1. Import & load libraries

```
In [ ]:
         %pip cache purge
         %pip install mne
         %pip install matplotlib
         %pip install numpy
         %pip install pandas
         %pip install scikit-learn
In [ ]:
         pip list
In [ ]:
         import mne
         from mne.datasets import eegbci
         from mne.io import read_raw_edf
         from mne.io import concatenate raws
         from mne.preprocessing import ICA
         import numpy as np
         import pandas as pd
         import matplotlib.pyplot as plt
         from io import BytesIO
         from PIL import Image
         import os
         import re
         import warnings
         import glob
         from sklearn.decomposition import PCA
         from sklearn.preprocessing import StandardScaler
         from typing import List
In [ ]:
         warnings.filterwarnings("ignore", message="FigureCanvasAgg is non-interactive, and
         warnings.filterwarnings("ignore", category=RuntimeWarning, message="Channel locati
```

2. Info

Experimental Protocol

This data set consists of over 1500 one- and two-minute EEG recordings, obtained from **109 volunteers**, as described below.

Subjects performed different motor/imagery tasks while 64-channel EEG were recorded using the BCI2000 system (http://www.bci2000.org). Each subject performed *14 experimental runs*: two one-minute baseline runs (one with eyes open, one with eyes closed), and three two-minute runs of each of the four following tasks:

- TASK 1: A target appears on either the left or the right side of the screen. The subject opens and closes the corresponding fist until the target disappears. Then the subject relaxes.
- **TASK 2**: A target appears on either the left or the right side of the screen. The subject imagines opening and closing the corresponding fist until the target disappears. Then the subject relaxes.
- **TASK 3**: A target appears on either the top or the bottom of the screen. The subject opens and closes either both fists (if the target is on top) or both feet (if the target is on the bottom) until the target disappears. Then the subject relaxes.
- **TASK 4**: A target appears on either the top or the bottom of the screen. The subject imagines opening and closing either both fists (if the target is on top) or both feet (if the target is on the bottom) until the target disappears. Then the subject relaxes.

Description of data:

The experimental runs were:

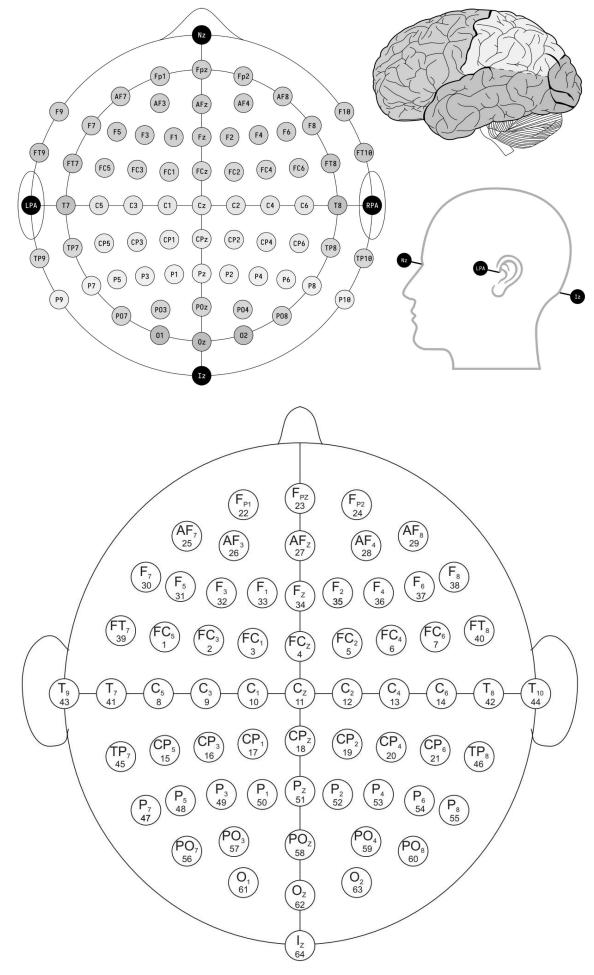
- Baseline, eyes open
- Baseline, eyes closed
- Task 1 (open and close left or right fist)
- Task 2 (imagine opening and closing left or right fist)
- Task 3 (open and close both fists or both feet)
- Task 4 (imagine opening and closing both fists or both feet)

Each annotation includes one of three codes (T0, T1, or T2):

- **T0** corresponds to rest
- **T1** corresponds to onset of motion (real or imagined) of the left fist (in runs 3, 4, 7, 8, 11, and 12) both fists (in runs 5, 6, 9, 10, 13, and 14)
- **T2** corresponds to onset of motion (real or imagined) of the right fist (in runs 3, 4, 7, 8, 11, and 12) both feet (in runs 5, 6, 9, 10, 13, and 14)

Run	Task
1	Baseline, eyes open
2	Baseline, eyes closed
3, 7, 11	Motor execution: left vs right hand
4, 8, 12	Motor imagery: left vs right hand
5, 9, 13	Motor execution: hands vs feet
6, 10, 14	Motor imagery: hands vs feet

The EEGs were recorded from 64 electrodes as per the international system (excluding electrodes Nz, F9, F10, FT9, FT10, A1, A2, TP9, TP10, P9, and P10)



3. Load data

```
In [ ]:
         def load_data(subjects, runs, data_dir=".../data/files/"):
             Load and preprocess EEG data for given subjects and runs.
             all raws = []
             for subject in subjects:
                 print(f"\n=== Loading data from volunteer {subject} ===")
                 try:
                     # Download data to the specified directory
                     raw fnames = mne.datasets.eegbci.load data(subject, runs, path=data di
                     raws = [mne.io.read raw edf(f, preload=True, verbose=True) for f in ra
                     raw = mne.concatenate raws(raws)
                 except Exception as e:
                     warnings.warn(f"Skipping subject {subject} due to an error: {e}")
                     continue
                 # Set standard montage
                     raw.set montage("standard 1005", on missing="ignore")
                 except Exception as e:
                     warnings.warn(f"Could not set montage for subject {subject}: {e}")
                 # Extract events from annotations
                 try:
                     events, _ = mne.events_from_annotations(raw)
                     new_annot = mne.annotations_from_events(
                         events=events,
                         event desc=new labels events,
                         sfreq=raw.info['sfreq'],
                         orig time=raw.info['meas date']
                     raw.set_annotations(new_annot)
                 except Exception as e:
                     warnings.warn(f"Could not update event labels for subject {subject}: {
                 all raws.append(raw)
             if not all raws:
                 raise ValueError("No valid EEG data loaded. Check subject and run IDs.")
             # Concatenate all subjects' data
             return mne.concatenate_raws(all_raws)
In [ ]:
         subjects = [1] # subjects to load (from 1 to 109 volunteers)
         runs = [3] # experimental runs for each subject
         # runs = [1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12, 13, 14]
         raw_data = load_data(subjects, runs)
In [ ]:
         print(raw data)
In [ ]:
         def summarize edf files(data dir="../data/files/"):
             Recursively summarize the contents of all .edf files in the given directory.
             edf files = glob.glob(os.path.join(data dir, "**/*.edf"), recursive=True)
```

if not edf_files:

```
return
             print(f"Found {len(edf files)} EDF files in {data dir}**:\n")
             for edf file in edf files:
                 try:
                     raw = mne.io.read_raw_edf(edf_file, preload=False, verbose=False)
                     info = raw.info
                     rel path = os.path.relpath(edf file, data dir) # Get relative path fo
                     print(f"File: {rel path}")
                     print(f" - Channels: {len(info['ch names'])}")
                     print(f" - Length: {len(raw)}")
                     print(f" - Sampling Frequency: {info['sfreq']} Hz")
                     print("-" * 40)
                 except Exception as e:
                     print(f"Error reading {edf file}: {e}")
         # Run the function
         summarize_edf_files()
In [ ]:
         print(raw_data)
         print(raw data.info)
         print(raw data.annotations)
         print(raw data.annotations.description)
         print(raw data.annotations.onset)
         print(raw_data.info['ch_names'])
In [ ]:
         eegbci.standardize(raw data) # Standardize channel names
         print(raw data.info)
```

print("No EDF files found in the directory or subdirectories.")

```
print(raw_data.info['ch_names'])
```

```
In [ ]:
         montage = mne.channels.make standard montage('standard 1005')
         raw_data.set_montage(montage)
```

4. Show events

```
In [ ]:
         # Show the events
         events, event id = mne.events from annotations(raw data)
         print(event id)
         print(events)
```

```
In [ ]:
    event_id = {
        'rest' if k == np.str_('T0') else
        'hands' if k == np.str_('T1') else
        'feets': v
        for k, v in event_id.items()
    }
    print(event_id)
    print(events)
```

5. Select EEG channels

```
In []: # Select only EEG channels for further analysis
    picks = mne.pick_types(raw_data.info, meg=True, eeg=True, stim=False, eog=False, e
    print(picks.shape)
    print(picks)
In []: raw_data.plot(picks=picks);
```

6. Show PSD Power Spectral Density

The Power Spectral Density (PSD) is a way to analyze the frequency content of a signal. It tells us how the power of a signal is distributed across different frequencies.

The PSD describes how the power (or variance) of a signal is distributed over different frequency components.

It is computed using the Fourier Transform, which decomposes a time-domain signal into its frequency components.

7. Apply ICA Independent Component Analysis

ICA (Independent Component Analysis) is a technique used to separate mixed signals into independent components. In EEG/MEG analysis, it is mainly used to remove artifacts such as eye blinks, eye movements, and muscle noise.

ICA decomposes a signal into a set of statistically independent components, allowing us to identify and remove noise sources without affecting neural signals.

ICA is useful for:

```
    Removing eye blink artifacts (blinks)
```

- Removing eye movement and muscle artifacts
- Separating neural activity from external noise

```
In [ ]:
         # Configure ICA with 25 components
         raw_data_ica = raw_data.copy()
         raw data ica filtered = raw data ica.filter(1, 70, picks=picks)
         ica = ICA(n_components=25, random_state=42, method='fastica', max_iter=800)
         # Fit ICA to the data
         ica.fit(raw data ica filtered, picks=picks)
         # Plot ICA components
         ica.plot sources(raw data ica filtered, picks=range(0, 25))
         plt.show()
In [ ]:
         ica.apply(raw data ica filtered)
In [ ]:
         raw data ica_filtered.plot(picks=picks);
In [ ]:
         # Function to convert MNE plot to an image
         def raw plot to image(raw data, picks):
             buf = BvtesIO()
             fig = raw_data.plot(picks=picks, show=False)
             fig.savefig(buf, format='png', bbox_inches='tight', dpi=150) # Reduce empty s
             plt.close(fig)
             buf.seek(0)
             return np.array(Image.open(buf))
         # Create figure with tight layout
         fig, axes = plt.subplots(1, 2, figsize=(14, 6))
         fig.suptitle('Raw Data BEFORE ICA vs. AFTER ICA', fontsize=16, fontweight='bold')
         # PLot BEFORE ICA
         img_before = raw_plot_to_image(raw_data, picks)
         axes[0].imshow(img_before)
         axes[0].set_title('raw_data BEFORE ICA', fontsize=12)
         axes[0].axis('off') # Hide axes completely
         axes[0].spines[:].set_visible(False) # Hide borders
         # PLot AFTER ICA
         img after = raw plot to image(raw data ica filtered, picks)
         axes[1].imshow(img after)
         axes[1].set_title('raw_data AFTER ICA', fontsize=12)
         axes[1].axis('off') # Hide axes completely
         axes[1].spines[:].set_visible(False)
         # Use tight_layout to optimize spacing
         plt.tight layout(pad=0.1, w pad=0.1, h pad=0.1) # Reduce the space between subplo
         plt.show()
In [ ]:
         psd ica raw = raw data ica filtered.compute psd(picks=picks, fmax=80)
         psd ica raw.plot();
```

8. Notch filter

A Notch Filter (also called a Band-stop filter) is used to remove specific unwanted frequencies from a signal, particularly when a narrow frequency band causes interference or noise. In signal processing, the "notch" refers to the removal of frequencies within a small range, leaving the other frequencies untouched.

How It Works:

- Passband and Stopband:
 - The passband is the range of frequencies that the filter allows to pass through without attenuation.
 - The stopband is the range of frequencies that the filter suppresses.
 - A notch filter specifically targets and reduces a narrow band of frequencies (the notch), while passing frequencies outside of that band.
- Frequency Range:
 - The notch filter is designed to attenuate a specific frequency (or a small range of frequencies) while allowing the other frequencies to pass through. This is particularly useful when dealing with known interference frequencies, such as the power line frequency (50 Hz or 60 Hz) that can appear in many electrical signals.

Applications of Notch Filters:

- Power line interference: In electrical signals, the 50 Hz or 60 Hz power line frequency is a common source of noise. The notch filter is used to remove this frequency without affecting the rest of the signal.
- Electroencephalography (EEG): In EEG data, notch filters are commonly applied to remove noise caused by electrical equipment, such as power line interference.
- Audio processing: It can also be used to remove hum or buzz noises caused by equipment, such as electrical hum from a microphone or speakers.
- Communication systems: To filter out specific unwanted frequencies or interference.

```
In []: # # Notch filter
# notch_freq = 60
# raw_data.notch_filter(notch_freq, fir_design='firwin')
# raw_data.compute_psd().plot()

In []: # # Band-pass filter keep only alpha and beta waves
# low_cutoff = 8
# high_cutoff = 30
# raw_data.filter(low_cutoff, high_cutoff, fir_design='firwin')
# raw_data.compute_psd().plot()

In []: # raw_data.compute_psd().plot()
# raw_data.compute_psd().plot(average=True)
```

```
In [ ]:
         raw_filtered.plot_psd(average=False)
         plt.show()
In [ ]:
         data = raw filtered.copy().get data()
         # Standardization
         scaler = StandardScaler()
         data standardized = scaler.fit_transform(data.T).T
In [ ]:
         # Covariance Matrix Computation
         covariance matrix = np.cov(data standardized)
         # Eigenvalue and Eigenvector Decomposition
         eigenvalues, eigenvectors = np.linalg.eig(covariance matrix)
         # avoiding complex domain parts of eigenvalues
         eigenvalues = np.real(eigenvalues)
         eigenvectors = np.real(eigenvectors)
         # Feature Vector Formation
         # Sort eigenvalues and their corresponding eigenvectors
         idx = np.argsort(eigenvalues)[::-1]
         eigenvalues = eigenvalues[idx]
         eigenvectors = eigenvectors[:, idx]
In [ ]:
         # Covariance Matrix Computation
         covariance matrix = np.cov(data standardized)
         # Eigenvalue and Eigenvector Decomposition
         eigenvalues, eigenvectors = np.linalg.eig(covariance_matrix)
         # avoidng complex domain parts of eigenvalues
         eigenvalues = np.real(eigenvalues)
         eigenvectors = np.real(eigenvectors)
         # Feature Vector Formation
         # Sort eigenvalues and their corresponding eigenvectors
         idx = np.argsort(eigenvalues)[::-1]
         eigenvalues = eigenvalues[idx]
         eigenvectors = eigenvectors[:, idx]
In [ ]:
         # Calculate the cumulative explained variance
         explained variance ratio = np.cumsum(eigenvalues) / np.sum(eigenvalues) * 100
         # Create a DataFrame with the number of components and cumulative variance
         df explained variance = pd.DataFrame({
             'Number of Components': range(1, len(eigenvalues) + 1),
             'Cumulative Explained Variance (%)': explained_variance_ratio
         })
         # Display the DataFrame 10 first rows
         print(f"{df_explained_variance.head(10)}\n\n")
         # Select the top k eigenvectors
         k = 10 # Number of principal components to keep
         eigenvectors reduced = eigenvectors[:, :k]
```

```
# Recast the Data
data_pca = np.dot(eigenvectors_reduced.T, data_standardized)

# Visualize the cumulative explained variance
plt.figure(figsize=(12, 6))
plt.plot(range(1, k + 1), explained_variance_ratio[:k], marker='o', linestyle='--'
plt.title('Cumulative Explained Variance by PCA Components')
plt.xlabel('Number of PCA Components')
plt.ylabel('Cumulative Explained Variance (%)')
plt.ylabel('Cumulative Explained Variance (%)')
plt.sticks(range(1, k + 1))
plt.grid()
plt.show()
```