

**1ST WORKSHOP ON ARTIFICIAL INTELLIGENCE
FOR BIOMEDICAL DATA – AIBIO**

Self-Attention as a Predictor of EEG Anomalies

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Overview

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Introduction & Background

Self-Attention as a Predictor of EEG Anomalies

Introduction & Background

- EEG signals are highly sensitive, low-amplitude recordings easily contaminated by **artifacts** (noise not generated by brain activity).
- Artifacts may arise from physiological (muscle tension, sweating) or technical sources (electrode detachment).
- What counts as “noise” is often **task-dependent**: a feature irrelevant for one application may be meaningful for another.
- Traditional denoising via **reconstruction/prediction errors** (Autoencoders, LSTMs) ignores contextual relevance.
- **Our idea**: Train an attention-based model on a downstream task (e.g., sleep stage classification) and use its attention patterns to infer anomalies without explicit artifact labels.

Research Methodology

Self-Attention as a Predictor of EEG Anomalies

- Counterfactual explanations provide **instance-based insights** for time-series classifiers.
- The goal is to explain why a classifier predicts a certain label:
 - Dataset: $D = \{x^{(i)}\}_{i=1}^N$, each $x^{(i)} \in \mathbb{R}^d$.
 - Classifier: $C : \mathcal{X} \rightarrow \mathcal{Y}$, labels $\mathcal{Y} = \{1, \dots, n\}$.
 - For input x , predicted label $y = C(x)$.
- For misclassified instances x_m with $C(x_m) \neq y^*(x_m)$, find **minimal modification** x'_m such that $C(x'_m) = y^*(x_m)$ and x'_m is close to x_m .
- $\Delta x_m = x'_m - x_m$ reveals dominant patterns influencing the classifier's decision.

Experiments

Self-Attention as a Predictor of EEG Anomalies

Data Preprocessing

We use the **BOAS EEG dataset**, with 128 full-night recordings from 2 channels (256 Hz), to explain classifier errors across 4 sleep stages (N1, N2, N3, REM).

- **EEG Data:**

- 30s epochs ($n_s = 7680$ samples, $n_c = 2$).
- FFT \rightarrow 0.4-30 Hz filtering \rightarrow segment into $n'_s = 300$ spectral slices.
- Extract 3 features per slice (frequency, phase, amplitude).

- **Classifier:** Two-stage convolutional network over sequences of $k = 5$ epochs:

$$X_t^f = [e_{t-k+1}, \dots, e_t] \rightarrow \hat{y}_t$$

- **Autoencoders:** Hybrid networks with convolutional and attention layers:

$$X_f^t = e_t \oplus \text{pos} \longrightarrow \hat{X}_f^t \text{ (reconstructed input)}$$

Training Process & Hyperparameters

- We pass the test dataset through each class-specific autoencoder, then classify the restyled outputs using the original classifier.
- High **classification accuracy** on restyled signals indicates the autoencoders have learned the patterns that the classifier uses for each sleep stage.

Metric	N1	N2	N3	REM
Accuracy	0.9997	0.9998	0.9260	0.9986

Results & Discussion

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Conclusion & Future Work

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Conclusion



- **xSTAE** explains classifier errors by restyling misclassified EEG instances into correctly classified ones.
- Autoencoders balance **identity loss** (keep instance similar) and **classification loss** (push to correct label), revealing features the classifier missed.
- Contributions:
 - Ground counterfactual explanations in time-series EEG classification.
 - Identify spectral representations suitable for EEG signals.
 - Validate on open BOAS dataset and release full experimental setup.

Future Work

- Explore **alternative identity losses** to highlight meaningful changes (e.g., bigger local changes, selective brainwave bands).
- Conduct **expert trials** to refine interpretability of restyled EEGs.
- Investigate linking insights from misclassifications to **actionable guidance** at the data or confidence level, keeping xSTAE model-agnostic.

Thank you for your attention!



Thank you for your attention! Any questions?

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