

Blood Flow in the Human Circulatory System

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Report presents modern techniques for modeling the motion of blood within a Human's Macrocirculatory System. A hemodynamics literature review is presented, summarizing key findings and methodologies. This is followed by a comprehensive mathematical and computational

Keywords: *computational hemodynamics, 0D blood-flow, 1D blood-flow, 2D-blood-flow, PINN's, finite element methods, discontinuous galerkin, Lax-Wendroff, fluid-structure interaction (FSI)*

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1 Preliminaries

Notation

\mathbb{R}	set of real numbers
\mathbb{R}^+	set of positive real numbers
\mathbb{R}^-	set of negative real numbers
\mathbb{R}^n	n-dimensional real vector space
$\Omega \subset \mathbb{R}^n$	a connected open subset of \mathbb{R}^n
$\overline{\Omega}$	the closure of Ω
$\partial\Omega$	the boundary of Ω
dx	Lebesgue measure on \mathbb{R}^n
dS	surface measure on $\partial\Omega$
dV	volume measure on Ω
∇	gradient operator
$\Delta = \nabla^2 = \nabla \cdot \nabla(\cdot)$	Laplace operator
div	divergence of a vector field
div	divergence of a tensor
v_i	i -th component of vector v
$\langle \cdot, \cdot \rangle_X$	inner product on vector space X
$\langle u, v \rangle$	inner product of vectors $u, v \in \mathbb{R}^n$
$\frac{\partial}{\partial \hat{n}} = \langle \nabla, \hat{n} \rangle$	normal derivative on $\partial\Omega$
$\ \cdot\ $	L^2 -norm
$C^k(\Omega)$	space of k times continuously differentiable functions on Ω
$C_0^k(\Omega)$	space of k times continuously differentiable functions with compact support in Ω
$C_0^k(\overline{\Omega})$	space of k times continuously differentiable functions which have bounded and uniformly continuous derivatives up to order k with compact support in Ω
$C_0^\infty(\Omega)$	space of smooth functions with compact support in Ω
$L^p(\Omega)$	Lebesgue space of p -integrable functions on Ω

Symbols and Abbreviations

\therefore	consequently
$::$	because
\Rightarrow	implies
\iff	if and only if
$:=$	defines
\equiv	equivalence
a.e.	almost everywhere
e.g.	"exempli gratia" (for example)
i.e.	"id est" (that means)
s.t.	such that
m.b.s.	m.b.s.
w.r.t.	with respect to
wlog	without loss of generality
ODE	Ordinary Differential Equation
PDE	Partial Differential Equation
PDES	System of Partial Differential Equations
IC	Initial Condition
BC	Boundary Condition
0D	Zero dimensional
1D	One dimensional
2D	Two dimensional
3D	Three dimensional
FSI	Fluid-Structure Interaction
WHO	World-Health Organization
SB	Stenotic Blockage
bpm	beats per minute
RBC	Red Blood Cell

Parameters and Units

ρ	density of blood	$\left[\frac{kg}{m^3} \right]$
η	dynamic viscosity	$\left[Pa \cdot s \right]$
μ	kinematic viscosity	$\left[\frac{m^2}{s} \right]$
τ	shear stress	
$\dot{\gamma}$	shear rate	
R	radius of vessel with diameter $2R$	
\mathbf{u}	velocity field	
p	pressure field	
W_0	Womersley number	$\left[- \right]$
Re	Reynolds number	$\left[- \right]$
Pe	Péclet number	$\left[- \right]$
c	concentration of a material element	
D	diffusion coefficient	$\left[\frac{m^2}{s} \right]$
t	time	$\left[s \right]$
T	terminal time	$\left[s \right], t > 0$
ω	angular frequency	$\left[\frac{rad}{s} \right]$
\mathbf{f}_b	body force per unit volume	$\left[\frac{N}{m^3} \right]$

Mathematical Foundations

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2 Appendix

Bibliography

Code Listings

Optional Space for supplementary code listings of computations done while investigating

Code 1: Algorithm 16.5

```
1     function foo()
2         println("Hello World")
3     end
```