



3D-Printed 4-Bar Linkage Prosthetic Knee

Team:

Faith Holowczak,
Gia Garino,
Christopher Joa Chi Lang,
Lianis Santiago,
Victor Mendoza

Mentor: Dr. Nidal Alif



Abstract



1 billion people live with disabilities in low- and middle-income countries, where access to healthcare and prosthetic services is severely limited.



Among them, 4 million are lower-limb amputees, many of whom lack access to affordable and functional prosthetic options.



This project develops a low-cost, 3D-printed prosthetic knee, optimized through refined geometry, printable materials, and validation through FEA and prototyping.

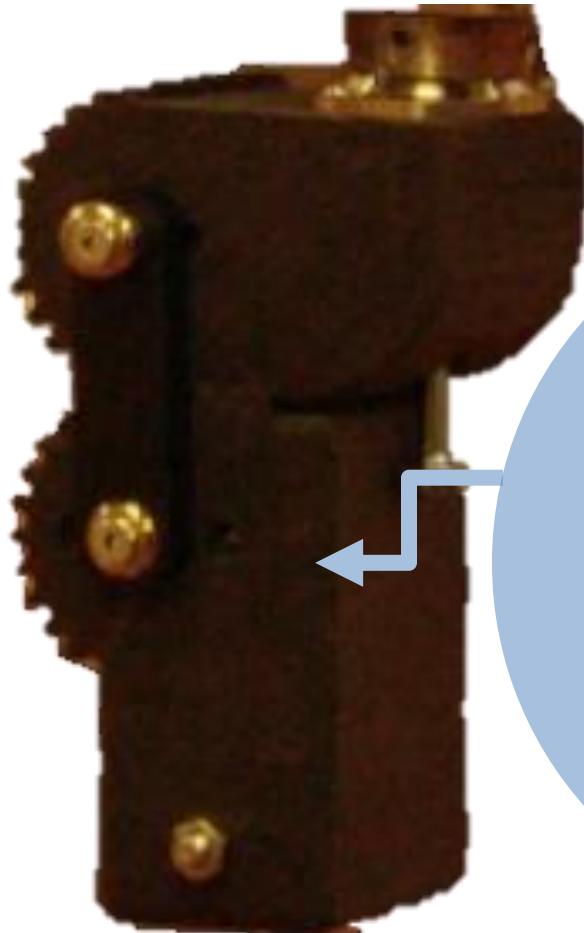


Figure 1: World map of 3D printing hubs



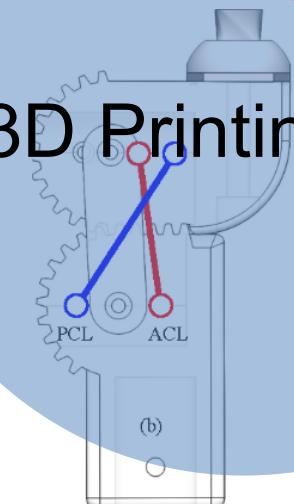
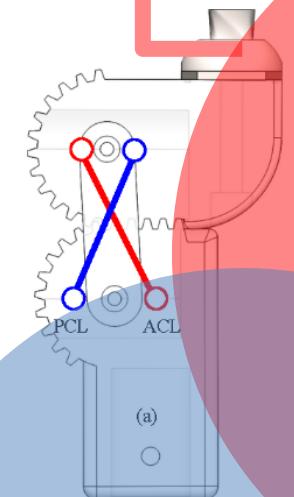
Proposed Solution

3D Printed Gear Mesh Knee



Four-Bar
Linkage

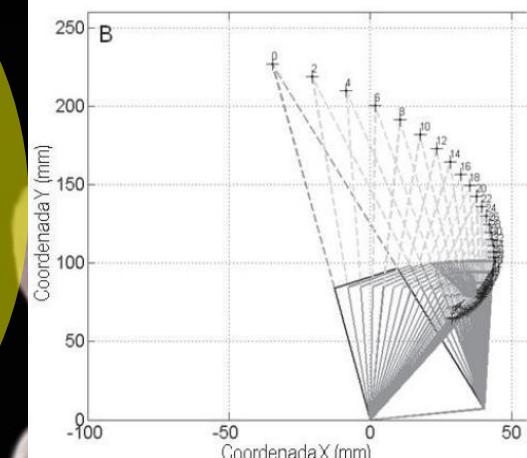
3D Printing



Four-Bars Linkage

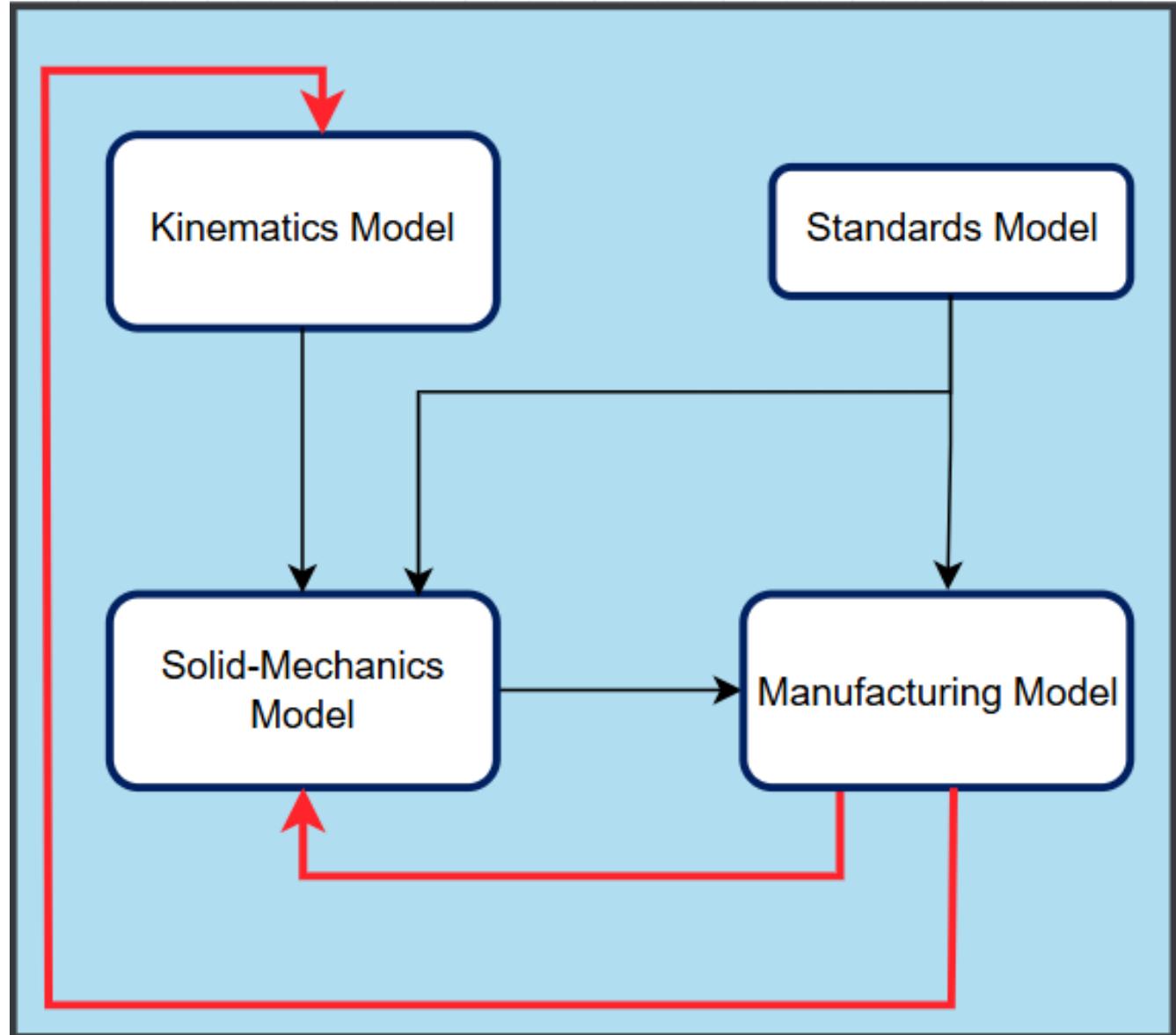
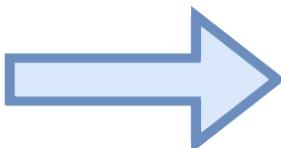


Optimization
Algorithms

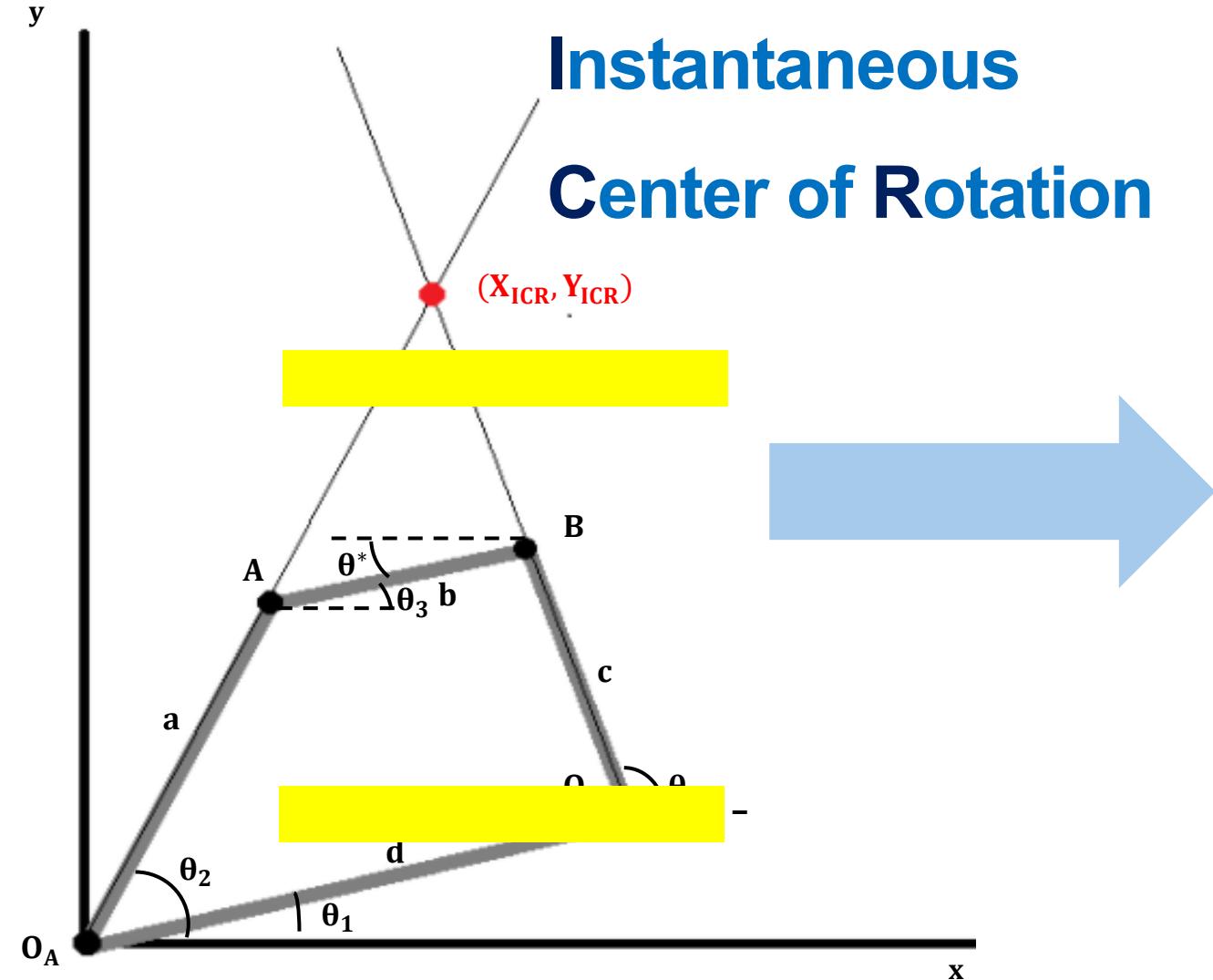


Plan of Action

3D Printed Four-Bar
Knee



Kinematic Analysis



Instantaneous
Center of Rotation

Governing Kinematic Equations:

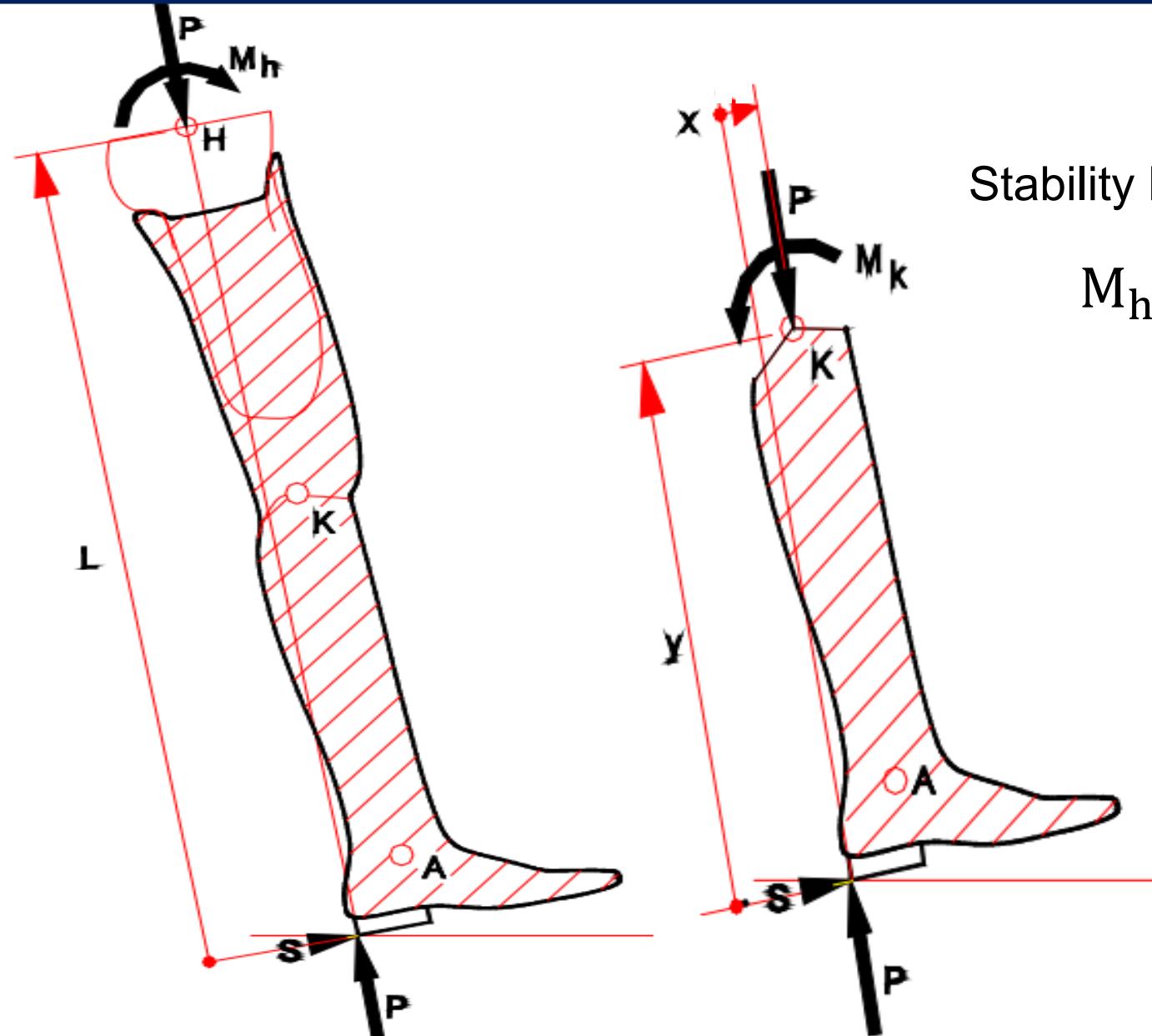
ICR Trajectory in the x-direction :

$$X_{ICR} = \frac{X_{O_B} \tan \theta_4 - Y_{O_B}}{\tan \theta_4 - \tan \theta_2} - d \cos \theta_1 - X_{O_B}$$
$$= f_1(a, b, c, d, \theta_1, \theta_2, \theta_R, \theta^*)$$

ICR Trajectory in the y-direction :

$$Y_{ICR} = \frac{(X_{O_B} \tan \theta_4 - Y_{O_B}) \tan \theta_2}{\tan \theta_4 - \tan \theta_2} - d \sin \theta_1 + Y_{O_B}$$
$$= f_4(a, b, c, d, \theta_1, \theta_2, \theta_R, \theta^*)$$

Ensuring Stability



Stability Equation:

$$M_h = \left(\frac{L}{y} \right) (Px - M_k)$$

$$M_h = PL \left(\frac{x}{y} \right)$$

M_k = Moment from Extension System

P = Axial Load Force

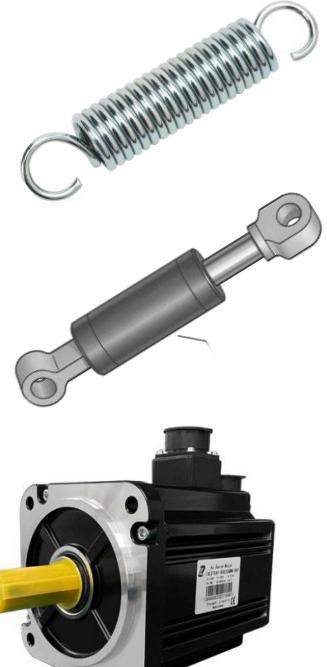
L = Distance Hip – Point of Contact

M_k = Moment from Extension System

y = Distance ICR – Load Line



- Remove Extra Extension System.
- Minimize x/y ratio.



Ensuring Control

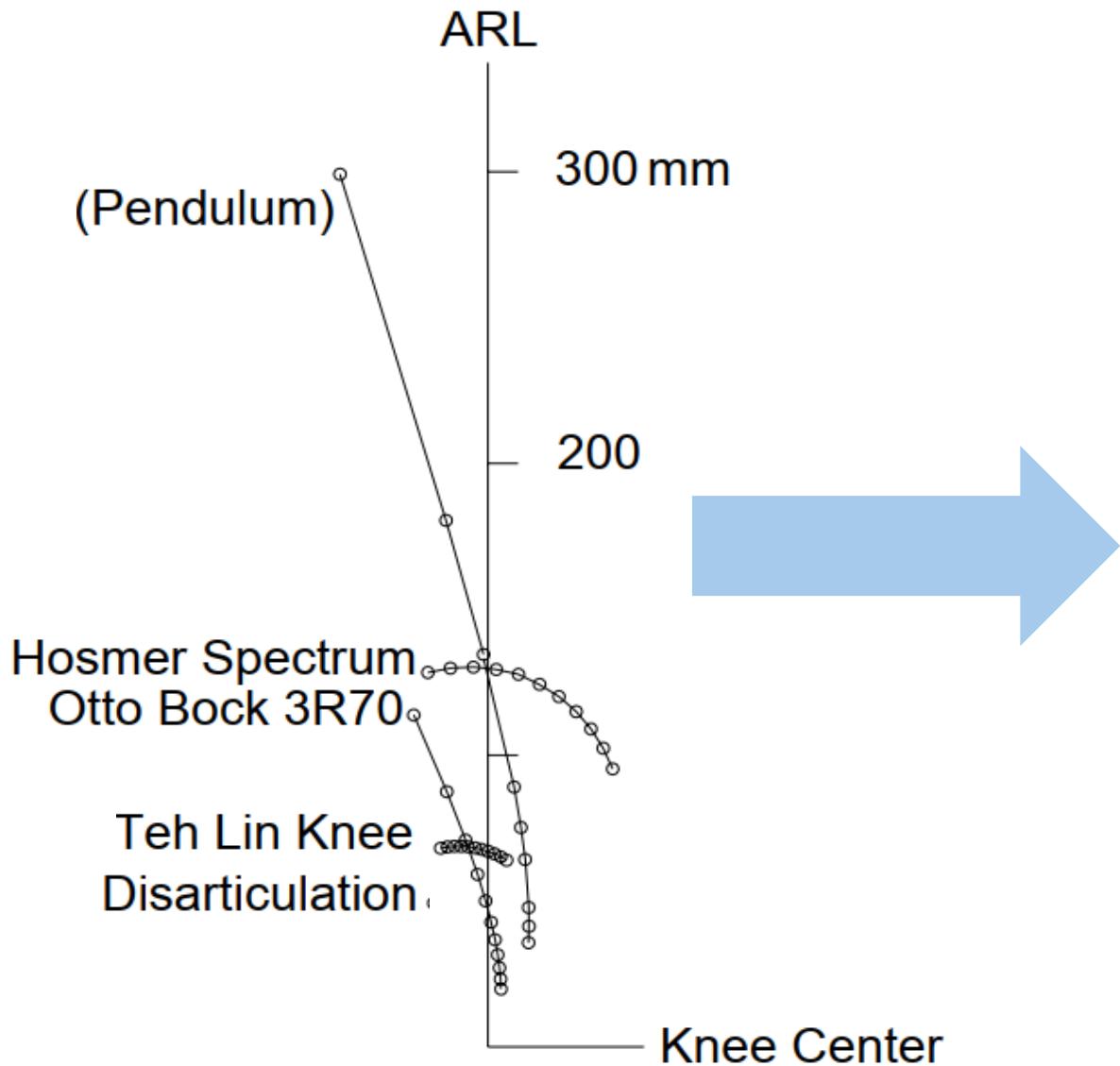


Figure 2: ICR Trajectories for Different Knees

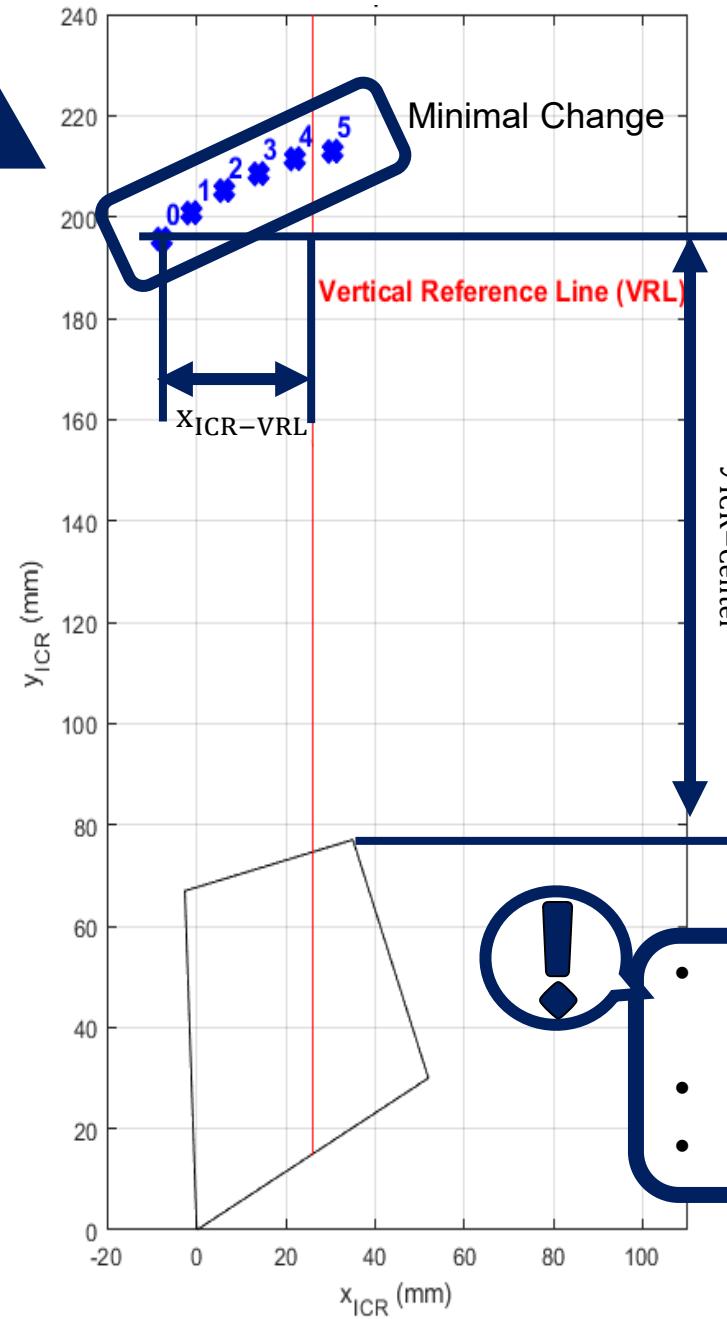


Figure 3: Metrics for Stability

Trajectory Selection

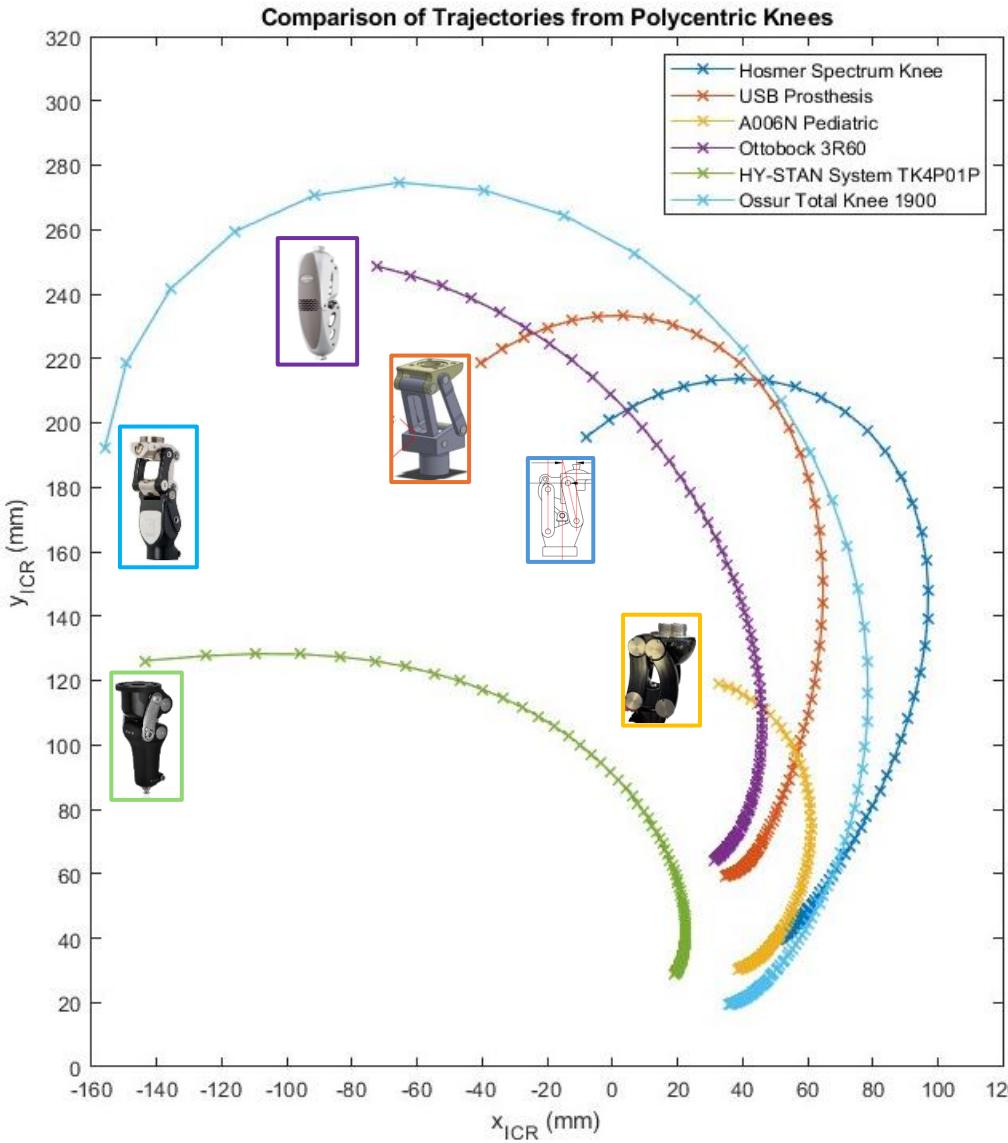


Figure 4: Comparative Study of Knees from the Market

| Knee | x-distance (mm) | y-distance (mm) |
|------------------------|-----------------|-----------------|
| Hosmer Spectrum Knee | 34 | 119 |
| USB Prosthesis | 60 | 123 |
| A006N Pediatric | -17 | 66 |
| Ottobock 3R60 | 93 | 157 |
| HY-STAN System TK4P01P | 158 | 95 |
| Ossur Total Knee 1900 | 172 | 157 |

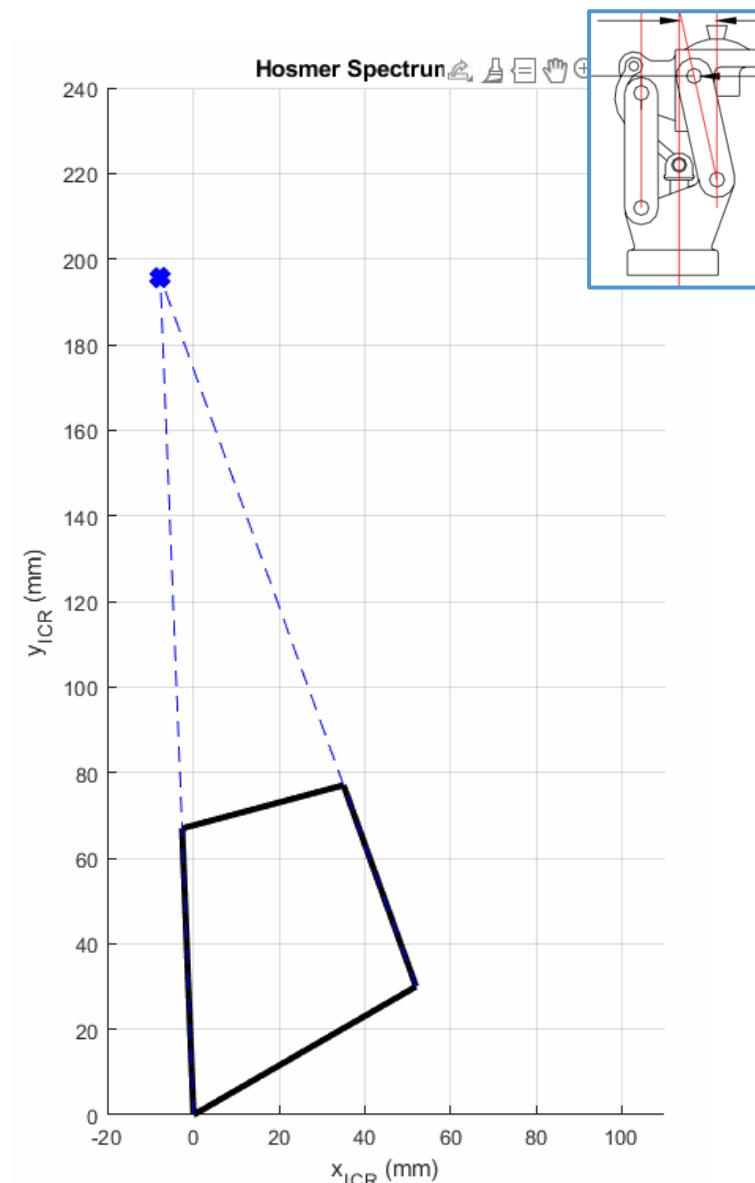
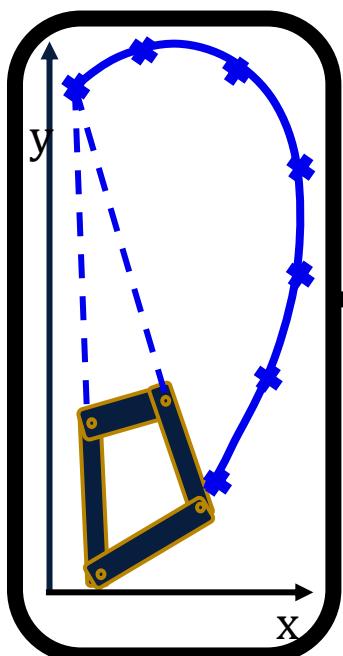


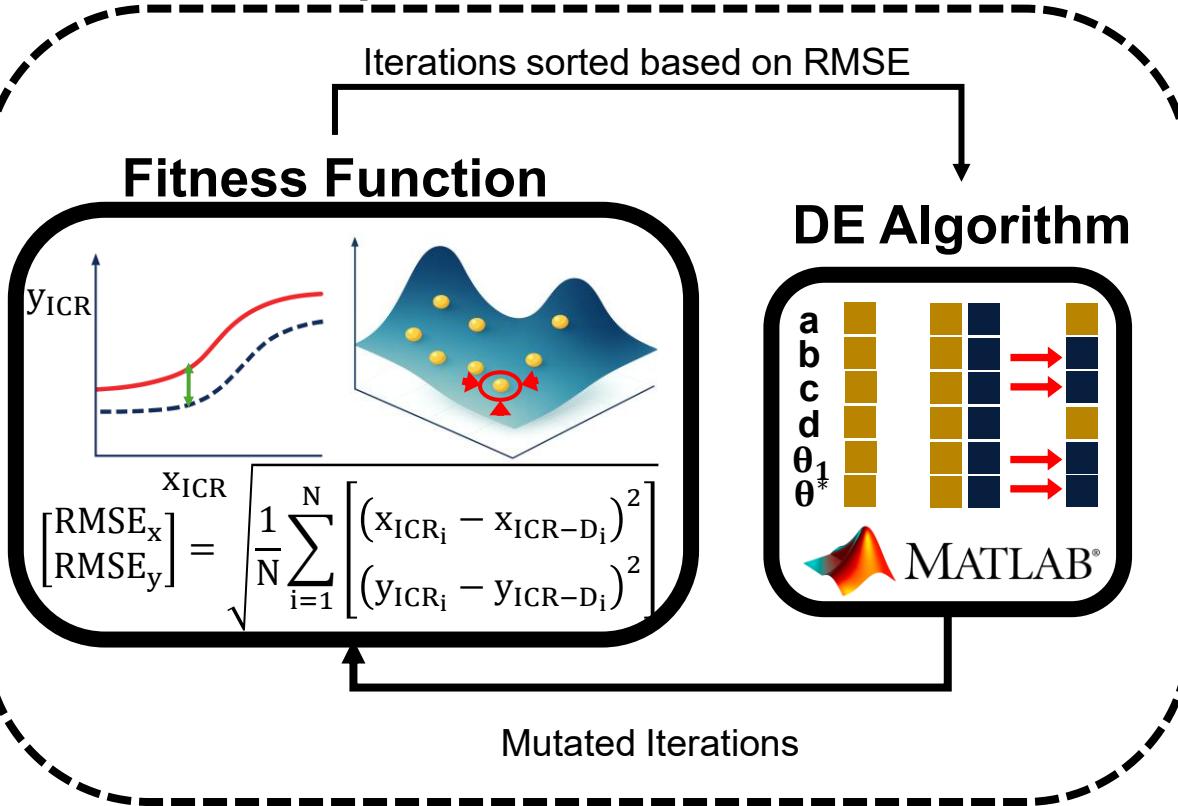
Figure 5: Hosmer Spectrum Knee ICR Trajectory

Kinematic Analysis

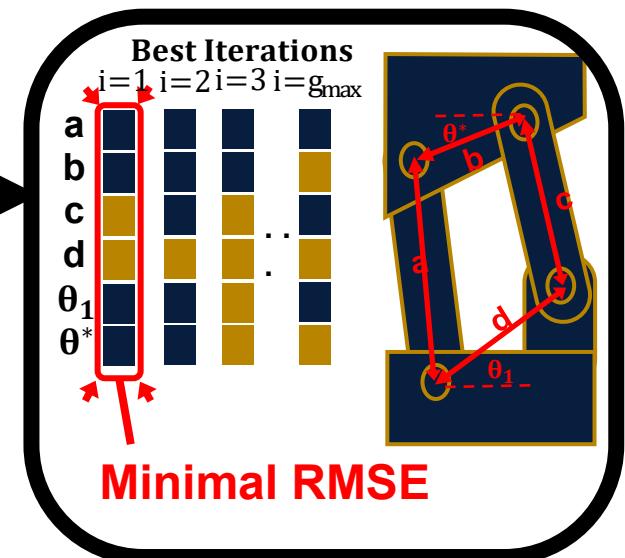
Desired ICR Trajectory
& Initial Dimensions



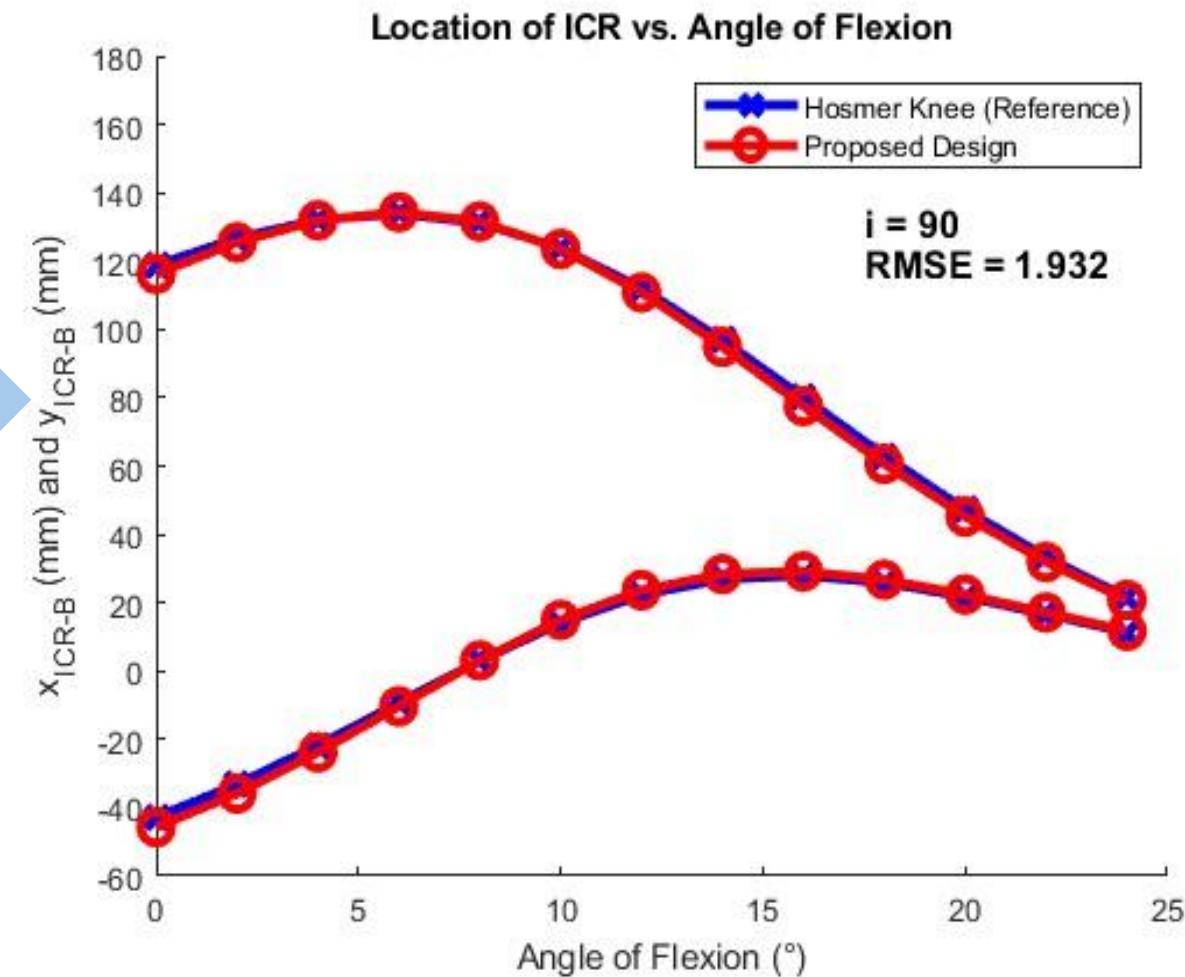
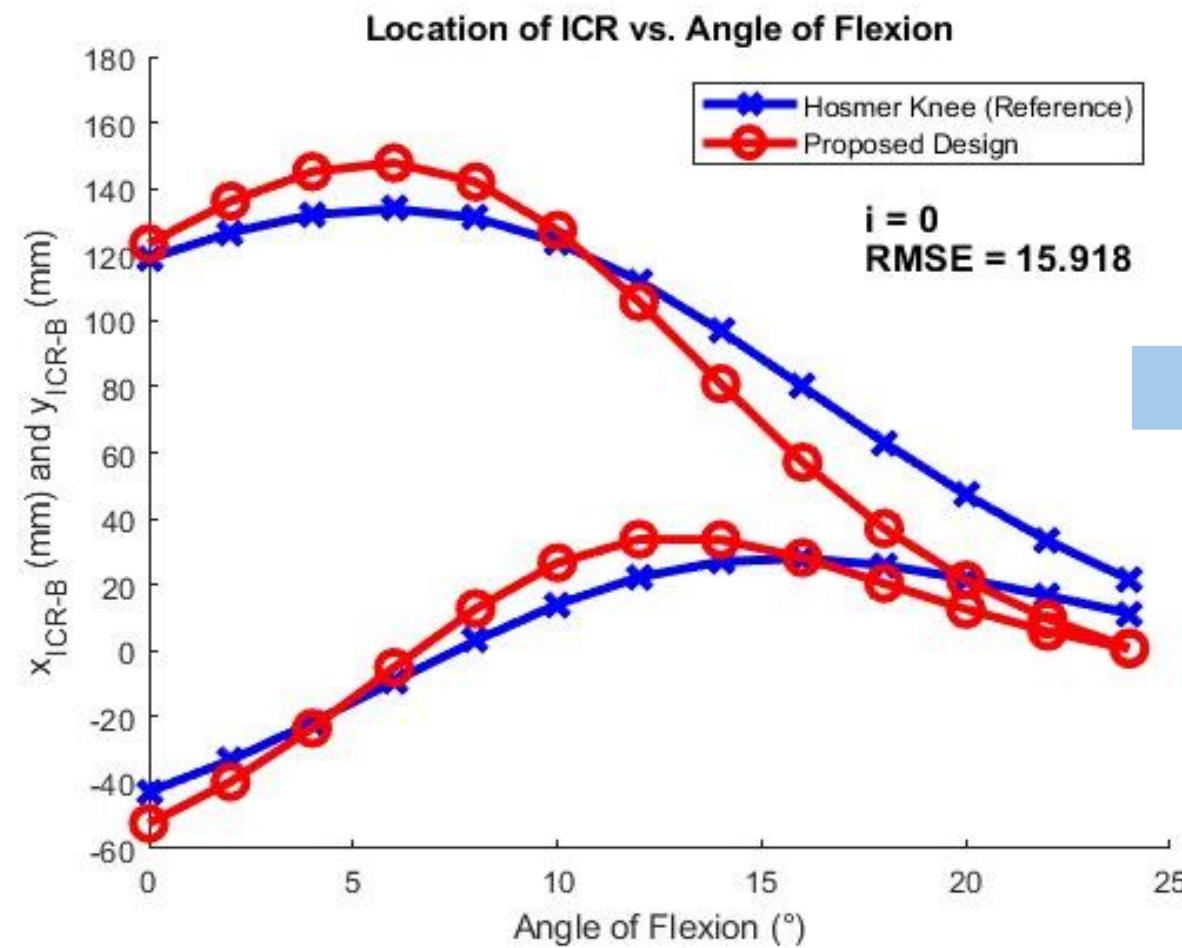
Optimization Process



Final Dimensions with
Minimum RMSE

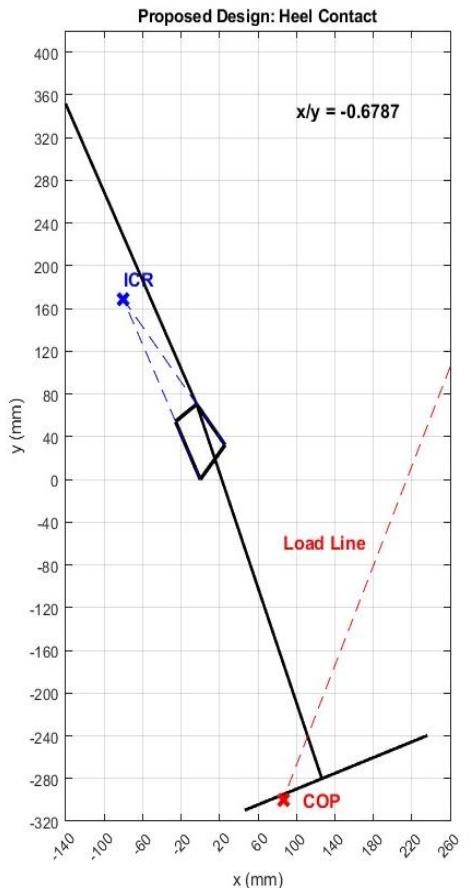
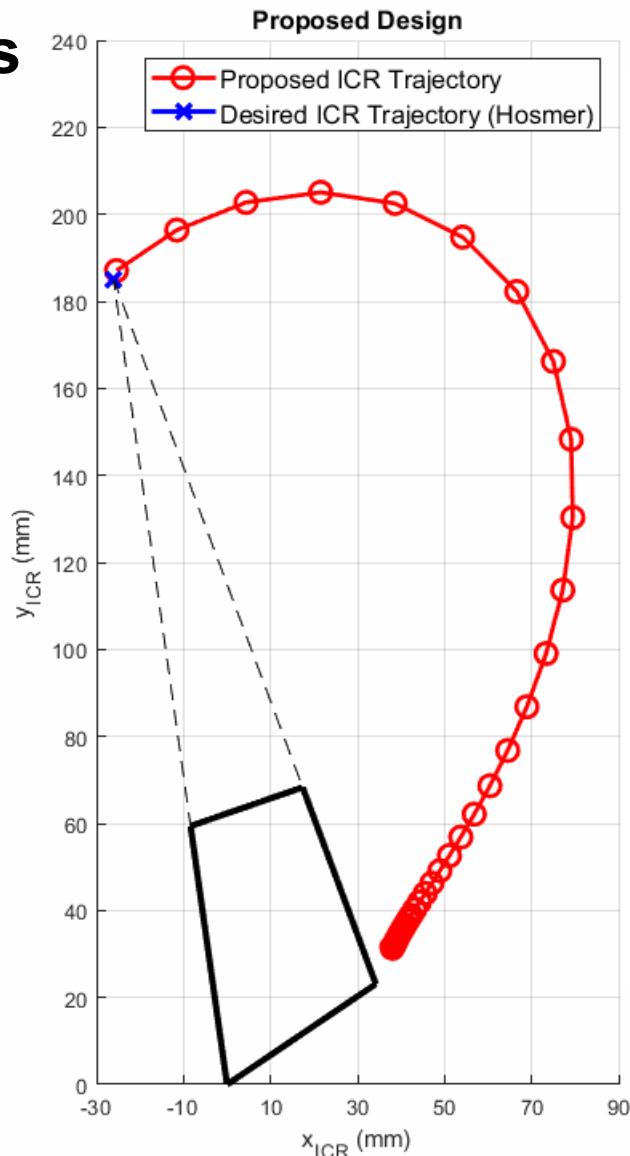
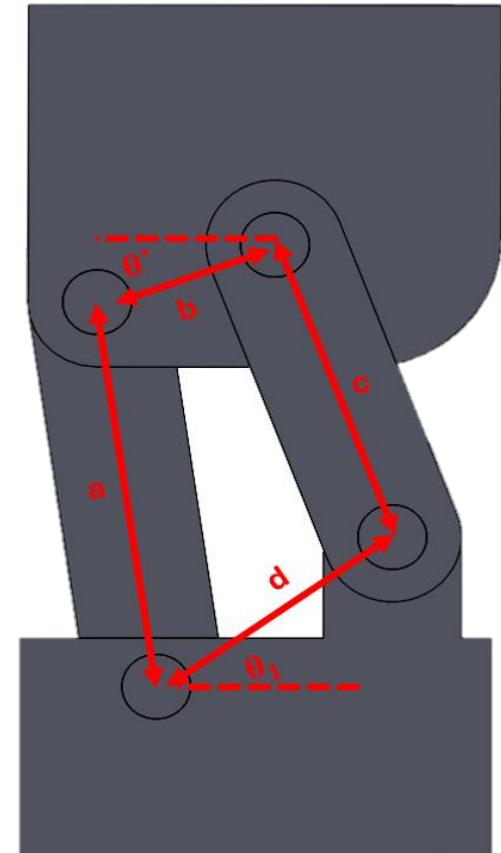


Kinematic Analysis

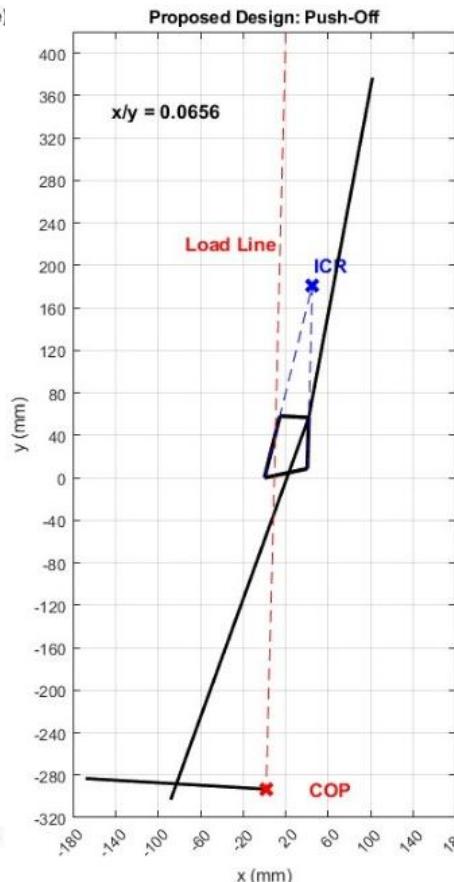
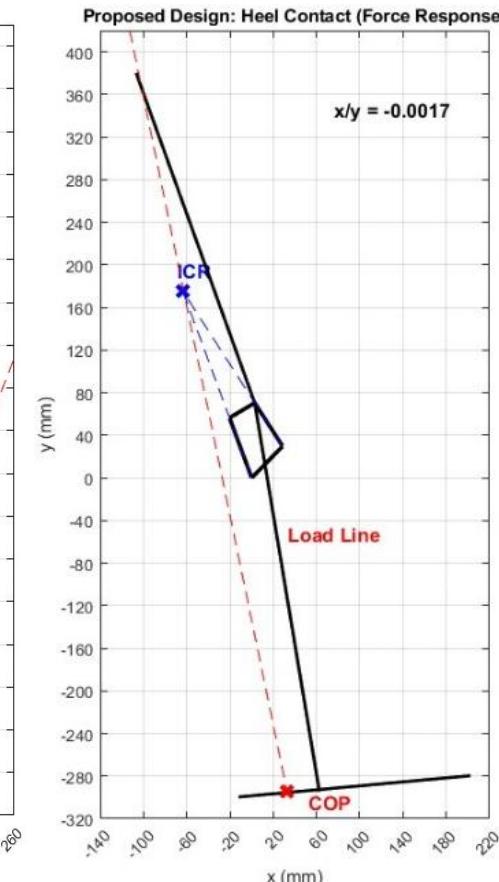


Kinematic Analysis

Final Dimensions



Stability Check



$$\begin{aligned} a &= 60.00 \text{ mm} \\ b &= 27.24 \text{ mm} \end{aligned}$$

$$\begin{aligned} c &= 48.24 \text{ mm} \\ d &= 41.26 \text{ mm} \end{aligned}$$

$$\begin{aligned} \theta_1 &= 34.04^\circ \\ \theta^* &= 19.06^\circ \end{aligned}$$

PLA Experiment

Young's Modulus & Yield Strength

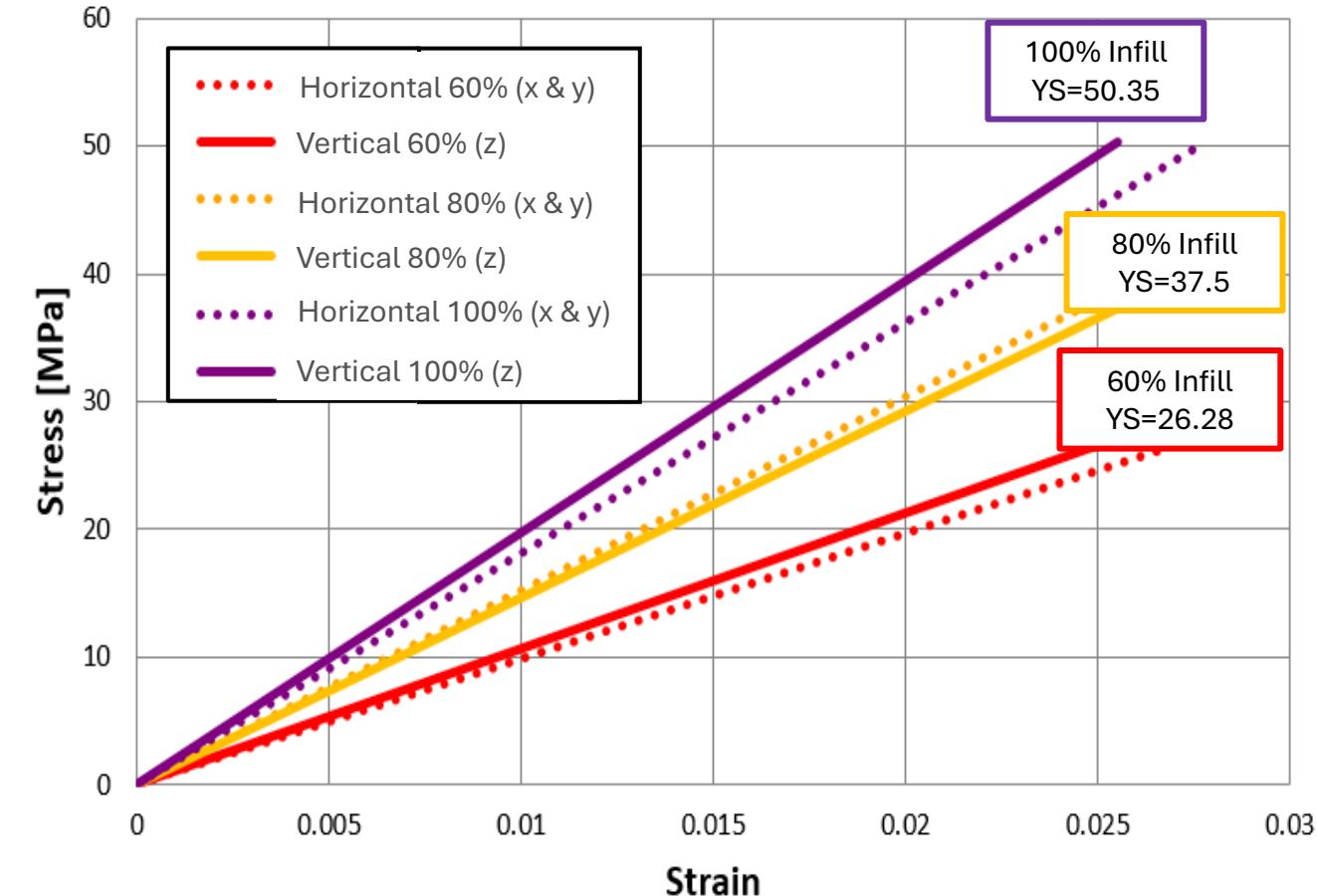


Figure 6: Mechanical Properties from PLA of Best Trials



Figure 7: MTS Criterion C43

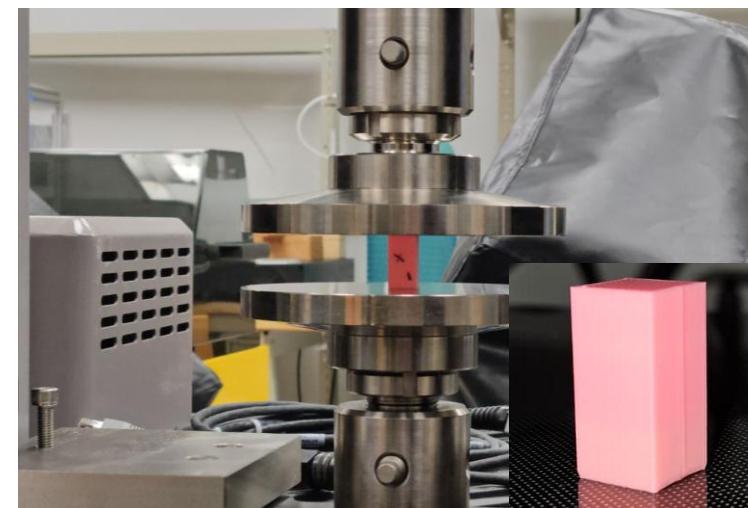
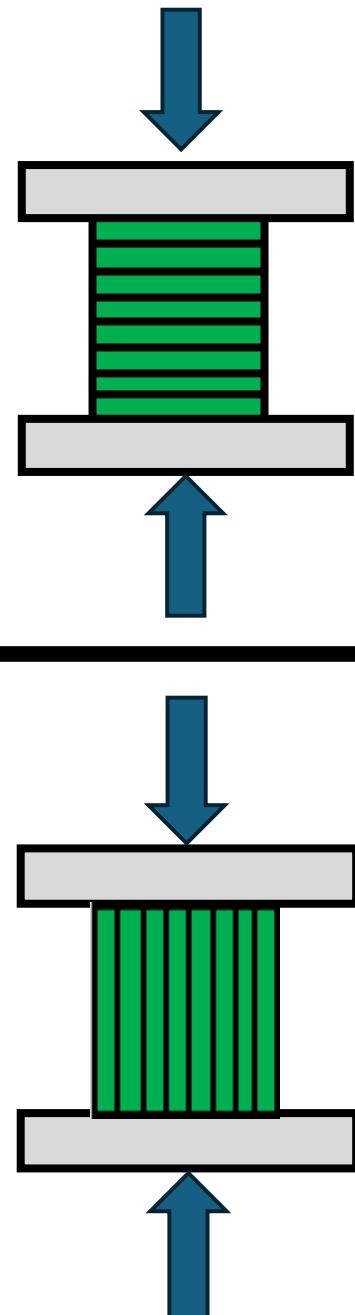


Figure 8: Compression on PLA



Standards Model

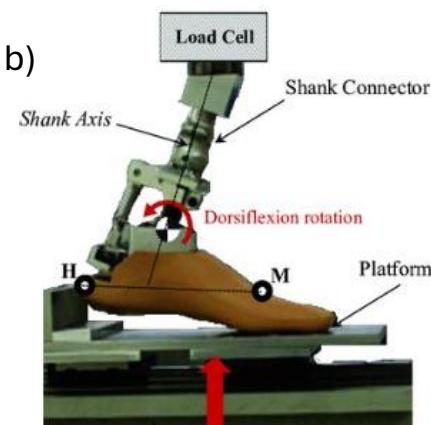
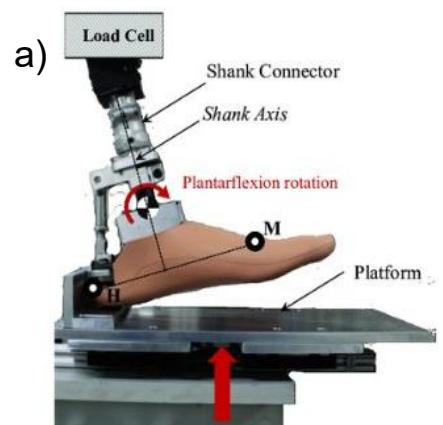
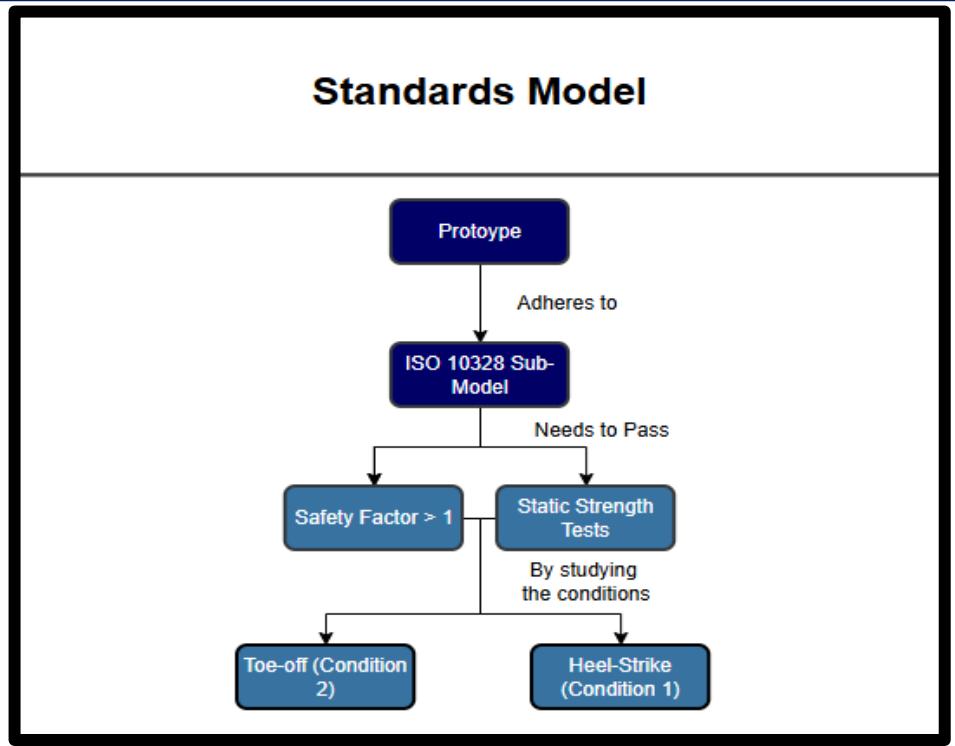


Figure 8: ISO 10328 a) Condition 1 and b) Condition 2

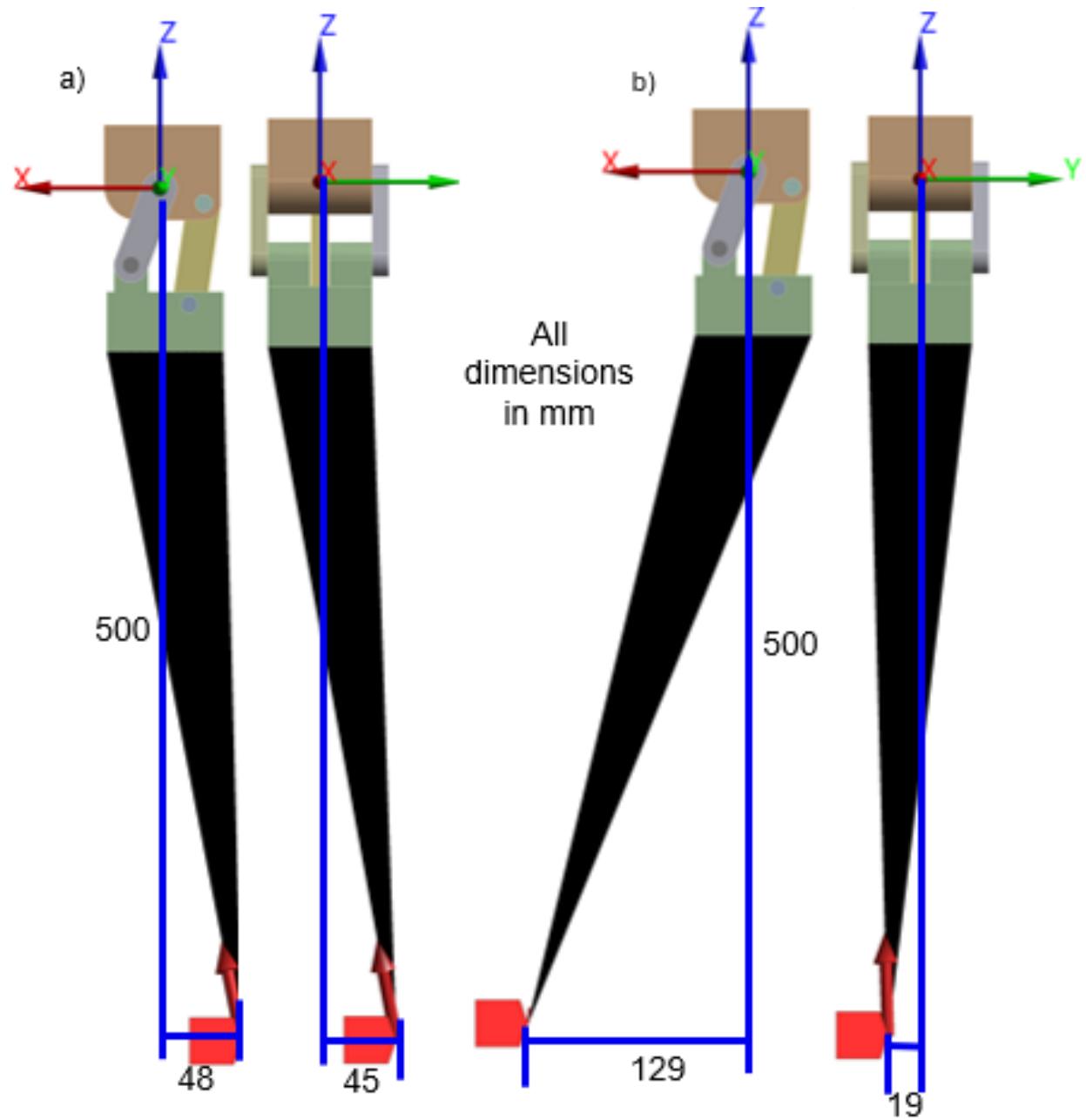
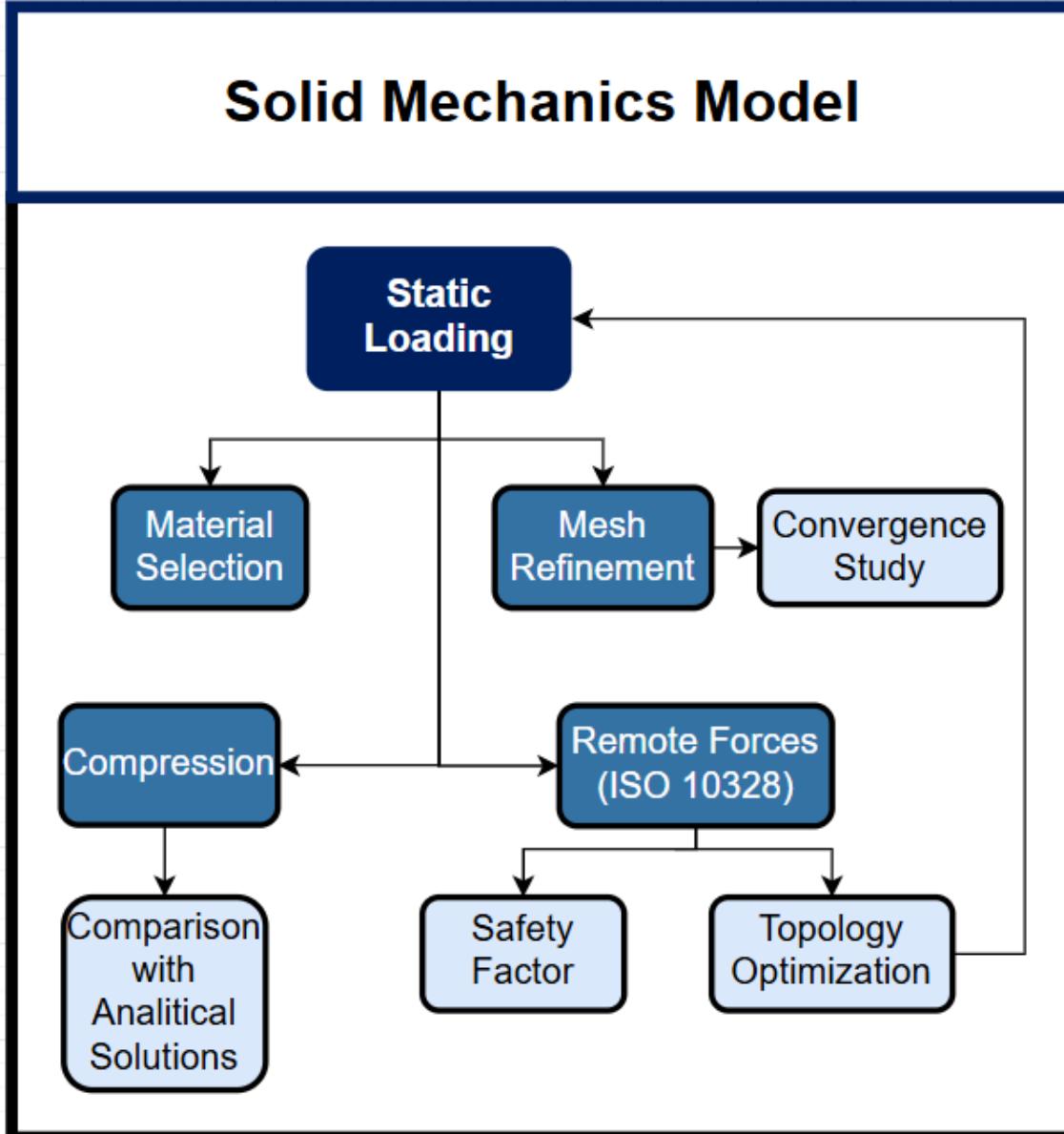


Figure 9: ISO 10328 Offsets. (a) Condition 1 & (b) Condition 2

Finite Element Analysis



| Property | PLA | 18-8 Stainless Steel |
|-----------------------|-------|----------------------|
| Young's Modulus [GPa] | 2.94 | 193 |
| Poisson's Ratio | 0.33 | 0.29 |
| Yield Strength [MPa] | 50.35 | 207 |

Mesh Settings:

- Mesh Method: Tetrahedral, Quadratic
- Final Mesh Size: 1.2 mm
- Pins axially Constrained

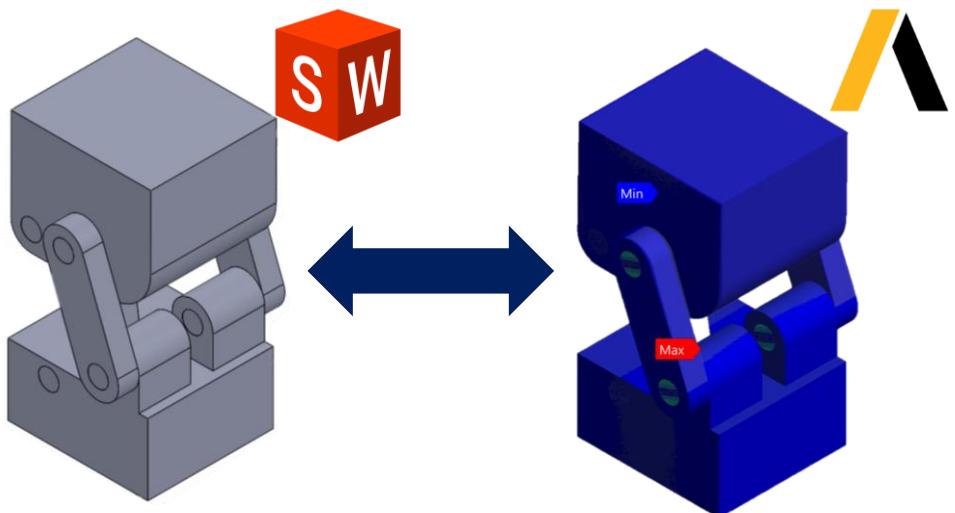
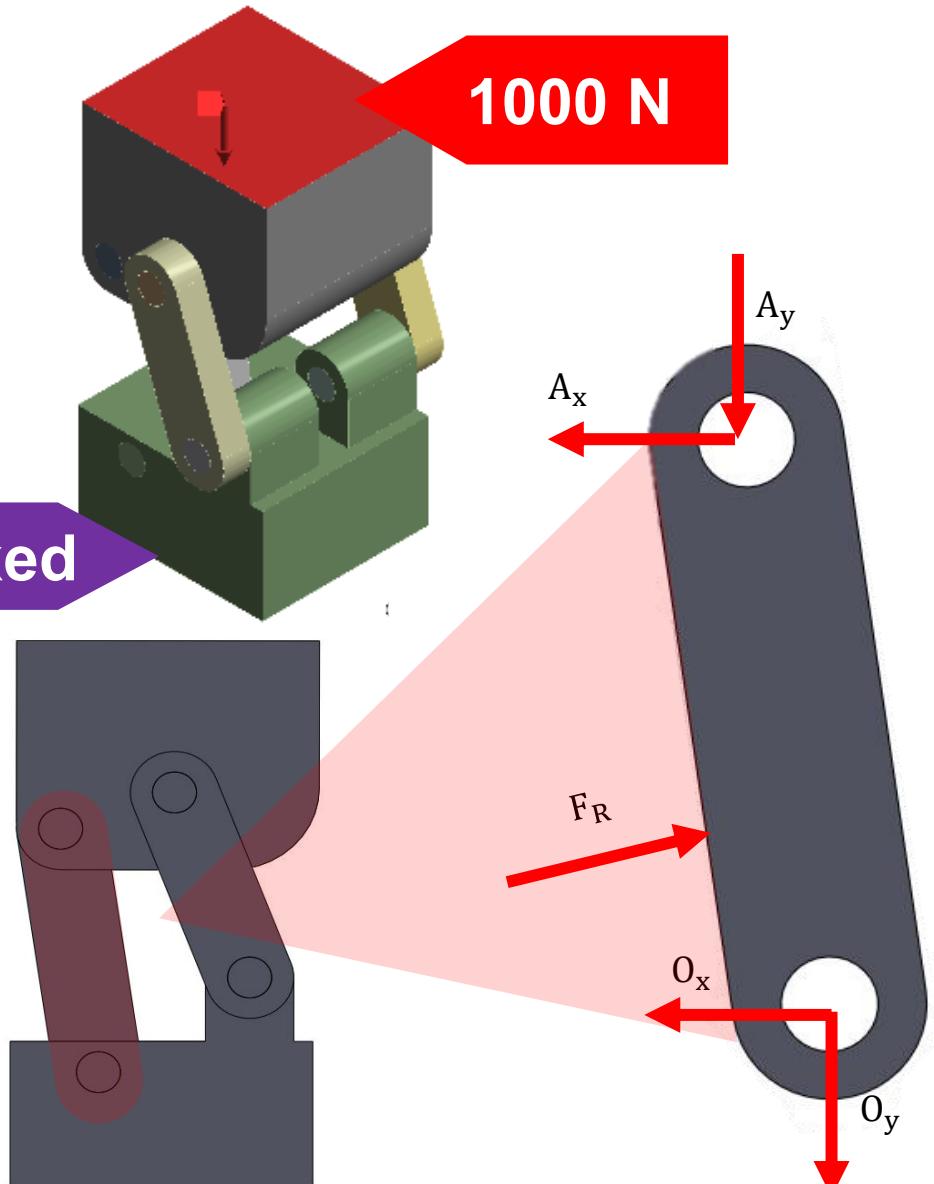


Figure 10: Preliminary Design

Compression



Central Bar Results:

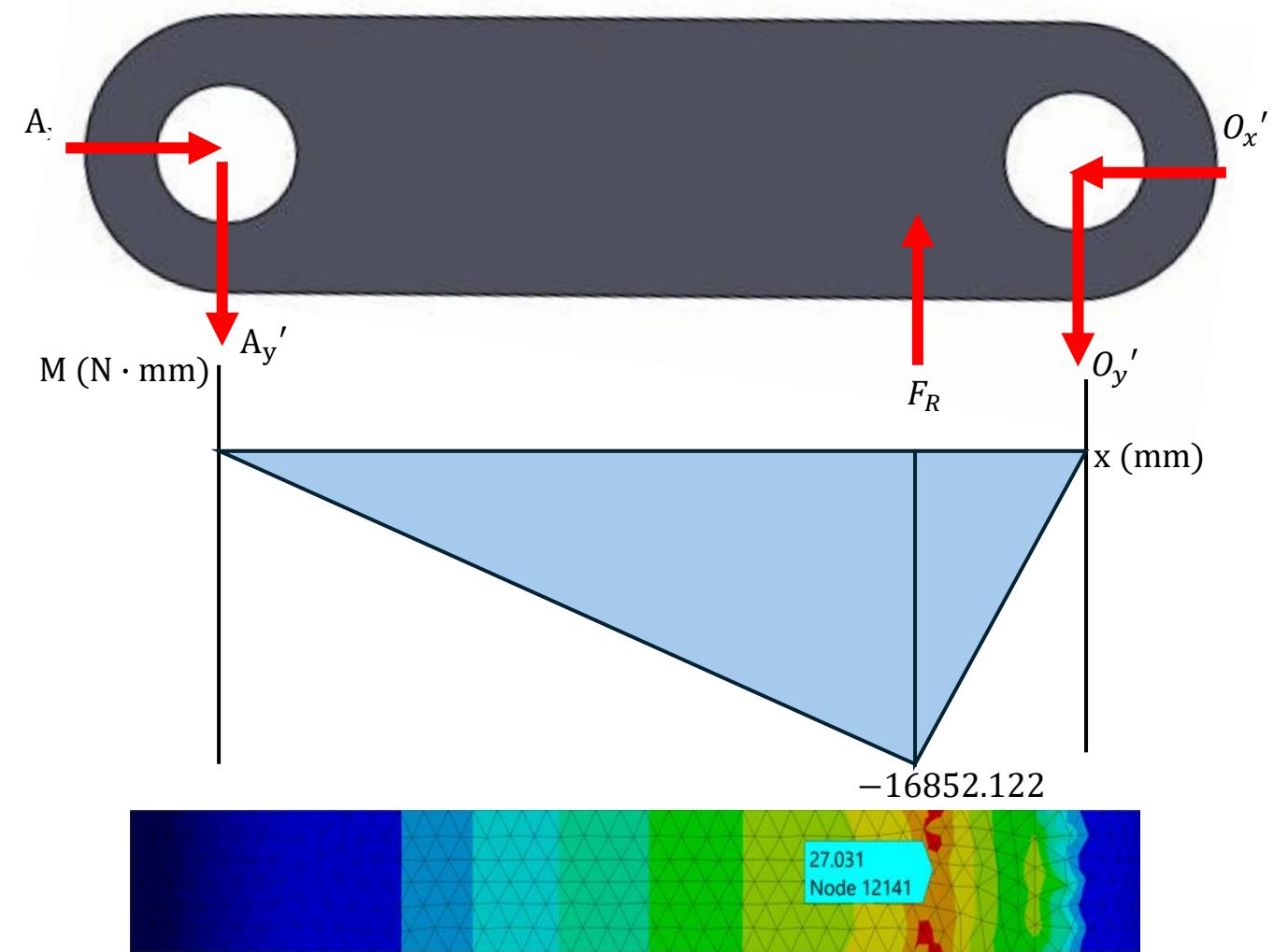
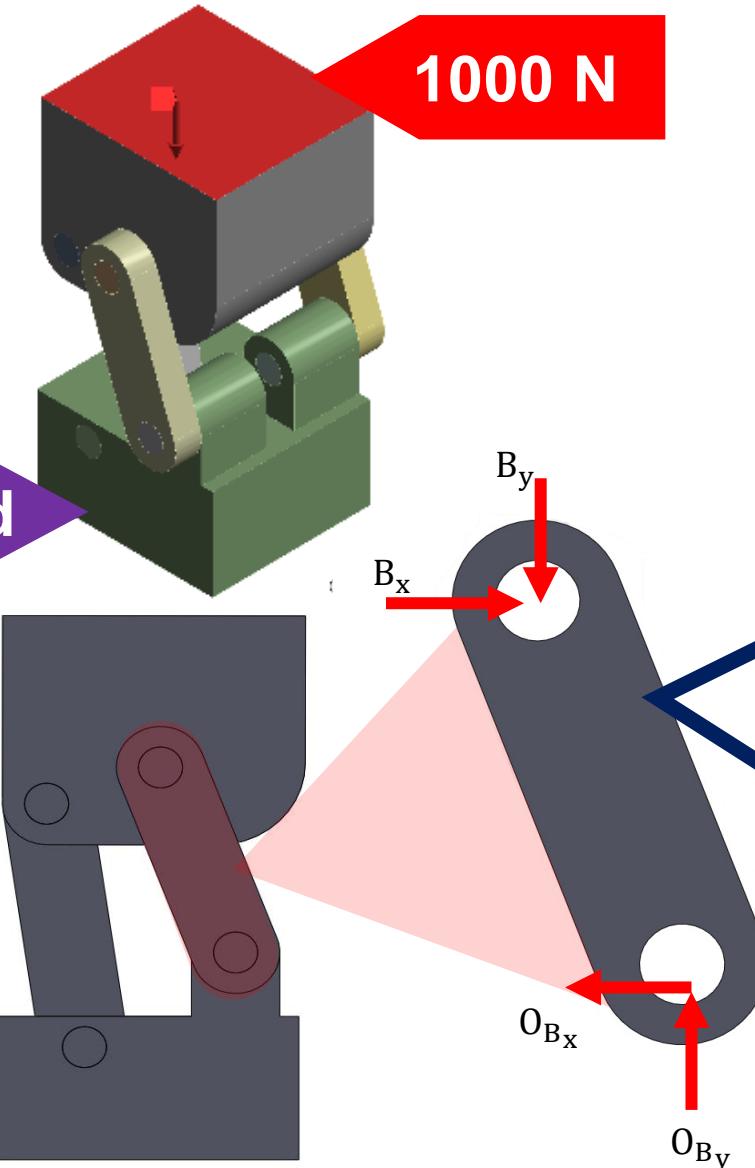


Figure 11: Moment Diagram from Central Bar

- Proper distribution of stresses in FEA simulation.
- Error of 6.97% on FEA when compared with analytical calculations.

Compression



Side Bars Results

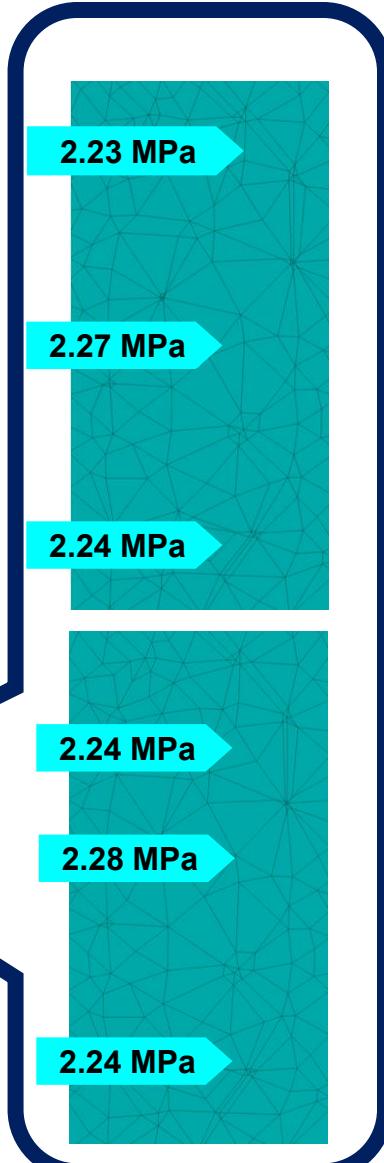


Figure 12: Stresses at Cross Sections from Side Bars

A: Static Structural
Equivalent Stress 6
Type: Equivalent (von-Mises) Stress
Unit: MPa
Time: 1 s
11/3/2025 11:32:21 AM

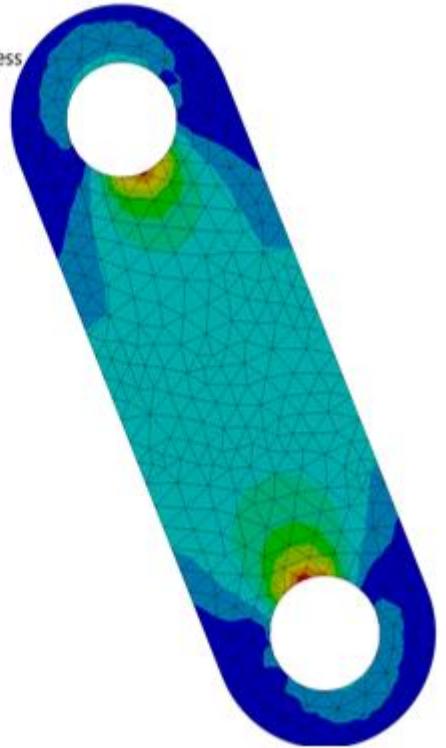
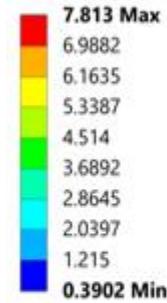


Figure 13: Stress Plot from Side Bar

- Proper distribution of stresses in FEA simulation: showing bearing stress and stress concentration.
- Error of 0.247% on FEA when compared with analytical calculations.

Oblique Forces



Required Design Modifications

Pins & holes:

High bearing stress; thicken bars or increase pin/hole size.

Central bar:

High bending/contact stress; increase width/thickness or raise stopper height.

Base:

Local stress at bar contact; reinforce contact region.

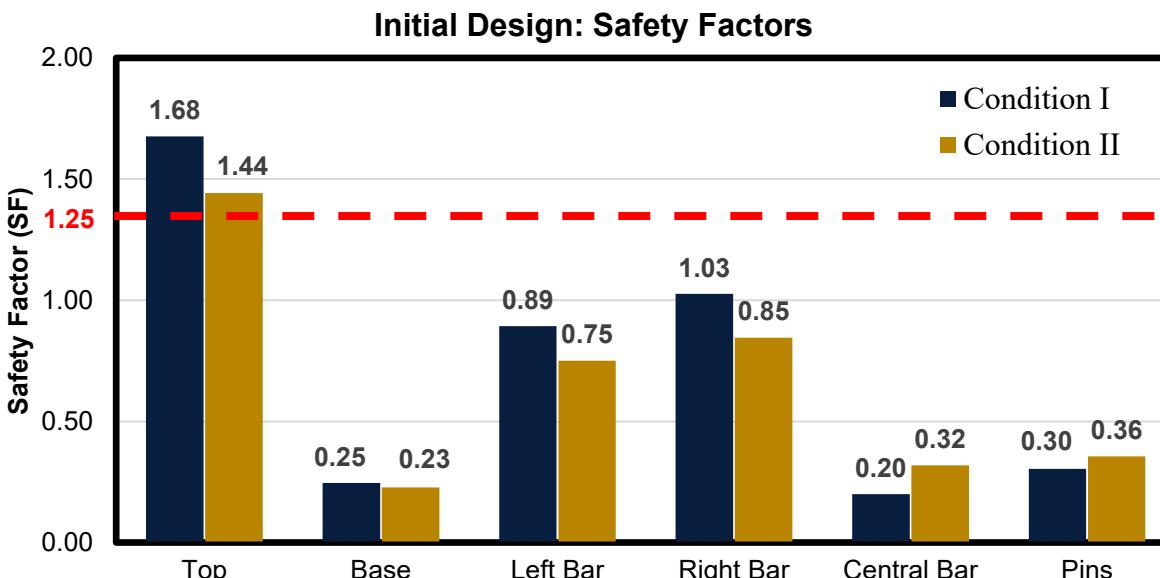


Figure 14: Safety Factors from Initial Design

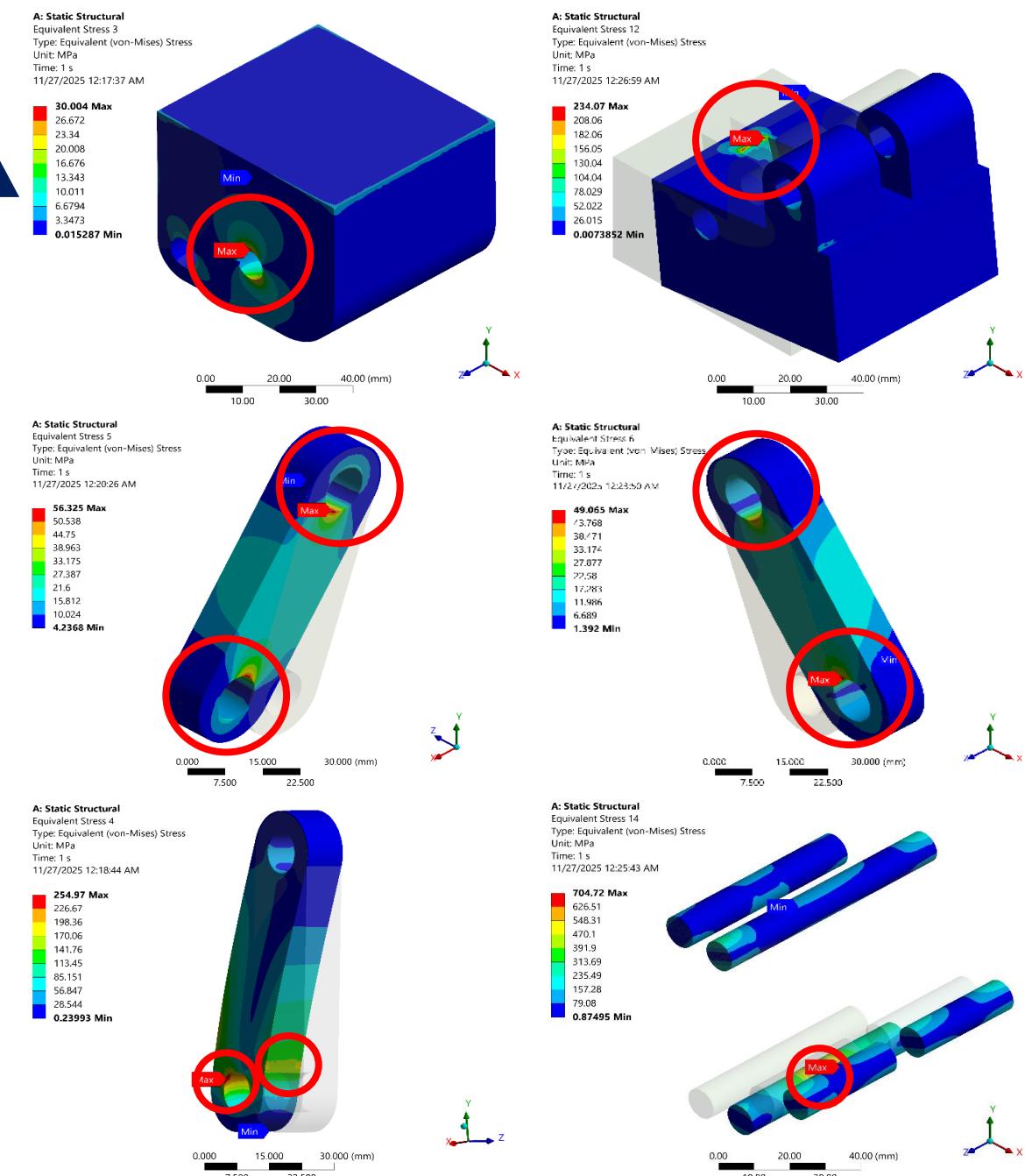


Figure 15: Stress Plots from each Individual Part (Condition 1)

Topology Optimization

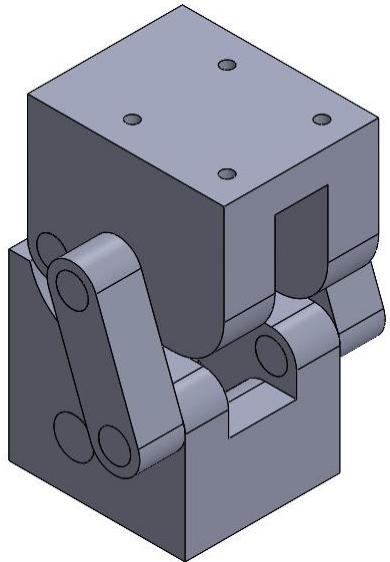


Figure 16: Design 2

✓ **Pins & holes:**

Pin diameters increased from 10 mm to 12.7 mm ($\frac{1}{2}$ in) and 15.875 mm ($\frac{5}{8}$ in).

✓ **Central bar:**

Increased thickness from... to

✓ **Base:**

Increased height of stopper from to

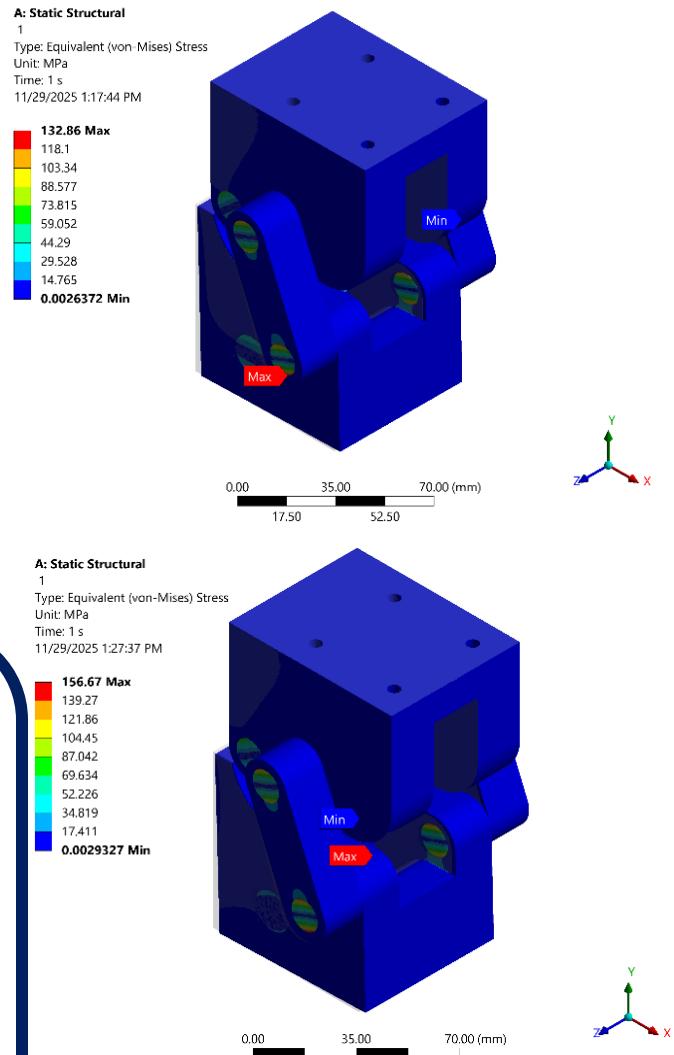


Figure 17: Stress Plots for Design 2.
a) Condition 1 & b) Condition 2

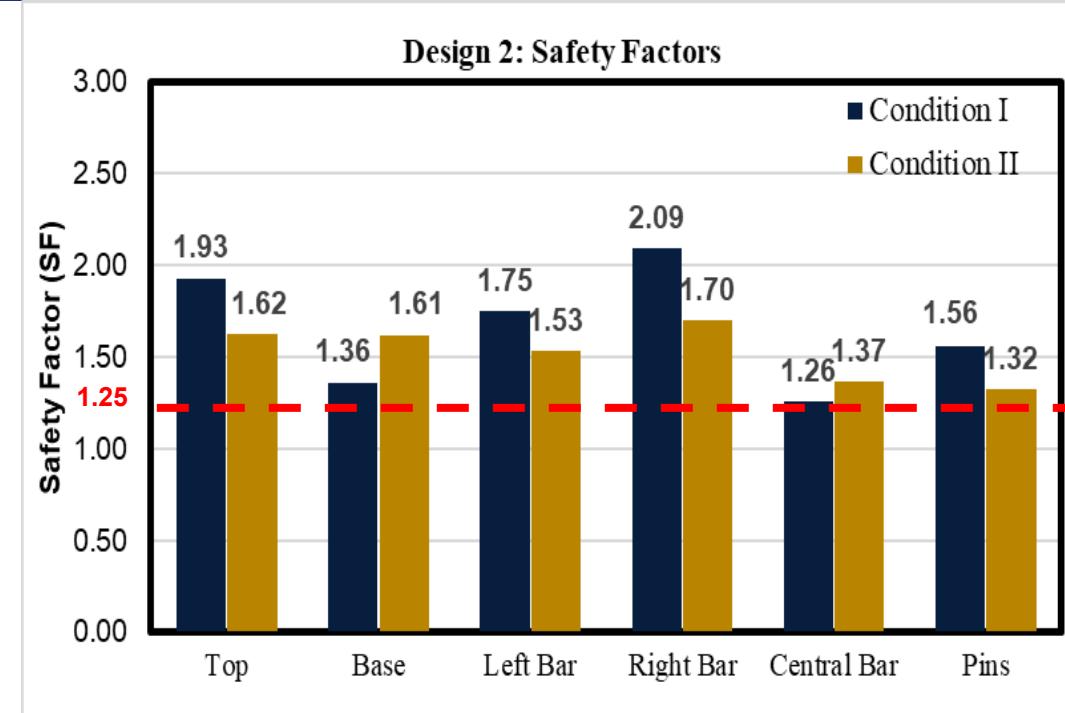


Figure 18: Safety Factors from Design 2

- ❑ Sections with safety factor exceeding 1.25, making possible the removal of material to satisfy:

Weight ≤ 80 kg

Topology Optimization

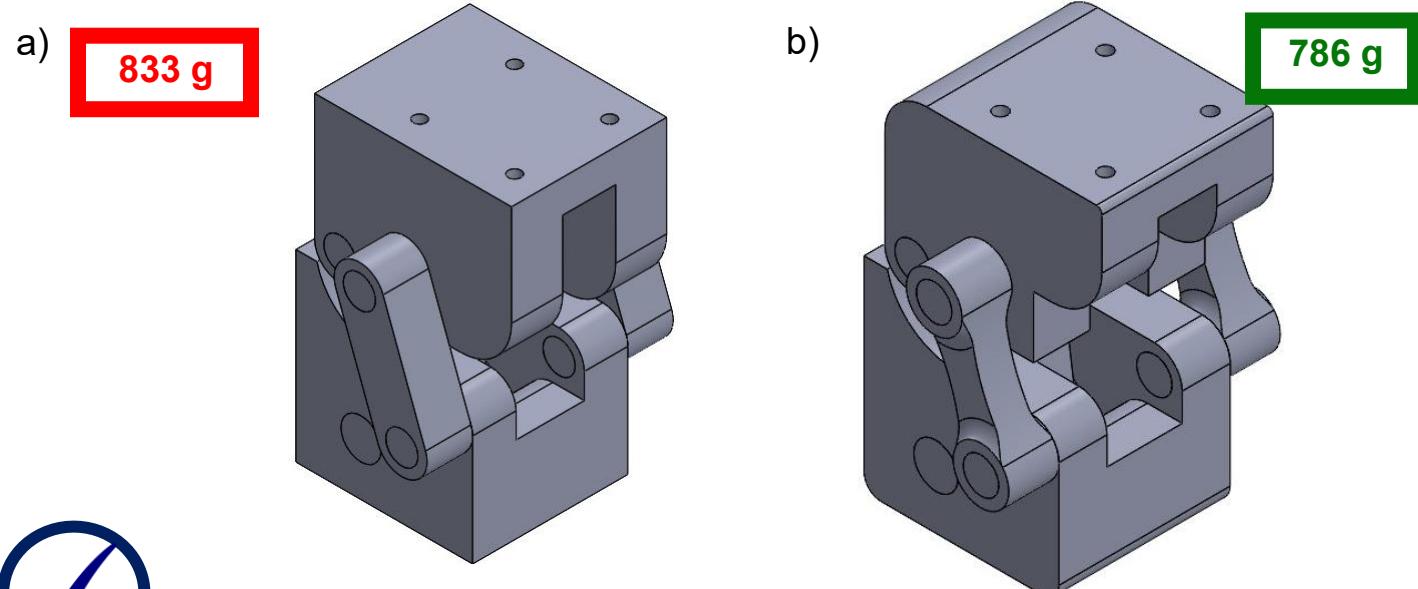


Figure 19: Comparison between a) Design 2 & b) Final Design

- ✓ Material removed through bottom, front, and rear fillet.
- ✓ Central and front top sections trimmed.
- ✓ Top pin divided and trimmed, lowering mass.
- ✓ Side bars with reduced width and thickness.

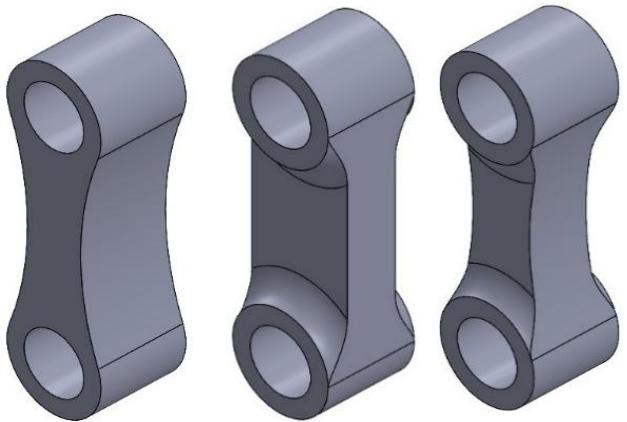


Figure 20: Side Bar Iterations

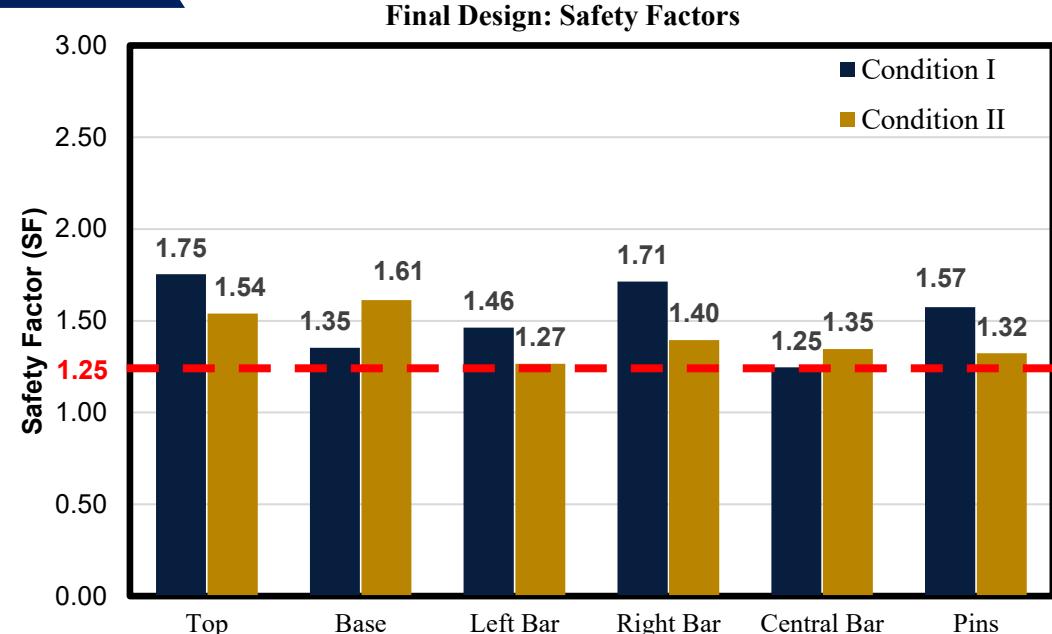


Figure 21: Safety Factors from Final Design

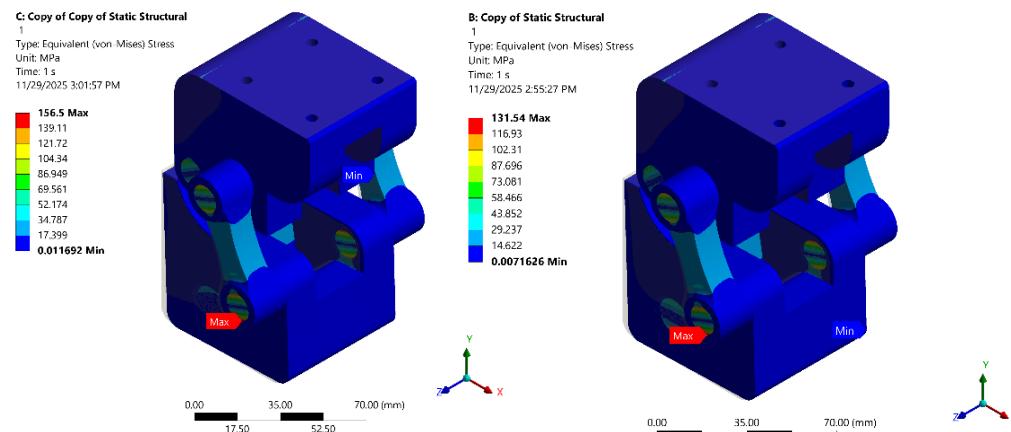
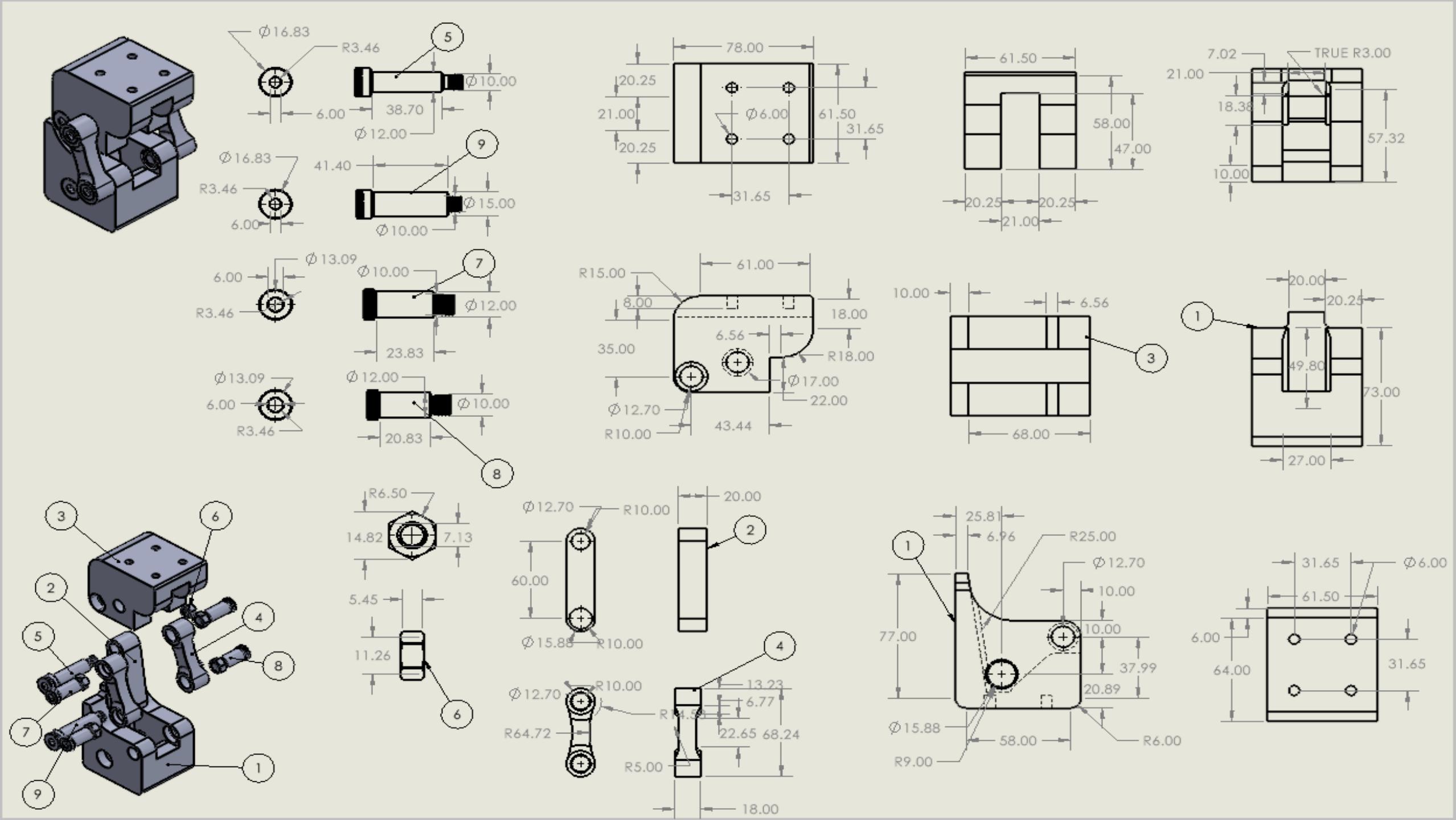


Figure 22: Stress Plots from Final Design



Manufacturing

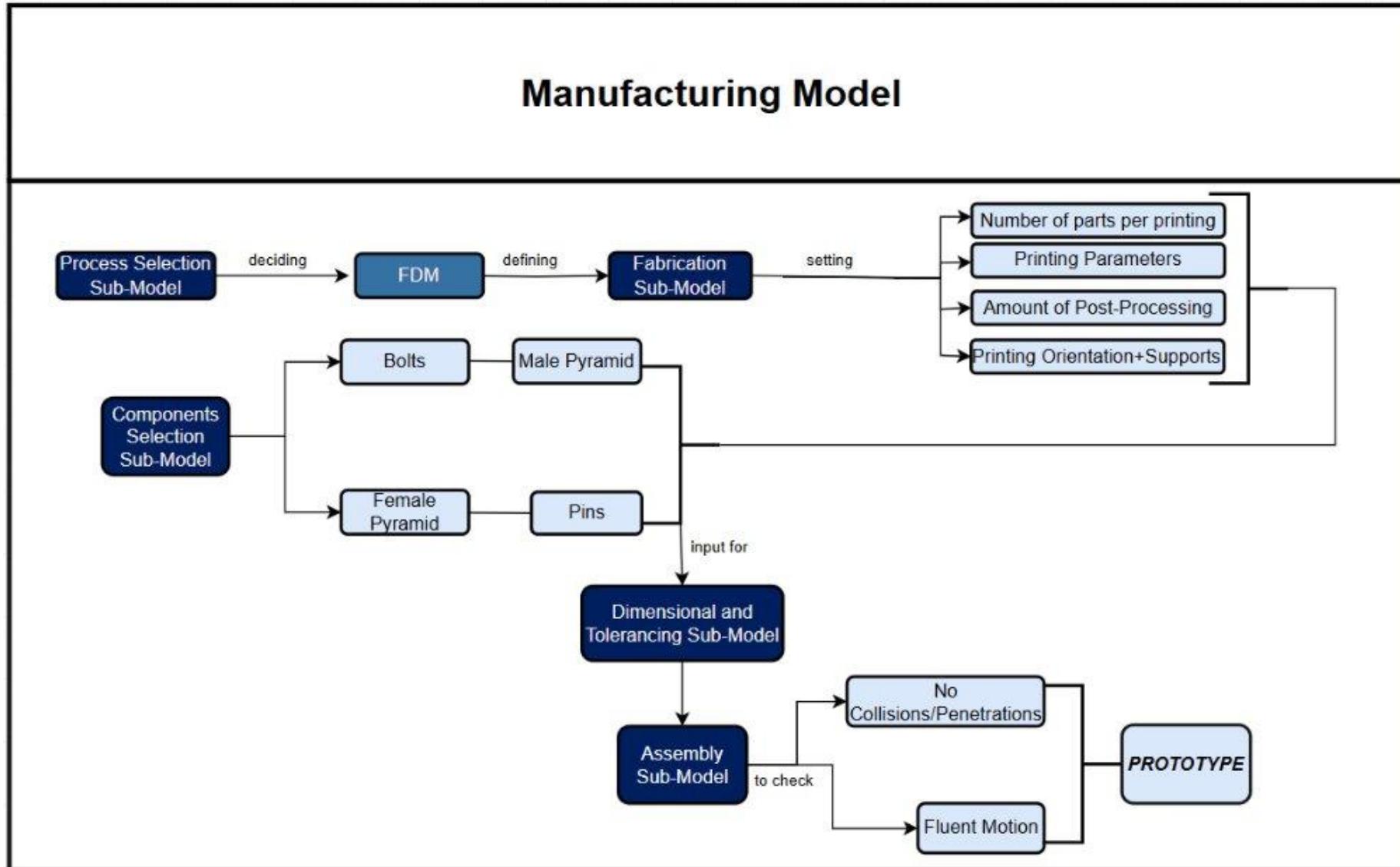


Figure 23: Prusa MK4



Figure 24: Prototype 1 Assembly

3D Printed Prototype



Figure 25: Side Bars and Central Bar



Figure 26: Top



Figure 27: Base

Assembly

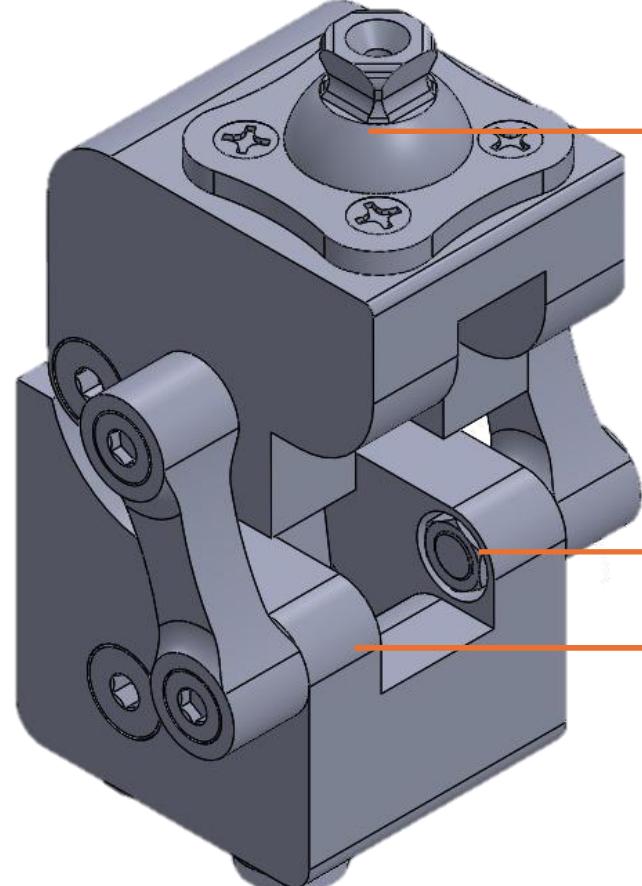


Figure 28: Isometric View of Final Design

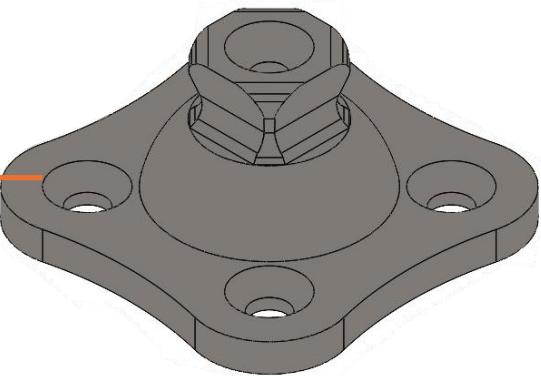


Figure 29: Pyramid Adapter

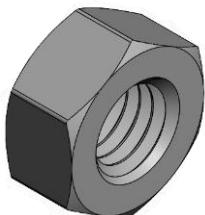


Figure 30: M8 Hex Nut



Figure 31: Shoulder Screw

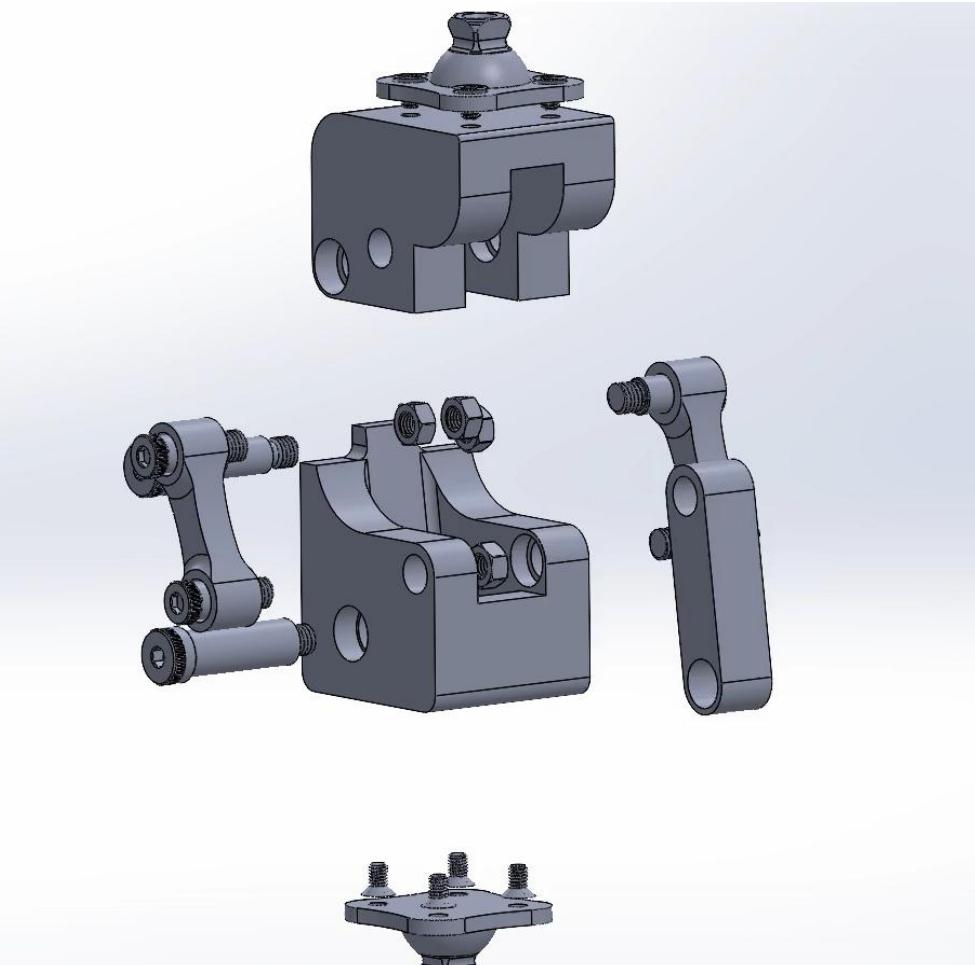


Figure 32: Assembly Process

Conclusions

Cost of \$98.09 with adapters



22.6% more expensive, but still acceptable if adapters are re-used

RMSE of 6.560 using DE



39% reduction compared with GA

Lowest Safety Factor of 1.2472



Meets ISO 10328 for heel contact & push-off

93.37° maximum flexion motion



Within 90°–100° sitting range

Joint weight equal to 786 g



12.2% lighter
(but +106 g more than Remotion)



THANK YOU.

Post-Processing

1

Epoxy Resin Coating:

- Coat parts with a layer of epoxy resin and let cure.
- Allows for a protective outer layer to form and increases the mechanical strength of the components.



2

Wet Sanding:

- Epoxy resin allows for the PLA to be primed for sanding by creating a thermal barrier.
- Wet sand with different grits used in progression, starting at 150 grit and finishing at 600 grit



3

UV Clear Top-Coat:

- Spray part with a UV-resistant acrylic clear coat to protect the epoxy surface from photodegradation,
- Prolonged UV exposure can cause epoxy resins to lose mechanical integrity over time

