

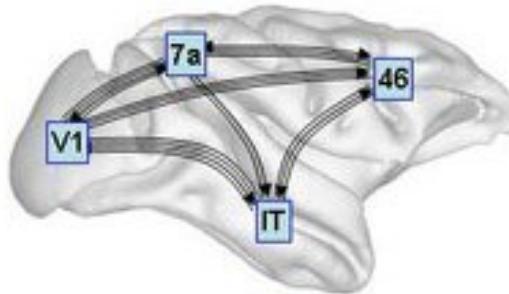
Models of Connectivity: Dynamic Causal Modelling for fMRI

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CP Course 2020, Zürich, Switzerland

Structural, functional & effective connectivity



anatomical/structural

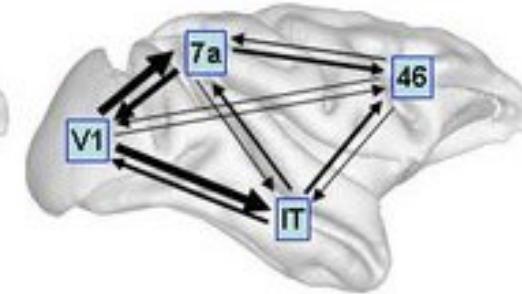
- presence of physical connections

→ DWI, tractography, tracer studies (animals)

functional

- statistical dependency between regional time series

→ correlations, ICA



Sporns 2007, Scholarpedia

effective

- direct influences between neuronal populations

→ DCM

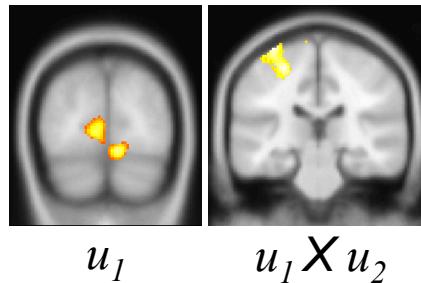
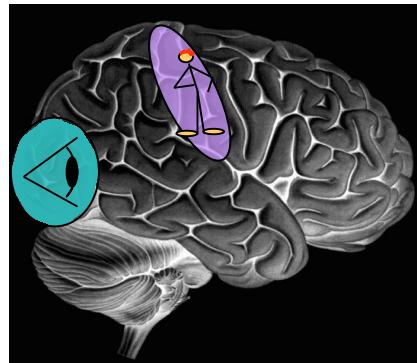
Context-independent

Mechanism - free

Mechanistic

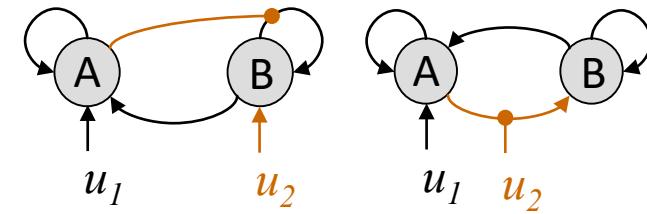
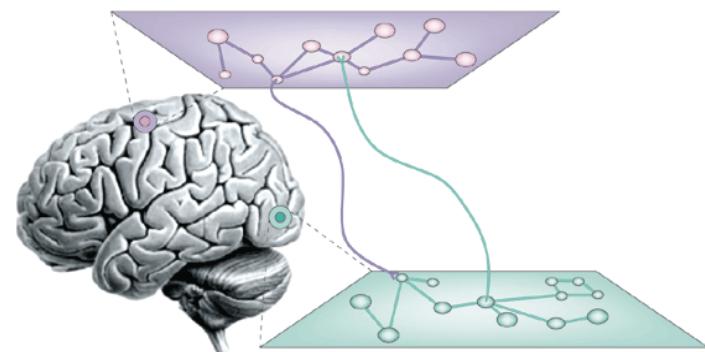
Specialisation vs. Integration

Functional Specialisation



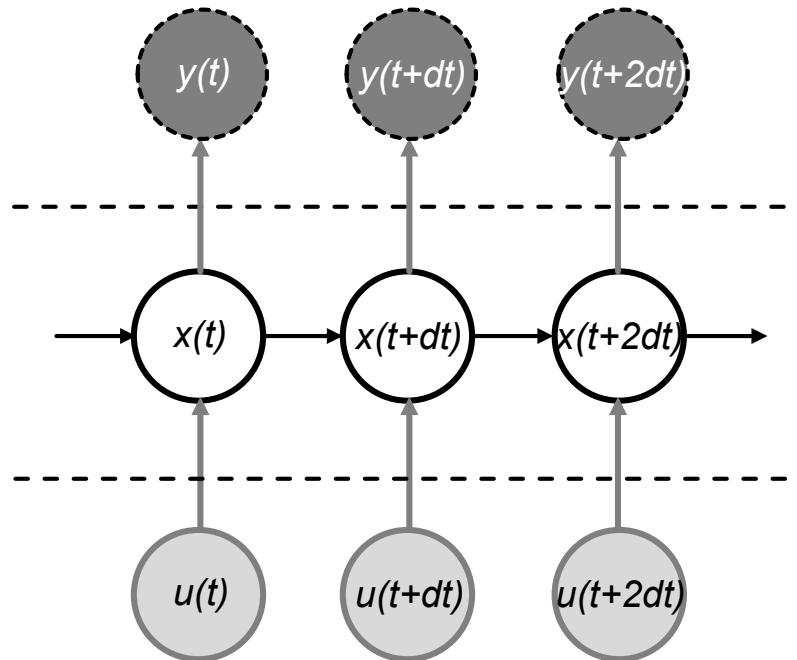
«**Where**, in the brain, did my experimental manipulation have an effect?»

Functional Integration



«**How** did my experimental manipulation propagate through the network?»

A reminder – generative models



Observed data (fMRI)

$$y = g(x, \theta) + \varepsilon$$

Hidden states (Brain activity)

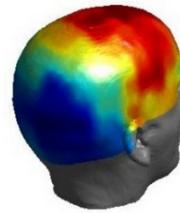
$$\frac{dx}{dt} = f(x, u, \theta) + \omega$$

Inputs (Exp. manipulations)

$$u(t)$$

Dynamic causal modelling

EEG,
MEG

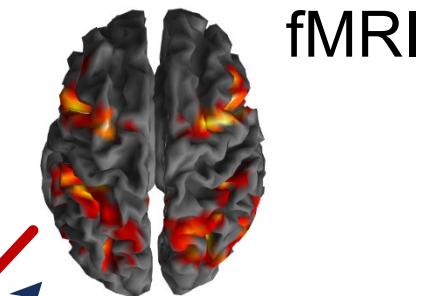


Model inversion:
Estimating
neuronal
mechanisms

Forward model:
Predicting
measured activity

$$y = g(x, \theta) + \varepsilon$$

DCM for EEG
→ Next lecture
→ Jean Daunizeau



State equation:
Describing neuronal
dynamics (and
hemodynamics)



$$\frac{dx}{dt} = f(x, u, \theta) + \omega$$



University of
Zurich^{UZH}



Translational Neuromodeling Unit

ETH zürich

Dynamic causal modelling



ACADEMIC
PRESS

Available online at www.sciencedirect.com



NeuroImage 19 (2003) 1273–1302

NeuroImage

www.elsevier.com/locate/ynimsg

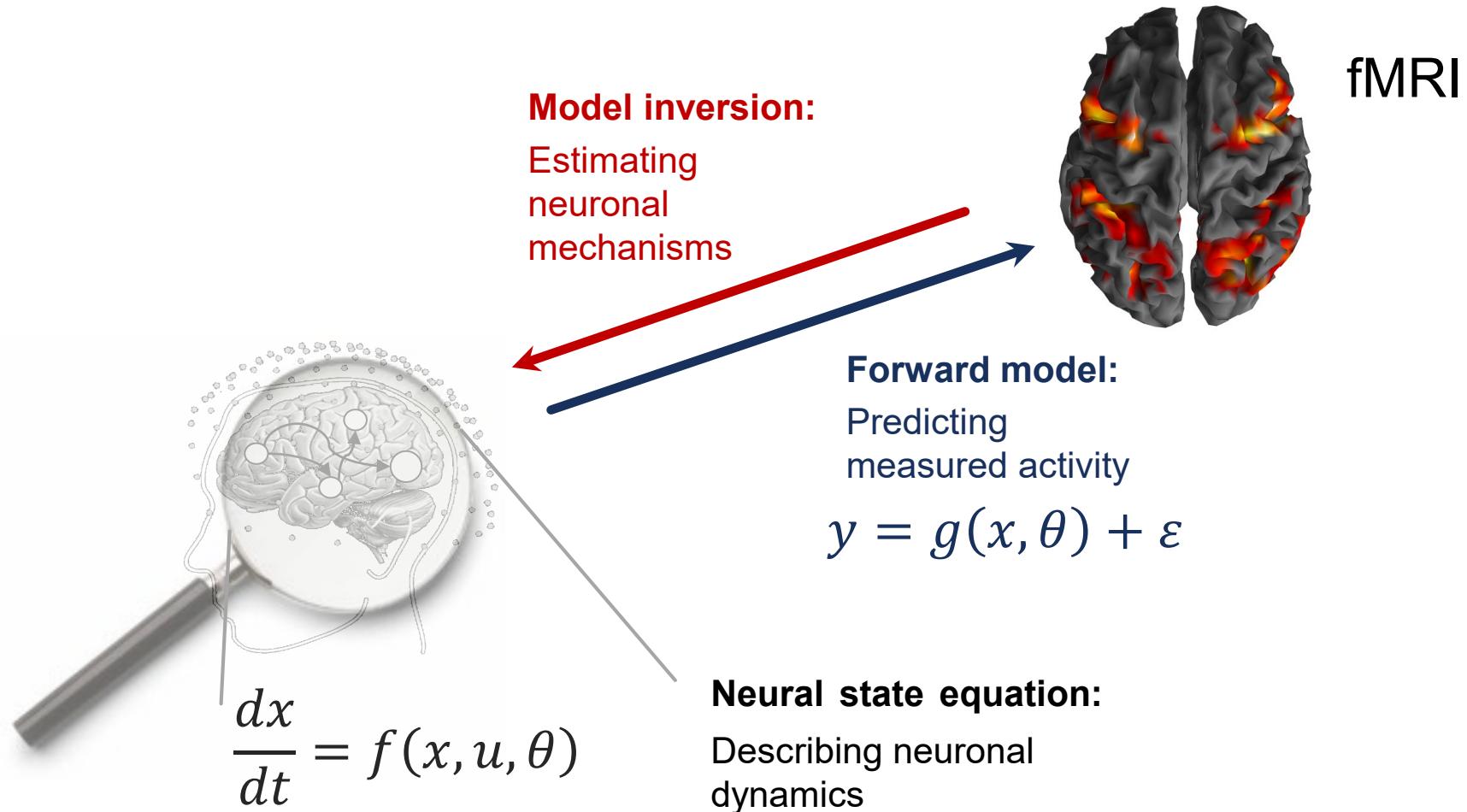
Dynamic causal modelling

K.J. Friston,* L. Harrison, and W. Penny

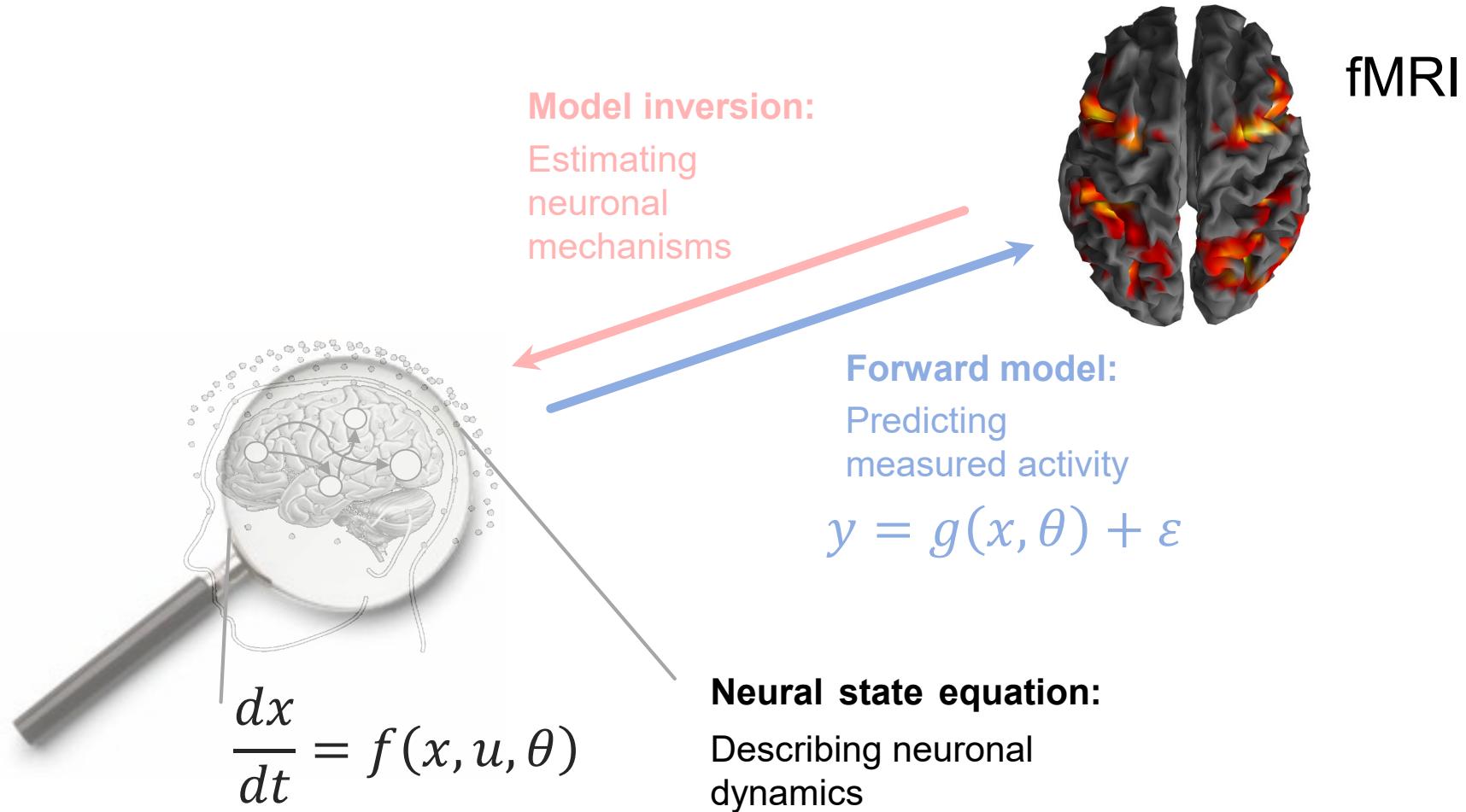
The Wellcome Department of Imaging Neuroscience, Institute of Neurology, Queen Square, London WC1N 3BG, UK

Received 18 October 2002; revised 7 March 2003; accepted 2 April 2003

DCM for fMRI - Overview



DCM for fMRI - Overview





Neuronal state equations

$$\frac{dx}{dt} = f(x, u)$$



Neuronal state equations

$$\frac{dx}{dt} = f(x, u) \approx f(x_0, 0) + \frac{\partial f}{\partial x} x + \frac{\partial f}{\partial u} u + \frac{\partial^2 f}{\partial x \partial u} ux + \frac{\partial^2 f}{\partial x^2} \frac{x^2}{2} + \dots$$

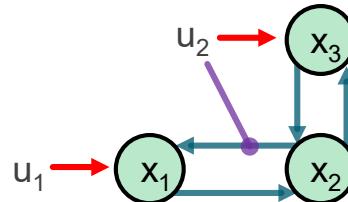
bilinear model

Neuronal state equations

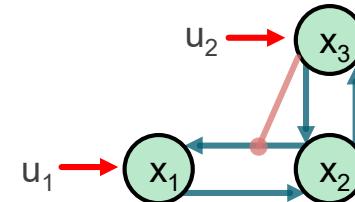
$$\frac{dx}{dt} = f(x, u) \approx f(x_0, 0) + \frac{\partial f}{\partial x} x + \frac{\partial f}{\partial u} u + \frac{\partial^2 f}{\partial x \partial u} u x + \frac{\partial^2 f}{\partial x^2} \frac{x^2}{2} + \dots$$

A C B D

bilinear model

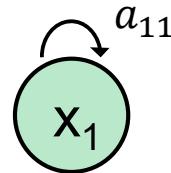


nonlinear model

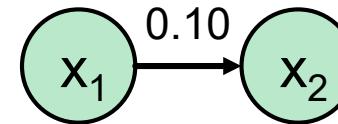
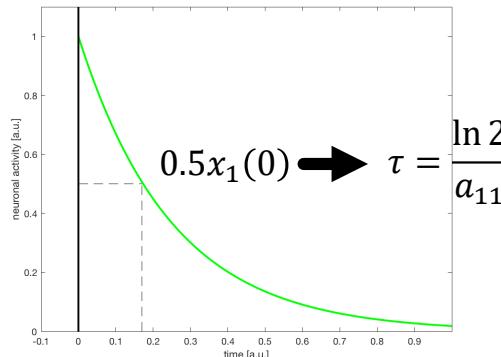


Neuronal state equations

DCM effective connectivity parameters are rate constants



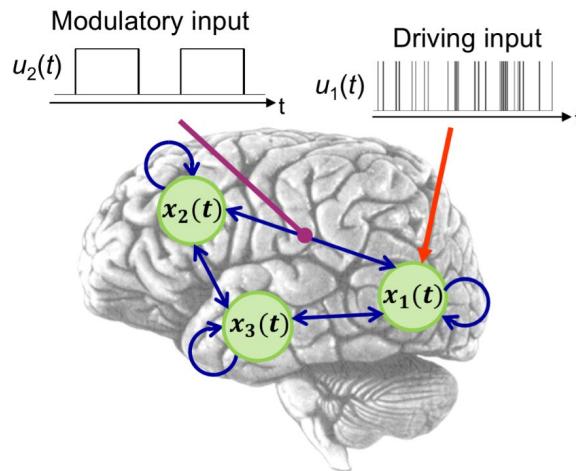
$$\frac{dx_1}{dt} = a_{11}x_1 \longrightarrow x_1(t) = x_1(0) \cdot \exp(a_{11}t)$$



If $x_1 \rightarrow x_2$ is 0.10s^{-1} , this means that, per unit time, the increase in activity in x_2 corresponds to 10% of the current activity in x_1

Neuronal state equations

Interim summary: bilinear neuronal state equation



$$\frac{dx}{dt} = \underbrace{\left(A + \sum_{j=1}^m u_j B^{(j)} \right)}_{\text{connectivity}} x + \underbrace{Cu}_{\text{External inputs}}$$

State change

External inputs

Current state

connectivity

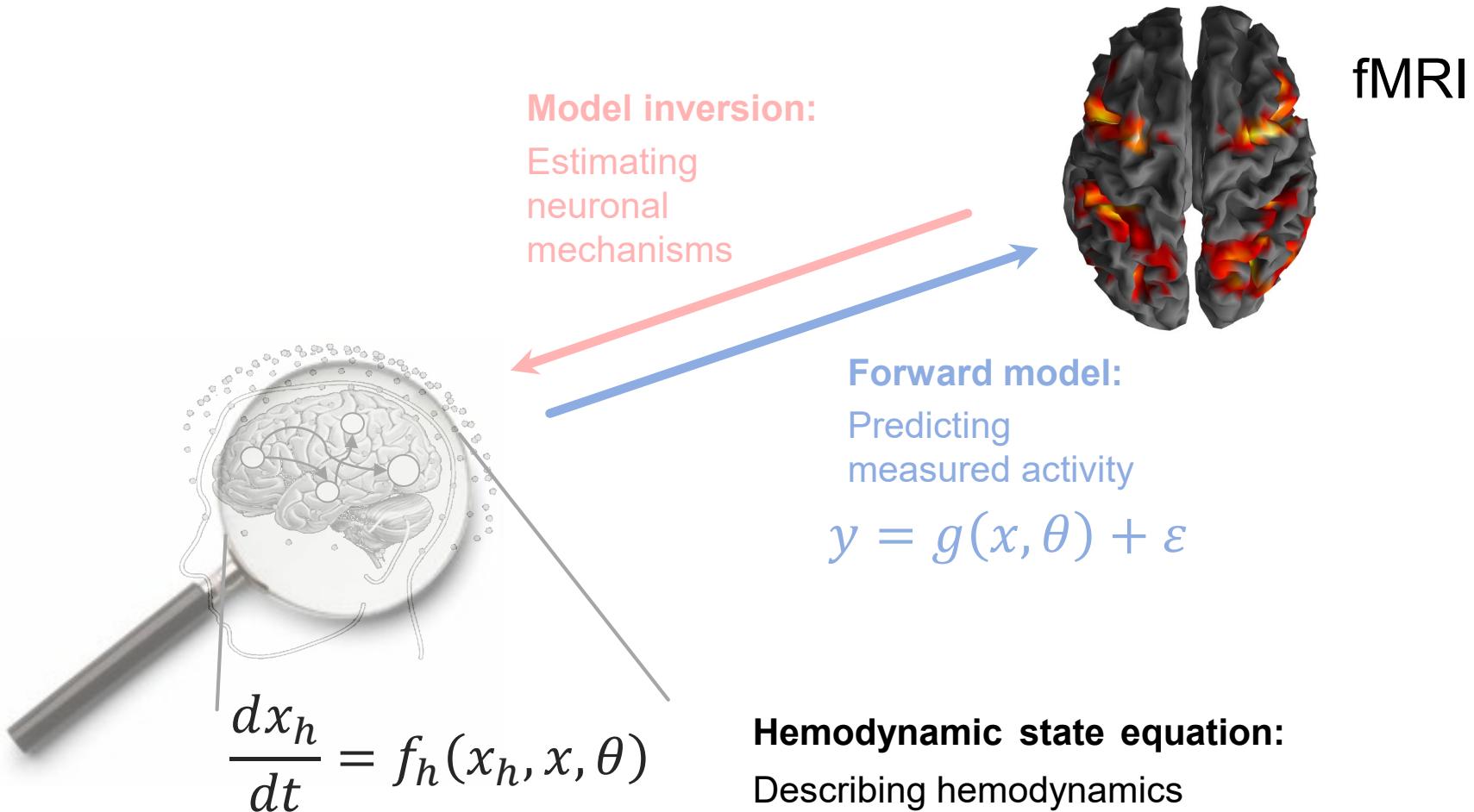
$\theta = \{A, B^{(1)}, \dots, B^{(m)}, C\}$

Endogenous connectivity

Modulatory connectivity

Driving inputs

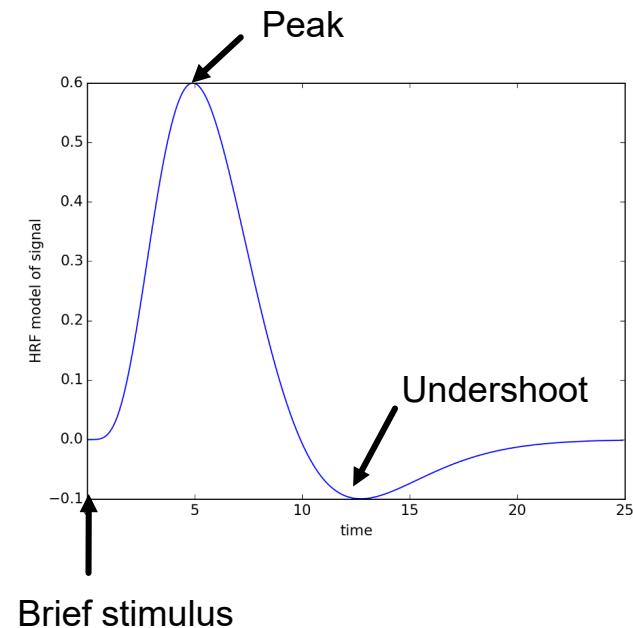
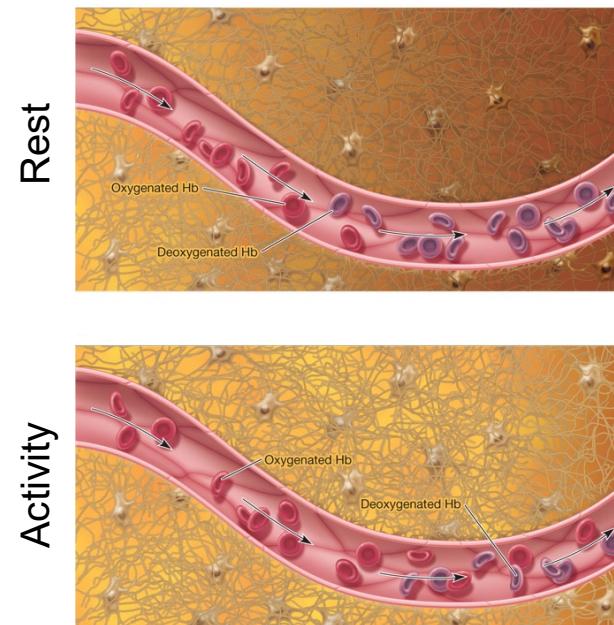
DCM for fMRI - Overview



The hemodynamic response

Neuronal dynamics only indirectly observable via hemodynamic response

- ↑ neuronal activity
- ↑ blood flow
- ↑ oxygenated Hb
- ↑ T2*
- ↑ fMRI signal



The hemodynamic model

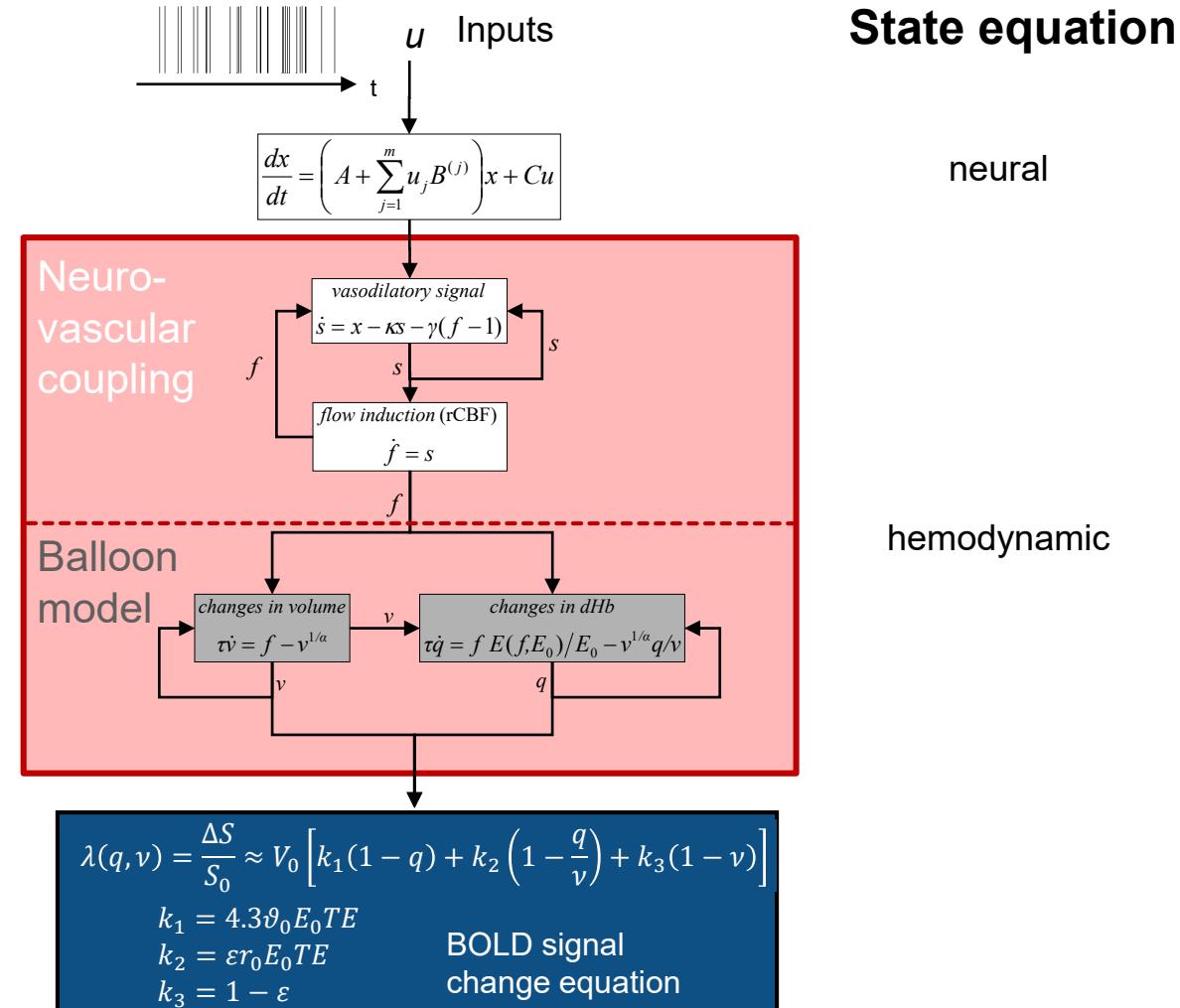
6 parameters:

$$\theta^h = \{\kappa, \gamma, \tau, \alpha, \rho, \varepsilon\}$$

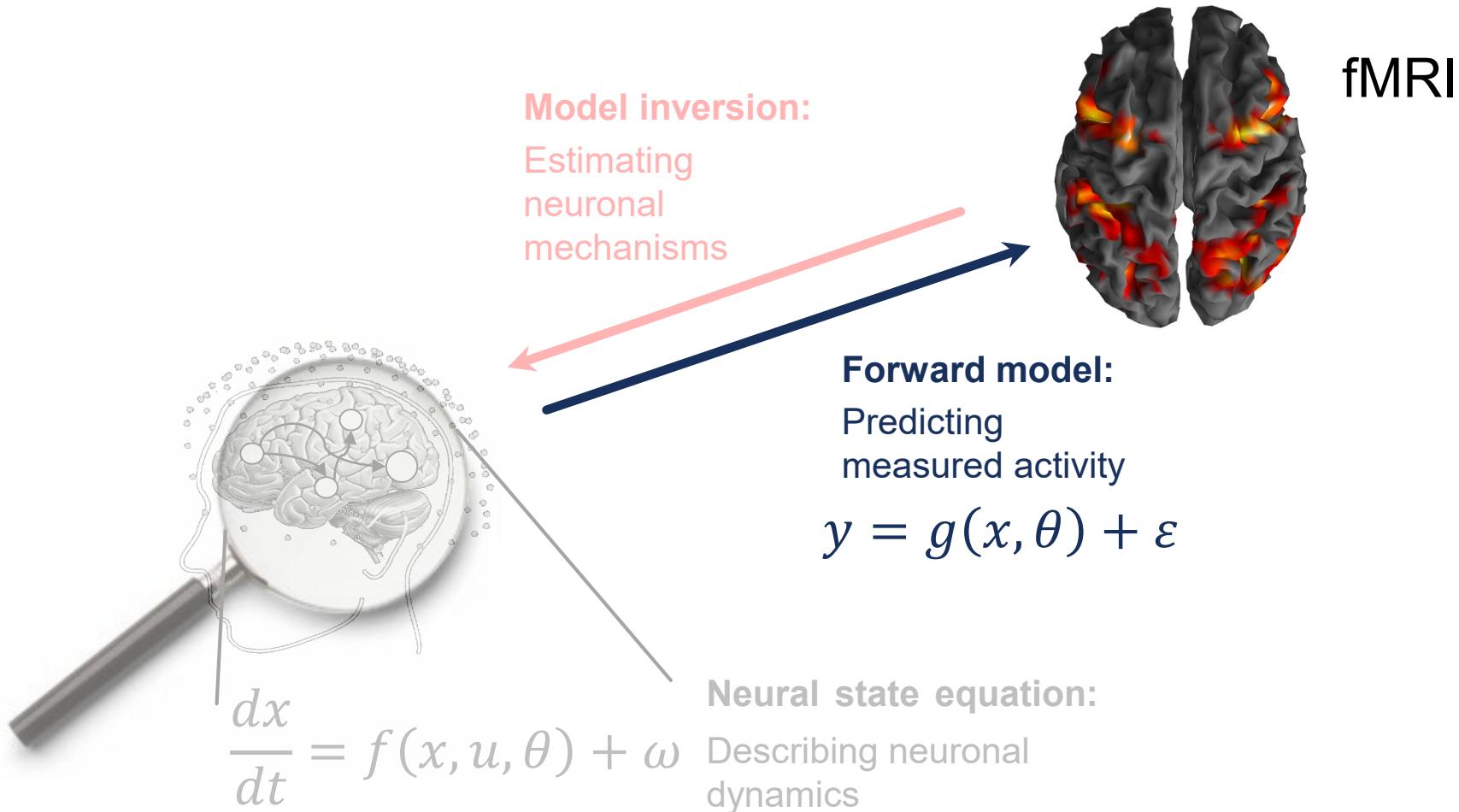
Important for model fitting,
but typically of no interest
for statistical inference.

Region specific HRF

→ Parameters computed
separately for each region



DCM for fMRI - Overview





The BOLD signal equation

Resting blood
volume

Deoxyhemoglobin
content

Blood
volume



$$\lambda(q, \nu) = \frac{\Delta S}{S_0} \approx V_0 \left[k_1(1 - q) + k_2 \left(1 - \frac{q}{\nu} \right) + k_3(1 - \nu) \right]$$

BOLD-Signal Parameters:

$$k_1 = 4.3 \vartheta_0 E_0 TE$$

$$k_2 = \varepsilon r_0 E_0 TE$$

$$k_3 = 1 - \varepsilon$$

$$V_0 = 0.04 \quad E_0 = 0.32 - 0.4$$

At 1.5 Tesla

$$\vartheta_0 \approx 40.3 \text{ s}^{-1}$$

$$r_0 \approx 25 \text{ s}^{-1}$$

$$TE \approx 0.04 \text{ s}$$

$$\varepsilon \approx 1.28$$

At 3 Tesla

$$\vartheta_0 \approx 80.6 \text{ s}^{-1}$$

$$r_0 \approx 110 \text{ s}^{-1}$$

$$TE \approx 0.035 \text{ s}$$

$$\varepsilon \approx 0.47$$

At 7 Tesla

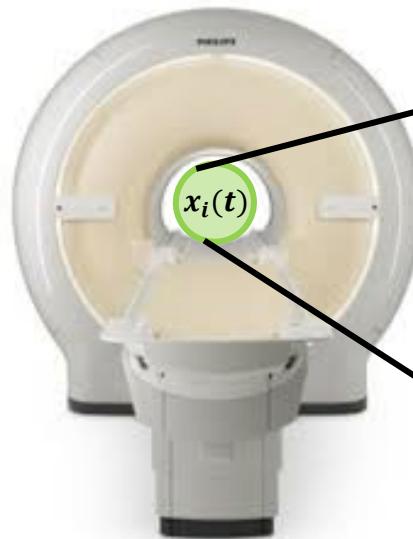
$$\vartheta_0 \approx 188 \text{ s}^{-1}$$

$$r_0 \approx 340 \text{ s}^{-1}$$

$$TE \approx 0.025 \text{ s}$$

$$\varepsilon \approx 0.026$$

From neural activity to the BOLD signal: Summary



Neurovascular coupling

Vasodilation (s) and
blood flow changes (f)

Balloon model

Relative blood
volume (v) and
deoxyHB (q)

x

f

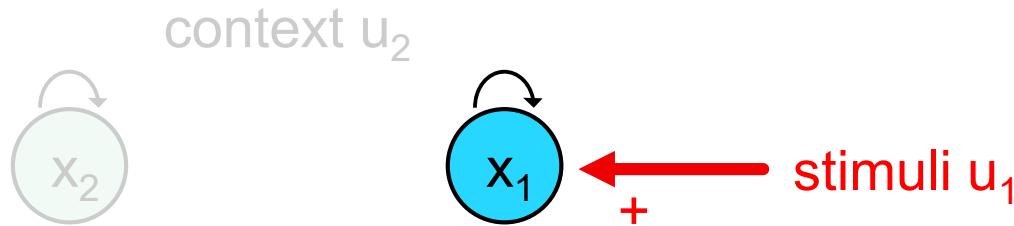
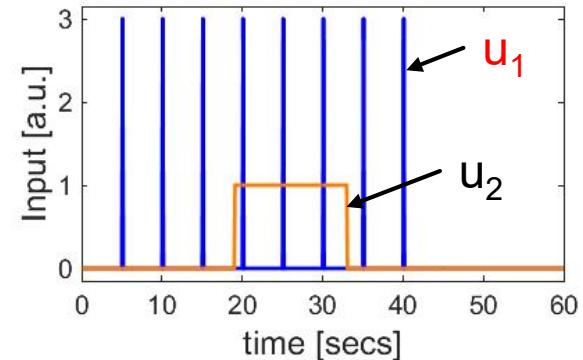
v, q

BOLD signal is a direct function of v and q

$$y = \frac{\Delta S}{S_0} = g(v, q) + \varepsilon$$

Simulation example: What can DCM explain?

Example: single node

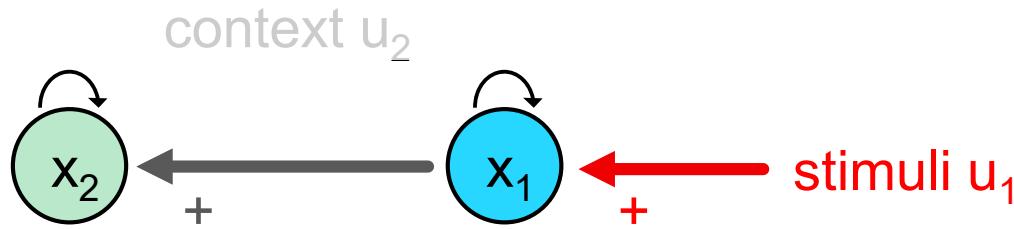


$$\frac{dx}{dt} = Ax + u_2 B^{(2)}x + Cu_1$$

$$\begin{bmatrix} \dot{x}_1 \\ \dot{x}_2 \end{bmatrix} = \begin{bmatrix} a_{11} & 0 \\ 0 & a_{22} \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + u_2 \begin{bmatrix} 0 & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + \begin{bmatrix} c_{11} & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} u_1 \\ u_2 \end{bmatrix}$$

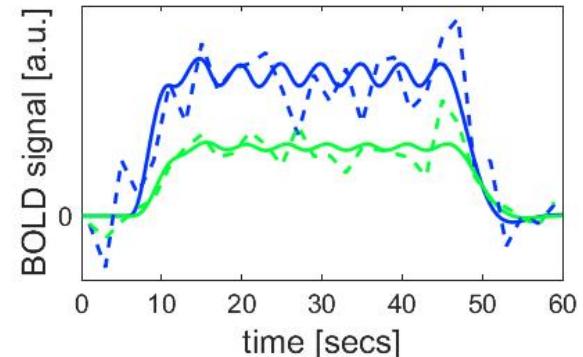
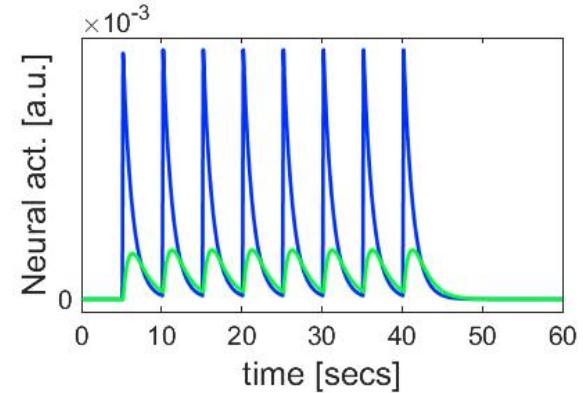
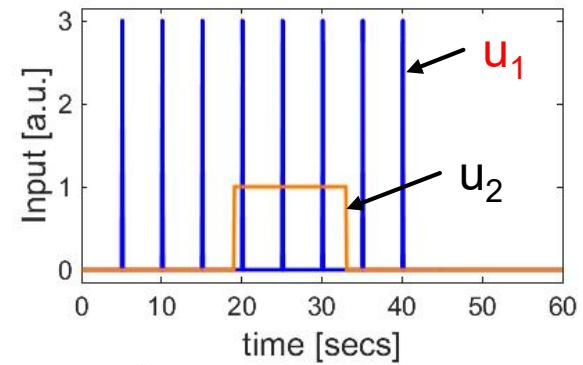
Simulation example: What can DCM explain?

Example: two connected node



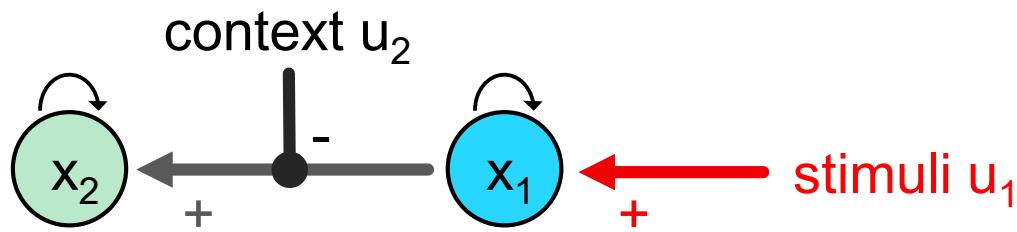
$$\frac{dx}{dt} = Ax + u_2 B^{(2)}x + Cu_1$$

$$\begin{bmatrix} \dot{x}_1 \\ \dot{x}_2 \end{bmatrix} = \begin{bmatrix} a_{11} & 0 \\ a_{21} & a_{22} \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + u_2 \begin{bmatrix} 0 & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + \begin{bmatrix} c_{11} & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} u_1 \\ u_2 \end{bmatrix}$$



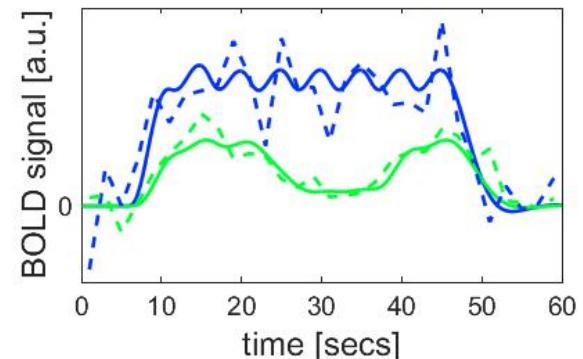
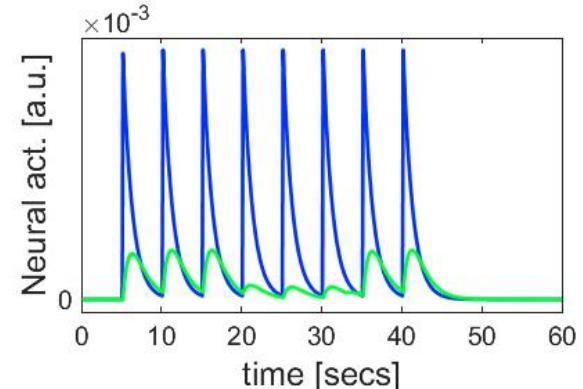
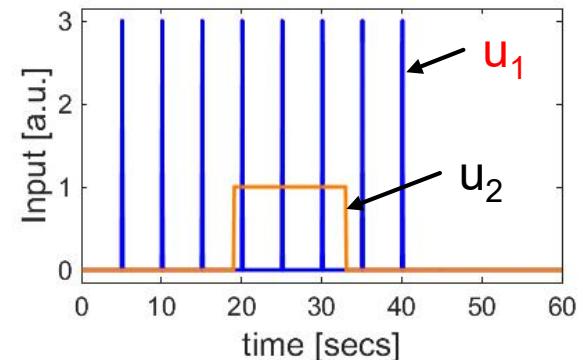
Simulation example: What can DCM explain?

Example: modulation of connection



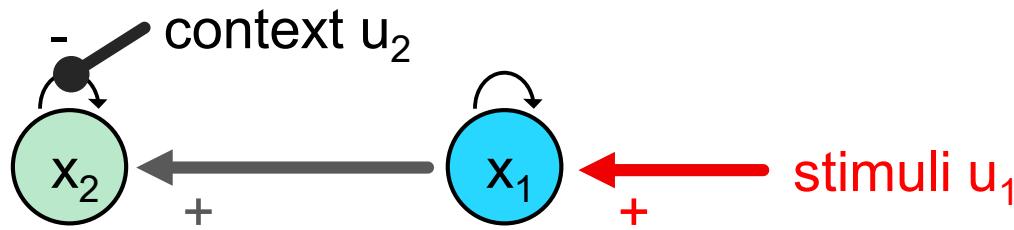
$$\frac{dx}{dt} = Ax + u_2 B^{(2)}x + Cu_1$$

$$\begin{bmatrix} \dot{x}_1 \\ \dot{x}_2 \end{bmatrix} = \begin{bmatrix} a_{11} & 0 \\ a_{21} & a_{22} \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + u_2 \begin{bmatrix} 0 & 0 \\ b_{21}^{(2)} & 0 \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + \begin{bmatrix} c_{11} & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} u_1 \\ u_2 \end{bmatrix}$$



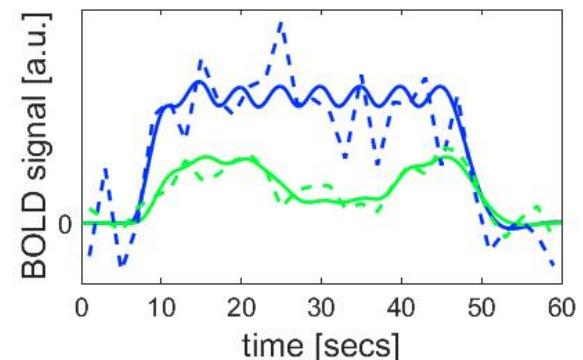
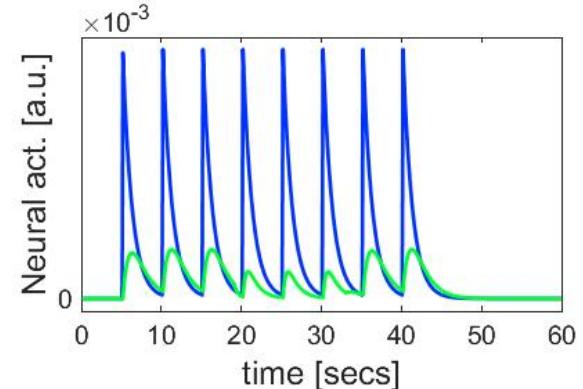
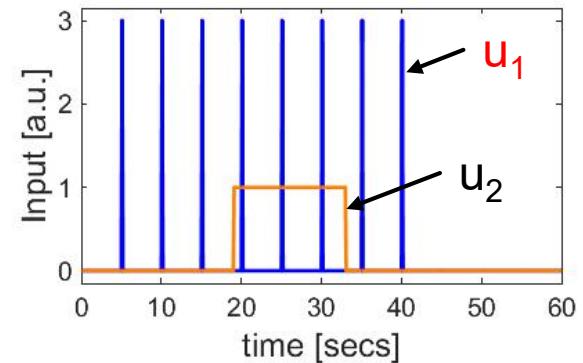
Simulation example: What can DCM explain?

Example: modulation of inhibitory self-connection



$$\frac{dx}{dt} = Ax + u_2 B^{(2)}x + Cu_1$$

$$\begin{bmatrix} \dot{x}_1 \\ \dot{x}_2 \end{bmatrix} = \begin{bmatrix} a_{11} & 0 \\ a_{21} & a_{22} \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + u_2 \begin{bmatrix} 0 & 0 \\ 0 & b_{22}^{(2)} \end{bmatrix} \cdot \begin{bmatrix} x_1 \\ x_2 \end{bmatrix} + \begin{bmatrix} c_{11} & 0 \\ 0 & 0 \end{bmatrix} \cdot \begin{bmatrix} u_1 \\ u_2 \end{bmatrix}$$



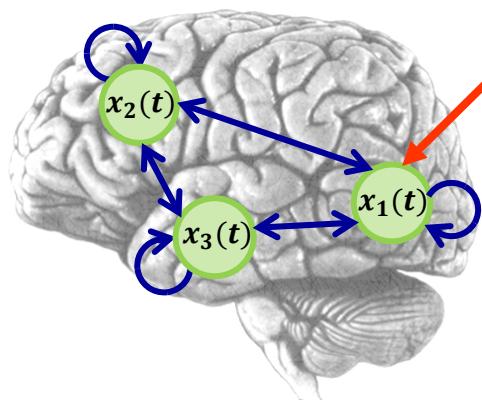
DCM for fMRI

A simple model of
a neural network

... described as a
dynamical system

... causes the data
(BOLD signal).

...



Neural node



Input



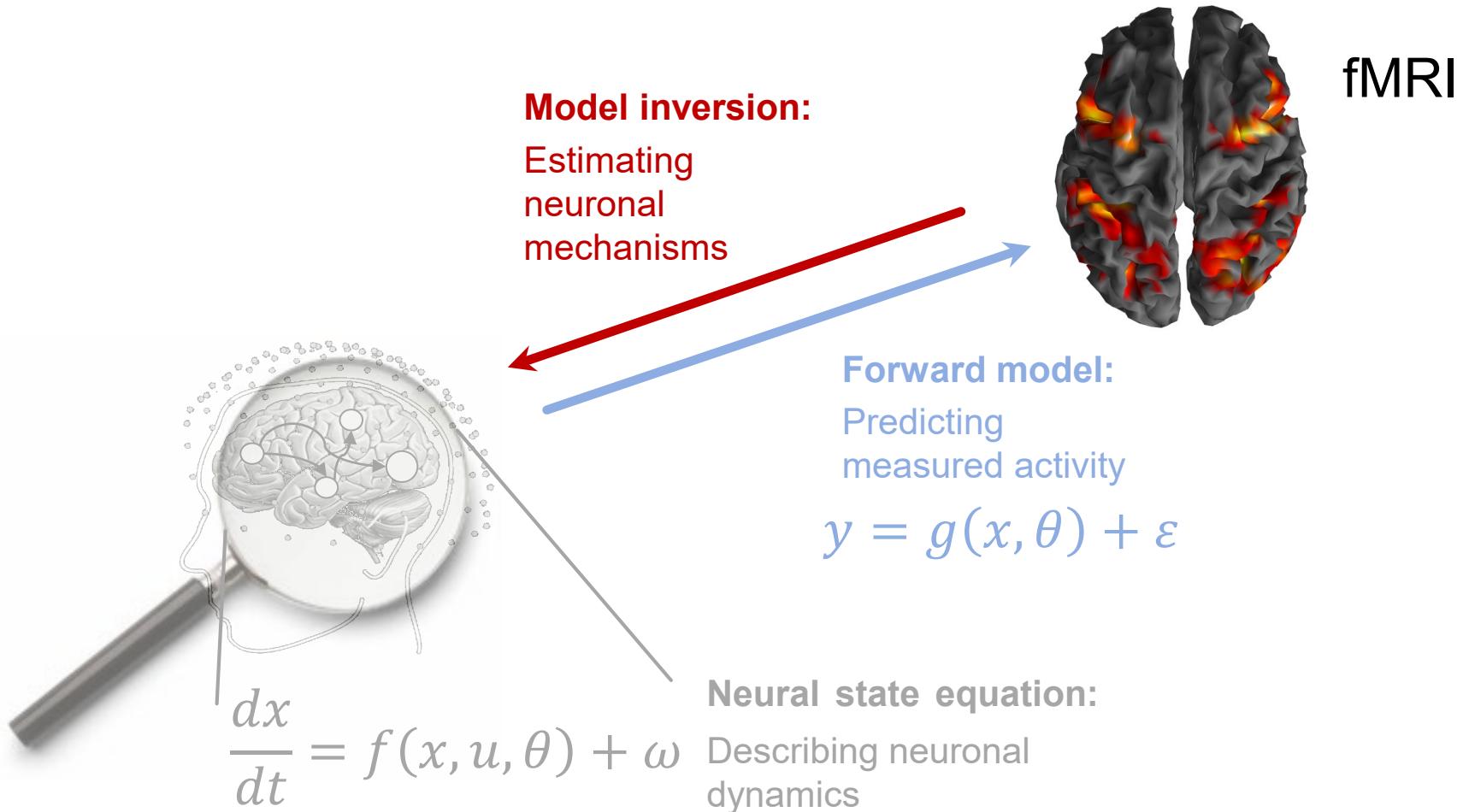
Connections

$$\dot{x} = f(x, u, \theta)$$

$$y = g(x, \theta) + \varepsilon$$

Let the system run with input (u) and parameters (θ), and you will get a BOLD signal time course y that you can compare to the measured data.

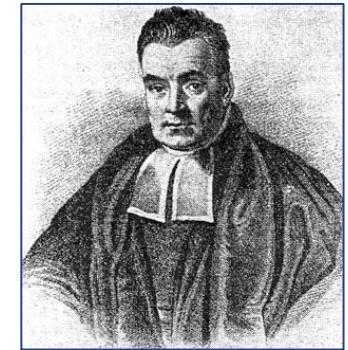
DCM for fMRI - Overview



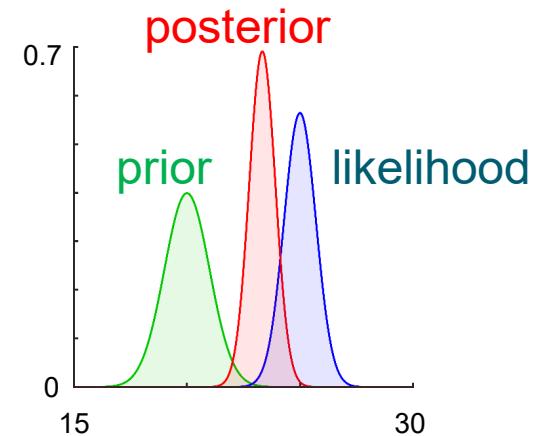
Bayes' theorem

$$\text{posterior } p(\theta|y, m) = \frac{\text{likelihood prior}}{\text{model evidence}}$$

likelihood prior
 $p(y|\theta, m)p(\theta|m)$
 $p(y|m)$
model evidence



Reverend Thomas Bayes
(1702-1761)





The likelihood function for DCM

$$p(y(t)|\theta, m) = \mathcal{N}(y(t); g(\theta^n, \theta^h, u), \theta^\sigma)$$

likelihood

Assume data is normally distributed around the prediction from the dynamical model (Gaussian noise)

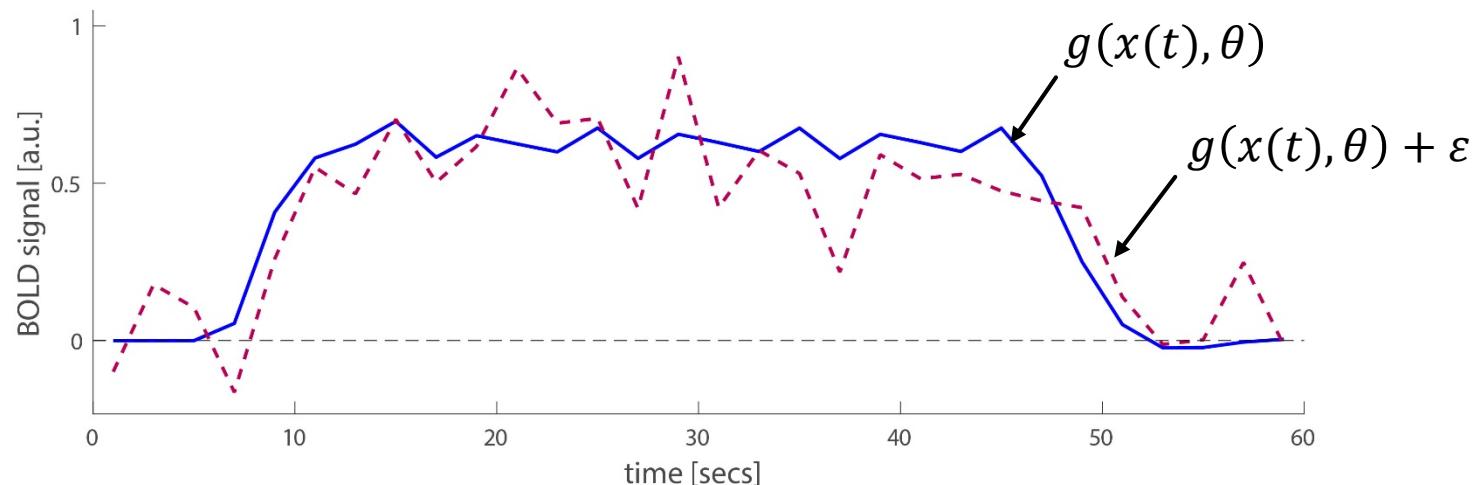
$$y(t) = g(x(t), \theta) + \varepsilon$$

$\varepsilon \sim \mathcal{N}(0, \sigma^2 I)$ Data is prediction plus Gaussian noise

The likelihood function for DCM

$$p(y(t)|\theta, m) = \mathcal{N}(y(t); g(\theta^n, \theta^h, u), \theta^\sigma)$$

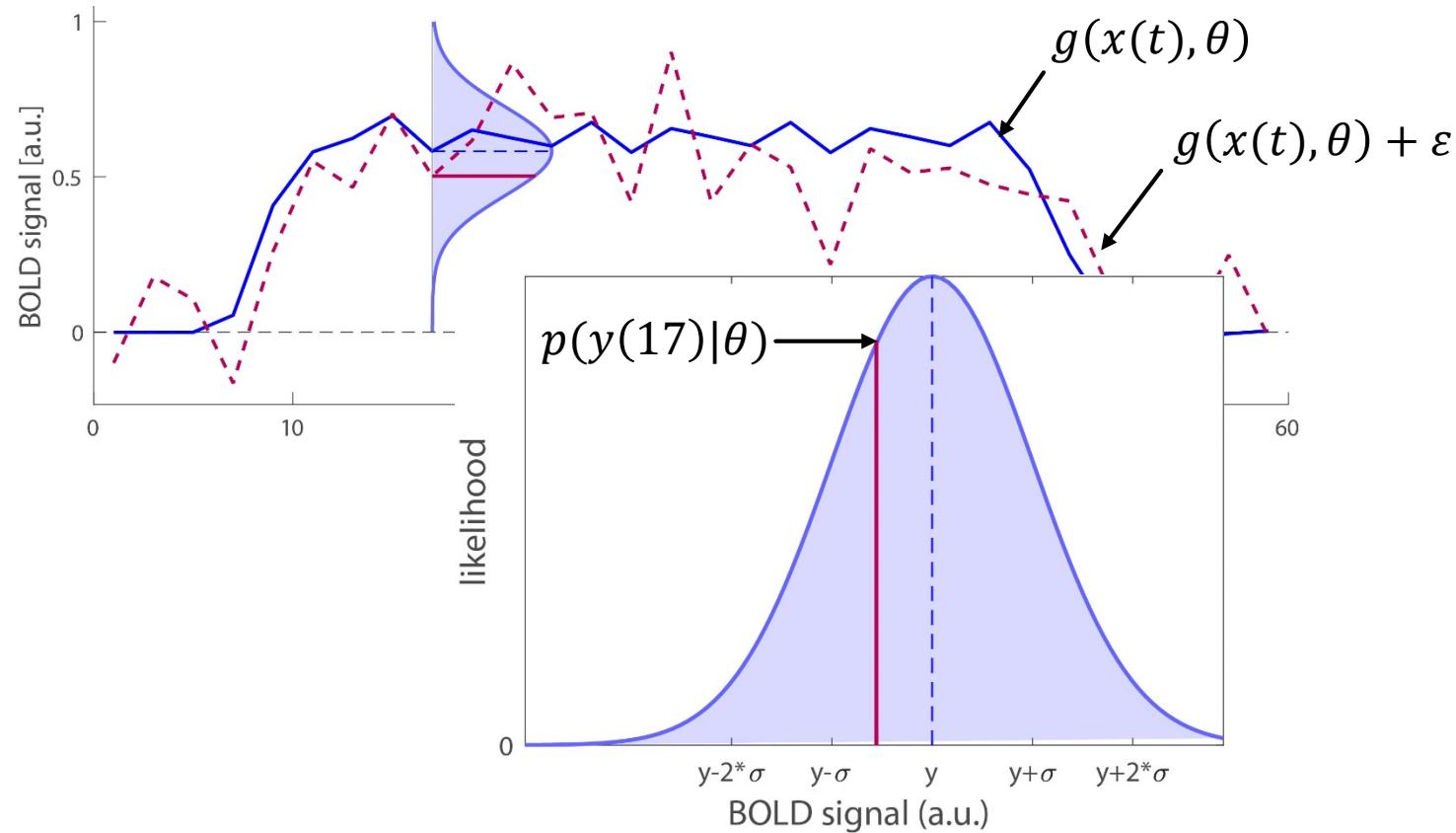
likelihood



The likelihood function for DCM

$$p(y(t)|\theta, m) = \mathcal{N}(y(t); g(\theta^n, \theta^h, u), \theta^\sigma)$$

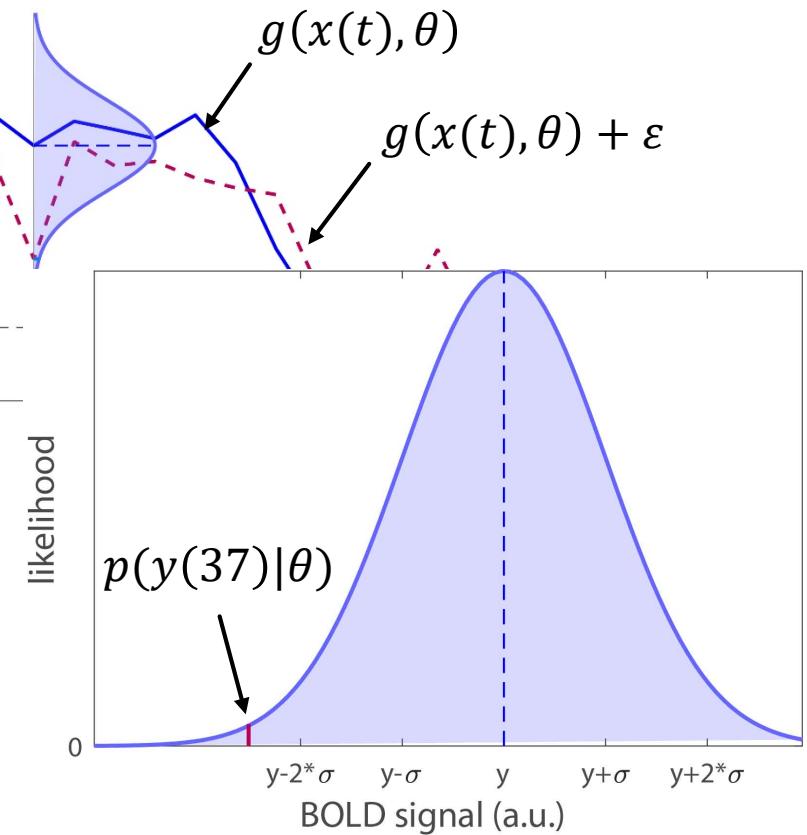
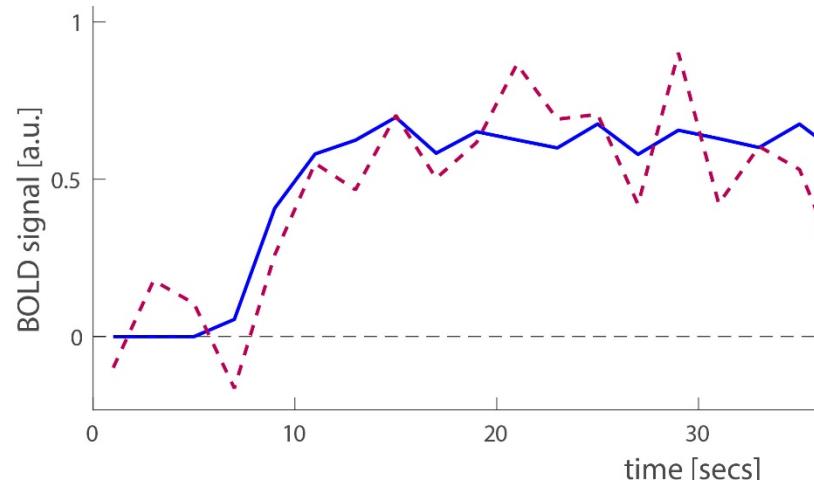
likelihood



The likelihood function for DCM

$$p(y(t)|\theta, m) = \mathcal{N}(y(t); g(\theta^n, \theta^h, u), \theta^\sigma)$$

likelihood



Priors

$$p(\theta|y, m) = \frac{p(y|\theta, m)p(\theta|m)}{p(y|m)}$$

prior

Neuronal parameters:

- self-connections: principled (to “ensure” that the system is stable)
- other parameters (between—region connections, modulation, inputs): shrinkage priors

Hemodynamic parameters:

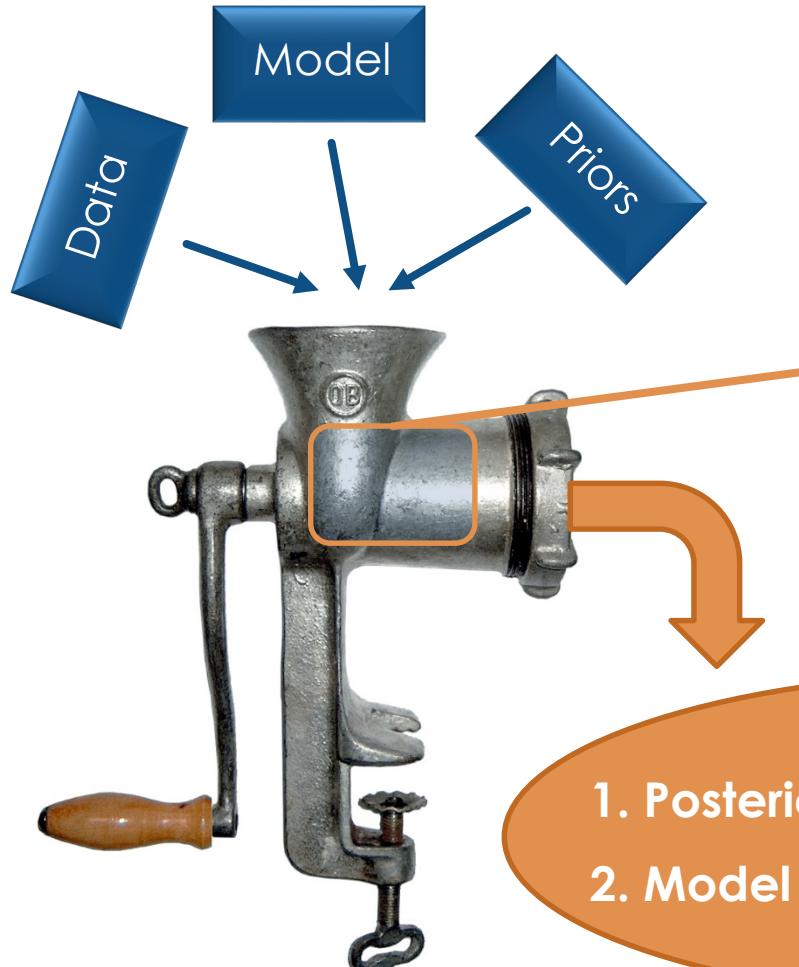
- empirical

Noise prior:

- assume relatively noisy data

(not default in SPM12 → set DCM.options.hE = 0; DCM.options.hC = 1)

Model estimation: running the machinery



Free energy approximation
Variational Bayes

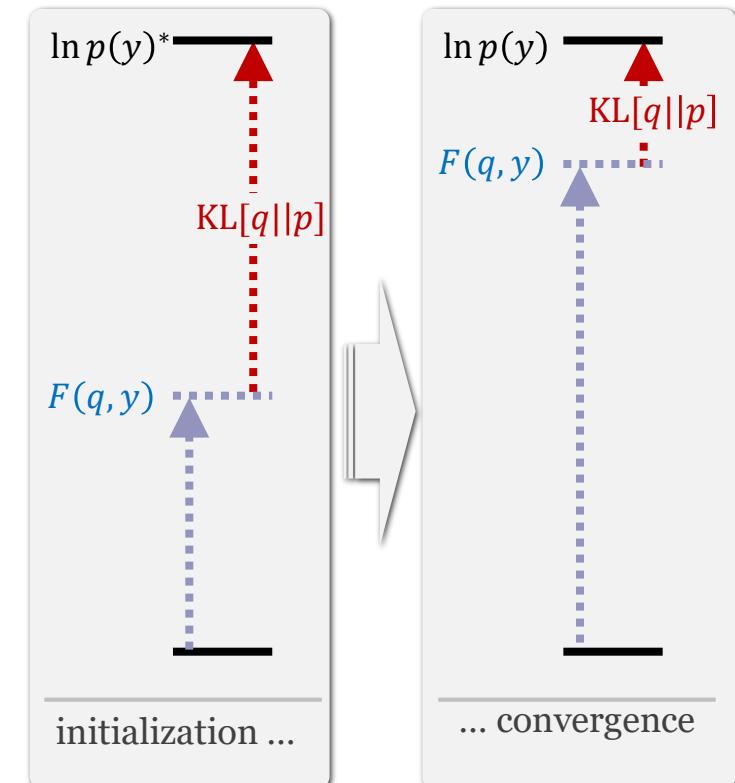
Thermodynamic integration
MCMC

Inversion – variational Free Energy approximation to model evidence

model evidence

$$\ln p(y) = \underbrace{\text{KL}[q||p]}_{\substack{\text{divergence} \\ \geq 0 \\ (\text{unknown})}} + \underbrace{F(q, y)}_{\substack{\text{neg. free energy} \\ (\text{easy to evaluate} \\ \text{for a given } q)}}$$

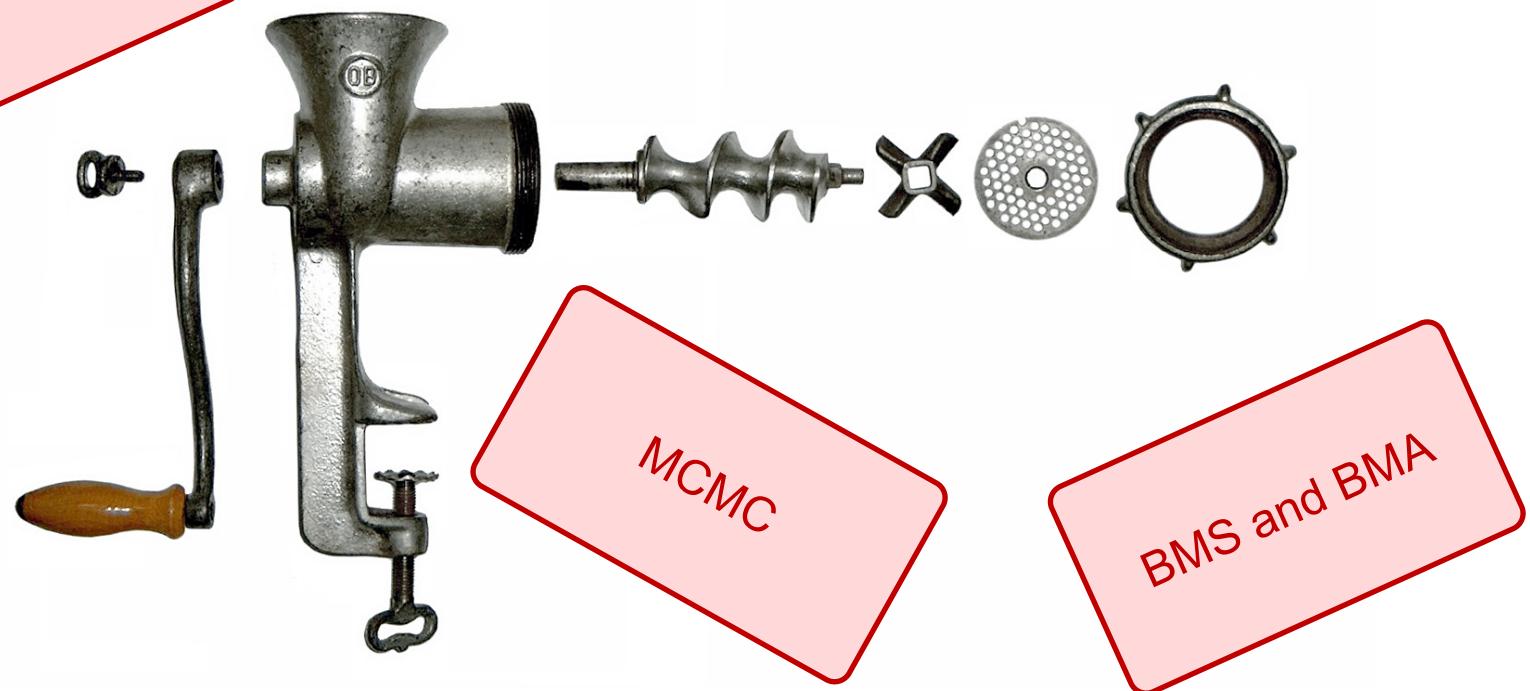
When $F(q, y)$ is maximized,
 $q(\theta)$ is our best estimate of
the true posterior.





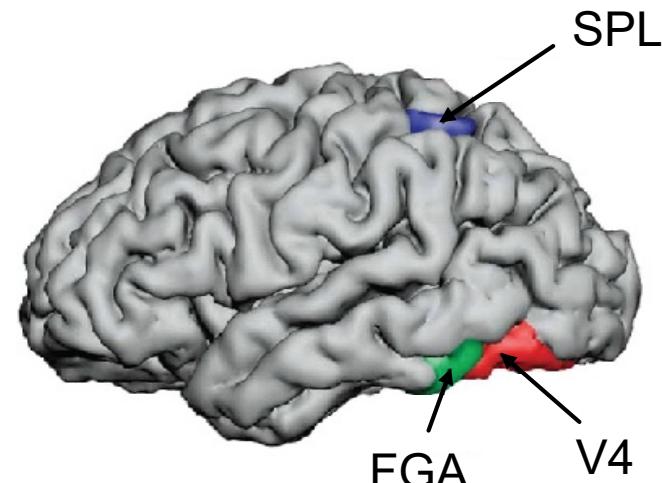
Model estimation: running the machinery

Variational Bayes



Example: Model Selection

- Specific sensory stimuli lead to unusual, additional experiences
- Grapheme-color synesthesia: **color**
- Involuntary, automatic; stable over time, prevalence ~4%
- Potential cause: aberrant **cross-activation/coupling** between brain areas
 - grapheme encoding area (FGA)
 - color area (V4)
 - superior parietal lobule (SPL)

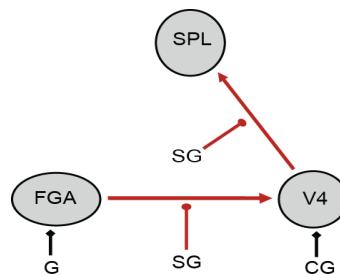


Hubbard, 2007

Bottom-up or Top-down “cross-activation”?

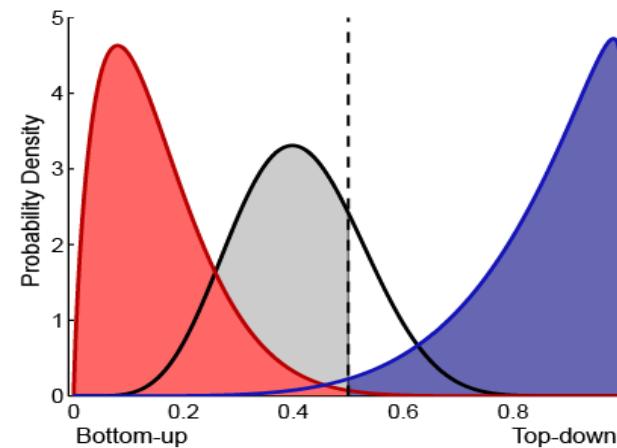
Bottom-up

(Ramachandran & Hubbard, 2001)



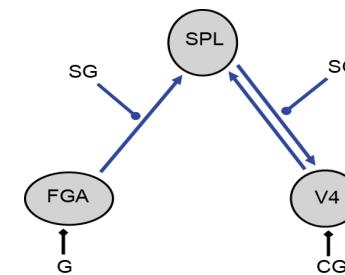
Projectors

ABC

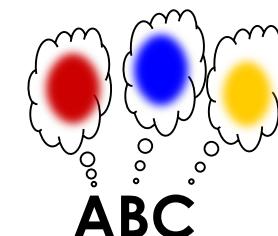


Top-down

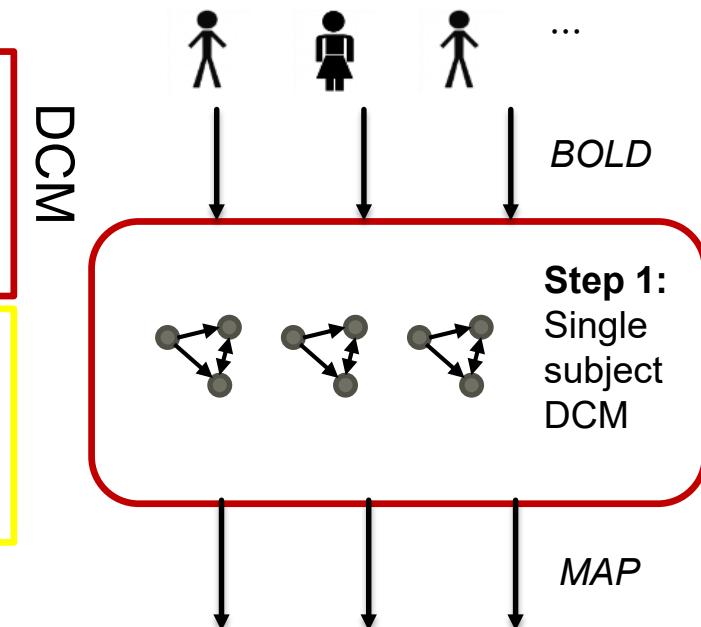
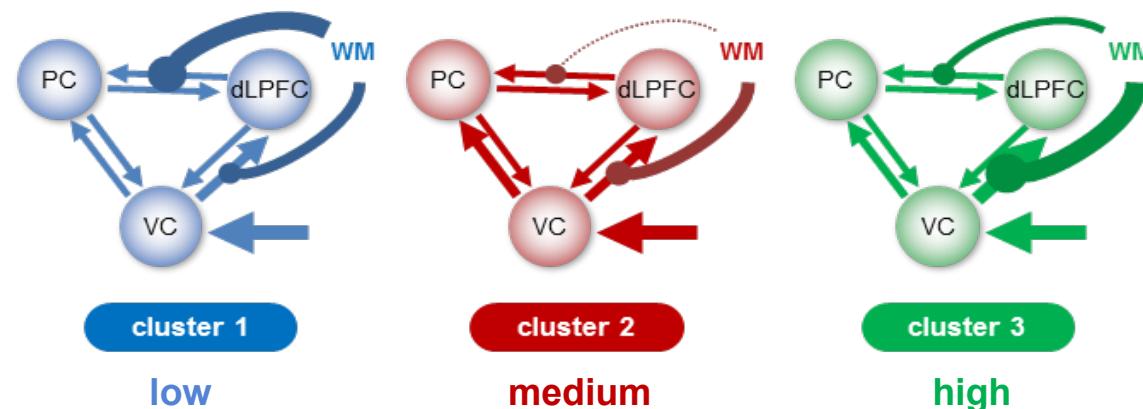
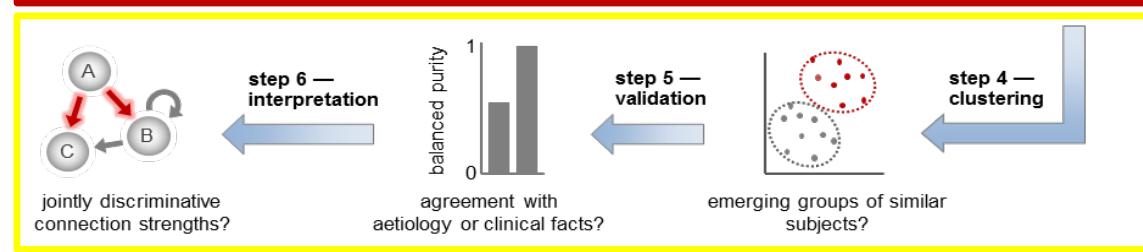
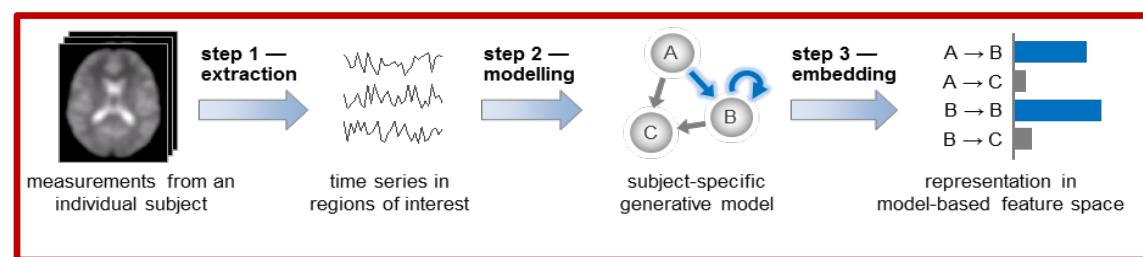
(Grossenbacher & Lovelace, 2001)



Associators



Example: DCM for physiologically plausible feature extraction (Generative embedding)





What questions can we answer using DCM?

Model comparison

What is the functional architecture of a network of brain regions?

→ Synesthesia

Are optimal models different between groups?

→ Synesthesia

Which connections are modulated by experimental manipulations?

Parameter inference

Are parameters different between individuals/groups?

Use parameters as physiologically informed summary statistics

→ Generative embedding

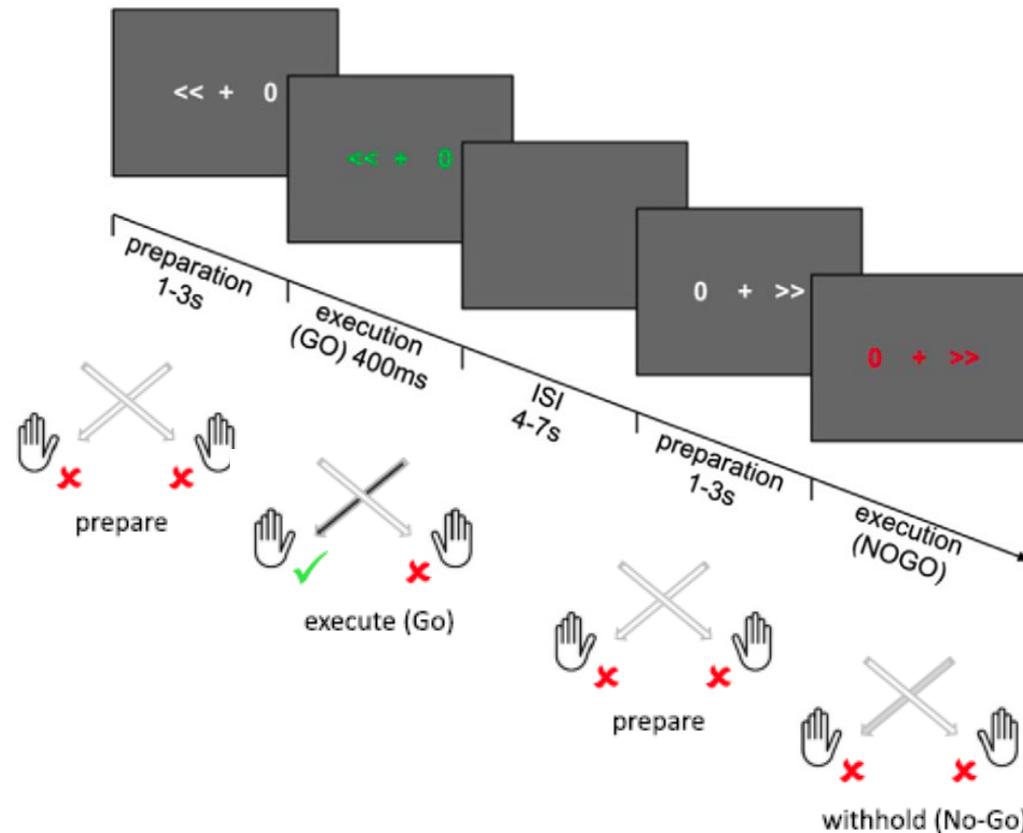
... and of course many more!



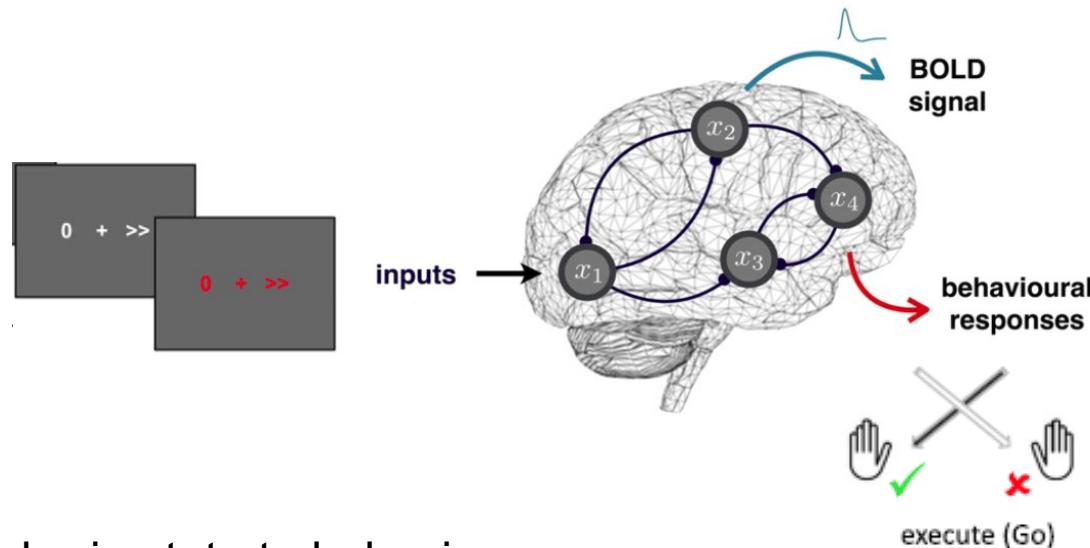
Limitations

- DCMs only have inputs, no outputs
 - Limits the study of behavioral paradigms
- Local minima
 - Variational approximation can get stuck in local minima of free energy
- Size of networks
 - Standard inversion too slow for large networks (>10 nodes).
- Regularization through fixed priors:
 - Regularization based on other data → empirical Bayes.

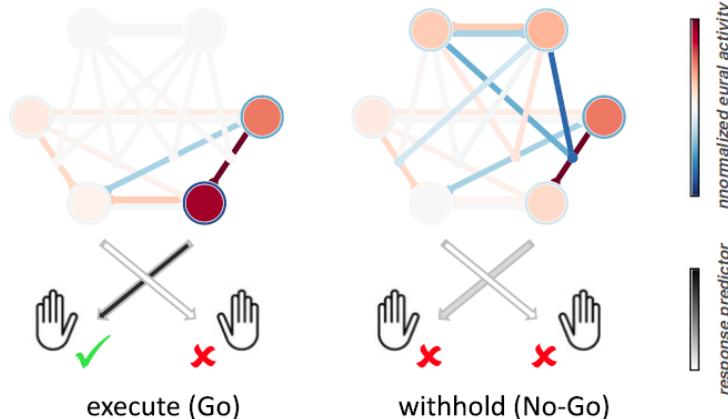
Behavioral DCM – A step towards a neurocomputational model



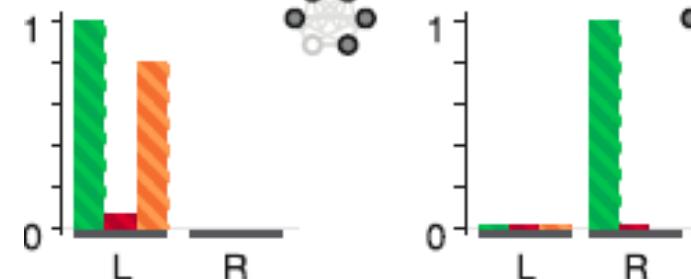
Behavioral DCM – A step towards a neurocomputational model



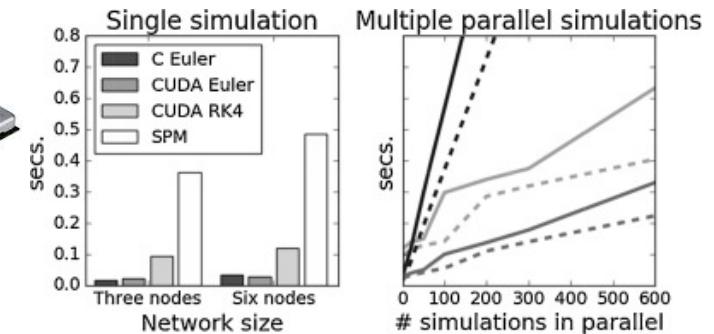
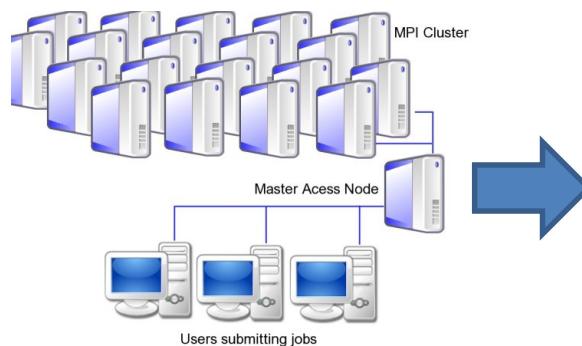
Mapping brain state to behavior



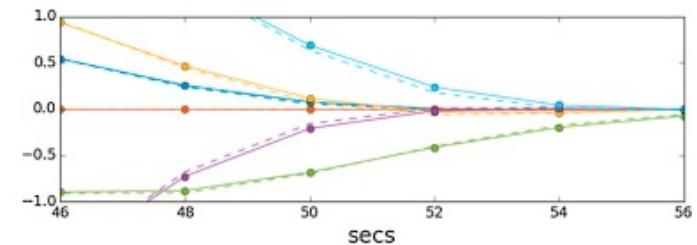
Lesion simulations



MCMC inversion of DCMs: Massively parallel DCM - mpdcm



$$\begin{aligned} \dot{x} &= f(x, u_1, \theta_1) \\ \dot{x} &= f(x, u_2, \theta_2) \\ &\vdots \\ \dot{x} &= f(x, u_n, \theta_n) \end{aligned} \quad \left. \right\} \text{mpdcm_integrate(dcms)} \quad \begin{bmatrix} y_1 \\ y_2 \\ \vdots \\ y_n \end{bmatrix}$$



- Fast inversion of DCMs
 - MCMC based inversion possible
- **Thermodynamic Integration** (alternative to Free Energy)



Recent additions to DCM for fMRI

- Massively parallel dynamic causal modelling
 - **mpdcm** Aponte et al., J Neuroscience Methods, 2016
- Regression dynamic causal modelling
 - **rDCM** Frässle et al., Neuroimage, 2017
- Hierarchical unsupervised generative embedding
 - **HUGE** Yu et al., Neuroimage, 2019

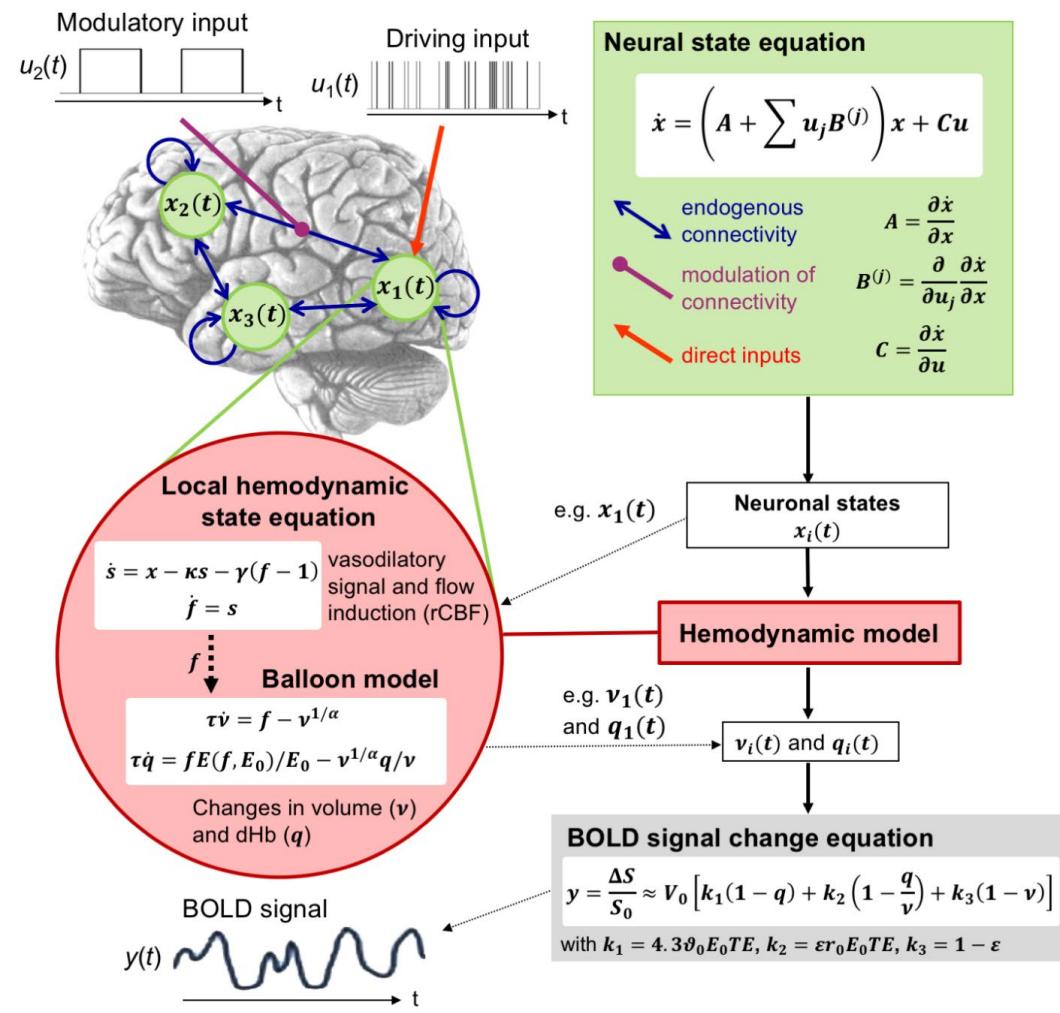
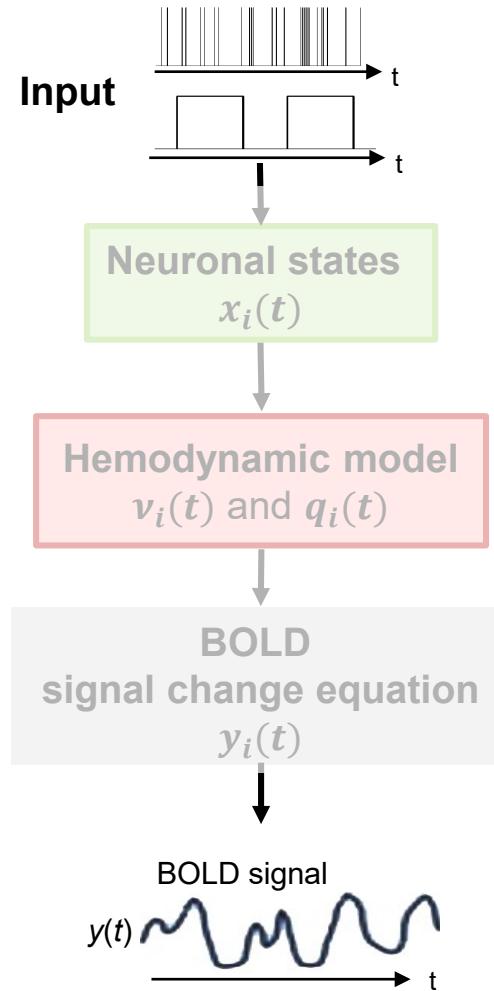
Models of Connectivity:
Advanced
→ Today, 10:50
→ Stefan Frässle
and Yu Yao

Available in TAPAS:
www.translationalneuromodeling.org/tapas

Summary – Generative model



Summary – Generative Model

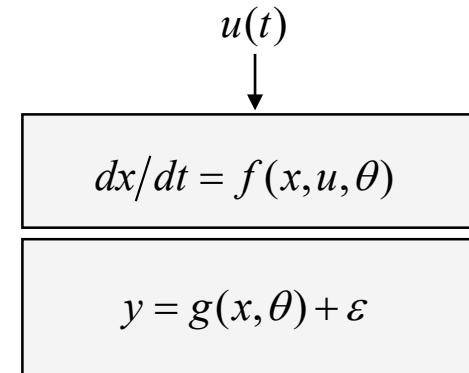


Summary - Bayesian System Identification

Neural (and hemo-)
dynamics

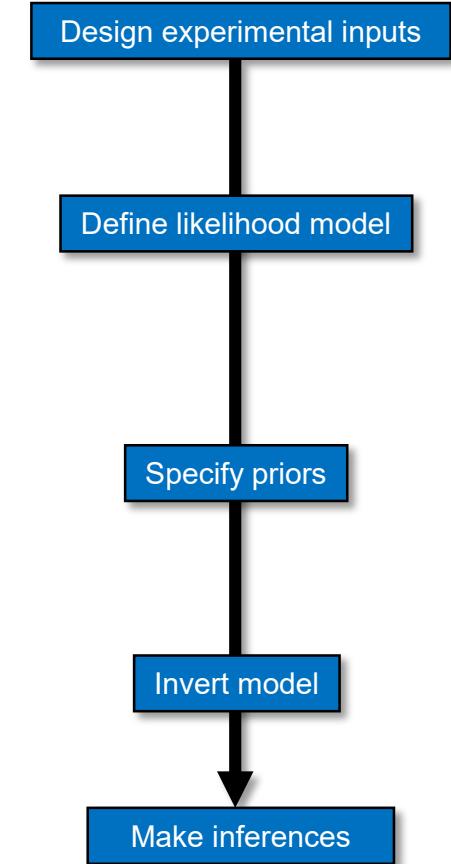
Observer function

Inference on
model structure
Inference on
parameters



$$p(y | \theta, m) = N(g(\theta), \Sigma(\theta))$$
$$p(\theta, m) = N(\mu_\theta, \Sigma_\theta)$$

$$p(y | m) = \int p(y | \theta, m) p(\theta) d\theta$$
$$p(\theta | y, m) = \frac{p(y | \theta, m) p(\theta, m)}{p(y | m)}$$





DCM software note

Basic functionality for DCM for fMRI is provided within

SPM

<https://www.fil.ion.ucl.ac.uk/spm/>



Thank you!

Many thanks to Stefan Frässle,
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List with suggested DCM literature in Appendix of this presentation!



DCM literature (1)

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- Friston KJ, Li B, Daunizeau J, Stephan KE (2011) Network discovery with DCM. *NeuroImage* 56: 1202–1221.
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- **Frässle S, Lomakina EI, Razi A, Friston KJ, Buhmann JM, Stephan KE (2017) Regression DCM for fMRI. *NeuroImage* 155:406-421.**



DCM literature (2)

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- Li B, Daunizeau J, Stephan KE, Penny WD, Friston KJ (2011). Stochastic DCM and generalised filtering. *NeuroImage* 58: 442-457
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- **Raman S, Deserno L, Schlagenhauf F, Stephan KE (2016). A hierarchical model for integrating unsupervised generative embedding and empirical Bayes. *Journal of Neuroscience Methods* 269: 6-20.**
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DCM literature (3)

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- **Yao Y, Raman SS, Schiek M, Leff A, Frässle S, Stephan KE (2018). Variational Bayesian Inversion for Hierarchical Unsupervised Generative Embedding (HUGE). *NeuroImage*, 179: 604-619**