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11 12	Custom-molded headcases have limited efficacy in reducing head motion for fMRI
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38 Abstract

Effectively minimizing head motion continues to be a challenge for the collection of functional magnetic resonance imaging (fMRI) data. The development of individual-specific custom molded headcases have been offered as a promising solution to minimizing motion during data collection, but to date, only a single published investigation into their efficacy exists in the literature. That study found headcases to be effective in reducing motion during short resting state fMRI scans (Power et al, 2019). In the present work, we examine the efficacy of these same headcases in reducing motion for a larger group of participants engaged in naturalistic scanning paradigms that consist of long movie-watching scans (~20-45min), as well as speaking aloud inside the MRI. Unlike previous work, we find no reliable reduction in head motion during movie viewing when comparing participants with headcases to those who were simply situated with foam pillows or foam pillows with medical tape. Surprisingly, we also find that for those wearing headcases, head motion is worse while talking relative to those situated with just foam pillows. These differences appear to be driven by large brief rotations of the head as well as translations in the z-plane as participants speak. Smaller, constant head movements appear equivalent with or without headcases. The largest reductions in head motion are observable when participants were situated with both foam pillows and medical tape, consistent with recent work by Kraus and colleagues (2019). Altogether, this work suggests that in a non-clinical, non-developmental population, custom-molded headcases may provide limited efficacy in reducing head motion beyond existing tools available to researchers. We hope this work can help improve the quality of custom headcases, motivate the investigation of additional solutions, as well as help researchers make more informed decisions about their data acquisition procedures.

Keywords

fMRI, head-motion, framewise-displacement, naturalistic-paradigms, head-mold

1. Introduction

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92 93 Head motion is a pernicious problem in functional magnetic resonance neuroimaging (fMRI) research and has been estimated to account for 30-90% of the total signal variance (Friston et al., 1996). Notably, motion during scans produces highly variable signal disruptions that dramatically change the readout of the global and voxel signals (Power et al., 2012; Satterthwaite et al., 2013; Van Dijk et al., 2012). Head motion is often exacerbated in developmental and clinical populations (Satterthwaite et al., 2012; Vanderwal et al., 2015) and makes it difficult to estimate task-specific activations when motion is correlated with stimulus onsets (Bullmore et al., 1999). Functional connectivity analyses (fcMRI) are particularly susceptible to head motion, which introduces spurious but systematic correlations across brain regions (Power et al., 2012; Van Dijk et al., 2012; Yan et al., 2013). Spurious correlations demonstrate regional variability and are often more pronounced in prefrontal areas including the default and prefrontal networks (Van Dijk et al., 2012; Yan et al., 2013).

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A large body of work continues to investigate various post-acquisition preprocessing and analytic strategies to mitigate the effects of head motion on the fMRI signal, including but not limited to: ICA-based nuisance removal, PCA-based nuisance regression, voxel-specific realignment regression (including Volterra expansion), scrubbing, white-matter and cerebrospinal fluid space nuisance regression, and global signal regression (Behzadi et al., 2007; Friston et al., 1996; Hallquist et al., 2013; Jo et al., 2013; Mowinckel et al., 2012; Muschelli et al., 2014; Power et al., 2012; Satterthwaite et al., 2012; Siegel et al., 2014; Tyszka et al., 2014; Yan et al., 2013) (for a review see: (Power et al., 2015). However, another class of solutions involves *minimizing* head motion during the acquisition of brain volumes. While some technical solutions like prospective acquisition correction (Thesen et al., 2000) have been used to correct motion in near real-time, more common solutions involve situating individuals within the scanner in a way that restricts movement of the head in the first place. Such techniques include the use of foam head-coil stabilizers and a bite-bar, thermoplastic masks over the nose and brow, general foam padding packed into the head-coil, visual feedback systems that allow participants to adjust their head position during a study, and tactile feedback using medical tape (Bettinardi et al., 1991; Fitzsimmons et al., 1997; Krause et al., 2019; Menon et al., 1997; Power et al., 2019; Thulborn, 1999; Zaitsev et al., 2015). Other techniques include training, mock-scanning, and using specialized movie stimuli to improve compliance in developmental and clinical populations (Vanderwal et al., 2019). While these approaches have proved promising, they can also make collecting data more logistically challenging and can increase participant discomfort, resulting in poor widespread adoption except in the case of developmental or clinical populations (Zaitsev et al., 2015).

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A recent novel solution involves the use of custom-molded head stabilizers ("headcases"), developed on a per-individual basis and conformant to an individual's unique anatomy. These custom head molds are milled from rigid styrofoam and distributed by the commercial company Caseforge (https://caseforge.co). Molds are produced from 3D optical scans of each participant's head, providing a custom fit that accounts for the shape of each individual's skull,

neck, and facial structure. Taking such factors into account has been claimed to prevent motion and more precisely position participants within a scanner, while also increasing comfort. While advertised as a promising alternative to previous approaches for reducing motion during acquisition, to date, only a single systematic investigation of the efficacy of these claims has been published in the literature (Power et al., 2019). One additional single participant dataset with and without headcases is also publicly available, but has been primarily used to investigate respiratory oscillations during multiband acquisition (Etzel & Braver, 2018). In their investigation, Power et al (2019) found that the use of headcases reduced motion during brief (4.8 min) resting state fMRI (rsfMRI) acquisitions in a group of 14 participants aged 7-28 years old. Their primary findings describe how headcases (1) decreased head motion in both rotational and translational axes, (2) reduced the fraction of a scan with large motions measured using mean and median Framewise Displacement (a composite measure of head motion calculated from the realignment of functional volumes (Power et al., 2012, 2015)), and (3) reduced the size of the small, constant motions throughout the scan.

In the present work we test the efficacy of these same custom-molded headcases in the context of "naturalistic" experimental designs that involve movie watching and talking aloud in the scanner environment. Many recent studies have utilized this "task-free" approach to probe neural representations and cognition because it can capture a larger degree of individual variability in cognitive and neural responding (Vanderwal et al., 2019). This approach also provides researchers with an opportunity to utilize rich datasets to ask a variety of questions, free of the constraints that come with pre-committing to a particular experimental design (Kriegeskorte et al., 2008). However, many of these studies often involve much longer acquisition times ranging from ~15 minute continuous runs e.g. (Haxby et al., 2011) up to ~45 minutes e.g. (Chang et al., 2018) providing more opportunities for participants to move (Meissner et al., 2019). Some studies additionally ask participants to speak aloud during scanning, certainly exacerbating head motion, as participants must enunciate organically, while lying as still as possible (Baldassano et al., 2017; Chen et al., 2017; Silbert et al., 2014; Stephens et al., 2010; Zadbood et al., 2017). These designs provide an excellent opportunity to examine the efficacy of custom headcases in reducing motion under more demanding situations that increase the likelihood of movement.

Therefore, the present work builds upon the examination by Power et al (2019) in several key ways: a) we compare movement from datasets representative of recent naturalistic experiments using much longer acquisitions (\sim 45 continuous run); b) we report between group comparisons with larger sample sizes (N=26-35 vs N=14); c) we take advantage of between group comparisons that are matched on nearly every acquisition feature (i.e. scanner site, parameters, stimulus, etc.) or experimental task (i.e. active verbal recall of a previously watched movie) when matching acquisition features is not possible; d) compare movement from datasets in which participants are speaking aloud, providing a more rigorous test of the performance of headcases under more demanding scenarios. For consistency and direct comparison, we utilize the same approach as Power (2019), focusing primarily on Framewise Displacement as a global metric for head motion (Power et al., 2012, 2015), rather than changes in signal variability which

can be driven by stimulus content or participant specific idiosyncrasies (e.g. attention, self-relevance) (Finn et al., 2019). We also examine individual translational and rotational motion axes when participants talk aloud, to better identify the directions in which head motion is exacerbated.

Our principal analyses focus on comparisons of the utility of custom-designed headcases while participants *view* a single episode of a television show or *talk* aloud about the narrative of that television show. Viewing comparisons comprise two datasets collected in an identical fashion at the same site, from the same population, viewing the same episode either with or without headcases. These comparisons also include an additional dataset collected in a similar fashion albeit at a different site, from a different but comparable population, using different acquisition parameters without headcases. This particular dataset served as an additional control to ensure that any differences (or lack thereof) between the two similarly acquired datasets were not driven by site, stimulus, or population idiosyncrasies. Talking comparisons comprise two of the three viewing datasets which were collected at different sites, but involved the same experimental task: freely recalling aloud the narrative of each respective television episode with minimal time constraints.

2. Methods

All reported analyses are comprised of observations from three different datasets. Datasets 1 and 3 come from previously published studies (Chang et al., 2018) and (Chen et al., 2017). A more detailed description of the data collection and preprocessing procedures are available in those initial publications, but we provide an abbreviated summary of the methods here. Separate manuscripts using Dataset 2 are forthcoming, but the subset of data used in the current manuscript was collected in a fashion identical to Dataset 1 with the addition of custom-molded headcases manufactured by Caseforge. Datasets 1 and 2 were collected at Dartmouth College while Dataset 3 was collected at Princeton University. All participants provided informed written consent in accordance with the experimental guidelines set by their respective institutions: the Committee for the Protection of Human Subjects at Dartmouth College and the Institutional Review Board at Princeton University.

2.1 Dataset 1 (FNL no-headcase)

2.1.1 Participants & Procedure

Thirty-five (M_{age} = 19.0; SD_{age} = 1.07; 26 female) Dartmouth College undergraduate students were recruited from introductory psychology and neuroscience courses, participating for either monetary compensation (\$20/hr) or for partial course credit. Each participant watched one episode of the television drama *Friday Night Lights* (FNL) while undergoing one continuous run of fMRI. Audio was delivered using MR compatible in-ear headphones (Sensimetrics S14 https://www.sens.com/products/model-s14/). Participants were situated in the scanner with foam pillows and medical tape attached to their foreheads which provided tactile feedback (Krause et

al., 2019) regarding head motion. Participants were also carefully instructed to lie as still as possible. For more details, see methods for Study 2 in (Chang et al., 2018).

2.1.2 Imaging Acquisition

Data were acquired at the Dartmouth Brain Imaging Center (DBIC) on a 3T Siemens Magnetom Prisma scanner (Siemens, Erlangen, Germany) with a 32-channel phased-array head coil. Raw DICOM images were converted to NIfTI images and stored in the brain imaging data structure (BIDS) format using ReproIn from the ReproNim framework (K. J. Gorgolewski et al., 2016; Visconti di Oleggio Castello et al., 2018). Functional blood-oxygenation-level-dependent (BOLD) images were acquired in an interleaved fashion using gradient-echo echo-planar imaging with pre-scan normalization, fat suppression, an in-plane acceleration factor of two (i.e. GRAPPA 2), and no multiband (i.e. simultaneous multi-slice; SMS) acceleration: TR/TE: 2000/25ms, flip angle = 75°, resolution = 3mm³ isotropic voxels, matrix size = 80 x 80, FOV = 240 x 240mm², 40 axial slices with full brain coverage and no gap, anterior-posterior phase encoding. Functional images were acquired in a single continuous run of 45.47 minutes (1364 TRs) which began and ended with 5 TRs of fixation.

2.2 Dataset 2 (FNL with headcase)

2.2.1 Participants

Thirty-six ($M_{age} = 22.77$; $SD_{age} = 4.73$; 27 female) Dartmouth College undergraduate and graduate students were enrolled for a three-part study, participating for either monetary compensation (\$20/hr) or for partial course credit. All reported data and analyses come from a subset of part-one and part-three of this study. One participant rescinded their desire to participate half-way through the first session and was consequently dropped from the dataset entirely. A total of 7 subjects were excluded from all reported analyses due to issues with their customized headcases: 4 participants' reported extreme discomfort with their headcases during the first session, which resulted in no headcase use in subsequent sessions; 3 participants used only the front or back of their headcases along with additional foam padding due to discomfort. Two additional participants in this sample did not use headcases at all, but were situated in the scanner using foam pillows and medical tape as in Dataset 1. This resulted in a total of 26 participants with headcases and 2 without headcases. These two participants were combined with participants from Dataset 1 for all *viewing* comparisons reported below, but were not included in any *talking* comparisons.

2.2.2 Procedure

Across three experimental sessions that took place within approximately one week, participants watched the first four episodes of the television show *Friday Night Lights* and performed several memory tasks that involved talking aloud while undergoing fMRI. All reported analyses consist of motion estimates while *viewing* the first episode during session one, and *talking* about all four episodes during a spoken recall task in session three. This recall task was similar in nature to the recall task used by Chen and colleagues (2017), in Dataset 3 (see below). Participants were asked to recall aloud the narrative events of all four episodes they had previously seen. They

were given 1 minute to plan their responses and were asked to try to speak for a minimum of 10 minutes and a maximum of 30 minutes. This task was manually ended by experimenters when individuals verbally indicated they were finished or automatically ended when the maximum recall time elapsed. Audio recordings were acquired using a MR-compatible microphone and recording system (Optoacoustic FOMRI III+ http://www.optoacoustics.com/medical/fomri-iii/features).

2.2.3 Headcase production

Prior to coming in for the multi-part study, participants were asked to visit the lab to have their heads scanned with a handheld 3D scanner purchased from the CaseForge company. 360° scans of each participant's head were acquired using procedures provided by CaseForge, which were identical to those reported by Power et al (2019). Participants wore a swim cap while being 3D photographed, as hair shape interfered with the quality and fit of the resulting case molds. Images were uploaded to the Caseforge website which verified the quality of scans and subsequently shipped a two piece customized styrofoam mold consisting of a front and back half. Headcases were utilized in lieu of any additional padding within the head coil of the MRI machine during acquisition. As in Dataset 1, participants were instructed to lie as still as possible, particularly when speaking aloud. All headcases used in this dataset were manufactured in late 2017 through August 2018.

2.2.4 Imaging Acquisition

Data were acquired at the Dartmouth Brain Imaging Center (DBIC) on a 3T Siemens Magnetom Prisma scanner (Siemens, Erlangen, Germany) with a 32-channel phased-array head coil in a manner identical to Dataset 1. Reported analyses come from a single continuous *viewing* run of 45.47 minutes (1364 TRs) which began and ended with 5 TRs of fixation and a variably ranged *talking* run ($M_{Minutes}$ = 20.09; $SD_{Minutes}$ = 6.52; $Min_{Minutes}$ = 12.1; $Max_{Minutes}$ = 31.2) which began with 5 TRs of fixation and ended with 15 TRs of fixation.

2.3 Dataset 3 (Sherlock)

2.3.1 Participants & Procedure

Twenty-two participants (M_{age} = 20.8, 10 female) from the Princeton community were recruited for monetary compensation (\$20/hr). Of this sample, 17 met exclusionary criteria in the published sample by Chen et al (2017) and thus were used in all reported analyses. We direct readers to the aforementioned manuscript for full procedural details, but in brief: participants watched a 48-min segment of the BBC television series *Sherlock* and subsequently verbally recalled the narrative of the show aloud while undergoing fMRI. During the recall task participants were instructed to talk for a minimum of 10 minutes, and were allowed to talk for as long as they wished. Experimenters manually ended the scanning run during the recall task based on verbal indication from participants. Participants were situated with foam padding and instructed to remain very still while viewing and speaking.

2.3.2 Imaging Acquisition

Data were collected on a 3T full-body scanner (Siemens Skyra) with a 20-channel head coil. Functional images were acquired using a T2*-weighted echo-planar imaging (EPI) pulse sequence (TR 1500 ms, TE 28 ms, flip angle = 64°, whole-brain coverage 27 slices of 4 mm thickness, in-plane resolution 3 × 3 mm2, FOV 192 × 192 mm2), with ascending interleaved acquisition. Reported analyses come from two *viewing* runs of 23 and 25 minutes long and a variably ranged *talking* run ($M_{Minutes}$ = 22.23; $SD_{Minutes}$ = 8.62; $Min_{Minutes}$ = 10.95; $Max_{Minutes}$ = 44.15).

2.4 Motion Estimation and Comparison

 For all three datasets, head position and motion was estimated using the FSL tool MCFLIRT (Jenkinson et al., 2002) by realigning each volume to the mean volume of the run. This yielded three translation and three rotation estimates at each volume. These parameters were used to calculate Framewise Displacement (FD) using the approach in Power et al. (2012) and implemented in nipype (K. Gorgolewski et al., 2011). This metric reflects the summation of the absolute-value backwards-differences of each parameter. Angular rotation parameters were converted to arc displacement using a 50mm radius prior to summation (Power et al., 2012, 2015, 2019). For each participant, these motion time-series were used to calculate five summary statistics following the approach in Power et al (2019): mean and median displacement (FD_{Mean}, FD_{Median}), proportion of high-motion volumes that exceeded 0.3mm of displacement (Spike_{Proportion}), and mean and median displacement excluding high-motion volumes (FD_{MeanFiltered}, FD_{MedianFiletered}). In Dataset 3, because participants viewed the stimulus across two separate runs, motion estimates were first calculated and summarized *within run* and the average of each pair of summary statistics was used for all analyses.

In order to account for different numbers of individuals in each dataset, all group comparisons were performed using permuted independent-groups non-equal variance t-tests implemented in Pymer4 (Jolly, 2018). First, for each comparison, a t-statistic was computed using Scipy (Jones et al., 2001--). Then, group labels (i.e. with or without headcase) were randomly shuffled while retaining the original group sizes and a new t-statistic was computed. This procedure was repeated 5,000 times to generate a null distribution of t-statistics. P-values were calculated by computing the number of permutations that were greater than or equal to the original t-statistic with adjustment to avoid non-zero p-values (Phipson & Smyth, 2010). Bootstrapped 95% confidence intervals around the mean difference between groups for each metric were also computed in Pymer4 by resampling with replacement from each group 5000 times while preserving the original group sizes.

To further interrogate non-significant results, equivalence tests were performed using the two-one-sided-tests (TOST) procedure (Lakens et al., 2018; Schuirmann, 1981) implemented in the pingouin python statistics library (Vallat, 2018). This was performed to estimate whether any non-significant differences between groups fell within a predefined range of *practical*

equivalence. In other words, non-significant group differences in motion alone do not provide information about practical differences between groups that may still be of interest to fMRI researchers, as small differences may still be detectable with large enough sample sizes. We chose the equivalence bounds of +/- 0.05mm for the *viewing* condition based upon the findings from Power et al (2019), and a larger range of +/- 0.15mm for the *talking* condition given the increased motion as a result of speaking aloud in the scanner. In the *viewing* condition, comparisons were made between the FNL without headcases (Dataset 1) and FNL with headcases (Dataset 2) samples, while in the *talking* condition, comparisons were made between the Sherlock (Dataset 3) and FNL with headcases (Dataset 2) samples. For each comparison, two parametric, one-tailed, independent-groups, non-equal variance t-tests were performed by adding/subtracting the equivalence bounds to the mean of one sample prior to running each comparison (Vallat, 2018). Consistent with prior conventions, the reported p-value reflects the larger of these two one-sided tests (Lakens et al., 2018).

3. Results

3.1 Lack of overall motion reduction with headcases while viewing a movie

Based on previous findings (Power et al., 2019), we expected to see reliable reductions in head motion when participants were fitted with custom headcases during fMRI scanning. However, while viewing the same stimulus (episode 1 of *Friday Night Lights*), collected on the same scanner, at the same site, with the same acquisition parameters, we found no significant difference in FD_{Mean} (Fig 1 top row, left column, blue and pink bars). Participants with headcases moved equivalent amounts on average (M = 0.129; SD = 0.102) compared to participants situated with only foam pillows and medical tape (M = 0.113; SD = 0.045), t = -0.758, p = 0.494. This was also true when comparing FD_{Median} , FNL with-case (M = 0.078; SD = 0.03), FNL no-case (M = 0.085; SD = 0.029), t = 0.857, p = .393, and the proportion of volumes with motion in excess of 0.3mm (Spike_{Proportion}) FNL with-case (M = 0.06; SD = 0.075), FNL no-case (M = 0.045; SD = 0.048), t = -0.917, t = 0.363 (Fig 1 middle and bottom rows, left column, blue and pink bars).

Despite being matched on nearly every dimension, we sought to ensure that our non-headcase sample exhibited motion typical of the range observed in similar naturalistic imaging studies, thus ensuring a fair comparison to our headcase sample. To do so, we compared motion estimates from our FNL non-headcase sample to those from a previously published dataset, in which individuals watched the first 48 minutes of the crime drama *Sherlock* (Chen et al., 2017) and were situated with foam pillows. Our non-headcase sample exhibited no significant differences in FD_{Mean} t = -0.703, p = .489, or $Spike_{Proportion}$ t = 0.723, p = .466, but did exhibit a significantly lower FD_{Median} , t = -2.061, p = .045. This translated to a significantly lower FD_{Median} for our *FNL headcase* sample relative to *Sherlock*, t = 2.60, p = .015. This suggests that motion in our non-headcase sample was comparable (and even slightly lower) relative to a similar existing non-headcase dataset. This also suggests that the lack of a significant difference

between our non-headcase and headcase samples was unlikely due to something particularly unique about this dataset (Table 1).

However, because a lack of statistically significant differences does not necessarily provide evidence for the null, we instead tried to better quantify these null results using equivalence testing (Schuirmann, 1981). Using the TOST procedure, we defined +/- 0.05mm as the equivalence bounds of our comparisons, i.e. a range of mean-differences in head motion that fMRI researchers may consider "statistically equivalent" in (Lakens et al., 2018). This range was set based upon the reported within-participant average improvement in FD_{Mean} by Power et al (2019) as a result of headcase use. We found that the observed mean differences and bootstrapped 95% confidence intervals for all motion metrics (Table 1) between headcase and non-headcase participants participants fell within this equivalence range: FD_{Mean} $p = 0.061^{1}$; FD_{Median} p < .001 (Fig 3, left column, blue points). Together, these findings suggest that headcases provide limited efficacy in reducing overall head motion in longer, more arduous, scanning scenarios that present more opportunities for participants to move.

3.2 Lack of small motion reduction with headcases while viewing a movie

Following the approach of Power et al (2019), we repeated the previous analysis, this time excluding high-motion volumes per individual (FD > 0.3mm) prior to computing and comparing summary statistics. This analysis assesses the efficacy of headcases in reducing smaller, constant head movements by ignoring parts of each individual's scan that contain substantial motion. Our findings are largely similar to the previous results. We found no significant differences in FD_{MeanFiltered} (Fig 2 top row, left column, blue and pink bars) or FD_{MedianFiltered} when comparing participants with and without headcases viewing the same stimulus. The FD_{Mean} of participants with headcases was equivalent on average (M = 0.085; SD = 0.026) compared to participants situated with only foam pillows and headtape (M = 0.093; SD = 0.025), t = 1.186, p = .244. This was also true of FD_{Median}, FNL with-case (M = 0.073; SD = 0.025), FNL no-case (M = 0.081; SD = 0.025), t = 1.33, p = .192. Equivalence tests using the same range as before also suggested that observed differences in FD_{MeanFiltered} and FD_{MedianFiltered} were of practical equivalence, ps < .001 (Fig 3, left panel, red points).

Our control analyses comparing $FD_{MeanFiltered}$ and $FD_{MedianFiltered}$ between our non-headcase sample and the *Sherlock* sample of participants without headcases produced similar results. We observed no significant difference in $FD_{MeanFiltered}$, t = -1.541, p = .134, but did observe a difference in $FD_{MedianFiltered}$ t = -2.368, p = .022. This translated to a significant $FD_{MeanFiltered}$ difference between the *Sherlock* sample and *FNL headcase* sample t = 2.43, p = .022 as well as a significant $FD_{MedianFiltered}$ t = 3.319, p = .002 (Fig 2 bottom row, left column; Table 2).

¹ Reporting conventions for TOST results typically reflect the *higher* p-value of each one-sided test. In this case the higher value reflects the *lower bound* of -0.05mm which reflects a motion *increase* as a result of using headcases. Observed mean differences however, are fully contained within the *upper bound* of 0.05mm p < 0.001, which reflects a motion *decrease* and is likely of more interest to fMRI researchers.

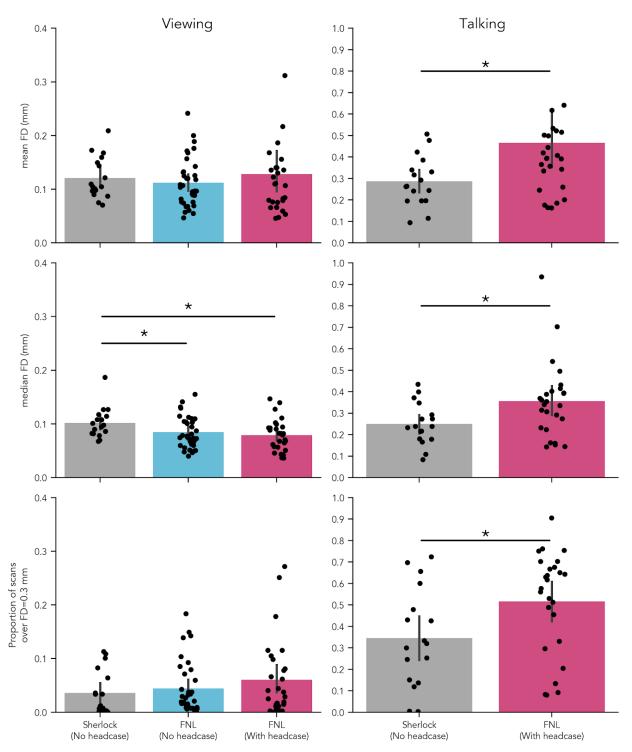


Figure 1 | Headcase effects on Framewise Displacement when viewing and speaking inside the scanner

Top row: average of participant mean FD; middle row: average of participant median FD; bottom row: proportion of

TRs in which FD exceeded 0.3mm. Blue and pink bars reflect two groups of participants who watched the same

stimulus (Friday Night Lights) under the same data collection procedures (e.g. parameters, scanner site) except for

the use of headcases. The grey bars reflect a group of subjects who watched a different stimulus (Sherlock) collected

at a different site with different acquisition parameters. Sherlock participants, however, performed the same talking

task inside the scanner albeit without headcases (right column). No significant improvement in mean or median FD or

proportion of high motion TRs was observed with the use of headcases during viewing between participants watching the same stimulus. However, a significant difference was observed between the median FD of the Sherlock sample and both no headcase and headcase wearing FNL samples. During talking however, all metrics suggested a significant increase in motion while wearing headcases.

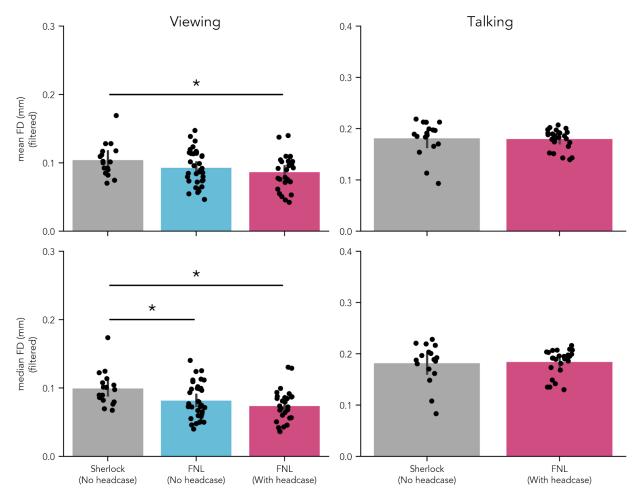


Figure 2 | Headcase effects on Framewise Displacement excluding high motion volumes

Mean and median FD differences after removing high motion TRs (FD > 0.3mm). Headcases demonstrated no detectable improvement in small head motions either during viewing or during talking. However, the Sherlock sample showed increased median FD during viewing relative to both FNL samples. Motion in the Sherlock sample was significantly higher than both FNL samples during viewing. Mean FD was higher in the Sherlock sample relative to the FNL sample with headcases.

3.3 Lack of overall motion reduction with headcases while talking aloud

While the previous analyses focused on a passive experimental "task" with a single long continuous run, our second set of analyses focused on an even more pernicious scenario for motion in neuroimaging - speaking during the scan. While several recent studies have utilized verbalization tasks in the scanner (Chen et al., 2017; Silbert et al., 2014; Stephens et al., 2010; Zadbood et al., 2017), none have compared the efficacy of custom headcases in mitigating

talking-induced head motion to our knowledge. We expected that even if headcases provided minimal reduction of head motion during passive viewing, perhaps due to increased participant compliance (Vanderwal et al., 2019), they *should* provide maximal benefit when participants move their heads as a consequence of task demands (i.e. talking). However, to our surprise, we did not find evidence supporting this hypothesis, and in some cases found the *opposite* result. When comparing *Sherlock* participants without headcases to our *FNL headcase* participants in the talking task, we found that participants wearing headcases exhibited *increased* motion across all metrics² (Fig 1 right column). Participants wearing headcases exhibited higher FD_{Mean} (M = 0.467; SD = 0.362) compared to *Sherlock* participants (M = 0.287; SD = 0.116), t = -2.353, p = .009. They also exhibited higher FD_{Median} (M = 0.356; SD = 0.177) relative to participants without headcases (M = 0.25; SD = 0.097), t = -2.534, p = .013, as well as a larger proportion of high-motion volumes (Spike_{Proportion}): with headcase (M = 0.516; SD = 0.237), without headcase (M = 0.345; SD = 0.23), t = -2.353, p = .025. These results suggest that headcases lack the efficacy to mitigate large head movement (e.g. > 0.3mm) observed in more pernicious scenarios like speaking during a scan, despite the extra restriction they place on participants (Table 3).

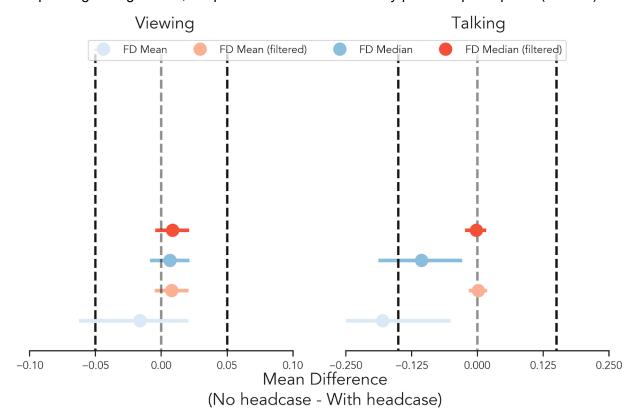


Figure 3 | Equivalence tests of motion estimates with and without headcases

Plots depict whether mean differences between groups fall within bounds of practical value to fMRI researchers. Mean differences within these bounds can be interpreted as "statistically equivalent" (Lakens et al., 2018). Darker dashed lines indicate the upper and lower bounds of the equivalence tests, while the lighter dashed lines reflect a

 $^{^2}$ We reran these comparisons excluding two headcase participants who exhibited particularly high-levels of motion overall (FD_{Mean} >= 1mm; data points not depicted in Figures), but found that headcase participants still exhibited significantly higher FD_{mean} albeit equivalent levels of motion reflected in FD_{Median} and Spike_{Proportion} (see Supplementary Materials).

difference of 0. The upper positive bound (right dashed lines) in each plot tests whether head motion *decreased* by at least 0.05mm (viewing) or 0.15mm (talking) when wearing headcases. The lower negative bound (left dashed line) tests whether head motion *increased* by at least 0.05mm (viewing) or 0.15mm (talking). In all cases, motion statistics were significantly below the upper equivalence bound suggesting that observed mean reductions in motion while wearing headcases are unlikely to be as large as 0.05mm when viewing or 0.15mm when talking. Estimates that included high motion volumes during the talking condition (right blue points) also fell below the lower equivalence bound, suggesting that in some situations headcases may exacerbate motion by at least 0.15mm.

3.4 Lack of small motion reduction with headcases while talking aloud

We once again repeated the previous comparison after excluding high-motion volumes per individual to examine the efficacy of headcases on smaller head movements while talking. Headcases demonstrated no significant reduction in FD_{MeanFiltered} between our sample (M = 0.18; SD = 0.019) and the *Sherlock* sample (M = 0.181; SD = 0.034) t = 0.19, p = .857. This was also true when examining FD_{MedianFiltered}: with head case (M = 0.184; SD = 0.025), without headcase (M = 0.182; SD = 0.039), t = -0.222, p = .829. To further quantify these null results (Fig 4 right column), we again performed equivalence testing using the TOST procedure, this time with larger equivalence bounds of +/- 0.15mm given the motion-inducing nature of the task. We found that for both FD_{MeanFiltered} and FD_{MedianFiltered}, observed differences in motion fell within this range of practical equivalence (Fig 5 right column, red points), ps < .001. These findings suggest that when specifically examining the reduction of smaller head movements induced while talking aloud, at best, headcases may be as efficacious as foam pillows alone (Table 3).

3.5 Causes of increased motion while wearing headcases and talking

Next, we explored what may have caused more motion while participants wearing headcases spoke aloud. We speculated that the interaction between lower jaw movements and head restriction may have paradoxically focused motion in the z-axis translation (moving head inward/outward parallel to the main axis of the scanner bore) and pitch-axis (nodding head up and down) rotation motion parameters. In other words, we hypothesized that because participants were largely restricted in every direction, but were freely moving their lower jaws, movements of the head may have been exacerbated in these planes as headcases provide no restriction of chin or lower jaw movement or tactile feedback. To test this hypothesis, we repeated our group comparison while participants talked separately for each axis of translation and rotation (Fig 4). Specifically, we compared displacement in the x, y, z, pitch, roll, and yaw axes using each participant's mean, median, and standard deviation displacement. Across all three summary statistics, we found significantly greater displacement in all rotation axes (pitch, roll, yaw), all ps < 0.05 (Table 4). We also found marginally greater mean displacement in the z-axis, p = 0.056, and significantly greater variability of displacement in both the x and z axes ps < 0.05. These findings suggest that observed differences in overall ${\rm FD}_{\rm Mean}$, ${\rm FD}_{\rm Median}$ and Spike_{Proportion} may have been driven by participants rotating their heads during talking, despite being constrained by headcases.

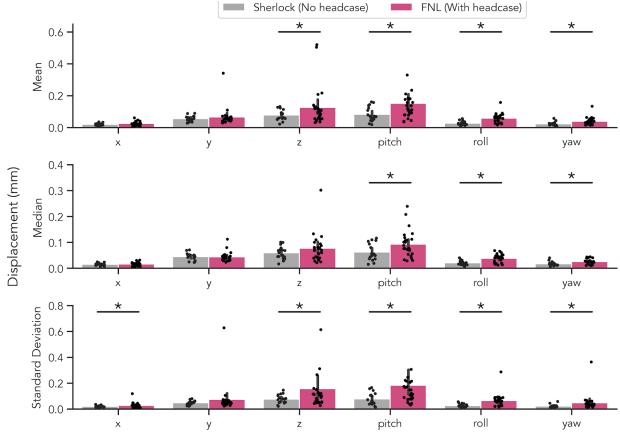


Figure 4 | Headcase effect on individual motion parameters while talking

Differences in average displacement for each motion parameter as a function of headcase use while talking (Sherlock and FNL samples). Each plot depicts the absolute value of the backwards-differenced parameter estimate (i.e. the values ultimately summed to computed FD). Top row: average of each participant's mean displacement; middle row: median displacement; bottom row: standard deviation of displacement. In all metrics, headcase participants demonstrated significantly more displacement in all rotation directions (pitch, roll, yaw) with pitch demonstrating the largest differences, likely as a result of bottom-jaw induced head movement. Significant differences were also observed in the z-axis for mean displacement and the x and z-axes for standard deviation of displacement.

4. Discussion

Using three fMRI datasets, we tested the efficacy of custom-molded headcases in reducing head motion during longer naturalistic tasks (viewing a movie or talking aloud). Unlike previous work (Power et al., 2019), which demonstrated an overall reduction in head motion when individuals wore headcases during a brief rsfMRI scan, we found that headcases provided little benefit in reducing head motion. Between group comparisons (with and without headcase) of "task-free" movie-watching indicated no significant reduction in overall head motion indexed by mean and median Framewise Displacement (FD), no reduction in the proportion of high-motion volumes (volumes in which FD exceeded 0.3mm), and no reduction in motion within small-motion volumes only (volumes in which FD was below 0.3mm). These findings are

unlikely to be driven by sampling idiosyncrasies as participants were recruited from the same population (Dartmouth College community) and scanned using the same equipment with identical acquisition parameters and stimulus. On the contrary, this population as a whole displayed less overall motion relative to a similar population that also underwent a naturalistic movie-viewing paradigm collected at a different site (Princeton University) (Chen et al., 2017). Additionally, overall motion estimates for participants in our samples were approximately similar to participants in the same age range within the sample examined by Power et al (2019).

Surprisingly, we found that participants who wore headcases produced *more* motion than those who did not during a naturalistic memory recall task, in which they spoke aloud inside the scanner. This seems to have been driven by individual volumes with large movements (FD exceeding 0.3mm), as group comparisons excluding these volumes yielded no significant differences between groups. These larger movements occurred in specific translation directions (i.e., z-axis) and across all rotational axes during talking. These findings suggest that headcases may be inadequate at restricting larger movements and in fact, may paradoxically amplify motion in scenarios that researchers might expect head motion to be worse (talking). With this finding in mind, we speculate that it is possible that by trying to restrict head motion while moving their lower jaws, participants rotate their heads *more* when wearing headcases (relative to foam pillows) increasing overall motion.

These null differences along with equivalence tests (Lakens et al., 2018) using effect sizes from previous work (Power et al., 2019) highlight the limited efficacy of headcases in reducing head motion. Researchers must balance a tradeoff between the added time, money, and effort of data quality improvement procedures and their expected benefit. For Caseforge headcases specifically, researchers must order a special 3D camera from the company, photograph each participant in a separate session prior to MRI scanning, and await the arrival of each case, and in some cases repeat this procedure if new cases contain defects or fit poorly. In our experience, nearly 20% of participants experienced discomfort when using headcases for extended periods of time precluding their use altogether or requiring adjusted procedures like using the front or back of the case only. This adds additional time and logistical challenges to data collection on top of the existing challenges that collecting MRI data requires. Because headcases are by definition personalized for each individual, they offer no reusability if these same participants are no longer available for future scanning sessions. This may encourage researchers at a given institution to encourage repeated sampling of a small subset of participants for whom headcases exist, decreasing the generalizability of empirical findings (Henrich et al., 2010; Yarkoni, 2019).

In the datasets analyzed here, each participant without a headcase was situated with foam pillows only (Dataset 3) or both foam pillows and medical tape (Dataset 1). We found this procedure to be adequate and flexible in a non-clinical, non-developmental population without the added burden of acquiring headcases. Interestingly, we found that participants for whom medical tape was used actually produced less overall motion relative to those who were situated with foam pillows alone (*FNL no headcase* vs *Sherlock*). We believe that this was driven by the

tactile feedback on participants' foreheads provided by the tape rather than any additional movement constraints. This is consistent with recent findings by Kraus et al (2019) who observed less within-run, between-run, and drifting head motion when using medical tape. Specifically, they observed that the efficacy of tactile feedback scaled with the amount of motion observed without tactile feedback, making this procedure particularly appealing when participants are likely to move a lot. Their findings also appear to be independent of behavioral tasks performed in the scanner and are efficacious even in situations when a participant is deliberately asked to move their head (Krause et al., 2019). Another promising alternative is the use of inflatable head pillows (e.g. Pearltec MULTIPAD Positioning System, Newmatic Medical, 2020) which may offer a compromise between completely head conforming designs like headcases and more general approaches like foam pillows. However, to our knowledge a systematic investigation using inflatable pillows has not yet been conducted.

The goal of the present work is to provide an in-depth analysis of the utility of headcases in reducing head motion³. Currently, there is only a single published investigation on the efficacy of headcases conducted using a small sample of 14 individuals and a short rsfMRI scan of 4.8 minutes (Power et al., 2019). Our work adds to the existing literature to help researchers make a more informed decision about their data collection procedures. We are grateful that companies like Caseforge are working on developing fast, customizable, and accessible pipelines to battle the pernicious issue of head motion for fMRI and hope that these results may lead to improvements in the design and manufacturing processes. Through private communication with Caseforge (Gao, 2019), we were notified that the headcases used in our sample (and presumably those used by Power et al (2019)) were the first generation of their kind and that more improvements to the reliability and comfort of headcases have been made in the second and forthcoming generations. While we are unable to test these claims, they provide promise for reducing the attrition rate we observed and further reducing head motion. Our sample also consisted of a non-clinical, non-development population. Such populations often exhibit increased head motion, a scenario in which headcases may provide more observable benefits (Vanderwal et al., 2015). The figures presented in Power et al (2019) support this notion as the largest motion reductions occurred for younger participants (7-14 years old). We speculate as to whether training procedures combined with tactile feedback might be similarly successful as participants can be taught to monitor their own movements (Krause et al., 2019).

In conclusion, we provide data and comparisons that speak to the efficacy of customized headcases under highly demanding data acquisition conditions: long task-free runs of movie-watching and active verbalization. Unlike previous work, we find that customized headcases provide no significant benefits for the reduction of head motion in a non-clinical, non-developmental population. We encourage future researchers to perform additional comparisons using alternative procedures for reducing headmotion (e.g., inflatable pillows, medical tape, headcases, etc). Together these investigations can better help the broader

³ Head cases have also been advertised to ensure that an individual's head is in the same position at the iso-center of the magnetic and head coil across sessions. We were unable to evaluate this in the present work and instead focused on motion mitigation.

neuroimaging community adopt the most ideal practices to mitigate motion from contaminating fMRI data (Zaitsev et al., 2015).

Open Practices Statement

All code and data required to reproduce the analyses and figures in this manuscript is available on github at https://github.com/cosanlab/headcase and on OSF at https://osf.io/qf6vx. A preprint of this manuscript is available on bioRxiv.

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Author contributions

E.J. and S.S. collected and analyzed the data. E.J., S.S., and L.J.C. wrote the manuscript.

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Table 1. Head case comparisons while *viewing* movies

Comparison	Condition	Metric	$M_{ m extit{Difference}}$	t	$ ho_{\scriptscriptstyle perm}$
FNL no-case - FNL with-case	Viewing	FD_Mean	-0.016 (-0.063 0.02)	-0.758	0.494
FNL no-case - FNL with-case	Viewing	FD _{Median}	0.007 (-0.009 0.021)	0.857	0.393
FNL no-case - FNL with-case	Viewing	Spike _{Proportion}	-0.015 (-0.049 0.015)	-0.917	0.363
FNL no-case - Sherlock	Viewing	FD_Mean	-0.008 (-0.032 0.015)	-0.703	0.489
FNL no-case - Sherlock	Viewing	FD_Median	-0.017 (-0.034 -0.002)	-2.061	0.045
FNL no-case - Sherlock	Viewing	Spike _{Proportion}	0.009 (-0.016 0.033)	0.723	0.466
Sherlock - FNL with-case	Viewing	FD_Mean	-0.008 (-0.053 0.031)	-0.349	0.776
Sherlock - FNL with-case	Viewing	FD _{Median}	0.024 (0.007 0.042)	2.6	0.015
Sherlock - FNL with-case	Viewing	Spike _{Proportion}	-0.024 (-0.06 0.009)	-1.375	0.185

Table 2. Head case comparisons while *viewing* movies after excluding high motion TRs

Comparison	Condition	Metric	$M_{ extit{Difference}}$	t	$ ho_{\scriptscriptstyle perm}$
FNL no-case - FNL with-case	Viewing	FD _{MeanFilterd}	0.008 (-0.005 0.021)	1.186	0.244
FNL no-case - FNL with-case	Viewing	FD _{MedianFiltered}	0.009 (-0.005 0.021)	1.33	0.192
FNL no-case - Sherlock	Viewing	$FD_MeanFiltered$	-0.011 (-0.025 0.002)	-1.541	0.134
FNL no-case - Sherlock	Viewing	FD _{MedianFiltered}	-0.018 (-0.032 -0.004)	-2.368	0.022
Sherlock - FNL with-case	Viewing	$FD_{MeanFiltered}$	0.019 (0.005 0.034)	2.43	0.022
Sherlock - FNL with-case	Viewing	FD _{MedianFiltered}	0.026 (0.012 0.042)	3.319	0.002

Table 3. Head case comparisons while *talking*. Filtered values reflect comparisons after excluding high motion TRs.

Comparison	Condition	Metric	$M_{ extit{Difference}}$	t	$ ho_{ m {\it perm}}$
Sherlock - FNL with-case	Talking	FD_Mean	-0.18 (-0.343 -0.051)	-2.353	0.009
Sherlock - FNL with-case	Talking	FD_Median	-0.106 (-0.188 -0.029)	-2.534	0.013
Sherlock - FNL with-case	Talking	Spike _{Proportion}	-0.171 (-0.306 -0.032)	-2.353	0.025
Sherlock - FNL with-case	Talking	FD _{MeanFiltered}	0.002 (-0.016 0.018)	0.190	0.857
Sherlock - FNL with-case	Talking	FD _{MedianFiltered}	-0.002 (-0.024 0.017)	-0.222	0.829

Table 4. Head case comparisons while *talking*. Values reflect mean differences and bootstrapped 95% confidence intervals for motion parameters without headcase - with headcase.

Motion Parameter	Metric	Mean _{Difference}	t	$oldsymbol{ ho}_{perm}$
Х	Mean	-0.005 (-0.011 0.001)	-1.614	0.122
Υ	Mean	-0.01 (-0.037 0.009)	-0.838	0.588
Z	Mean	-0.048 (-0.102 -0.005)	-1.898	0.056
Pitch	Mean	-0.069 (-0.132 -0.02)	-2.356	0.007
Roll	Mean	-0.031 (-0.045 -0.019)	-4.596	< 0.001
Yaw	Mean	-0.016 (-0.028 -0.006)	-2.953	0.002
Х	Median	-0.001 (-0.005 0.002)	-0.608	0.552
Υ	Median	0.001 (-0.009 0.01)	0.171	0.874
Z	Median	-0.017 (-0.043 0.004)	-1.425	0.166
Pitch	Median	-0.031 (-0.055 -0.007)	-2.374	0.023
Roll	Median	-0.018 (-0.025 -0.011)	-4.674	< 0.001
Yaw	Median	-0.008 (-0.014 -0.002)	-2.748	0.011
Х	SD	-0.009 (-0.019 -0.001)	-1.890	0.043
Υ	SD	-0.026 (-0.075 0.004)	-1.141	0.216

Z	SD	-0.082 (-0.179 -0.01)	-1.838	0.040
Pitch	SD	-0.105 (-0.231 -0.026)	-1.896	0.004
Roll	SD	-0.038 (-0.061 -0.021)	-3.574	0.000
Yaw	SD	-0.027 (-0.057 -0.008)	-2.009	0.001

- 763
 Baldassano, C., Chen, J., Zadbood, A., Pillow, J. W., Hasson, U., & Norman, K. A. (2017).
- Discovering Event Structure in Continuous Narrative Perception and Memory. *Neuron*,
- 765 95(3), 709–721.e5.
- Behzadi, Y., Restom, K., Liau, J., & Liu, T. T. (2007). A component based noise correction
- method (CompCor) for BOLD and perfusion based fMRI. *NeuroImage*, 37(1), 90–101.
- Bettinardi, V., Scardaoni, R., Gilardi, M. C., Rizzo, G., Perani, D., Paulesu, E., Striano, G.,
- Triulzi, F., & Fazio, F. (1991). Head holder for PET, CT, and MR studies. *Journal of*
- 770 Computer Assisted Tomography, 15(5), 886–892.
- Bullmore, E. T., Brammer, M. J., Rabe-Hesketh, S., Curtis, V. A., Morris, R. G., Williams, S. C.
- R., Sharma, T., & McGuire, P. K. (1999). Methods for diagnosis and treatment of
- stimulus-correlated motion in generic brain activation studies using fMRI. *Human Brain*
- 774 *Mapping*, 7(1), 38–48.
- 775 Caseforge Inc. (2020). Caseforge. https://caseforge.co/
- Chang, L. J., Jolly, E., Cheong, J. H., & Rapuano, K. (2018). Endogenous variation in
- ventromedial prefrontal cortex state dynamics during naturalistic viewing reflects affective
- experience. *bioRxiv*. https://www.biorxiv.org/content/10.1101/487892v1.abstract
- 779 Chen, J., Leong, Y. C., Honey, C. J., Yong, C. H., Norman, K. A., & Hasson, U. (2017). Shared
- memories reveal shared structure in neural activity across individuals. *Nature*
- 781 *Neuroscience*, 20(1), 115–125.
- 782 Etzel, J. A., & Braver, T. S. (2018). *multibandCFtests* [Data set]. Openneuro.
- 783 https://doi.org/10.18112/OPENNEURO.DS001544.V1.1.0
- Finn, E. S., Glerean, E., Khojandi, A. Y., Nielson, D., Molfese, P. J., Handwerker, D. A., &
- 785 Bandettini, P. (2019). *Idiosynchrony: From shared responses to individual differences*
- 786 during naturalistic neuroimaging. https://doi.org/10.31234/osf.io/yeu89

- Fitzsimmons, J. R., Scott, J. D., Peterson, D. M., Wolverton, B. L., Webster, C. S., & Lang, P. J.
- 788 (1997). Integrated RF coil with stabilization for fMRI human cortex. *Magnetic Resonance in*
- 789 Medicine: Official Journal of the Society of Magnetic Resonance in Medicine / Society of
- 790 Magnetic Resonance in Medicine, 38(1), 15–18.
- 791 Friston, K. J., Williams, S., Howard, R., Frackowiak, R. S. J., & Turner, R. (1996).
- Movement-related effects in fMRI time-series. Magnetic Resonance in Medicine: Official
- Journal of the Society of Magnetic Resonance in Medicine / Society of Magnetic
- 794 Resonance in Medicine, 35(3), 346–355.
- Gorgolewski, K., Burns, C. D., Madison, C., Clark, D., Halchenko, Y. O., Waskom, M. L., &
- Ghosh, S. S. (2011). Nipype: a flexible, lightweight and extensible neuroimaging data
- processing framework in python. *Frontiers in Neuroinformatics*, 5, 13.
- Gorgolewski, K. J., Auer, T., Calhoun, V. D., Craddock, R. C., Das, S., Duff, E. P., Flandin, G.,
- Ghosh, S. S., Glatard, T., Halchenko, Y. O., Handwerker, D. A., Hanke, M., Keator, D., Li,
- X., Michael, Z., Maumet, C., Nichols, B. N., Nichols, T. E., Pellman, J., ... Poldrack, R. A.
- 801 (2016). The brain imaging data structure, a format for organizing and describing outputs of
- neuroimaging experiments. *Scientific Data*, 3, 160044.
- Hallquist, M. N., Hwang, K., & Luna, B. (2013). The nuisance of nuisance regression: spectral
- misspecification in a common approach to resting-state fMRI preprocessing reintroduces
- noise and obscures functional connectivity. *NeuroImage*, *82*, 208–225.
- Haxby, J. V., Guntupalli, J. S., Connolly, A. C., Halchenko, Y. O., Conroy, B. R., Gobbini, M. I.,
- Hanke, M., & Ramadge, P. J. (2011). A common, high-dimensional model of the
- representational space in human ventral temporal cortex. *Neuron*, 72(2), 404–416.
- Henrich, J., Heine, S. J., & Norenzayan, A. (2010). Beyond WEIRD: Towards a broad-based
- behavioral science. *The Behavioral and Brain Sciences*, 33(2-3), 111.

- Jenkinson, M., Bannister, P., Brady, M., & Smith, S. (2002). Improved optimization for the robust
- and accurate linear registration and motion correction of brain images. *NeuroImage*, 17(2),
- 813 825–841.
- Jo, H. J., Gotts, S. J., Reynolds, R. C., Bandettini, P. A., Martin, A., Cox, R. W., & Saad, Z. S.
- 815 (2013). Effective Preprocessing Procedures Virtually Eliminate Distance-Dependent Motion
- Artifacts in Resting State FMRI. *Journal of Applied Mathematics*, 2013.
- 817 https://doi.org/10.1155/2013/935154
- Jolly, E. (2018). Pymer4: Connecting R and Python for Linear Mixed Modeling. *Journal of Open*
- 819 *Source Software*, *3*(31), 862.
- Jones, E., Oliphant, T., & Peterson, P. (2001--). {SciPy}: Open source scientific tools for
- 821 *{Python}*. http://www.scipy.org
- Krause, F., Benjamins, C., Eck, J., Lührs, M., van Hoof, R., & Goebel, R. (2019). Active head
- motion reduction in magnetic resonance imaging using tactile feedback. *Human Brain*
- 824 *Mapping*, 40(14), 4026–4037.
- Kriegeskorte, N., Mur, M., & Bandettini, P. (2008). Representational similarity
- analysis--connecting the branches of systems neuroscience. *Frontiers in Systems*
- 827 Neuroscience, 2. https://www.ncbi.nlm.nih.gov/pmc/articles/pmc2605405/
- Lakens, D., Scheel, A. M., & Isager, P. M. (2018). Equivalence Testing for Psychological
- Research: A Tutorial. Advances in Methods and Practices in Psychological Science, 1(2),
- 830 259–269.
- Meissner, T. W., Walbrin, J., Nordt, M., Koldewyn, K., & Weigelt, S. (2019). Let's take a break:
- Head motion during fMRI tasks is reduced in children and adults if data acquisition is
- distributed across sessions or days. *bioRxiv*, 816116.
- Menon, V., Lim, K. O., Anderson, J. H., Johnson, J., & Pfefferbaum, A. (1997). Design and

835 efficacy of a head-coil bite bar for reducing movement-related artifacts during functional 836 MRI scanning. Behavior Research Methods, Instruments, & Computers: A Journal of the 837 Psychonomic Society, Inc, 29(4), 589-594. 838 Mowinckel, A. M., Espeseth, T., & Westlye, L. T. (2012). Network-specific effects of age and 839 in-scanner subject motion: a resting-state fMRI study of 238 healthy adults. NeuroImage, 840 63(3), 1364–1373. Muschelli, J., Nebel, M. B., Caffo, B. S., Barber, A. D., Pekar, J. J., & Mostofsky, S. H. (2014). 841 842 Reduction of motion-related artifacts in resting state fMRI using aCompCor. NeuroImage, 843 96, 22–35. 844 Newmatic Medical. (2020). Pearltec MULTIPAD Positioning System. 845 https://www.newmaticmedical.com/positioners/p/MULTIPAD-Positioning-System/ 846 Optoacoustics. (2020). FOMRI III+. http://www.optoacoustics.com/medical/fomri-iii/features 847 Phipson, B., & Smyth, G. K. (2010). Permutation P-values should never be zero: calculating 848 exact P-values when permutations are randomly drawn. Statistical Applications in Genetics 849 and Molecular Biology, 9, Article39. 850 Power, J. D., Barnes, K. A., Snyder, A. Z., Schlaggar, B. L., & Petersen, S. E. (2012). Spurious 851 but systematic correlations in functional connectivity MRI networks arise from subject 852 motion. In *Neurolmage* (Vol. 59, Issue 3, pp. 2142–2154). 853 https://doi.org/10.1016/j.neuroimage.2011.10.018 854 Power, J. D., Schlaggar, B. L., & Petersen, S. E. (2015). Recent progress and outstanding 855 issues in motion correction in resting state fMRI. Neurolmage, 105, 536–551. 856 Power, J. D., Silver, B. M., Silverman, M. R., Ajodan, E. L., Bos, D. J., & Jones, R. M. (2019). 857 Customized head molds reduce motion during resting state fMRI scans. NeuroImage, 189, 141–149. 858

Eickhoff, S. B., Hakonarson, H., Gur, R. C., Gur, R. E., & Wolf, D. H. (2013). An improved 860 861 framework for confound regression and filtering for control of motion artifact in the preprocessing of resting-state functional connectivity data. NeuroImage, 64, 240-256. 862 863 Satterthwaite, T. D., Wolf, D. H., Loughead, J., Ruparel, K., Elliott, M. A., Hakonarson, H., Gur, R. C., & Gur, R. E. (2012). Impact of in-scanner head motion on multiple measures of 864 865 functional connectivity: relevance for studies of neurodevelopment in youth. Neurolmage, 866 *60*(1), 623–632. 867 Schuirmann, D. L. (1981). On hypothesis-testing to determine if the mean of a 868 normal-distribution is contained in a known interval. *Biometrics*, 37, 617–617. 869 Sensimetrics. (2020). S14 Inset Earphones for fMRI Research. 870 https://www.sens.com/products/model-s14/ 871 Siegel, J. S., Power, J. D., Dubis, J. W., Vogel, A. C., Church, J. A., Schlaggar, B. L., & 872 Petersen, S. E. (2014). Statistical improvements in functional magnetic resonance imaging 873 analyses produced by censoring high-motion data points. Human Brain Mapping, 35(5), 874 1981–1996. 875 Silbert, L. J., Honey, C. J., Simony, E., Poeppel, D., & Hasson, U. (2014). Coupled neural 876 systems underlie the production and comprehension of naturalistic narrative speech. 877 Proceedings of the National Academy of Sciences of the United States of America, 111(43), E4687-E4696. 878 879 Stephens, G. J., Silbert, L. J., & Hasson, U. (2010). Speaker-listener neural coupling underlies 880 successful communication. In Proceedings of the National Academy of Sciences (Vol. 107, 881 Issue 32, pp. 14425–14430). https://doi.org/10.1073/pnas.1008662107 Thesen, S., Heid, O., Mueller, E., & Schad, L. R. (2000). Prospective acquisition correction for 882

Satterthwaite, T. D., Elliott, M. A., Gerraty, R. T., Ruparel, K., Loughead, J., Calkins, M. E.,

- head motion with image-based tracking for real-time fMRI. *Magnetic Resonance in Medicine: An Official Journal of the International Society for Magnetic Resonance in Medicine*, 44(3), 457–465.
- Thulborn, K. R. (1999). Visual feedback to stabilize head position for fMRI. *Magnetic Resonance* in Medicine: Official Journal of the Society of Magnetic Resonance in Medicine / Society of Magnetic Resonance in Medicine, 41(5), 1039–1043.
- Tyszka, J. M., Kennedy, D. P., Paul, L. K., & Adolphs, R. (2014). Largely typical patterns of resting-state functional connectivity in high-functioning adults with autism. *Cerebral Cortex*, 24(7), 1894–1905.
- Vallat, R. (2018). Pingouin: statistics in Python. Journal of Open Source Software, 3(31), 1026.
- Vanderwal, T., Eilbott, J., & Castellanos, F. X. (2019). Movies in the magnet: Naturalistic paradigms in developmental functional neuroimaging. *Developmental Cognitive Neuroscience*, *36*, 100600.
- Vanderwal, T., Kelly, C., Eilbott, J., Mayes, L. C., & Castellanos, F. X. (2015). Inscapes: A movie paradigm to improve compliance in functional magnetic resonance imaging. *NeuroImage*, 122, 222–232.
- Van Dijk, K. R. A., Sabuncu, M. R., & Buckner, R. L. (2012). The influence of head motion on intrinsic functional connectivity MRI. *NeuroImage*, *59*(1), 431–438.
- Visconti di Oleggio Castello, M., Dobson, J. E., Sackett, T., Kodiweera, C., Haxby, J. V., Goncalves, M., Ghosh, S., & Halchenko, Y. O. (2018). *ReproNim/reproin: 0.1.1*. https://doi.org/10.5281/zenodo.1207118
- Yan, C.-G., Cheung, B., Kelly, C., Colcombe, S., Craddock, R. C., Di Martino, A., Li, Q., Zuo, X.-N., Castellanos, F. X., & Milham, M. P. (2013). A comprehensive assessment of regional variation in the impact of head micromovements on functional connectomics. *NeuroImage*,

76, 183–201.

- Yarkoni, T. (2019). The Generalizability Crisis. https://doi.org/10.31234/osf.io/jqw35
- Zadbood, A., Chen, J., Leong, Y. C., Norman, K. A., & Hasson, U. (2017). How We Transmit Memories to Other Brains: Constructing Shared Neural Representations Via Communication. *Cerebral Cortex*, 27(10), 4988–5000.
- Zaitsev, M., Maclaren, J., & Herbst, M. (2015). Motion artifacts in MRI: A complex problem with many partial solutions. *Journal of Magnetic Resonance Imaging: JMRI*, *42*(4), 887–901.