

Alzheimer's Disease: A Mathematical Model for Onset and Progression

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Original Authors: Bertsch, Franchi, Marcello, Tesi and Tosin 2016 [1]

Advanced Topics in Biomathematics

June 5th, 2025





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Introduction



- Alzheimer's Disease is one of the most common late life dementia
- Causes: still not totally clear, but experimental evidence suggest it is linked to the diffusion of "amyloid- β " peptide (amyloid cascade hypothesis) and the tau protein
- We will focus on $A\beta_{42}$ isomer



- Monomeric $A\beta$ peptides are naturally produced and removed by neurons
- For unknown reasons some neurons (damaged neurons) do not remove all this toxic protein
- Monomeric A β diffuses through the brain and agglomerates to form long, insoluble fibrils (senile plaques)
- Neural damage spreads in a neuron-to-neuron prion-like propagation (prionid hypothesis)



Mathematical Model



- Ω : portion of the cerebral tissue, with $x \in \Omega$ generic (space) point
- Time-scales:
 - Fast *s*-scale (hours): diffusion of $A\beta$
 - Slow *t*-scale (months): progression of disease

$$\Delta t = \varepsilon \Delta s$$
, $\varepsilon \ll 1$

- Variables:
 - $u_m(x, s)$: molar concentration of soluble A β polymers of length m at time s for m = 1, ..., N-1
 - $u_N(x,s)$: cluster of polymers of length $\geq N$, assumed to not move



Model for *m*-polymers, for m = 1, ..., N - 1:

$$\partial_{s} u_{m} = d_{m} \Delta u_{m} + \left[\frac{1}{2} \sum_{j=1}^{m-1} a_{j,m-j} u_{j} u_{m-j} - u_{m} \sum_{j=1}^{N} a_{m,j} u_{j} \right] - \sigma_{m} u_{m}$$

From experimental evidence and simplifications:

$$a_{i,j} = \alpha \frac{1}{ij}, \qquad \alpha > 0, \qquad a_{N,N} = 0$$



For the monomers u_1 we add a source term \mathcal{F} :

$$\partial_s u_1 = d_1 \Delta u_1 - u_1 \sum_{j=1}^N a_{1,j} u_j + \mathcal{F}$$

Large fibrils do not move (no diffusion):

$$\partial_s u_N = \frac{1}{2} \sum_{\substack{j+k \ge N \\ k,j < N}} a_{j,k} u_j u_k$$



Degree of neuron malfunctioning: $a \in [0, 1]$:

- \bullet $a \simeq 0$: healthy neuron
- $a \simeq 1$: dead neuron

Fraction of neurons close to x with degree of malfunctioning at time t (slow-scale) between a and a+da is:



Introduce the deterioration rate $\nu = \nu(x, a, t)$ as

$$\nu[f] = \int \int_{\Omega \times [0,1]} \mathcal{K}(x,a,y,b) f(y,b,t) dy db$$
$$+ \mathcal{S}(x,a,u_1(x,s),\ldots,u_{N-1}(x,s))$$

We can write an equation for f:

$$\partial_t f + \partial_a (f \nu[f]) = J[f]$$

The source term can be modeled in terms of f:

$$\mathcal{F} = \mathcal{F}[f] = \mathcal{C}_{\mathcal{F}} \int_0^1 (\mu_0 + a)(1-a)f(x,a,t)da$$



Typical assumption:

$$\mathcal{K}(x, a, y, b) = \mathcal{G}(x, a, b)H(x, y)$$

$$\mathcal{G}(x, a, b) = C_{\mathcal{G}}(b - a)^{+}, \qquad H(x, y) = h(|x - y|)$$

Assume that $\int_{|y|< r_0} h(|y|) dy = 1$. When $r_0 \to 0$

$$\nu[f] = \int_0^1 \mathcal{G}(x, a, b) f(x, b, t) db + \mathcal{S}(x, a, u_1, \dots, u_{N-1})$$

Final assumption:

$$\mathcal{S} = \mathcal{C}_{\mathcal{S}}(1-a) \left(\sum_{m=1}^{N-1} m u_m(x,s) - \bar{U} \right)^+$$



Final Model

$$\begin{cases} \partial_t f + \partial_a (f\nu[f]) = J[f] \\ \varepsilon \partial_t u_1 = d_1 \Delta u_1 - u_1 \sum_{j=1}^N a_{1,j} u_j + \mathcal{F}[f] - \sigma_1 u_1 \\ \varepsilon \partial_t u_m = d_m \Delta u_m + \frac{1}{2} \sum_{j=1}^{m-1} a_{j,m-j} u_j u_{m-j} \\ -u_m \sum_{j=1}^N a_{m,j} u_j - \sigma_m u_m \end{cases} \quad 2 \le m < N \\ \varepsilon \partial_t u_N = \frac{1}{2} \sum_{\substack{j+k \ge N \\ k,j < N}} a_{j,k} u_j u_k \end{cases}$$



Problem Setting and Discretization



Two-dimensional tranverse section of the brain

$$\Omega = [0, L_x] \times [0, L_y]$$

- Two inner holes for the cerebral ventricles
- Two small circles for the hippocampus

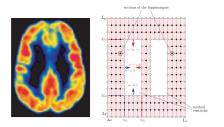


Figure: Real transverse section and numerical schematization of the brain.



 Outer Boundary: vanishing polymer flow, i.e., homogeneous Neumann condition

$$-rac{d_m}{arepsilon}
abla u_m\cdot\mathbf{n}=0 \qquad ext{on }\partial\Omega_{ ext{out}} \quad m=1,\ldots,N-1$$

■ Inner Boundary (ventricles): removal by the cerebrospinal fluid (CSF), i.e., Robin boundary condition

$$-\frac{d_m}{\varepsilon}\nabla u_m\cdot\mathbf{n}=\beta u_m\qquad\text{in }\partial\Omega_{\text{out}}\quad m=1,\ldots,N-1$$

Physiological Indicators



■ Macroscopic distribution of Neuron Malfunctioning:

$$A(x,t) = \int_0^1 af(x,a,t)da$$

Local brain atrophy:

$$\Phi(x,t) = \max\left\{0, \frac{A(x,t) - A_0}{1 - A_0}\right\}$$

■ Global Brain Atrophy:

$$\Phi(t) = \frac{1}{|\Omega|} \int_{\Omega} \Phi(x, t) dx$$

 Total Concentration of Soluble Amyloid in the Brain Occipital Region

$$U_{\mathcal{S}}(t) = \frac{1}{|\hat{\Omega}|} \int_{\hat{\Omega}} \sum_{m=1}^{N-1} m u_m(x, t) dx$$

Average quantity of AB deposits:

$$U_N(t) = \frac{1}{|\Omega|} \int_{\Omega} Nu_N(x, t) dx$$



Numerical Results and Simulations



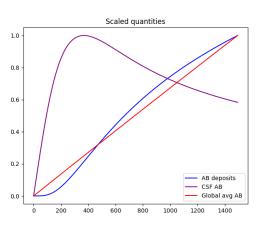


Figure: Plot of the (normalized) CSF A β , the A β deposits and the global average quantity with $\beta=100$ and N=5 isomers



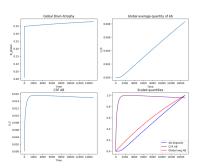


Figure: Simulation with $\beta=100$ and N=10 isomers

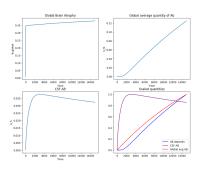


Figure: Simulation with $\beta = 0.0001$ and N = 10 isomers

Simulation of Neuron Malfunctioning



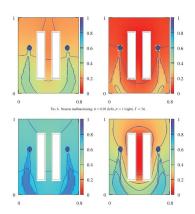


Figure: Plot of f from the paper.



Figure: Plot of f from our simulation at t = 1000



Figure: Plot of f from our simulation at t = 15000



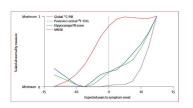


Figure: Clinical data

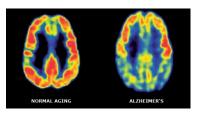


Figure: Comparison of PET images of an healthy and an ill brain



Conclusions



Pros:

- High level of flexibility
- Simulations comparable with clinical data
- Potentially useful to study new drugs

Cons:

- Preferential diffusion of the disease in the occipital region not captured
- Parameter estimation
- Removal process not well captured





Michiel Bertsch, Bruno Franchi, Norina Marcello, Maria Carla Tesi, and Andrea Tosin.

Alzheimer's disease: a mathematical model for onset and progression.

Mathematical Medicine and Biology A Journal of the IMA, 4 2016.



Thank you for the attention!



Figure: QR code to the GitHub repository with the presentation, the paper and the notebooks