



# Functional Magnetic Resonance Imaging

GitHub <a href="https://github.com/dcdace/fMRI">https://github.com/dcdace/fMRI</a> training

Dace [datza] Apšvalka February 2025

#### Outline

- Introduction
- Experimental design
- Data management
- Pre-processing
- Statistical analysis
- Practical demo





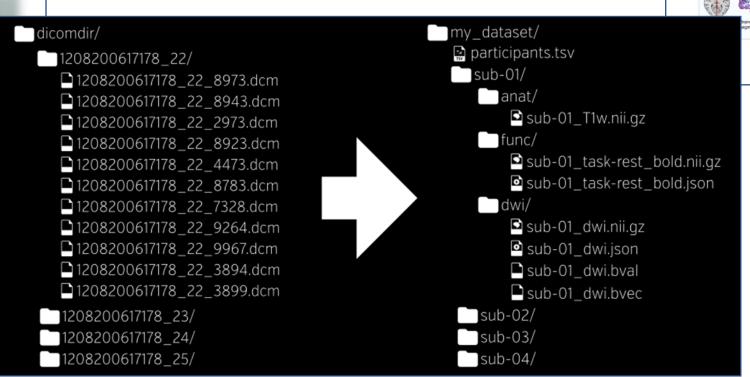
Pre-process

#### Collect the data

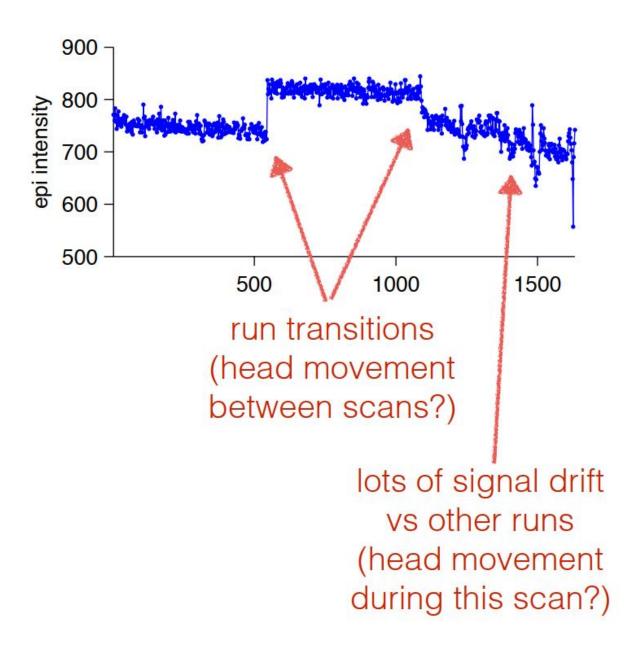


#### Why can't we analyse right away?

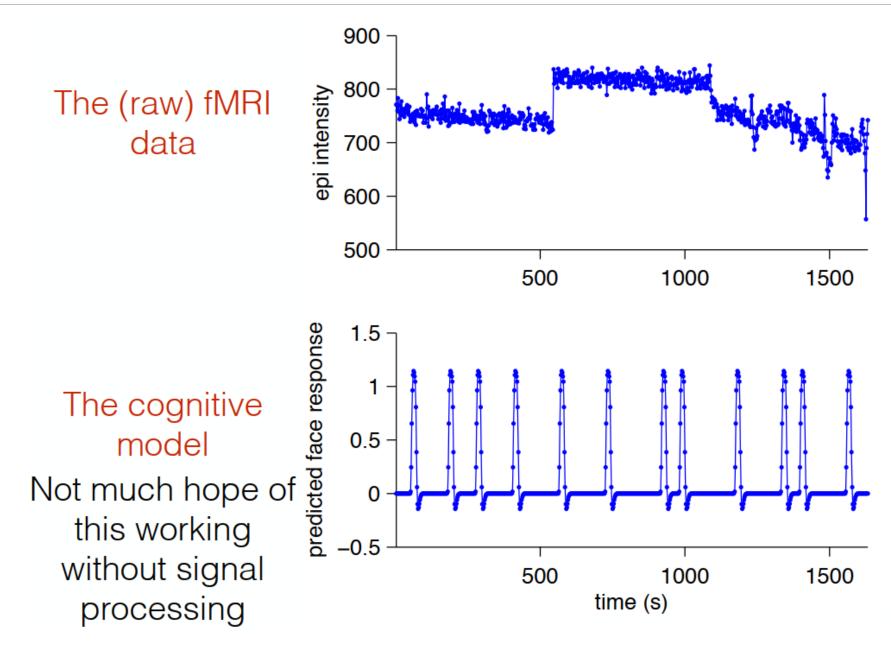
Pre-process & Analyse

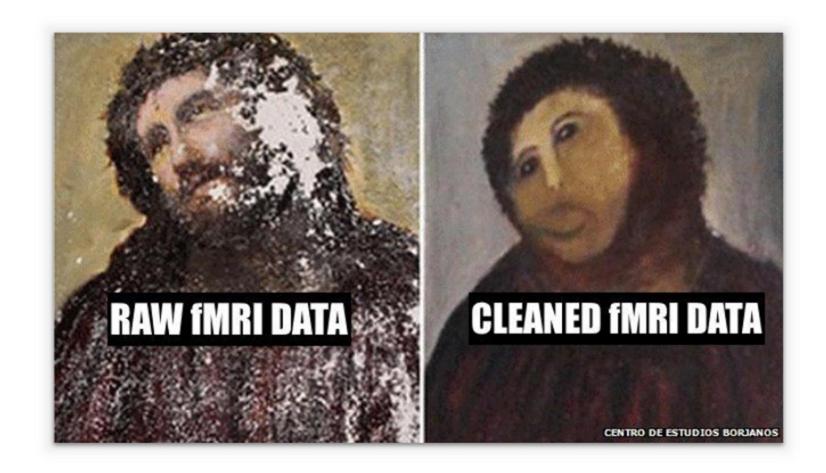


## Raw data in example voxel



## Raw data in example voxel





#### Problems with fMRI data

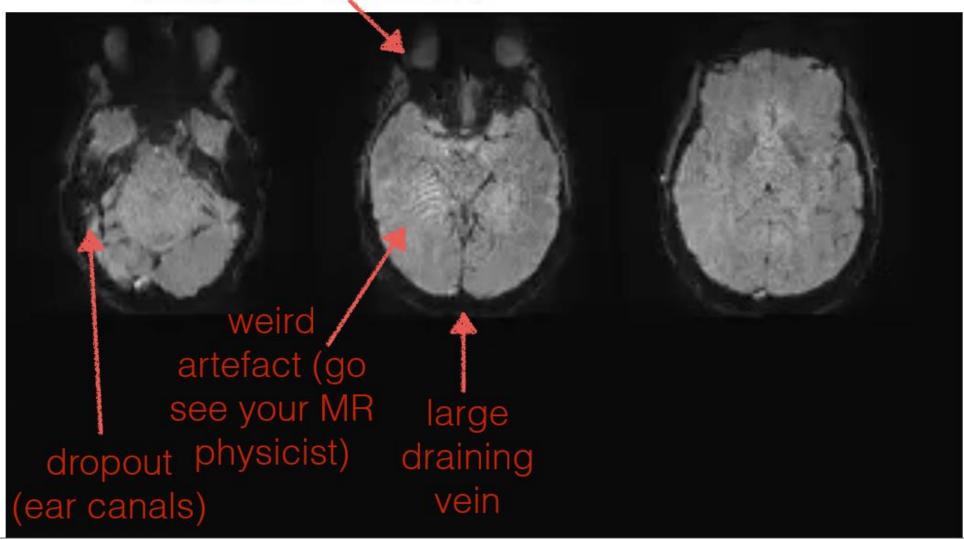
- Artefacts
- Head motion
- Slice timing
- Brain differences
- Noise
- ... and many others

#### Problems with fMRI data

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#### Artefacts

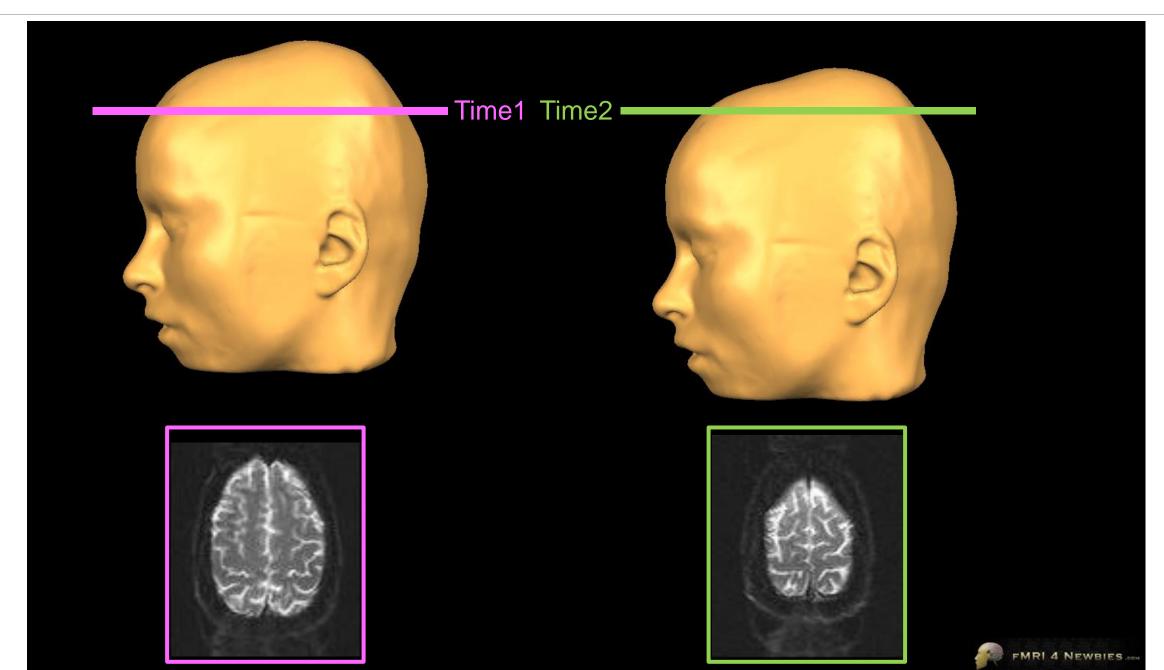
eye blink / movement effect (not just in eye balls!)



#### Problems with fMRI data

- Artefacts
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- ... and many others

# Head motion



#### Head motion correction

- Prevention is the best remedy
- Tell your subjects how to be good subjects
- Make sure the subject is comfortable going in
- Discourage any movements that would displace the head between scans



Bite bar



Thermoplastic mask

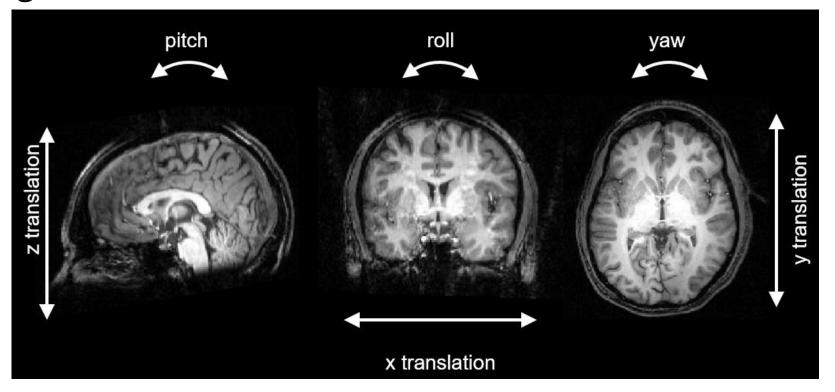


Vacuum pack

Often a bunch of foam padding works as well as anything

#### Head motion correction

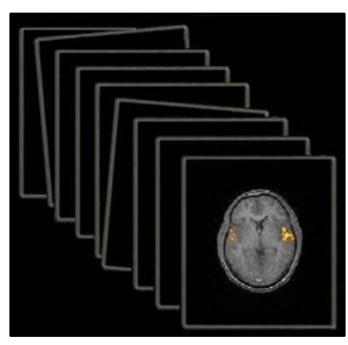
Spatial realignment



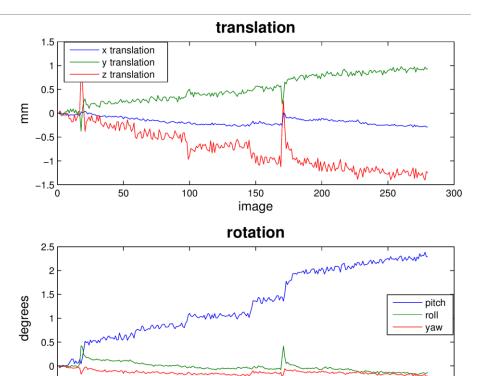
- Most algorithms assume a rigid body (= the brain doesn't deform with movement)
- Align each volume of the brain to a target volume using 6 parameters: 3 translations and 3 rotations
- Target volume: e.g., the mean image of the first run

#### Head motion correction

- Spatial realignment
  - Not expected to work perfectly, but it helps
  - Be suspicious of data with a lot of head movement!



Translation (mm)			Rotation (rad)		
Χ	У	Z	Pitch	Roll	Yaw
0.3417	0.3348	1.8892	0.0182	0.0065	0.001
0.2733	0.418	1.5832	0.0165	0.0063	0.0061
0.8953	0.4925	0.8524	0.0234	0.0123	0.0269
1.8179	1.5353	1.8285	0.0327	0.0222	0.0939
1.0054	0.3014	0.7574	0.0043	0.0197	0.0094
0.737	0.9508	1.0428	0.026	0.0171	0.0164



150

image

200

250

300

50

100

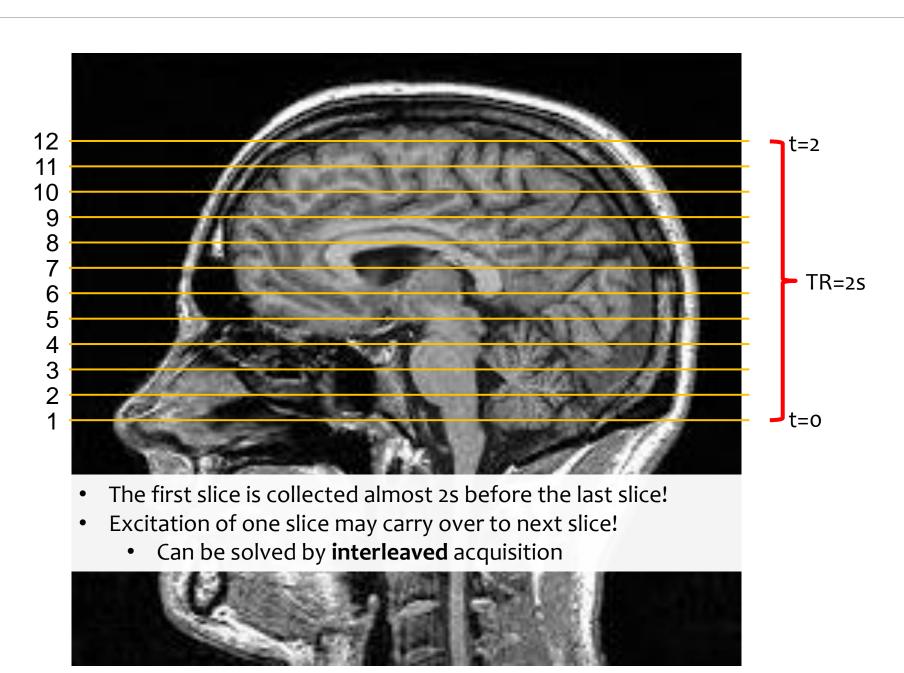
#### Problems with fMRI data

- Artefacts
- Head motion
- Slice timing
- Brain differences
- Noise
- ... and many others

## Slice timing

Typically, the fMRI data are acquired slice-by-slice – not the whole brain all at once

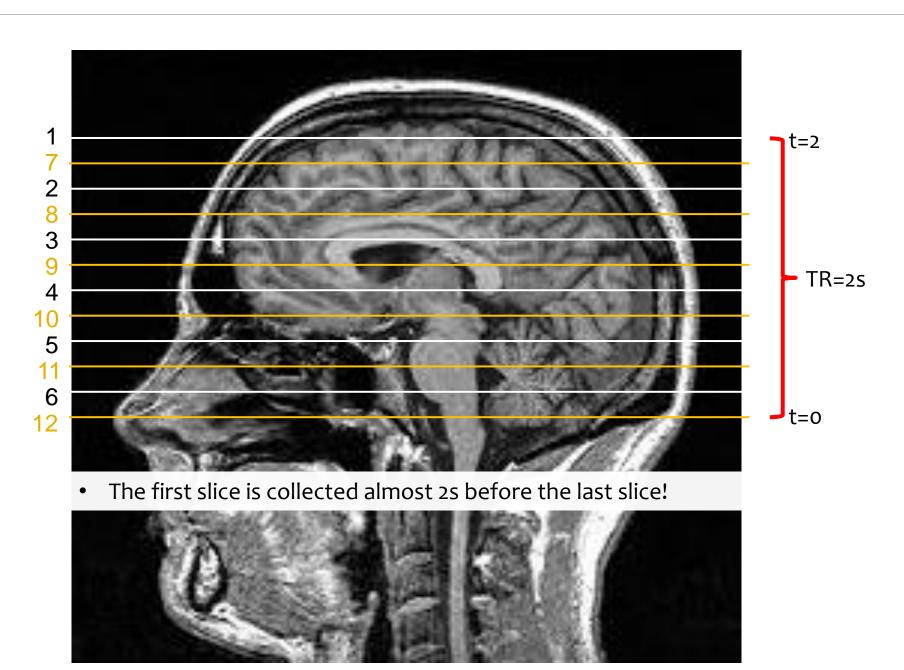
Order: **Ascending** 



# Slice timing

Typically, the fMRI data are acquired slice-by-slice – not the whole brain all at once

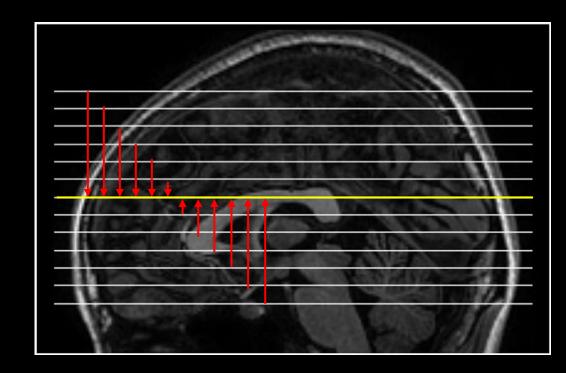
**Descending-Interleaved** 

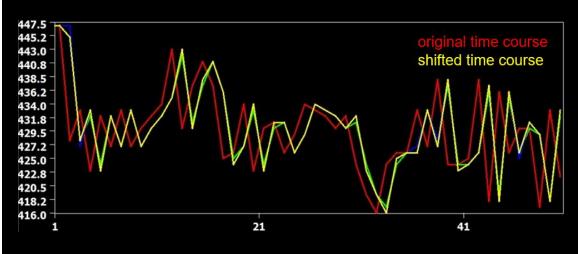


#### Slice time correction

#### Temporal interpolation

- Adjusts the timings of the slices so that it is as if they had been collected simultaneously
- Uses information from nearby time points to estimate the amplitude of the MR signal at the onset of each TR
- Key parameters
  - Reference slice
    - The only slice that is not interpolated
    - Typical choice is to use the middle slice
  - Slice order
  - TR
- No need to slice time correct if TR is very short (e.g., multi-band: multiple slices at the same time)







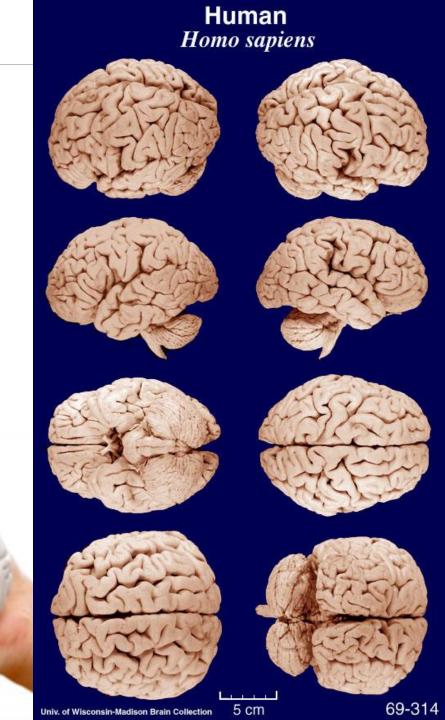
#### Problems with fMRI data

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- Noise
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# Brain differences – between subjects

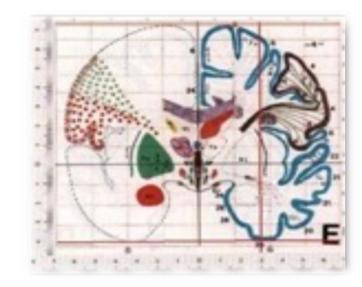
- Brain size can differ (up to 30%)
- Brain shape can differ

- Solution: normalise to a standard template
  - stretching, squeezing and warping each brain to the "standard brain"

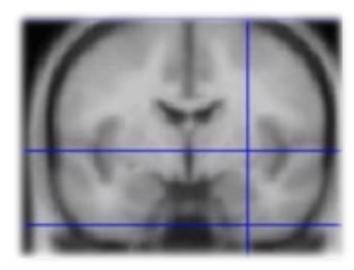


#### Standard brain template

- Talairach space
  - From atlas of Talairach and Tournoux (1988)
  - Based on single subject (60y, Female, Cadaver)



- MNI Montreal Neurological Institute
  - Average scan of 152 'normal' right-handed subjects
  - Approximated to Talairach space
  - Slightly larger



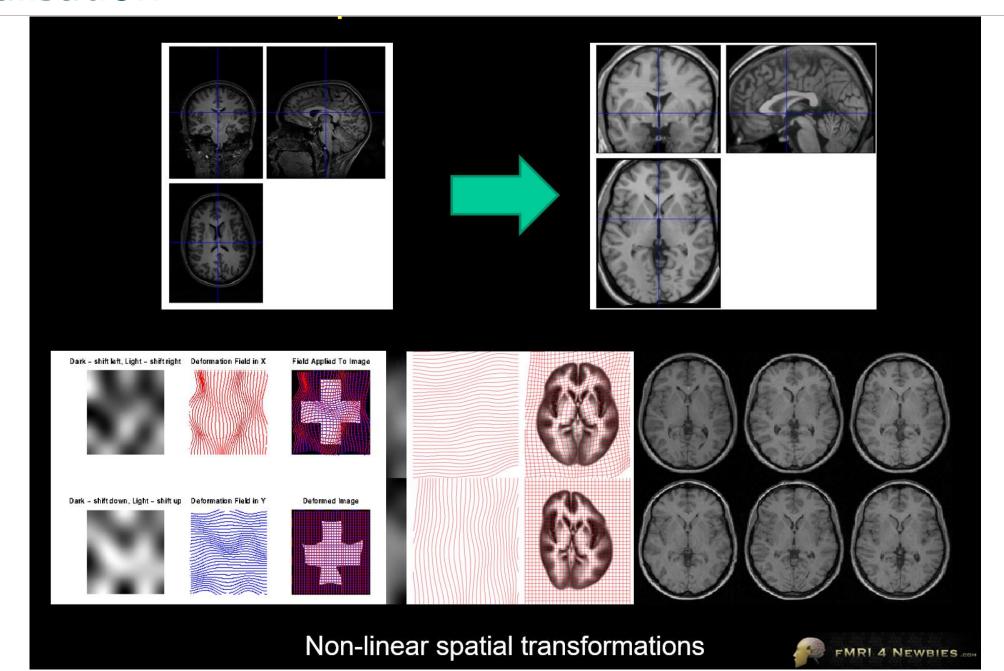


About the MNI space(s)

https://www.lead-dbs.org/about-the-mni-spaces/

- MNI305: 305 normal MRI brains were linearly coregistered (9-param) to 241 brains that had been coregistered (roughly) to the Talairach atlas. This was the first MNI template. It is T1 only.
- Colin27 original: Colin Holmes, a lab member of the MNI, was scanned 27 times. This was used as the standard template in SPM96. This template was matched to the MNI305. In the original release, only a T1 template was available.
- MNI152 linear: 152 normal images were linearly coregistered (9-param) to the 305 space. This was adopted to define standard anatomy by the International Consortium of Brain Mapping (ICBM) and is used by SPM from version 99 on. Only a T1 template is available.
  - SPM: Note that in later iterations, SPM defined its own "space" based on scans acquired within the IXI dataset, leveraging on the concept of segmentation-based normalizations (as applied in the Unified Segmentation, DARTEL and SHOOT approaches). This space, referred to as the IXI549Space is largely similar to MNI152 and of similar resolution (where it's likely safe to say that differences do not matter as much for most applications). Along the same lines, both spaces are unsuitable for use in DBS imaging, in our opinion. More info here.
- MNI152 NLIN 6th generation: Here, the 152 brains were nonlinearly registered into 305 space. Again, only a T1 template is available.
  - FSL: The FSLR is an adapted version of this space but in its asymmetric flavor (MNI152NLIN6Asym, hence different to the official one provided here). The template also provides surface coordinates references.
     More info here.
- Colin27 hires T1/T2 version (2008): The MNI also released a high-resolution version of the Colin27 space.
- MNI152 NLIN 2009: Finally, in 2009, the MNI released an updated version after again nonlinearly co-registering
  the 152 acquisitions. This template exhibits the best resolution and detail to date and is available in T1, T2, PD
  and T2-relaxometry versions. It has not (yet) been adopted by SPM or FSL though and it's anatomy is slightly
  different in direct comparison to the 6th generation templates. Moreover, it comes in three versions (two of
  which are explicitly mentioned here) that each have a symmetric and asymmetric subversion:
  - MNI152 NLIN 2009a: Probably the official new template in 1 × 1 × 1 mm resolution. It comes in T1, T2, PD and T2-relaxometry versions. There is a symmetric and an asymmetric version (latter not featureing T2-relaxometry).
  - MNI152 NLIN 2009b: The only of the novel templates available in 0.5 × 0.5 × 0.5 mm resolution. It is
    available in a T1, T2 and PD version. Due to the high resolution of this template, it has been adopted by
    Lead-DBS as the primary anatomy template. Lead-DBS uses the asymmetric version of this template.

#### Normalisation



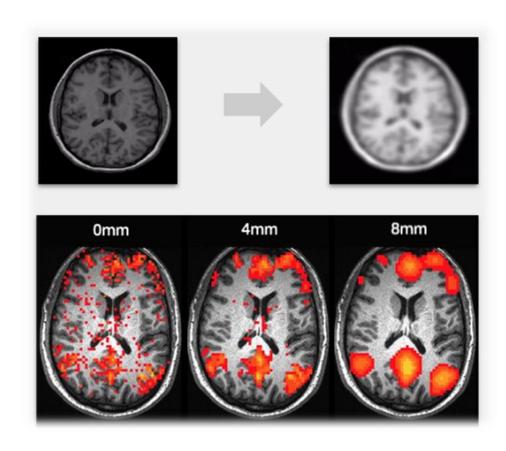
# Spatial smoothing

 Helps make residual errors in previous spatial pre-processing stages less problematic (e.g., imperfect normalisation, motion correction)

Can increase signal-to-noise ratio

 Necessary for validity of multiple corrections within random field theory

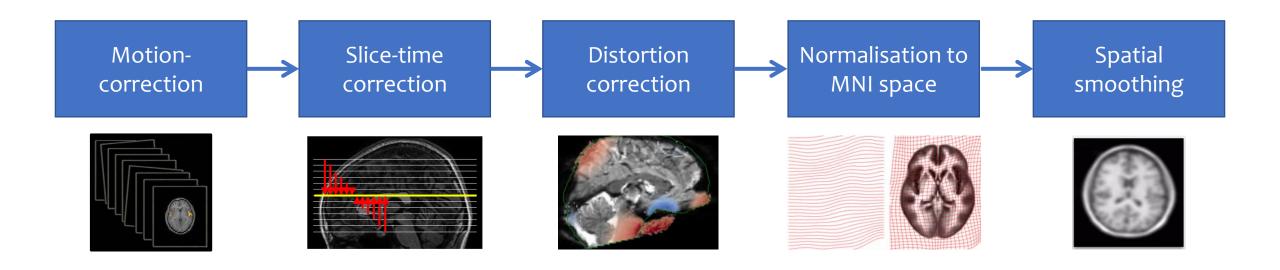
But it reduces the image resolution



#### Problems with fMRI data

- Artefacts
- Head motion
- Slice timing
- Brain differences
- Noise can be modelled in GLM
- ... and many others

# Typical pre-processing pipeline

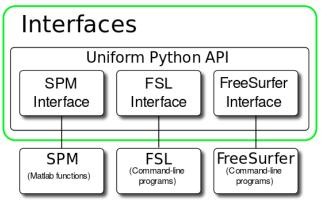


# Pre-processing tools

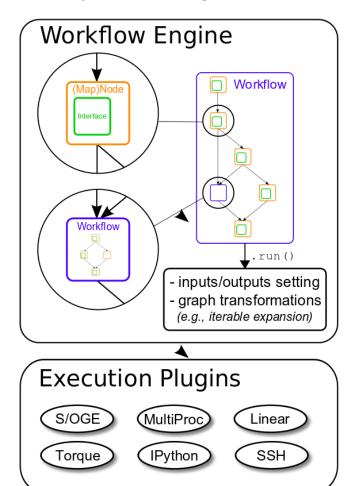


# Pre-processing tools





Idiosyncratic, Heterogeneous APIs



## Pre-processing tools

- fMRIPrep <a href="https://fmriprep.org/en/stable/">https://fmriprep.org/en/stable/</a>
  - Fully automated fMRI data pre-processing tool
  - The workflow is based on Nipype and encompasses a large set of tools from well-known neuroimaging packages, including FSL, ANTs, FreeSurfer, AFNI, and Nilearn. This pipeline was designed to provide the best software implementation for each state of pre-processing, and will be updated as newer and better neuroimaging software becomes available.
  - **Robustness** The pipeline adapts the pre-processing steps depending on the input dataset and should provide results as good as possible independently of scanner make, scanning parameters or presence of additional correction scans (such as fieldmaps).
  - **Ease of use** Thanks to dependence on the BIDS standard, manual parameter input is reduced to a minimum, allowing the pipeline to run in an automatic fashion.
  - "Glass box" philosophy Automation should not mean that one should not visually inspect the results or understand the methods. Thus, fMRIPrep provides visual reports for each subject, detailing the accuracy of the most important processing steps. This, combined with the documentation, can help researchers to understand the process and decide which subjects should be kept for the group level analysis.

#### **fMRIPrep**



T1-weighted

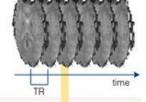
One or more (e.g. in longitudinal studies) T1w images





**BOLD** run

One run of one task (or resting-state) time-series of blood-oxygen level (BOLD) measurements





**Fuse & Conform** 

All T1w images are aligned and averaged to form a 3D reference image NIfTI headers are checked for validity



#### **INU Correction**

The T1w reference is run through the N4 algorithm to correct for intensity nonuniformity (INU)



Skull-stripping

Atlas-based brain extraction is performed on the reference T1w image



Functional preprocessing

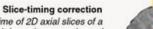
#### Generate reference & brain mask

Time-points showing non-steady state artifacts (excess of T1 contrast) are aligned and averaged to generate a reference image in native space



#### Estimation of head-motion

Parameters representing bulk head motion (due to involuntary drift, swallowing, etc.) of each timepoint with respect to the reference are estimated



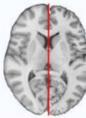
(Optional) When the acquisition time of 2D axial slices of a given timepoint is available, temporal dynamics are estimated and all slices resampled to the mid-timepoint of that TR





Brain atlas

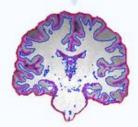
Default: MNI152 nonlinear asymmetric v2009c



Spatial normalization Non-linear, spatial

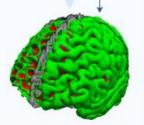


alignment to the brain



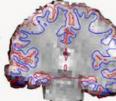
Brain tissue segmentation The brain-extracted image is

classified into CSF, GM and WM



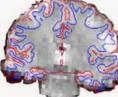
Surface reconstruction

Surfaces of the cortical sheet are reconstructed from the anatomical information (T1w reference, T2w)



#### Alignment to T1w reference

Registers activity in BOLD voxels to anatomical location



#### Susceptibility distortion estimation

(Optional) Find a deformation field that compensates for the distortion, when adequate acquisitions are present



#### Sample on surface

Sample the BOLD signal on the surfaces reconstructed from the anatomical data



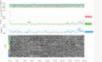
concatenating all pertinent transformations



#### Sample in native

"One-shot" resampling of the BOLD signal in its original grid, applying corrections





Calculate and store nuisance regressors such as noise components, motion parameters, global signals, etc.





# **Data**Organise & Manage



Notebook: nbo3\_Quality-Control-and-Preprocessing.ipynb

Pre-process

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