

Michael Breakspear

@drbreaky



I respectfully acknowledge the Awabakal people, the traditional custodians of the land on which we live and work in Newcastle



Modelling large-scale neural activity in brain disorders

a human (Roland Goecke)

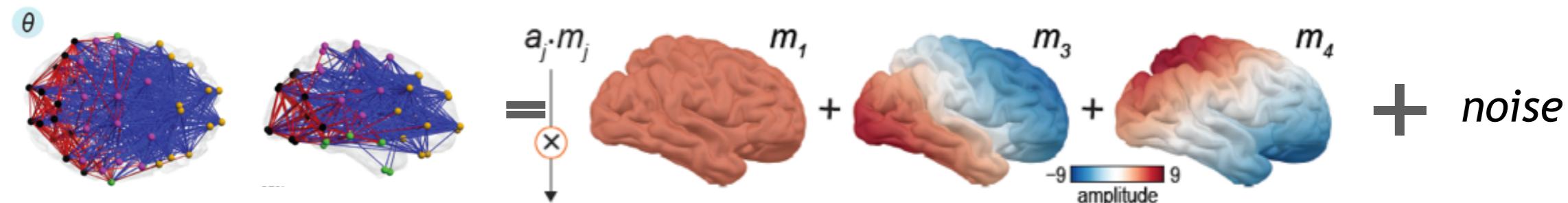


Humans are inherently dynamic machines, engaged in active action-perception with complex scenes and others

Positioned, embodied, metabolically hungry, social, ...

Modelling large-scale neural activity in brain disorders

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I: Population models : Basic principles

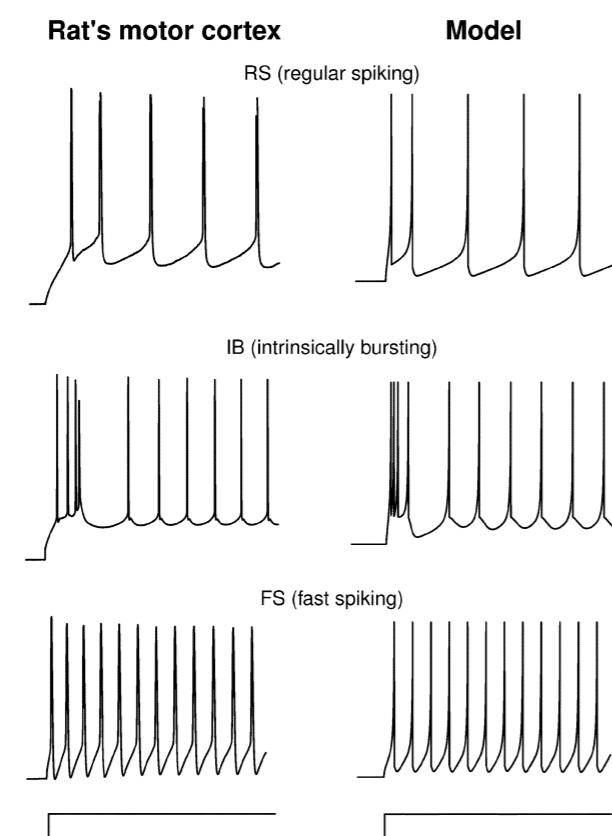
II: Nodes and neural masses

III: Neural fields + modes

IV: A few comments

I: Population models : Basic principles

The origin of spikes in single neurons was essentially solved by the Nobel-prize winning Hodgkin–Huxley model developed in the 1950s.



$$C \frac{dV}{dt} = g_{Na} m_\infty(V)(V - V_{Na}) + g_K n(V)(V - V_K) + g_L(V - V_L) + I,$$
$$\frac{dn}{dt} = \frac{n_\infty(V) - n}{\tau_n}.$$

where,

$$m_\infty(V) = \frac{m_{\max}}{1 + \exp[(V_m - V)/\sigma_m]},$$

$$n_\infty(V) = \frac{n_{\max}}{1 + \exp[(V_n - V)/\sigma_n]},$$

Drawing directly from detailed neurophysiological recordings of the squid giant axon, this model ascribes the origin of spikes to the interaction of fast depolarizing and slow hyperpolarizing currents, expressed in precise mathematical form

This (Nobel prize winning) success generated decades of spike-based theories of brain computation

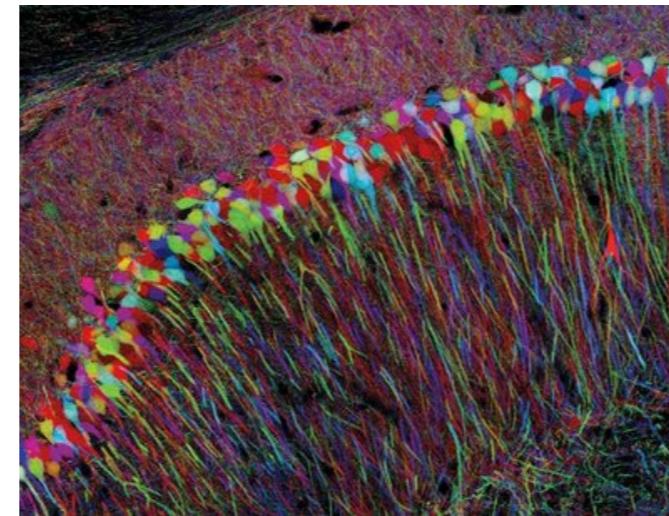
I: Population models : Basic principles

But individual neurons are buried within circuits of thousands of neurons which are themselves immersed in functional subsystems and large-scale brain networks

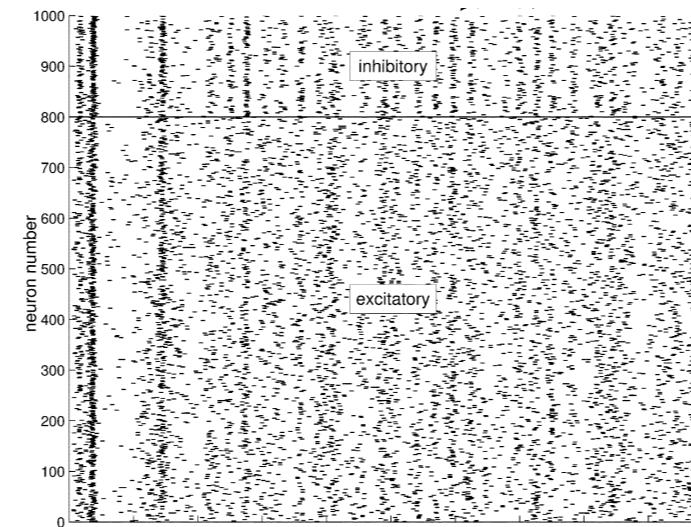


I: Population models : Basic principles

Local neural population



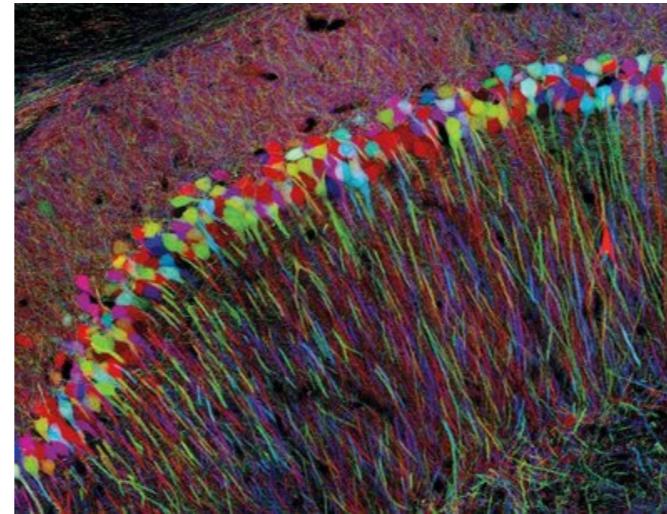
“Spike raster”
(individual states)



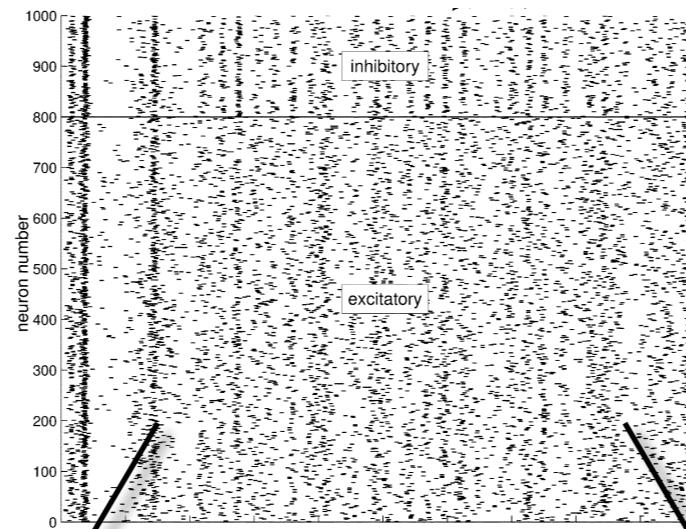
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I: Population models : Basic principles

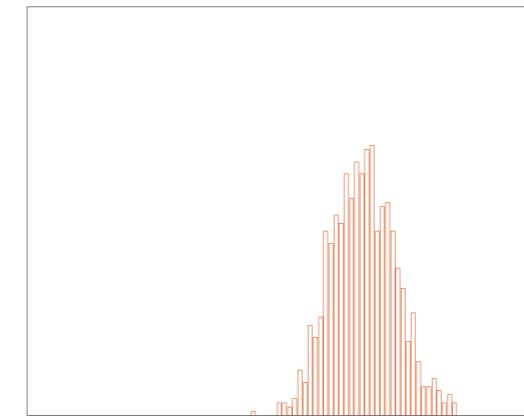
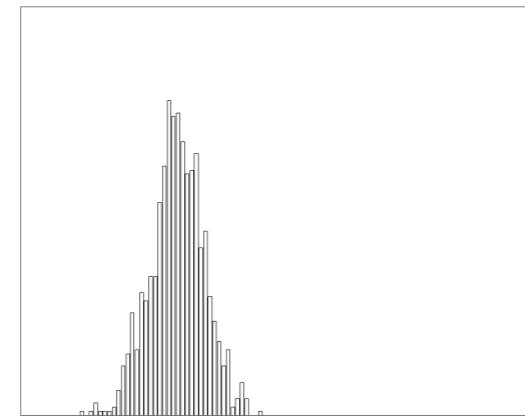
Local neural population



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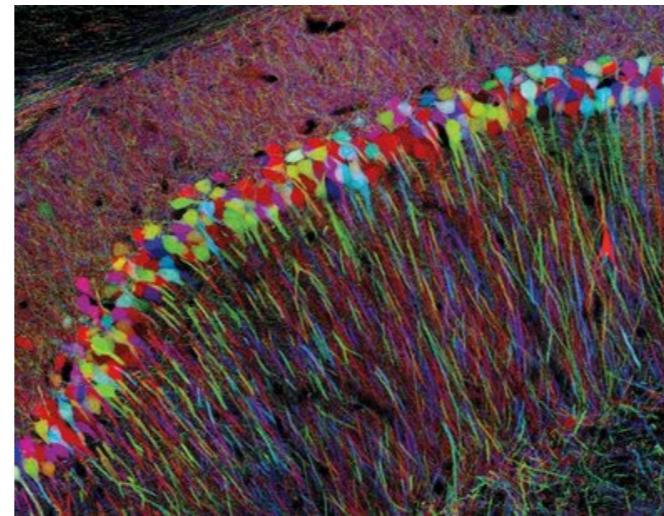
Empirical
histogram



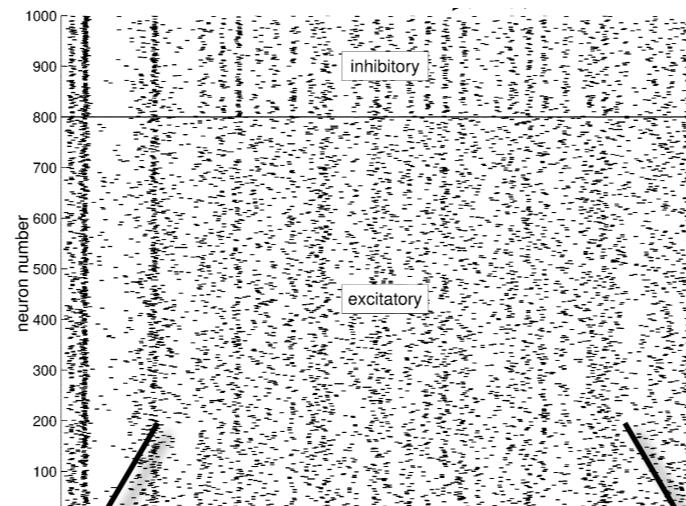
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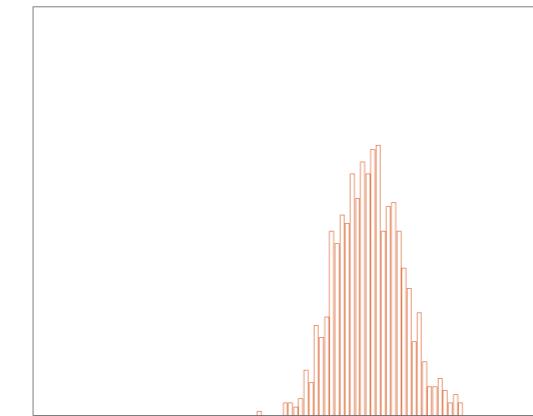
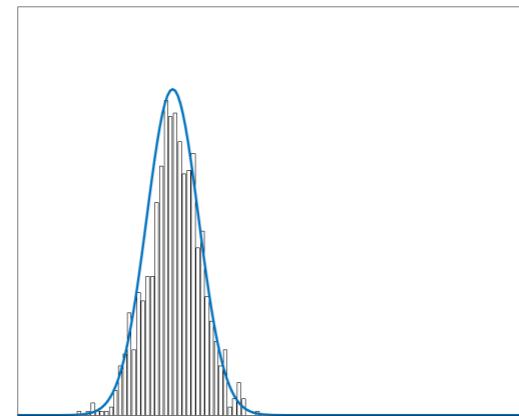
Local neural population



“Spike raster”
(individual states)



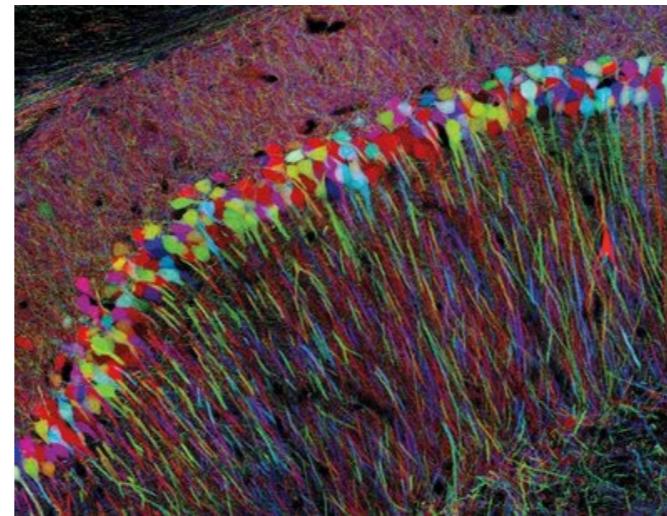
Mean field
approximation



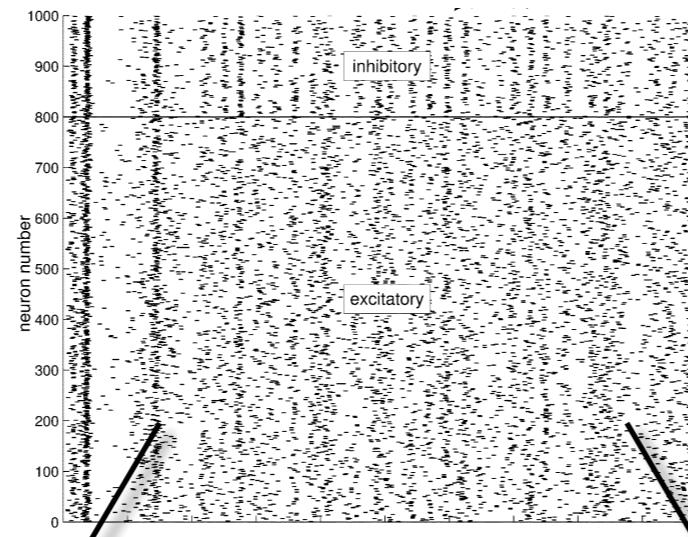
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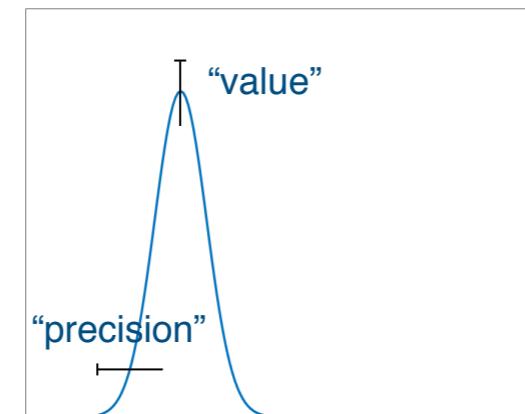
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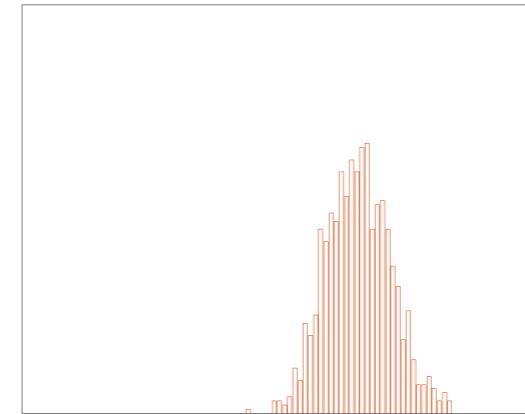
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Mean field
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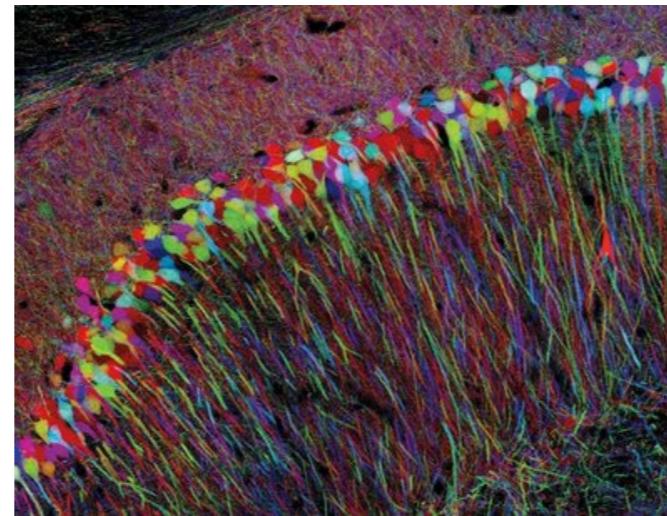


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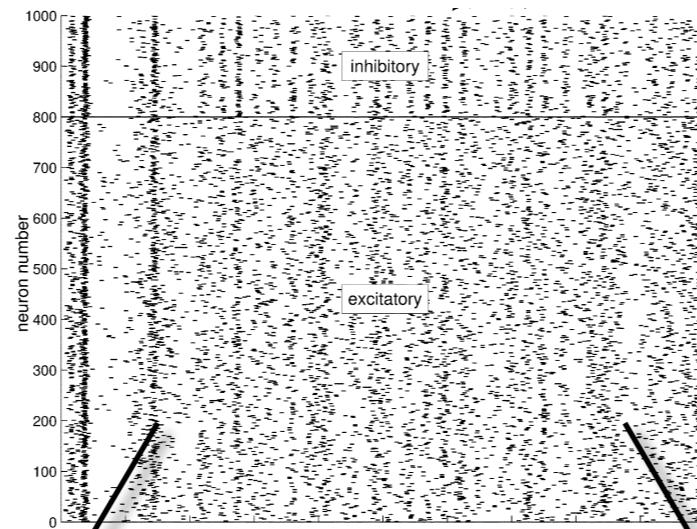


I: Population models : Basic principles

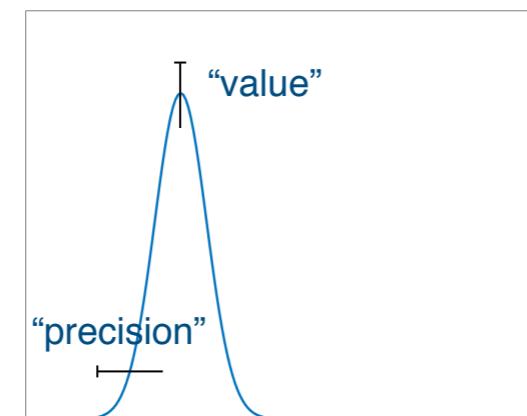
Local neural population



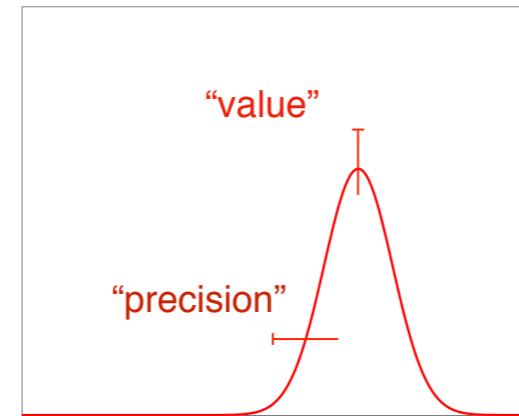
“Spike raster”
(individual states)



Mean field
approximation



$$\frac{\partial p}{\partial t} = D \frac{\partial^2 p}{\partial \theta^2} - \frac{\partial}{\partial \theta}(v p),$$

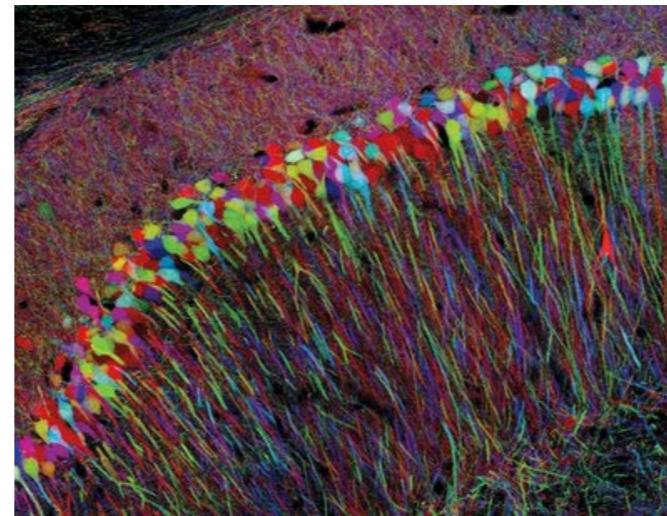


Forward temporal
evolution

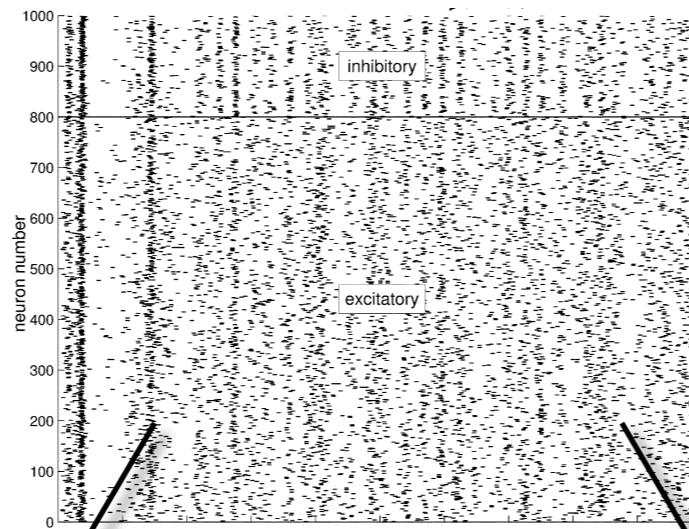
Same approach used widely in
physics - e.g. magnetism,
super-conductors, LCDs,
queueing, swarming

I: Population models : Basic principles

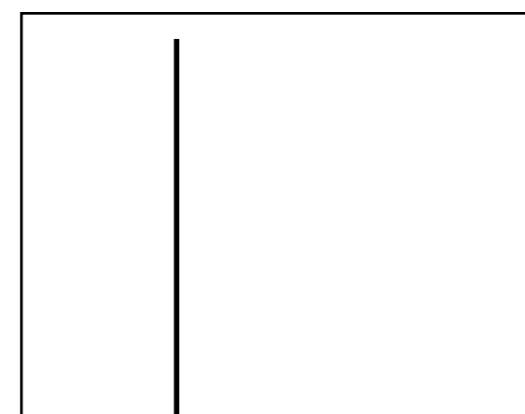
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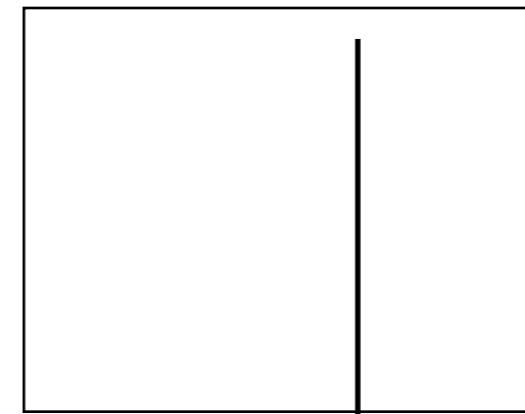
“Spike raster”
(individual states)



Neural mass
approximation



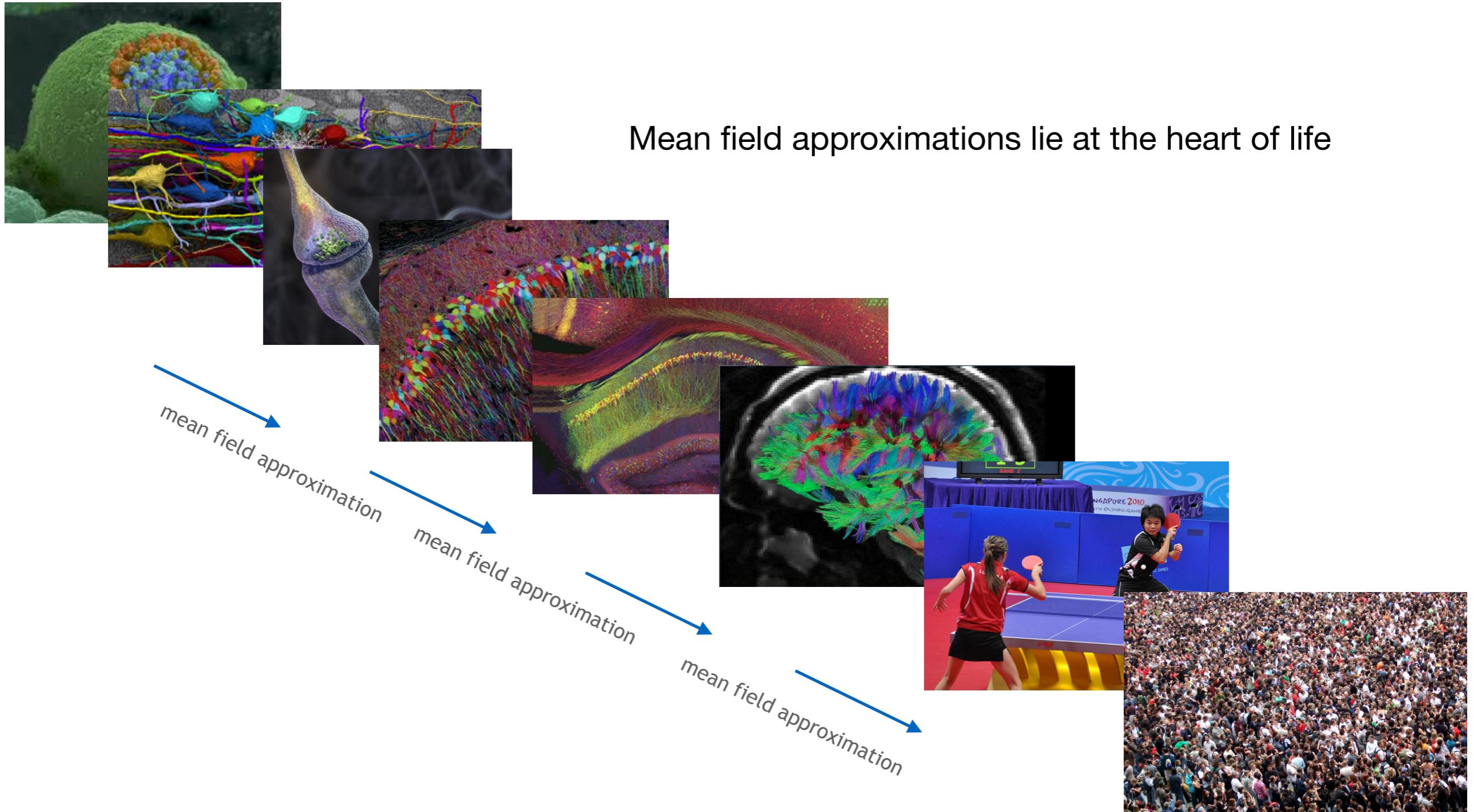
$$\frac{d\mathbf{X}}{dt} = f(\mathbf{X}) + I$$



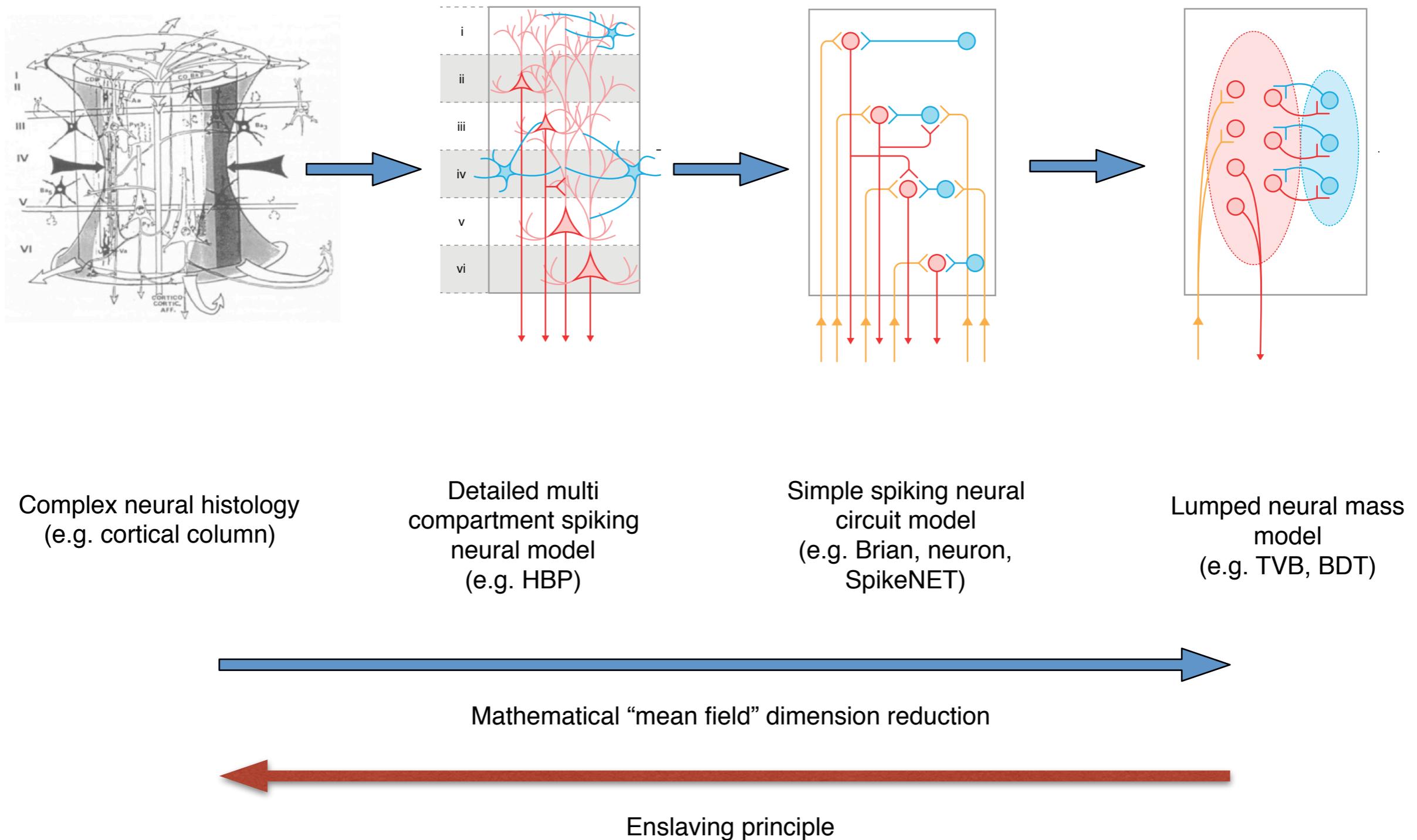
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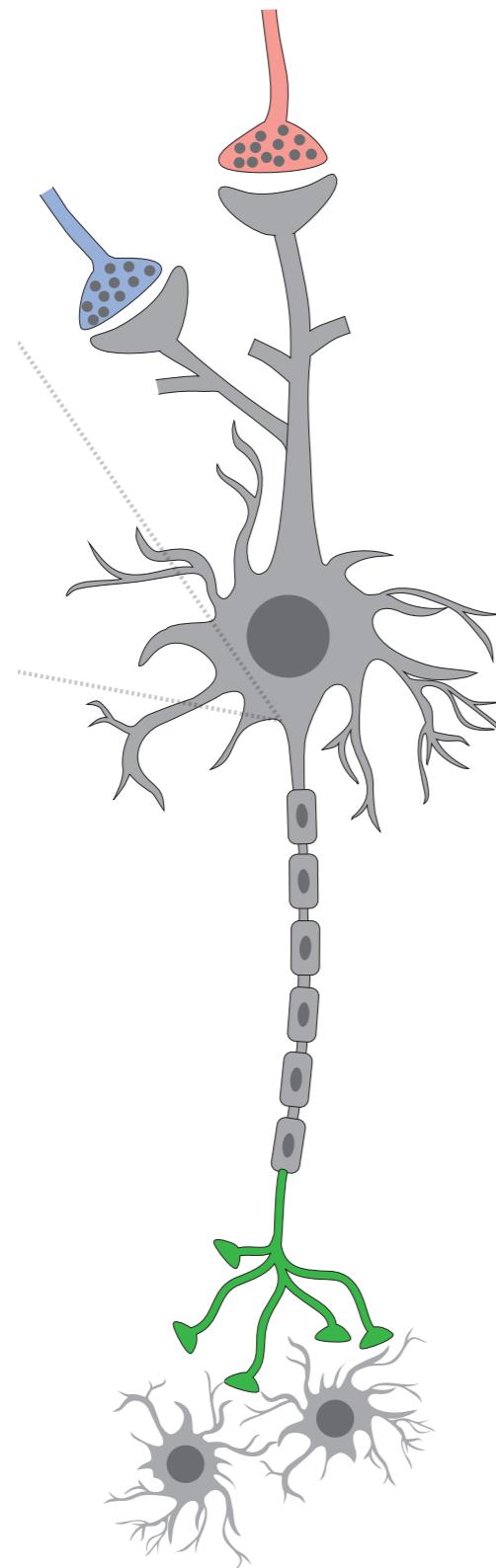
I: Population models : Basic principles



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Conductance based single neuron model

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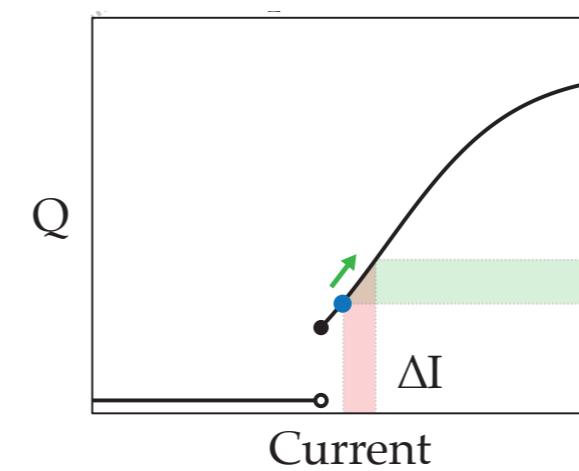
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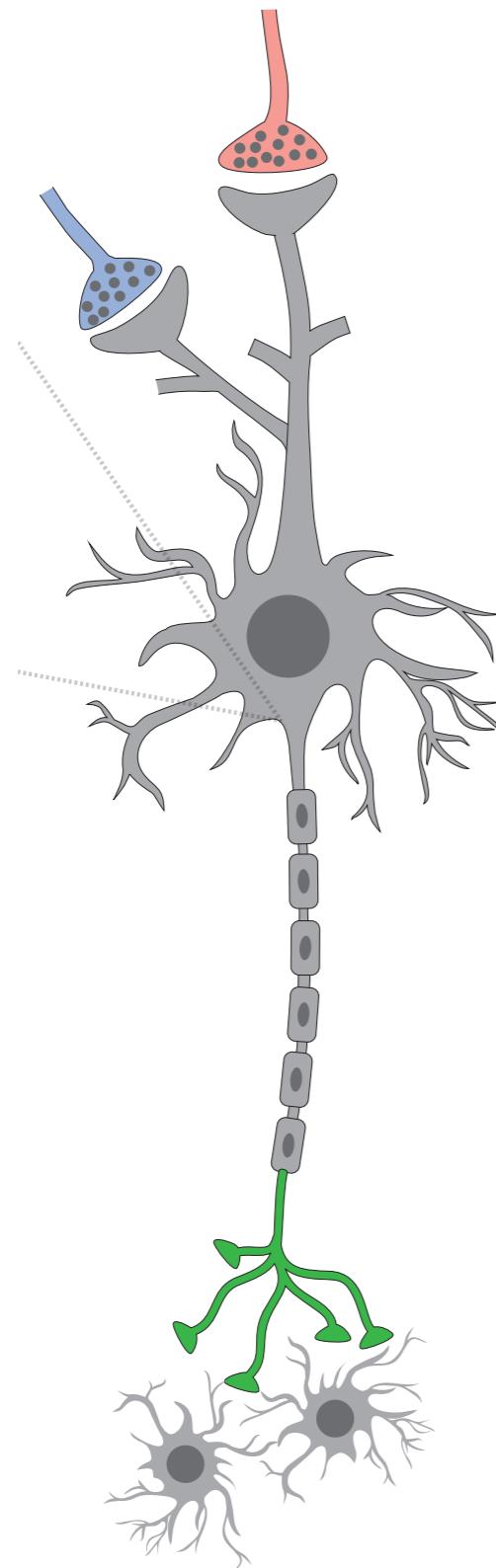
Bifurcation analysis of input current \leftrightarrow firing rate (Q)



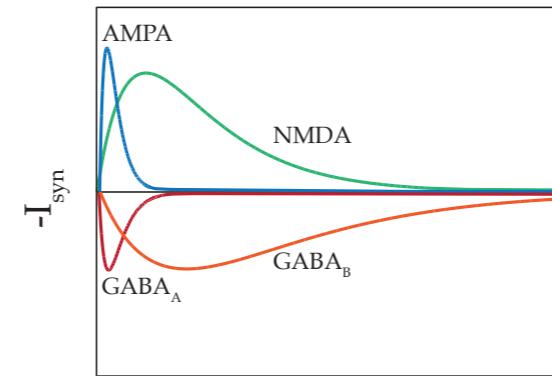
Mac Shine, Eli Muller



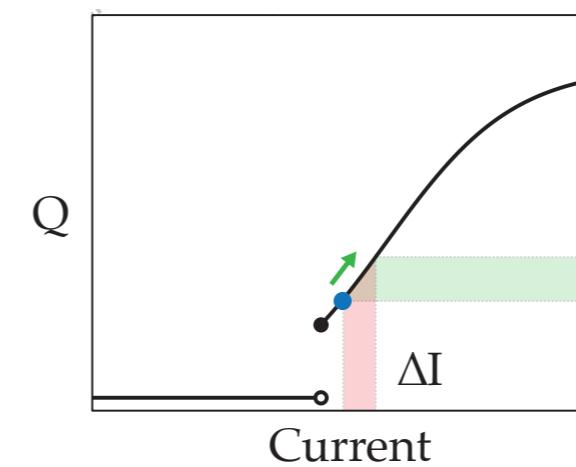
I: Population models : Basic principles



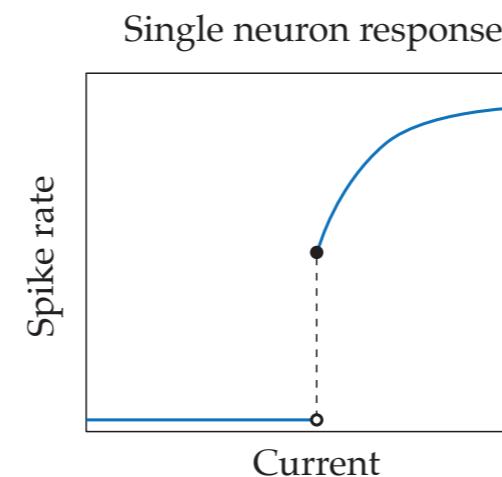
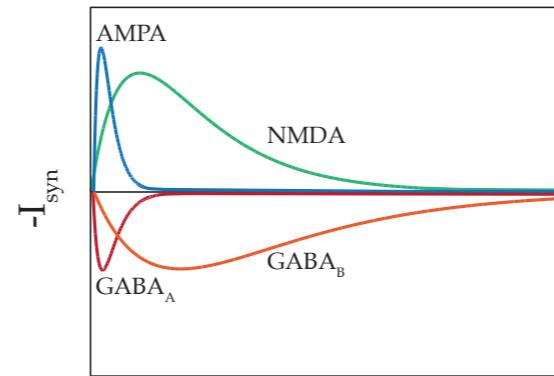
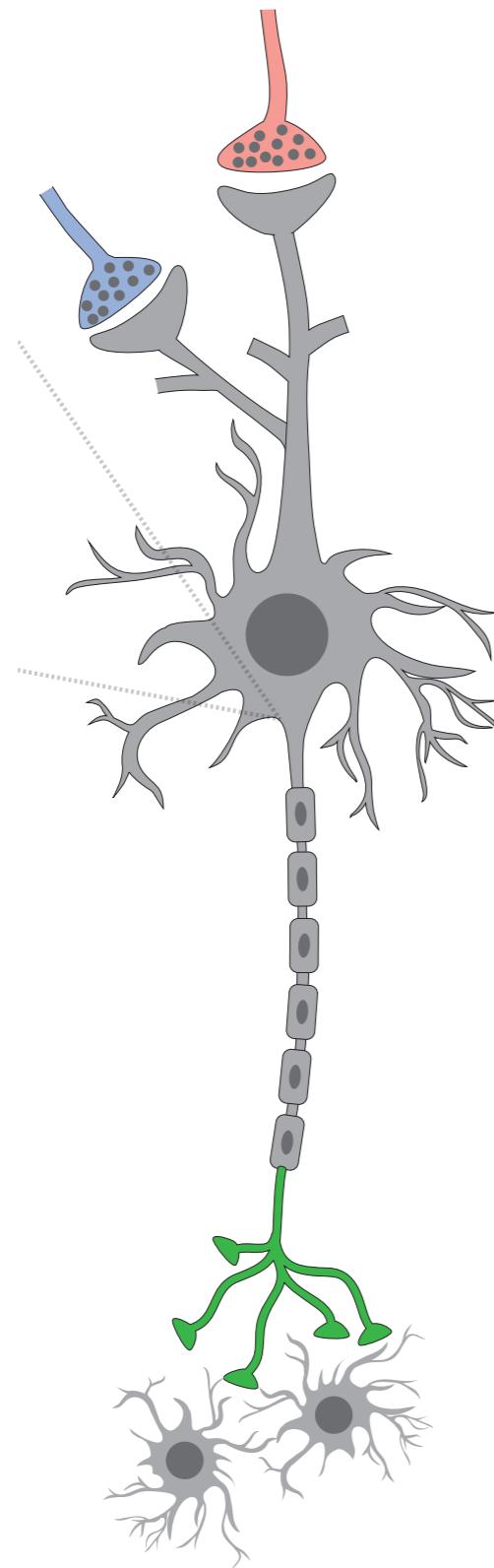
Add EPSP/IPSP input currents



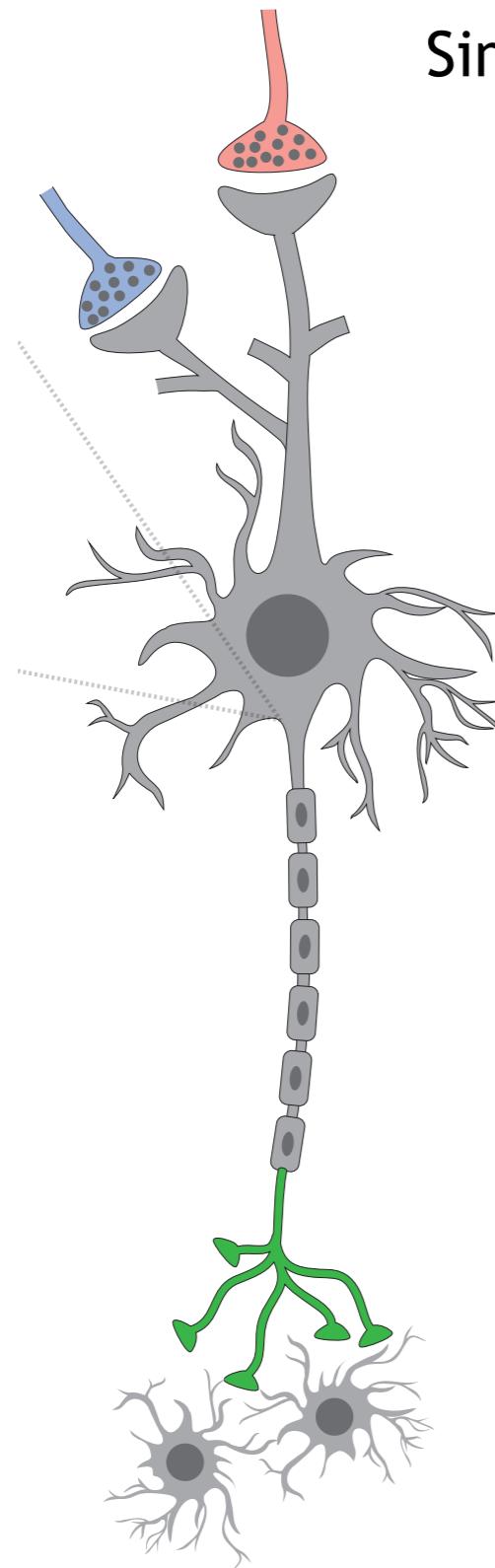
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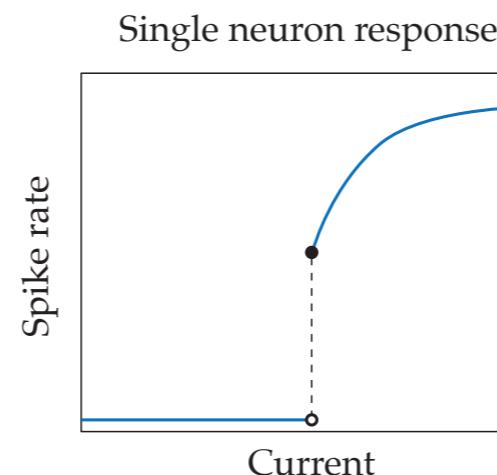
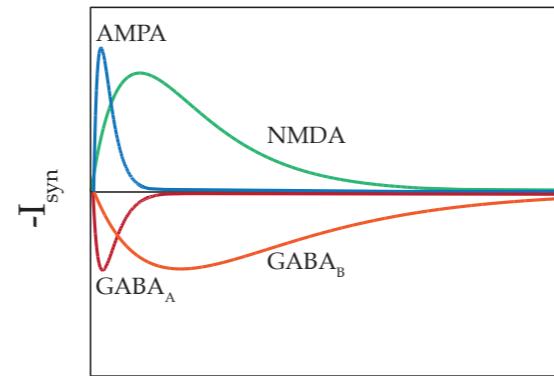
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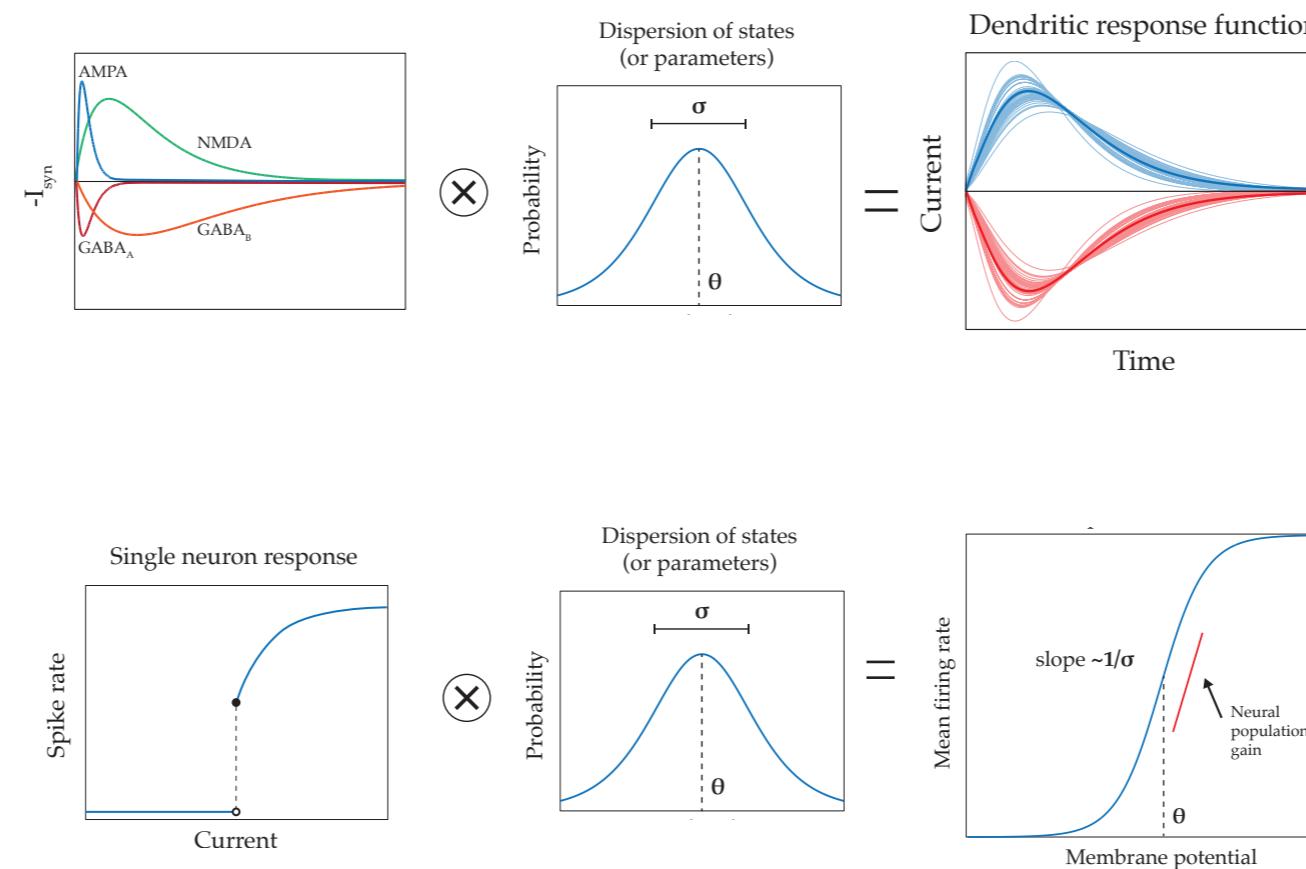
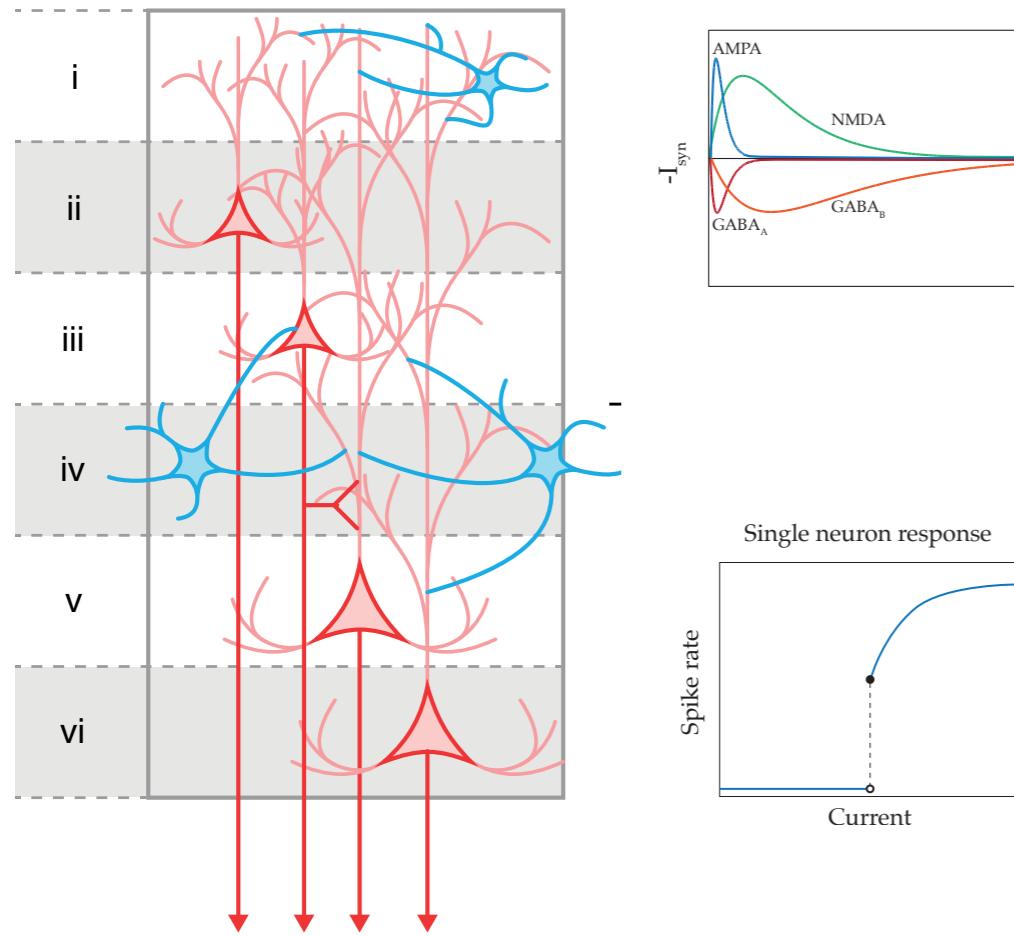


Simplified current-based single neuron model

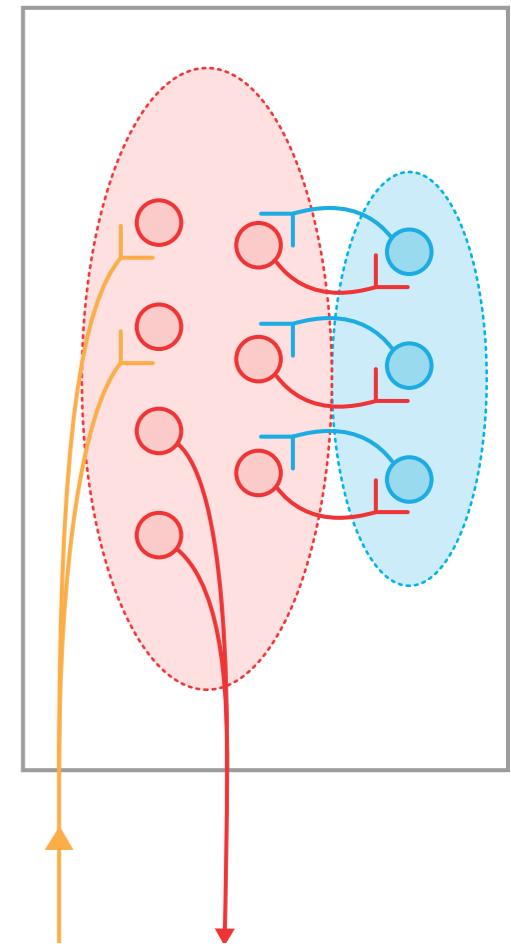


I: Population models : Basic principles

Simplified current-based single many-neuron model

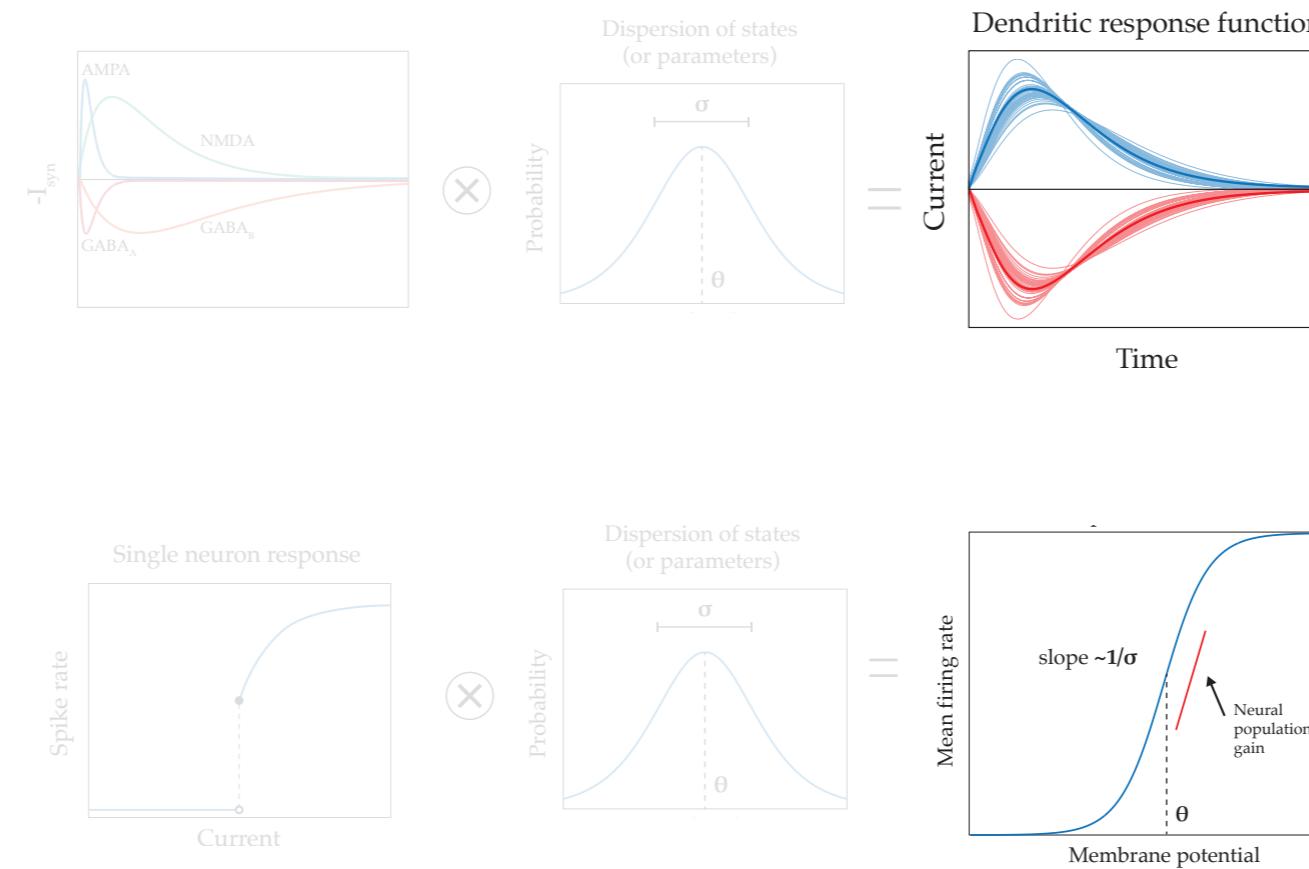
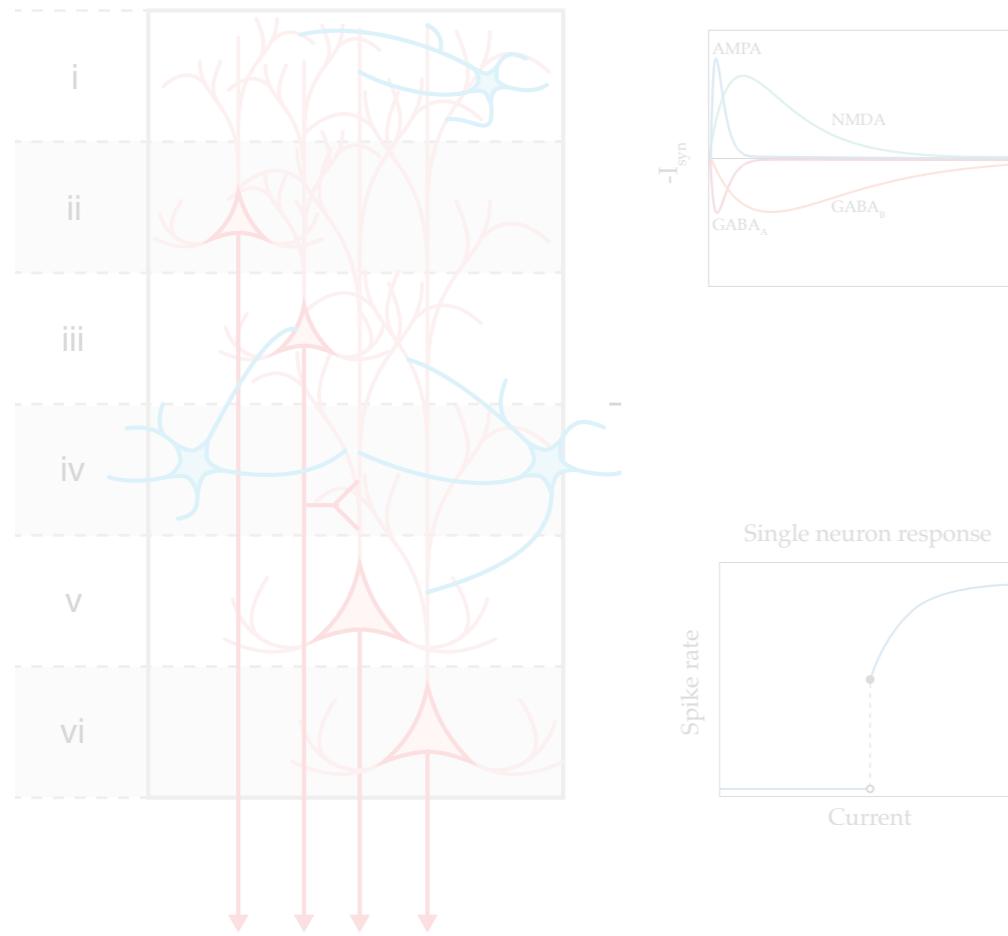


Neural mass model

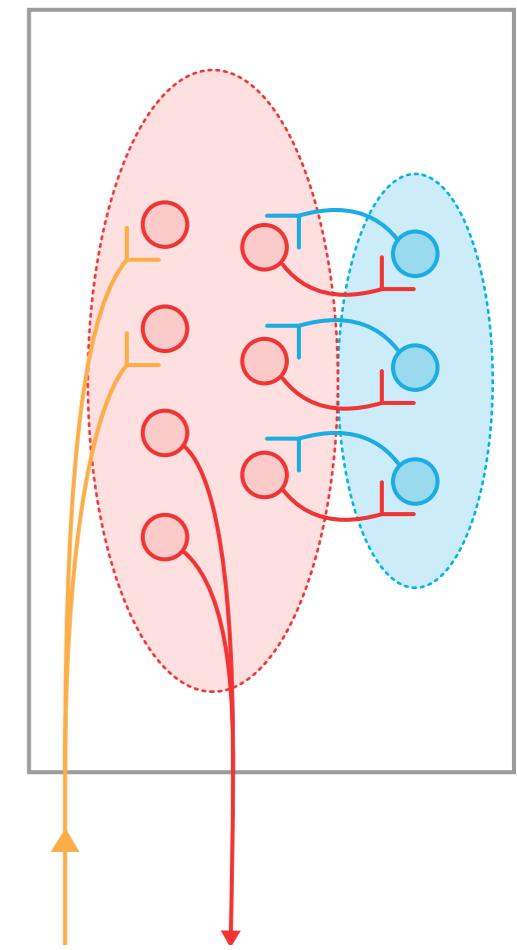


I: Population models : Basic principles

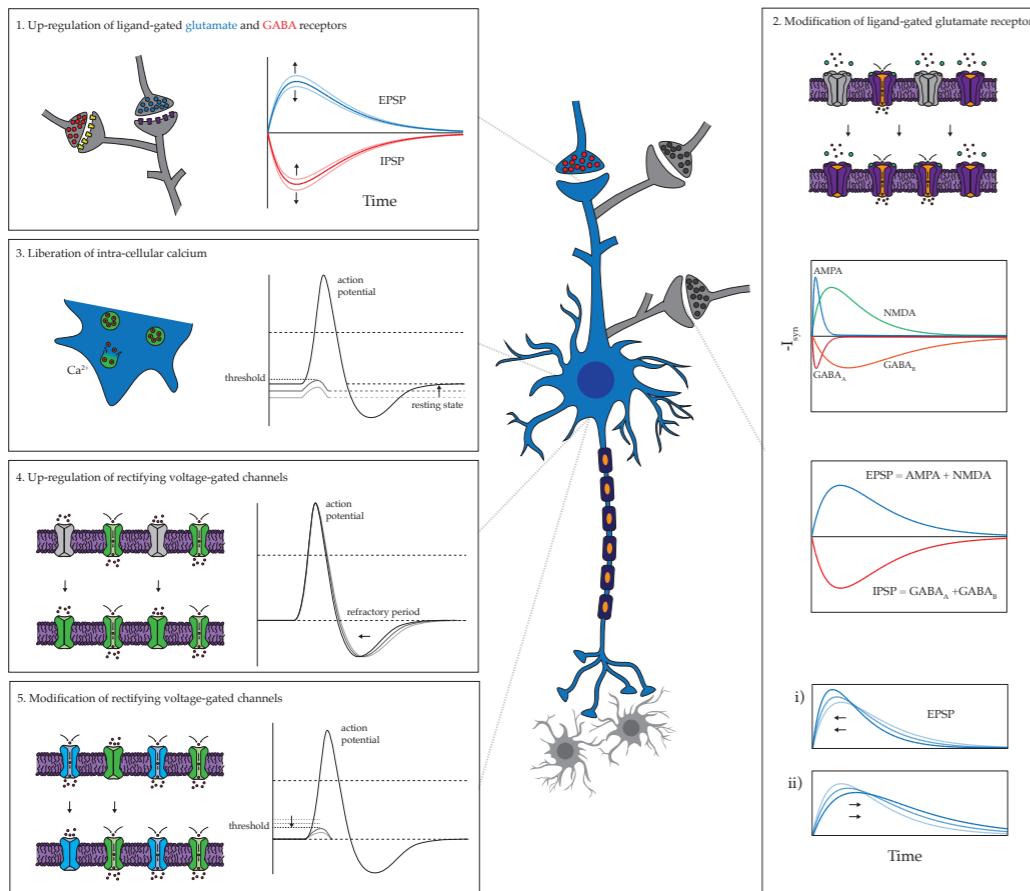
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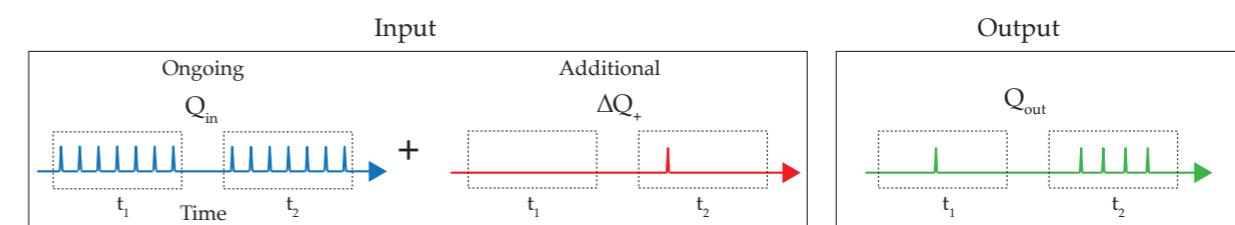
Neural mass model



I: Population models : Basic principles

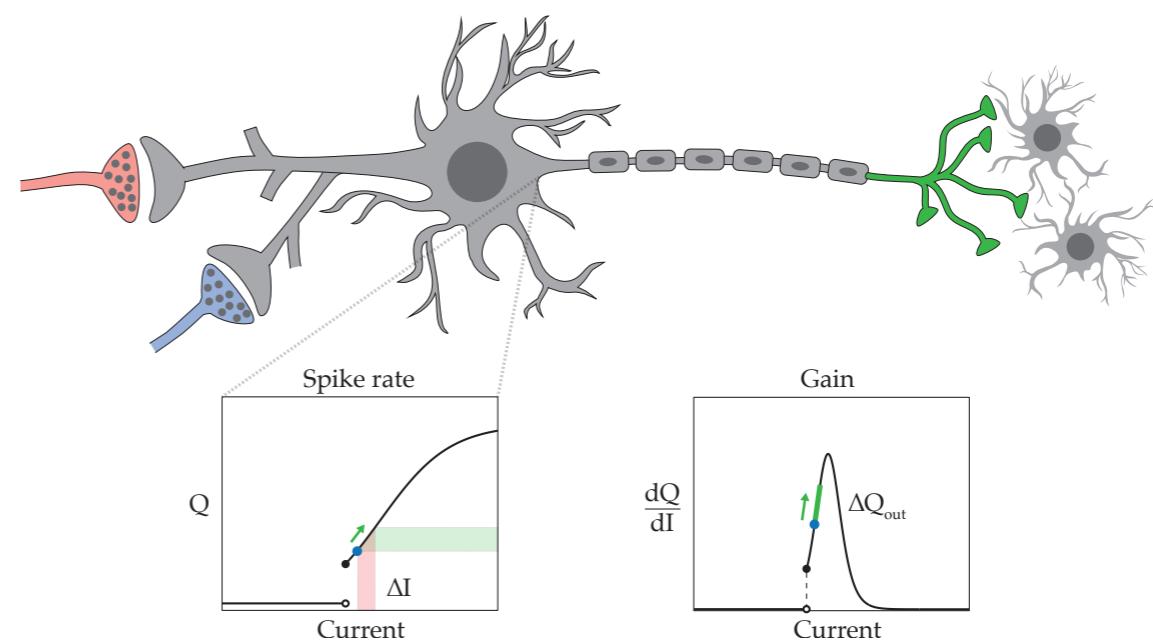


The properties of neurons are not fixed but are plastic, under the influence of ascending neuromodulatory systems



The gain (input-output) of a neuron is also state-dependent so that the response of a neuron to a spike train can be modulated by other inputs

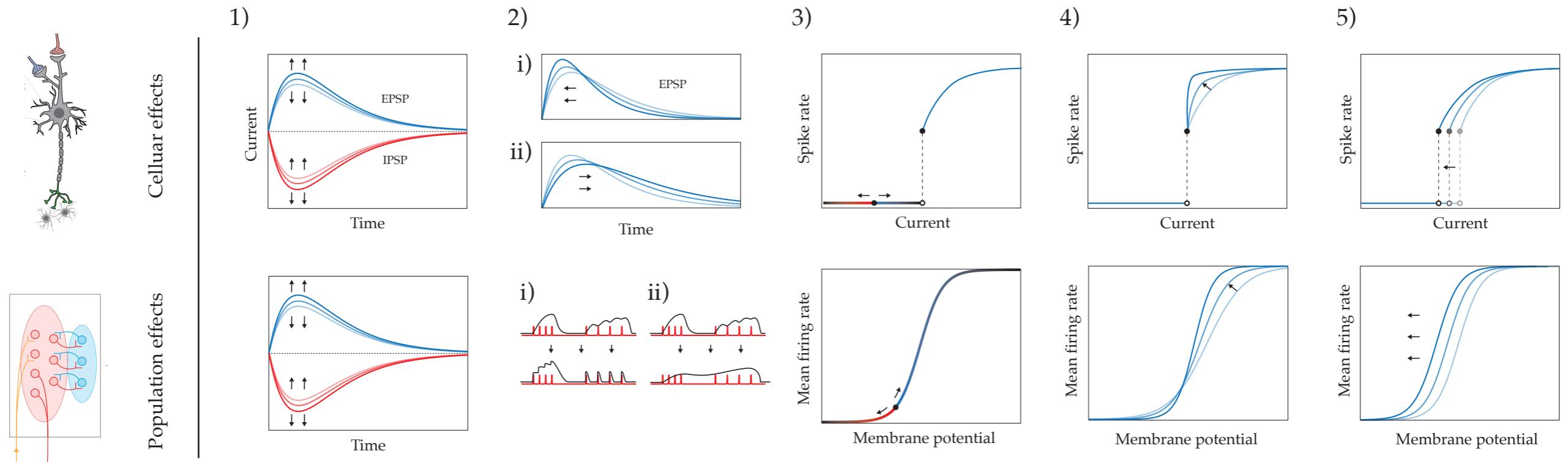
(cf Stephan et al. 2006)



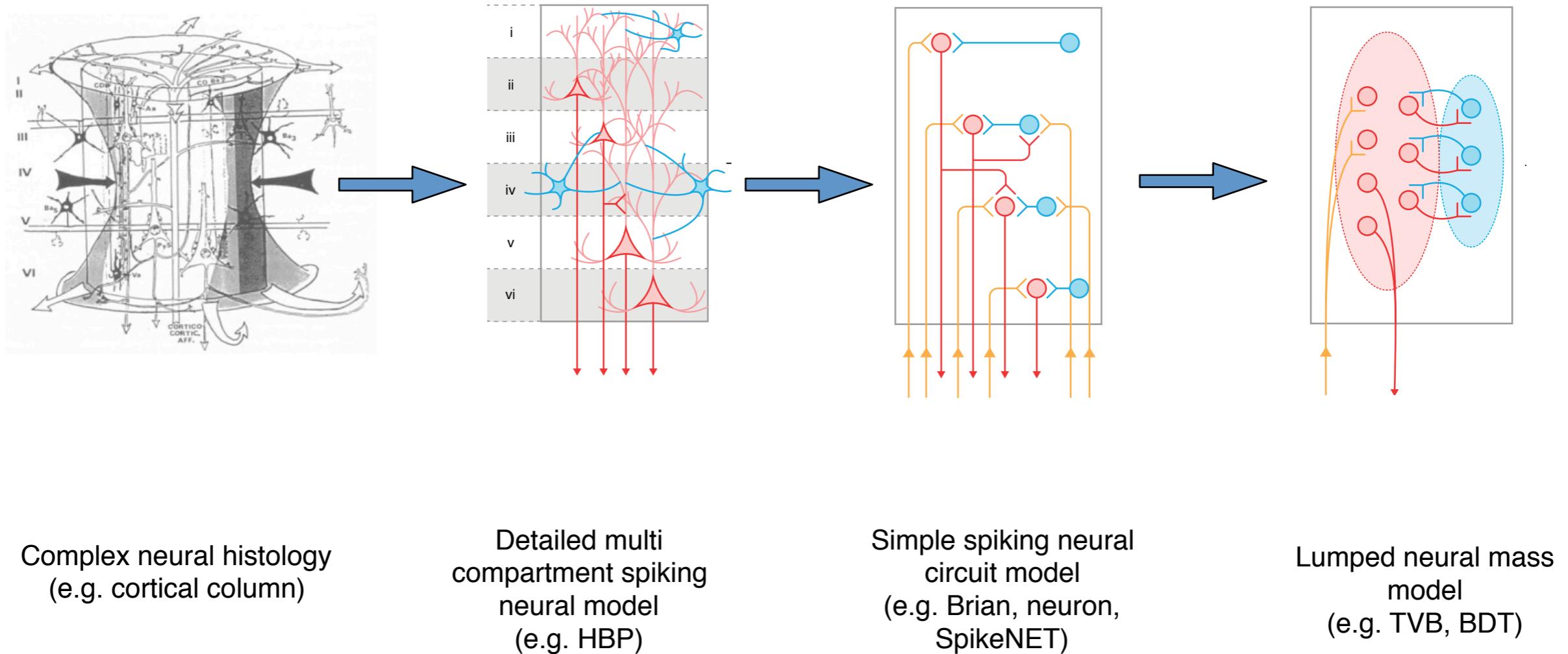
Mac Shine, Eli Muller

I: Population models : Basic principles

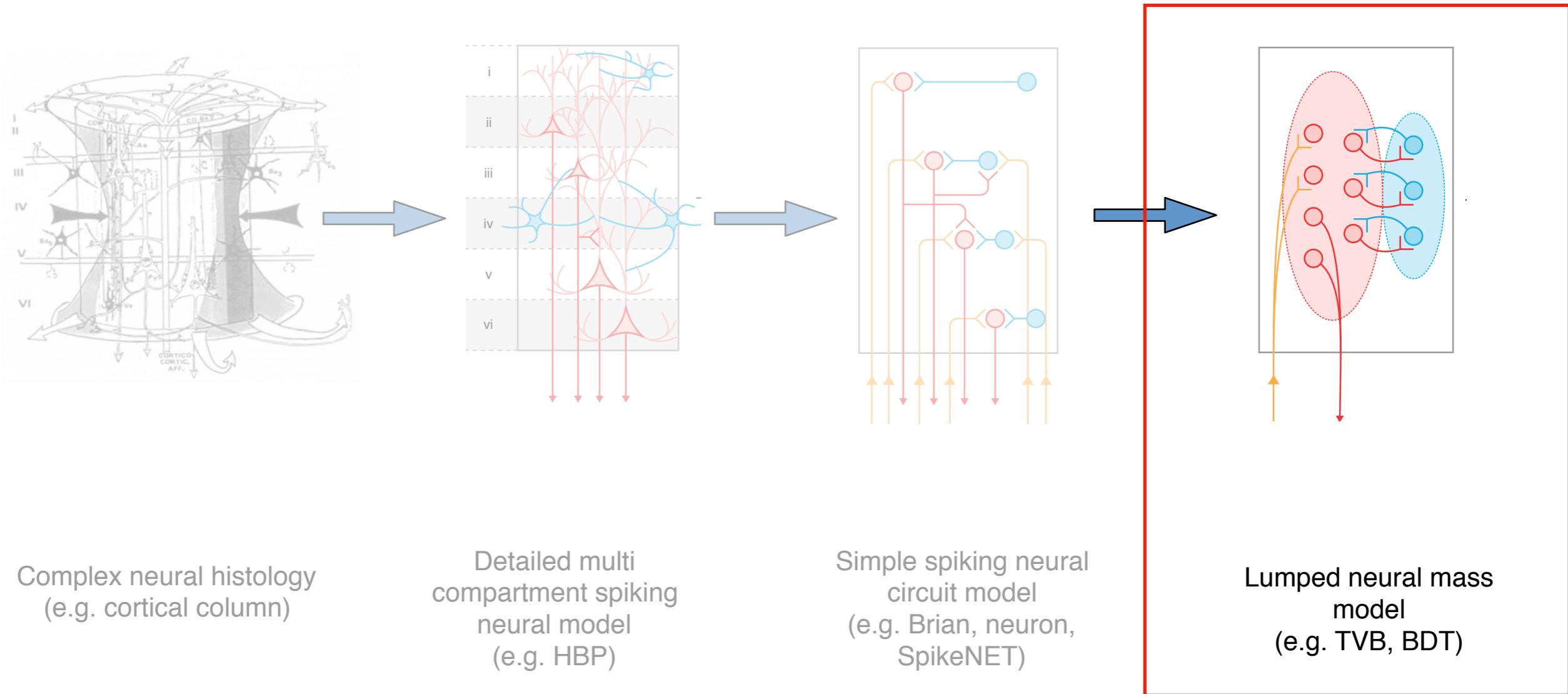
There are mean field effects for all of these mechanisms of single cell neuroplasticity and state-dependent gain modulation



I: Population models : Basic principles



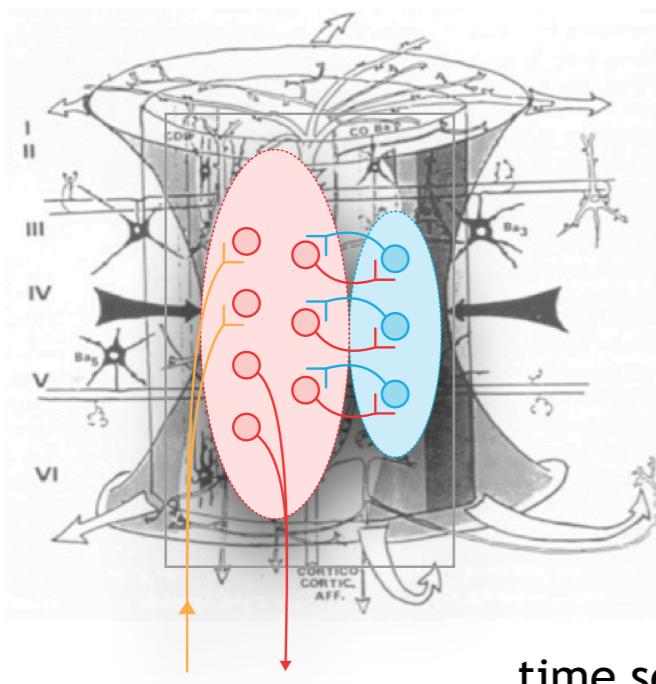
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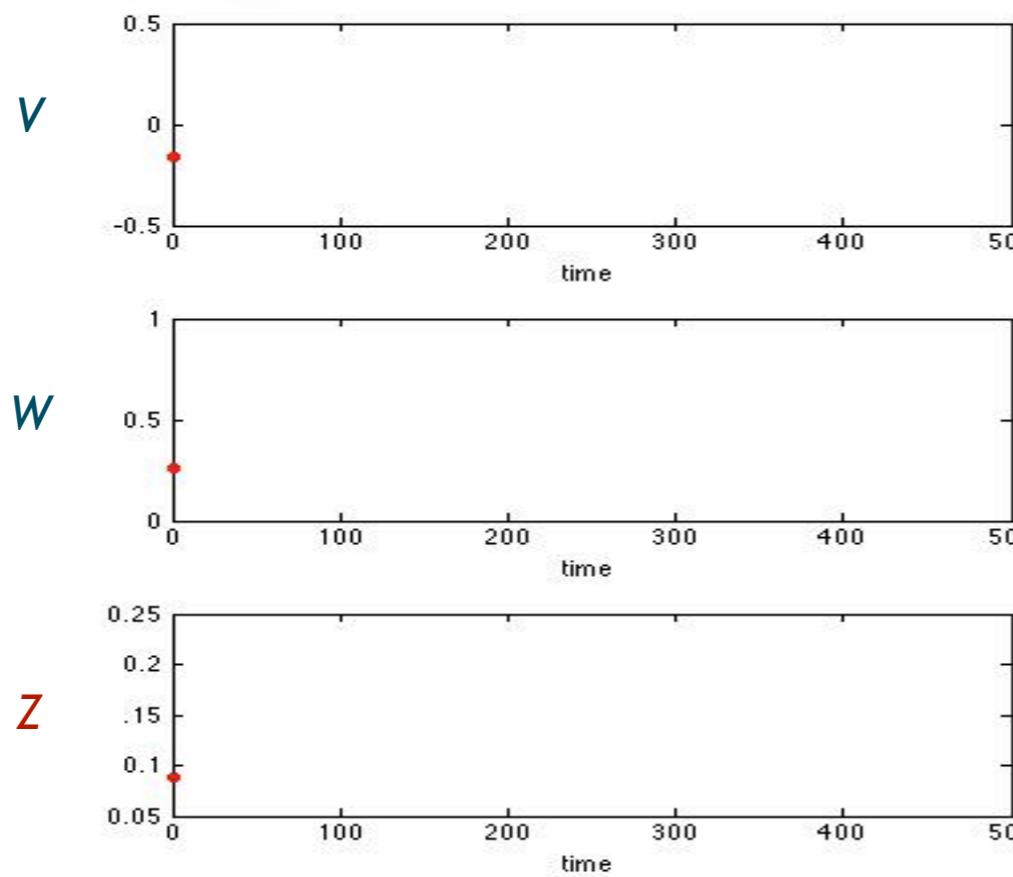
Neural mass and neural field models begin with local lumped (mean field) population models

II: Nodes and neural masses

Neural mass model



time series



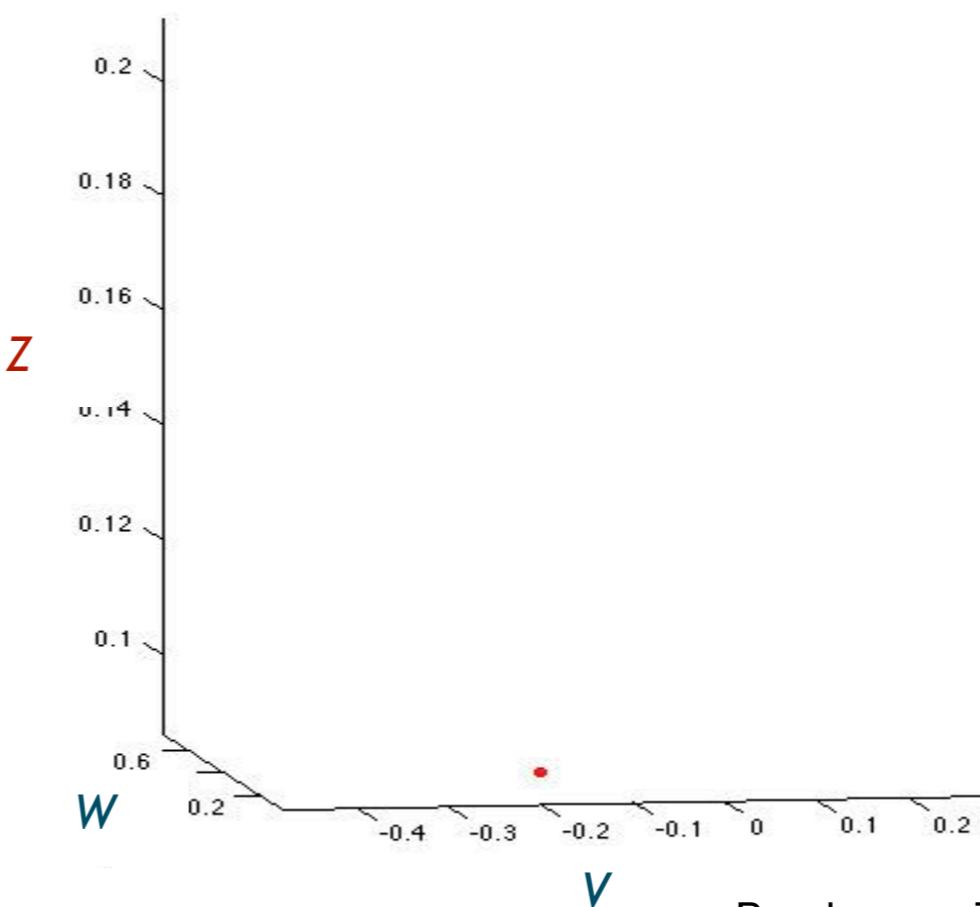
local “centre of mass” (average states over small area)

$$\frac{d\mathbf{X}}{dt} = f(\mathbf{X}) + \mathbf{I}$$

$$\mathbf{X} = \begin{cases} V & \text{pyramidal membrane potential} \\ W & \text{potassium channel conductance} \\ Z & \text{inhibitory membrane potential} \end{cases} \quad \begin{matrix} & (\text{fast}) \\ & \\ & (\text{slow}) \end{matrix}$$

“chaos”

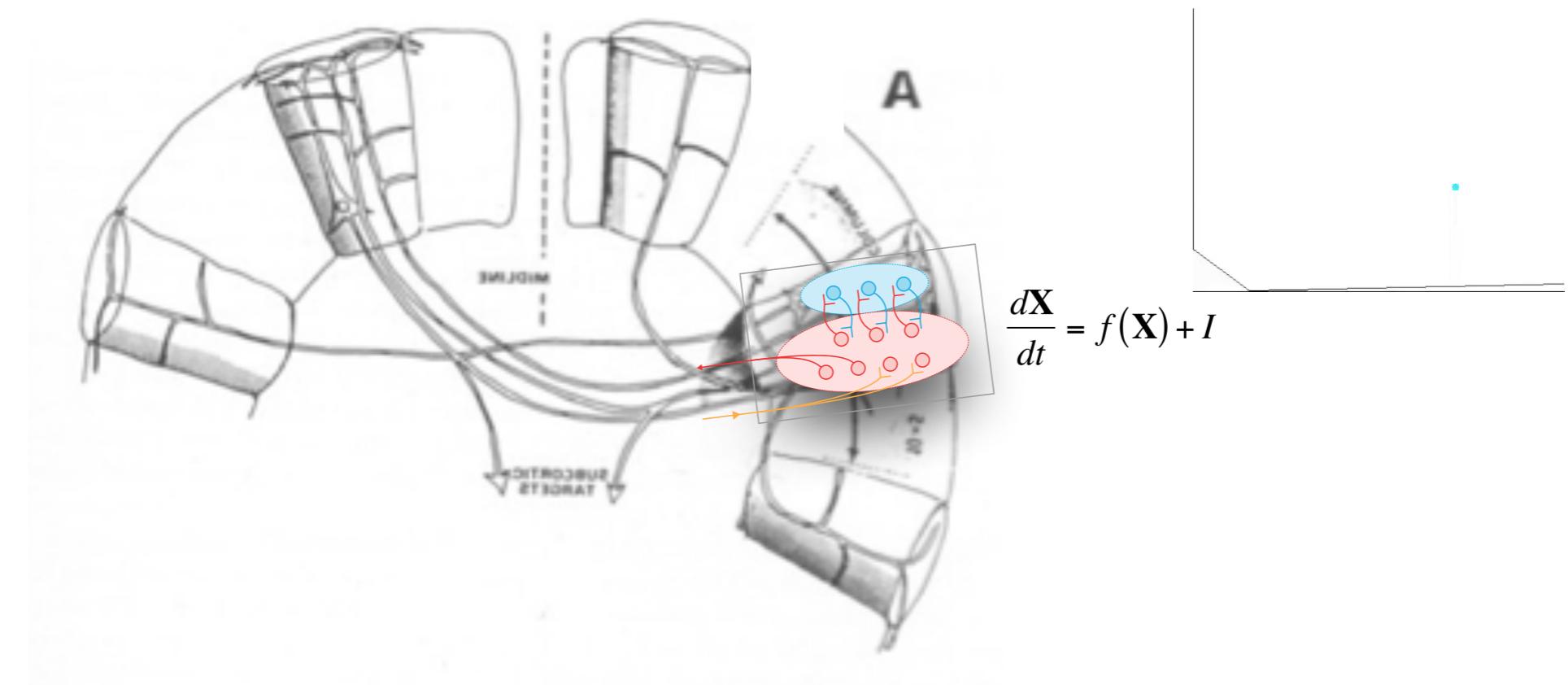
phase portrait



Breakspear, Terry, Friston (2003)

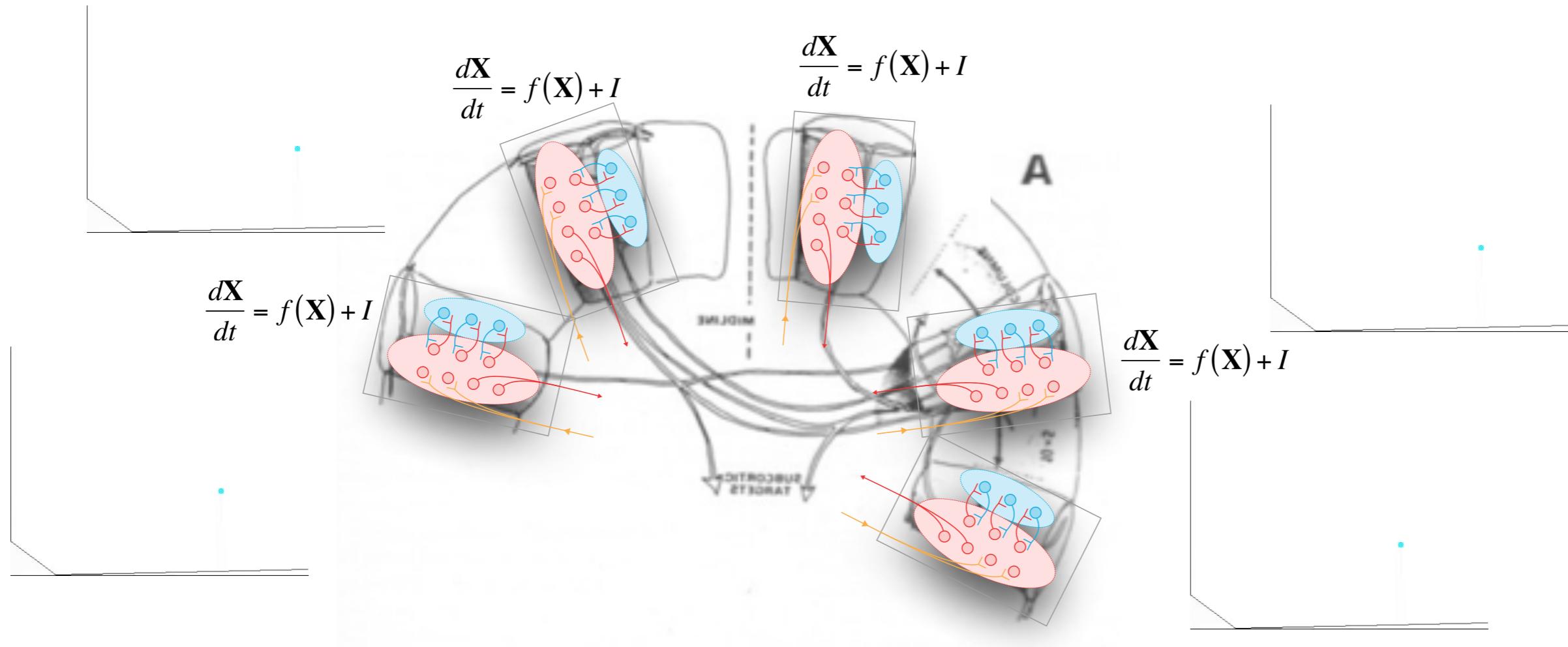
II: Nodes and neural masses

In neural mass models, a local neural mass model is placed at each of the brain's "nodes"



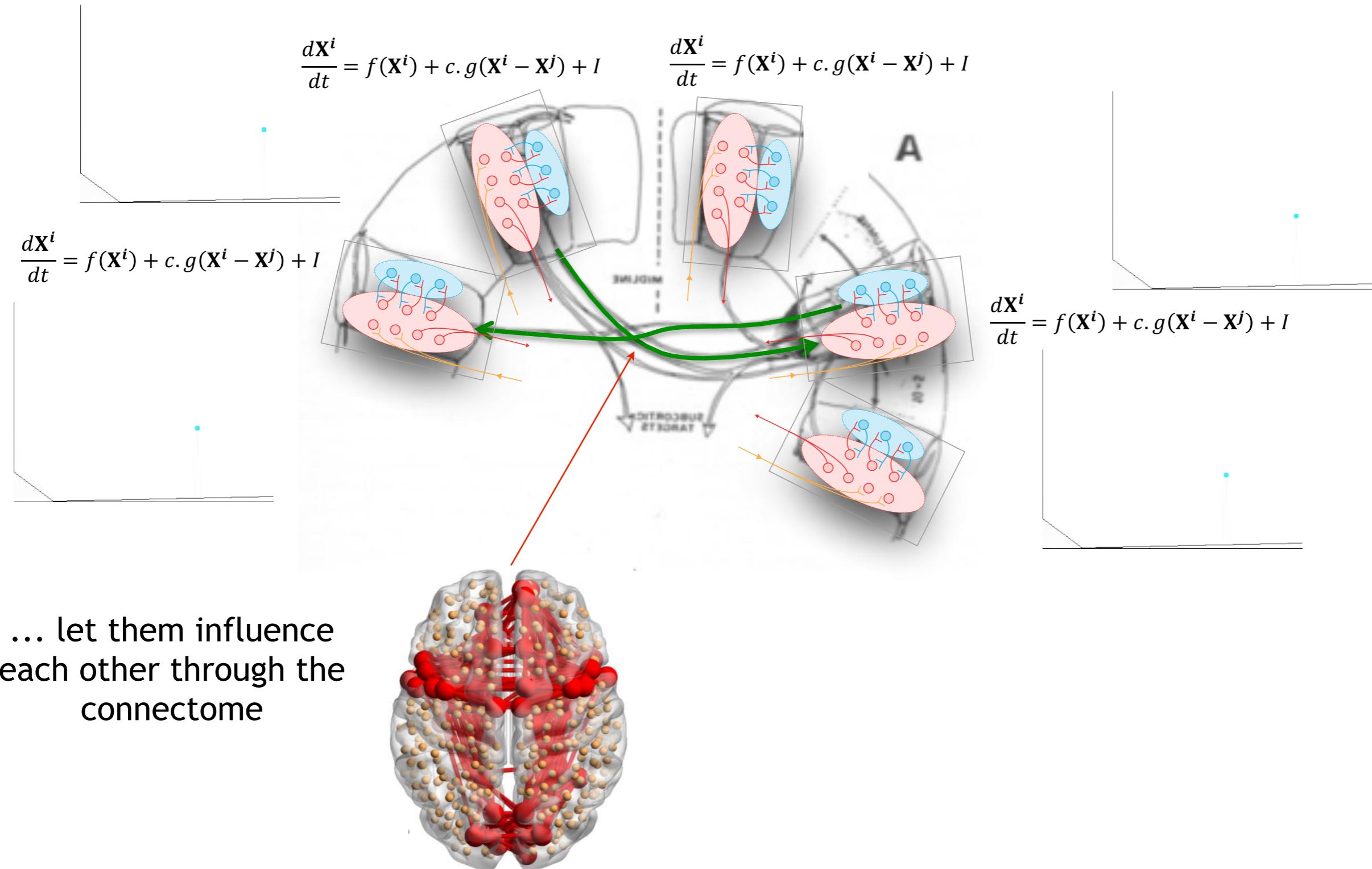
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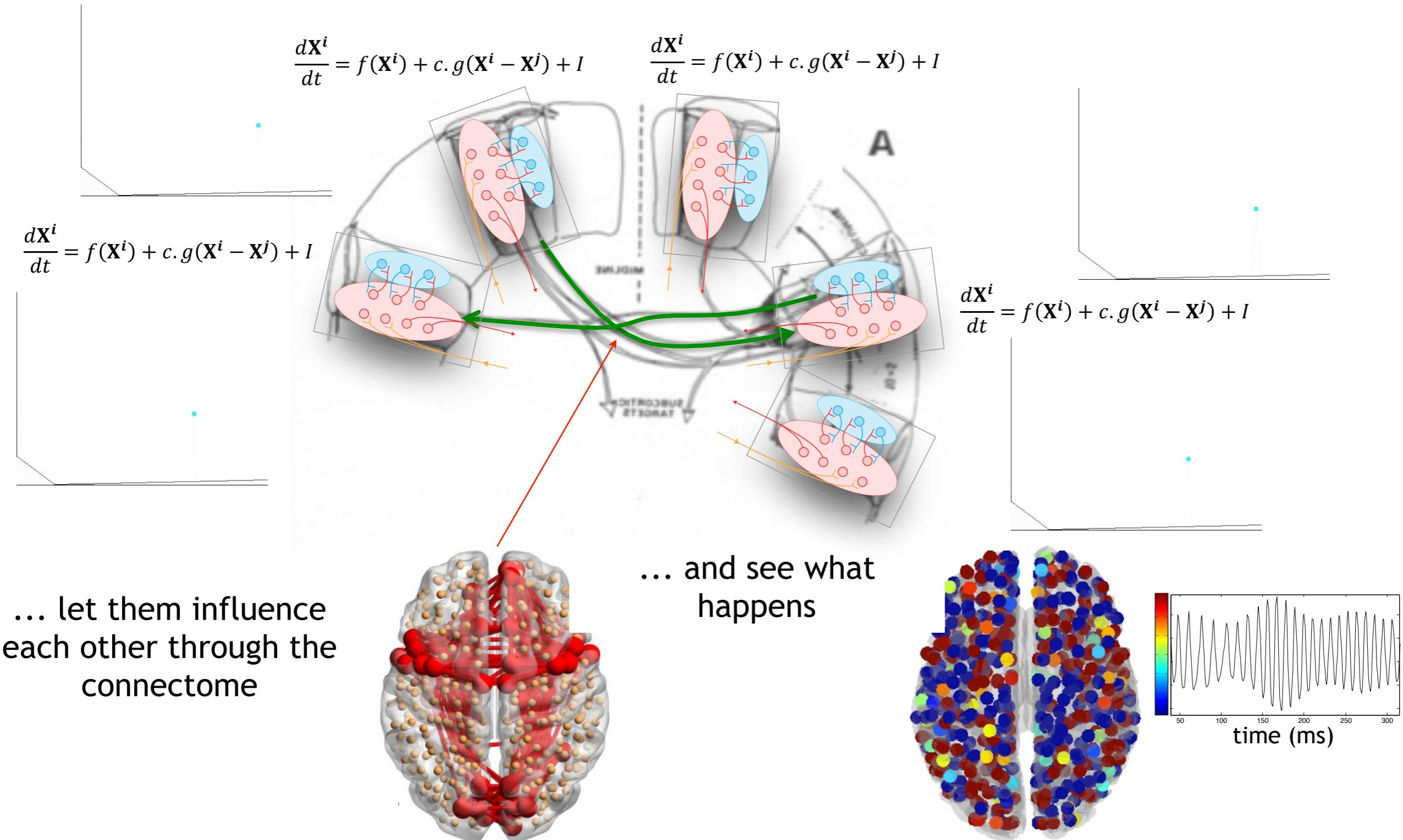
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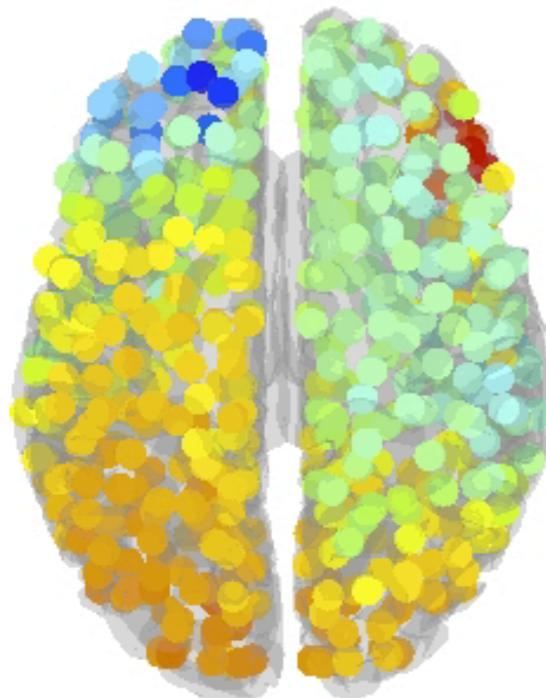
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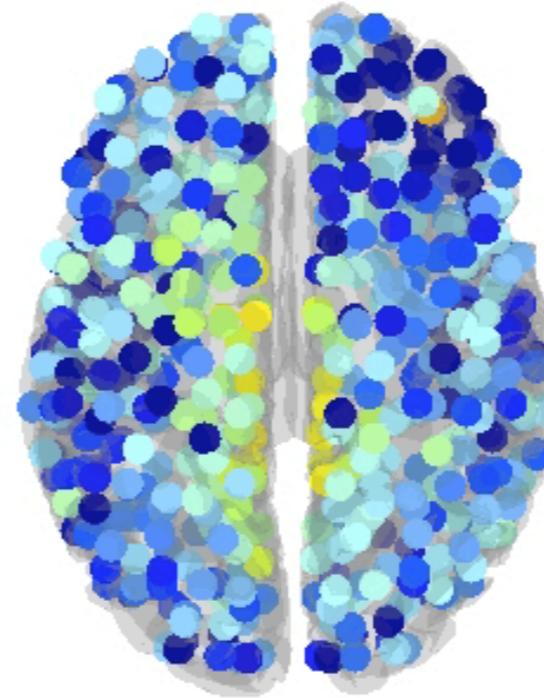


II: Nodes and neural masses

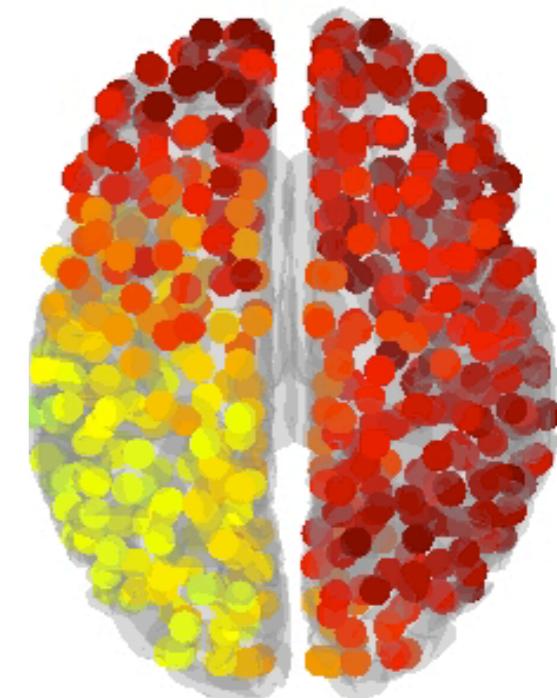
Strong coupling through the connectome leads to a variety of spatiotemporal patterns



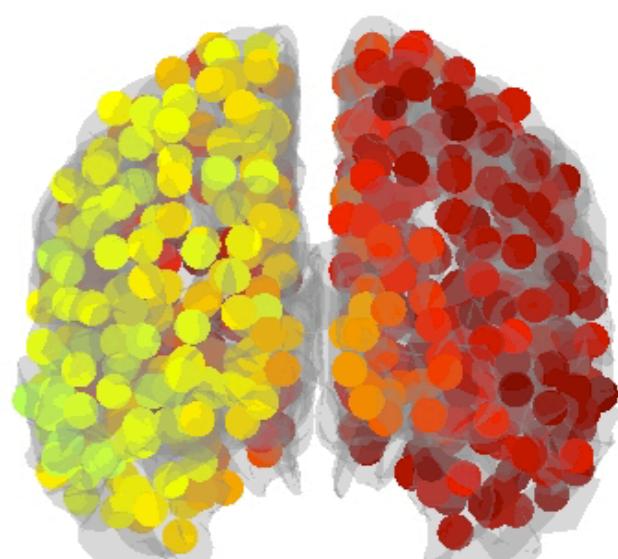
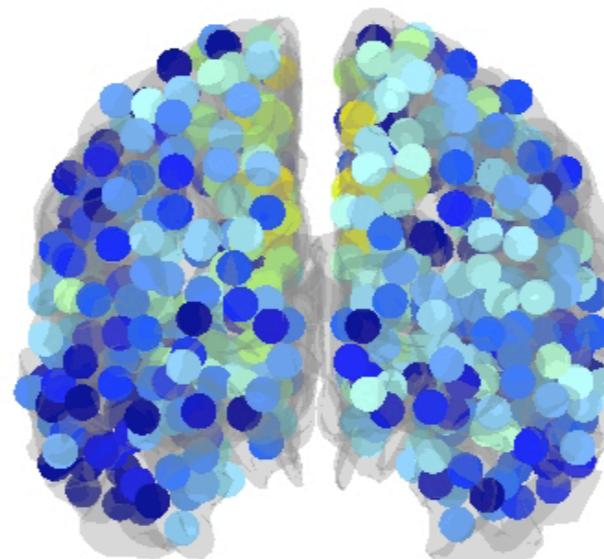
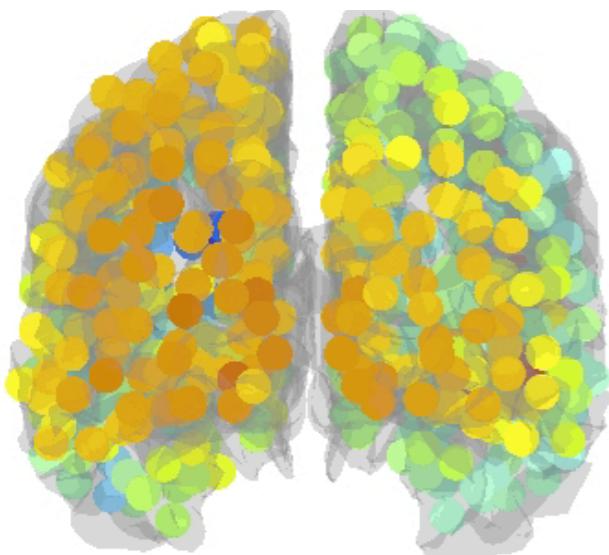
Rotating waves



Breathers



Travelling waves



II: Nodes and neural masses

Waves have recently been observed in a broad spectrum of functional neuroscience data, across species, functions, areas, data modalities

BRIEF COMMUNICATIONS

Traveling waves of activity in primary visual cortex during binocular rivalry

Sang-Hun Lee^{1,3}, Randolph Blake² & David J Heeger¹

VOLUME 8 | NUMBER 1 | JANUAR

**nature
neuroscience**

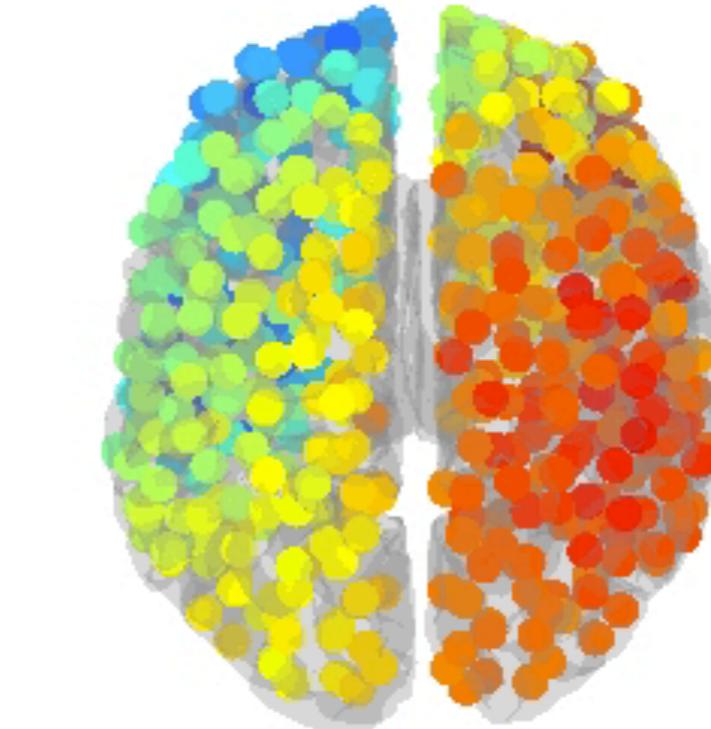
Propagating waves mediate information transfer in the motor cortex

Doug Rubino¹, Kay A Robbins² & Nicholas G Hatsopoulos¹

Neuron
Article

Reverberation of Recent Visual Experience in Spontaneous Cortical Waves

Feng Han,^{1,4} Natalia Caporale,^{2,4} and Yang Dan^{1,2,3,*}



**nature
COMMUNICATIONS**

ARTICLE

Received 24 Sep 2013 | Accepted 17 Mar 2014 | Published 28 Apr 2014

DOI: 10.1038/ncomms4675

OPEN

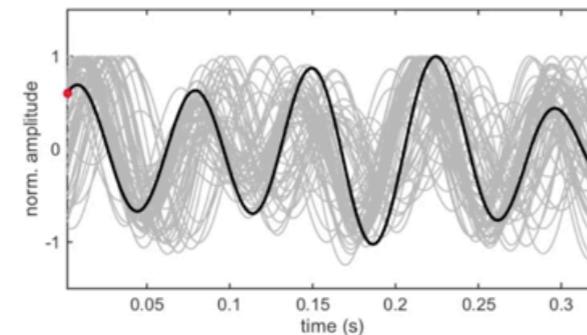
The stimulus-evoked population response in visual cortex of awake monkey is a propagating wave

Lyle Muller^{1,*}, Alexandre Reynaud^{2,*}, Frédéric Chavane² & Alain Destexhe¹

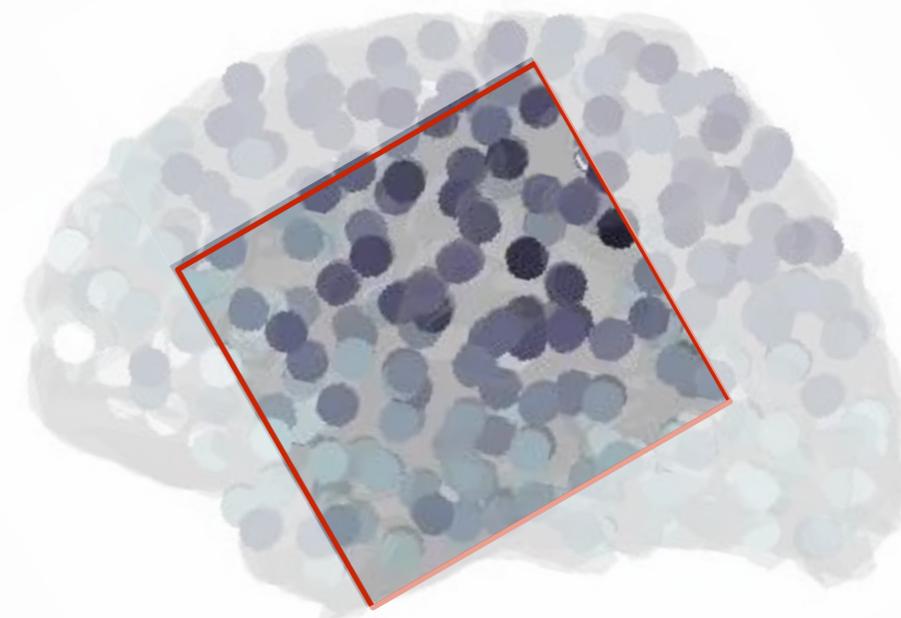
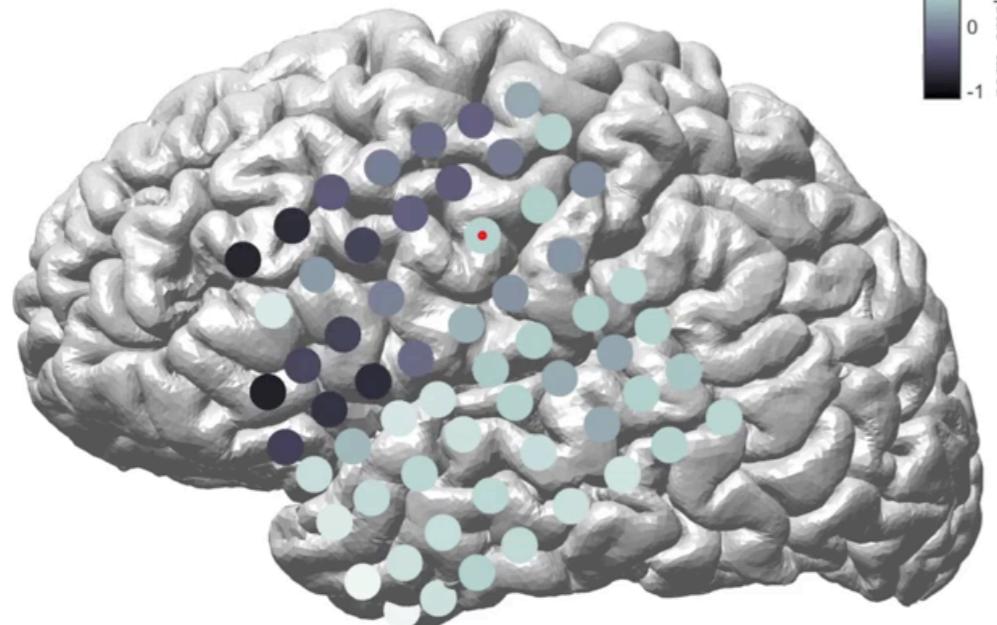
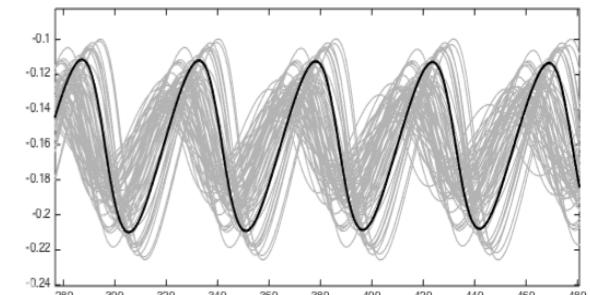
II: Nodes and neural masses

Interestingly, these predictions bear close relationship with waves in recently acquired human spindles waves during sleep

Data



Model



**Rotating waves during human sleep
spindles organize global patterns of
activity that repeat precisely through the
night**

Lyle Muller¹, Giovanni Piantoni², Dominik Koller¹, Sydney S Cash², Eric Halgren^{3,4},
Terrence J Sejnowski^{1*}



ARTICLE

<https://doi.org/10.1038/s41467-019-108999-0>

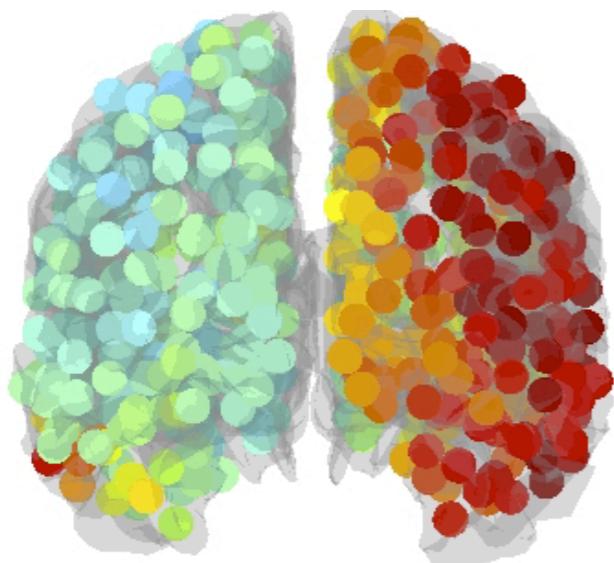
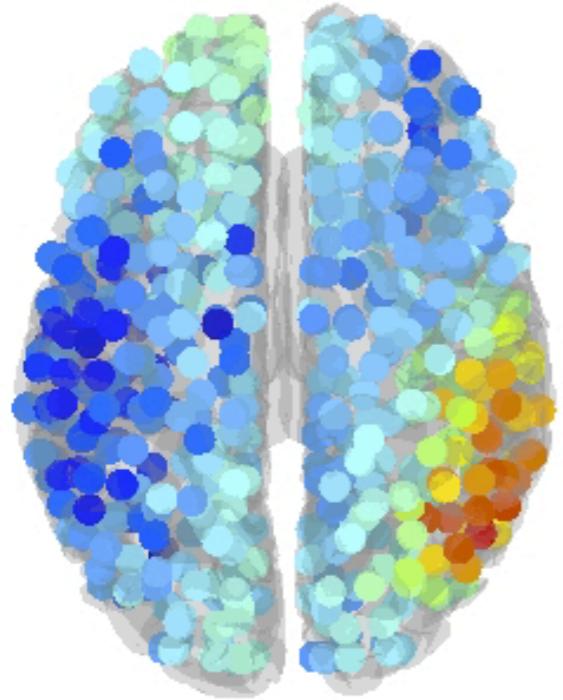
OPEN

Metastable brain waves

James A. Roberts^{1,2}, Leonardo L. Gollo^{1,2}, Romesh G. Abeysuriya³, Gloria Roberts^{4,5}, Philip B. Mitchell^{4,5},
Mark W. Woolrich³ & Michael Breakspear^{1,2,6,7}

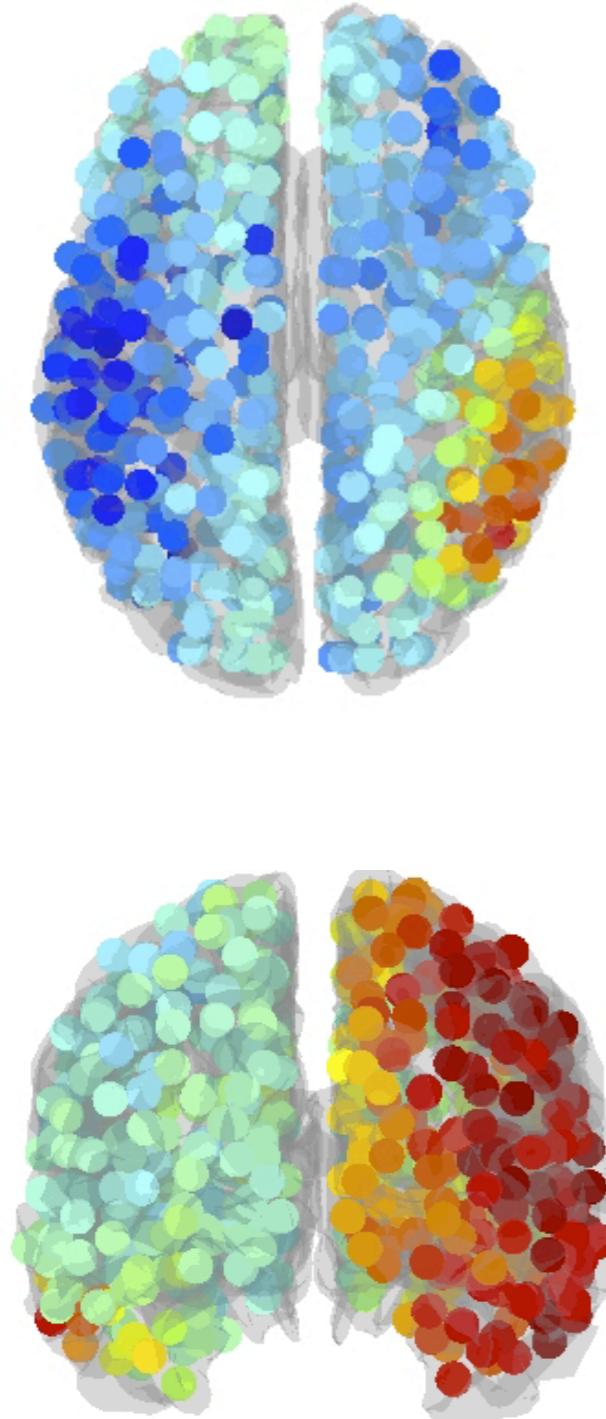
II: Nodes and neural masses

These dynamics spontaneously cycle through distinct spatiotemporal patterns

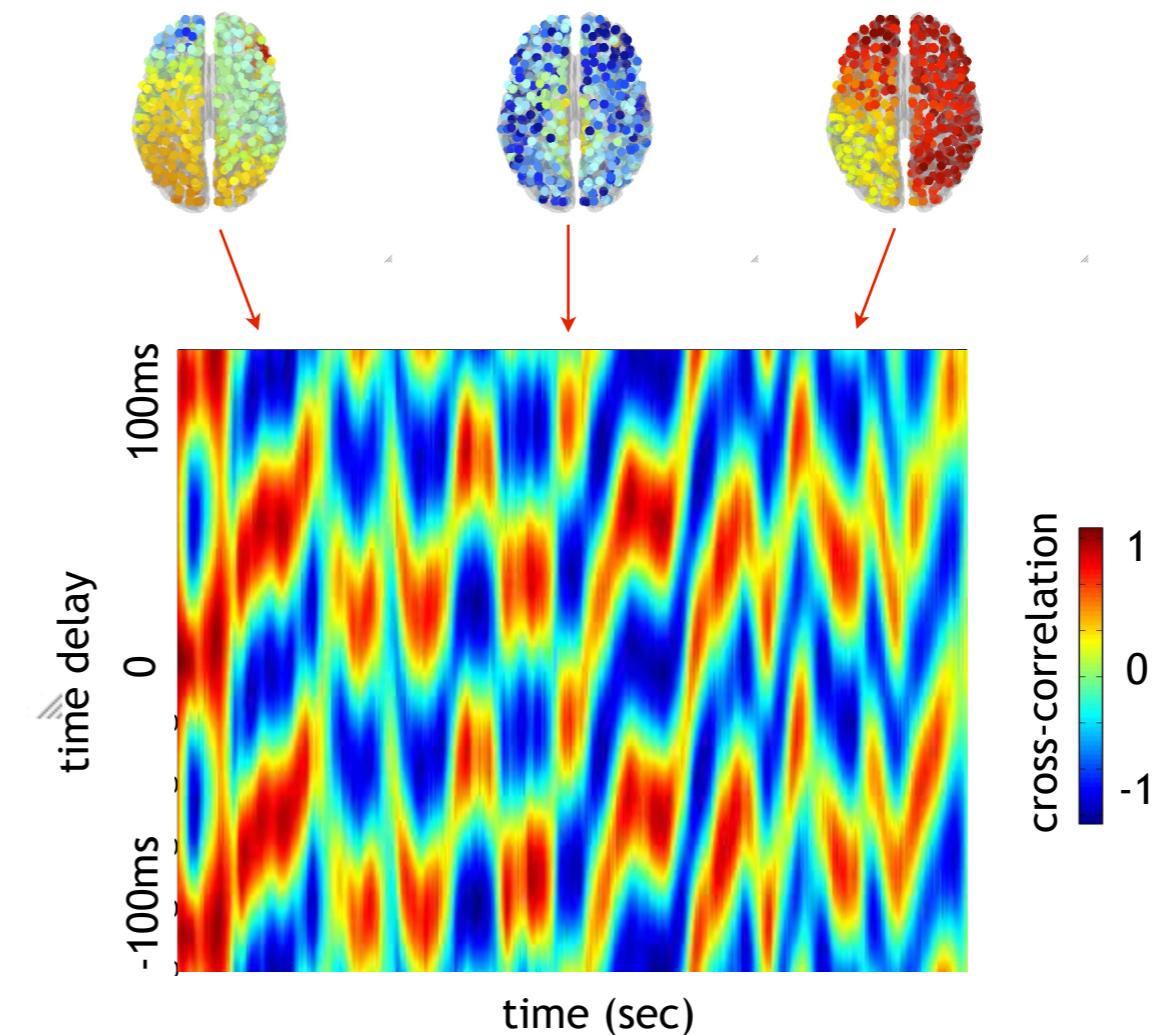


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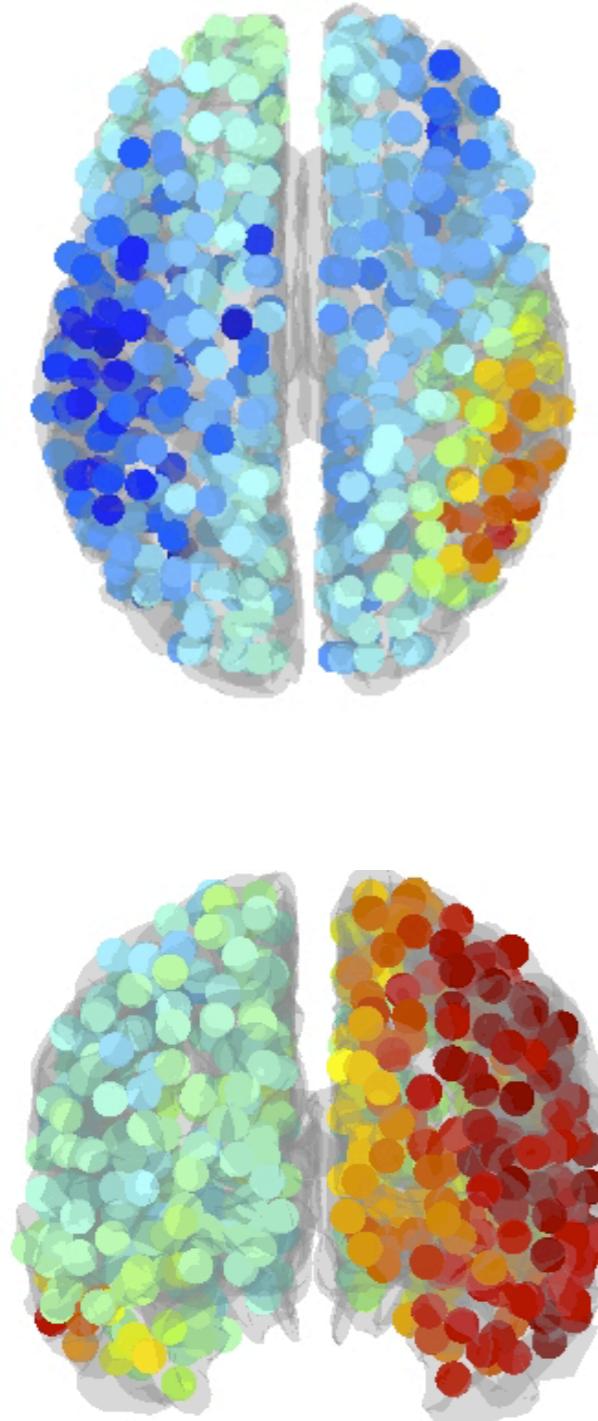


Each pattern is associated with a distinct “whole brain” correlation structure

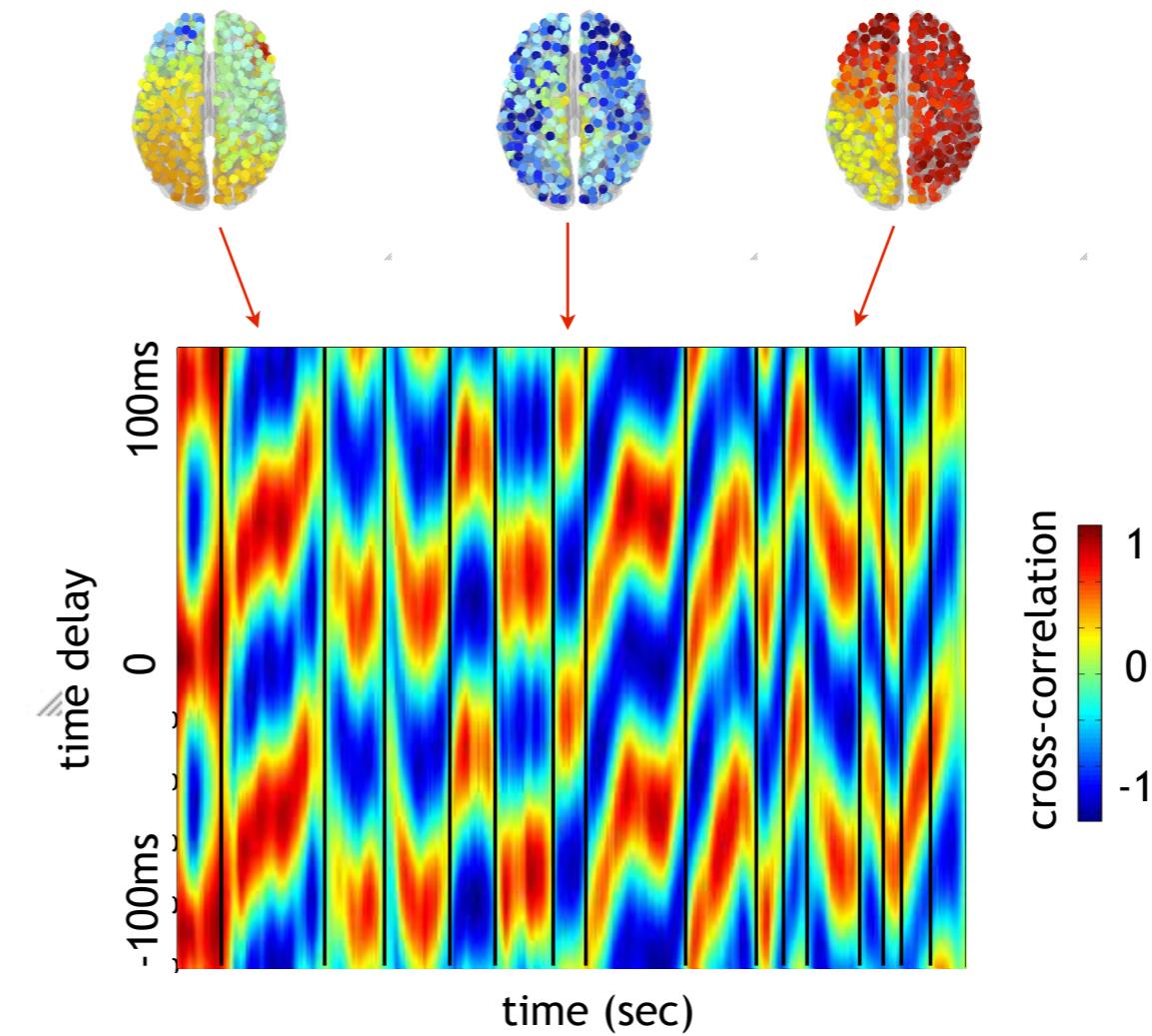


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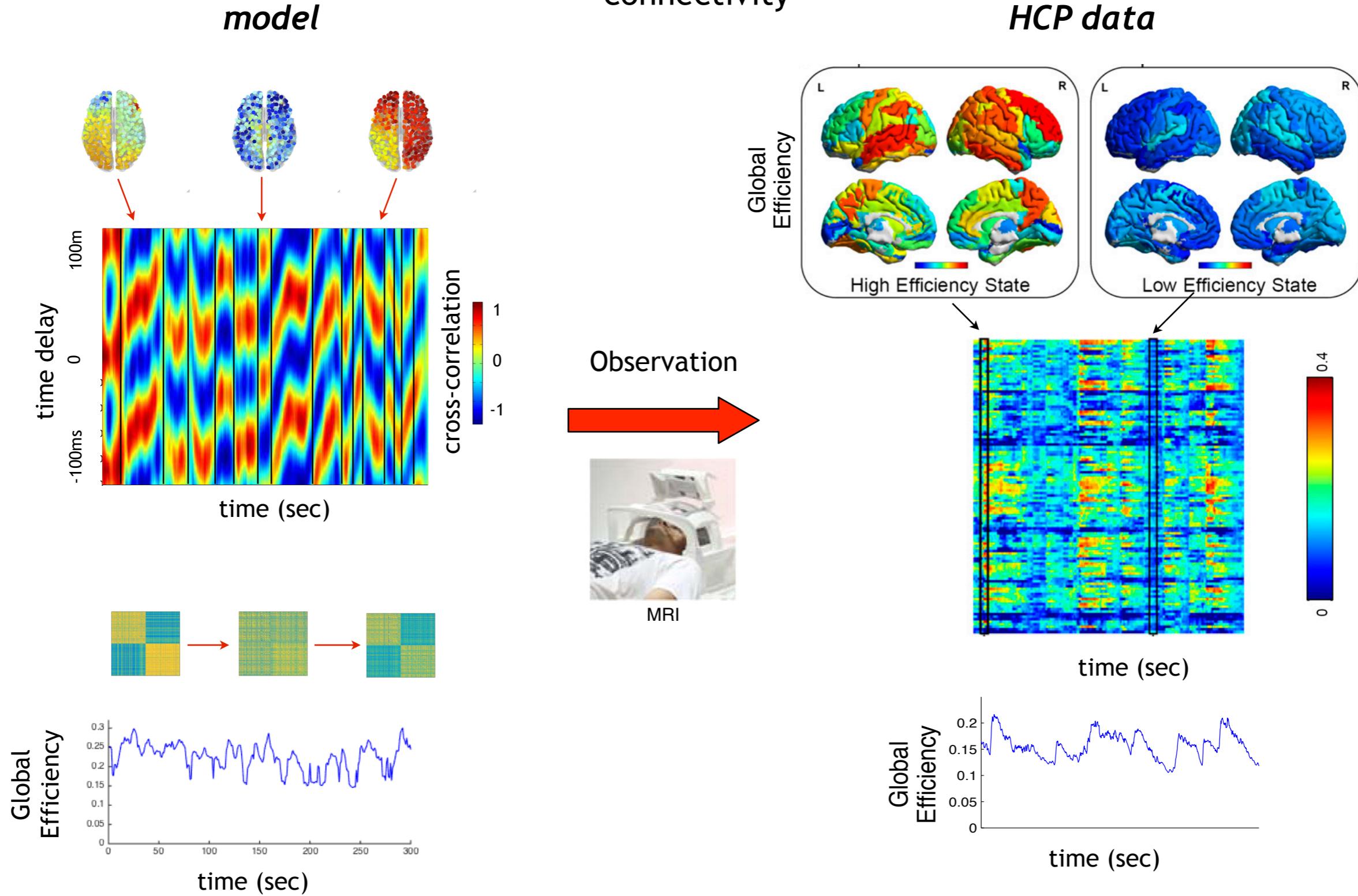
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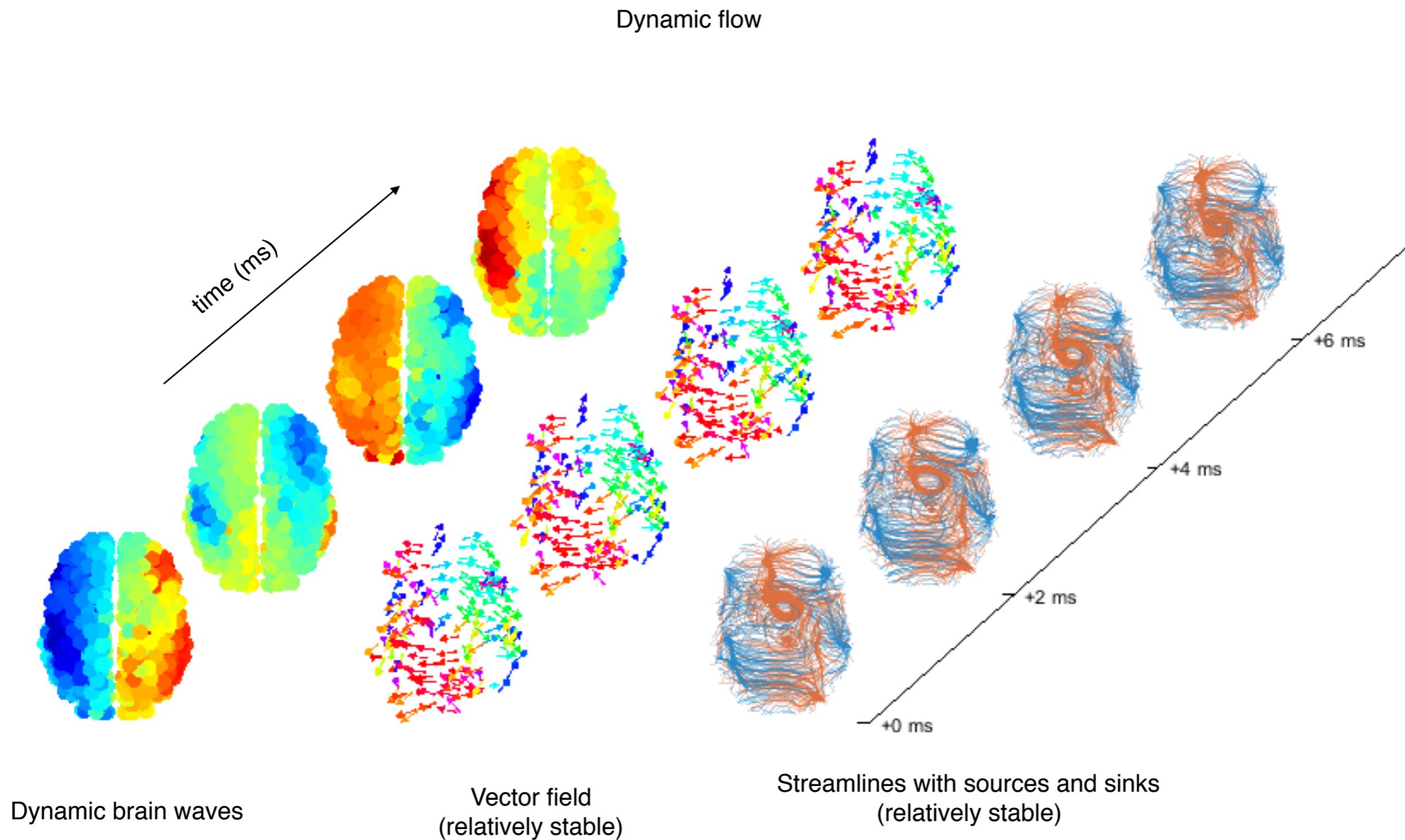
Transitions are associated with weak correlations which can be used to partition the data into metastable states

II: Nodes and neural masses

Such dynamics provide a plausible generative model for dynamic functional connectivity



II: Nodes and neural masses



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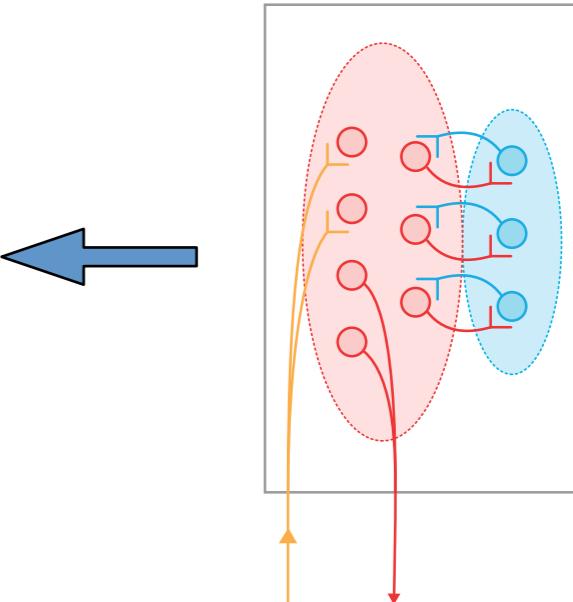
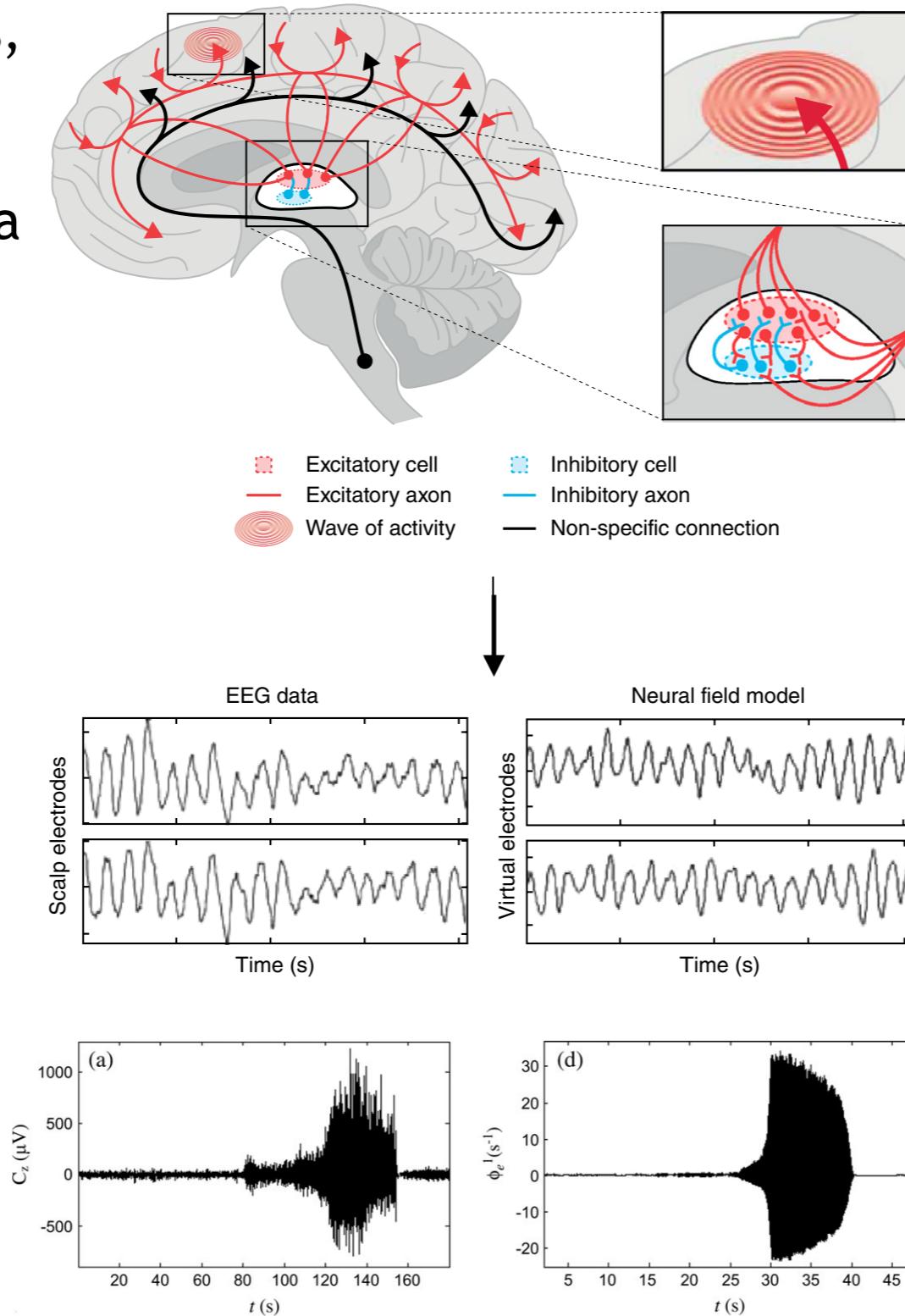


III: Neural fields + modes

$$\frac{1}{\gamma_e^2} \left(\frac{\partial^2}{\partial t^2} + 2\gamma_e^2 \frac{\partial}{\partial t} + \gamma_e^2 - \nu_e^2 \nabla^2 \right) \phi_e(\mathbf{x}, t) = Q_e(\mathbf{x}, t).$$

In neural field models,
population activity
spreads continuously
across the cortex via a
wave equation

Subcortical loops
create resonant
frequencies



Robinson et al (2001, 2002) PRE

Numerical and analytic
approaches then allow
prediction of brain
activity

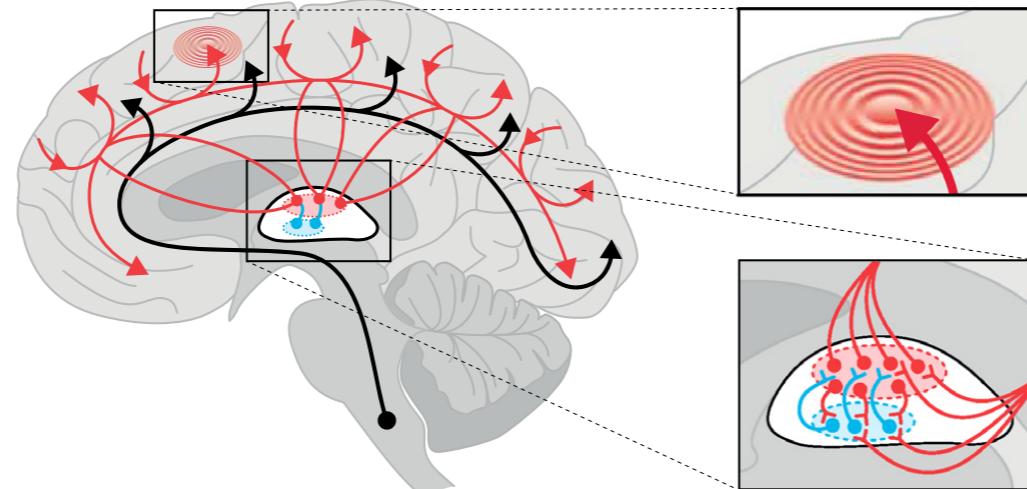
Seizures correspond to
nonlinear (Hopf)
bifurcations

Breakspear et al (2006) Cerebral Cortex

III: Neural fields + modes

Neural fields can also be decomposed into (eigen-)modes of spatiotemporal activity, each with their own spectral fingerprint

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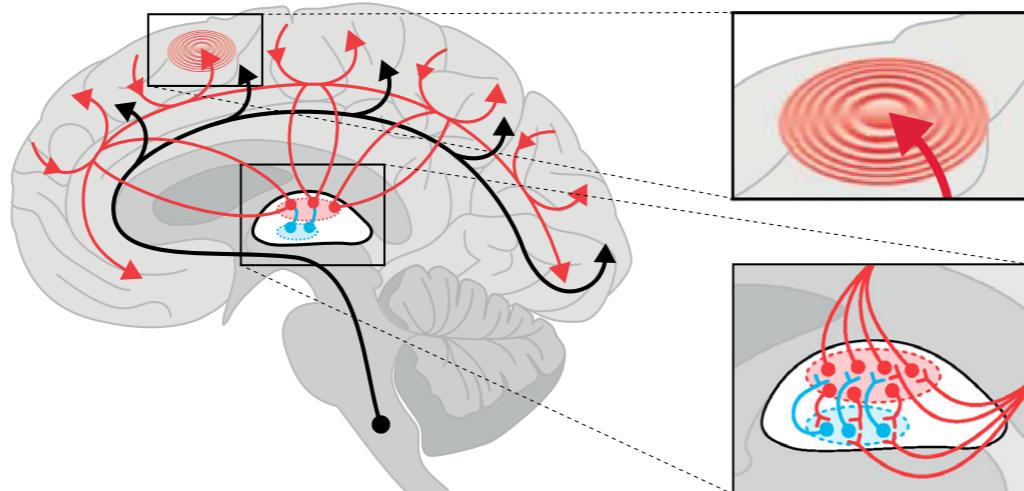


$$\begin{aligned}\nabla^2 y_\eta(\mathbf{r}) &= -k_\eta^2 y_\eta(\mathbf{r}), \\ D'(\omega_\eta) &= -k_\eta^2 r_{ee}^2.\end{aligned}$$

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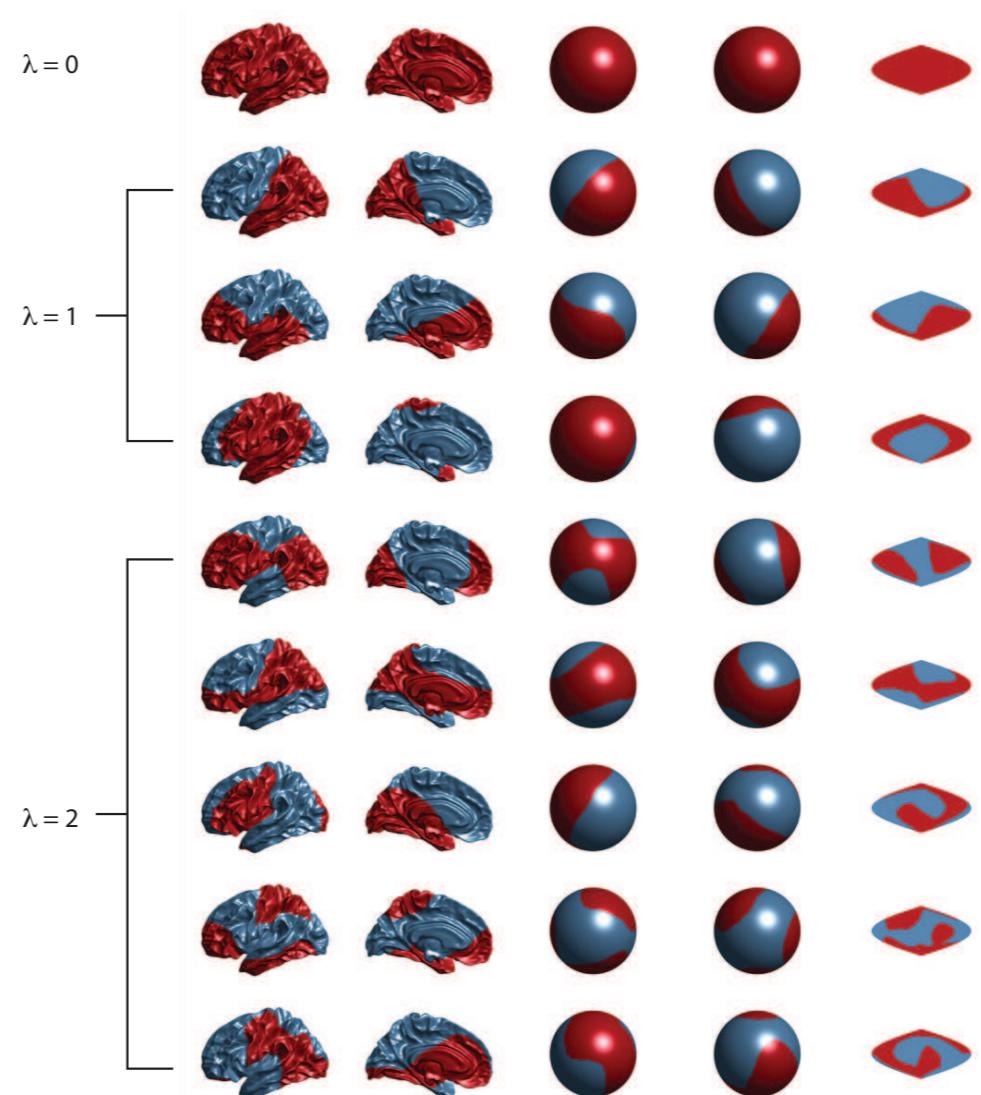


$$\begin{aligned}\nabla^2 y_\eta(\mathbf{r}) &= -k_\eta^2 y_\eta(\mathbf{r}), \\ D'(\omega_\eta) &= -k_\eta^2 r_{ee}^2.\end{aligned}$$

where,

$$\nabla^2 f = \sum_{i,j} \frac{1}{|g|^{1/2}} \frac{\partial}{\partial x^i} \left(|g|^{1/2} g^{ij} \frac{\partial f}{\partial x^j} \right),$$

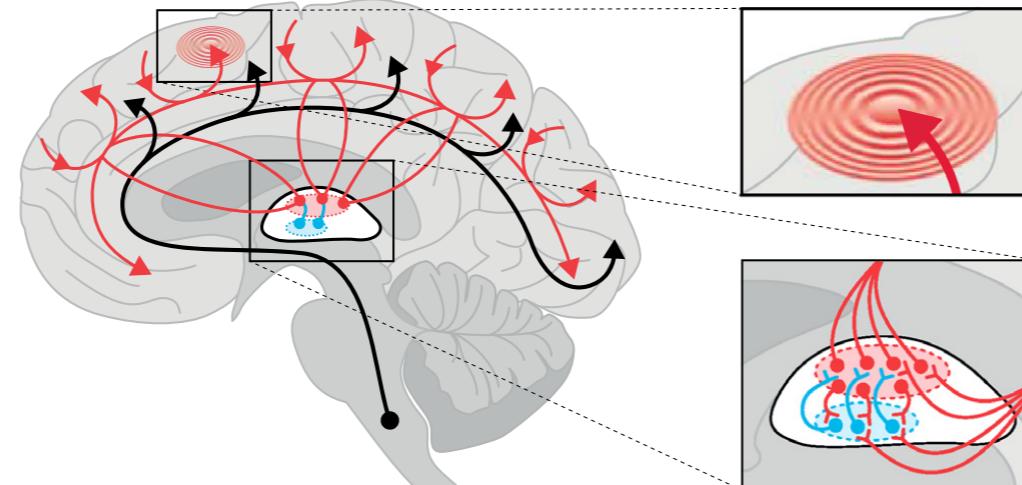
is the Laplace-Beltrami operator



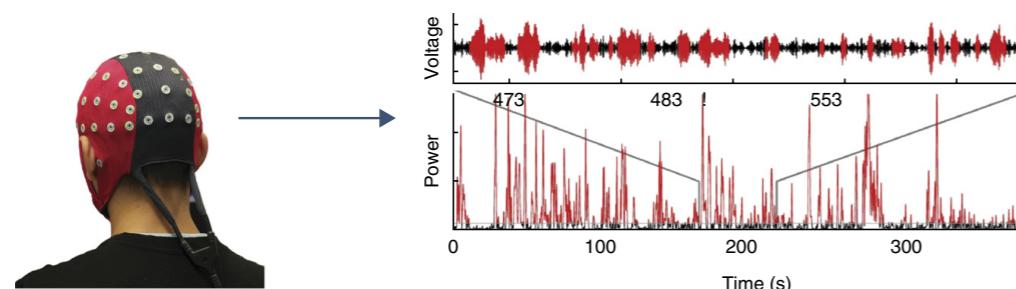
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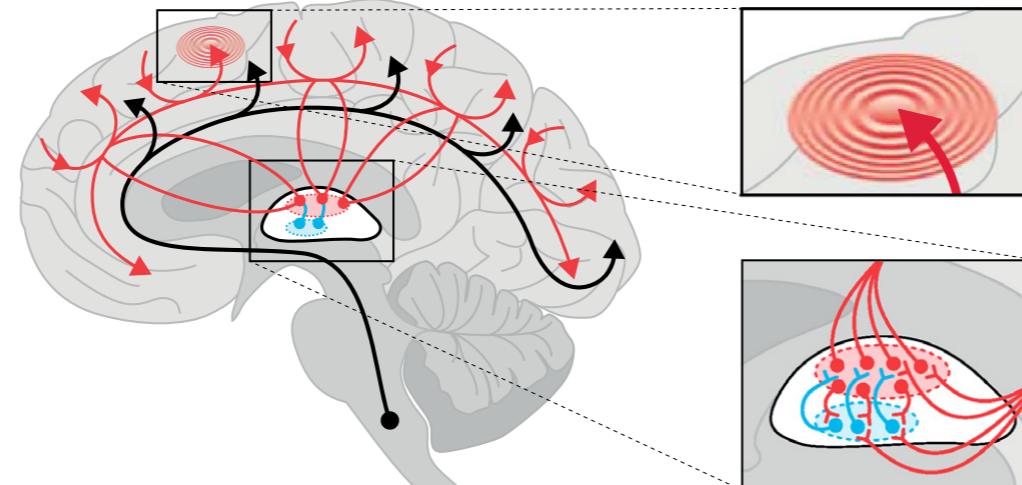
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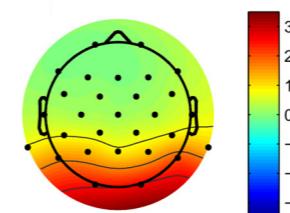
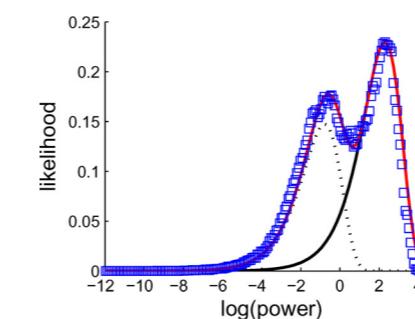
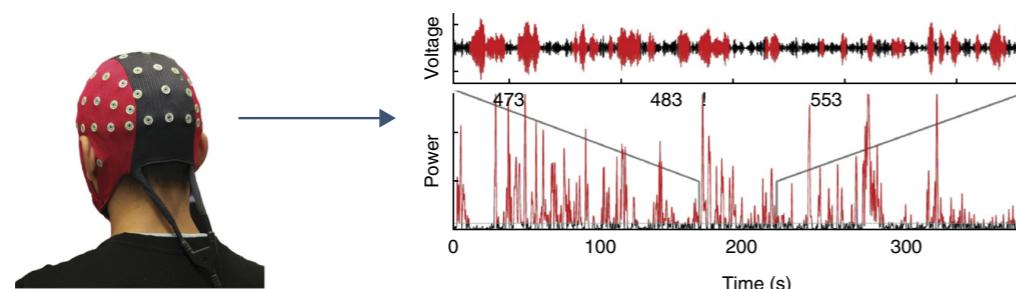
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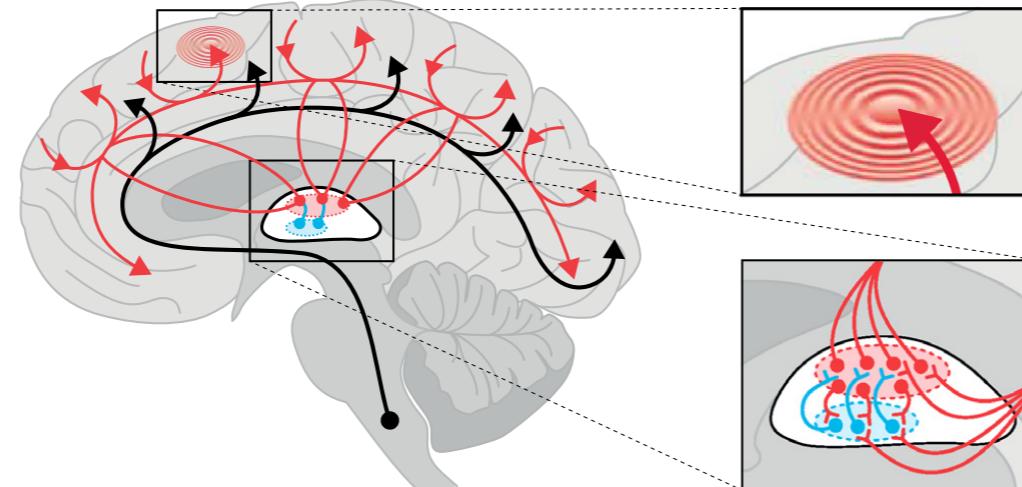
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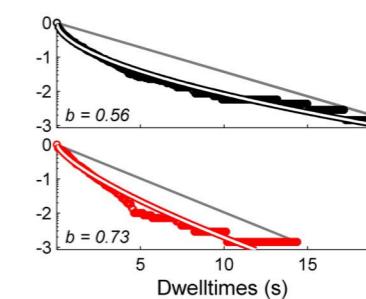
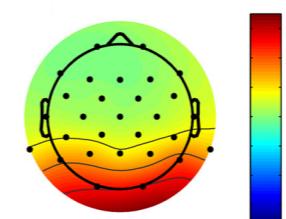
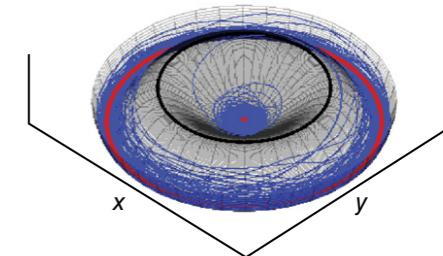
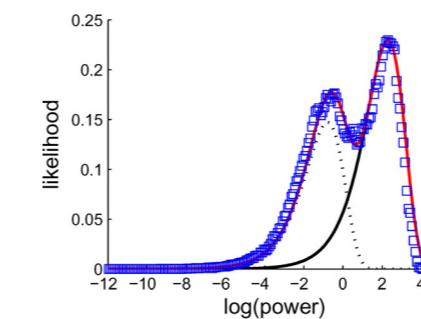
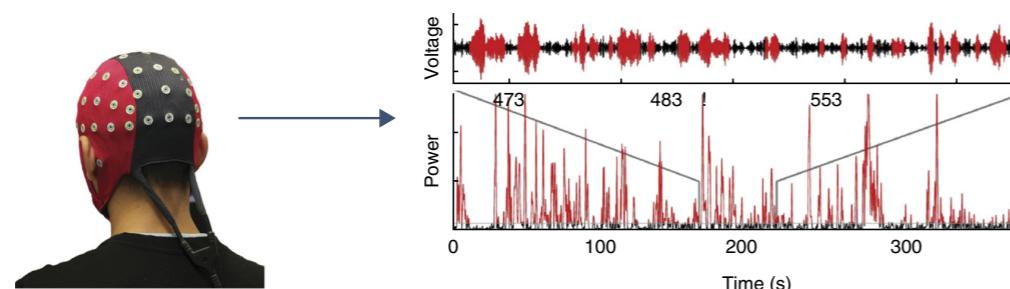
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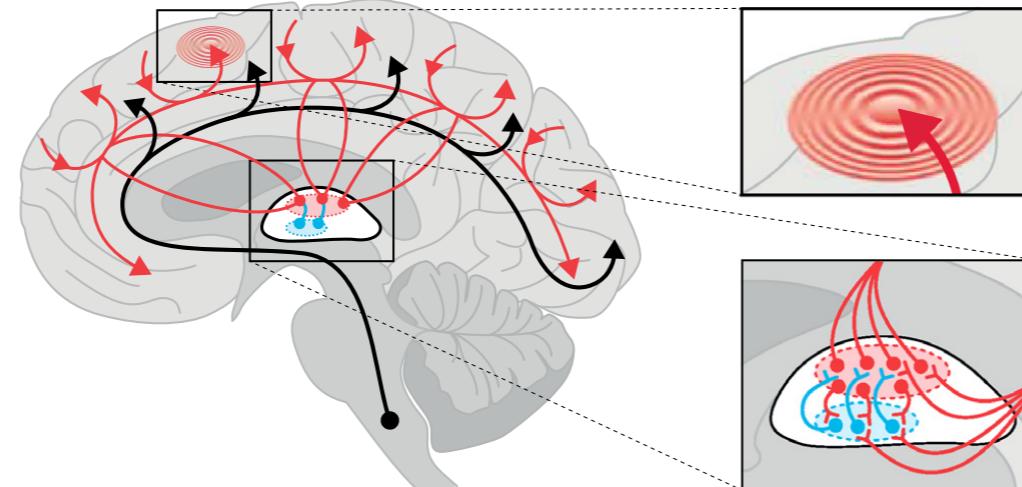
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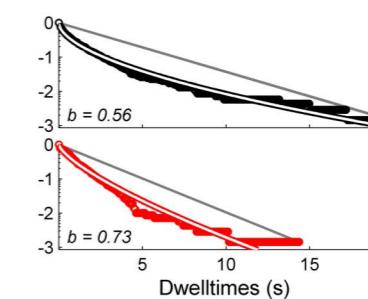
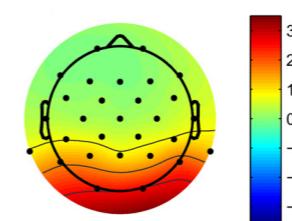
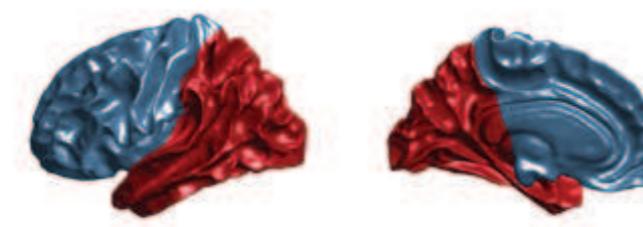
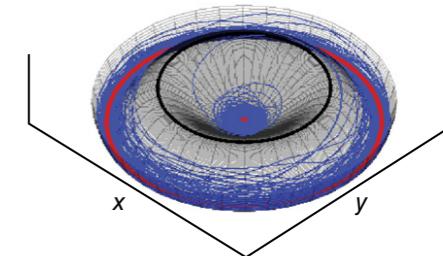
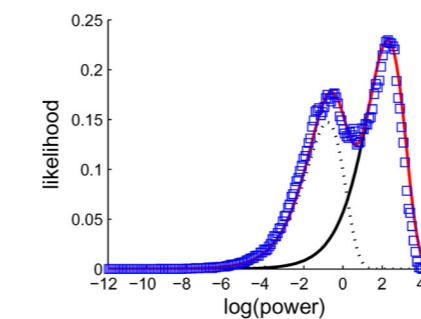
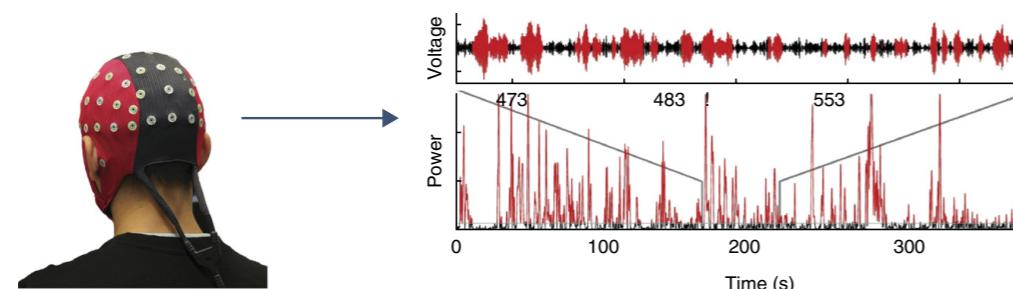
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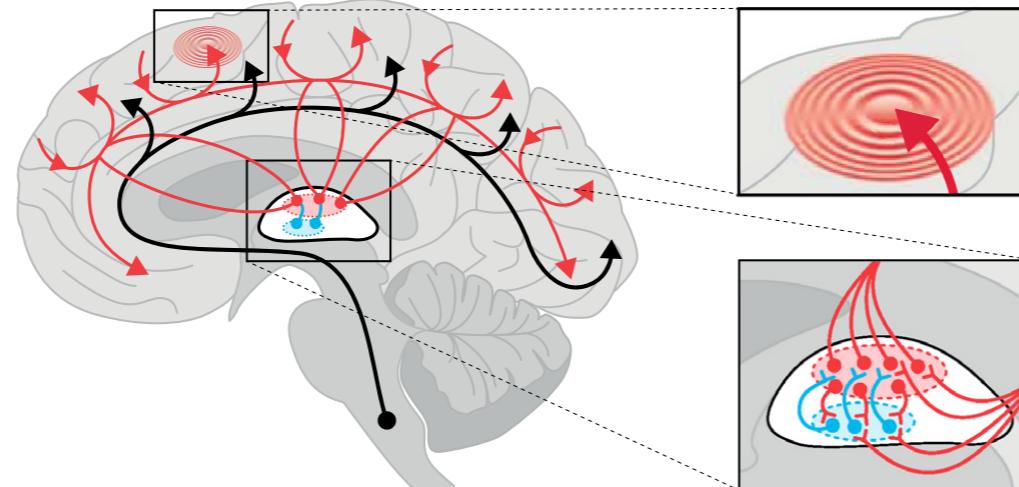
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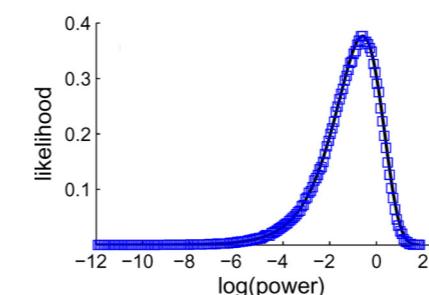
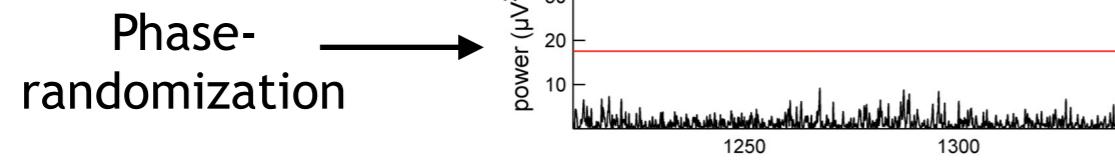
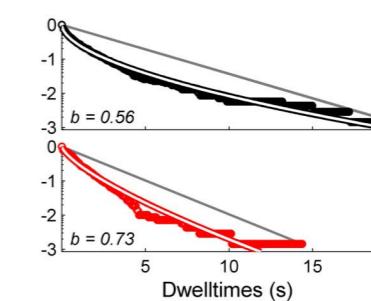
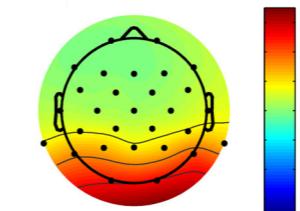
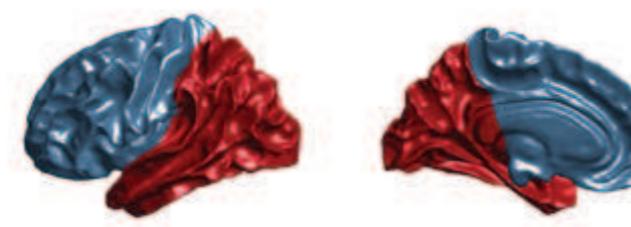
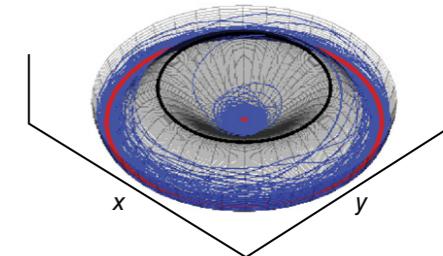
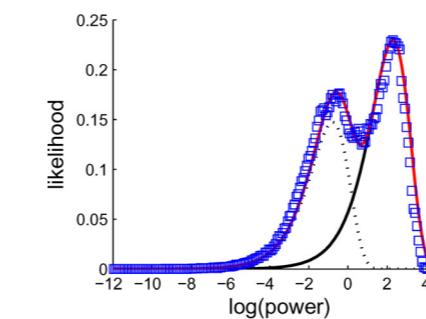
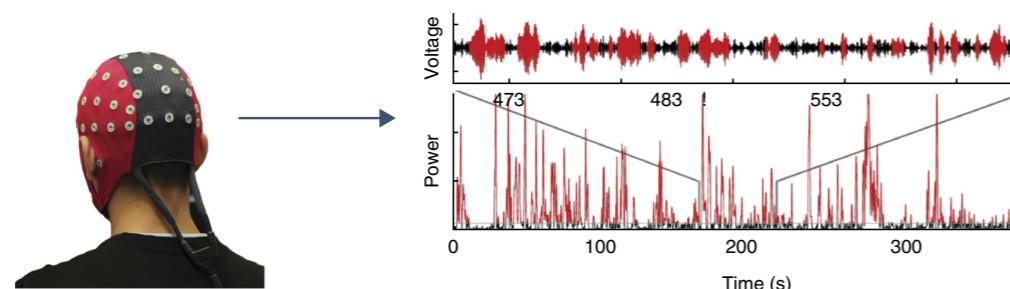
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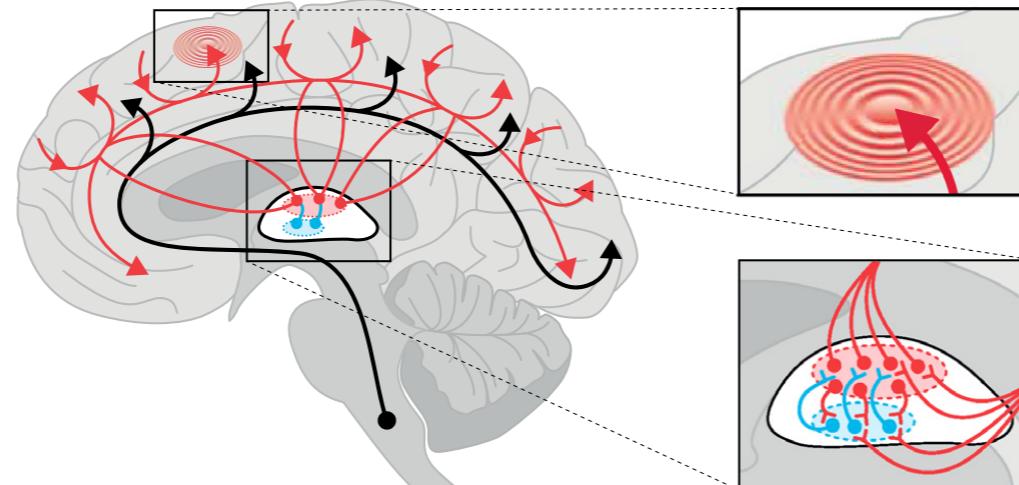
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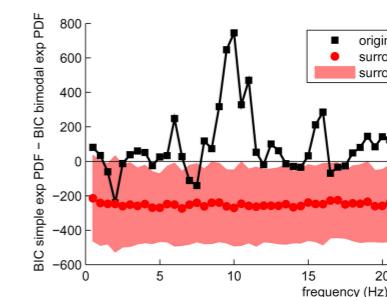
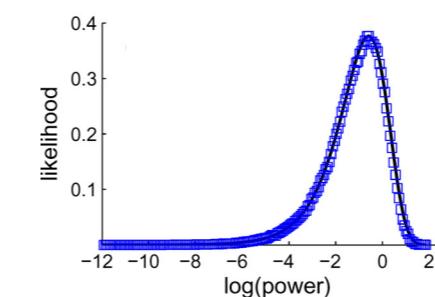
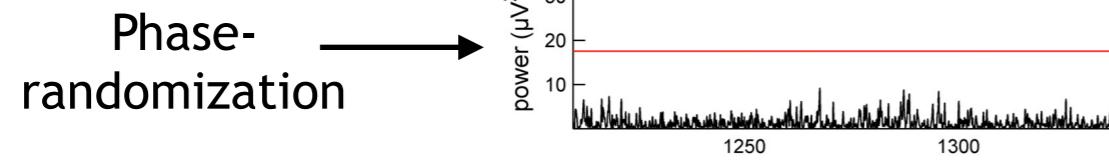
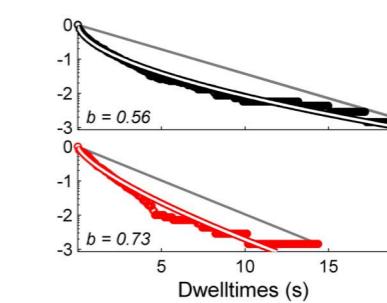
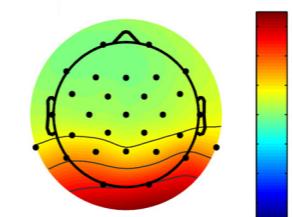
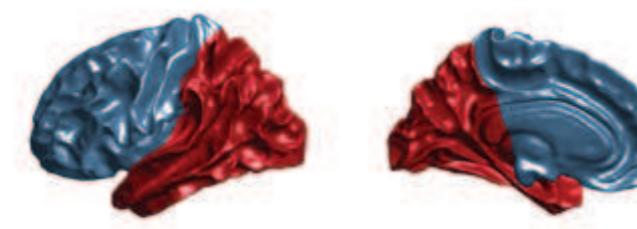
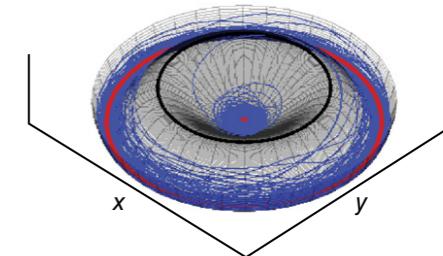
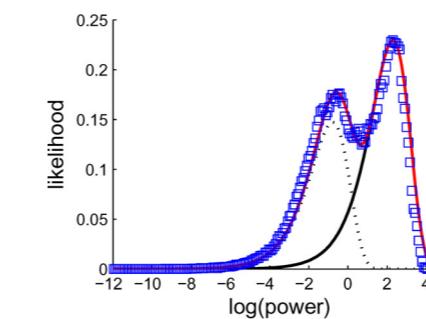
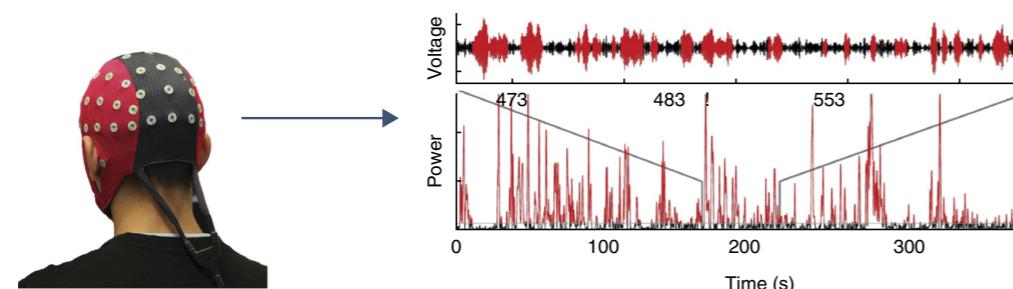
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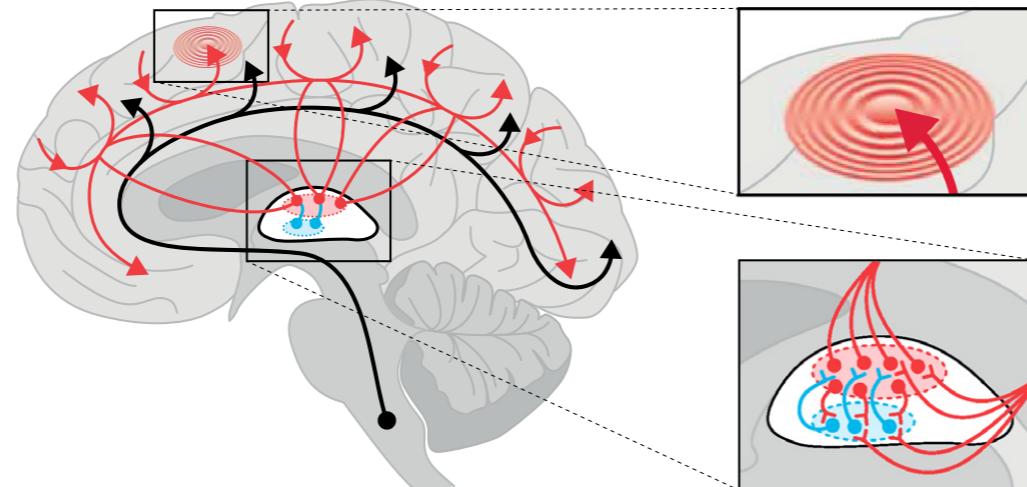


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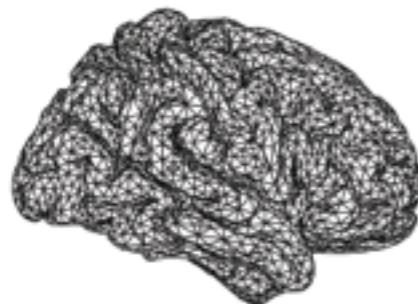


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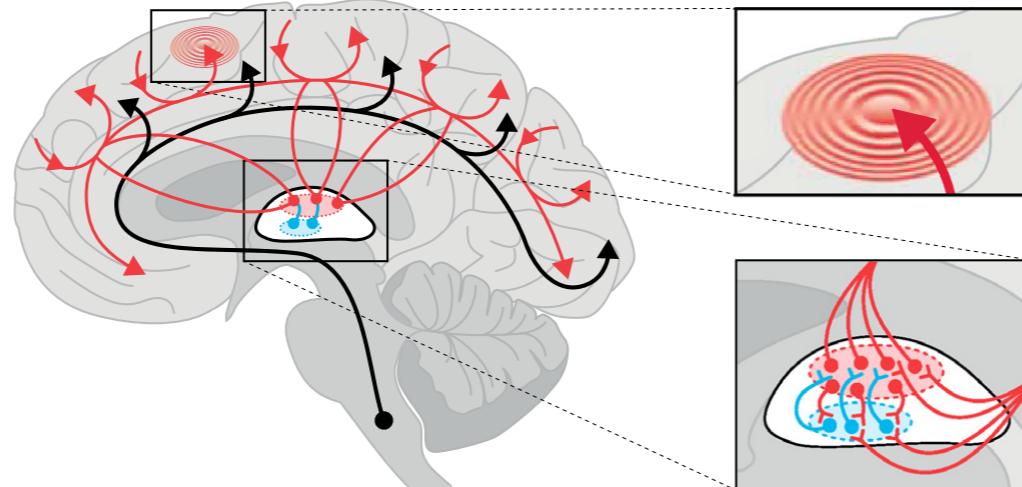
modes *noise*

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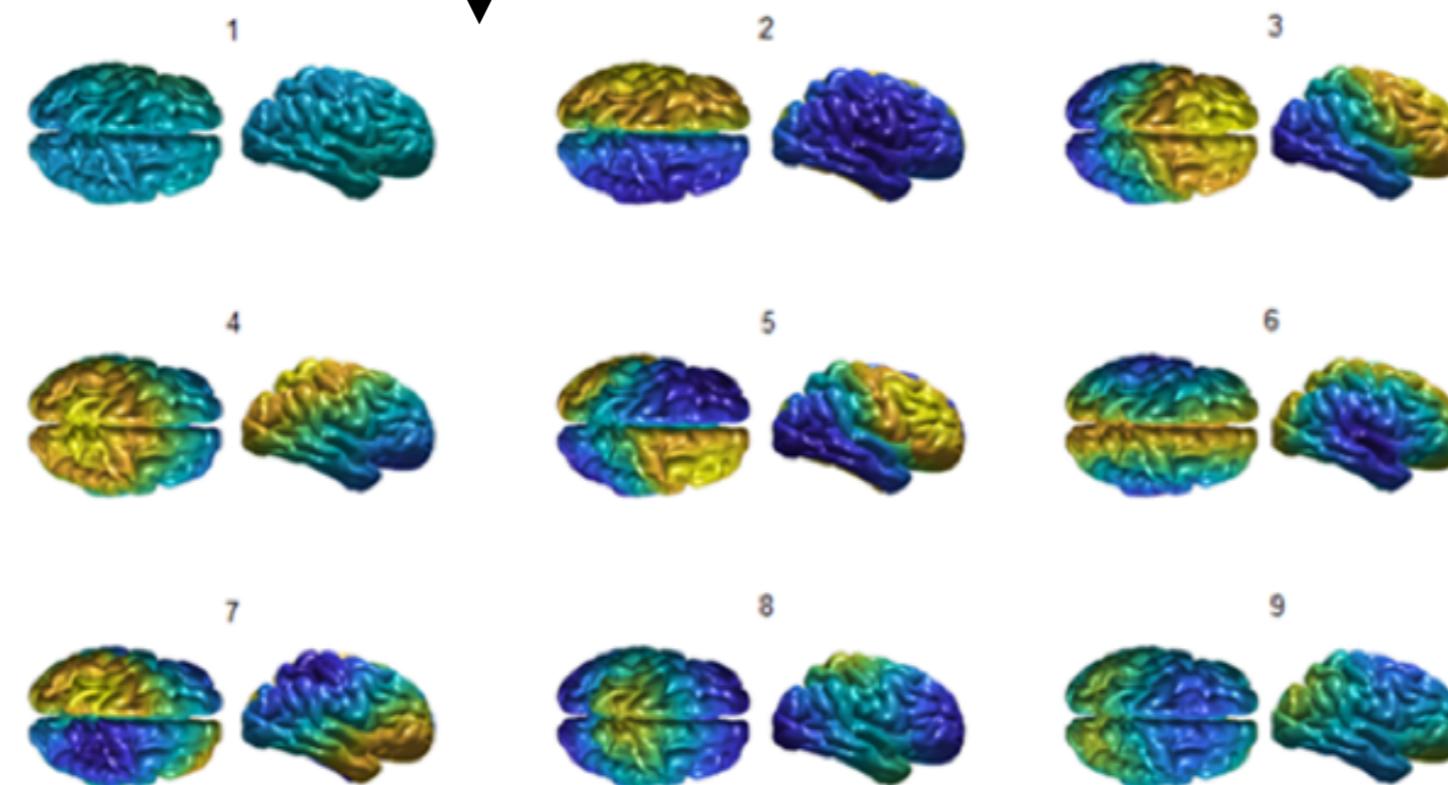


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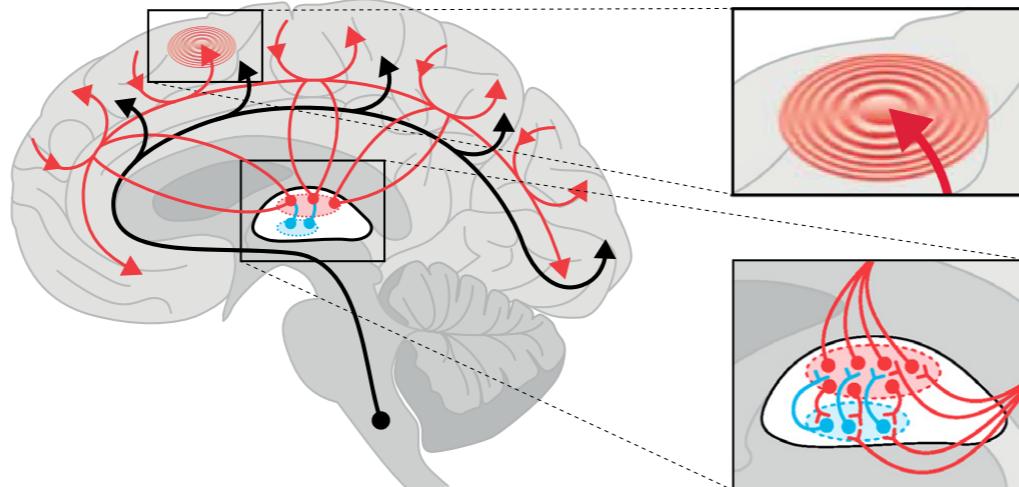


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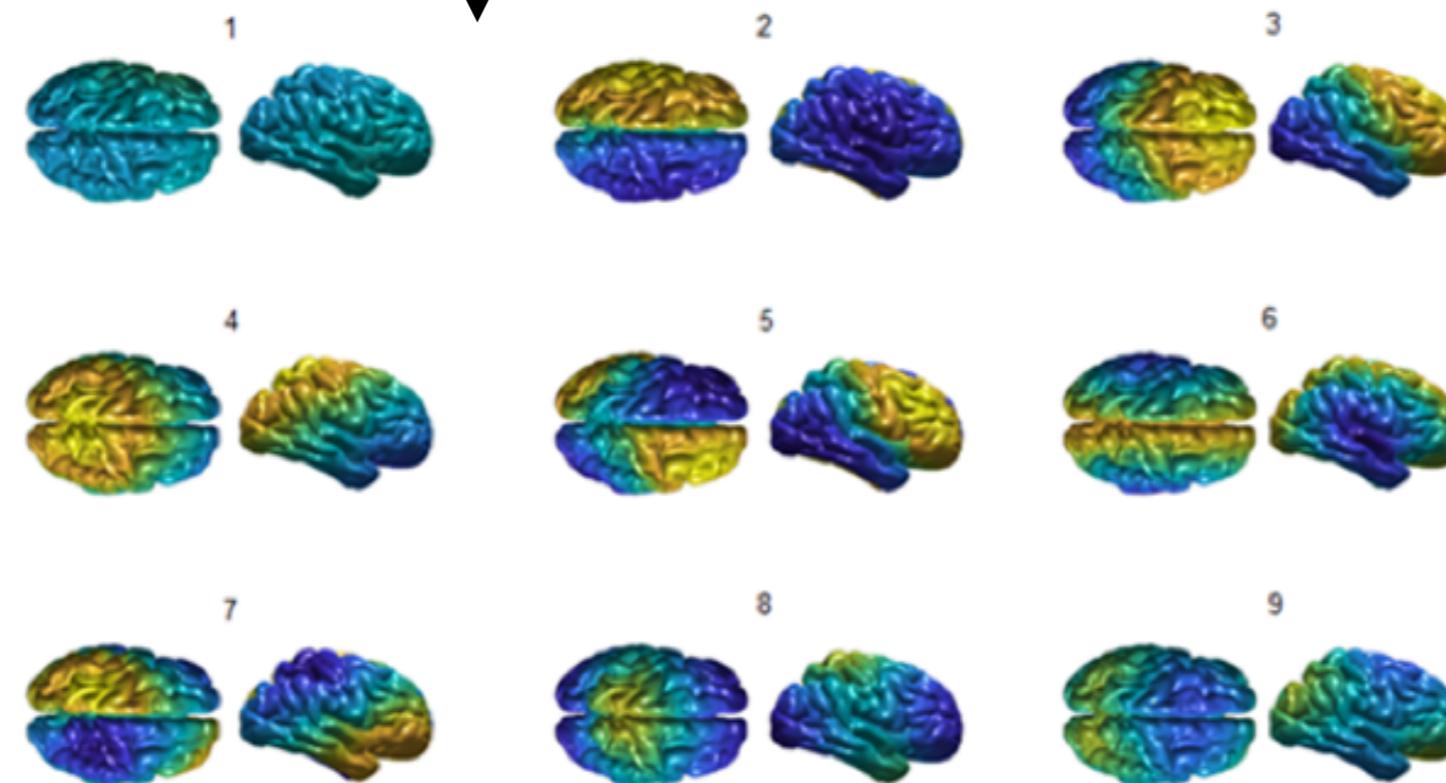
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Low frequency

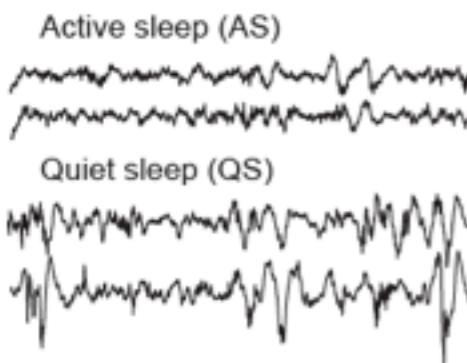


High frequency

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A Data acquisition

Multi-channel EEG

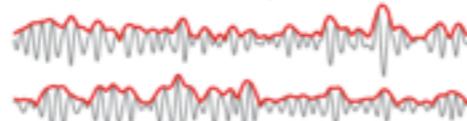


B Preprocessing

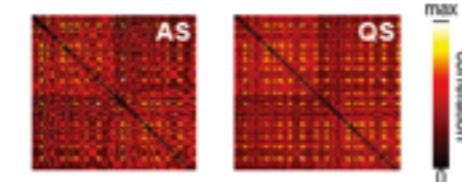
Head model



Amplitude envelopes

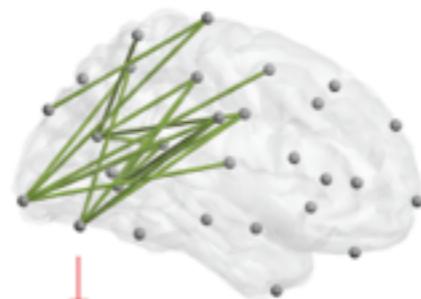


Connectivity

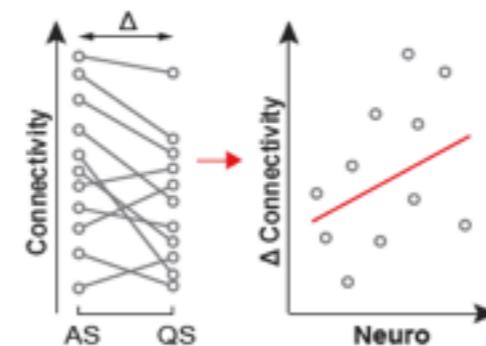


C Analysis

Network



Transitions

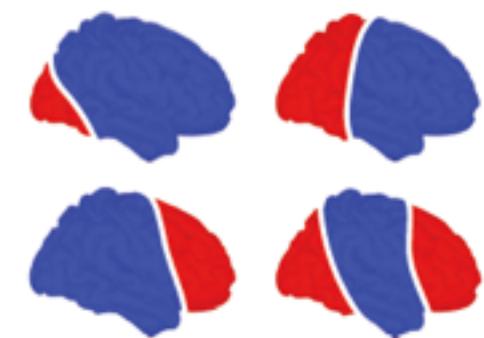


D Modeling

Cortical geometry



Eigenmodes



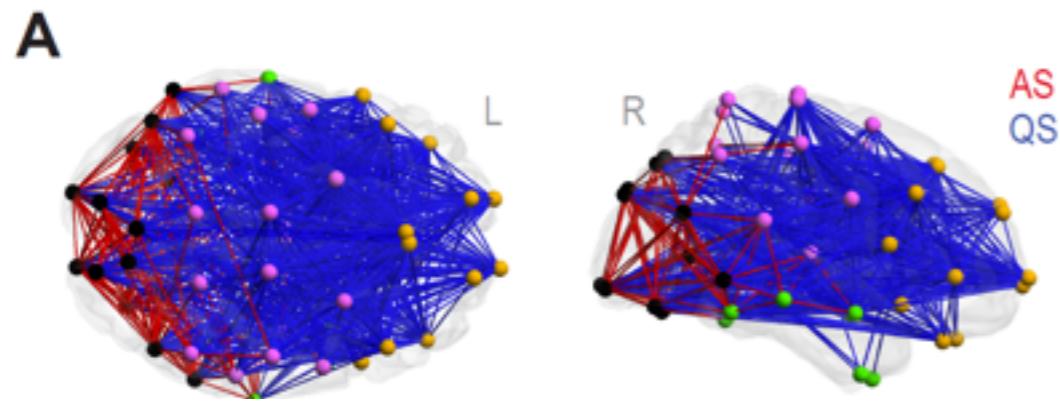
Scalp EEG data from extremely preterm (EP; $n=42$) and full-term (FT; $n=52$) neonates at term equivalent age

Source-reconstructed band limited (orthogonalized) functional connectivity

Contrasts of active sleep (AS) versus quiet sleep (QS) across groups

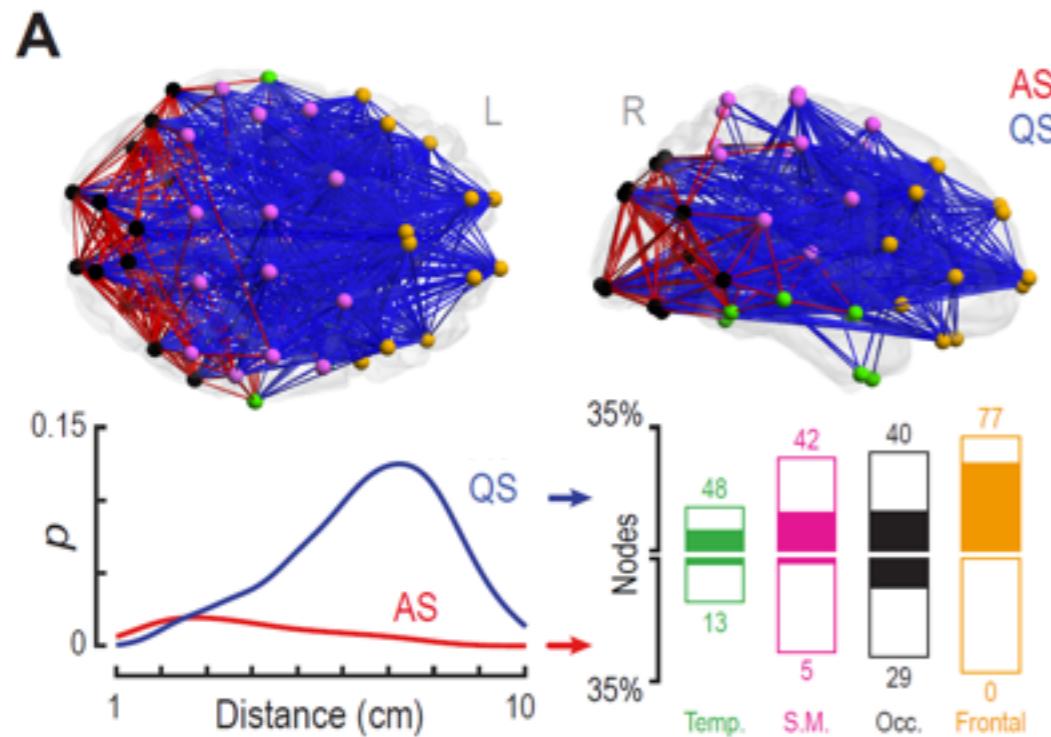
Neural field modelling

III: Neural fields + modes



Main effect of sleep (AS to QS):

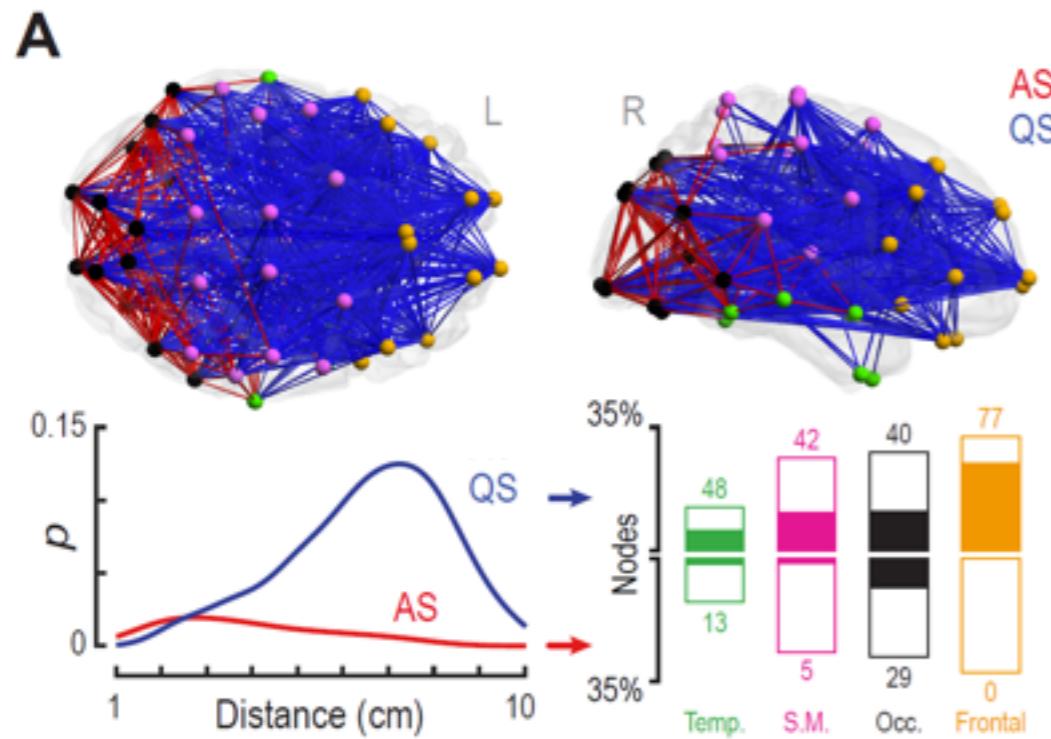
III: Neural fields + modes



Main effect of sleep (AS to QS):

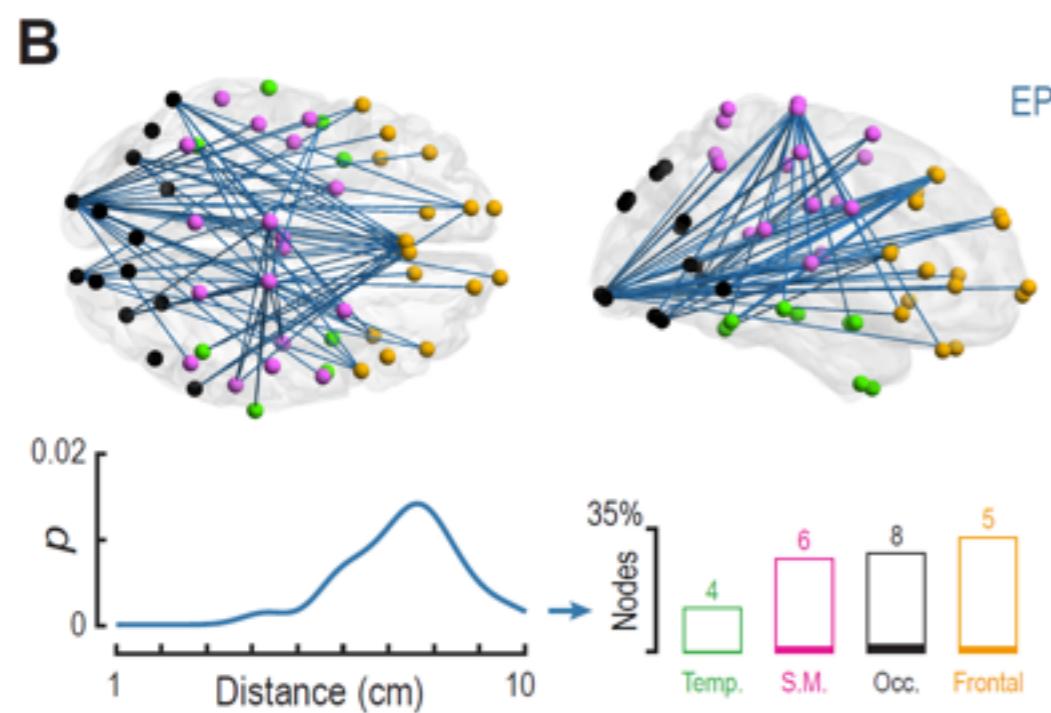
Transition heralds a reorganization toward greater, longer range and more anterior functional connectivity

III: Neural fields + modes



Main effect of sleep (AS to QS):

Transition heralds a reorganization toward greater, longer range and more anterior functional connectivity

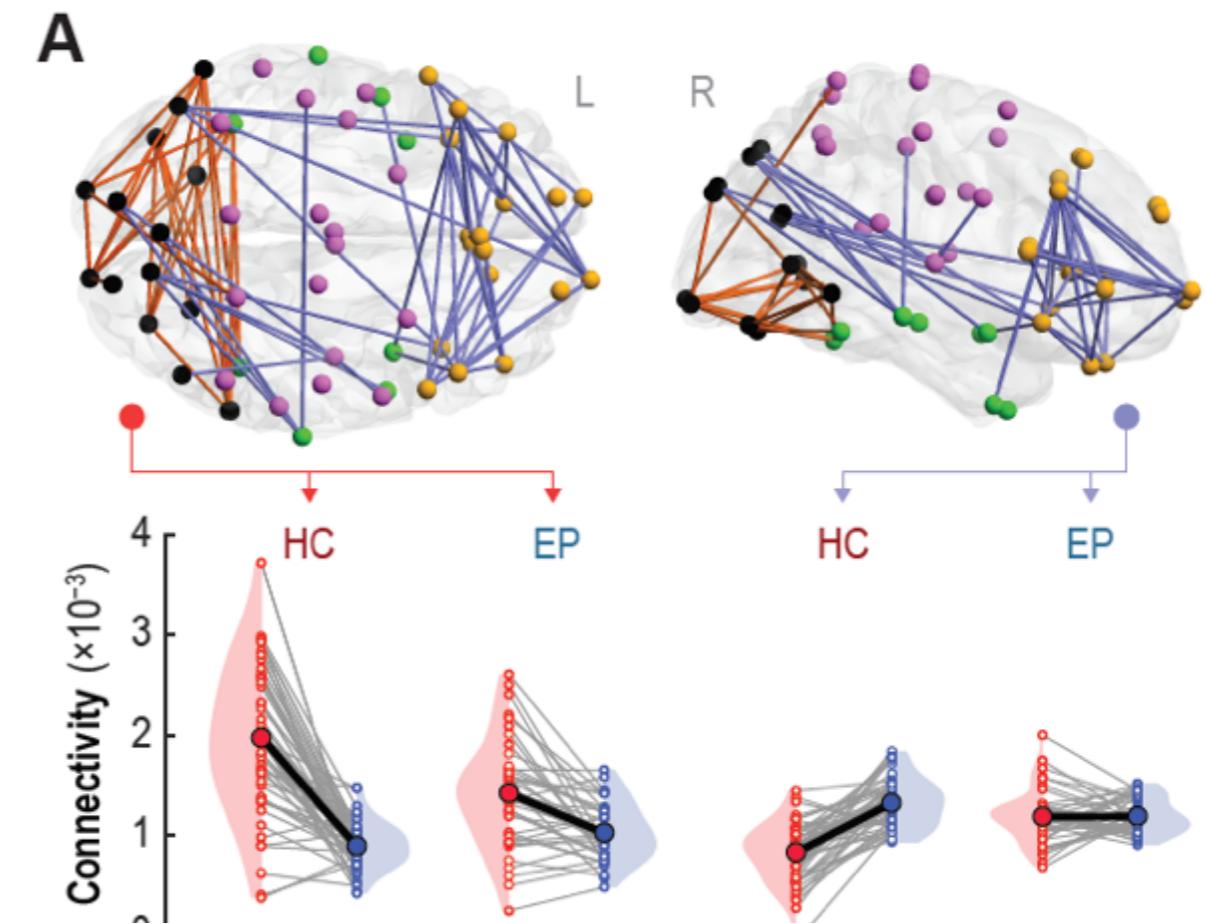


Main effect of group:

Across sleep states, preterm (EP) neonates possess a network of stronger long-range functional connectivity

III: Neural fields + modes

Sleep-group (interaction) effect:
Transition (AS to QS) in HC is
attenuated in EP in a largely
A-P network

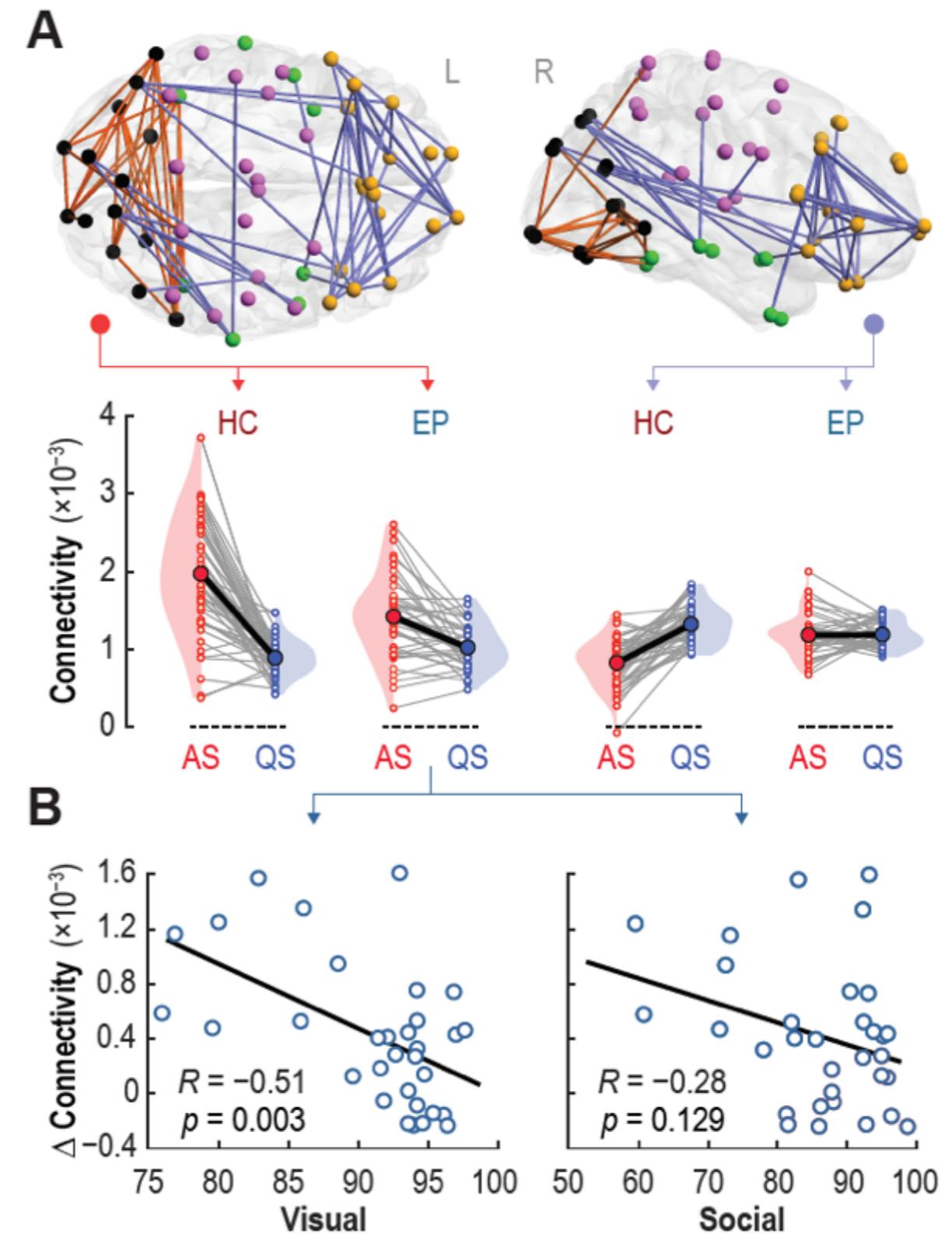


III: Neural fields + modes

Sleep-group (interaction) effect:

Transition (AS to QS) in HC is attenuated in EP in a largely A-P network

... which pre-empts visual performance at two years of life



III: Neural fields + modes



$$Y(\mathbf{x}, t) = \sum_j a_j m_j(\mathbf{x}) f(t) + \sigma \eta(\mathbf{x}, t),$$

III: Neural fields + modes



$$Y(x, t) = \sum_j a_j m_j(x) f(t) + \sigma \eta(x, t),$$

$$f(t) = \cos(\nu t) \cdot \cos(\omega t),$$

*carrier
frequency
(alpha)*

*low
frequency
fluctuations*

III: Neural fields + modes



solve
eigenmode
solution
on
neonatal
cortex

$$Y(\mathbf{x}, t) = \sum_j a_j m_j(\mathbf{x}) f(t) + \sigma \eta(\mathbf{x}, t),$$



$$\Delta_{\mathcal{G}} \psi_j(\nu_i) = \lambda_j \psi_j(\nu_i), \quad \forall \nu_i \in \mathcal{V}$$

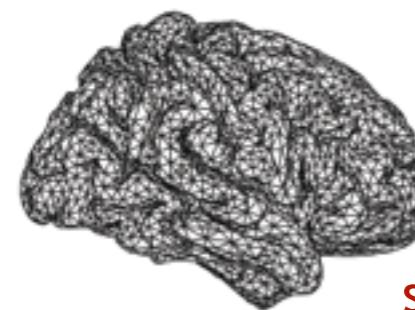
$$\Delta_{\mathcal{G}} = \frac{1}{2} \left((\mathbf{D} - \mathbf{A})^T (\mathbf{D} - \mathbf{A}) \right),$$

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III: Neural fields + modes



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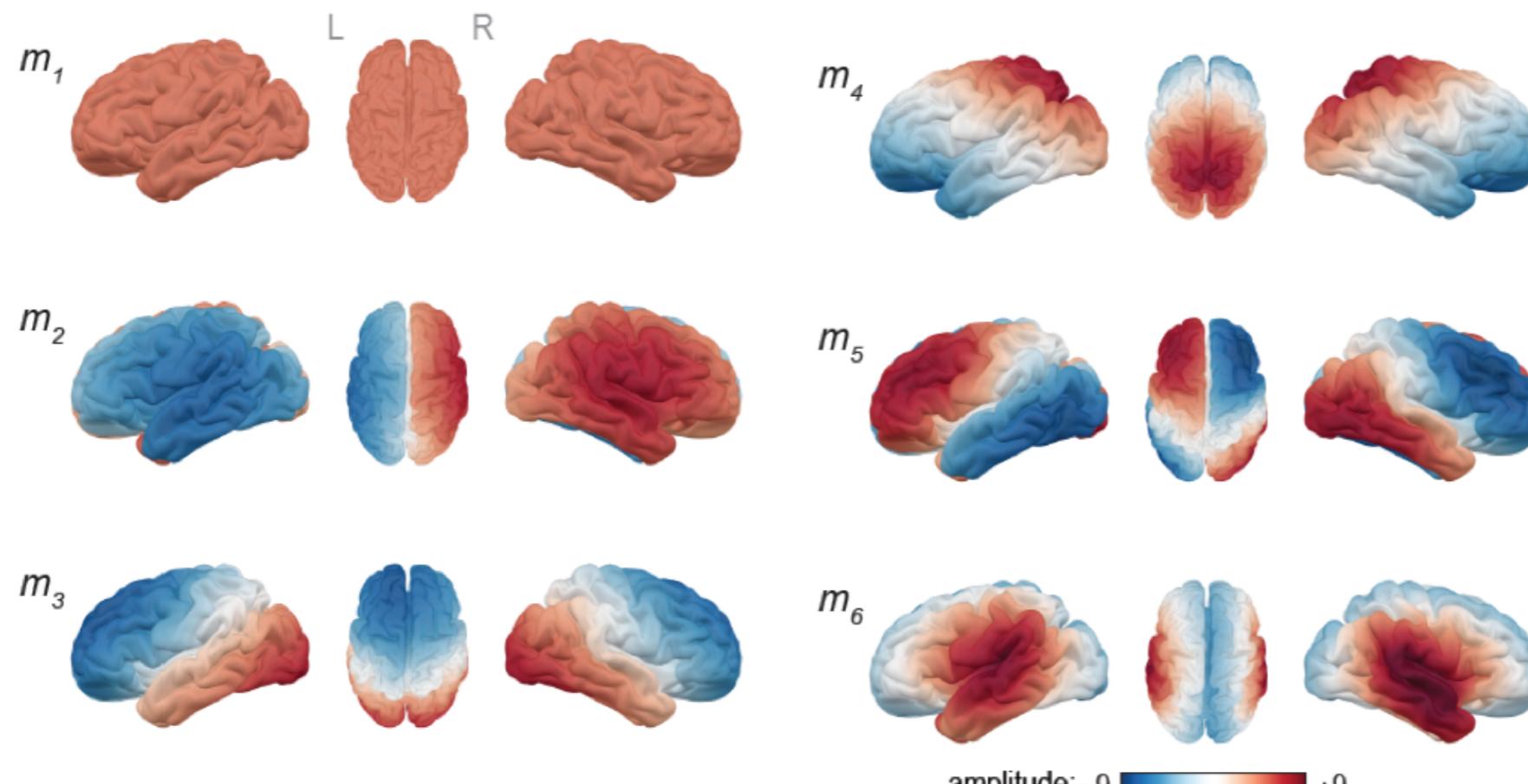
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III: Neural fields + modes



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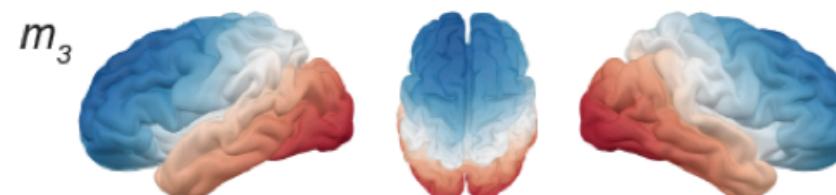
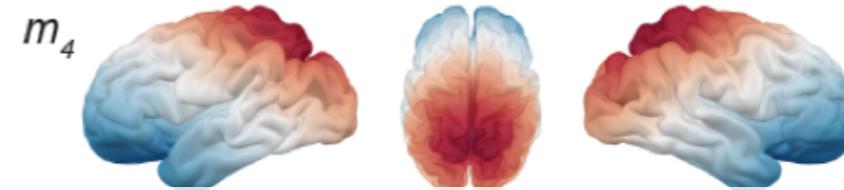
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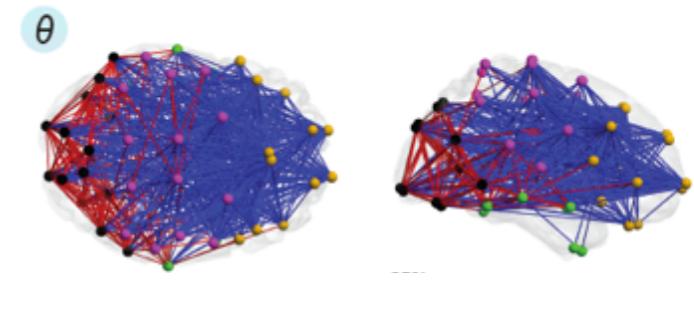
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amplitude: -9

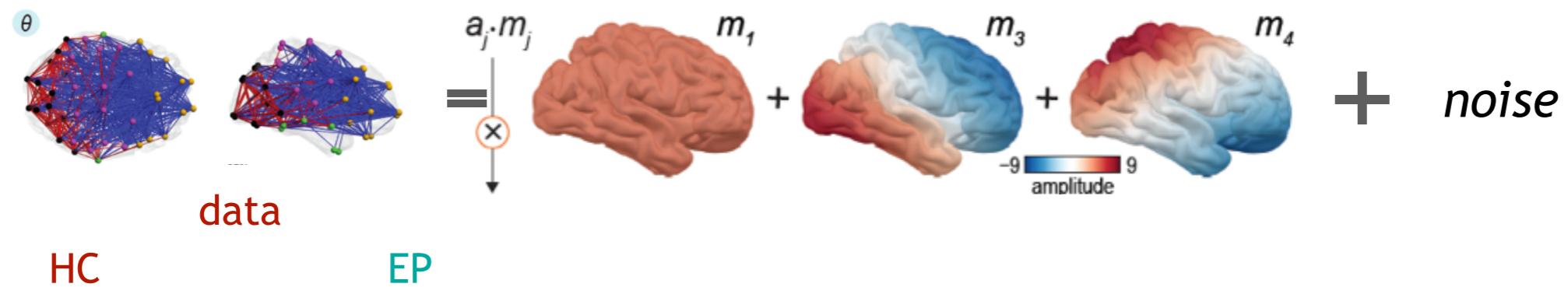


Choose first
(global) third and
fourth (A-P)
modes and solve
for each neonate

III: Neural fields + modes

$$Y(\mathbf{x}, t) = \sum_j a_j m_j(\mathbf{x}) f(t) + \sigma \eta(\mathbf{x}, t),$$

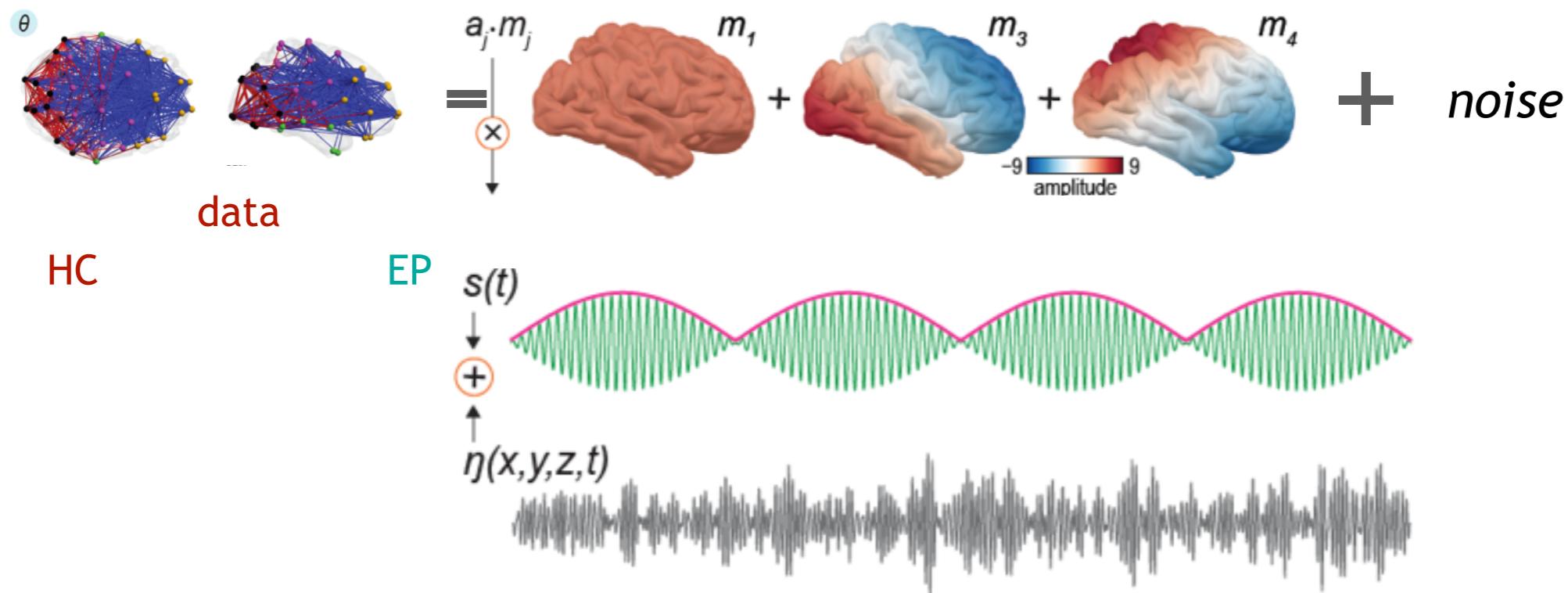
... and solve for each neonate



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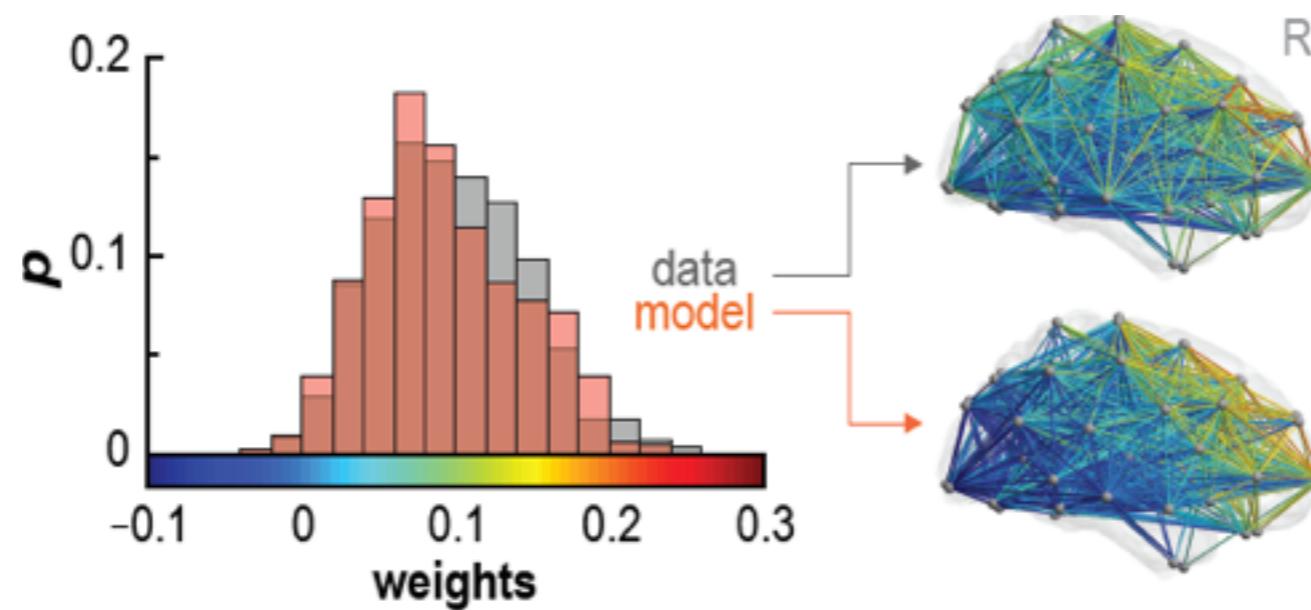
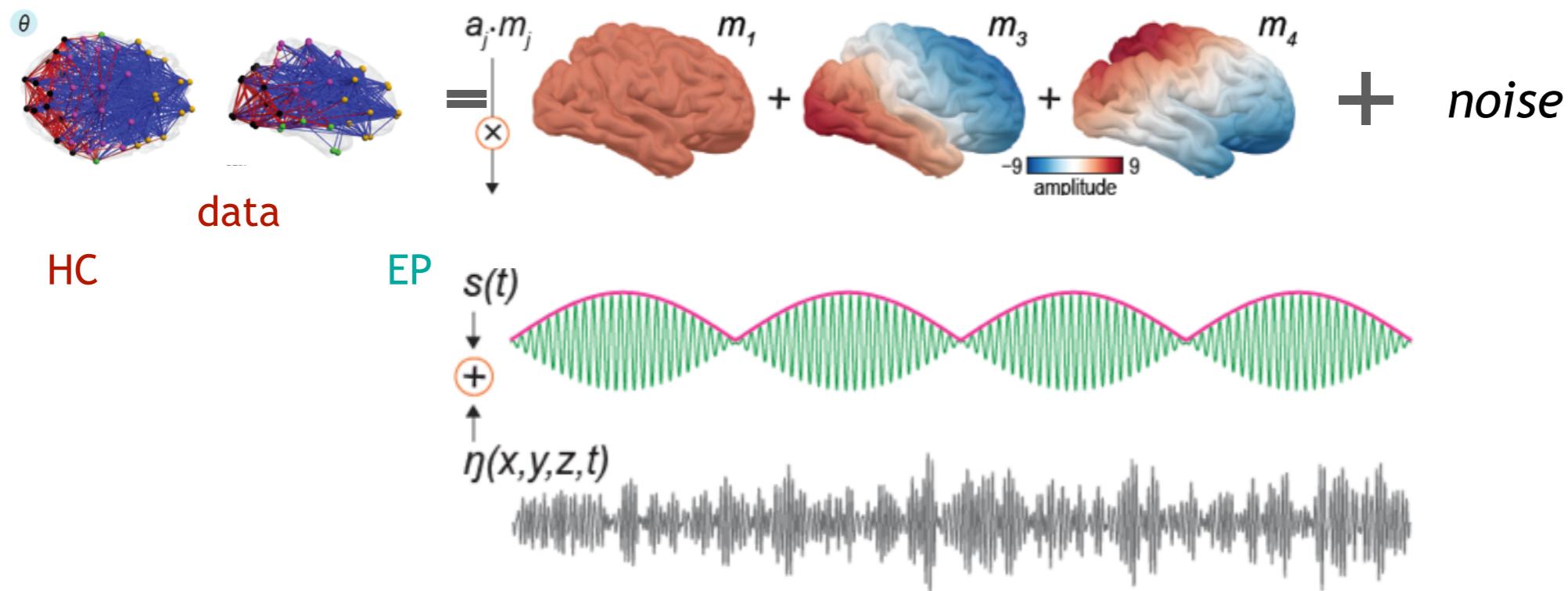
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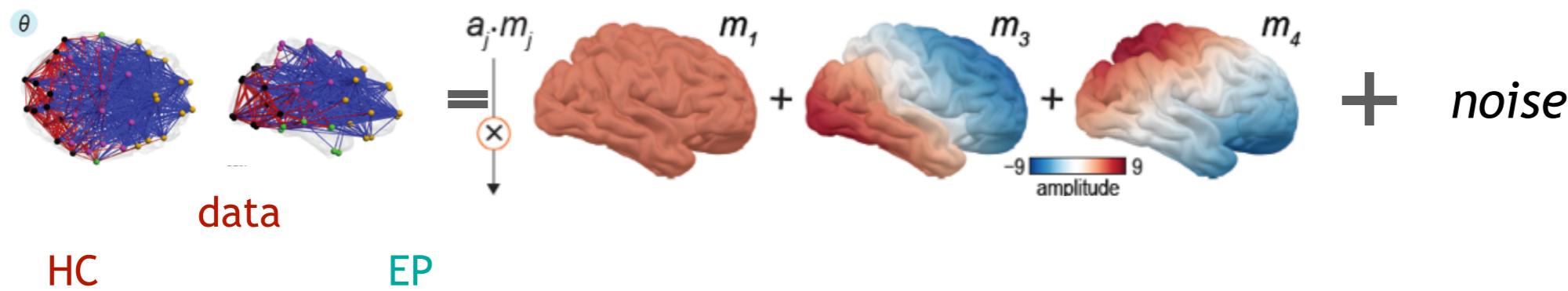
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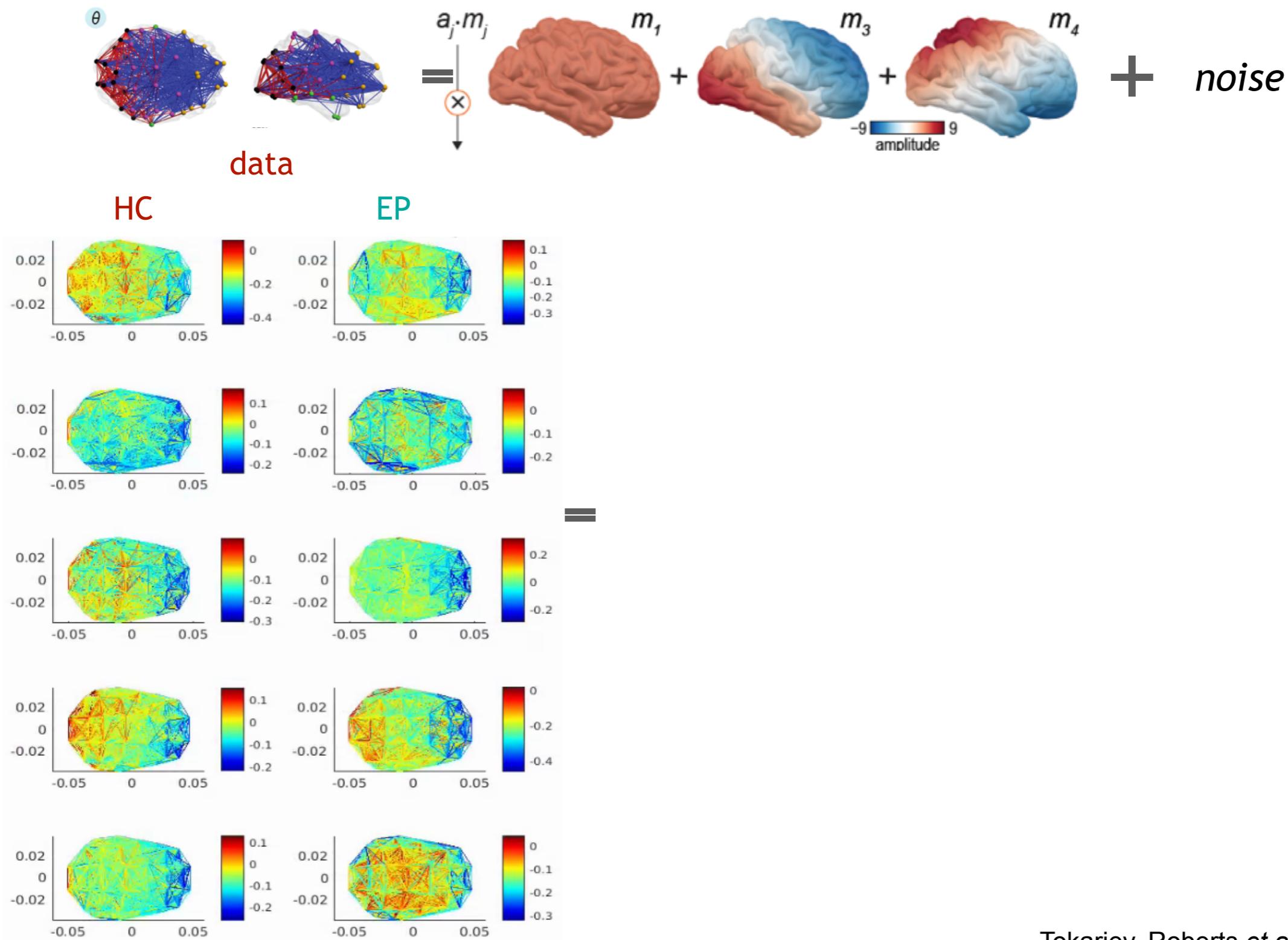


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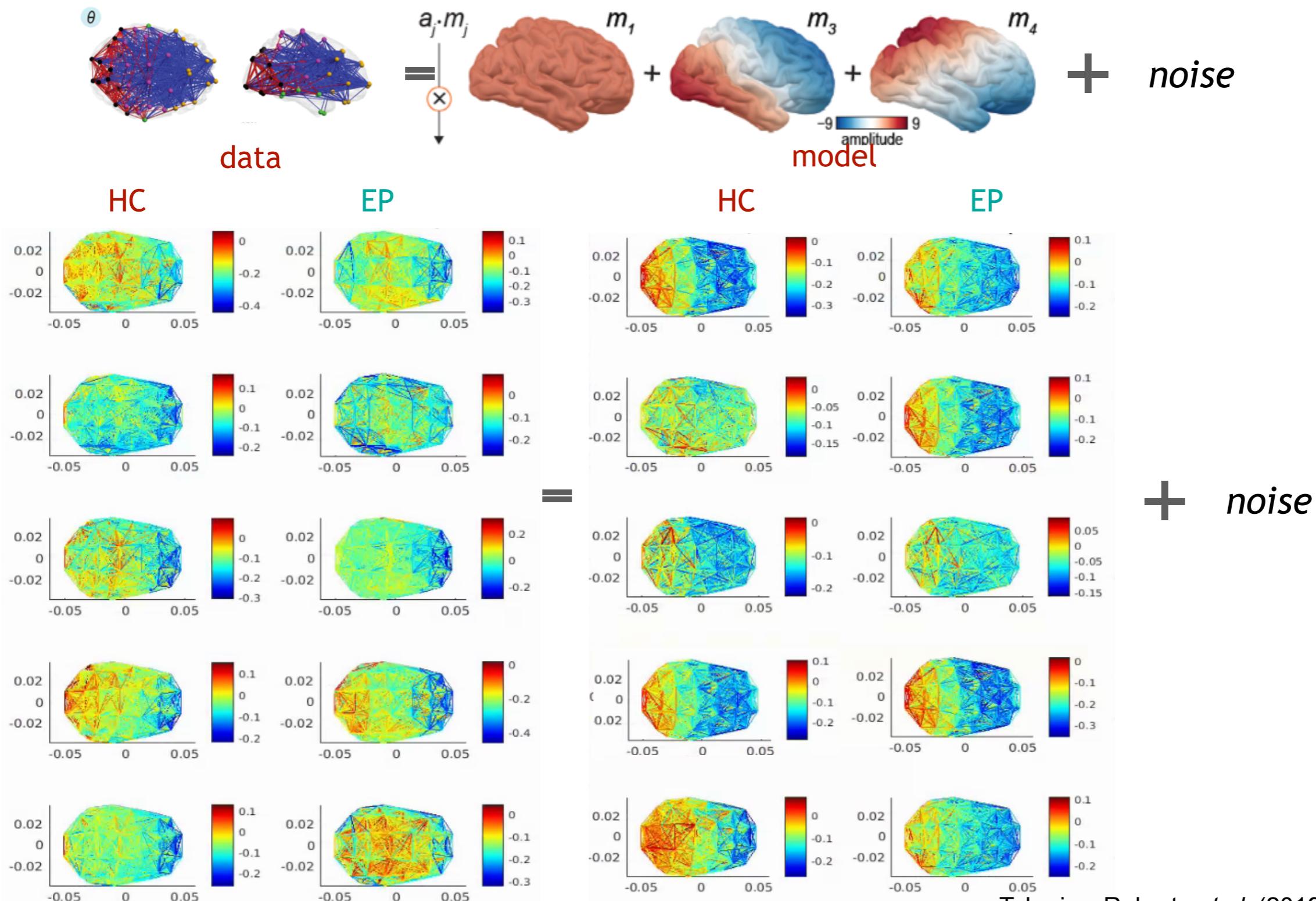
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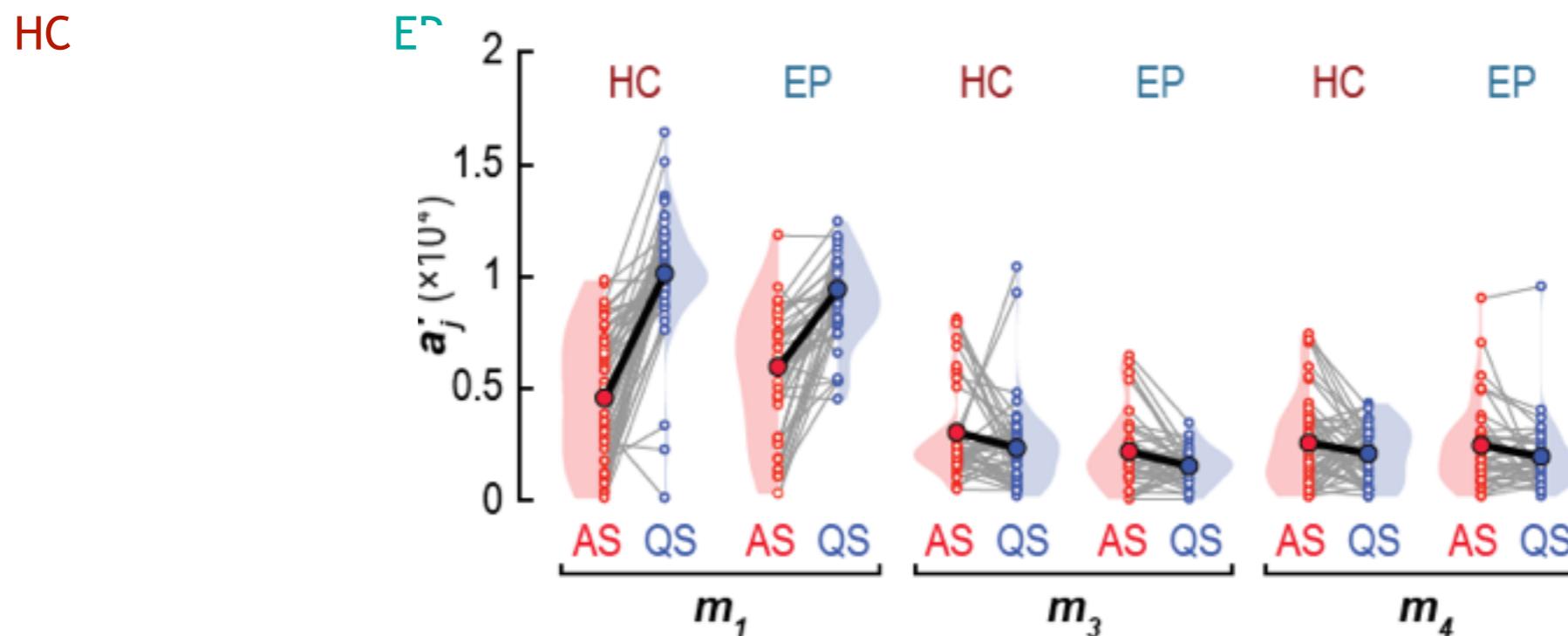
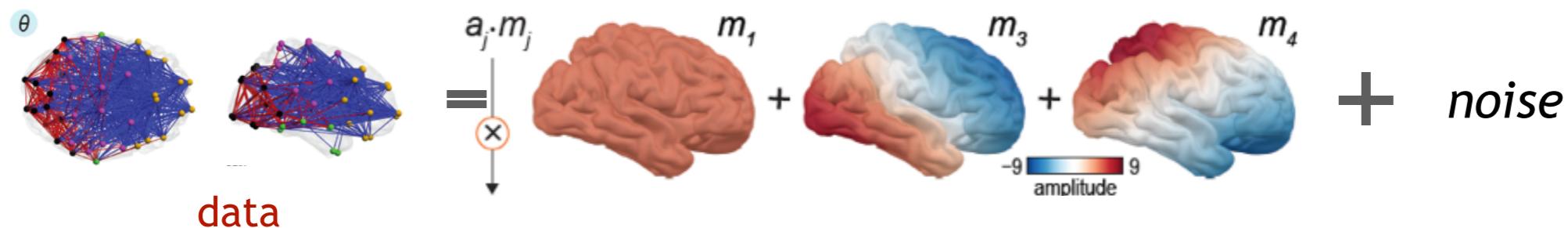
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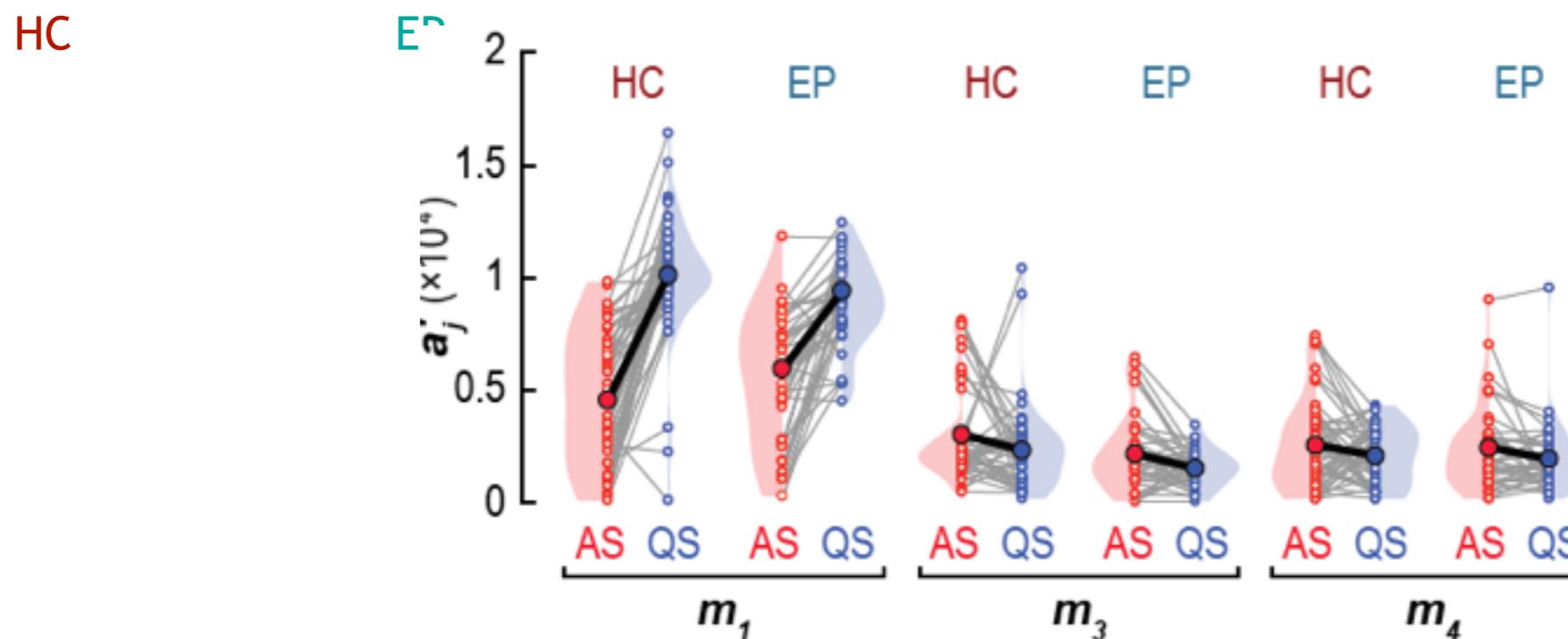
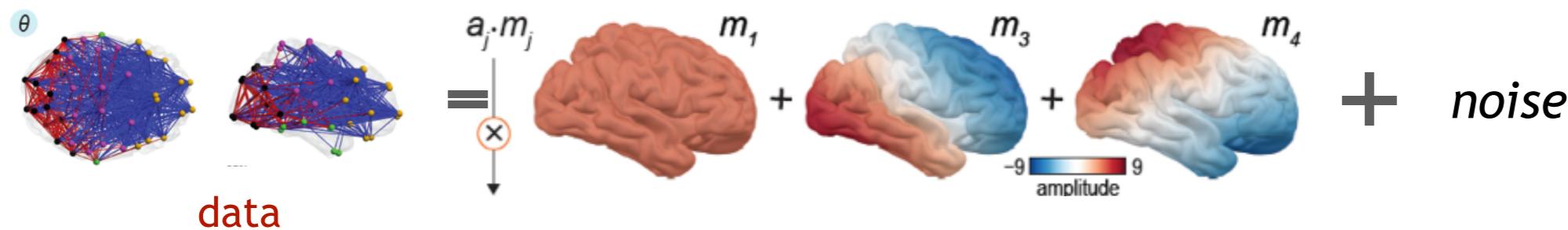
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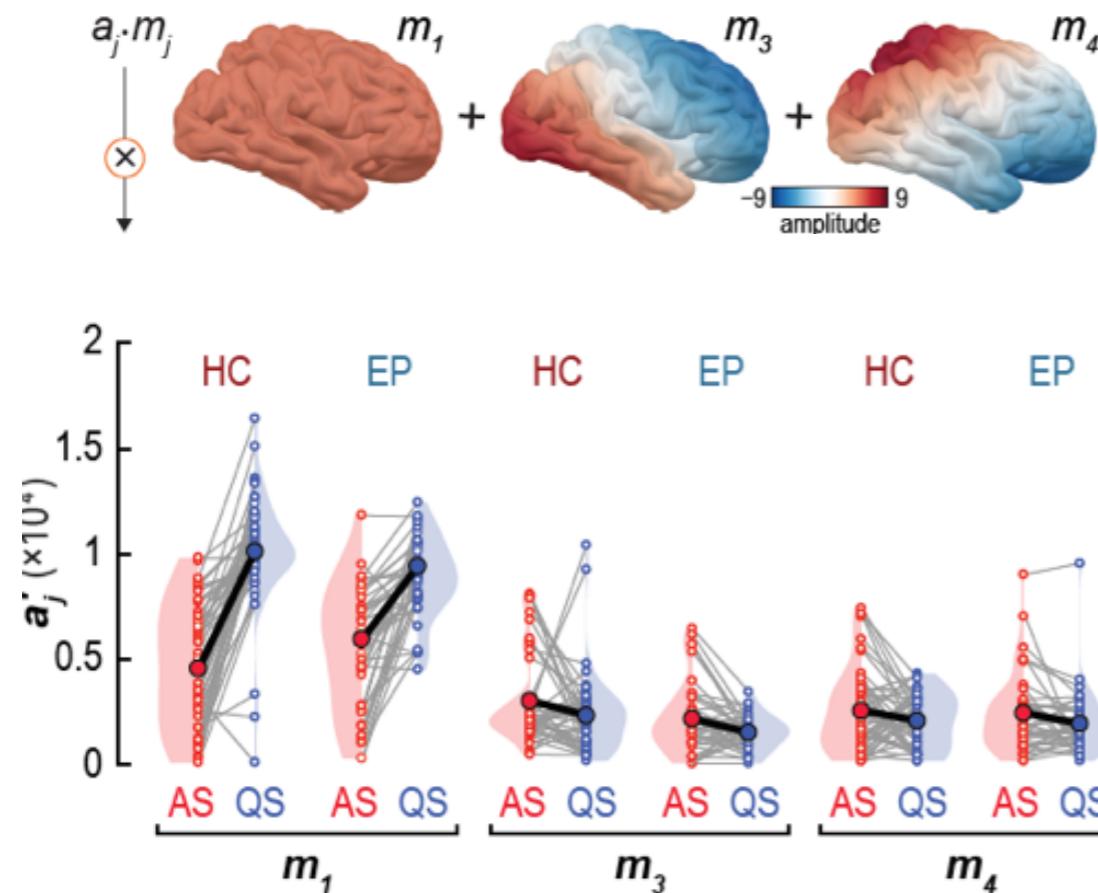
... and solve for each neonate



$$F_{1,92} = 7.76, p = 0.006$$

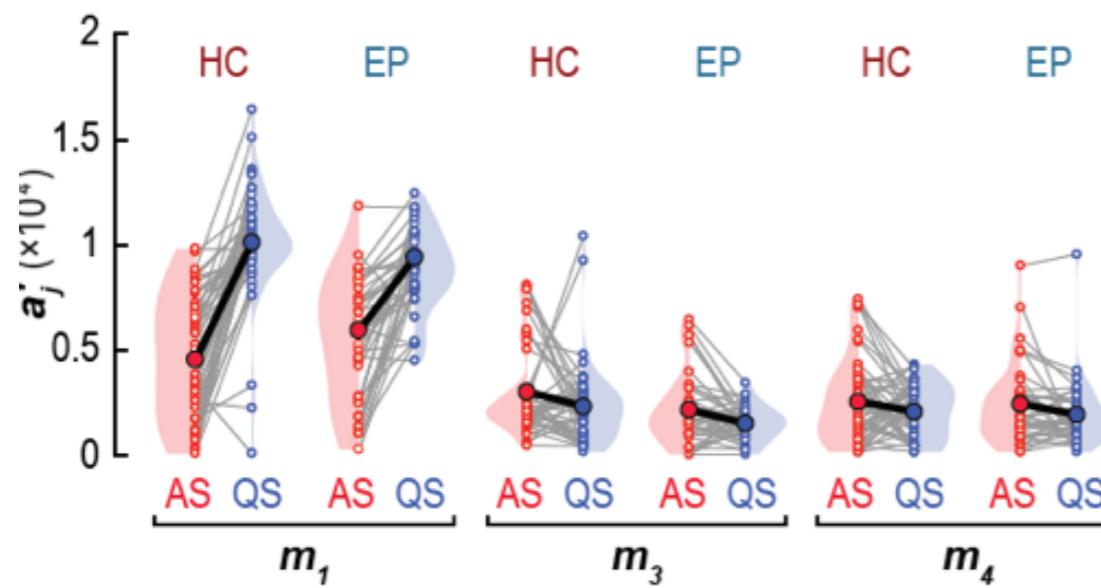
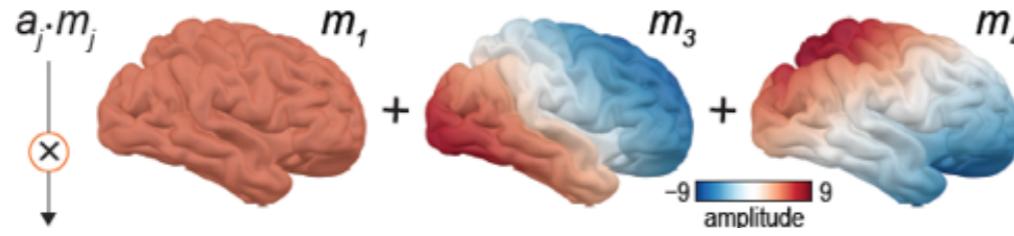
Significant group by sleep effect

III: Neural fields + modes



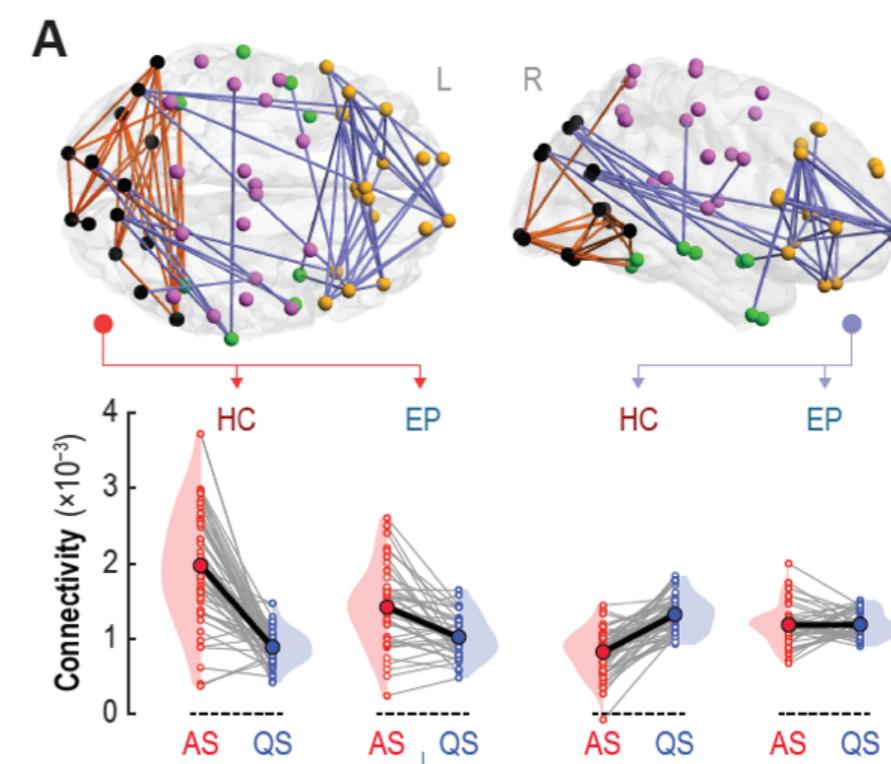
*Sleep-group (interaction) in
brain modes*

III: Neural fields + modes



Sleep-group (interaction) in brain modes

Sleep-group (interaction) in brain networks

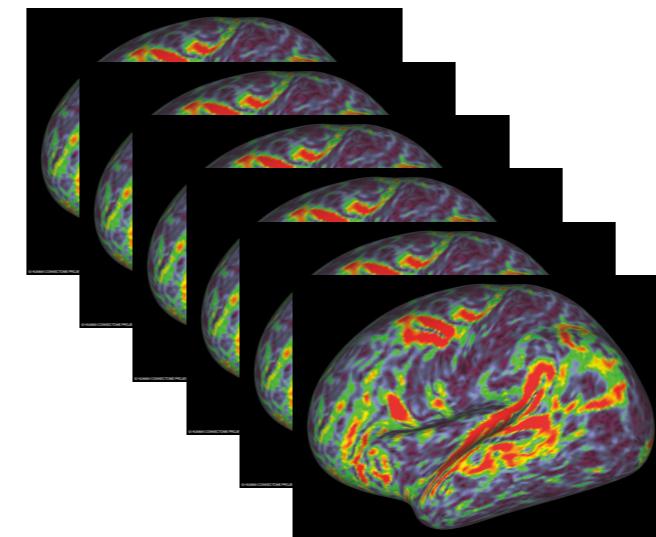


III: Neural fields + modes



CONNECTOME
COORDINATION FACILITY

1. 1000+ rs and 700 task fMRI



Ye Tian, Daniel Margulies, Andrew Zalesky

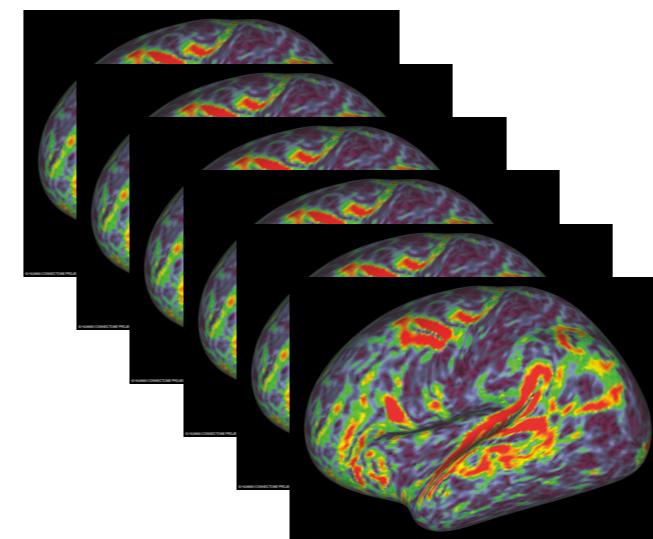


III: Neural fields + modes



CONNECTOME
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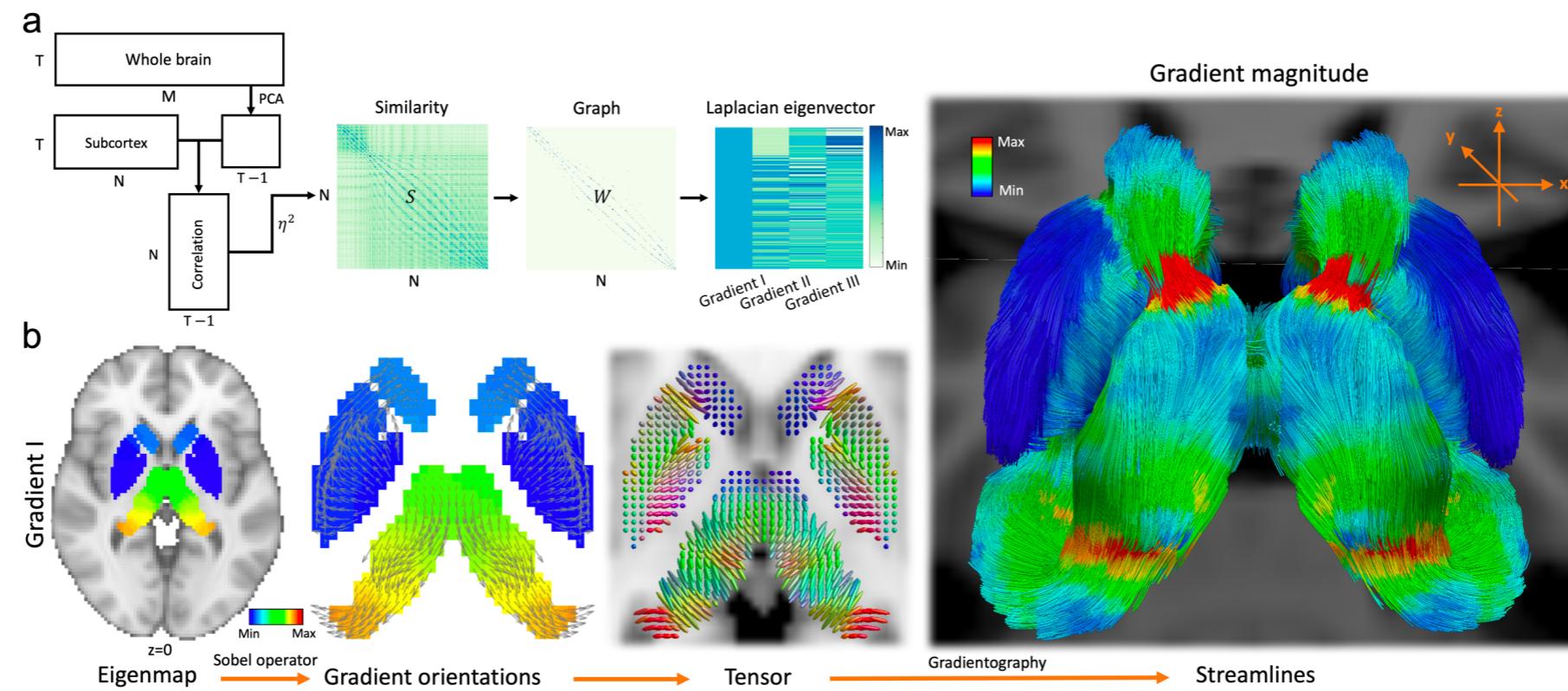
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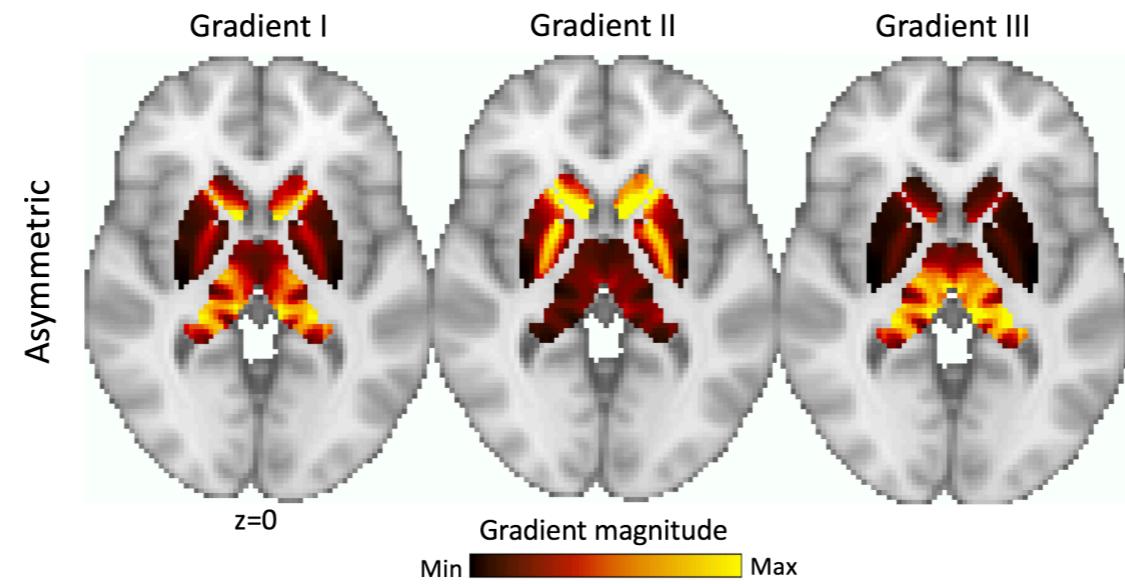


2. Eigenmodes of functional connectivity gradients



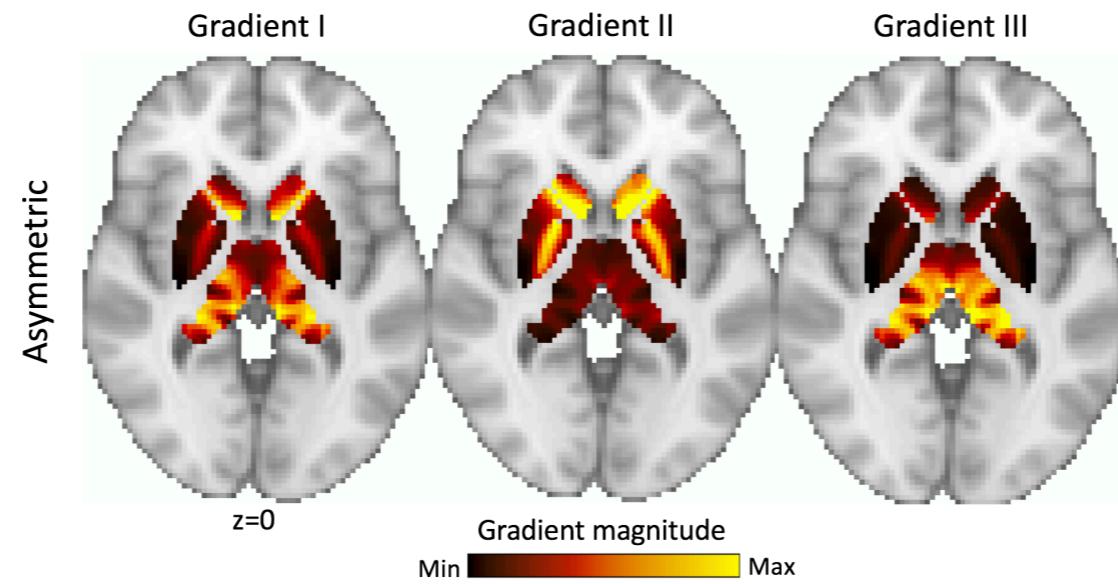
III: Neural fields + modes

3. Subcortical gradients modes

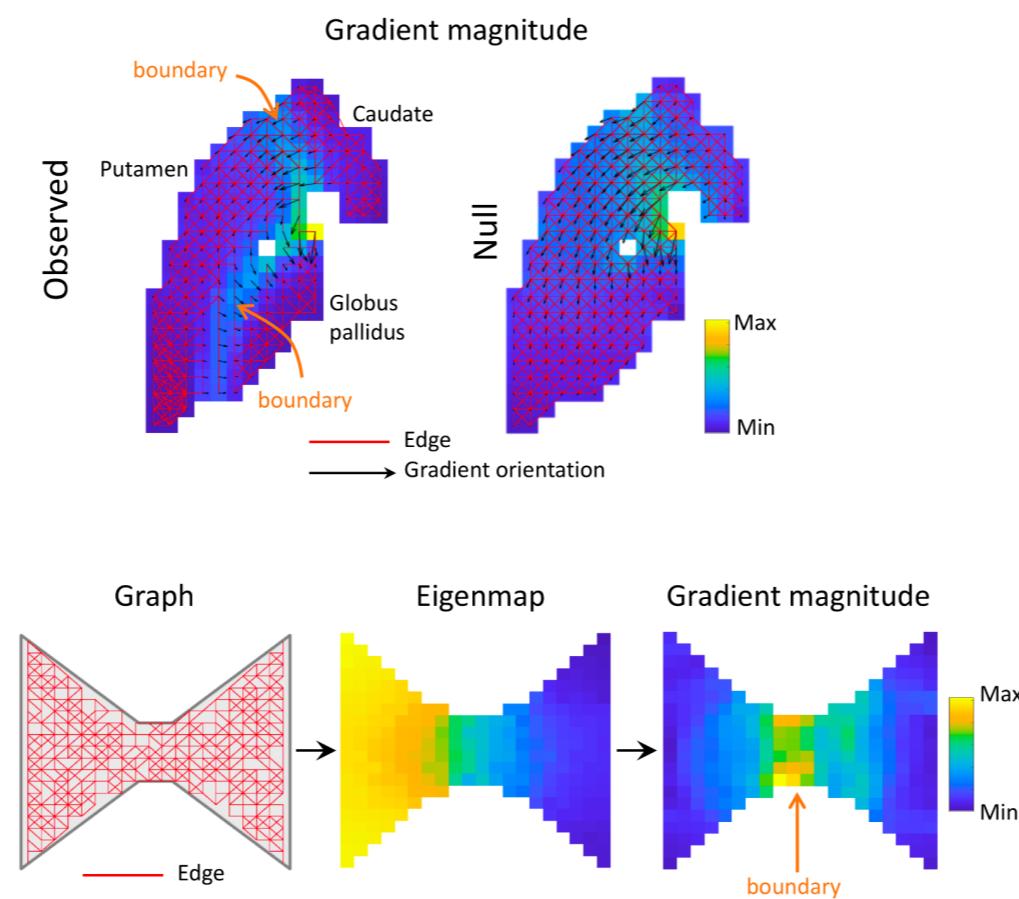


III: Neural fields + modes

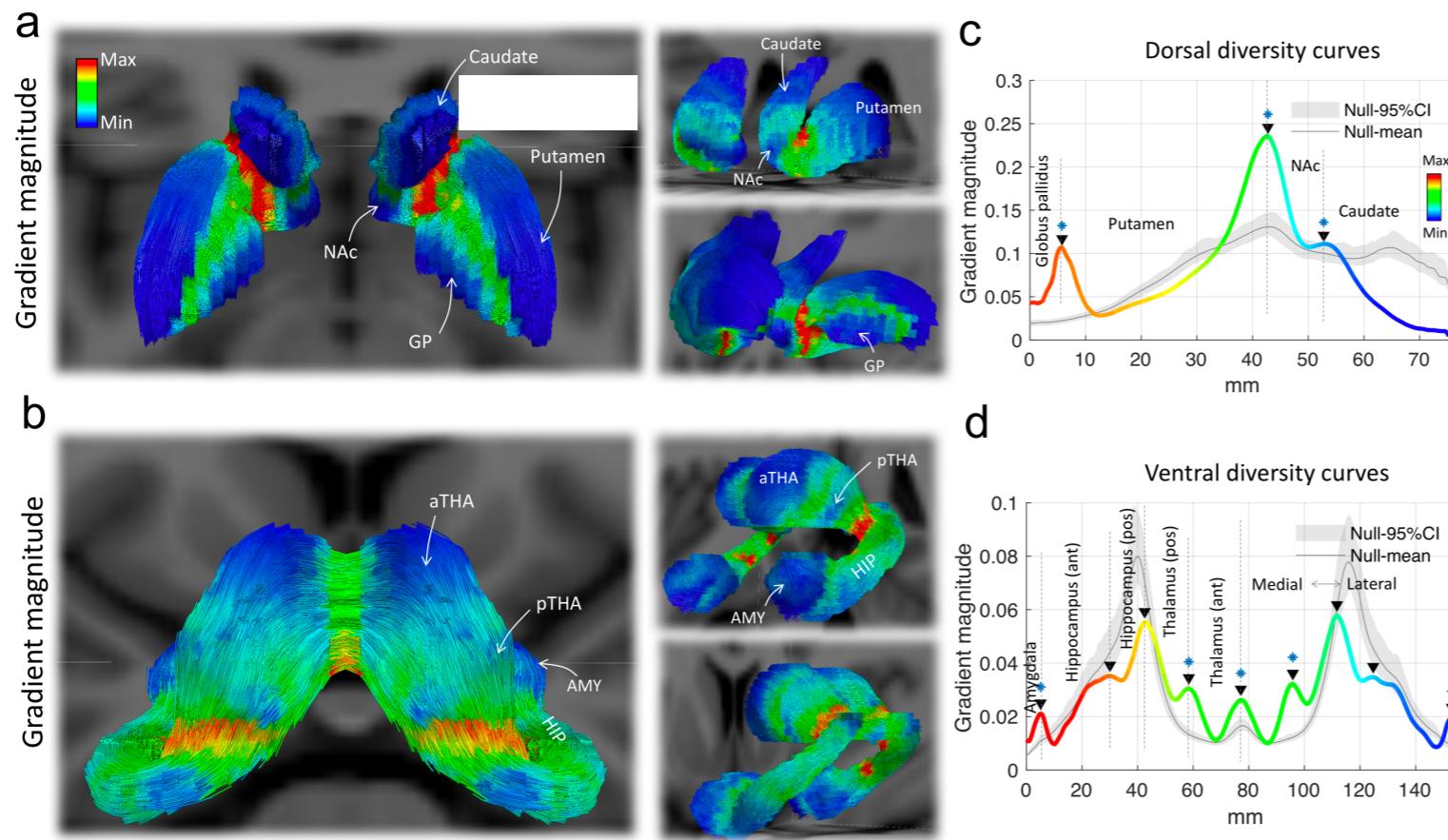
3. Subcortical gradients modes



4. Test empirical gradients against geometrically constrained nulls

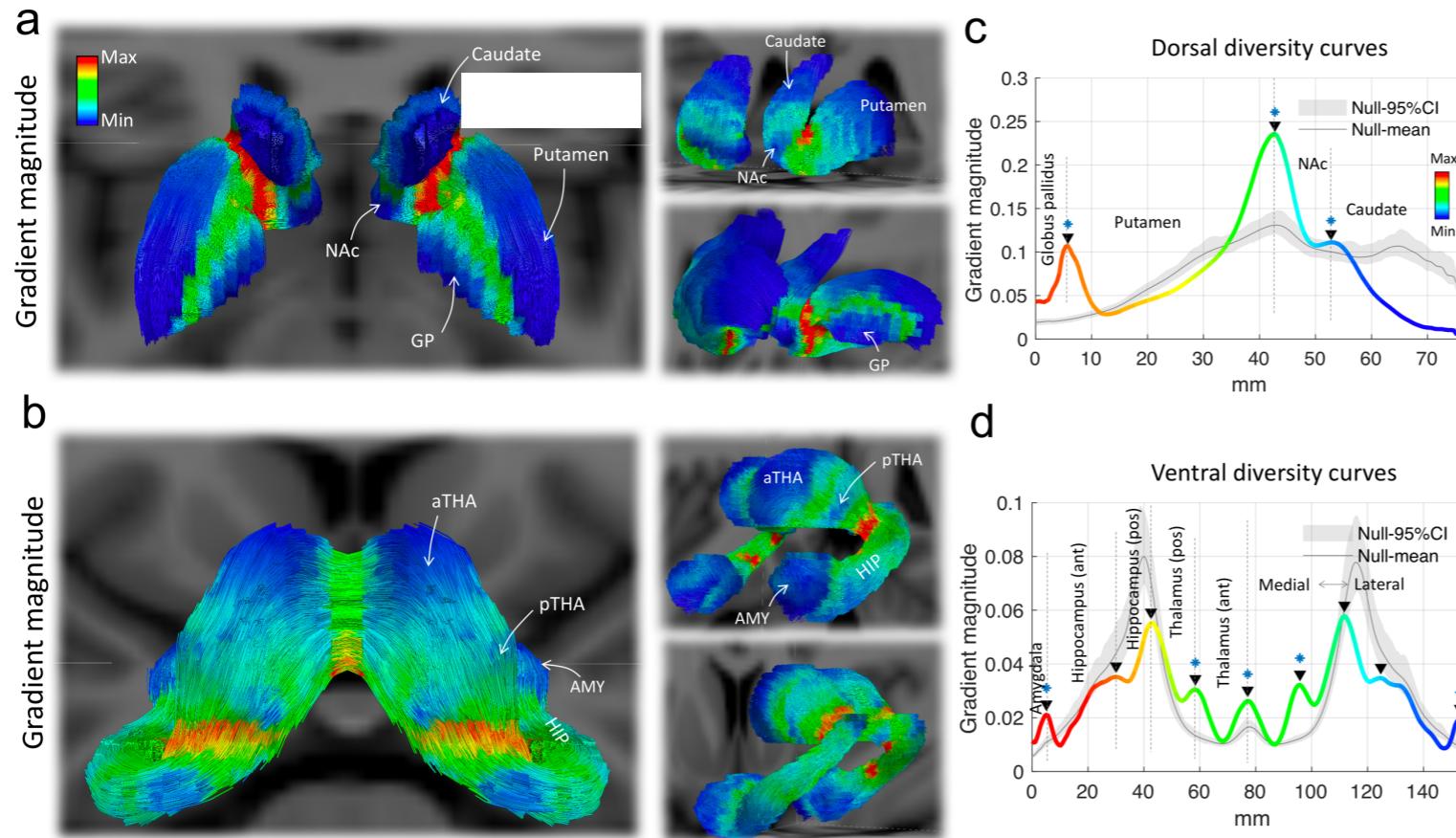


III: Neural fields + modes



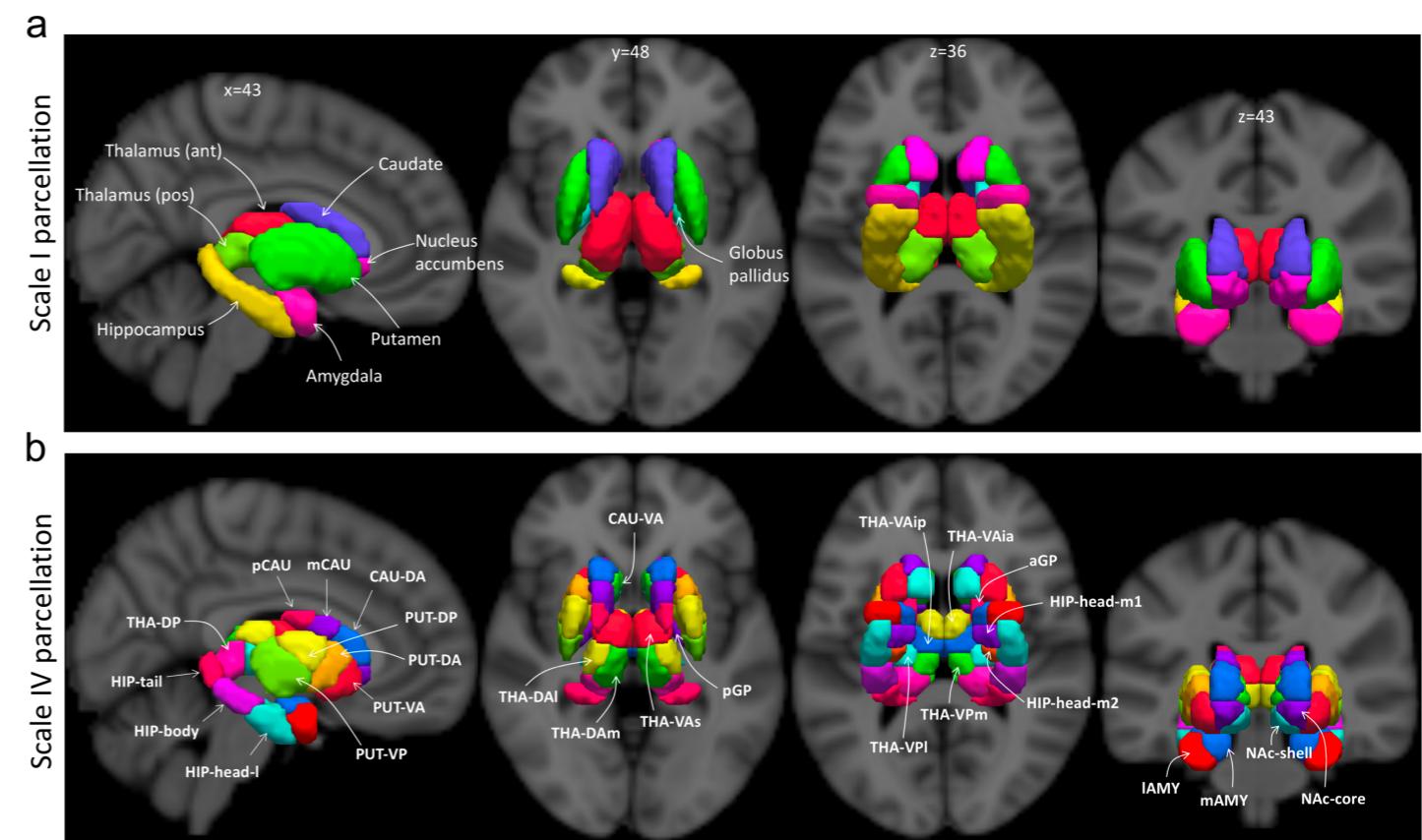
3. Gradient break-points

III: Neural fields + modes



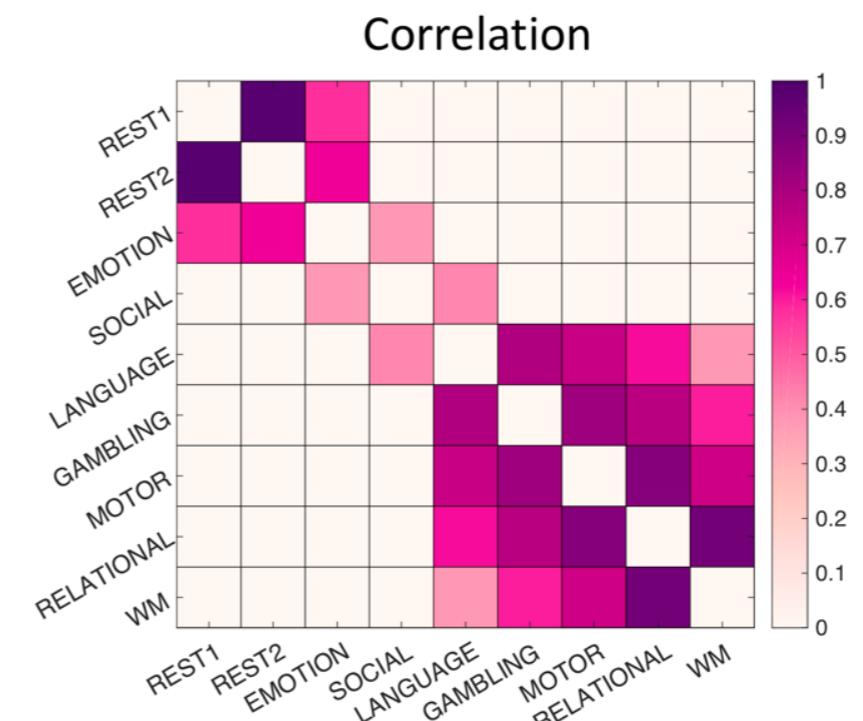
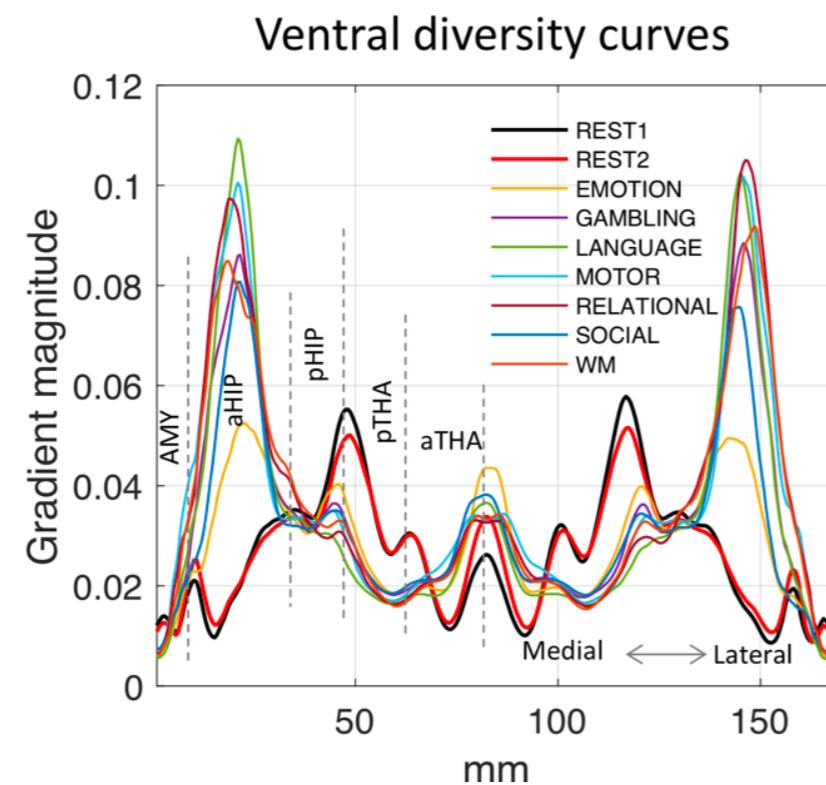
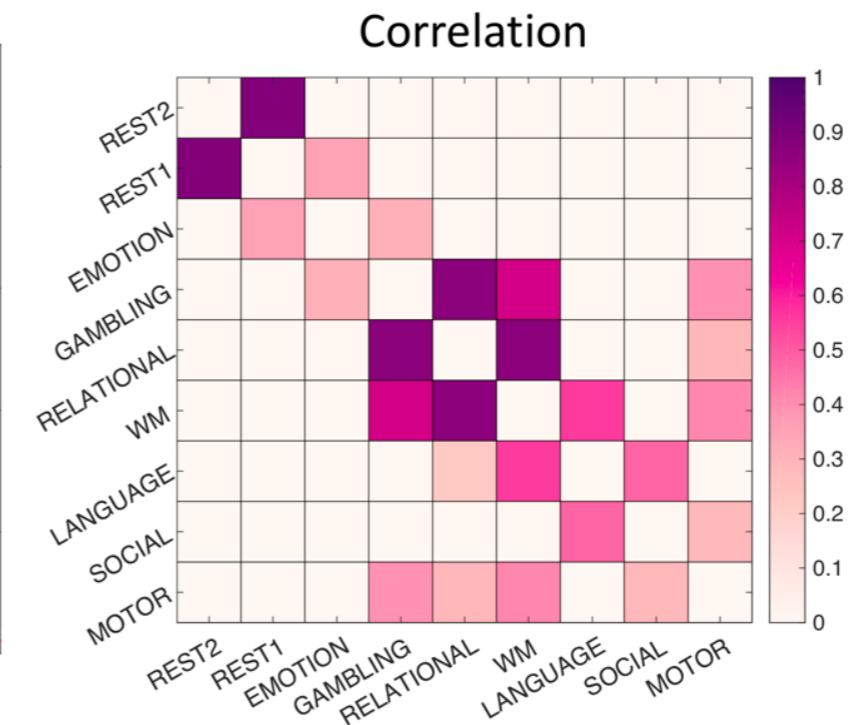
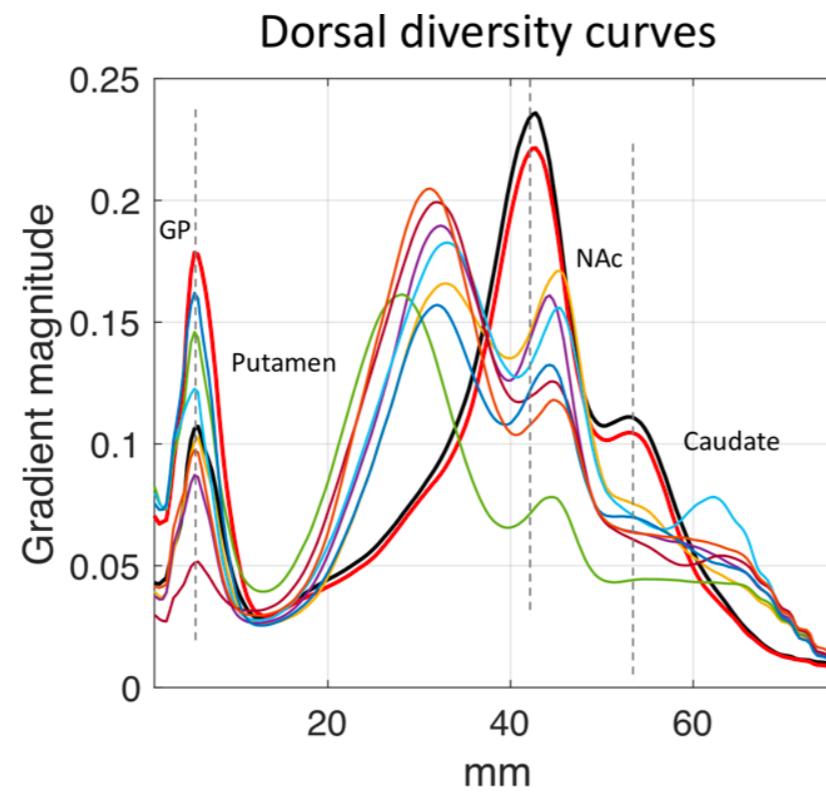
3. Gradient break-points

4. ... yields hierarchical parcellation

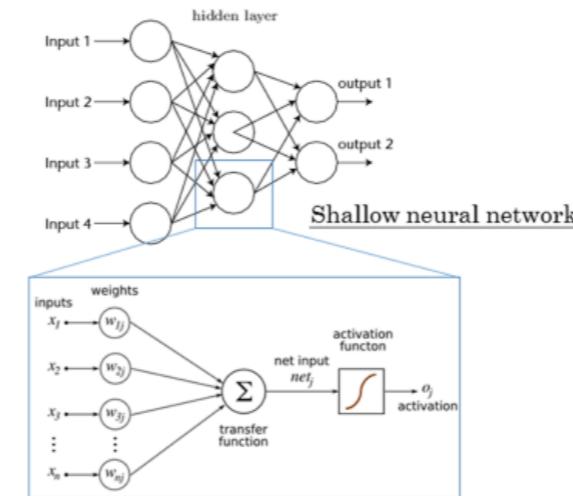
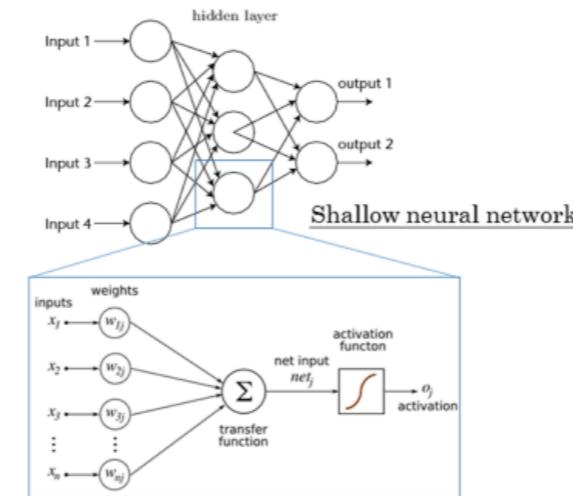


III: Neural fields + modes

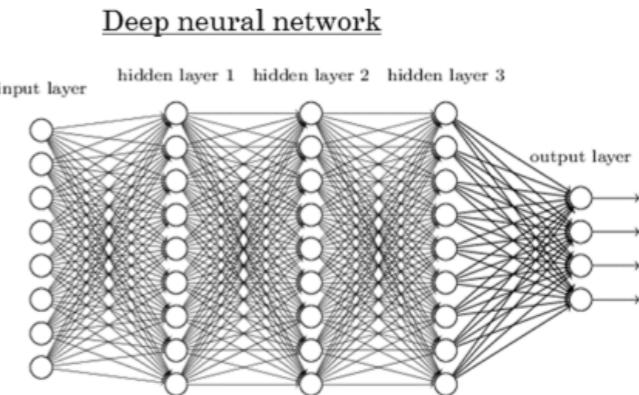
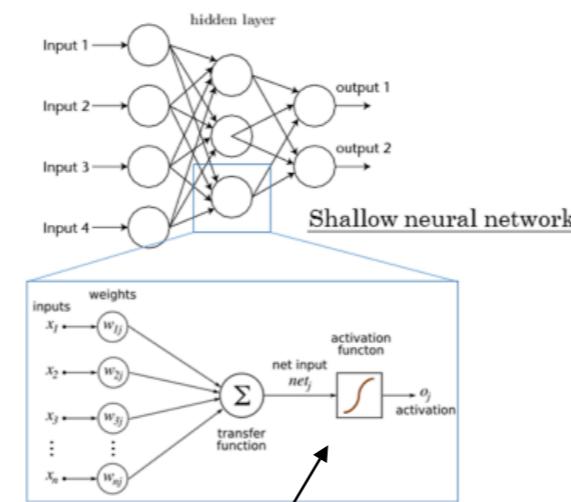
5. Task effects



IV: Linking brain states and mental states

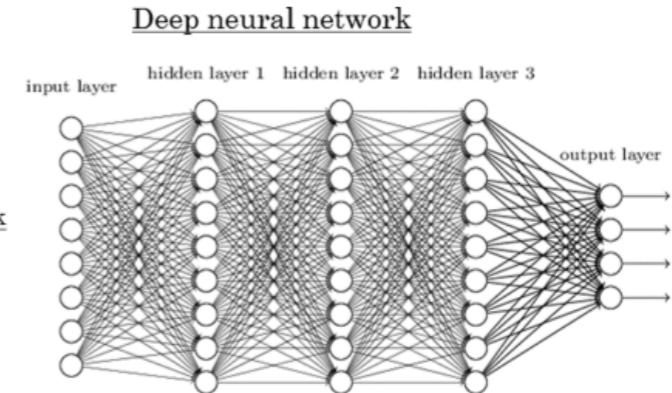
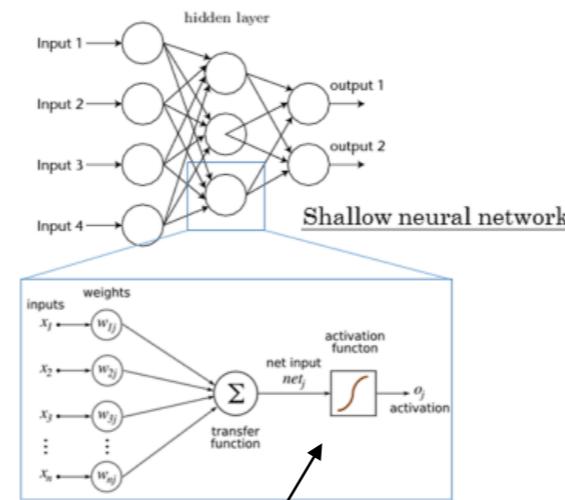


IV: Linking brain states and mental states



Gain control lies at the heart of conventional
neural networks and deep (“brain-like”)
architectures

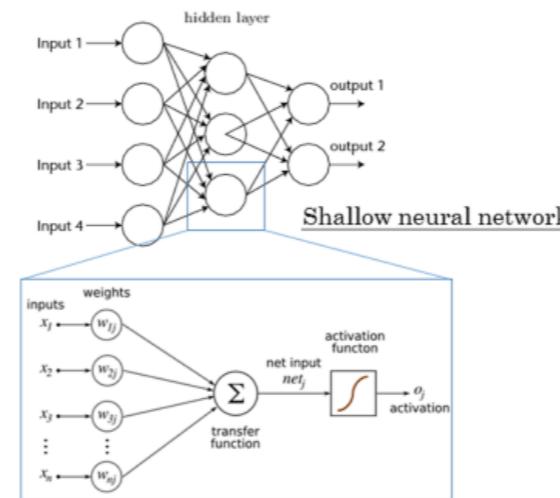
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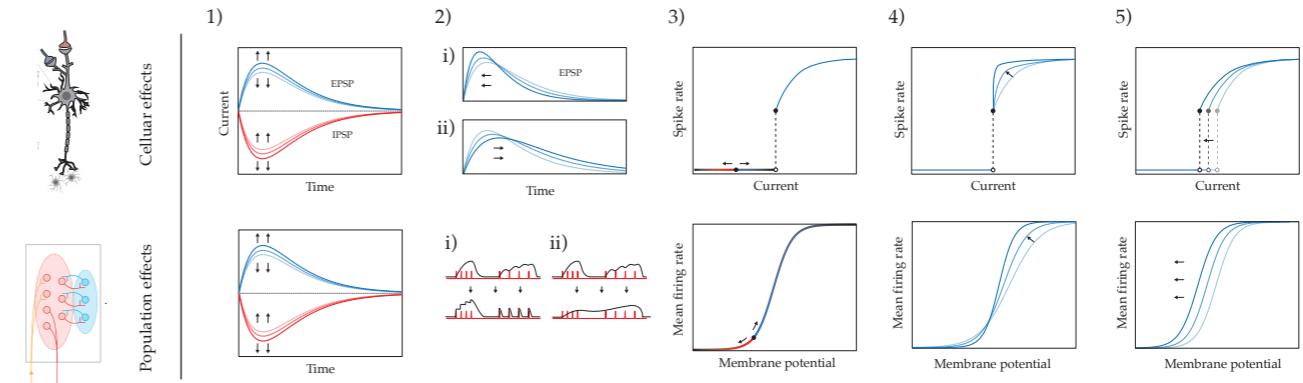
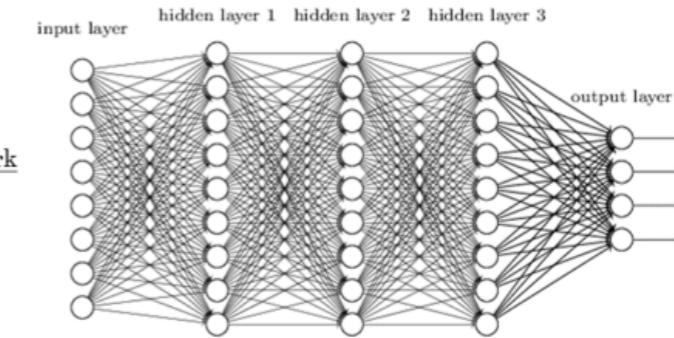
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neural networks and deep (“brain-like”)
architectures

Weights are adjusted when learning but the
system is otherwise essentially static

IV: Linking brain states and mental states



Deep neural network



Contrasts with the dynamic, multiscale, adaptive brain

Acknowledgements

Anton Tokariev, Sampsa Vanhatalo, Luca Cocchi, James Roberts, Mac Shine, Eli Muller, Ye Tian, Andrew Zalesky, Daniel Margulies



I respectfully acknowledge the Awabakal people, the traditional custodians of the land on which we live and work in Newcastle

