

Instructions for using a Mathematical Model of the Cardiovascular System Response to Fluid Perturbation (with Software Code)

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1. General Information

This software code provides a mathematical model of the cardiovascular system (CVS) response to fluid perturbation, developed and validated using data collected from animal (sheep and swine) subjects. The model is built in MATLAB Simulink environment and the goal is to generate a cohort of simulated subjects against a test subject. The simulated subjects lead to a prediction envelope, which is used to evaluate predictive capability performance of the mathematical model and show its ability to generate valid virtual CVS physiological responses to fluid perturbation for the future non-clinical simulated testing setups. These testing setups may be useful as part of assessing physiological closed-loop control algorithms for automated fluid resuscitation systems. The CVS mathematical model is a low-order lumped parameter model, designed for use with virtual cohort generation tools. It takes rates of hemorrhage, urine, and fluid infusion as inputs and produces outputs for hematocrit (HCT), blood volume (BV), heart rate (HR), stroke volume (SV), cardiac output (CO), and mean arterial blood pressure (BP). The mathematical model calibration is defined based on the maximum likelihood estimation of its parameters. A compartment-based virtual cohort generation tool described in [1] is used to simulate virtual subjects and generate a prediction envelope used for model predictive capability performance.

2. System Requirements

The software code was written in a MATLAB® R2023b environment and consists of a Simulink file "CVS_Model.mdl", and a script for prediction envelope generation for an example test data. The prediction envelope generator includes a core code "Cohort_Generation.m". The data from a representative test subject as well as mathematical model parameters calibrated against 26 animal datasets have been provided in mat files, entitled "Example_Data.mat" and "Calibrated_Parameters.mat", respectively. Software has been tested in MATLAB® R2023b environment, and it requires the Simulink Toolbox.

3. Data Preparation

HCT, HR, SV, CO and BP data from an individual subject are used for comparing generated prediction envelope with a test subject to see how the simulated subjects are capable in replicating test subjects. The data should be recorded from a subject under fluid perturbation. In this work, a 3-point median filter is applied to the collected physiological data. An individual sample dataset is included in the software for demonstration purposes. The dataset includes time instants and values for 3-hour median-filtered physiological data, fluid infusion, hemorrhage, and urine collected from a sheep subject undergoing a simulated hemorrhage [2].

4. Software Package Content

The software package includes 3 hours of physiological data, hemorrhage profile, fluid infusion profile, and urine from an individual subject that were used for predictive capability assessment. The package also includes calibrated parameters from 26 individual animal datasets used for leave-one-out cross validation of the example data. The mathematical model is presented in Simulink “CVS_Model.mdl”. Virtual cohort generation includes a main code “Cohort_Generation.m” that generates prediction envelopes for all physiological variables using the compartment method presented in [1]. Normalized interval score [1] for the generated prediction envelope was also included in the software package. The codes are presented in the appendix.

5. Input and Output of the Software Code

The input and output of the software code for generating prediction envelopes are as follows:

Inputs: i) time instants for measured physiological data “Hemo_Time”, ii) median-filtered measured physiological data “Hemo_HCT”, “Hemo_HR”, “Hemo_SV”, “Hemo_CO”, “Hemo_BP”, iii) fluid infusion “Infusion_inp”, iv) hemorrhage “Hemorrhage_inp”, and v) urine “Urine_inp” all provided for the test subject in “Example_Data.mat”, and vi) calibrated parameters from 26 animal subjects used for generating prediction envelope against the test subject provided by “Calibrated_Parameters.mat”. “Calibrated_Parameters.mat” is a 26x22 matrix, where each row includes calibrated model parameters for each training animal dataset. Outputs: prediction envelope plots and normalized interval score for generated envelopes, as well as the best simulated subject [1].

6. Mathematical Model Parameters

| | | |
|---------------|--------|---|
| BV parameters | A1 | BV state parameter for infusion |
| | A2 | BV state parameter for blood loss |
| | B_Gain | Infusion distribution factor |
| | B_Loss | Blood loss distribution factor |
| | Kp | BV proportional control gain |
| HR parameters | G1 | Constant gain for transient decrease in HR to infusion |
| | G2 | Constant gain for transient increase in HR to blood loss |
| | G3 | Constant gain for long term reference increase in HR to blood loss |
| | Pow1 | Power term for transient decrease in HR to infusion |
| | Pow2 | Power term for long term reference increase in HR to blood loss |
| | Kp4 | HR model proportional control gain for long term increase in HR to loss |
| | Ki4 | HR model integral control gain for long term increase in HR to loss |

| | | |
|---------------------|--------|--------------------------------------|
| SV parameters | Gsv1 | Proportional gain relating SV to BV |
| | Gsv2 | Proportional gain relating SV to HR |
| | A3 | SV model time constant |
| | SV_Tar | Target steady state SV |
| | Kp2 | SV model proportional control gain |
| BP parameters | A4 | BP model time constant |
| | Kp3 | BP model proportional control gain |
| | BP_Tar | Target steady state BP |
| Baseline parameters | Hct0 | Baseline hematocrit |
| | BV0 | Baseline BV |
| | HR0 | Baseline HR |
| | SV0 | Baseline SV |
| | TPR0 | Baseline total peripheral resistance |

7. Mathematical Model Use Conditions

The mathematical model is intended for use with CVS physiological data collected under hemorrhage and fluid infusion. The physiological data subject to only fluid infusion and in absence of hemorrhage could lead to different physiological state, e.g., fluid overload, which should not be used with the developed mathematical model. Data from sheep subjects were used in this study. Each animal subject underwent hemorrhage and fluid infusion, which lasted for 180 min. At the start of each animal study, a 25 ml/kg hemorrhagic shock was induced in the subjects which lasted for 15 min. At 30 min, fluid infusion was started which continued till the end of the experiment. This infusion was performed for resuscitation with a target mean arterial pressure of 90 mmHg. At 50 and 70 min marks, two small 5 ml/kg hemorrhagic shocks were induced, each lasted for 5 min. For more information about the animal study please refer to [2].

8. References

- [1] Varun Kanal, Pras Pathmanathan, Jin-Oh Hahn, George Kramer, Christopher Scully, and Ramin Bighamian, Development and Validation of a Mathematical Model of Heart Rate Response to Fluid Perturbation, Scientific Reports 12, 21463 (2022).
- [2] Abraham Rafie, Paul Rath, Michael Michell, Robert Kirschner, Donald Deyo, Donald Prough, James Grady, George Kramer, Hypotensive Resuscitation of Multiple Hemorrhages using Crystalloid and Colloids, Shock 22, 262-269 (2004).

Appendix

FDA Software Disclaimer: *This software and documentation (the "Software") were developed at the Food and Drug Administration (FDA) by employees of the Federal Government in the*

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A1: CVS Mathematical Model Simulink:

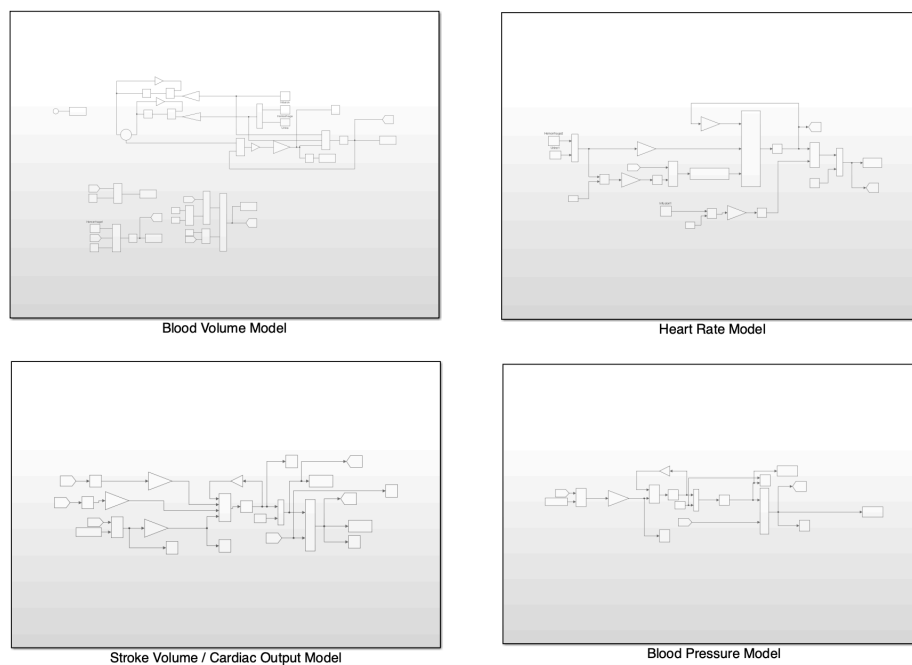


Figure 1: The entire model with 4 sub-models of BV, HR, SV (CO), and BP

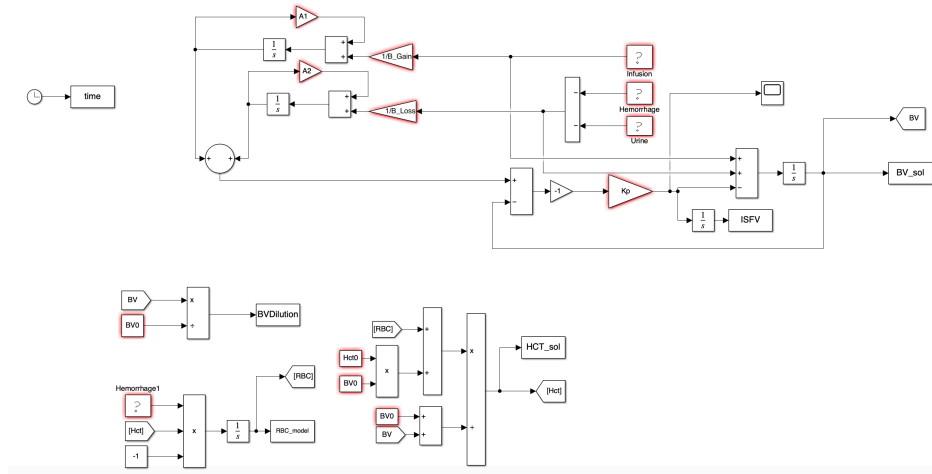


Figure 2: The BV sub-model

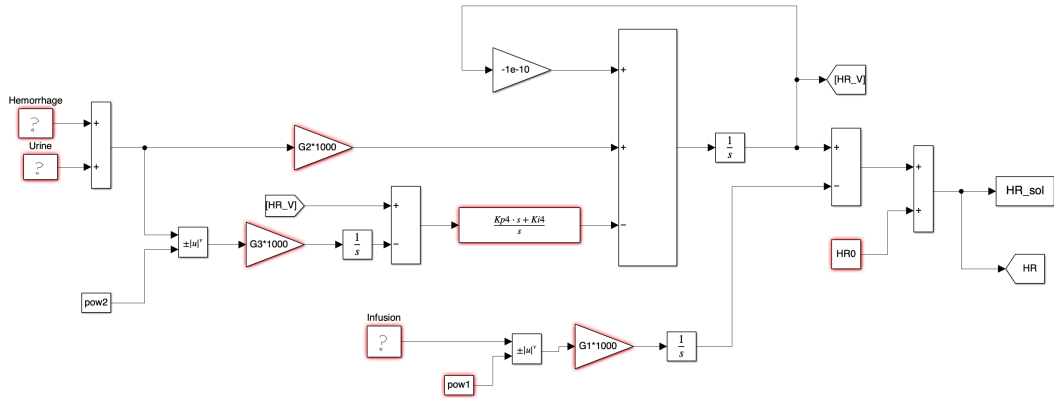


Figure 3: The HR sub-model

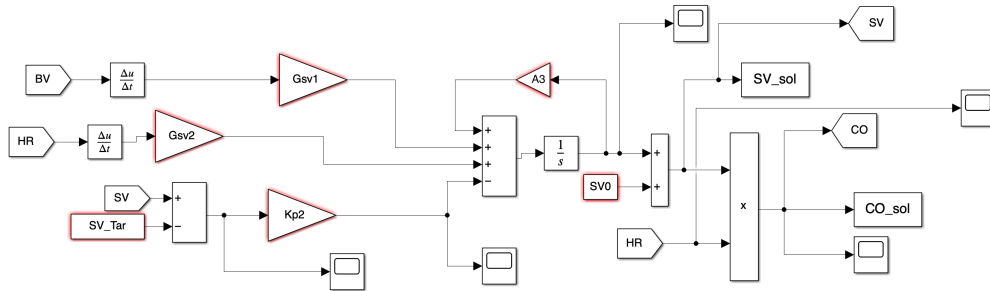


Figure 4: The SV (CO) sub-model

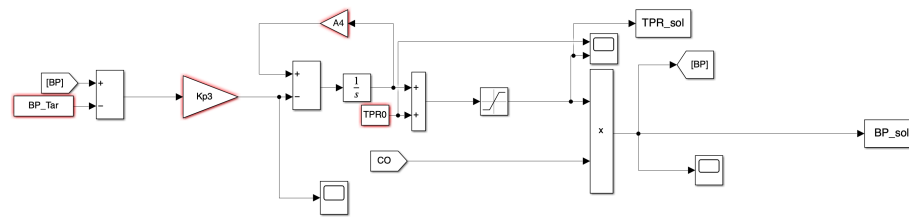


Figure 5: The BP sub-model

A2: Cohort Generation Code:

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BV and HR components of the model are published in the following papers:

BV model: Bighamian R, Hahn JO, Kramer G, Scully C. Accuracy assessment methods for physiological model selection toward evaluation of closed-loop controlled medical devices. PLoS One. 2021 Apr 30;16(4):e0251001. doi: 10.1371/journal.pone.0251001. PMID: 33930095; PMCID: PMC8087034.

HR model: Kanak V, Pathmanathan P, Hahn JO, Kramer G, Scully C, Bighamian R. Development and validation of a mathematical model of heart rate response to fluid perturbation. Sci Rep. 2022 Dec 12;12(1):21463. doi: 10.1038/s41598-022-25891-y. PMID: 36509856; PMCID: PMC9744837.

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```
clc
clear
close all
```

```
numsim = 10000;%number of all simulations
rand_IC = 0.1;%scaling factor for the baseline parameters normal distribution sampling
```

```
SamplingTime = 0.01; %sampling time for simulations
```

```
data = load('Example_Data'); %load one representative susjetc
```

```
Hemo_Time = data.DATASET.Measurements.HCT.Times; %Time and physioloigcal variables data
Infusion_inp = data.DATASET.Inputs.Infusion.Values;
Hemorrhage_inp = data.DATASET.Inputs.Hemorrhage.Values;
Urine_inp = data.DATASET.Inputs.UO.Values;
Hemo_HCT = 100*data.DATASET.Measurements.HCT.Values;
Hemo_CO = data.DATASET.Measurements.CO.Values;
Hemo_HR = data.DATASET.Measurements.HR.Values;
```

```

Hemo_SV = data.DATASET.Measurements.SV.Values/1000;
Hemo_MAP = data.DATASET.Measurements.MAP.Values;

%baseline values for BV,SV,Hematocrit
BV0_aux = data.DATASET.BV0;
SV0_aux = Hemo_SV(1);
Hct0_aux = Hemo_HCT(1);

simulation_time = (0:SamplingTime:180)'; %time vector for Simulink

%% load calibrated parameters from other 26 subjects
Par_aux = load('Calibrated_Parameters').Par_aux;

%% Sampling the parameters for the cohort
[A, B, C, D]=ndgrid(1:size(Par_aux,1),1:size(Par_aux,1),1:size(Par_aux,1),1:size(Par_aux,1));
A1=reshape(A,[],1);
B1=reshape(B,[],1);
C1=reshape(C,[],1);
D1=reshape(D,[],1);
d = [];
d=[A1,B1,C1,D1];
Cohort_1 = [];
for ii = 1:length(d) %making mixing virtual subjects
    Cohort_1(ii,:) = [Par_aux(d(ii,1),1:5) Par_aux(d(ii,2),6:10) Par_aux(d(ii,3),11:14) Par_aux(d(ii,4),15:22)];
end

[A, B, C]=ndgrid(1:size(Par_aux,1),1:size(Par_aux,1),1:size(Par_aux,1));
A1=reshape(A,[],1);
B1=reshape(B,[],1);
C1=reshape(C,[],1);
d = [];
d=[A1,B1,C1];
length(d)
Cohort_2 = [];
for ii = 1:length(d) %making average virtual subjects
    Cohort_2(ii,:) = (Par_aux(d(ii,1),:)+Par_aux(d(ii,2),:)+Par_aux(d(ii,3),:))/3;
end
ii;

Cohort = [Cohort_1;Cohort_2];%combining mixing and average cohorts of virtual subjects
n_size = length(Cohort);
%%
jj = 1;
jj_mat = randperm(n_size, numsim);
ccc = 1;
subject_par = [];
while jj <=numsim
    jj

    %specify model parameters from the virtual subjects
    x = Cohort(jj_mat(jj),:);
    A1=x(1);A2=x(2);B_Gain=x(3);B_Loss=x(4);Kp=x(5);
    Gsv1=x(6);Gsv2=x(7);A3=x(8);SV_Tar = x(9);Kp2=x(10);
    Kp3=x(11);A4=x(12);TPR0=x(13);BP_Tar=x(14);
    G1=x(15);G2=x(16);pow1=x(17);pow2=x(18);G3=x(19);Kp4=x(20);Ki4=x(21);HR0=x(22);

```

```

% randomize baseline values around the data baseline
HR0 = Hemo_HR(1)+rand_IC*Hemo_HR(1)*randn;
BV0 = BV0_aux+rand_IC*BVO_aux*randn;
SV0 = SV0_aux+rand_IC*SV0_aux*randn;
Hct0 = Hct0_aux+rand_IC*Hct0_aux*randn;
TPR0 = (Hemo_MAP(1)/Hemo_CO(1))+rand_IC*(Hemo_MAP(1)/Hemo_CO(1))*randn;

subject_par(jj,:) = [A1 A2 B_Gain B_Loss Kp Gsv1 Gsv2 A3 SV_Tar Kp2 ...
Kp3 A4 TPR0 BP_Tar G1 G2 pow1 pow2 G3 Kp4 Ki4 HR0 BV0 SV0 Hct0]; %subject model parameters

sim('CVS_Model');
response_BP(jj,:) = interp1(simulation_time,BP_sol,Hemo_Time);%down sample data to the times that physiological data
measurements are available
response_CO(jj,:) = interp1(simulation_time,CO_sol,Hemo_Time);
response_HCT(jj,:) = interp1(simulation_time,HCT_sol,Hemo_Time);
response_SV(jj,:) = interp1(simulation_time,SV_sol,Hemo_Time);
response_HR(jj,:) = interp1(simulation_time,HR_sol,Hemo_Time);

HCT_sol = [];
SV_sol = [];
CO_sol = [];
BP_sol = [];

jj = jj+1;
end
%%
for kk = 1:numsim %compute normalized root mean squared error (NRMSE)
HCT_rmse_nor(kk,1) = sqrt(mean((response_HCT(kk,:) - Hemo_HCT').^2))/(mean(Hemo_HCT));
SV_rmse_nor(kk,1) = sqrt(mean((response_SV(kk,:) - Hemo_CO'./Hemo_HR').^2))/mean(Hemo_CO./Hemo_HR);
HR_rmse_nor(kk,1) = sqrt(mean((response_HR(kk,:) - Hemo_HR').^2))/mean(Hemo_HR);
CO_rmse_nor(kk,1) = sqrt(mean((response_CO(kk,:) - Hemo_CO').^2))/mean(Hemo_CO);
BP_rmse_nor(kk,1) = sqrt(mean((response_BP(kk,:) - Hemo_MAP').^2))/mean(Hemo_MAP);

%compute normalized mean absolute error (NMAE)
HCT_MAE_nor(kk,1) = mean(abs(response_HCT(kk,:) - Hemo_HCT'))/(mean(Hemo_HCT));%Mean absolute error
SV_MAE_nor(kk,1) = mean(abs(response_SV(kk,:) - Hemo_CO'./Hemo_HR'))/mean(Hemo_CO./Hemo_HR);
HR_MAE_nor(kk,1) = mean(abs(response_HR(kk,:) - Hemo_HR'))/mean(Hemo_HR);
CO_MAE_nor(kk,1) = mean(abs(response_CO(kk,:) - Hemo_CO'))/mean(Hemo_CO);
BP_MAE_nor(kk,1) = mean(abs(response_BP(kk,:) - Hemo_MAP'))/mean(Hemo_MAP);

%NRMSE and NAME averaged across all variables to find best simulated subjects
mean_NRMSE (kk,1) =
(HCT_rmse_nor(kk,1)+SV_rmse_nor(kk,1)+HR_rmse_nor(kk,1)+CO_rmse_nor(kk,1)+BP_rmse_nor(kk,1))/5;
mean_NMAE (kk,1) = (HCT_MAE_nor(kk,1)+SV_MAE_nor(kk,1)+HR_MAE_nor(kk,1)+CO_MAE_nor(kk,1)+BP_MAE_nor(kk,1))/
5;

% max_NRMSE (kk,1) = HCT_rmse_nor(kk,1)+SV_rmse_nor(kk,1)+HR_rmse_nor(kk,1)+BP_rmse_nor(kk,1);
max_NRMSE (kk,1) =
max([HCT_rmse_nor(kk,1);SV_rmse_nor(kk,1);HR_rmse_nor(kk,1);CO_rmse_nor(kk,1);BP_rmse_nor(kk,1)]);
max_NMAE (kk,1) =
max([HCT_MAE_nor(kk,1);SV_MAE_nor(kk,1);HR_MAE_nor(kk,1);CO_MAE_nor(kk,1);BP_MAE_nor(kk,1)]);
end

```



```

% find best simulated subject in terms of NRMSE
min_ind = find(mean_NRMSE==min(mean_NRMSE));

figure(2) %plot the best simulated subject
subplot(231)
plot(simulation_time,1000*Infusion_inp,'LineWidth',2)
hold on
plot(simulation_time,-1000*Hemorrhage_inp,'--r','LineWidth',2)
set(gca,'XTick',0:30:180)
xlim([0 180])
ylabel('Fluid & Hemorrhage [ml/min]')
set(gca,'XTick',0:30:180)
legend('Fluid','Hemorrhage','Location','SouthEast')
grid on
box on

subplot(232)
plot(Hemo_Time,Hemo_HCT,'or','LineWidth',2)
hold on
plot(Hemo_Time,response_HCT(min_ind(1),:),'LineWidth',2)
ylabel('Hematocrit [%]')
xlim([0 180])
xticks([0 30 60 90 120 150 180])
grid on
box on

subplot(233)
plot(Hemo_Time,Hemo_HR,'or','LineWidth',2)
hold on
plot(Hemo_Time,response_HR(min_ind,:), 'LineWidth',2)
ylabel('HR [bpm]')
xlim([0 180])
xticks([0 30 60 90 120 150 180])
grid on
box on

subplot(234)
plot(Hemo_Time,((Hemo_CO)./Hemo_HR),'or','LineWidth',2)
hold on
plot(Hemo_Time,response_SV(min_ind,:), 'LineWidth',2)
ylabel('SV [l]')
xlim([0 180])
xticks([0 30 60 90 120 150 180])
xlabel('Time [min]')
grid on
box on

subplot(235)
plot(Hemo_Time,Hemo_CO,'or','LineWidth',2)
hold on
plot(Hemo_Time,response_CO(min_ind,:), 'LineWidth',2)
ylabel('CO [lpm]')
xlim([0 180])
xticks([0 30 60 90 120 150 180])

```

```

xlabel('Time [min]')
grid on
box on

subplot(236)
plot(Hemo_Time,Hemo_MAP,'or','LineWidth',2)
hold on
plot(Hemo_Time,response_BP(min_ind,:), 'LineWidth',2)
ylabel('BP [mmHg]')
xlim([0 180])
xticks([0 30 60 90 120 150 180])
xlabel('Time [min]')
grid on
box on

%%
for kk = 1:numsim %identify physiological simulations
    if min(response_HCT(kk,:)) >0 && max(response_HCT(kk,:))<50 && ...
        min(response_SV(kk,:))>0 && max(response_SV(kk,:))<0.1 && ...
        min(response_HR(kk,:))>0 && max(response_HR(kk,:))<300 && ...
        min(response_BP(kk,:))>0 && max(response_BP(kk,:))<150
        physiological_sims(kk) = 1;
    else
        physiological_sims(kk) = 0;
        max_NRMSE(kk,1) = 1000;
        max_NMAE(kk,1) = 1000;
    end
end

%identify relevant simulation (NRMSE<25%)
Relevant_sim = find(max_NRMSE<0.25);

figure(3) % plot prediction envelope made by relevant subjects
subplot(231)
plot(simulation_time,1000*Infusion_inp,'LineWidth',2)
hold on
plot(simulation_time,-1000*Hemorrhage_inp,'--r','LineWidth',2)
set(gca,'XTick',0:30:180)
xlim([0 180])
ylim([-100 80])
ylabel('Fluid & Hemorrhage [ml/min]')
set(gca,'XTick',0:30:180)
set(gca,'YTick',-100:20:80)
legend('Fluid','Hemorrhage','Location','SouthEast')
grid on
box on

subplot(232)
x = 1:1:length(Hemo_Time);
curve1_HCT = min(response_HCT(Relevant_sim,x));
curve2_HCT = max(response_HCT(Relevant_sim,x));
plot(Hemo_Time, curve1_HCT, 'b', 'LineWidth', 2);
hold on;
plot(Hemo_Time, curve2_HCT, 'b', 'LineWidth', 2);
x2 = [Hemo_Time', fliplr(Hemo_Time')];

```

```

inBetween = [curve1_HCT, flipr(curve2_HCT)];
fill(x2, inBetween, 'g');
hold on
plot(Hemo_Time, Hemo_HCT, 'or', 'LineWidth', 2)
inside_interval_HCT = length(find(Hemo_HCT >= curve1_HCT' & Hemo_HCT <= curve2_HCT'))/length(Hemo_HCT);
ylabel('Hematocrit [%]')
xlim([0 180])
xticks([0 30 60 90 120 150 180])
grid on
box on

```

```

subplot(233)
curve1_HR = min(response_HR(Relevant_sim, x));
curve2_HR = max(response_HR(Relevant_sim, x));
plot(Hemo_Time, curve1_HR, 'b', 'LineWidth', 2);
hold on;
plot(Hemo_Time, curve2_HR, 'b', 'LineWidth', 2);
inBetween = [curve1_HR, flipr(curve2_HR)];
fill(x2, inBetween, 'g');
hold on
plot(Hemo_Time, Hemo_HR, 'or', 'LineWidth', 2)
inside_interval_HR = length(find(Hemo_HR >= curve1_HR' & Hemo_HR <= curve2_HR'))/length(Hemo_HR);
ylabel('HR [bpm]')
xlim([0 180])
xticks([0 30 60 90 120 150 180])
grid on
box on

```

```

subplot(234)
curve1_SV = min(response_SV(Relevant_sim, x));
curve2_SV = max(response_SV(Relevant_sim, x));
plot(Hemo_Time, curve1_SV, 'b', 'LineWidth', 2);
hold on;
plot(Hemo_Time, curve2_SV, 'b', 'LineWidth', 2);
inBetween = [curve1_SV, flipr(curve2_SV)];
fill(x2, inBetween, 'g');
hold on
plot(Hemo_Time, ((Hemo_CO)./Hemo_HR), 'or', 'LineWidth', 2)
inside_interval_SV = length(find(Hemo_SV >= curve1_SV' & Hemo_SV <= curve2_SV'))/length(Hemo_SV);
ylabel('SV [l]')
xlim([0 180])
xticks([0 30 60 90 120 150 180])
xlabel('Time [min]')
grid on
box on

```

```

subplot(235)
curve1_CO = min(response_CO(Relevant_sim, x));
curve2_CO = max(response_CO(Relevant_sim, x));
plot(Hemo_Time, curve1_CO, 'b', 'LineWidth', 2);
hold on;
plot(Hemo_Time, curve2_CO, 'b', 'LineWidth', 2);
inBetween = [curve1_CO, flipr(curve2_CO)];
fill(x2, inBetween, 'g');
hold on

```

```

plot(Hemo_Time,Hemo_CO,'or','LineWidth',2)
inside_interval_CO = length(find(Hemo_CO>=curve1_CO' & Hemo_CO<=curve2_CO'))/length(Hemo_CO);
ylabel('CO [lpm]')
xlim([0 180])
xticks([0 30 60 90 120 150 180])
xlabel('Time [min]')
grid on
box on

subplot(236)
curve1_BP = min(response_BP(Relevant_sim,x));
curve2_BP = max(response_BP(Relevant_sim,x));
plot(Hemo_Time, curve1_BP, 'b', 'LineWidth', 2);
hold on;
plot(Hemo_Time, curve2_BP, 'b', 'LineWidth', 2);
inBetween = [curve1_BP, flipr(curve2_BP)];
fill(x2, inBetween, 'g');
hold on
plot(Hemo_Time,Hemo_MAP,'or','LineWidth',2)
inside_interval_BP = length(find(Hemo_MAP>=curve1_BP' & Hemo_MAP<=curve2_BP'))/length(Hemo_MAP);
ylabel('BP [mmHg]')
xlim([0 180])
xticks([0 30 60 90 120 150 180])
xlabel('Time [min]')
grid on
box on

%%
% min NRMSE and min NAME
min_max_NRMSE = min(max_NRMSE);
min_mean_NMAE = min(mean_NMAE);

%statistics of simulated subjects
physiological_sims_size = length(find(physiological_sims==1));
relevant_sims_size = length(Relevant_sim);
Average_percent_in_interval =
(inside_interval_HCT+inside_interval_HR+inside_interval_SV+inside_interval_CO+inside_interval_BP)/5;
%% compute normalized interval score for prediction envelopes
alpha = 0.05;
interval_score_HCT = [];
jj = 1;
for kk =1:length(Hemo_HCT)
    if Hemo_HCT(kk)<curve1_HCT(kk)
        interval_score_HCT(jj,1) = (2/alpha)*(curve1_HCT(kk)-Hemo_HCT(kk)) + curve2_HCT(kk)-curve1_HCT(kk);
    elseif Hemo_HCT(kk)>curve2_HCT(kk)
        interval_score_HCT(jj,1) = (2/alpha)*(Hemo_HCT(kk)-curve2_HCT(kk)) + curve2_HCT(kk)-curve1_HCT(kk);
    elseif Hemo_HCT(kk)>=curve1_HCT(kk) && Hemo_HCT(kk)<=curve2_HCT(kk)
        interval_score_HCT(jj,1) = curve2_HCT(kk)-curve1_HCT(kk);
    end
    jj = jj+1;
end
Normal_interval_score_HCT = (interval_score_HCT./Hemo_HCT)';

%HR
interval_score_HR = [];

```

```

jj = 1;
for kk =1:length(Hemo_HR)
    if Hemo_HR(kk)<curve1_HR(kk)
        interval_score_HR(jj,1) = (2/alpha)*(curve1_HR(kk)-Hemo_HR(kk)) + curve2_HR(kk)-curve1_HR(kk);
    elseif Hemo_HR(kk)>curve2_HR(kk)
        interval_score_HR(jj,1) = (2/alpha)*(Hemo_HR(kk)-curve2_HR(kk)) + curve2_HR(kk)-curve1_HR(kk);
    elseif Hemo_HR(kk)>=curve1_HR(kk) && Hemo_HR(kk)<=curve2_HR(kk)
        interval_score_HR(jj,1) = curve2_HR(kk)-curve1_HR(kk);
    end
    jj = jj+1;
end
Normal_interval_score_HR = (interval_score_HR./Hemo_HR)';

%SV
interval_score_SV = [];
jj = 1;
for kk =1:length(Hemo_SV)
    if Hemo_SV(kk)<curve1_SV(kk)
        interval_score_SV(jj,1) = (2/alpha)*(curve1_SV(kk)-Hemo_SV(kk)) + curve2_SV(kk)-curve1_SV(kk);
    elseif Hemo_SV(kk)>curve2_SV(kk)
        interval_score_SV(jj,1) = (2/alpha)*(Hemo_SV(kk)-curve2_SV(kk)) + curve2_SV(kk)-curve1_SV(kk);
    elseif Hemo_SV(kk)>=curve1_SV(kk) && Hemo_SV(kk)<=curve2_SV(kk)
        interval_score_SV(jj,1) = curve2_SV(kk)-curve1_SV(kk);
    end
    jj = jj+1;
end
Normal_interval_score_SV = (interval_score_SV./Hemo_SV)';

%CO
interval_score_CO = [];
jj = 1;
for kk =1:length(Hemo_CO)
    if Hemo_CO(kk)<curve1_CO(kk)
        interval_score_CO(jj,1) = (2/alpha)*(curve1_CO(kk)-Hemo_CO(kk)) + curve2_CO(kk)-curve1_CO(kk);
    elseif Hemo_CO(kk)>curve2_CO(kk)
        interval_score_CO(jj,1) = (2/alpha)*(Hemo_CO(kk)-curve2_CO(kk)) + curve2_CO(kk)-curve1_CO(kk);
    elseif Hemo_CO(kk)>=curve1_CO(kk) && Hemo_CO(kk)<=curve2_CO(kk)
        interval_score_CO(jj,1) = curve2_CO(kk)-curve1_CO(kk);
    end
    jj = jj+1;
end
Normal_interval_score_CO = (interval_score_CO./Hemo_CO)';

%BP
interval_score_BP = [];
jj = 1;
for kk =1:length(Hemo_MAP)
    if Hemo_MAP(kk)<curve1_BP(kk)
        interval_score_BP(jj,1) = (2/alpha)*(curve1_BP(kk)-Hemo_MAP(kk)) + curve2_BP(kk)-curve1_BP(kk);
    elseif Hemo_MAP(kk)>curve2_BP(kk)
        interval_score_BP(jj,1) = (2/alpha)*(Hemo_MAP(kk)-curve2_BP(kk)) + curve2_BP(kk)-curve1_BP(kk);
    elseif Hemo_MAP(kk)>=curve1_BP(kk) && Hemo_MAP(kk)<=curve2_BP(kk)
        interval_score_BP(jj,1) = curve2_BP(kk)-curve1_BP(kk);
    end
    jj = jj+1;
end

```

```

end
Normal_interval_score_BP = (interval_score_BP./Hemo_MAP)';

%normalized interval score for all physiological variables
Normal_interval_score =
[Normal_interval_score_HCT;Normal_interval_score_HR;Normal_interval_score_SV;Normal_interval_score_CO;Normal_interval
_score_BP]';
mean_Normal_interval_score = mean(Normal_interval_score);

```

A3: Example Prediction Envelope Results for 10000 Simulation Sample Size:

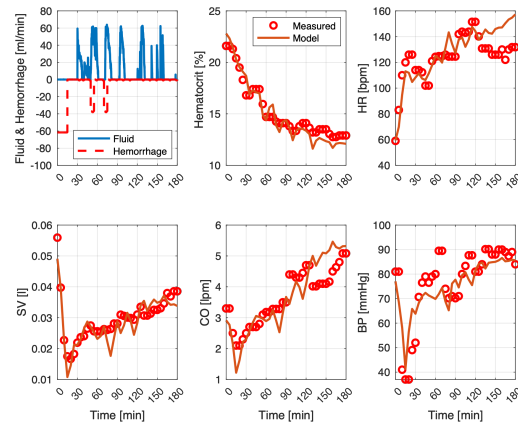


Figure 6: An example best simulated subject with minimum averaged NRMSE across all physiological variables

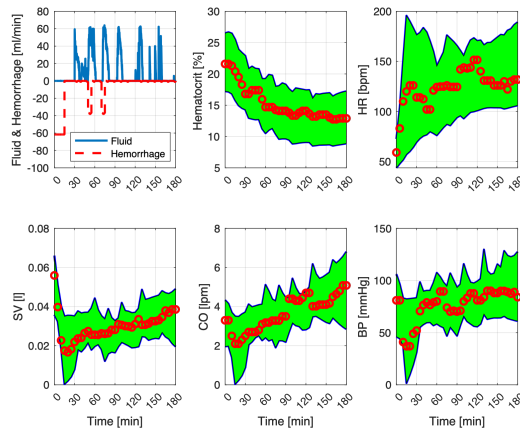


Figure 7: An example prediction envelope generated by relevant physiological simulations