

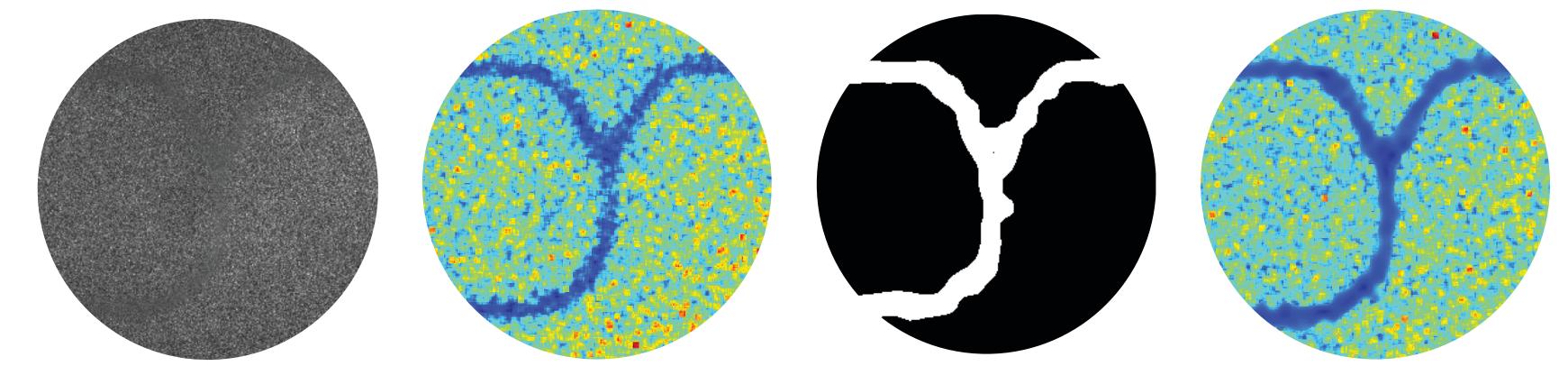
# Blood Vessel Visualization of Raw Speckle Images

## Wavelet Approach

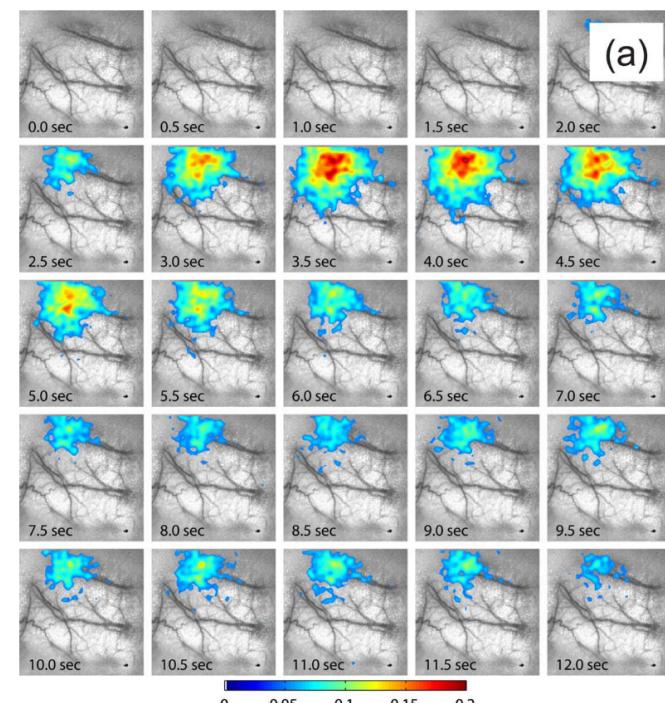
Francisco López-Tiro

# Introduction

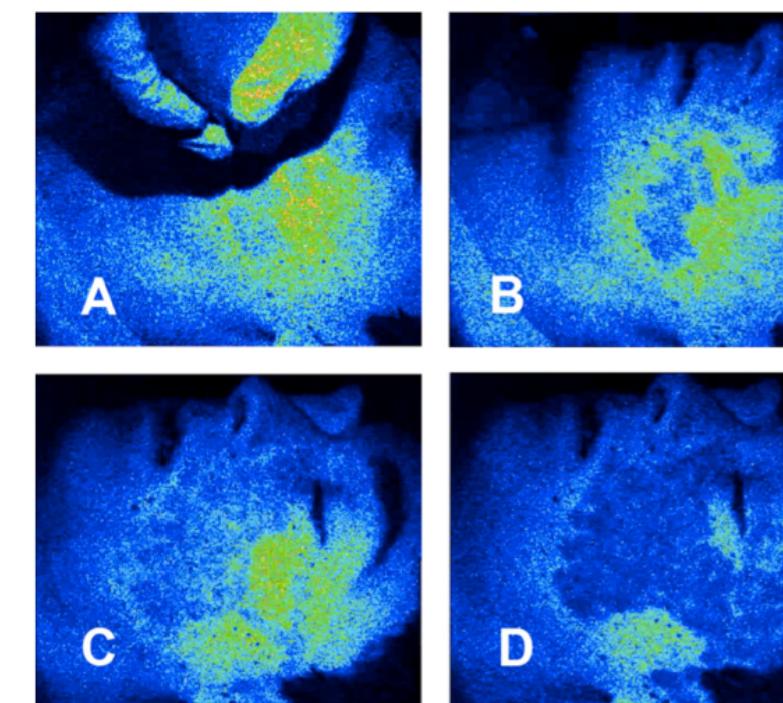
## Visualization and localization



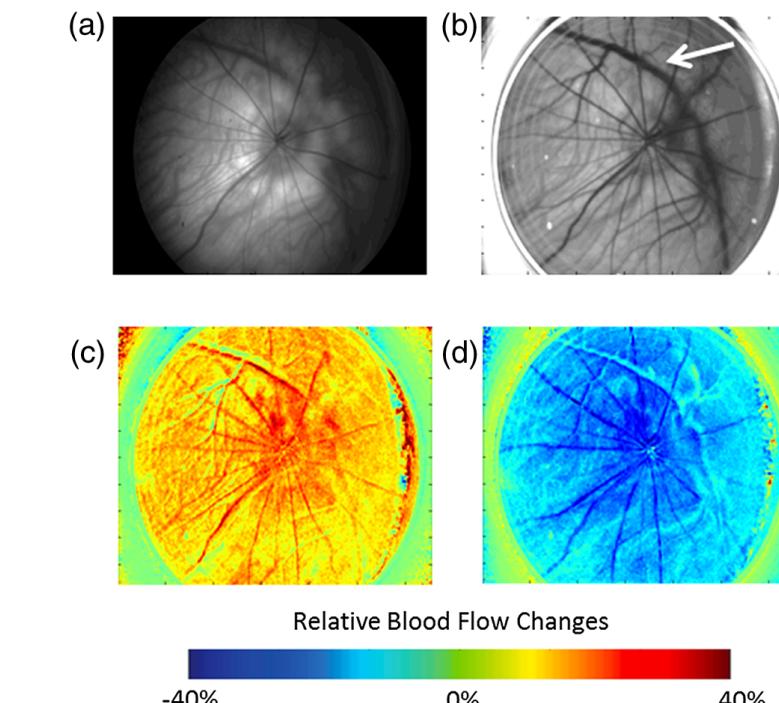
- **Visualization and localization of blood vessels (VLBV)** is important for different biomedical applications, such as neuroscience, dermatology and ophthalmology<sup>1</sup>.



(a) Brain activation and blood flow changes in the brain<sup>1</sup>.



(b) Assessment of photodynamic therapy in Port Wine Stains<sup>2</sup>.



(c) Visual stimulation and blood flow analysis in the retina<sup>3</sup>.

- **Laser Speckle Imaging (LSI)** is the most widely used non-invasive technique for measuring blood flow and is based on the speckle phenomenon<sup>4</sup>.

<sup>1</sup>[Boas et al., 2010]. "Laser speckle contrast imaging in biomedical optics". Journal of biomedical optics.

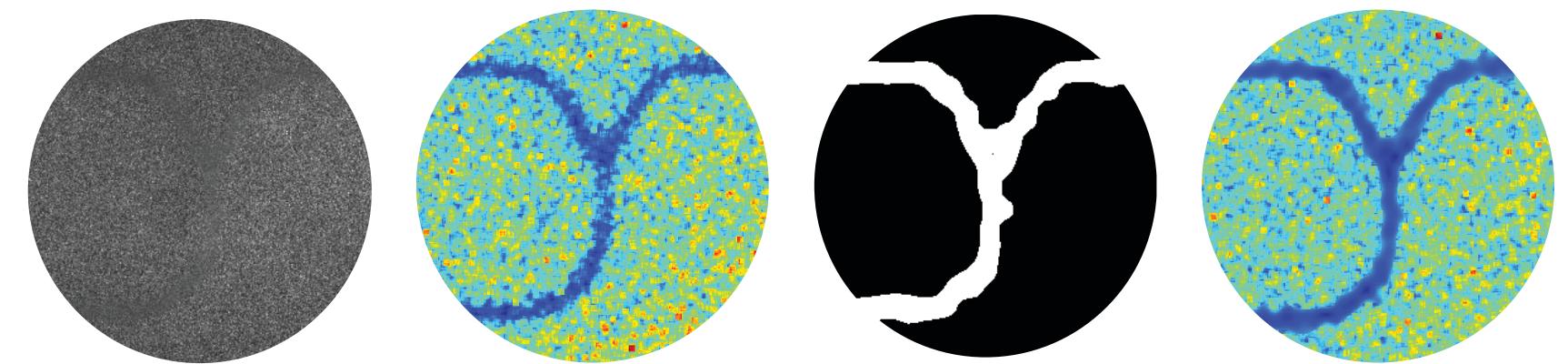
<sup>2</sup>[Choi et al., 2016]. "The role of laser speckle imaging in port-wine stain research: Recent advances and opportunities". IEEE Journal of Selected Topics in Quantum Electronics.

<sup>3</sup>[Ponticorvo et al., 2013]. "Laser speckle contrast imaging of blood flow in rat retinas using an endoscope". Journal of biomedical optics.

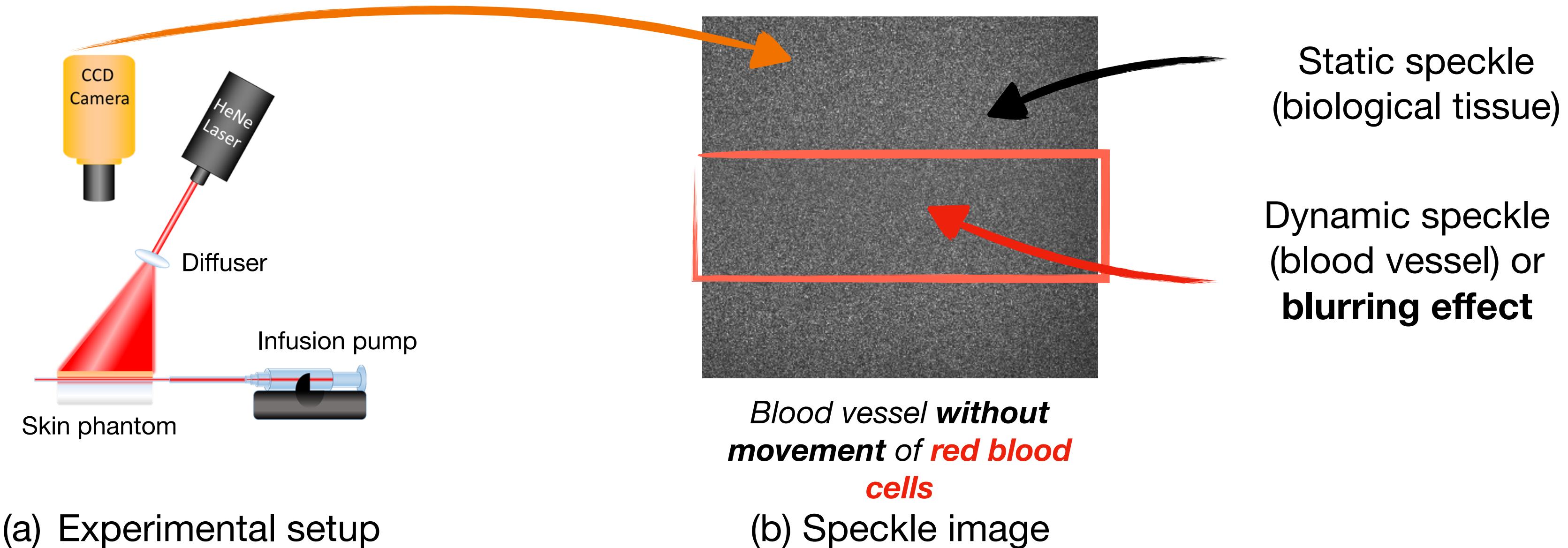
<sup>4</sup>[Briers, et al., 2013]. "Laser speckle contrast imaging: theoretical and practical limitations". Journal of biomedical optics.

# Introduction

## Laser Speckle Imaging (LSI)



- Speckle is a scattering phenomenon. It appears by interaction between photons, of a coherent light laser, and a rough surface such as biological tissue<sup>5</sup>.



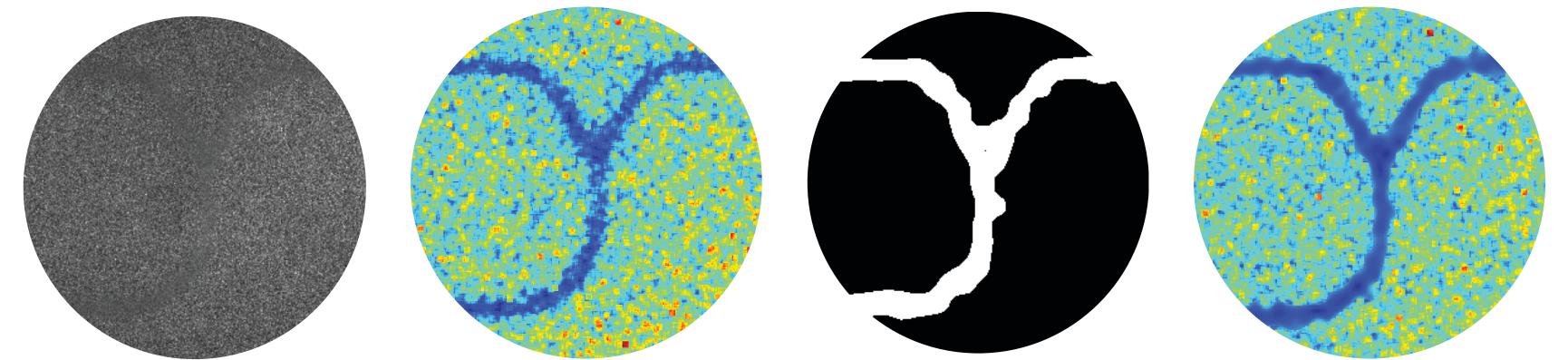
- The movement of particles (i.e. blood cells) inside a rough surface generates a **blurring effect (BE)**. LSI technique is used to analyze the **BE**<sup>6</sup>.

<sup>5</sup>[Aizu and Asakura, 1991]. "Bio-speckle phenomena and their application to the evaluation of blood flow". Optics & Laser Technology.

<sup>6</sup>[Draijer et al., 2009]. "Review of laser speckle contrast techniques for visualizing tissue perfusion". Lasers in medical science.

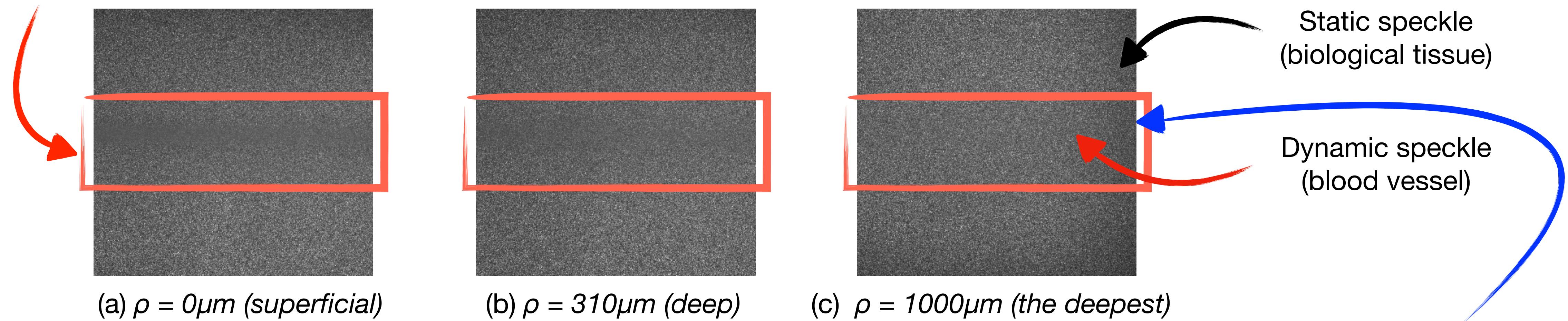
# Introduction

## Laser Speckle Imaging (LSI)



- The main limitation of **LSI** is related to **VLBV**. Speckle images noise increases when the depth of the blood vessels ( $\rho$ ), inside the skin, is higher. It is due to strongly scattering of static structures<sup>7</sup>.

This is a good BE!



Visualization of straight in-vitro blood vessels in a speckle image to different depths ( $\rho$ ).

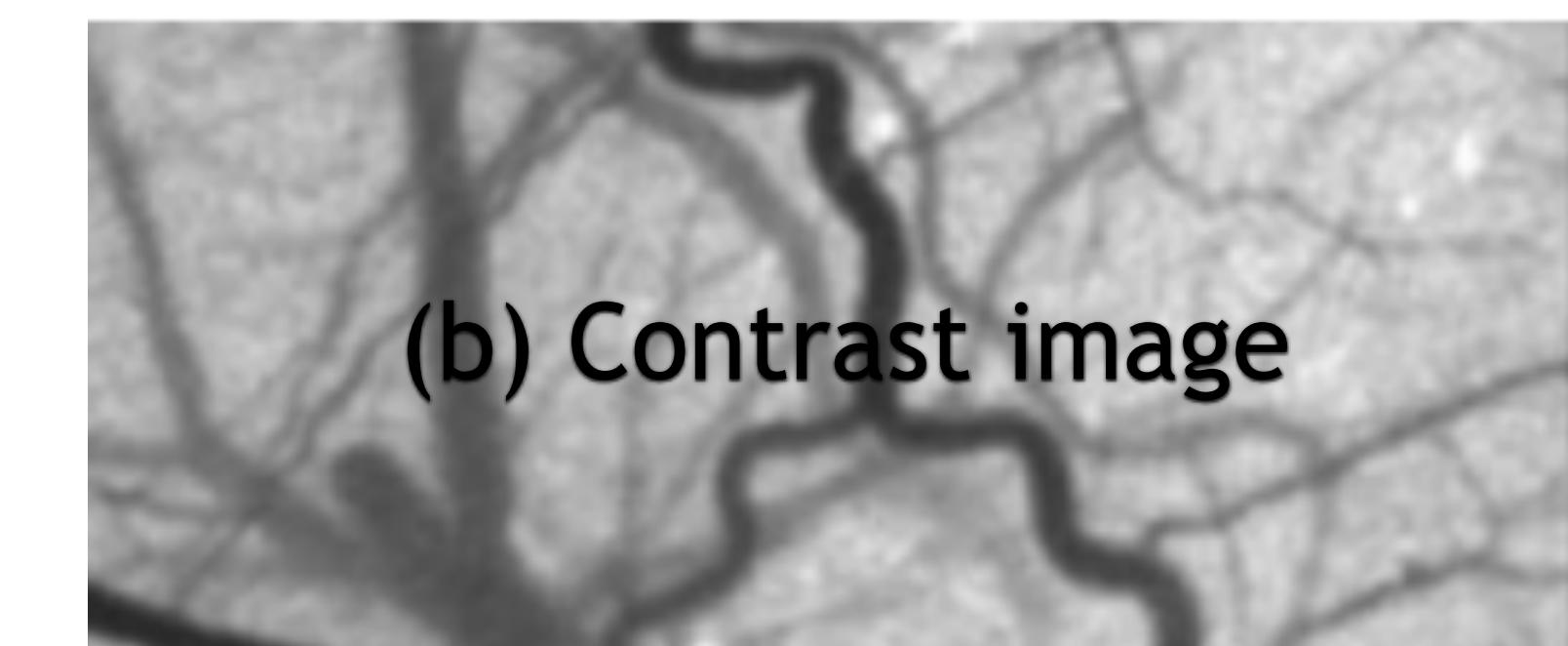
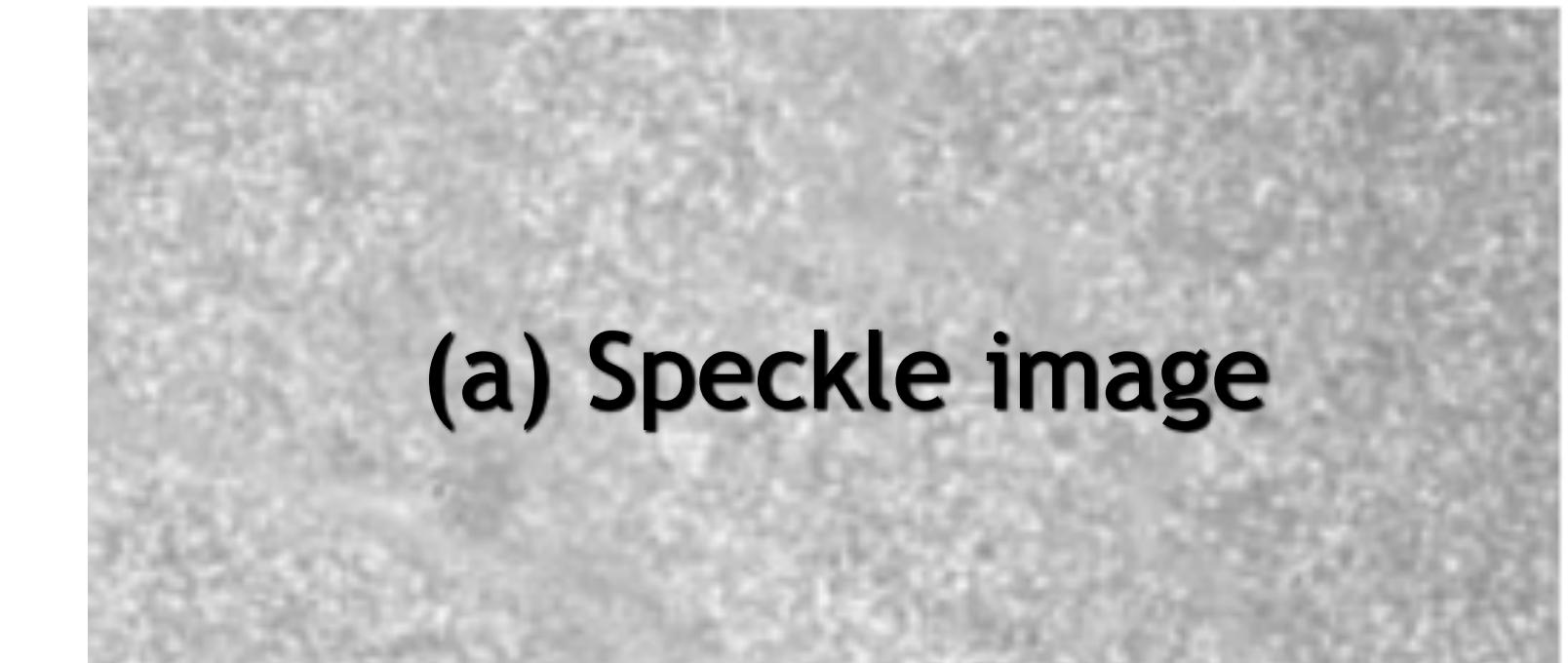
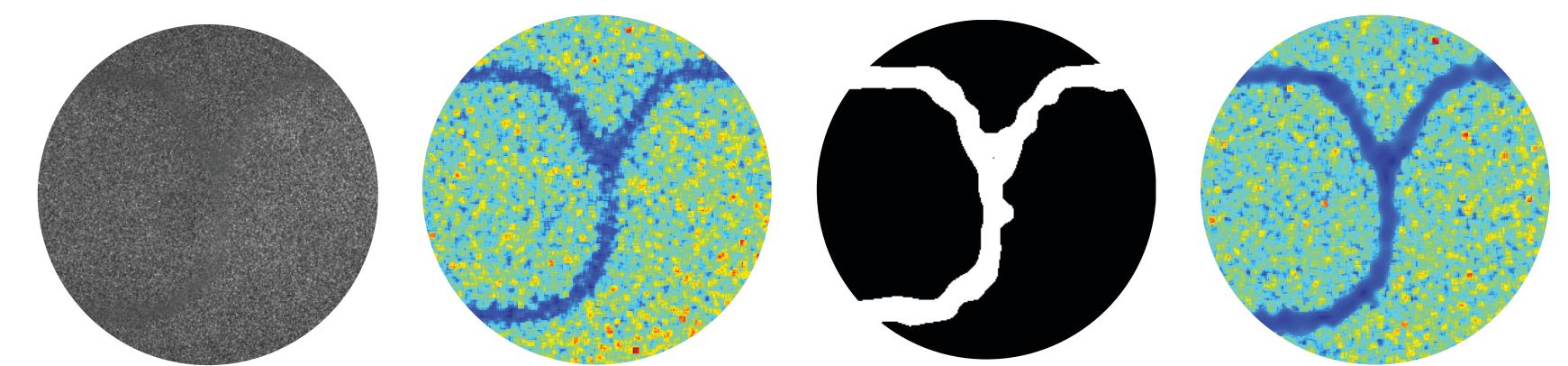
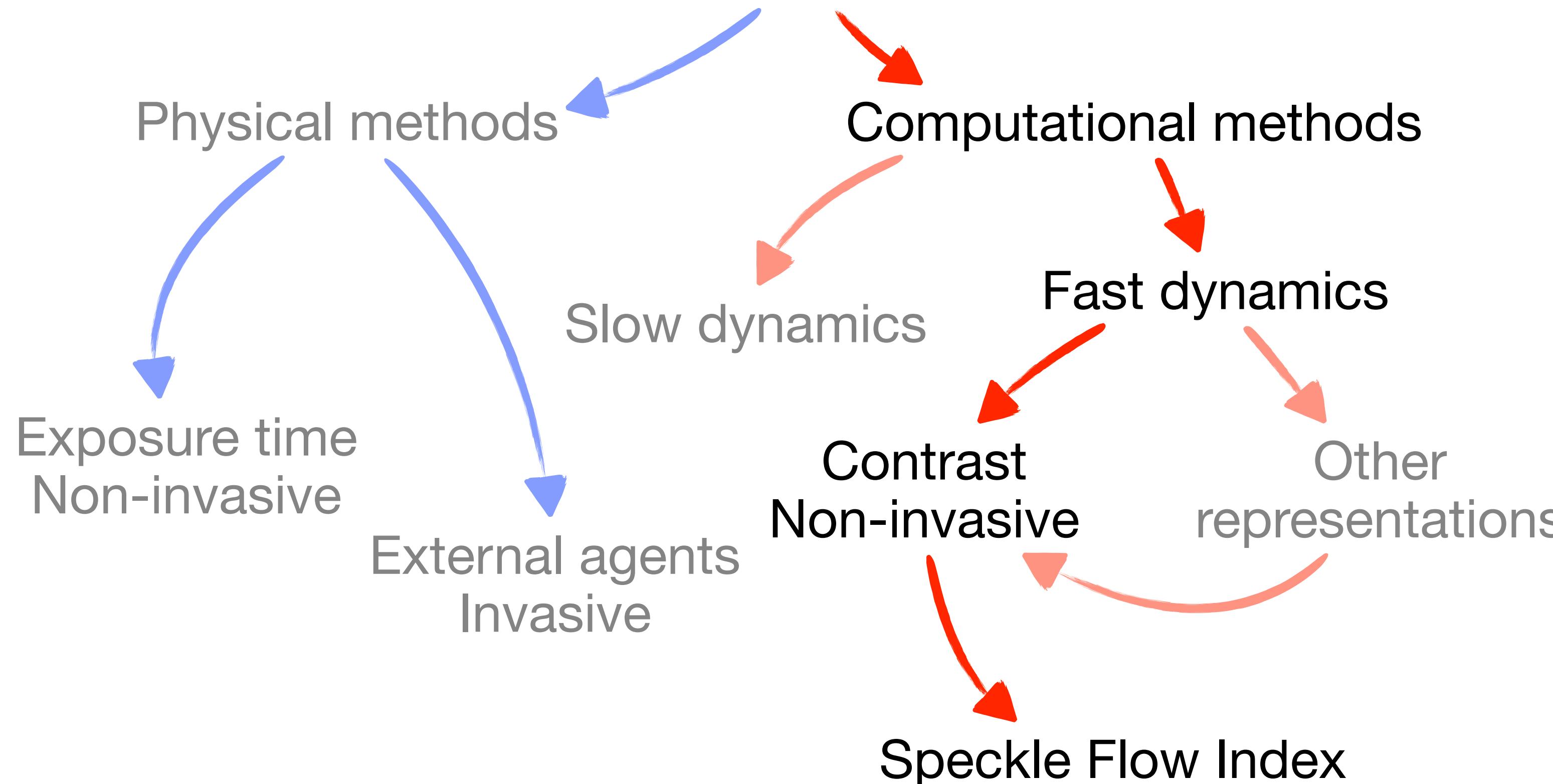
This is a bad BE!

<sup>7</sup>[Vaz et al., 2016]. "Laser speckle imaging to monitor microvascular blood flow: a review". IEEE reviews in biomedical engineering.

# Introduction

## Laser Speckle Imaging (LSI)

### Visualization and localization of blood vessels

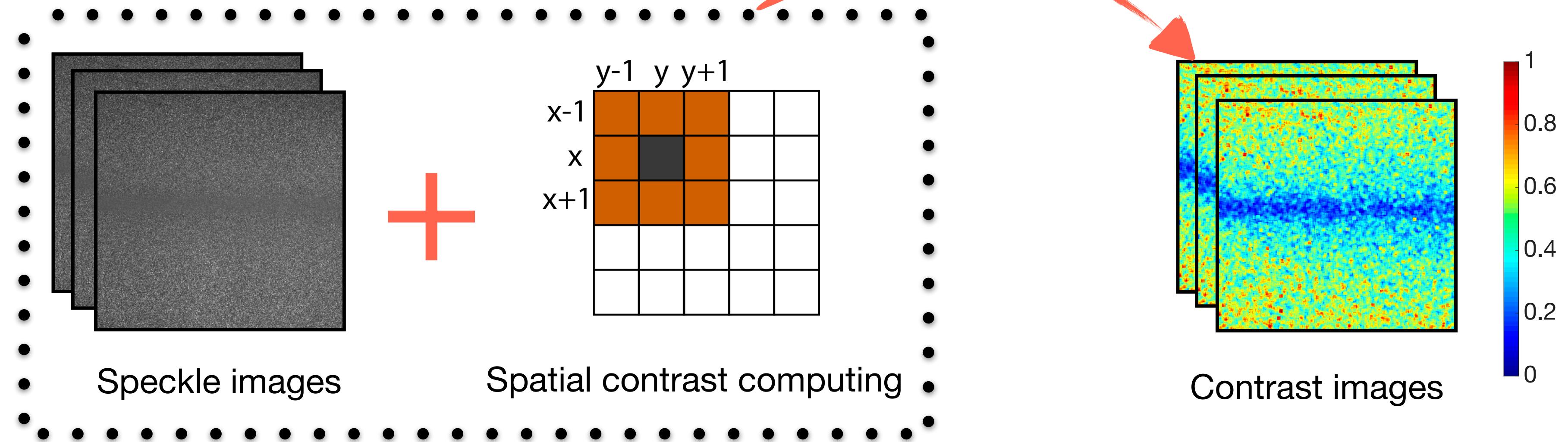


Computational methods<sup>7</sup>.  
Fast dynamics with contrast representation.  
(a) speckle image, and (b) contrast image.

<sup>7</sup>[Vaz et al., 2016]. "Laser speckle imaging to monitor microvascular blood flow: a review". IEEE reviews in biomedical engineering.

# Concepts

## Contrast to improve VLBV

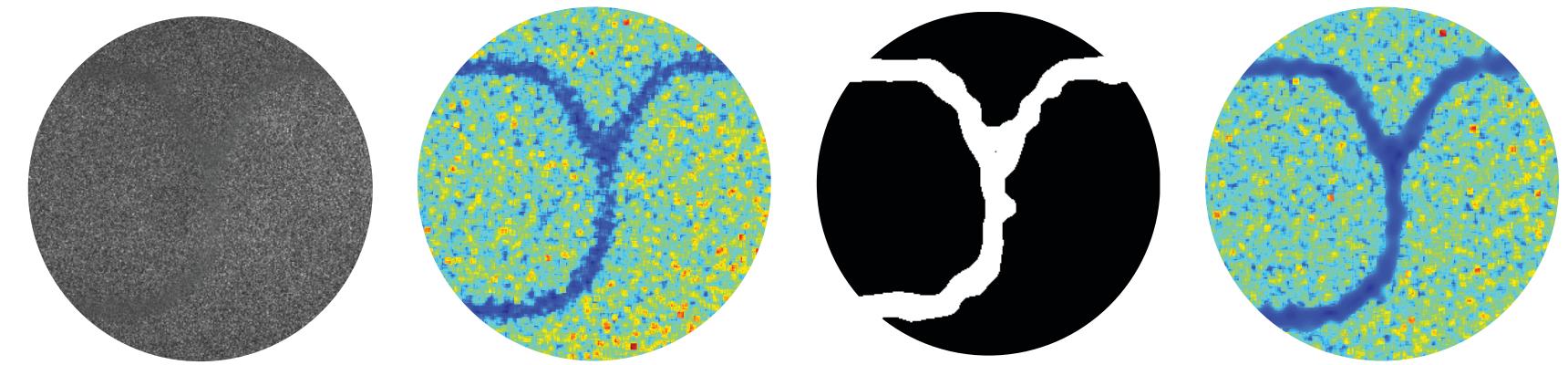


- Contrast ( $K$ ) in speckle images can be calculated using traditional methods, such as spatial contrast ( $sK$ )<sup>7</sup>.
- $K$  is the ratio between standard deviation and the average intensity,  $\sigma(W)$  and  $I(W)$ , respectively, in a  $d \times d$  analysis window.

<sup>7</sup>[Vaz et al., 2016]. "Laser speckle imaging to monitor microvascular blood flow: a review". IEEE reviews in biomedical engineering.

# State of the art

## Related work



Work	Improve	Sample	Resume
Morphological Approach <sup>8</sup> (MA)	Localization	In-vitro B-S (0 to 900um)	Contrast + mathematical morphology
Principal Component Analysis <sup>9</sup> (PCA)	Both	In-vitro S (0 to 1mm)	PCA processing + contrast, and K-Nearest Neighbors
Space-directional Contrast <sup>10</sup> (sdK)	Visualization	In-vitro S (0 to 400um)	Contrast processing with an anisotropic window in 4 directions
Gaussian Sliding Window <sup>11</sup> (GSW)	Visualization	In-vivo	Contrast + gaussian filtering
Homogeneity representation <sup>12</sup> (HR)	Localization	In-vitro B-S (0 to 900um)	Homogeneity and kurtosis analysis
Haar wavelet <sup>13</sup> (Haar)	Visualization	In-vivo	Contrast + Wavelet Transform (simple level)
Ours - Wavelet Approach (WA)	Both	In-vitro B-S (0 to 900um)	Contrast + Wavelet Transform (automatic selection of level) + area criteria

<sup>8</sup>[Morales-Vargas et al., 2018]. "A morphological approach for locating blood vessels in laser contrast speckle imaging". In 2018 IEEE International Instrumentation and Measurement Technology Conference (I2MTC), IEEE.

<sup>9</sup>[Arias-Cruz et al., 2019]. "Visualization of in vitro deep blood vessels using principal component analysis based laser speckle imaging". Biomedical Optics Express.

<sup>10</sup>[Perez-Corona et al., 2018] "Space-directional laser speckle contrast imaging to improve blood vessels visualization". In 2018 IEEE International Instrumentation and Measurement Technology Conference (I2MTC), IEEE.

<sup>11</sup>[Postnikov et al., 2019]. "Gaussian sliding window for robust processing laser speckle contrast images", International journal for numerical methods in biomedical engineering.

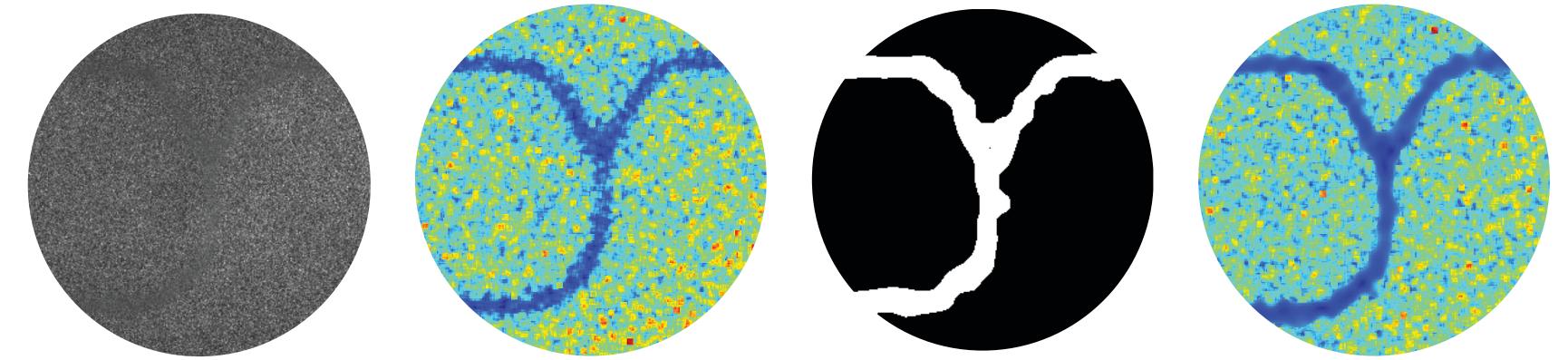
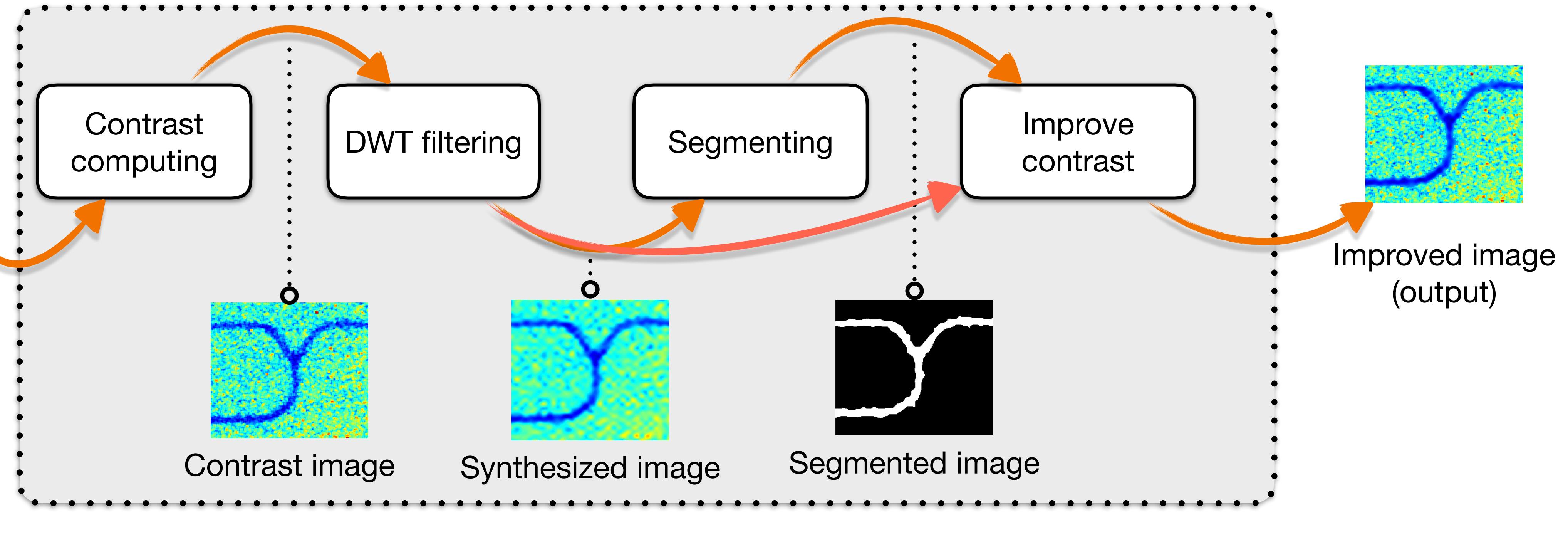
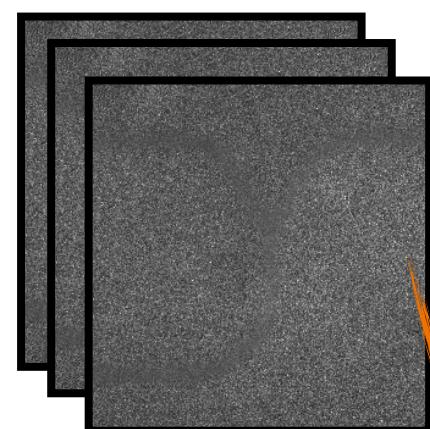
<sup>12</sup>[Peregrina-Barreto et al., 2017]. "Use of kurtosis for locating deep blood vessels in raw speckle imaging using a homogeneity representation". Journal of biomedical optics.

<sup>13</sup>[Postnikov, et al., 2018]. "MATLAB for laser speckle contrast analysis (LASCA): a practice-based approach". Saratov Fall Meeting 2017: Fifth International Symposium on Optics and Biophotonics: Laser Physics and Photonics XIX; Computational Biophysics and Analysis of Biomedical Data IV.

# This work

## Methodology

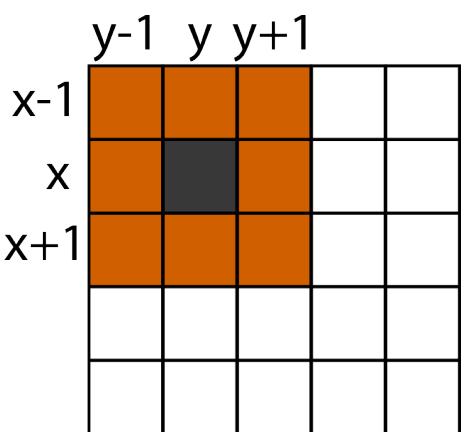
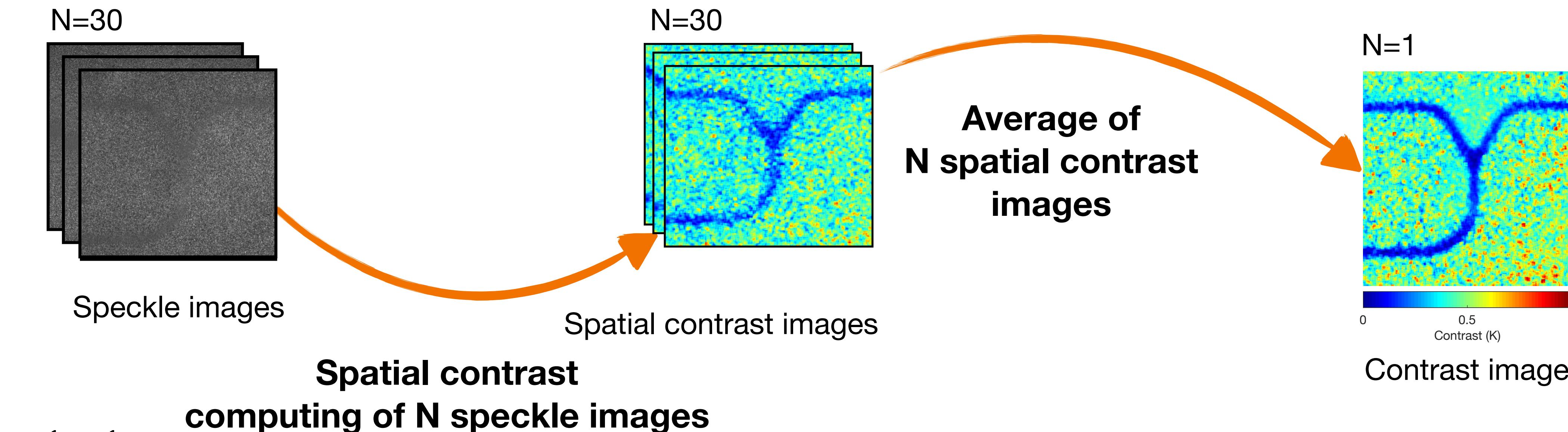
Speckle images  
(input)



# This work

## Contrast computing

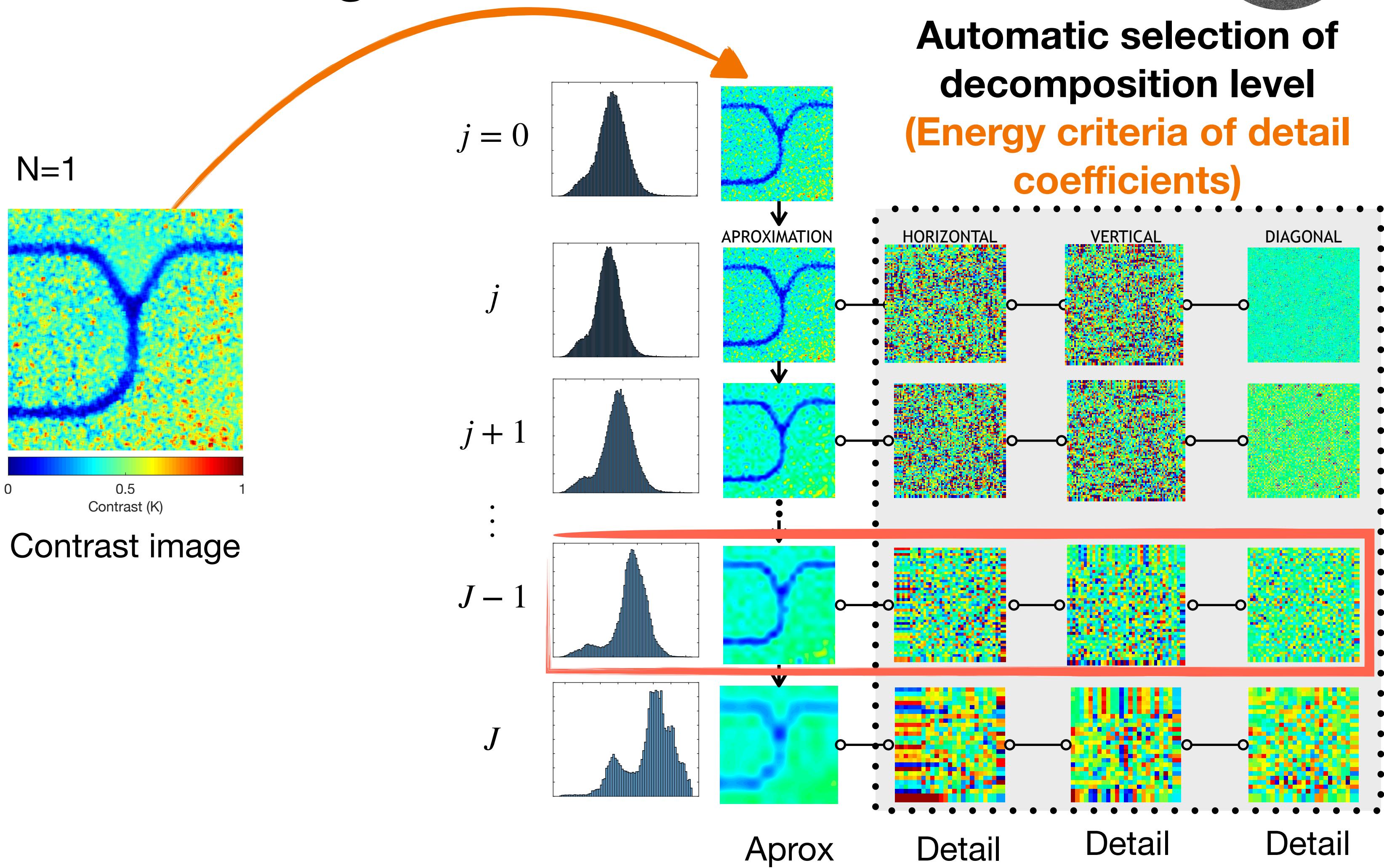
- Contrast ( $K$ ) in speckle images can be calculated using traditional methods, such as spatial contrast ( $sK$ )<sup>7</sup>.



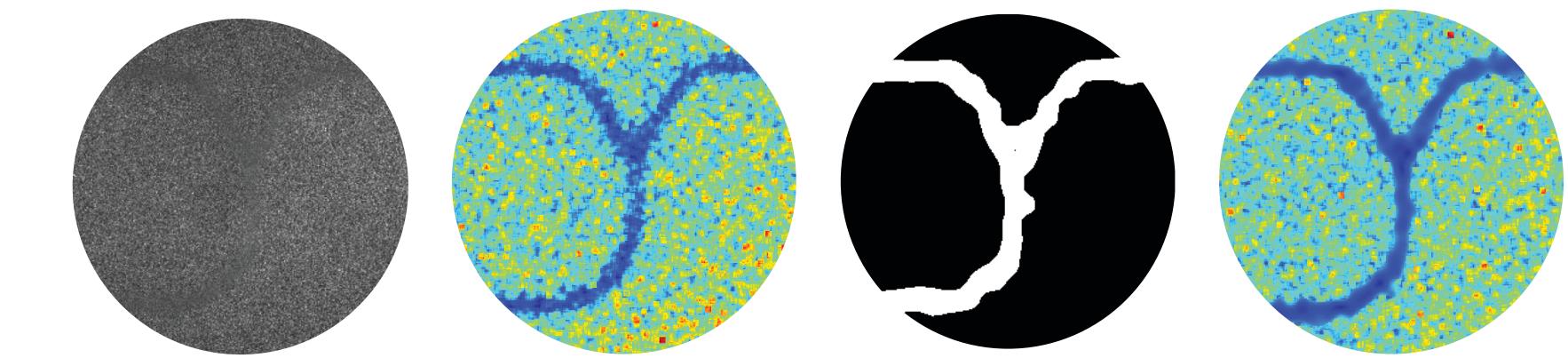
<sup>7</sup>[Vaz et al., 2016]. "Laser speckle imaging to monitor microvascular blood flow: a review". IEEE reviews in biomedical engineering.

# This work

## DWT filtering

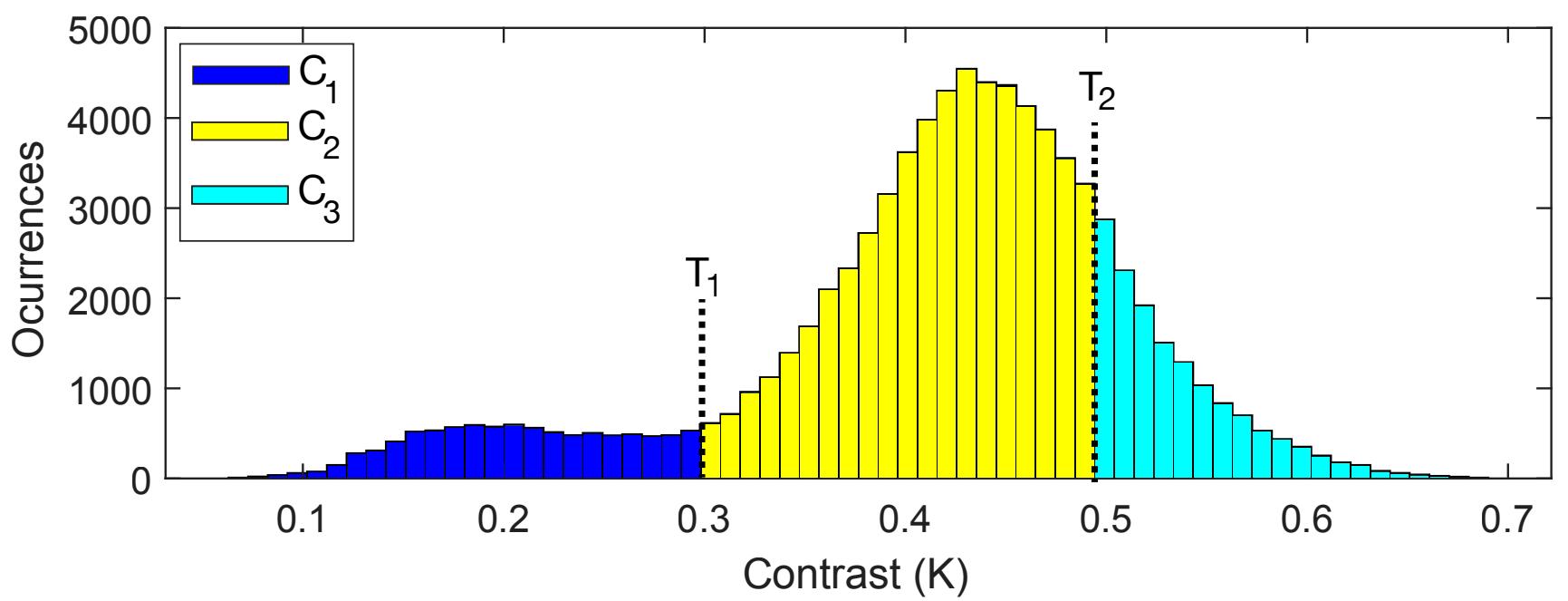
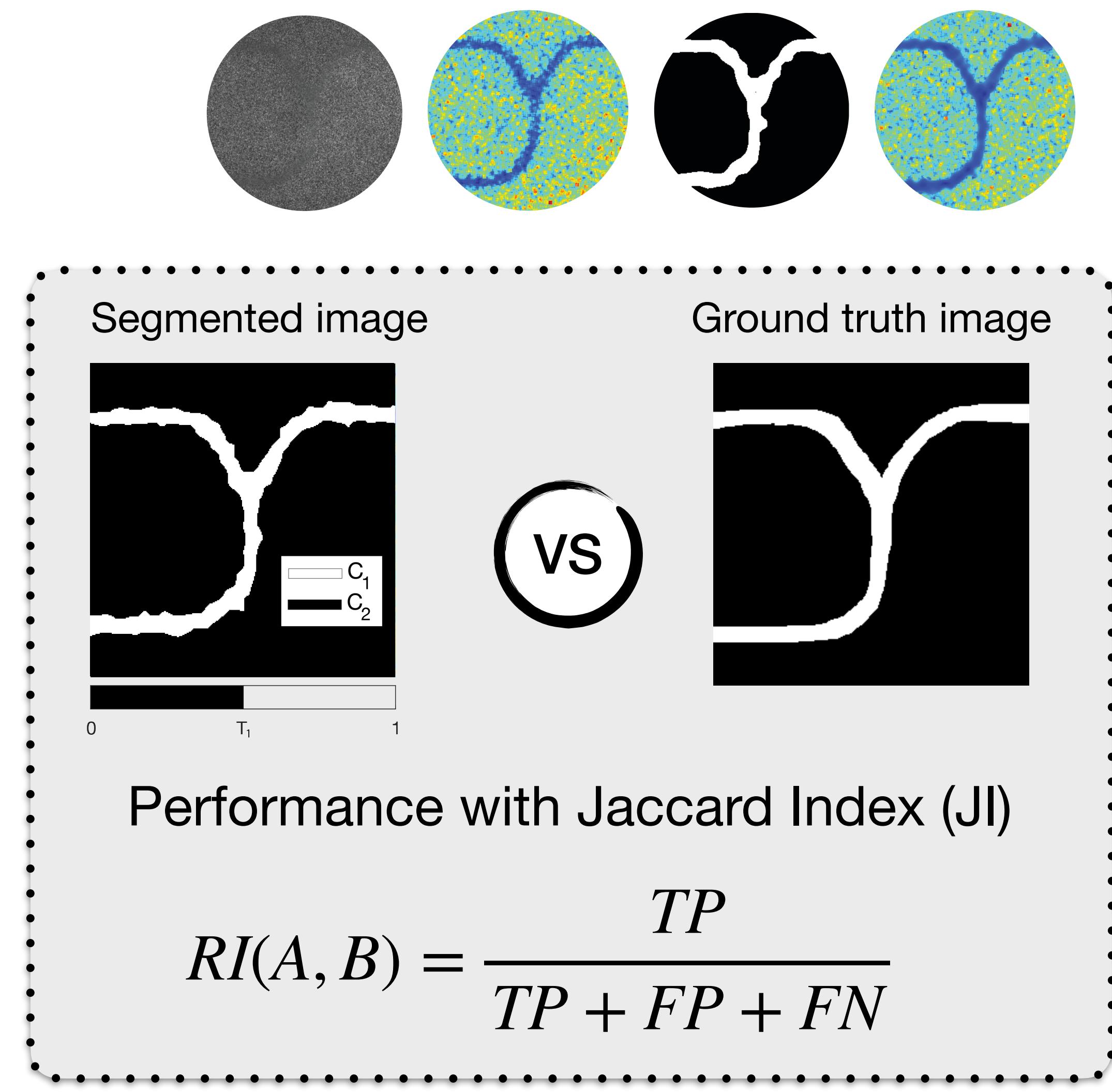
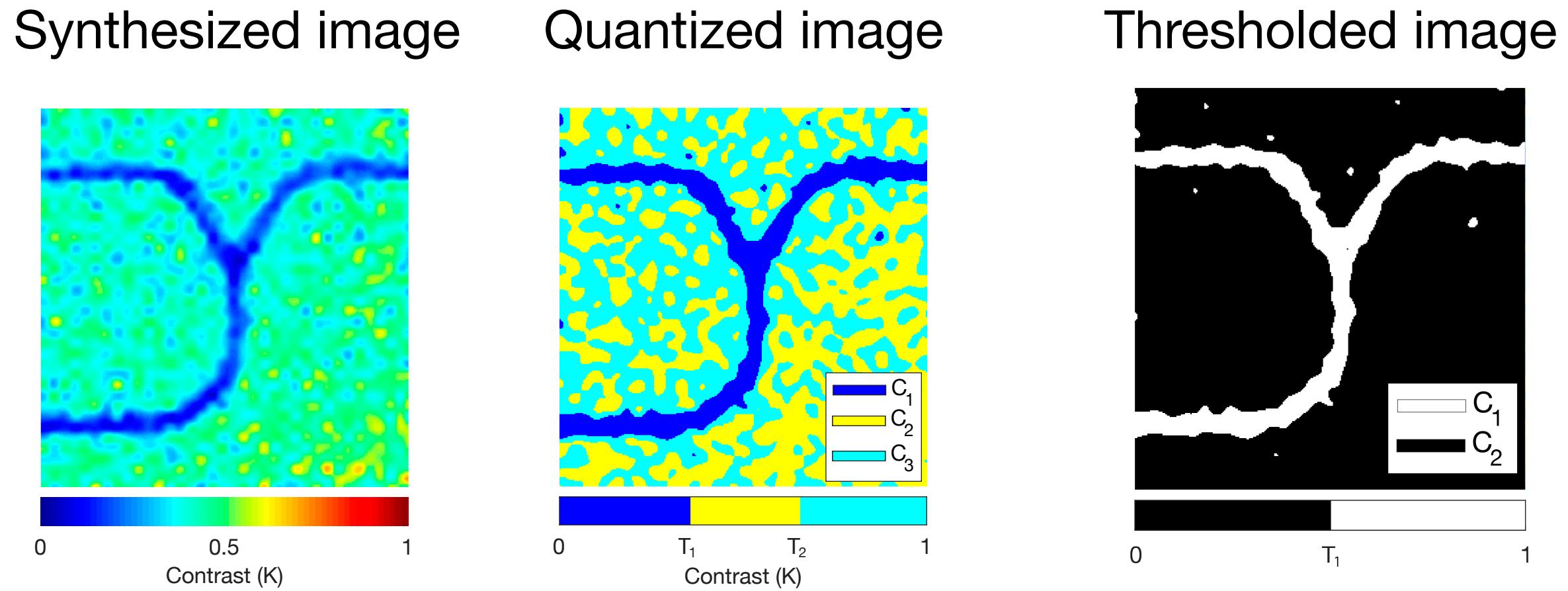


**Automatic selection of  
decomposition level  
(Energy criteria of detail  
coefficients)**



# This work

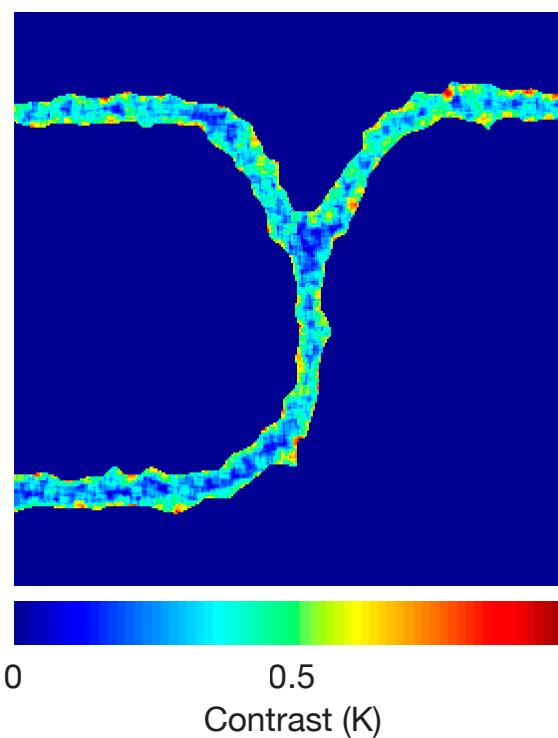
## Thresholding and segmenting



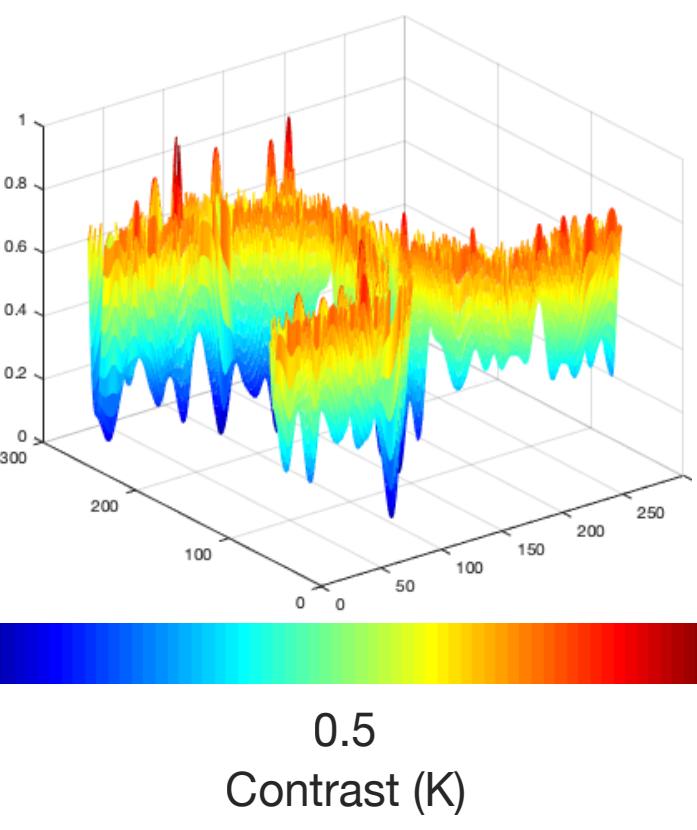
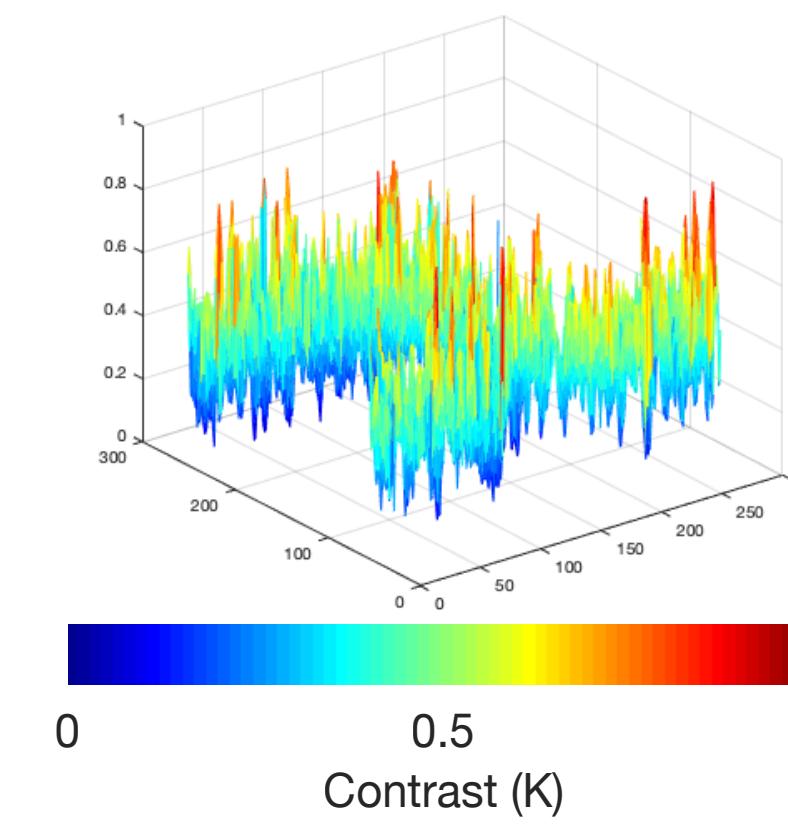
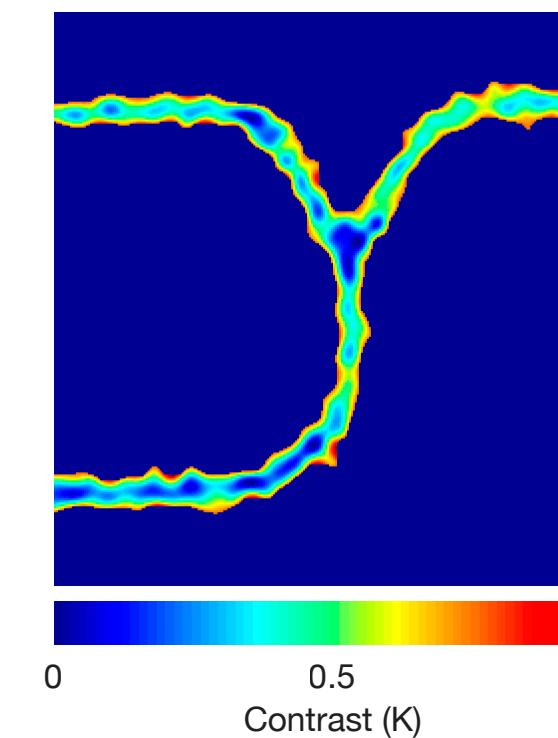
# This work

## Thresholding and segmenting

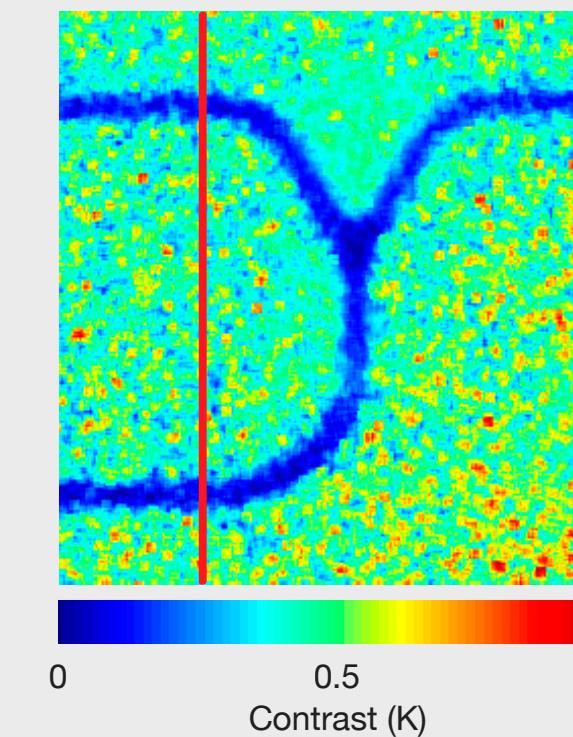
Contrast map



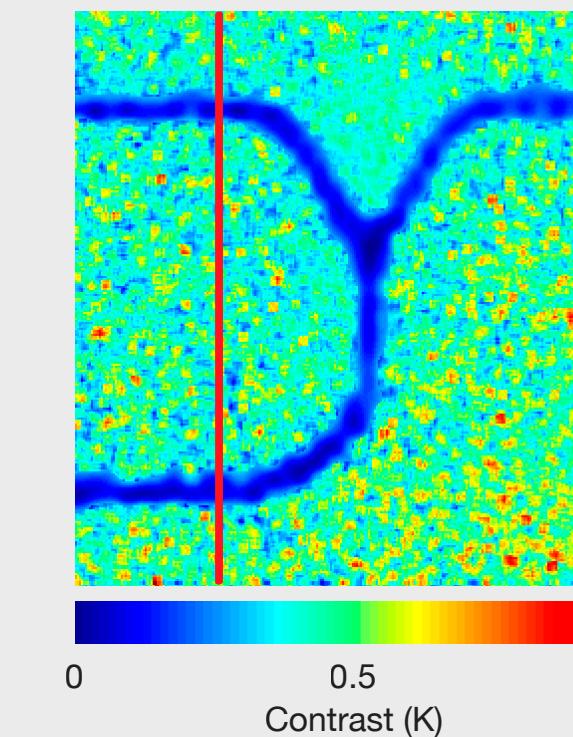
Synthesized map



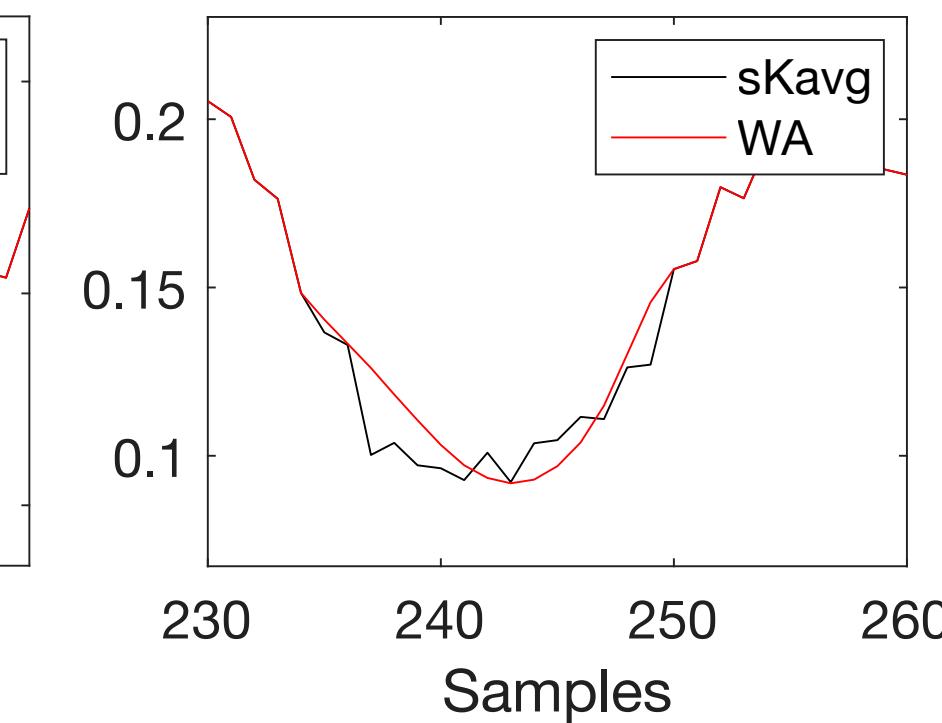
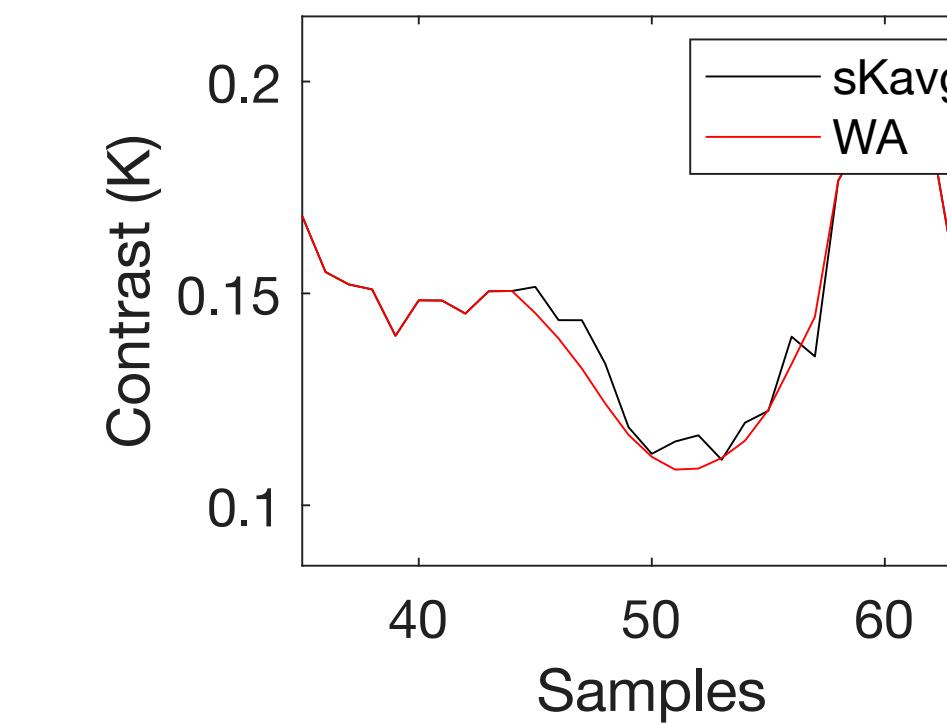
Contrast image  
(input)



Improved image  
(output)



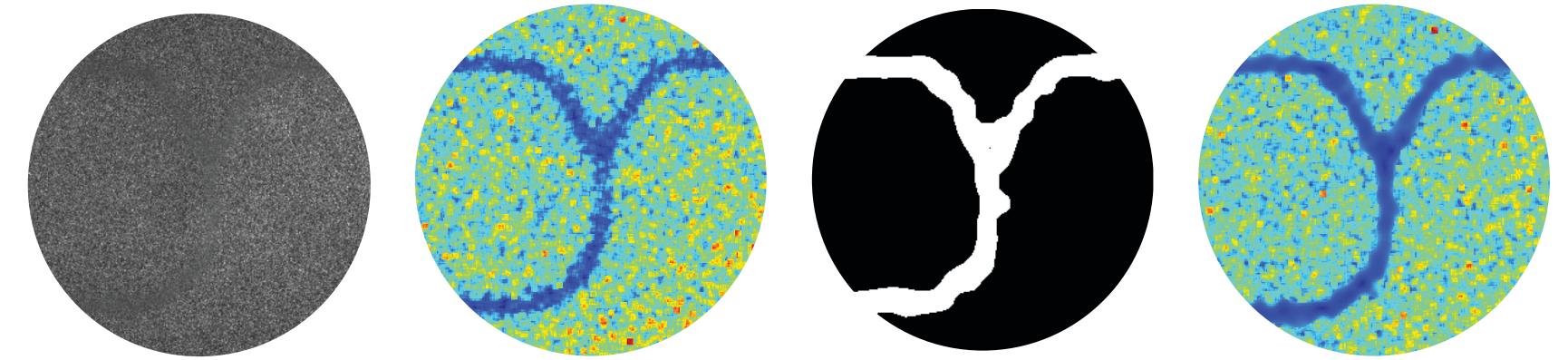
## Performance with CNR



# Experiments and results

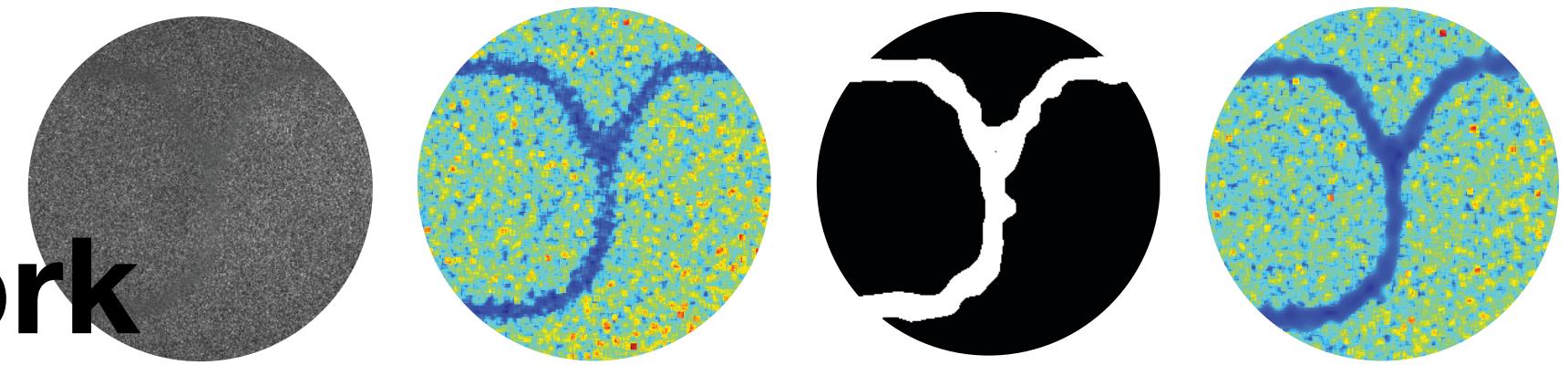
## Dataset

- The dataset consist of
  - **14 speckle packages**, each one of package contains 30 in-vitro straight or bifurcated blood vessels speckle images.
  - **8 blood vessels depths** ( $0\mu m$ ,  $200\mu m$ ,  $300\mu m$ ,  $400\mu m$ ,  $500\mu m$ ,  $600\mu m$ ,  $700\mu m$ , and  $900\mu m$ ).
  - The **dimensions of the in-vitro images for straight vessels and bifurcated vessels** are  $344 \times 329$  pixels and  $280 \times 288$  pixels, respectively
  - The **ground truth** (GT) is a binary image [0,1] and it is obtained by labeling of the blood vessel at  $0\mu m$  depth.
  - The **contrast images** are calculated with the spatial contrast averaged algorithm (sKavg) with an analysis window  $W = 5 \times 5$ .

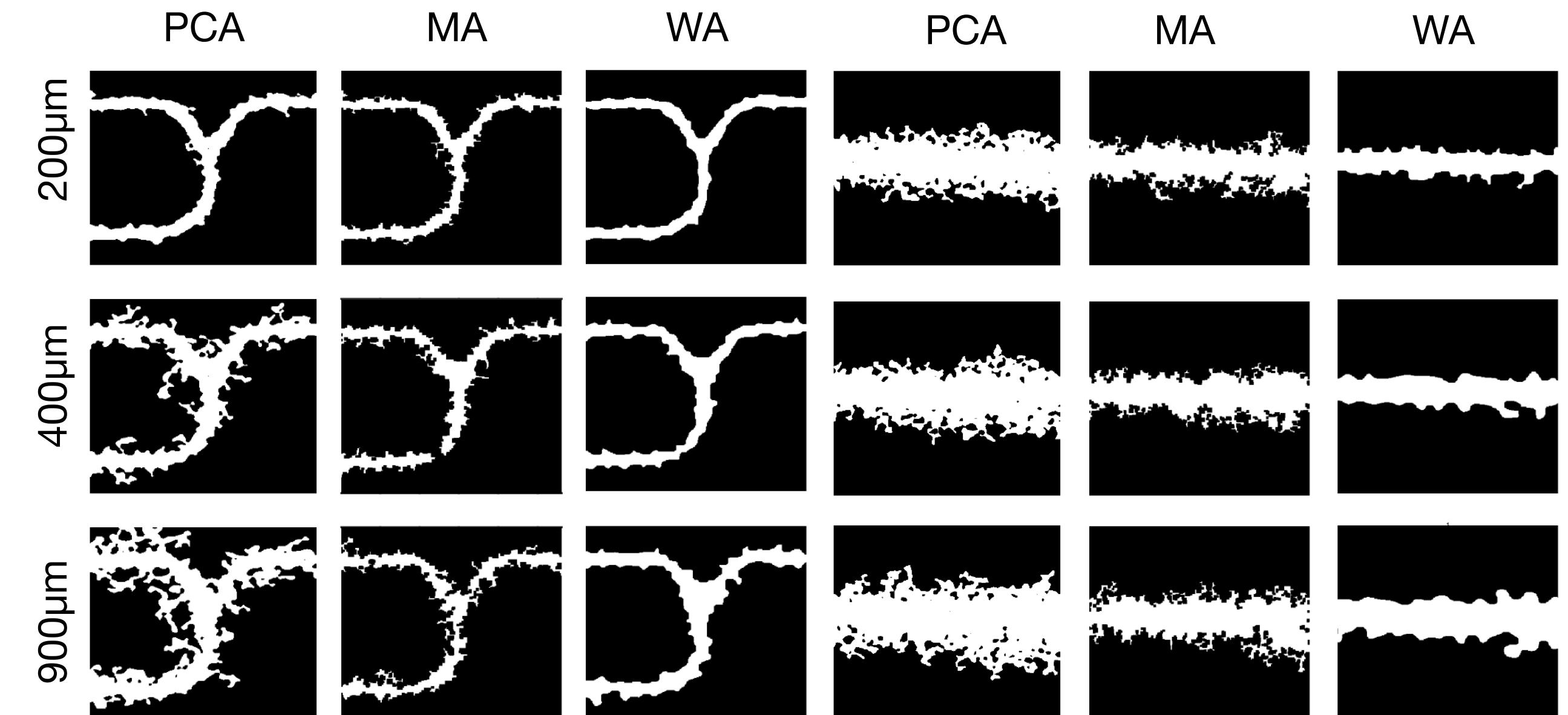


# Experiments and results

## Localization: comparison with related work



Depth μm	PCA <sup>9</sup>	MA <sup>8</sup>	WA
0	35.62±03.26%	<b>50.31±00.04%</b>	<b>83.94±02.09%</b>
200	46.18±17.21%	<b>60.82±10.58%</b>	<b>74.24±04.89%</b>
300	<b>59.14±03.45%</b>	<b>70.74±00.42%</b>	<b>73.15±04.55%</b>
400	32.48±08.84%	<b>57.60±08.87%</b>	<b>59.81±11.83%</b>
500	25.80±06.57%	52.66±07.22%	45.36±11.67%
600	23.96±03.14%	43.89±01.53%	37.78±06.44%
700	23.42±03.85%	43.04±01.31%	38.13±08.58%
900	19.90±01.54%	29.64±13.21%	31.03±02.77%
Avg	<b>33.31±05.98%</b>	<b>49.74±18.49%</b>	<b>55.43±06.60%</b>



- The WA model is useful for improving contrast quality in blood vessels up to 500μm.

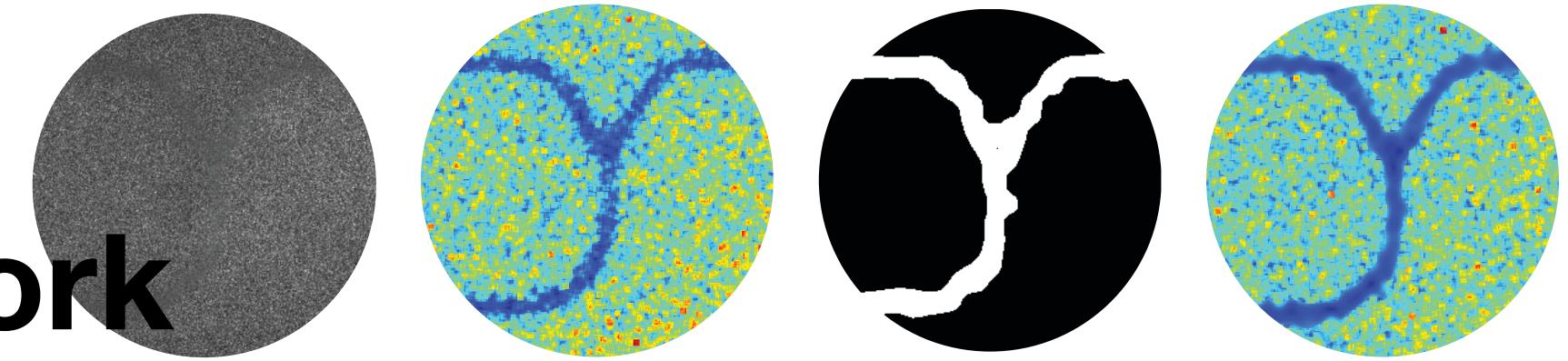
<sup>8</sup>[Morales-Vargas et al., 2018]. "A morphological approach for locating blood vessels in laser contrast speckle imaging". In 2018 IEEE International Instrumentation and Measurement Technology Conference (I2MTC), IEEE

<sup>9</sup>[Arias-Cruz et al., 2019]. "Visualization of in vitro deep blood vessels using principal component analysis based laser speckle imaging". Biomedical Optics Express.

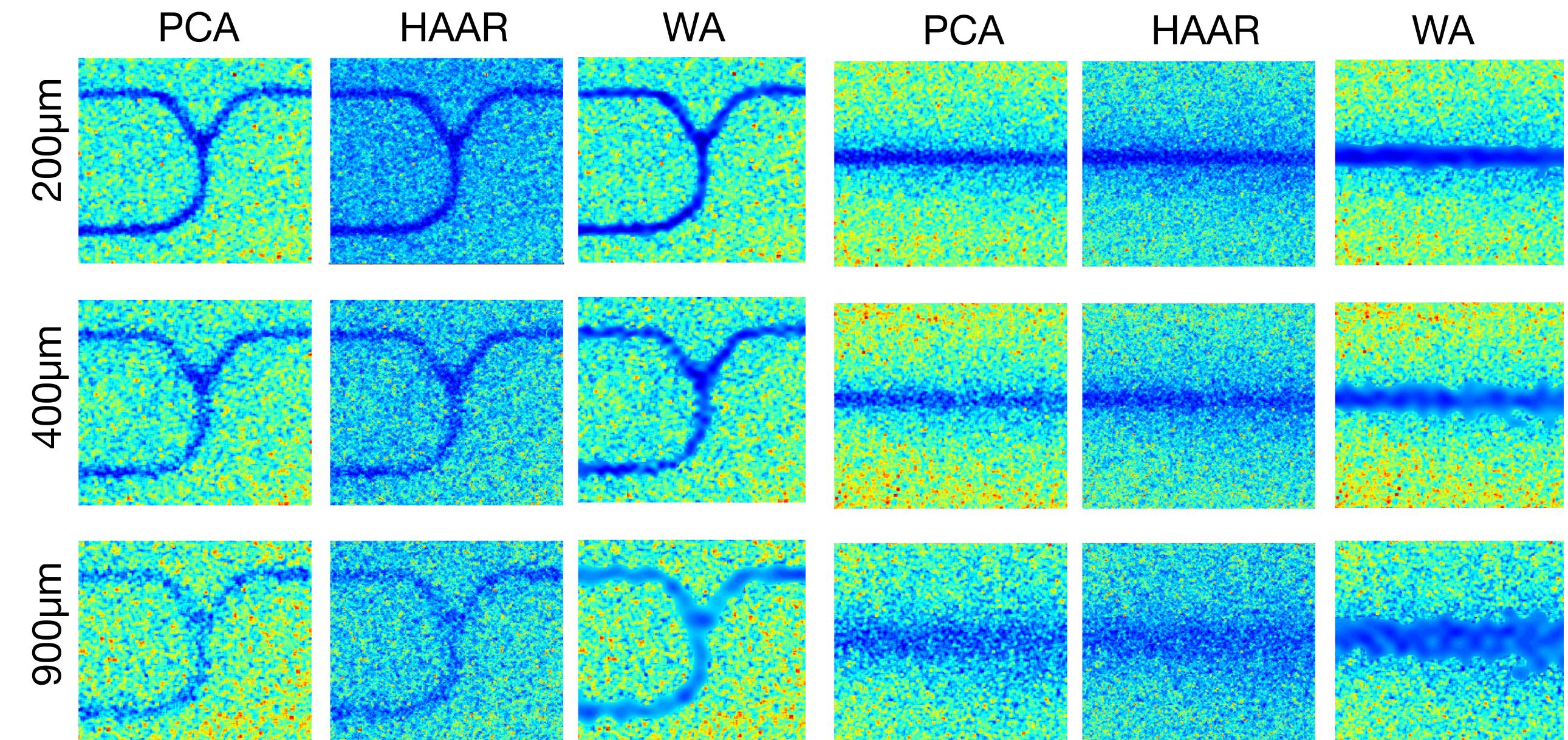
<sup>13</sup>[Postnikov, et al., 2018]. "MATLAB for laser speckle contrast analysis (LASCA): a practice-based approach". Saratov Fall Meeting 2017: Fifth International Symposium on Optics and Biophotonics: Laser Physics and Photonics XIX; Computational Biophysics and Analysis of Biomedical Data IV.

# Experiments and results

## Visualization: comparison with related work



Depth μm	PCA <sup>9</sup>	HAAR <sup>13</sup>	WA
0	2.64±0.42	1.86±0.23	<b>2.97±0.14</b>
200	2.29±0.28	1.54±0.51	<b>3.56±0.21</b>
300	2.12±0.33	1.37±0.49	<b>2.50±0.25</b>
400	1.90±0.38	1.26±0.55	<b>3.04±0.31</b>
500	1.46±0.77	0.95±0.53	<b>2.49±0.45</b>
600	1.31±0.79	0.84±0.38	2.29±1.54
700	1.12±0.91	0.72±0.52	1.66±1.98
900	1.09±0.79	1.15±0.23	1.28±1.04
Avg	<b>1.74±0.58</b>	<b>1.74±0.42</b>	<b>2.47±0.74</b>



- The WA model is useful for locating blood vessels up to 400μm.

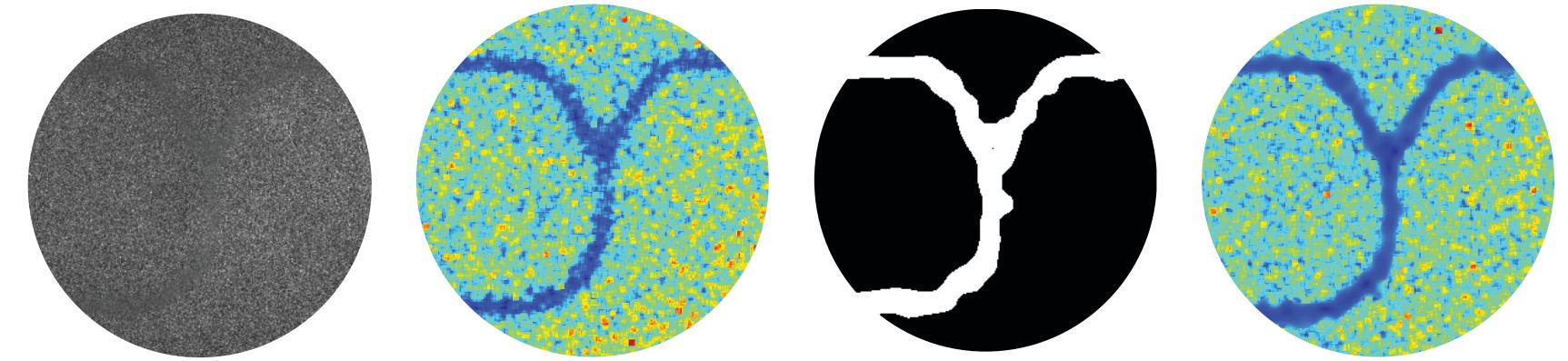
<sup>8</sup>[Morales-Vargas et al., 2018]. "A morphological approach for locating blood vessels in laser contrast speckle imaging". In 2018 IEEE International Instrumentation and Measurement Technology Conference (I2MTC), IEEE

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# Conclusions

## Wavelet Approach



- The visualization and localization is an important task to determine the presence of blood vessels in the biological tissue.
- This work presented a methodology based on a wavelet approach to attenuate noise in contrast images, and improve the localization of blood vessels.
- The results obtained have shown that automatic filtering reduces contrast noise from superficial ( $100\mu\text{m}$ ) and deep (up to  $500\mu\text{m}$ ) blood vessels.

Thank you for your attention!

Questions?

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