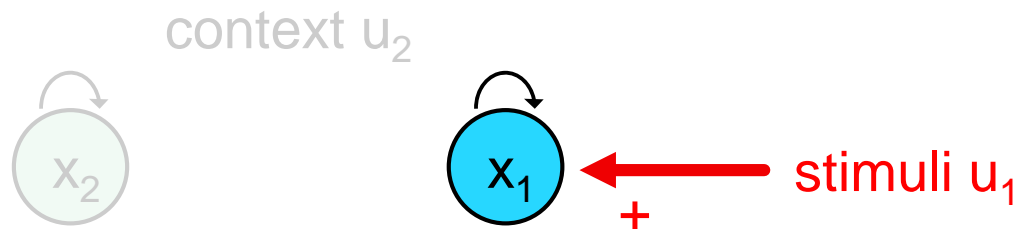


BOLD signal is a **direct function** of v and q

$$y = \frac{\Delta S}{S_0} = g(v, q) + \varepsilon$$

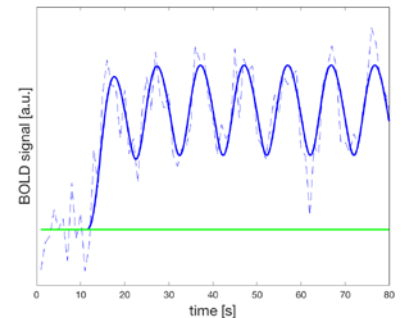
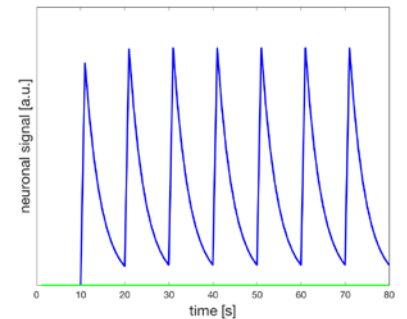
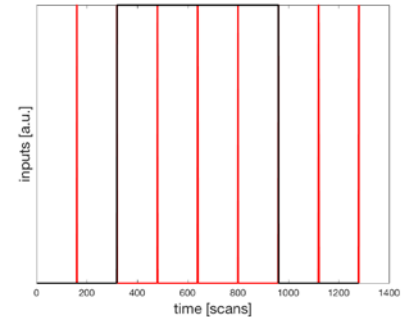
Simulation example: What can DCM explain?

Example: single node



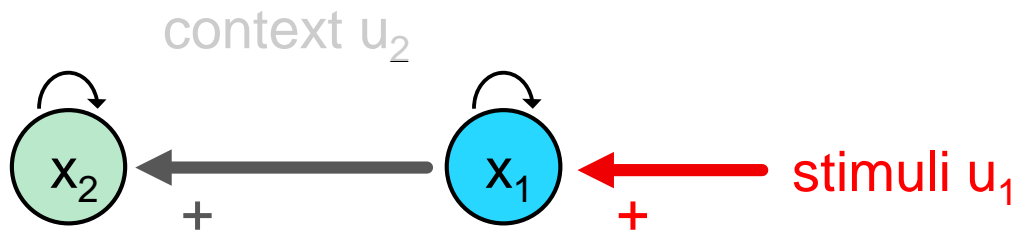
$$\frac{dx}{dt} = Ax + u_2 B^{(2)}x + Cu_1$$

$$\begin{bmatrix} \dot{x}_1 \\ \dot{x}_2 \end{bmatrix} = \begin{bmatrix} a_{11} & 0 \\ 0 & a_{22} \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + u_2 \begin{bmatrix} 0 & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + \begin{bmatrix} c_{11} & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} u_1 \\ u_2 \end{bmatrix}$$



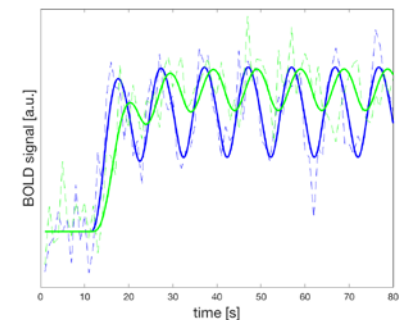
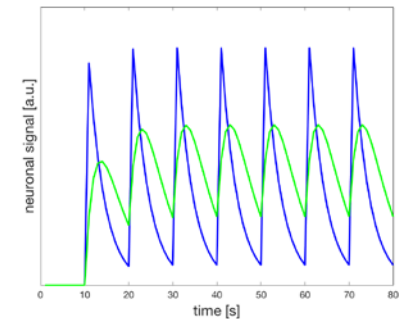
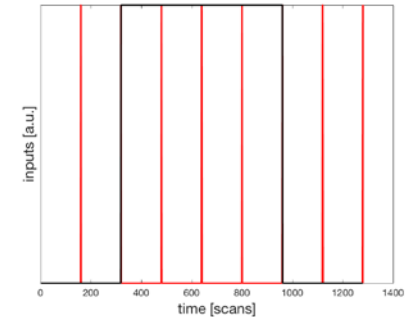
Simulation example: What can DCM explain?

Example: two connected node



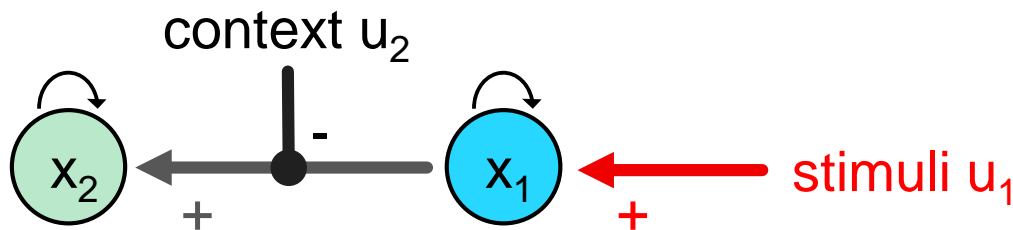
$$\frac{dx}{dt} = Ax + u_2 B^{(2)}x + Cu_1$$

$$\begin{bmatrix} \dot{x}_1 \\ \dot{x}_2 \end{bmatrix} = \begin{bmatrix} a_{11} & 0 \\ a_{21} & a_{22} \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + u_2 \begin{bmatrix} 0 & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + \begin{bmatrix} c_{11} & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} u_1 \\ u_2 \end{bmatrix}$$



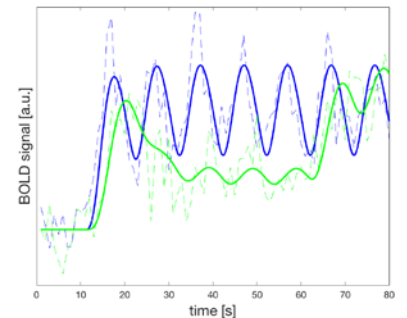
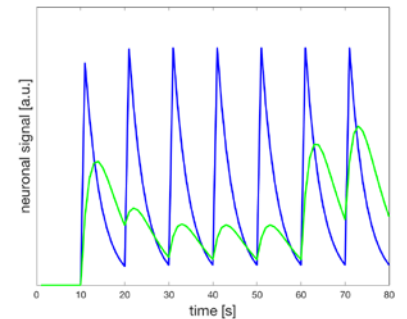
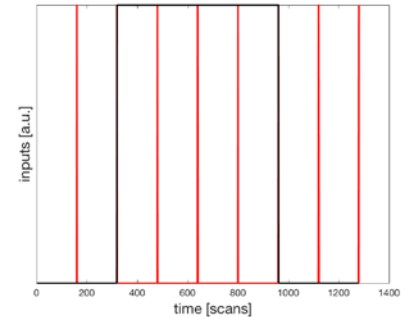
Simulation example: What can DCM explain?

Example: modulation of connection



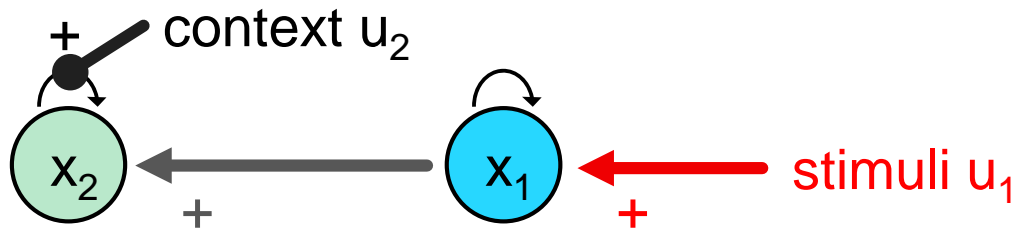
$$\frac{dx}{dt} = Ax + u_2 B^{(2)}x + Cu_1$$

$$\begin{bmatrix} \dot{x}_1 \\ \dot{x}_2 \end{bmatrix} = \begin{bmatrix} a_{11} & 0 \\ a_{21} & a_{22} \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + u_2 \begin{bmatrix} 0 & 0 \\ b_{21}^{(2)} & 0 \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + \begin{bmatrix} c_{11} & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} u_1 \\ u_2 \end{bmatrix}$$



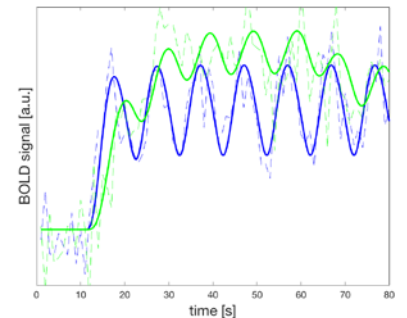
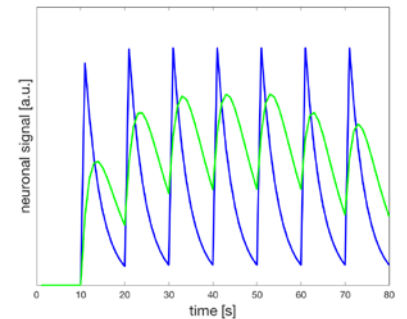
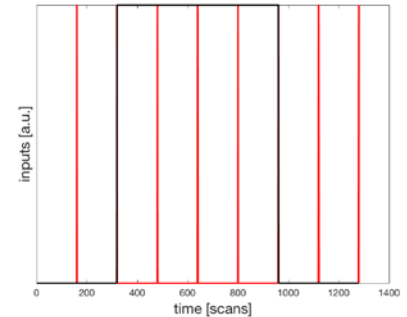
Simulation example: What can DCM explain?

Example: modulation of inhibitory self-connection



$$\frac{dx}{dt} = Ax + u_2 B^{(2)}x + Cu_1$$

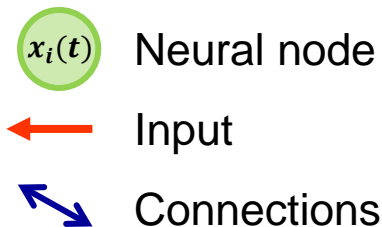
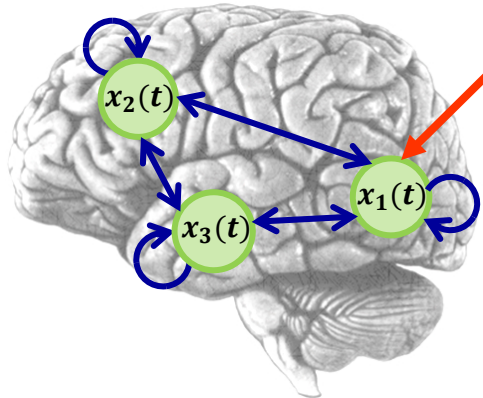
$$\begin{bmatrix} \dot{x}_1 \\ \dot{x}_2 \end{bmatrix} = \begin{bmatrix} a_{11} & 0 \\ a_{21} & a_{22} \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + u_2 \begin{bmatrix} 0 & 0 \\ 0 & b_{22}^{(2)} \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + \begin{bmatrix} c_{11} & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} u_1 \\ u_2 \end{bmatrix}$$



DCM for fMRI

A simple model of
a neural network

...



... described as a
dynamical system

...

$$\dot{x} = f(x, u, \theta)$$

... causes the data
(BOLD signal).

$$y = g(x, \theta) + \varepsilon$$

Let the system run with input (u) and parameters (θ), and you will get a BOLD signal time course y that you can compare to the measured data.

DCM for fMRI - Overview

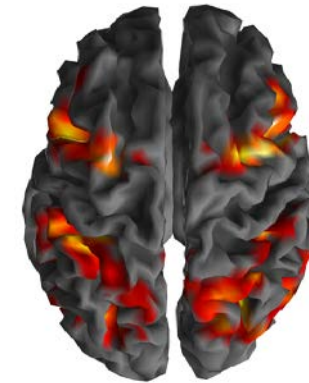
Model inversion:
Estimating
neuronal
mechanisms

Forward model:
Predicting
measured activity

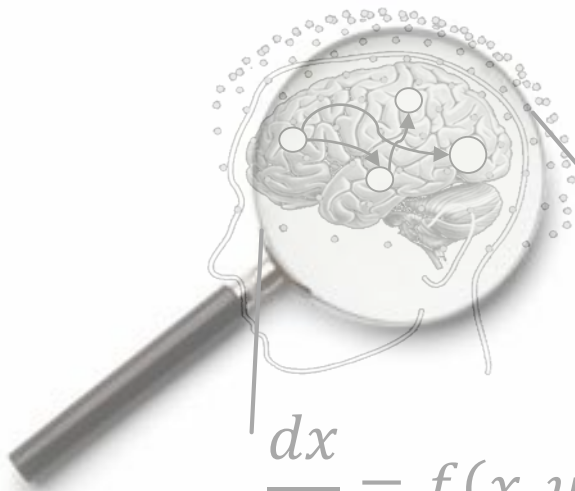
$$y = g(x, \theta) + \varepsilon$$

Neural state equation:
Describing neuronal
dynamics

$$\frac{dx}{dt} = f(x, u, \theta) + \omega$$



fMRI

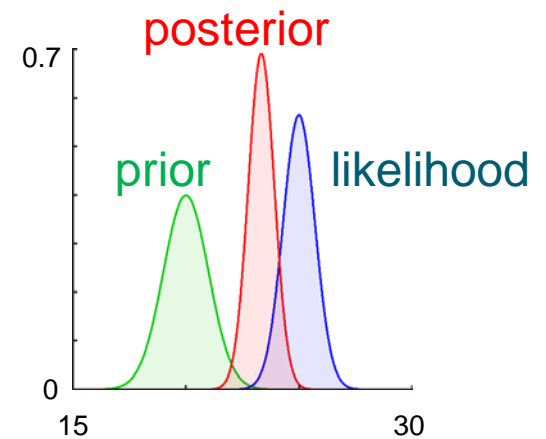


Bayes' theorem

$$\text{posterior } p(\theta|y, m) = \frac{\text{likelihood } p(y|\theta, m) \text{ prior } p(\theta|m)}{\text{model evidence } p(y|m)}$$



Reverend Thomas Bayes
(1702-1761)



The likelihood function for DCM

$$p(y(t)|\theta, m) = \mathcal{N}(y(t); g(\theta^n, \theta^h, u), \theta^\sigma)$$

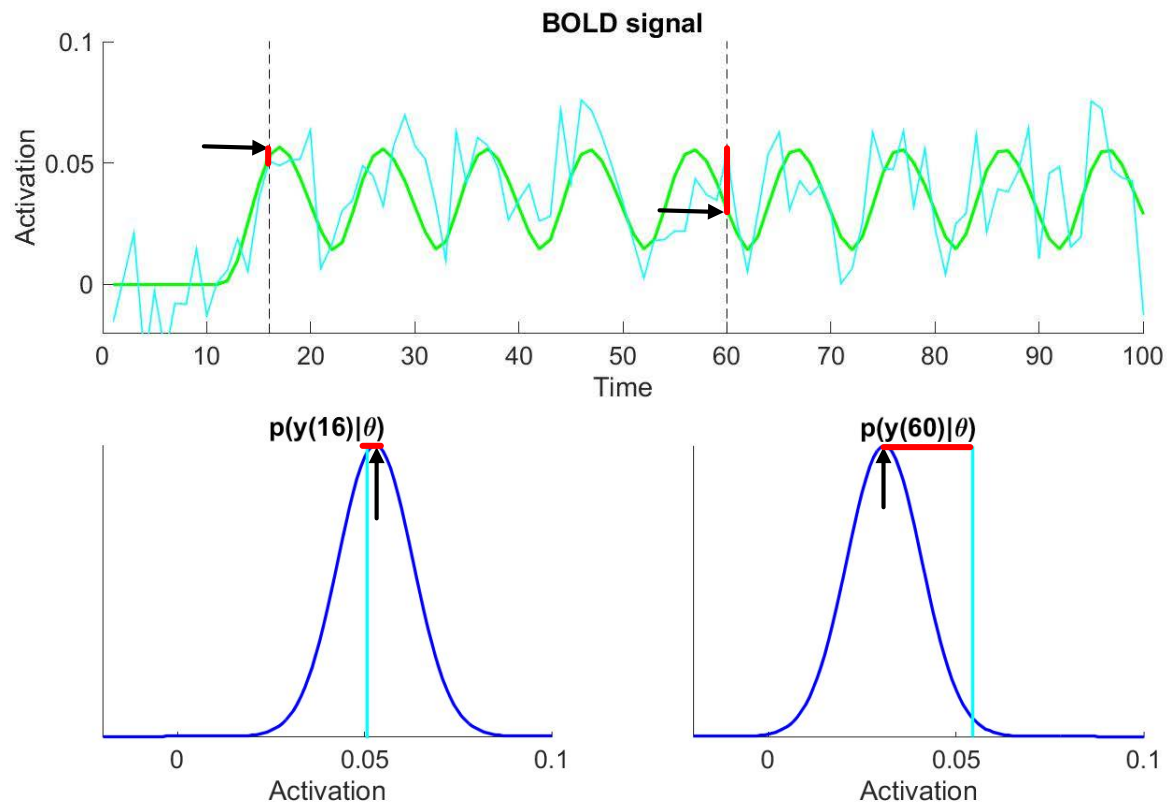
likelihood

Assume data is normally distributed around the prediction from the dynamical model (Gaussian noise)

The likelihood function for DCM

$$p(y(t)|\theta, m) = \mathcal{N}(y(t); g(\theta^n, \theta^h, u), \theta^\sigma)$$

likelihood



Priors

$$p(\theta|y, m) = \frac{p(y|\theta, m) \overset{\text{prior}}{p(\theta|m)}}{p(y|m)}$$

Neuronal parameters:

- self-connections: principled (to ensure that the system is stable)
- other parameters (between—region connections, modulation, inputs): shrinkage priors

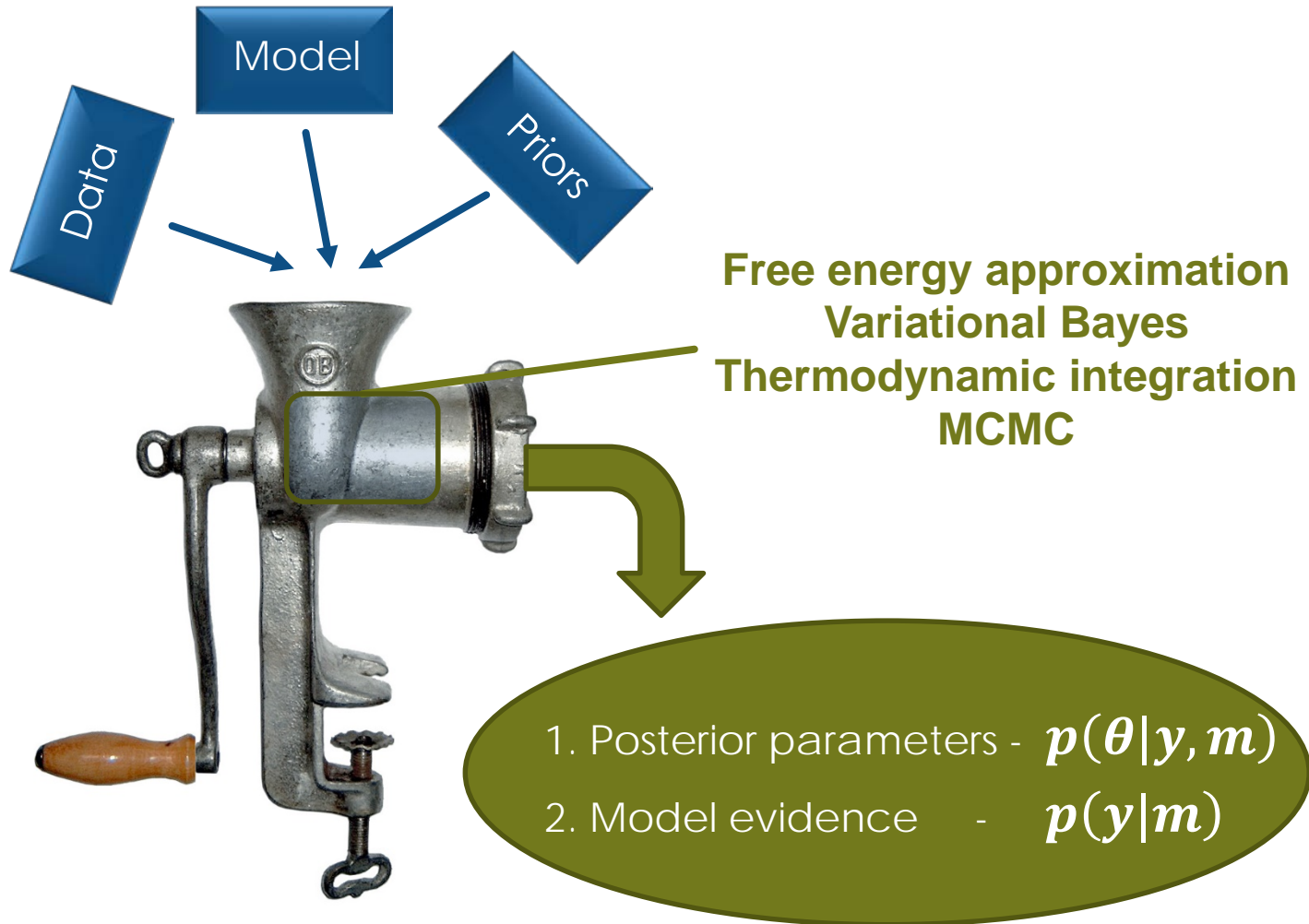
Hemodynamic parameters:

- empirical

Noise prior:

- assume relatively noisy data

Model estimation: running the machinery

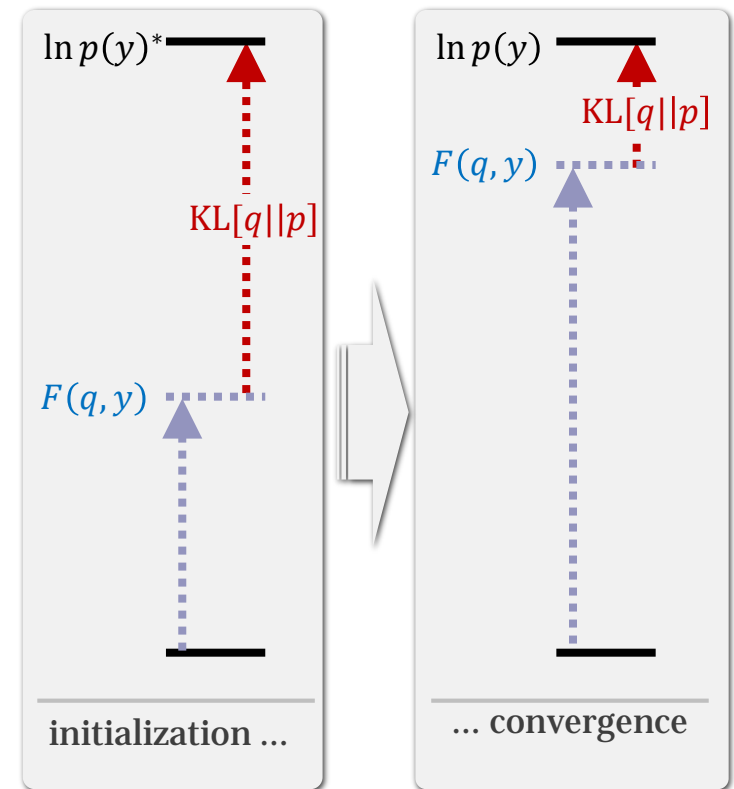


Inversion – variational Free Energy approximation to model evidence

model evidence

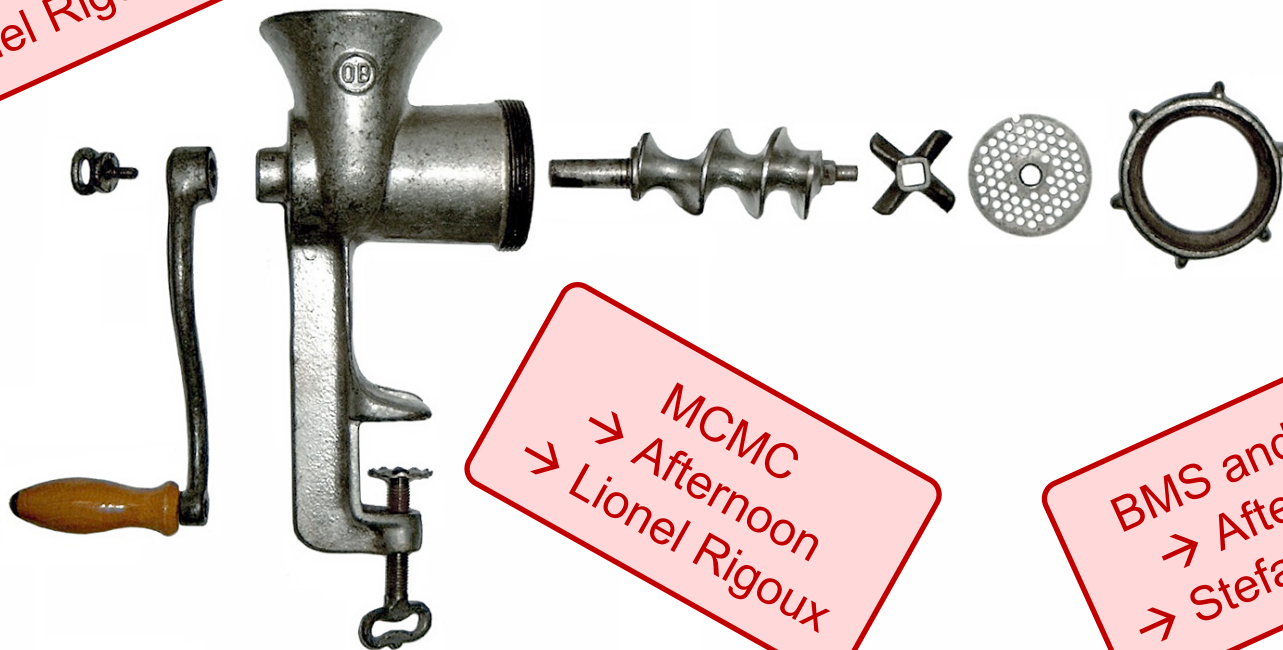
$$\ln p(y) = \underbrace{\text{KL}[q||p]}_{\substack{\text{divergence} \\ \geq 0 \\ \text{(unknown)}}} + \underbrace{F(q, y)}_{\substack{\text{neg. free energy} \\ \text{(easy to evaluate} \\ \text{for a given } q)}}$$

When $F(q, y)$ is maximized,
 $q(\theta)$ is our best estimate of
the true posterior.



Model estimation: running the machinery

Variational Bayes
→ Afternoon
→ Lionel Rigoux

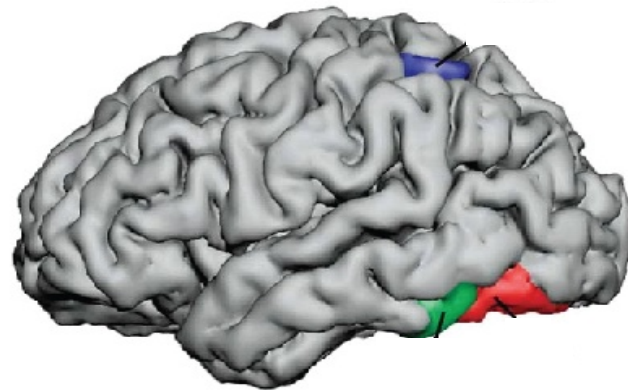


MCMC
→ Afternoon
→ Lionel Rigoux

BMS and BMA
→ Afternoon
→ Stefan Frässle

Example: Model Selection

- Specific sensory stimuli lead to unusual, additional experiences
- Grapheme-color synesthesia: **color**
- Involuntary, automatic; stable over time, prevalence ~4%
- Potential cause: aberrant **cross-activation/coupling** between brain areas
 - grapheme encoding area (FGA)
 - color area V4
 - superior parietal lobule (SPL)

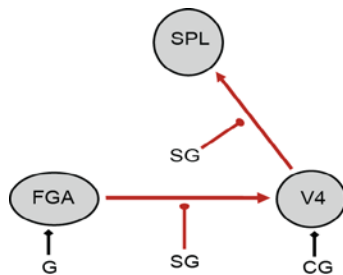


Hubbard, 2007

Bottom-up or Top-down “cross-activation”?

Bottom-up

(Ramachandran & Hubbard, 2001)

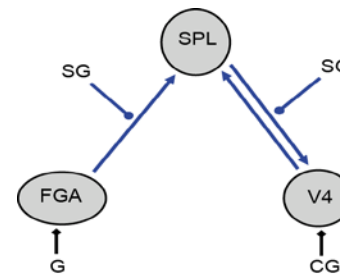


Projectors

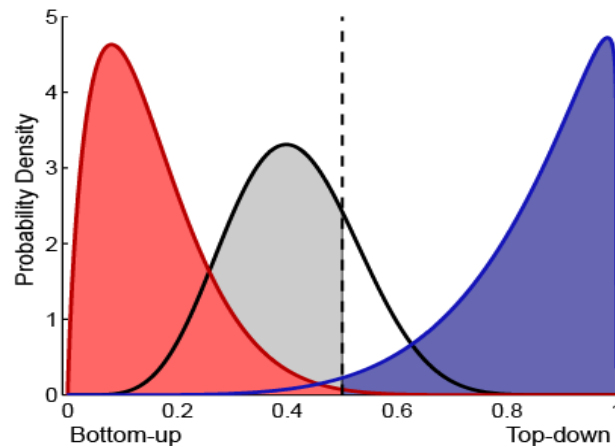
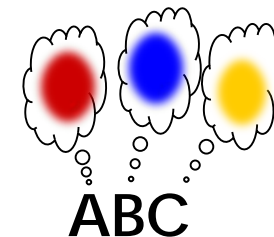
ABC

Top-down

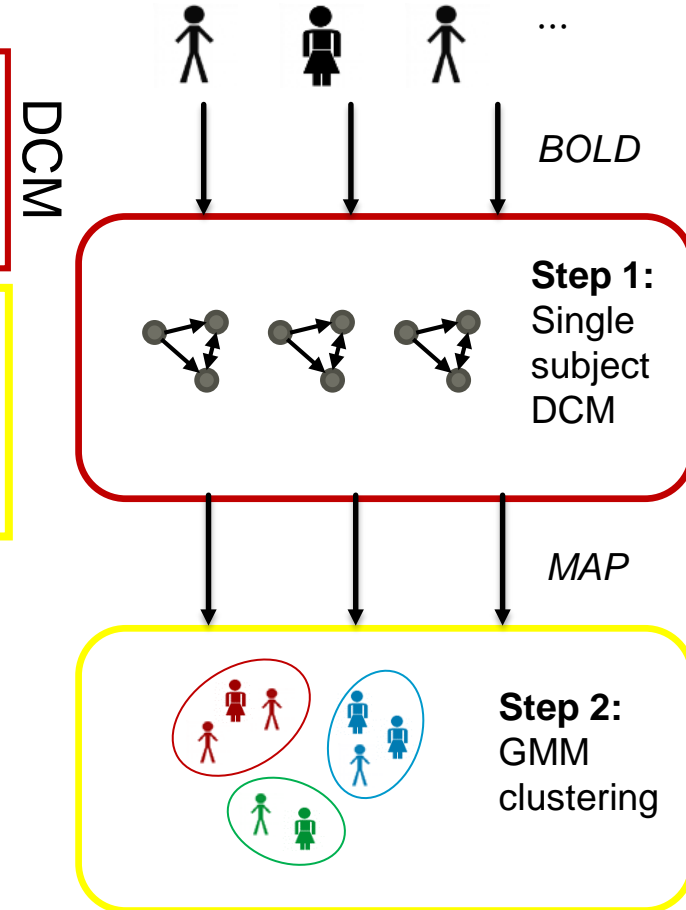
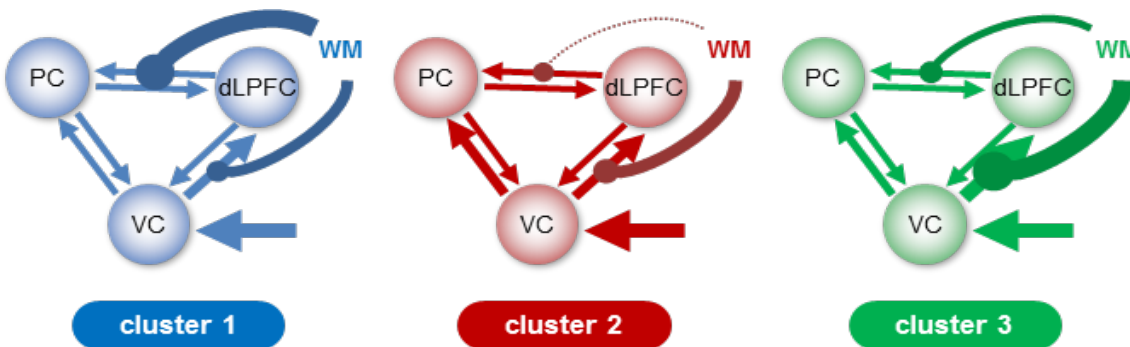
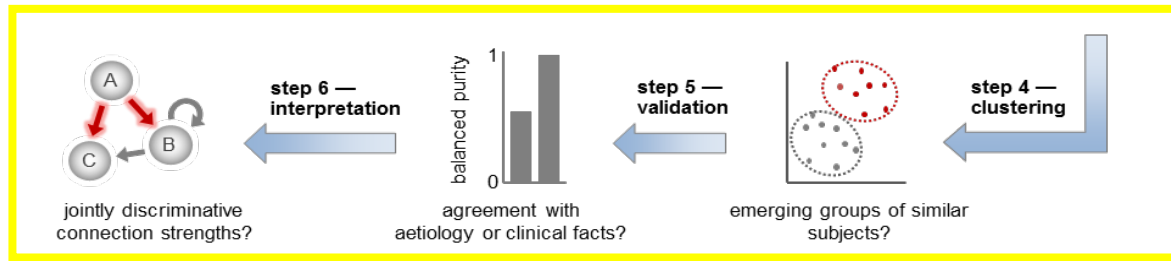
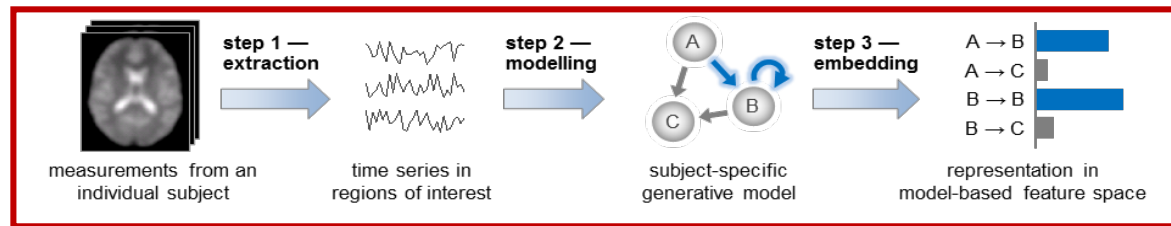
(Grossenbacher & Lovelace, 2001)



Associators



Example: DCM for physiologically plausible feature extraction



What questions can we answer using DCM?

Model comparison

What is the functional architecture of a network of brain regions?

→ Synesthesia

Are optimal models different between groups?

→ Synesthesia

Which connections are modulated by experimental manipulations?

Parameter inference

Are parameters different between individuals/groups?

Use parameters as physiologically informed summary statistics

→ Generative embedding

... and of course many more!

DCM software note

Basic functionality for DCM for fMRI is provided within

SPM

<https://www.fil.ion.ucl.ac.uk/spm/>

Limitations

- Local minima:
 - Variational approximation can get stuck in local minima of free energy

- Size of networks:
 - Standard inversion gets prohibitively slow for large networks (more than 10 nodes).

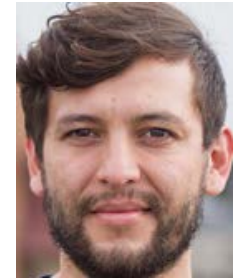
- Regularization through fixed priors:
 - Current regularization depends on priors only. Regularization based on group (all subjects) would be better → empirical Bayes.

Recent additions to DCM for fMRI

- Massively parallel dynamic causal modelling

➤ **mpdcm**

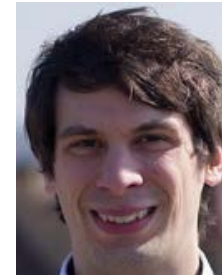
Eduardo Aponte



- Regression dynamic causal modelling

➤ **rDCM**

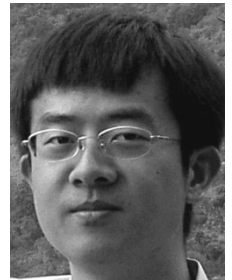
Stefan Frässle



- Hierarchical unsupervised generative embedding

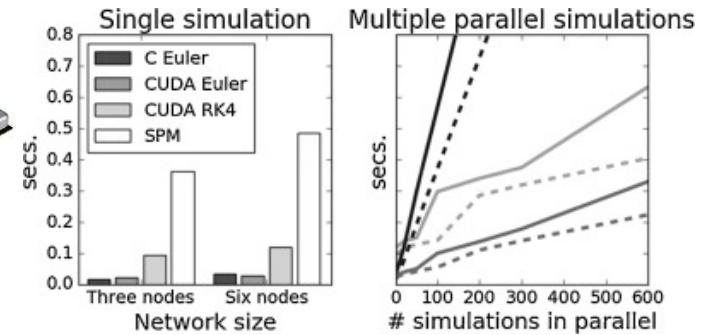
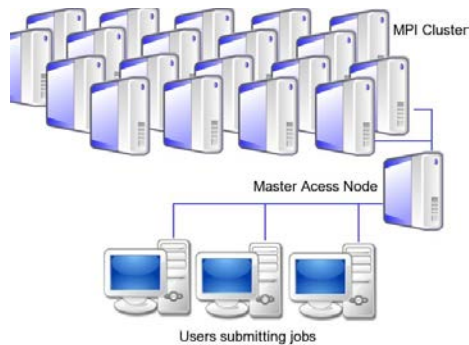
➤ **HUGE**

Yu Yao

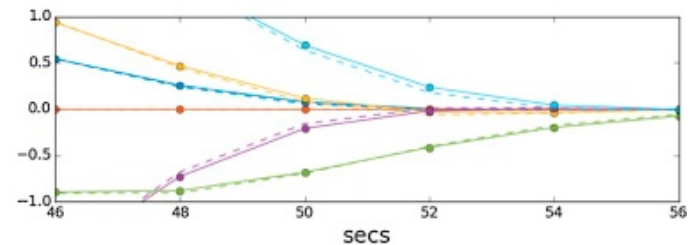


Available in TAPAS:
www.translationalneuromodeling.org/tapas

Massively parallel DCM - mpdcm



$$\left. \begin{array}{l} \dot{x} = f(x, u_1, \theta_1) \\ \dot{x} = f(x, u_2, \theta_2) \\ \vdots \\ \dot{x} = f(x, u_1, \theta_1) \end{array} \right\} \text{mpdcm_integrate(dcms)} \left\{ \begin{array}{l} y_1 \\ y_2 \\ \vdots \\ y_3 \end{array} \right.$$



- Fast inversion of DCMs
- MCMC based inversion possible
- **Thermodynamic Integration** (alternative to Free Energy)

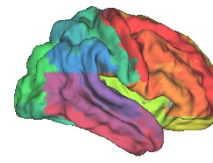


Regression DCM - rDCM

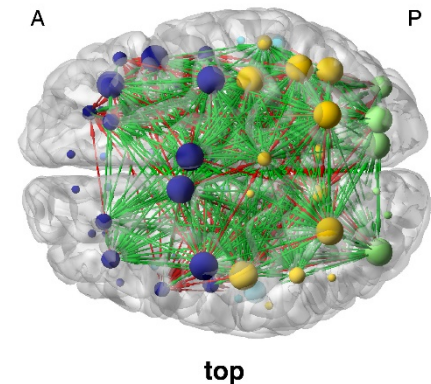
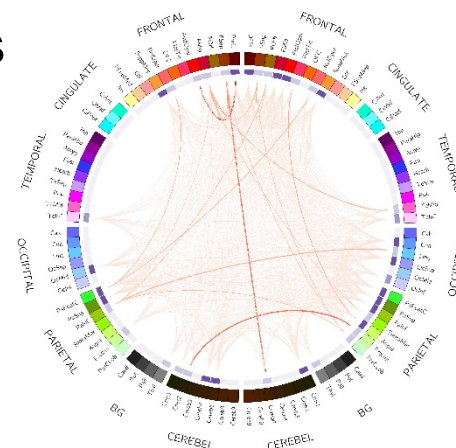
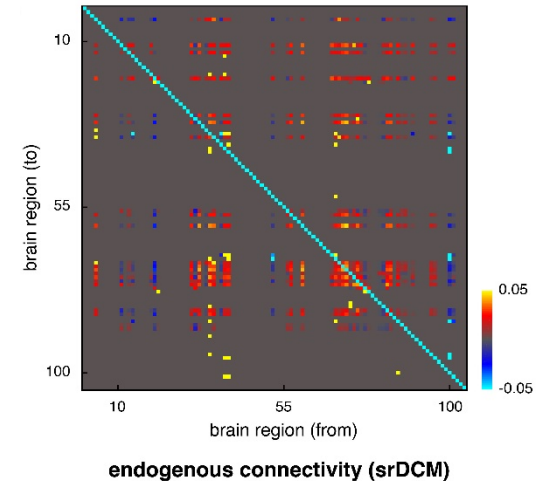
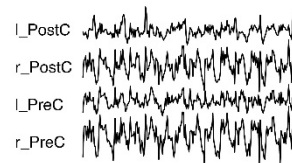
- Extremely efficient model inversion
- Graceful scaling to large networks
- Network pruning as part of model inversion (sparsity constraints)
- **Inference of whole-brain connectogram (~100 nodes and 10000 connections)**



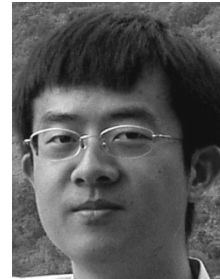
AAL parcellation



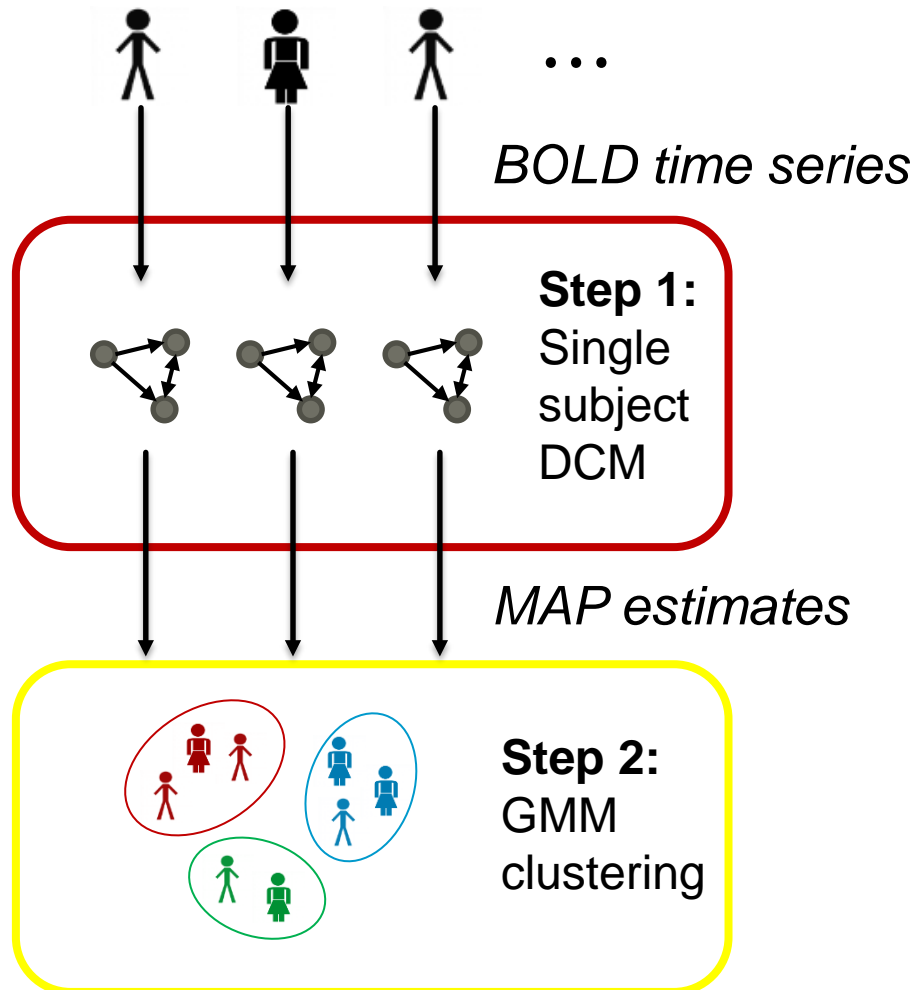
BOLD signal time series



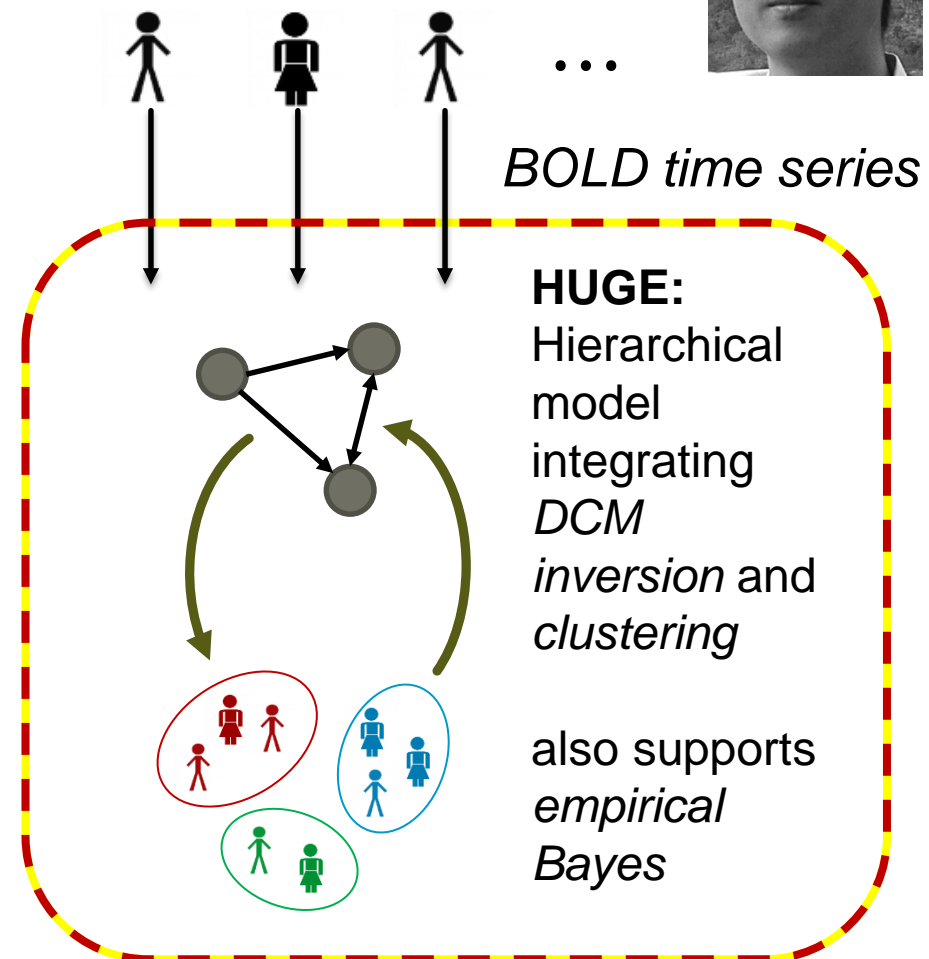
Hierarchical Unsupervised Generative Embedding (HUGE)



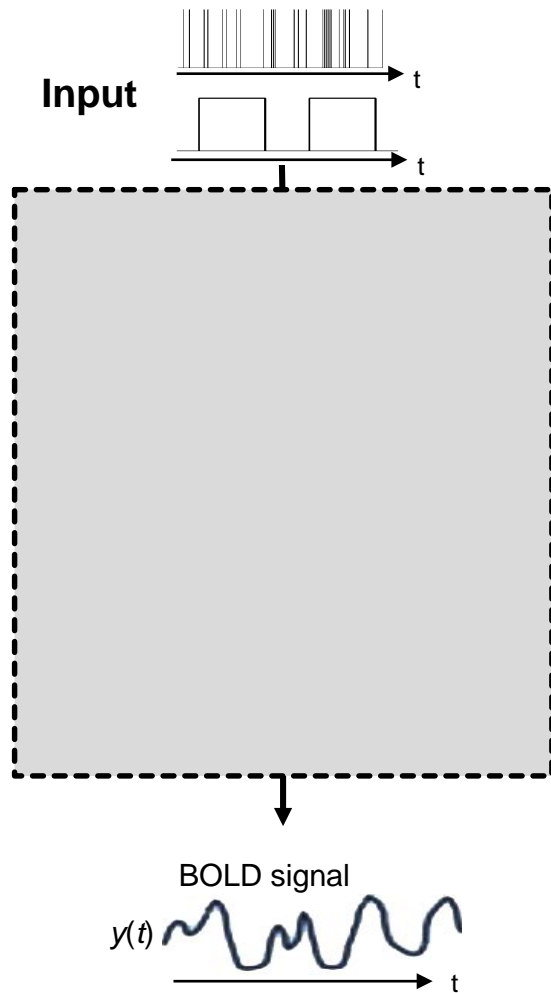
Generative Embedding



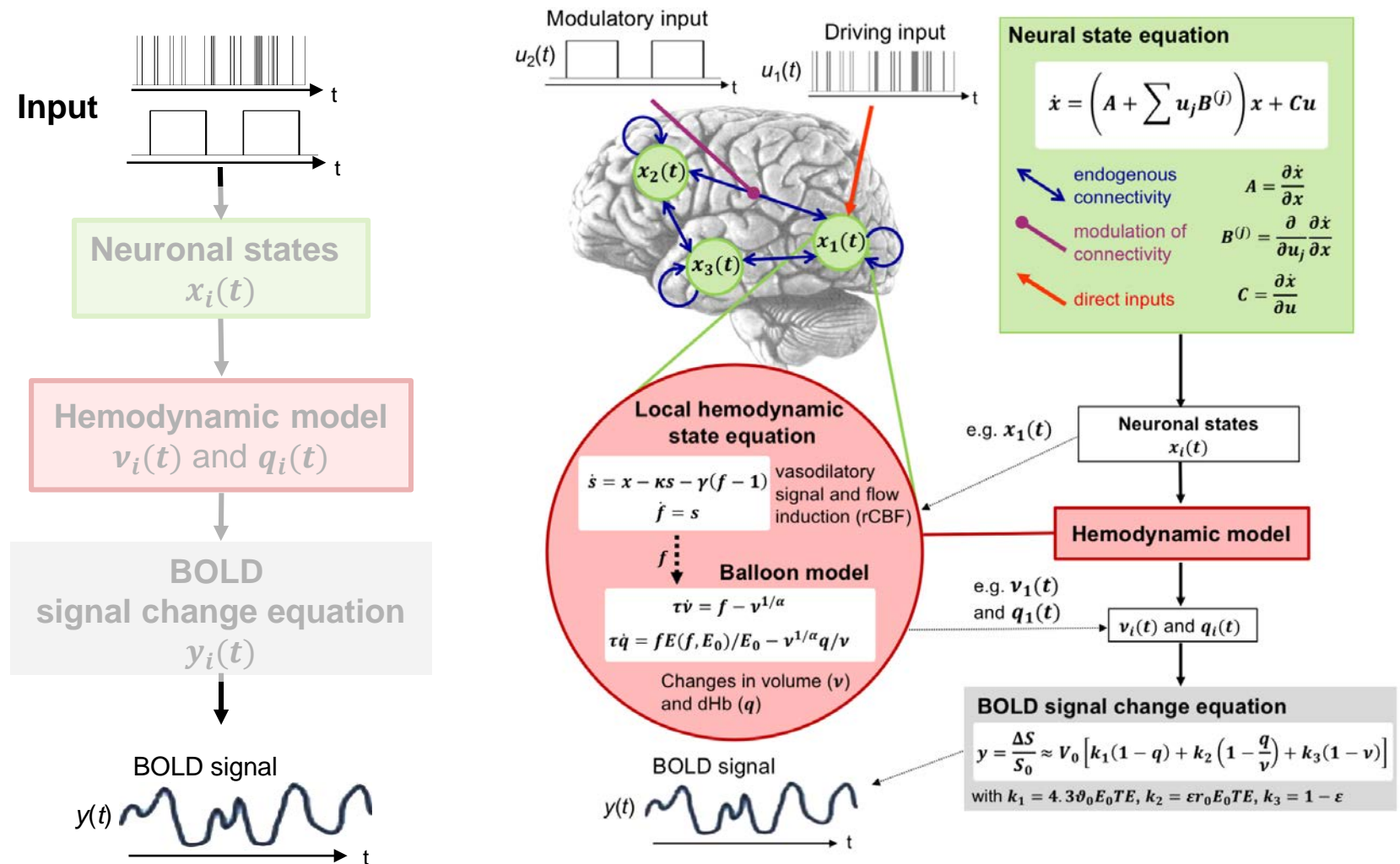
HUGE



Summary – Generative model



Summary – Generative Model



Summary - Bayesian System Identification

Neural (and hemo-)
dynamics

Observer function

$u(t)$



$$dx/dt = f(x, u, \theta)$$

$$y = g(x, \theta) + \varepsilon$$

$$p(y | \theta, m) = N(g(\theta), \Sigma(\theta))$$

$$p(\theta, m) = N(\mu_\theta, \Sigma_\theta)$$

Inference on
model structure

Inference on
parameters

$$p(y | m) = \int p(y | \theta, m) p(\theta) d\theta$$

$$p(\theta | y, m) = \frac{p(y | \theta, m) p(\theta, m)}{p(y | m)}$$

Design experimental inputs

Define likelihood model

Specify priors

Invert model

Make inferences



Thank you!

Many thanks to Stefan Frässle,
Klaas Enno Stephan, Hanneke den Ouden
and Jean Daunizeau for many of the slides!

List with suggested DCM literature in Appendix of this presentation!

DCM literature (1)

- **Aponte EA, Raman S, Sengupta B, Penny WD, Stephan KE, Heinzle J (2016). mpdcm: A Toolbox for Massively Parallel Dynamic Causal Modeling. Journal of Neuroscience Methods 257: 7-16.**
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- Daunizeau J, David, O, Stephan KE (2011) Dynamic Causal Modelling: A critical review of the biophysical and statistical foundations. Neurolmage 58: 312-322.
- Daunizeau J, Stephan KE, Friston KJ (2012) Stochastic Dynamic Causal Modelling of fMRI data: Should we care about neural noise? Neurolmage 62: 464-481.
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- Friston KJ, Mattout J, Trujill-Barreto, Ashburner J, Penny W (2007) Variational free energy and the Laplace approximation. Neurolmage 34: 220-234.
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- Friston KJ, Li B, Daunizeau J, Stephan KE (2011) Network discovery with DCM. Neurolmage 56: 1202–1221.
- Friston K, Penny W (2011) Post hoc Bayesian model selection. Neuroimage 56: 2089-2099.
- Friston KJ, Kahan J, Biswal B, Razi A (2014) A DCM for resting state fMRI. Neuroimage 94:396-407.
- Frässle S, Yao Y, Schöbi S, Aponte EA, Heinzle J, Stephan KE (in press) Generative models for clinical applications in computational psychiatry. Wiley Interdisciplinary Reviews: Cognitive Science.
- **Frässle S, Lomakina EI, Razi A, Friston KJ, Buhmann JM, Stephan KE (2017) Regression DCM for fMRI. Neurolmage 155:406-421.**

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- Li B, Daunizeau J, Stephan KE, Penny WD, Friston KJ (2011). Stochastic DCM and generalised filtering. *NeuroImage* 58: 442-457
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- Penny WD, Stephan KE, Mechelli A, Friston KJ (2004a) Comparing dynamic causal models. *NeuroImage* 22:1157-1172.
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- Penny WD, Stephan KE, Daunizeau J, Joao M, Friston K, Schofield T, Leff AP (2010) Comparing Families of Dynamic Causal Models. *PLoS Computational Biology* 6: e1000709.
- Penny WD (2012) Comparing dynamic causal models using AIC, BIC and free energy. *Neuroimage* 59: 319-330
- **Raman S, Deserno L, Schlagenhauf F, Stephan KE (2016). A hierarchical model for integrating unsupervised generative embedding and empirical Bayes. *Journal of Neuroscience Methods* 269: 6-20.**
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- Stephan KE, Harrison LM, Penny WD, Friston KJ (2004) Biophysical models of fMRI responses. *Curr Opin Neurobiol* 14:629-635.
- Stephan KE, Weiskopf N, Drysdale PM, Robinson PA, Friston KJ (2007) Comparing hemodynamic models with DCM. *NeuroImage* 38:387-401.
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- Stephan KE, Weiskopf N, Drysdale PM, Robinson PA, Friston KJ (2007) Comparing hemodynamic models with DCM. *NeuroImage* 38:387-401.
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- Stephan KE, Mathys C (2014). Computational approaches to psychiatry. *Current Opinion in Neurobiology* 25: 85-92.
- **Yao Y, Raman SS, Schiek M, Leff A, Frässle S, Stephan KE (2018). Variational Bayesian Inversion for Hierarchical Unsupervised Generative Embedding (HUGE). *NeuroImage*, 179: 604-619**