

THE UNIVERSITY OF CHICAGO

COUPLING TRANSCRIPTIONAL DYNAMICS AND DNA STRUCTURE WITH
SINGLE MOLECULE LOCALIZATION MICROSCOPY

A THESIS SUBMITTED TO
THE FACULTY OF THE DIVISION OF THE PHYSICAL SCIENCES
IN CANDIDACY FOR THE DEGREE OF
DOCTOR OF PHILOSOPHY

DEPARTMENT OF PHYSICS

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CHICAGO, ILLINOIS
SPRING 20XX

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ABSTRACT

Eukaryotic transcription is episodic, consisting of a series of transcriptional bursts, Bursty transcriptional dynamics are well-exemplified by the transient expression of pro-inflammatory guanylate binding proteins (GBPs) - a group interferon-inducible GTPases that restrict the replication of intracellular pathogens [XXX]. Classical models of gene regulation explain transcriptional bursts by invoking stochastic binding and unbinding of transcription factors, RNA polymerase and mediator proteins at enhancer or promoter sequences. However, more recent studies have pointed towards a more cooperative picture of transcriptional control where phase-separated aggregates of DNA, RNA, and proteins form higher-order structures to control gene expression. For example, both chromatin immunoprecipitation and super resolution imaging have captured the phase separation of super-enhancer-binding proteins MED1 and BRD4 in transcriptional condensates at the *Essrb* genomic locus [XXX]. Furthermore, fluorescence microscopy techniques have colocalized MED1 and BRD4 with the GBP gene cluster alongside a reduction in the degree of disorder of 3D chromatin structure in murine macrophages after infection with *Mycobacterium tuberculosis*. Taken together, these results suggest that phase separation may play a role in the reorganization of chromatin structure during transcriptional control of innate immune response genes [XXX]. Here, we hypothesize that phase separation reduces the entropy of chromatin structure in order to induce bursty gene expression. Using single molecule localization microscopy (SMLM) to obtain super-resolution images of the H2B protein, we intend to demonstrate simultaneous (i) loss of disorder in chromatin structure (ii) formation of transcriptional condensates containing MED1 and BRD4 and (iii) non-Poissonian gene expression. The following sections discuss recent the biological evidence in more detail and summarize the single molecule microscopy techniques and biophysical models we employ to study the interactions between transcriptional condensates and the chromatin scaffold.

CHAPTER 1

SINGLE MOLECULE LOCALIZATION MICROSCOPY

1.1 Gaussian point spread functions in single molecule localization microscopy

Most detectors used for imaging have many elements (pixels) so that we can record an image projected onto the detector by a system of lenses. In fluorescence imaging, this is usually a relay consisting of an objective lens and a tube lens to focus the image onto the camera. Due to diffraction, any point emitter, such as a single fluorescent molecule, will be registered as a diffraction limited spot. The profile of that spot is often described as a Gaussian point spread function

$$G(x, y) = \frac{1}{2\pi\sigma^2} e^{-\frac{(x-x_0)^2 + (y-y_0)^2}{2\sigma^2}} + B_0 \quad (1.1)$$

Modern cameras used in light microscopy, such as scientific complementary metal oxide semiconductor (sCMOS) cameras, are powered by the photoelectric effect. Electrons within each pixel, called photoelectrons, absorb enough energy from incoming photons to be promoted to the conduction band to give electrical current which can be detected. Integration of photoelectrons during the exposure time results in a monochrome image captured by a camera. The image of a single point particle, such as a fluorescent molecule, can be thought of as two-dimensional histogram of photon arrivals and a discretized form of the classical intensity profile $G(x, y)$. The value at a pixel approaches an integral of this density over the pixel:

$$\mu_k = I_0 \lambda_k = I_0 \int_{\text{pixel}} G(x, y) dx dy \quad (1.2)$$

where $I_0 = \eta N_0 \Delta t$. The parameter η is the quantum efficiency and Δt is the exposure

time. N_0 represents the number of photons emitted per unit time, which may be itself a Poisson random variable; however, this is inconsequential since it is a fixed value for a single image of a fluorescent molecule. The value of the integral λ_k at a pixel k defines the fraction of I_0 photons observed at that pixel during the camera exposure. Since the 2D Gaussian in (1.1) has cylindrical symmetry, it is separable, and we can write

$$\lambda_k = \frac{1}{2\pi\sigma^2} \left(\int_{x_k}^{x_{k+1}} e^{-\frac{(x-x_0)^2}{2\sigma^2}} dx \right) \left(\int_{y_k}^{y_{k+1}} e^{-\frac{(y-y_0)^2}{2\sigma^2}} dy \right)$$

We can then express the Gaussian integrals over a pixel by making use of the following property of the error function

$$\frac{1}{\sqrt{2\pi}\sigma} \int_a^b e^{-\frac{(x-\mu)^2}{2\sigma^2}} = \frac{1}{2} \left(\operatorname{erf} \left(\frac{b-\mu}{\sqrt{2}\sigma} \right) - \operatorname{erf} \left(\frac{a-\mu}{\sqrt{2}\sigma} \right) \right)$$

Now, suppose the particle is known to be located at (x_0, y_0) and some square pixel k is centered on coordinates (x, y) and has a width a . Then λ_k at this pixel is

$$\lambda_k(x, y) = \lambda_x(x)\lambda_y(y) \tag{1.3}$$

where

$$\begin{aligned} \lambda_x(x) &= \frac{1}{2} \left(\operatorname{erf} \left(\frac{x + a/2 - x_0}{\sqrt{2}\sigma} \right) - \operatorname{erf} \left(\frac{x - a/2 - x_0}{\sqrt{2}\sigma} \right) \right) \\ \lambda_y(y) &= \frac{1}{2} \left(\operatorname{erf} \left(\frac{y + a/2 - y_0}{\sqrt{2}\sigma} \right) - \operatorname{erf} \left(\frac{y - a/2 - y_0}{\sqrt{2}\sigma} \right) \right) \end{aligned}$$

We are now prepared to write the shot-noise limited signal, which is a vector with units of phototelectrons

$$\vec{S} = [\text{Poisson}(\lambda_1), \text{Poisson}(\lambda_2), \dots, \text{Poisson}(\lambda_N)] \quad (1.4)$$

However this noise model is incomplete, because detectors often suffer from dark noise, which may refer to readout noise or dark current, and contributes to a nonzero signal even in the absence of incident light. Dark current is due to statistical fluctuations in the photoelectron count due to thermal fluctuations. Readout noise is introduced by the amplifier circuit during the conversion of photoelectron charge to a voltage. Here, we use the Hamamatsu ORCA v3 CMOS camera, which is air cooled to -10C and has very low dark current - around 0.06 electrons/pixel/second - and can therefore be safely ignored for exposure times on the order of milliseconds. Readout noise has been often neglected in localization algorithms because its presence in EMCCD cameras is small enough that it can be ignored within the tolerances of the localization precision. In the case of sCMOS cameras, however, the readout noise of each pixel is significantly higher and, in addition, every pixel has its own noise and gain characteristic sometimes with dramatic pixel-to-pixel variations.

On the other hand, readout noise is not negligible, and must be represented as a vector-valued random variable. It is important to note that we cannot measure the contribution by readout noise before amplification and therefore it must be expressed in units of ADU. This is in contrast to \vec{S} , which can be expressed in units of photoelectrons, because these statistical fluctuations can be predicted to be Poisson by quantum mechanics. The number of photoelectrons S_k is multiplied by a gain factor g_k which has units of $[\text{ADU}/e^-]$, which generally must be measured for each pixel. Here, we will always assume that readout noise per pixel ξ_k is Gaussian with some pixel-specific offset o_k and variance σ_k^2 .

We will now define a vector which represents the image we measure, in units of ADU:

$$\vec{H} = \vec{S} + \vec{\xi} \quad (1.5)$$

What we are after is the joint distribution $P(\vec{H})$. A fundamental result in probability theory is that the distribution of H_k is the convolution of the distributions of S_k and ξ_k ,

$$\begin{aligned} P(H_k|\theta) &= P(S_k) \otimes P(\xi_k) \\ &= A \sum_{q=0}^{\infty} \frac{1}{q!} e^{-\mu_k} \mu_k^q \frac{1}{\sqrt{2\pi}\sigma_k} e^{-\frac{(H_k - g_k q - o_k)^2}{2\sigma_k^2}} \end{aligned}$$

In practice, this expression is difficult to work with, so we look for an analytical approximation. In the following analysis we use a Poisson approximation of (1.6) - insert Komogonov distance argument from nanoscopy paper. In the Poisson approximation, the model log-likelihood is surprisingly simple

$$\begin{aligned} \ell(\vec{H}) &= \log \prod_k \frac{e^{-\mu_k} \mu_k^{n_k}}{n_k!} \\ &= \sum_k n_k \log \mu_k - \log n_k! - \mu_k \end{aligned}$$

1.1.1 The Cramer-Rao lower bound

Assuming each pixel is an independent random variable, then the likelihood of the dataset (or equivalently the joint distribution on pixels) is simply a product $\mathcal{L}(H|\theta) = \prod_k P(H_k|\theta)$. Now suppose we are given a sample from $\mathcal{L}(H|\theta)$ with unknown θ . A general task in Bayesian inference is to determine θ from the data under the model \mathcal{M} . We may then ask - does the likelihood \mathcal{L} vary as we vary the parameters? If the likelihood is flat, all parameter sets are equally likely and the data does not appear to carry much information about the parameters. Moreover, if \mathcal{L} has a number of bumps or inflection points, then we expect that maybe some parameter sets are more likely than others. The “bumpiness” of the likelihood surface is

called the Fisher information - a fundamental concept in information geometry. The Fisher information matrix $I(\theta)$ can be directly related to the curvature of the KL-Divergence over the parameter space

$$\begin{aligned}
\nabla_{\theta'}^2 D_{KL}[\mathcal{L}(H|\theta) \parallel \mathcal{L}(H|\theta')] &= -\nabla_{\theta'} \int \mathcal{L}(H|\theta) \nabla_{\theta'} \log \mathcal{L}(H|\theta') dH \\
&= -\int \mathcal{L}(H|\theta) \nabla_{\theta'}^2 \log \mathcal{L}(H|\theta') dH \\
&= -\mathbb{E}_{\theta}[\nabla_{\theta'}^2 \log \mathcal{L}(H|\theta')] \\
&= \mathbf{I}(\theta)
\end{aligned}$$

We often call the Hessian matrix the *score*. The Fisher information is the result of averaging the score over the parameter space. To be clear, the score is a function of the *data*, not the parameters. It is a measure of sensitivity of the likelihood to changes in the parameters. Of course, the Fisher information matrix also depends on the parameterization chosen. Looking at (1.4), the likelihood is a hierarchical function that maps a vector space Θ to a vector space Λ to a scalar value. Formally, we define $T : \Theta \rightarrow \Lambda$ and $W : \Lambda \rightarrow \mathbb{R}$. The parameter vector $(x_0, y_0, \sigma) \in \Theta$, the Poisson rate vector $\boldsymbol{\lambda} \in \Lambda$ and $\mathcal{L} \in \mathbb{R}$. To get the Hessian, we need the chain-rule for Hessian matrices.

$$\mathbf{H}_{(L,\theta)} = \mathbf{J}_{(\lambda,\theta)}^T \mathbf{H}_{(L,\lambda)} \mathbf{J}_{(\lambda,\theta)} + (J_{(L,\lambda)} \otimes I_n) \mathbf{H}_{(\lambda,\theta)}$$

In the second term of the equation, we have a Kronecker product between the Jacobian matrix of the likelihood with respect to the parameters of the hierarchical model ($J_{(L,\lambda)}$) and the $n \times n$ identity matrix (I_n), denoted as $J_{(L,\lambda)} \otimes I_n$. This Kronecker product gives a diagonal matrix where the elements along the diagonal are the elements of the vector $J_{(L,\lambda)}$.

This provides a concise way of summarizing the operation:

$$((J_{(L,\lambda)} \otimes I_n) \mathbf{H}_{(\lambda,\theta)})_{ij} = \sum_k \mathbf{J}_{(L,\lambda)}^{ij} \mathbf{H}_{(\lambda,\theta)}^{ijk}$$

Note that we sum over the last index to get a 3 x 3 matrix, which is not directly obvious in the compact notation.

CHAPTER 2

INFERRING DNA STRUCTURE FROM

SUPER-RESOLUTION MICROSCOPY IMAGES

CHAPTER 3

DISCRETE MODELING OF TRANSCRIPTIONAL KINETICS

3.1 The ergodic theorem

3.2 The chemical master equation

The central assumption underlying a Markov process, is the memoryless property

$$P(X_t|X_{t-1}, X_{t-2}, \dots, X_{t-N}) = P(X_t|X_{t-1})$$

A single Markov chain is the set of states $\mathbf{X} = \{X_1, X_2, \dots, X_N\}$. Such a set can be generated provided that $P(X_t|X_{t-1})$ is known. To capture $P(X_t|X_{t-1})$ for all possible pairs X_t and X_{t-1} , we define a square transition matrix $T \in \mathcal{R}^{N \times N}$ where $N = |\Omega|$. As such, the elements of T represent the probability of a transition from a state ω_j to ω_i in a unit time

$$T_{ij} = \Pr(X_t = \omega_i, | X_{t-1} = \omega_j)$$

Under these definitions, the row T_i represents the present time, and is a conditional probability distribution $P(\omega|X_{t-1} = \omega_j)$ which requires that

$$\sum_j T_{ij} = \sum_j P(X_t = \omega_j | X_{t-1} = \omega_i) = 1$$

The matrix T is not necessarily symmetric $T_{ij} \neq T_{ji}$. One should note that the columns T_j *do not* define a probability distribution $P(X_t = \omega_i | X_{t-1} = \omega_j)$ and therefore do not necessarily sum to unity. The probability $P(X_t = \omega_i | X_{t-1} = \omega_j)$ has no meaning in this context, since we have defined the rows to represent a probability of the future given the present. We simply sample $X_t \sim P(X_t = \omega_j | X_{t-1} = \omega_i)$, assign $i = j$, and repeat. It directly follows from the fundamental rules of probability, the first order dynamics for a

particular state ω_i : $P(\omega_i, t)$ is given by

$$P(\omega_i, t + dt) = P(\omega_i, t) + \mathcal{J}_i dt \quad (3.1)$$

The net probability current \mathcal{J}_i must be

$$\mathcal{J}_i = \sum_j T_{ij} P(\omega_j, t) - \sum_j T_{ji} P(\omega_i, t)$$

The first is a sum on a column and the second a sum on a row. This can be simplified further by noticing that the normalization condition implies

$$\begin{aligned} T_{ij} &= 1 - \sum_j T_{ij} (1 - \delta_{ij}) \\ &= 1 - \sum_j T_{ij} + \sum_j T_{ij} \delta_{ij} \end{aligned}$$

$$\begin{aligned} \mathcal{J}_i &= \sum_j T_{ij} P(\omega_j, t) - \sum_j T_{ji} P(\omega_i, t) \\ &= \sum_i \left(1 - \sum_j T_{ij} + \sum_j T_{ij} \delta_{ij} \right) P(\omega_j, t) - \sum_j T_{ji} P(\omega_i, t) \\ &= |\Omega| - |\Omega| + \sum_i \sum_j T_{ij} P(\omega_j, t) \delta_{ij} - \sum_j T_{ji} P(\omega_i, t) \\ &= \sum_j T_{ji} P(\omega_j, t) - \sum_j T_{ji} P(\omega_i, t) \end{aligned}$$

Notice that the Kronecker delta effectively just swaps the index. Taking the limit of (1.1), we arrive at the **master equation**

$$\frac{\partial P(\omega_i)}{\partial t} = \sum_j T_{ji}P(\omega_j, t) - T_{ij}P(\omega_i, t)$$

It is common to then define an operator \mathbf{W} s.t. $W_{ij} = T_{ij}$ and $W_{ii} = -\sum_j T_{ij}$

$$\frac{dP(\omega_i)}{dt} = \sum_j W_{ij}P(\omega_j) \rightarrow \frac{dP(\boldsymbol{\omega})}{dt} = \mathcal{J}(\boldsymbol{\omega}) = \mathbf{W}P(\boldsymbol{\omega})$$

This operator form has a solution in terms of a matrix exponential

$$P(\boldsymbol{\omega}, t) = \exp(\mathcal{J}(\boldsymbol{\omega}))$$

This matrix exponential is intractable for large $|\Omega|$. However, in the Finite State Projection algorithm, it is possible to truncate the state space $\Omega \rightarrow \tilde{\Omega}$ and obtain good estimates $\tilde{P}(\boldsymbol{\omega}, t)$ with some certificate of accuracy.

3.3 ODE model for the ensemble average

We can define the following system of ODEs for a autorepressive gene circuit

$$\frac{dm}{dt} = \frac{\beta_m}{1 + (p/k)^n} - \gamma_m m, \quad (3.2)$$

$$\frac{dr}{dt} = \beta_r m - \gamma_r r, \quad (3.3)$$

$$\frac{dp}{dt} = \beta_p r - \gamma_p p, \quad (3.4)$$

We can greatly reduce the number of parameters by nondimensionalizing the system. To that end, we define a characteristic time scale t_0 and characteristic "length" scales for

each variable: m_0, r_0, p_0 . The choice of these characteristic scale will become apparent after writing the nondimensionalized ODEs out for a general case. The derivatives transform as

$$\frac{dm}{dt} \rightarrow \frac{m_0}{t_0} \frac{dm'}{d\tau}, \quad \frac{dr}{dt} \rightarrow \frac{r_0}{t_0} \frac{dr'}{d\tau}, \quad \frac{dp}{dt} \rightarrow \frac{p_0}{t_0} \frac{dp'}{d\tau}$$

Our general system of nondimensionalized ODEs reads:

$$\begin{aligned} \frac{dm'}{d\tau} &= \frac{t_0 \beta_m}{m_0(1 + (p_0 p'/k)^n)} - \gamma_m t_0 m' \\ \frac{dr'}{d\tau} &= \frac{\beta_r t_0 m_0 m'}{r_0} - \gamma_r t_0 r' \\ \frac{dp'}{d\tau} &= \frac{\beta_p t_0 r_0 r'}{p_0} - \gamma_p t_0 p' \end{aligned}$$

Define the characteristic scales as: $t_0 = 1/\gamma_m$, $m_0 = \gamma_m^2 k / \beta_r \beta_p$, $r_0 = \gamma_m k / \beta_p$, and $p_0 = k$. Making these substitutions, we have

$$\begin{aligned} \frac{dm'}{d\tau} &= \frac{\beta}{(1 + (p')^n)} - m' \\ \frac{dr'}{d\tau} &= m' - \frac{\gamma_r}{\gamma_m} r' \\ \frac{dp'}{d\tau} &= r' - \gamma p' \end{aligned}$$

3.3.1 Telegraph model of gene expression

We will begin by writing the the system of ODEs describing the dynamics of the first moment

$$\frac{dm}{dt} = \beta_m(1 - m) - \gamma_m m \quad (3.5)$$

$$\frac{dr}{dt} = \beta_r m - \gamma_r r \quad (3.6)$$

$$(3.7)$$

This system has 4 parameters, making it difficult to directly visualize interesting relationships between parameterization and dynamics. Therefore, we will nondimensionalize this system

$$\frac{dm'}{dt} = \frac{t_0}{m_0} \beta_m - \frac{t_0}{m_0} \beta_m m_0 m' - \frac{t_0}{m_0} \gamma_m m_0 m' \quad (3.8)$$

$$\frac{dr'}{dt} = \frac{t_0}{m_0} \beta_r m_0 m' - \frac{t_0}{m_0} \gamma_r r_0 r' \quad (3.9)$$

$$(3.10)$$

Let $t_0 = 1/\gamma_m$, $m_0 = \beta_m/\gamma_m$, $r_0 = \beta_m \beta_r / \gamma_m^2$, $\gamma = \gamma_r / \gamma_m$, $\beta = \beta_m / \gamma_m$, and we have

$$\frac{dm'}{dt} = 1 - \beta m' - m' \quad (3.11)$$

$$\frac{dr'}{dt} = m' - \gamma r' \quad (3.12)$$

$$(3.13)$$

Appendices

APPENDIX A

DERIVATION OF THE FOKKER PLANCK EQUATION

A.0.1 Variational Bayes

Variational inference attempts to approximate the true posterior distribution $p(\theta|x)$ with a variational distribution $q(\theta)$, which we assume to be Gaussian. We try to minimize the KL-divergence between the variational distribution and the true posterior:

$$\begin{aligned}
D_{\text{KL}}(q(\theta)||p(\theta|x)) &= \mathbb{E}_{\theta \sim q(\theta)} \left(\log \frac{q(\theta)}{p(\theta|x)} \right) \\
&= \mathbb{E}_{\theta \sim q(\theta)} \left(\log \frac{q(\theta)p(x)}{p(\theta, x)} \right) \\
&= \log p(x) + \mathbb{E}_{\theta \sim q(\theta)} \left(\log \frac{q(\theta)}{p(x|\theta)p(\theta)} \right) \\
&= \log p(x) + \mathbb{E}_{\theta \sim q(\theta)} (\log q(\theta) - \log p(x|\theta) - \log p(\theta)) \\
&= \log p(x) + H(q) - \mathbb{E}_{\theta \sim q(\theta)} (\log p(x|\theta) + \log p(\theta))
\end{aligned}$$

Clearly the KL-divergence is minimized by minimizing this expectation. It is common to define the evidence lower bound (ELBO).

$$\mathcal{L}(x, \theta) = - \mathbb{E}_{\theta \sim q(\theta)} (\log q(\theta) - \log p(x|\theta) - \log p(\theta))$$

It is name such because

$$\log p(x) = D_{\text{KL}}(q(\theta)||p(\theta|x)) + \mathcal{L}(x, \theta) \geq \mathcal{L}(x, \theta)$$

The ELBO can be minimized when the variational distribution is easy to sample from,

for example a multivariate normal distribution and when the likelihood is tractable. The gradients of the ELBO

$$\nabla_{\Phi} \mathcal{L}(x, \theta) = - \mathbb{E}_{\theta \sim q(\theta)} (\log q(\theta) - \log p(x|\theta) - \log p(\theta))$$

multivariate Gaussian distribution:

$$p(x|\mu, \Sigma) = \frac{1}{(2\pi)^{k/2} |\Sigma|^{1/2}} \exp \left(-\frac{1}{2} (x - \mu)^T \Sigma^{-1} (x - \mu) \right)$$

Where:

x is a k -dimensional random variable μ is the mean vector Σ is the covariance matrix k is the dimension of x And the gradient with respect to mean:

$$\frac{\partial}{\partial \mu} \log p(x|\mu, \Sigma) = -\Sigma^{-1}(x - \mu)$$

And the gradient with respect to covariance matrix:

$$\frac{\partial}{\partial \Sigma} \log p(x|\mu, \Sigma) = -\frac{1}{2} \Sigma^{-1} + \frac{1}{2} \Sigma^{-1} (x - \mu)(x - \mu)^T \Sigma^{-1}$$

You can use these equations to calculate the gradient of the log-multivariate Gaussian distribution with respect to the mean and covariance matrix.

A.0.2 Kramers-Moyal Expansion

Given many instantiations of a stochastic variable x , we can construct a normalized histogram over all observations as a function of time $P(x, t)$. However, in order to systematically explore the relationship between the parameterization of the process and $P(x, t)$ we require an expression for $\dot{P}(x, t)$. If we make a fundamental assumption that the evolution of $P(x, t)$ follows a Markov process i.e. its evolution has the memoryless property, then we can write

$$P(x', t) = \int T(x', t|x, t - \tau) P(x, t - \tau) dx \quad (\text{A.1})$$

which is known as the Chapman-Kolmogorov equation. The factor $T(x', t|x, t - \tau)$ is

known as the *transition operator* in a Markov process and determines the evolution of $P(x, t)$ in time. We proceed by writing $T(x', t|x, t - \tau)$ in a form referred to as the Kramers-Moyal expansion

$$\begin{aligned} T(x', t|x, t - \tau) &= \int \delta(u - x') T(u, t|x, t - \tau) du \\ &= \int \delta(x + u - x' - x) T(u, t|x, t - \tau) du \end{aligned}$$

If we use the Taylor expansion of the δ -function

$$\delta(x + u - x' - x) = \sum_{n=0}^{\infty} \frac{(u - x)^n}{n!} \left(-\frac{\partial}{\partial x} \right)^n \delta(x - x')$$

Inserting this into the result from above, pulling out terms independent of u and swapping the order of the sum and integration gives

$$T(x', t|x, t - \tau) = \sum_{n=0}^{\infty} \frac{1}{n!} \left(-\frac{\partial}{\partial x} \right)^n \delta(x - x') \int (u - x)^n T(u, t|x, t - \tau) du \quad (\text{A.2})$$

$$= \sum_{n=0}^{\infty} \frac{1}{n!} \left(-\frac{\partial}{\partial x} \right)^n \delta(x - x') M_n(x, t) \quad (\text{A.3})$$

noticing that $M_n(x, t) = \int (u - x)^n T(u, t|x, t - \tau) du$ is just the n th moment of the transition operator T . Plugging (2.6) back in to (2.4) gives

$$P(x, t) = \int \left(1 + \sum_{n=1}^{\infty} \frac{1}{n!} \left(-\frac{\partial}{\partial x} \right)^n M_n(x, t) \right) \delta(x - x') P(x, t - \tau) dx \quad (\text{A.4})$$

$$= P(x', t - \tau) + \sum_{n=1}^{\infty} \frac{1}{n!} \left(-\frac{\partial}{\partial x} \right)^n [M_n(x, t) P(x, t)] \quad (\text{A.5})$$

Approximating the derivative as a finite difference and taking the limit $\tau \rightarrow 0$ gives

$$\dot{P}(x, t) = \lim_{\tau \rightarrow 0} \left(\frac{P(x, t) - P(x, t - \tau)}{\tau} \right) \quad (\text{A.6})$$

$$= \sum_{n=1}^{\infty} \frac{1}{n!} \left(-\frac{\partial}{\partial x} \right)^n [M_n(x, t) P(x, t)] \quad (\text{A.7})$$

which is formally known as the Kramers-Moyal (KM) expansion. The Fokker-Planck equation is a special case of (2.10) where we neglect terms $n > 2$ in the *diffusion approximation*.

Consider the following Ito stochastic differential equation

$$d\vec{x} = F(\vec{x}, t) + G(\vec{x}, t)dW$$

The SDE given above corresponds to the Kramers-Moyal expansion (KME) of a transition density $T(x', t'|x, t)$ see (Risken 1989) for a full derivation.

$$\frac{\partial P(x, t)}{\partial t} = \sum_{n=1}^{\infty} \frac{1}{n!} \left(-\frac{\partial}{\partial x} \right)^n [M_n(x, t) P(x, t)] \quad (\text{A.8})$$

where M_n is the n th moment of the transition density. In the diffusion approximation,

the KME becomes the Fokker-Planck equation (FPE) (Risken 1989). For the sake of demonstration, consider the univariate case with random variable x and the form of $T(x', t'|x, t)$ is a Gaussian with mean $\mu(t)$ and variance $\sigma^2(t)$. In this scenario, the FPE applies because $M_n = 0$ for all $n > 2$. Given that the drift $M_1(x, t) = \mu(t)$ and the diffusion $M_2(x, t) = \sigma^2(t)$, the FPE reads

$$\frac{\partial P(x, t)}{\partial t} = \left(-\frac{\partial}{\partial x} M^{(1)}(t) + \frac{1}{2} \frac{\partial^2}{\partial x^2} M^{(2)}(t) \right) P(x, t) \quad (\text{A.9})$$

We can additionally define the term in parentheses as a differential operator acting on $P(x, t)$

$$\hat{\mathcal{L}}_{FP} = \left(-\frac{\partial}{\partial x} M^{(1)}(t) + \frac{1}{2} \frac{\partial^2}{\partial x^2} M^{(2)}(t) \right) \quad (\text{A.10})$$

It is common to additionally define the probability current $J(x, t)$ as

$$J(x, t) = \left(M^{(1)}(t) - \frac{1}{2} \frac{\partial}{\partial x} M^{(2)}(t) \right) P(x, t) \quad (\text{A.11})$$

This definition provides some useful intuition. The value of $J(x, t)$ is the net probability flux into the interval between x and $x + dx$ at time t . This also allows us to write the FPE as a continuity equation

$$\frac{\partial P(x, t)}{\partial t} = -\frac{\partial J(x, t)}{\partial x} \quad (\text{A.12})$$

3.1 Poisson processes

The Poisson process can be derived very quickly by noticing that it is simply the continuous-time limit of the Binomial distribution.

$$B(m; t) = \binom{n}{m} \lambda^m (1 - \lambda)^{n-m}$$

Since λ is the fraction of successes, the expected number of successes is $\mu = n\lambda$

$$\begin{aligned} B(m; t) &= \binom{n}{m} \left(\frac{\mu}{n}\right)^m \left(1 - \frac{\mu}{n}\right)^{n-m} \\ &= \binom{n}{m} \left(\frac{\mu}{n}\right)^m \left(1 - \frac{\mu}{n}\right)^n \left(1 - \frac{\mu}{n}\right)^{-m} \end{aligned}$$

$$\begin{aligned} B(m; t) &= \frac{n!}{m!(n-m)!} \left(\frac{\mu}{n}\right)^m \left(1 - \frac{\mu}{n}\right)^n \left(1 - \frac{\mu}{n}\right)^{-m} \\ &= \frac{n!}{(n-m)!} \left(\frac{1}{n}\right)^m \left(1 - \frac{\mu}{n}\right)^{-m} \frac{\mu^m \left(1 - \frac{\mu}{n}\right)^n}{m!} \end{aligned}$$

In the first term, we can take the first m subterms of the numerator $n! = n(n-1)\dots(n-m)$ and, since $n \gg m$, each term will cancel with one factor of n from the term $1/n^m$. This leaves

$$B(m; t) = \frac{(n-m)!}{(n-m)!} \left(1 - \frac{\mu}{n}\right)^{-m} \frac{\mu^m \exp(-\mu)}{m!}$$

We now take the continuous time limit i.e. $n \rightarrow \infty$ and, again, since $m \ll n$ we are left with

$$\lim_{n \rightarrow \infty} B(m; t) = \frac{\mu^m \exp(-\mu)}{m!}$$

If an event can be detected with probability γ , the rate of the Poisson process will be reduced by that factor i.e., $\lambda' = \gamma\lambda$. Therefore, the mean and variance of the process becomes $\mu = \gamma\lambda\Delta t$