

AI-driven fusion of neurological work-up for assessment of biological Alzheimer's disease

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1 Abstract

2 Alzheimer's disease (AD) diagnosis hinges on detecting amyloid beta ($A\beta$) plaques and neurofibrillary tau
3 (τ) tangles. While amyloid PET imaging is now clinically approved, tau PET remains largely restricted to
4 research settings. These imaging techniques, though valuable, are expensive and often difficult to access,
5 limiting their widespread use in routine clinical practice. Here, we introduce a computational framework
6 that leverages multimodal data from seven distinct cohorts comprising 12,185 participants to estimate indi-
7 vidual PET profiles, both global and regional, using more accessible data modalities, such as demographics,
8 medical history, medication use, fluid measurements, functional and neuropsychological assessments, and
9 structural MRIs. Our approach achieved an area under the receiver operating characteristic curve of 0.79
10 and 0.84 in classifying persons with positive $A\beta$ and τ status, respectively. Model predictions were consis-
11 tent with various biomarker and cognitive profiles, as well as with different degrees of protein abnormalities
12 observed in post-mortem examinations. Furthermore, the regional volumes identified by the model as im-
13 portant aligned with the spatial distributions of the standardized uptake value ratio for regional τ labels.
14 Our model offers a practical approach to identify potential candidates for newly approved anti-amyloid
15 treatments and AD clinical trials for combined amyloid and tau therapies by utilizing standard neurological
16 evaluation data.

1 Introduction

2 Alzheimer's disease (AD) is biologically defined by the progressive accumulation of amyloid beta ($A\beta$)
3 plaques and neurofibrillary tau (τ) tangles ¹. These proteinopathies develop years before symptom onset,
4 presenting a window for early therapeutic interventions ². The temporal progression of these biomarkers also
5 facilitates biological staging of AD, guiding treatment strategies and timing ³. While amyloid positron emis-
6 sion tomography (PET) imaging is clinically approved for detecting $A\beta$, τ PET remains largely restricted
7 to research settings ⁴. These imaging modalities provide critical insights into disease progression but are
8 expensive and not widely accessible, limiting their routine clinical use compared to conventional modalities
9 such as structural magnetic resonance imaging (MRI) and neurocognitive assessments. Cerebrospinal fluid
10 (CSF) testing offers high sensitivity for amyloid detection but lacks the ability to stage disease progression,
11 which tau PET imaging currently provides ⁴. PET imaging influences clinical decision-making ⁵ and re-
12 mains integral to identifying candidates for disease-modifying therapies and clinical trials ^{6–8}. However,
13 its restricted accessibility in routine care settings underscores the need for cost-effective, scalable screening
14 methods that preserve PET's staging precision while overcoming logistical barriers.

15 The escalating costs associated with AD drug development underscore the necessity for precise disease stag-
16 ing. From 1995 to 2021, AD research and development incurred an estimated \$42.5 billion expenditures,
17 with a staggering 95% failure rate ⁹. A large portion of these costs stems from the screening process re-
18 quired to determine patient eligibility based on $A\beta$ PET positivity status ⁹. However, emerging evidence
19 suggests that τ pathology is more strongly linked with cognitive decline and disease progression ¹⁰. The
20 TRAILBLAZER-ALZ 2 clinical trial demonstrated that Donanemab, an amyloid-lowering therapy, was
21 most effective in patients with lower τ PET burden ⁶, highlighting the critical role of τ staging in deter-
22 mining therapeutic response. These findings highlight the urgent need for scalable approaches to estimate τ
23 burden, bridging the gap between research and clinical practice to optimize patient selection for emerging
24 AD therapies ^{11,12}.

25 Emerging technologies and frameworks, including plasma biomarkers such as p-tau 217, offer potential for
26 early AD detection ^{13,14}. While these biomarkers can predict $A\beta$ PET status with performance comparable
27 to cerebrospinal fluid (CSF) analyses in certain cohorts ¹⁵, their ability to accurately predict tau PET status
28 across diverse populations is less established ^{14,16}. Further, these biomarkers lack the ability to capture the
29 spatial distribution of tau pathology in the brain, which is essential for accurate biological assessment of
30 AD ^{4,17,18}. Variability due to non-neurological factors such as body mass index, cardiovascular and renal
31 health can also affect their clinical efficacy ^{19,20}. Finally, the generalizability and accuracy of cut-off points
32 in racially and ethnically diverse samples have not yet been demonstrated, raising questions about their
33 readiness to enter standard clinical workflows ²¹. Therefore, while promising, plasma biomarkers are not
34 yet a standalone solution, and there is a need for integrated and accessible models capable of accurately
35 pre-screening and stratifying patients based on their $A\beta$ and τ status, as well as disease stage ^{4,11}.

36 Machine learning (ML) models have shown promise in addressing some of the logistical challenges of PET
37 scans by predicting $A\beta$ or τ PET status using less invasive data such as demographics, MRIs and cognitive
38 assessments ^{22–30}. However, these models often face limitations, including development on relatively small
39 cohorts, reliance on emerging plasma biomarkers, lack of external validation and adaptability to real-world
40 settings where data availability varies. By leveraging standard-of-care data, there is an opportunity to de-
41 velop a cost-effective pre-screening process that reliably estimates both amyloid and tau pathology, enabling
42 broader access to advanced diagnostics and targeted treatments.

43 Here, we propose a transformer-based ML framework designed to integrate multimodal data and predict
44 global A β , tau burden in a pre-defined meta-temporal region (meta- τ) encompassing medial and neocortical
45 temporal regions ³¹, and regional tau PET statuses. By incorporating demographic information, medical his-
46 tory, neuropsychological assessments, genetic markers, neuroimaging and other relevant clinically obtained
47 data, we sought to create a flexible computational framework that could be implemented in real-world set-
48 tings, where complete feature sets are rarely available. Additionally, since tau pathology alone is not specific
49 to AD ³², we aimed to output a combined prediction of both A β and τ accumulation to enhance specificity
50 for AD. This approach not only fills the gaps in existing research by providing integrated models for con-
51 current A β on τ pathology prediction, but also facilitates a cost-effective participant selection process that
52 can streamline clinical trials and research. Finally, by outputting probabilities that align with established
53 biological stages, our modeling framework could concurrently identify and stage AD.

1 Results

2 Our modeling framework was developed through training on a large, diverse dataset with multimodal fea-
3 tures (Fig. 1 & Tables S1-S9), and rigorously tested on an external dataset (Table 1). We evaluated our
4 framework's alignment with PET-estimated A β and τ burden and biomarker profiles, and assessed its abil-
5 ity to capture the synergistic relationship between A β and τ . Additionally, we constructed a graph network
6 using Shapley values of brain volumes for each regional tau label and validated the model's regional tau
7 predictions against tau PET SUVr values in the same regions. Finally, we compared the model predictions
8 with postmortem findings, ensuring that the predicted probabilities reflected the severity of the underlying
9 pathology.

10 **Model performance on A β and τ status** We first evaluated our model's performance in predicting
11 global A β and meta- τ status. The receiver operating characteristic (ROC) and precision-recall (PR) curves
12 illustrate the model's performance in predicting A β and tau positivity (Figs. 2a-b). The ROC curves show
13 that the model achieves slightly higher sensitivity and specificity for τ (AUROC = 0.84) compared to A β
14 (AUROC = 0.79). However, the PR curves indicate greater reliability in identifying true positive cases for
15 A β (AUPR = 0.78) than for tau (AUPR = 0.60), despite the higher ROC for tau. This could be attributed
16 to class imbalance or lower prevalence of τ positivity in the dataset, leading to a higher rate of false posi-
17 tives in τ predictions. Additional performance metrics are provided in Extended Table 1a. Supplementary
18 Tables S10 and S11 detail the performance metrics for the internal validation set (NACC) and the combined
19 ADNI-HABS external set, respectively. Notably, the ADNI dataset had 54% fewer features than the held-
20 out NACC* test set, and the HABS dataset had 72% fewer features. Despite these constraints in feature
21 availability, our model maintained robust performance, highlighting its flexibility and ability to handle in-
22 complete feature sets without significant loss of accuracy. In Extended Data Fig. 1, we reported AUROC
23 and AUPR metrics stratified by age, gender and race. The consistent performance across these subgroups
24 indicates that our model is potentially applicable to diverse populations.

25 To assess the impact of different types of clinical features on model performance, we evaluated the model's
26 predictions for A β and meta-temporal tau (meta- τ) status by successively adding different feature groups.
27 Following the typical order of assessments in neurological work-up protocols for cognitive impairment, our
28 analyses aimed to identify incremental gains, if any, when each new test is added to the work-up process
29 (Figs. 2c-d). The plasma biomarker available at testing, the A β 42/40 ratio, and the APOE- ϵ 4 tests are
30 included last due to their relatively limited availability in clinical settings. For A β prediction, the AUROC
31 improved from 0.59 with only person-level history to 0.79 when all features were included, with the AUPR
32 values increasing in parallel from 0.55 to 0.78. Tau prediction models showed a comparable increase in AU-
33 ROC from 0.53 with only patient history to 0.84 with all features. Notably, the addition of MRI data led to a
34 substantial improvement in meta- τ AUROC from 0.53 to 0.74. Subsequent additions of neuropsychological
35 battery scores provided additional improvements, highlighting that the integration of multiple modalities of
36 data leads to better overall performance.

37 To evaluate our model's robustness to the absence of specific feature sets, we systematically removed groups
38 of features from the full model. For A β predictions, removing any single feature set had minimal impact on
39 AUROC values, which remained between 0.74 and 0.80. This highlights the strength of our random feature
40 masking strategy, which allowed the model to make meaningful predictions even in the absence of certain
41 data types. Similarly, τ predictions were robust across feature exclusions, with the removal of the neuropsy-
42 chological battery resulting in the most significant drop in AUPR to 0.53. While our modeling strategy

43 afforded the flexibility in achieving high accuracy despite the absence of certain feature sets, the importance
44 of neuropsychological testing is underscored by the sensitivity of τ AUPR values to the removal of these
45 features. The results of our Shapley analysis (Extended Data Fig. 2a-b) provide additional support for this
46 interpretation, with neuropsychological testing, neuroimaging and APOE- ϵ 4 status having, on average, the
47 greatest impact on model output.

48 We quantified our model's performance on regional τ predictions and found that it achieved a macro-average
49 AUROC and AUPR of 0.80 and 0.42, respectively (Fig. 2e-f). Individual AUROC scores ranged from 0.71
50 to 0.84, indicating robust discriminative ability across different regions of interest (ROIs). The medial
51 temporal τ label achieved the highest AUPR of 0.60, suggesting that the model is particularly effective in
52 identifying true positive cases in this critical region (Extended Table 1b). These results suggest that our
53 transformer-based model effectively predicts regional tau accumulation, particularly excelling in the medial
54 and lateral temporal regions, where the combined AUROC and AUPR values were the highest.

55 We conducted a comparative analysis of our transformer-based model against CatBoost, a robust machine
56 learning approach, to evaluate performance in predicting $A\beta$ and τ pathology. For this purpose, we tested
57 our model without MRI embeddings, with the results detailed in Table S12. On the combined test set
58 from ADNI, HABS, and NACC*, CatBoost achieved an AUROC of 0.81 for $A\beta$ predictions and 0.83 for τ
59 predictions. The corresponding AUPR values were 0.79 for $A\beta$ and 0.53 for τ . In comparison, our model
60 demonstrated slightly lower AUROC for $A\beta$ predictions (0.79 vs. 0.81) but superior AUPR for τ predictions
61 (0.60 vs. 0.53), indicating more effective identification of true positive τ cases. Additionally, CatBoost's
62 balanced accuracy for $A\beta$ prediction stood at 0.64, while ours was 0.68, indicating a more effective balance
63 between sensitivity and specificity in our model. Further performance metrics for CatBoost are provided
64 in Table S13a. To deepen our analysis, we incrementally added features from clinical assessments in the
65 order typically collected during neurological work-ups to the CatBoost model. This step-by-step addition
66 is visualized in Extended Data Fig. 3, contrasting the performance of our model without MRI embeddings
67 (panel a) to that of CatBoost (panel b). Although CatBoost initially shows higher AUROC and AUPR upon
68 integrating medical history and neurological/physical examination data, our model surpasses these metrics
69 upon adding brain regional volumes, functional assessments, and neuropsychological tests. When MRI
70 embeddings are incorporated into our model (Fig. 2c), it achieves an AUROC comparable to CatBoost's
71 upon the addition of CDR scores and plasma $A\beta$ 42/40 ratios, with a marginally better AUPR. Overall, our
72 transformer-based architecture, with its attention mechanism and random feature masking, provides an end-
73 to-end framework that flexibly handles multi-modal inputs and performs effectively on imbalanced datasets.
74 This is especially evident in its superior performance for meta- τ and regional τ predictions, where CatBoost
75 exhibits a macro-average AUROC and AUPR of 0.77 and 0.38, respectively (Extended Data Fig. 3, Fig. 2c,
76 and Supplementary Tables S12, S13).

77 **Validation with biological outcomes** Even though our model was trained on binary classifications, we
78 aimed to assess its alignment with PET-based gradients of $A\beta$ and τ accumulation Fig. 3. As an additional
79 step towards facilitating clinical interpretability of our model outputs, we visualized how well the model's
80 predictions aligned with a commonly used clinical endpoint in AD trials, the Alzheimer's Disease Assess-
81 ment Scale-Cognitive Subscale (ADAS-Cog₁₃ or ADAS13). We observed a positive correlation between
82 P($A\beta$) and centiloid values (Pearson's $r = 0.58$, $p < 0.0001$; Fig. 3a), indicating that higher predicted $A\beta$
83 levels are associated with increased $A\beta$ plaque deposition, as confirmed by centiloid measurements. This
84 relationship aligned with more severe cognitive impairment, evidenced by higher scores on the ADAS13.
85 Similarly, we found a positive correlation between P(τ) and the log of meta- τ SUVR (Pearson's $r = 0.59$,

86 $p < 0.0001$; Fig. 3b), suggesting that higher model-predicted tau levels correlated with greater tau PET es-
87 timated pathology. An associated increase in ADAS-Cog₁₃ was again visible, indicating more pronounced
88 cognitive impairment at higher $P(\tau)$ values (Supplementary Table S14). We ran a similar analysis comparing
89 the regional τ probabilities to the log of the corresponding regional τ SUVR values and found the strongest
90 alignment for the medial temporal (Pearson's $r = 0.56$, $p < 0.0001$, Extended Data Fig. 4a) and lateral
91 temporal predictions (Pearson's $r = 0.52$, $p < 0.0001$, Extended Data Fig. 4b). Further statistical results are
92 reported in Supplementary Table S15.

93 We sought to evaluate our model's sensitivity for detecting $A\beta$ positivity in preclinical AD by comparing
94 $P(A\beta)$ between $A\beta$ PET-negative ($n = 590$) and $A\beta$ PET-positive ($n = 245$) cognitively unimpaired in-
95 dividuals from the ADNI and HABS cohorts. A Mann-Whitney U test revealed significantly lower $P(A\beta)$
96 values in $A\beta$ PET-negative cases compared to PET-positive cases ($U = 50727$, $p = 5.60 \times 10^{-12}$, Fig. 3c),
97 demonstrating the model's ability to distinguish between amyloid status groups even in the absence of cog-
98 nitive symptoms.

99 Finally, we aimed to evaluate the alignment of our model probabilities with established biomarker-defined
100 disease stages (A-T-, A+T-, A+MTL+, and A+NEO+) ⁴. A Kruskal-Wallis H test revealed that our com-
101 posite "AT" score derived from our models' amyloid and regional tau probabilities significantly differed across
102 disease stages ($H = 180.73$, $p = 6.15 \times 10^{-39}$; Fig. 3d). Post-hoc analysis using Dunn's test with Holm-
103 Bonferroni correction for multiple comparisons demonstrated significant differences between all pairwise
104 stage comparisons, with AT scores progressively increasing from A-T- to A+NEO+ stages. This relation-
105 ship suggests that our model-derived probabilities capture the biological progression of AD pathology as
106 defined by recently proposed staging systems ⁴. Detailed statistical results are provided in Supplementary
107 Table S16.

108 **Model ability to capture the synergistic relationship between $A\beta$ and τ** To demonstrate the effec-
109 tiveness of our model for pre-screening in AD clinical trials, we designed a validation approach that aligns
110 with the emerging interest in dual targeting of $A\beta$ and tau pathology, and in stratifying patients by disease
111 burden. Specifically, we assessed the sensitivity of the model outputs to the co-occurring core pathological
112 burden in amyloid PET positive cases. First, we examined how the model's predicted probability of $A\beta$
113 positivity, $P(A\beta)$ varied across different levels of tau PET defined pathology. Participants were categorized
114 into two groups based on their meta- τ SUVR values: a 'low/medium' group (below the 67th percentile) and a
115 'high' group (at or above the 67th percentile). In Fig. 4a, the left panel serves as a reference on the relation-
116 ship we expect when comparing centiloids and tau PET quantiles in our testing set, showing that centiloid
117 values significantly increased with higher τ burden. The one-sided Mann-Whitney U test confirmed this
118 trend, showing a significant difference in centiloid values across the τ tertiles ($U = 5047$, $p = 1.92 \times 10^{-13}$).
119 The right panel presents $P(A\beta)$ between these same quantiles, and similar statistically significant increases
120 in $P(A\beta)$ were seen between the low/medium and high groups ($U = 3707$, $p = 4.01 \times 10^{-20}$). These results
121 indicate that the model's $A\beta$ predictions are sensitive to varying levels of tau burden. Similarly, we assessed
122 how well our model's τ probabilities related to centiloid levels in $A\beta$ PET positive cases. First, we tested the
123 relationship between tau SUVR in the meta-temporal region across tertiles of $A\beta$ centiloids to obtain a refer-
124 ence for the quantitative relationship between $A\beta$ and tau pathologies, as shown in the left panel of Fig. 4b.
125 A one-sided Mann-Whitney test indicated that meta- τ SUVR was significantly higher in the high CL group
126 relative to the low/medium CL group ($U = 5876$, 6.78×10^{-10}). In the right panel, the model's predictions
127 for tau positivity, $P(\tau)$, captured similar biological gradients, with a one-sided Mann-Whitney test showing
128 significant differences in $P(\tau)$ across the same centiloid quantiles (6655.5 , $p = 3.17 \times 10^{-07}$). Detailed

129 statistical results are reported in Supplementary Table S17. Overall, these results demonstrate our model's
130 ability to capture the synergistic relationship between A β and tau pathologies, reinforcing its potential utility
131 in patient stratification for clinical trials targeting both pathologies individually or together.

132 We further compared the distributions of our model-predicted probabilities, P(A β) and P(τ), between parti-
133 cipants with the following PET-confirmed biomarker profiles: A β -, τ - and A β +, τ + (Fig. 4c). The Mann-
134 Whitney U test revealed significant differences in both P(A β) and P(τ) between biomarker-positive and
135 biomarker-negative groups ($U = 61430, p = 5.71 \times 10^{-44}$; $U = 60963, p = 1.63 \times 10^{-42}$, for A β and
136 τ respectively). The scatter plots indicate that A β +, τ + individuals consistently exhibited higher predicted
137 probabilities for both A β and τ compared to those in the A β -, τ - group. The associated boxplots and contour
138 plots collectively highlight key differences between the two groups, revealing higher concentrations and a
139 broader distribution of A β and τ in the A β +, τ + group compared to the negative group. The results also re-
140 veal a greater variability in tau levels for the A β +, τ + group, with the data extending to higher probabilities.
141 In contrast, the A β -, τ - group showed a tighter distribution and lower biomarker values.

142 **Spatial analysis** The accumulation and spatial progression of tau pathology in AD generally follows a
143 stereotypical pattern, beginning in the transentorhinal region, progressing into the limbic system, and even-
144 tually spreading to the neocortical associative areas and, ultimately, the primary sensory cortices ³³. We
145 created a visualization of mean Shapley values for regional volumes across predictions of regional τ pos-
146 itivity (Extended Data Fig. 5), ordering them following this stereotypical progression. This visualization
147 underscores the importance of the MTL, which consistently shows high Shapley values, highlighting its role
148 as the initial site of tau deposition and volumetric changes. To further evaluate the model's decision-making
149 processes when provided with brain regional volumes data, we conducted a graphical analysis to investigate
150 the relative importance attributed to community structures in our model. We then compared the SHAP-
151 derived community structures with tau PET-estimated graphs to assess the alignment between them. The
152 analysis revealed a statistically significant degree of concordance, particularly in the lateral temporal and
153 parietal lobes, suggesting that model-based representations capture meaningful regional distinctions consis-
154 tent with tau pathology (Fig. 5). Specifically, for the medial temporal τ positivity prediction, model-based
155 and reference community structures showed moderate agreement (AMI = 0.219, $p = 0.0014$). The lateral
156 temporal region prediction demonstrated a similar pattern (AMI = 0.176, $p = 0.0056$), while the medial
157 parietal (AMI = 0.134, $p = 0.0484$) and frontal (AMI = 0.138, $p = 0.0216$) predictions exhibited modest
158 similarity. The lateral parietal region achieved the highest agreement (AMI = 0.288, $p = 0.0016$), and the
159 occipital region showed moderate alignment (AMI = 0.233, $p = 0.0010$). Overall, while the partitions in the
160 model-based graphs are not identical to that of the SUVR graphs, there is a non-random correspondence be-
161 tween the two. This supports the idea that the model's network of regional interactions is reflecting aspects
162 of true tau pathology networks, rather than arbitrary groupings. These findings underscore the interpretabil-
163 ity of our approach and its potential to bridge the gap between predictive modeling and biological markers
164 of disease progression.

165 **Neuropathological validation** We validated our model's predictions of A β and tau positivity by com-
166 paring them with neuropathological markers of AD. The mean time difference between age at death and
167 age of assessments was 3.05 years. We observed a general increasing trend in the model probabilities with
168 the severity of the pathological markers. Figs. 6a-d illustrate this relationship by comparing the model's
169 probability scores, P(A β) and P(τ), against key pathological markers across progressive AD stages: Thal-
170 phases of A β plaques, Braak stages of neurofibrillary degeneration, and CERAD (Consortium to Establish
171 a Registry for Alzheimer's Disease) scores for neuritic and diffuse plaques. These markers, denoted as A0-

172 A3 (Thal phases), B0-B3 (Braak stages), and C0-C3 (CERAD scores for neuritic and diffuse plaques) all
173 exhibited a statistically significant upward trend in the median probability of $P(A\beta)$ and $P(\tau)$ as the stages
174 advanced ($p < 0.0001$ for Thal, Braak, and CERAD stages) (Tables S18 & S19). We also evaluated the
175 model's predictions in relation to cerebral amyloid angiopathy (CAA) (Fig. 6e), which is commonly ob-
176 served in postmortem AD cases. The model predicted significantly higher $P(A\beta)$ and $P(\tau)$ in individuals
177 with mild, moderate, or severe CAA compared to those without CAA ($p < 0.05$) (Table S19). These find-
178 ings indicate that our model's predicted probabilities for $A\beta$ and τ positivity closely align with the severity
179 of neuropathological markers, reinforcing the model's validity in reflecting underlying disease pathology.

1 Discussion

2 In this work, we present a transformer-based machine learning model that uses multimodal data to predict
3 individual-level A β and τ PET positivity status in a meta-temporal ROI and in regions associated with
4 progressing disease. Our model achieved strong performance on external data not used for model training,
5 with predictions closely matching postmortem findings. We showed that our model predictions aligned
6 with biological and cognitive outcomes, as well as with disease severity staging, underscoring its clinical
7 relevance. Additionally, the model's predictions of τ pathology in specific ROIs aligned with τ burdens
8 derived from regional SUVR observed on PET scans.

9 Our modeling framework demonstrates flexibility in handling cases with missing features through the use
10 of random feature masking. This approach allows the model to generate predictions and maintain accuracy
11 even when some features are unavailable, which is valuable in settings where all tests are not always accessible
12 for every individual. However, our findings also highlight that certain data inputs, such as neuroimaging
13 and APOE status provide critical information on the underlying pathology, given the improvement in per-
14 formance upon adding these features (Fig. 2c). For tau predictions, the removal of neuropsychological
15 battery scores significantly reduced the AUPR, underscoring its importance in accurate predictions. On the
16 other hand, our analysis suggests that certain features, such as clinical dementia rating (CDR) scores, could
17 potentially be excluded without significantly compromising the model's predictive power. This is likely
18 because our framework was developed by fine-tuning a model that already excels at classifying cognitive
19 status³⁴. This finding has practical implications for clinical settings, as CDR assessments require a trained
20 clinician to conduct in-depth interviews and additional testing, which can be time-consuming and costly.

21 Our results indicate that AI models can potentially enhance biomarker-guided assessment of biological AD
22 and facilitate participant selection in clinical trials targeting A β and τ , either individually or in combina-
23 tion. For example, in AD drug trials, models with high positive predictive values (PPV), can ensure that a
24 higher proportion of individuals flagged as likely to have positive A β or tau PET scans are true positives.
25 This could reduce the number of false positives that would need to be excluded later, improving the effi-
26 ciency and cost-effectiveness of the trial. Additionally, models with a high negative predictive value (NPV)
27 are clinically desirable as they accurately rule out individuals without the condition, reducing the need for
28 unnecessary PET scans and alleviating patient anxiety, thereby lowering both healthcare costs and patient
29 burden. In practice, our AI-based strategy could be integrated into AD screening as follows: persons un-
30 dergoing neurological evaluation would first be assessed using our AI model, which utilizes clinical and
31 imaging data to predict A β and τ status. The primary objective of this initial step would be to identify
32 persons who are unlikely to have A β or τ pathology, thereby ruling out low-risk cases. For individuals
33 whom the AI model does not confidently rule out as being A β or τ positive, PET imaging would then be
34 recommended. This approach ensures that PET scans are focused on cases where they are most likely to
35 provide a diagnostic benefit. In our testing cohort of 1,833 individuals with known A β PET status, our
36 model predictions demonstrate significant potential for cost savings. With an NPV of 75.35%, we can rule
37 out 587 cases from undergoing unnecessary A β PET scans. Similarly, in the test cohort of 844 individuals
38 with known tau PET status, our tau PET model achieved an NPV of 91.65%, suggesting to exclude 582
39 cases from requiring tau PET scans. Together, these models help avoid unnecessary imaging in low-risk
40 individuals, potentially saving over \$3.5 million, based on a \$3,000 cost per scan. Additionally, leveraging
41 the PPV of these models can enhance efficiency by identifying high-risk cases. Our A β PET model, with a
42 PPV of 62.05%, can ensure that 654 individuals receive the necessary scans, while the tau PET model, with
43 a PPV of 52.40%, can prioritize 109 high-risk cases for τ imaging.

44 In addition to predicting probabilities for A β and tau status, our model provides spatial characterization of
45 the disease, which correlated with disease stage. Our findings further demonstrate that the model-derived
46 volumetric regions of importance align with local patterns of tau deposition observed in PET imaging,
47 thereby validating the model's predictive capability (Fig. 5). This alignment can aid in differential diagno-
48 sis, enable more precise identification of disease stages and subtypes, and support personalized treatment
49 approaches based on regional tau pathology. While neurofibrillary tau tangles are a hallmark of AD, other
50 dementias such as frontotemporal dementia and chronic traumatic encephalopathy can also exhibit tau accu-
51 mulation^{32,35}. The presence of A β and the distribution of tau pathology, however, vary by type of dementia,
52 contributing to diverse clinical presentations and progression patterns^{36,37}. Through providing concurrent
53 predictions of A β and τ status, our model can aid in increasing specificity to biological AD. In a second
54 stage, our regional tau model could further enhance differential diagnosis by allowing comparison of pre-
55 dicted regional tau profiles with known tau patterns of other dementias. In typical AD, tau burden gradually
56 increases in the medial and neocortical temporal lobes before spreading to the parietal, frontal, and occipital
57 lobes³³. We have shown that our model's composite AT score effectively differentiates between disease
58 stages, distinguishing A+T- cases from A+MTL+ cases, thereby identifying tau pathology in regions that
59 are affected early in the disease course^{4,38}. Because tau PET is closely associated with biological disease
60 stage as well as cognitive decline, it has been proposed as a potential clinical endpoint for disease-modifying
61 treatments³⁹. Our model could thus serve as a pre-screening tool to not only identify the presence of disease
62 but also to delineate the stage of disease, refining the selection of candidates for potential clinical trials or
63 treatments. While our current dataset lacked sufficient data to fully validate the subtyping potential of our
64 model, the comprehensive regional profile of tau pathology it provides could eventually enable clinicians to
65 determine disease stage and subtype based on established tau deposition patterns in AD⁴⁰. This capability
66 offers promising directions for future research and clinical practice, potentially transforming how AD and
67 related disorders are diagnosed and managed.

68 Our study has a few limitations. Our model was developed and validated on seven distinct cohorts; however,
69 its generalizability across diverse populations and clinical settings remains to be determined, as the dataset
70 was predominantly composed of White participants. Additionally, we used a binary thresholding technique
71 to define A β and tau PET positivity, despite the variability in these definitions across different studies. Vari-
72 ous studies have adopted their own criteria for PET positivity, influenced by multiple factors. Nevertheless,
73 our modeling framework is flexible and can be adapted to different definitions of PET positivity (Figs. 3a-b).
74 Future work could extend this binary classification to an ordinal regression task with multiple categories,
75 providing a more quantitative approach to predicting PET status. Moreover, due to the limited number of
76 cases with blood-based biomarker data in our training dataset ($n = 255$), we were unable to fully leverage
77 these data to enhance the model's predictive accuracy. As novel plasma biomarkers become more widely
78 available, we anticipate that integrating them with existing medical data and neurocognitive evaluations will
79 likely enhance the accuracy of predicting AD pathology than relying on any single modality of data. While
80 our model could help identify individuals likely to have pathology associated with biological AD, extending
81 this framework to select participants for clinical trials is more complex than merely identifying those who
82 are A β and τ positive. Key barriers include limited awareness, fear of diagnosis, overstretched healthcare
83 systems, poor physician awareness, lack of effective treatments, lack of fast diagnostics, and low awareness
84 of clinical trials, causing many eligible participants to be lost before enrollment. Nevertheless, our frame-
85 work can provide an important first step in identifying individuals likely to have the disease, thereby enabling
86 more effective targeting of community outreach programs. Additionally, given preliminary evidence that tau
87 PET status and severity may impact treatment response in anti-amyloid therapies⁶, our model could serve
88 as a tool to predict which patients might benefit most from specific disease-modifying drugs. By stratifying
89 patients based on pathology severity subgroups, clinical trials can be more efficiently designed to assess

90 treatment efficacy in targeted subgroups, potentially improving outcomes and accelerating the development
91 of effective therapies.

92 In conclusion, by leveraging multimodal data from standard neurological work-up, our model shows promise
93 in identifying individuals with biological AD cost-effectively, reducing the reliance on expensive imaging
94 techniques like PET scans. Such frameworks highlight the potential of advanced machine learning tech-
95 niques to reduce the burden associated with participant selection for AD clinical trials. Future prospective
96 studies are needed to assess the accuracy of our approach in identifying biological AD and quantify the
97 economic benefits of using this method in selecting participants for clinical trials.

1 Methods

2 **Study population** This study involved a total of 12,185 participants drawn from seven different cohorts.
3 Written informed consents were obtained from all participants or their proxies, and approval was secured
4 from each cohort's respective institutional ethical review boards. The training set, consisting of 10,352 par-
5 ticipants, included individuals from the A4 study⁴¹, the National Alzheimer's Coordinating Center (NACC)
6⁴², the Open Access Series of Imaging Studies (OASIS)⁴³, the Australian Imaging, Biomarkers and Lifestyle
7 (AIBL) study of aging⁴⁴, and the Framingham Heart Study (FHS⁴⁵). All subjects in this study had an amy-
8 loid PET scan, but only 3,488 of these participants also underwent tau PET imaging. The training set
9 was further split into training (8281 participants) and validation (2071 participants) subsets using stratified
10 splitting across all labels, ensuring the label distribution remained consistent with the original dataset. The
11 test set comprised 1,833 participants from the Alzheimer's Disease Neuroimaging Initiative (ADNI)⁴⁶,
12 the Harvard Aging Brain Study (HABS)⁴⁷, and a subset of NACC subjects with neuropathological data.
13 Data collected included demographics, medical history, neuropsychological scores, physical and neurolog-
14 ical examinations, APOE e4 genotype, neuroimaging data, as well as CSF and blood biomarkers for model
15 training. All model evaluations at testing were performed without using CSF. In the study sample, 7,561
16 participants were A β PET negative and 4,624 were A β PET positive. Among those who underwent tau PET
17 assessments (n=3,488), 2655 were tau PET negative and 833 were tau PET positive on a meta-temporal re-
18 gion of interest (ROI). Table 1 provides a detailed overview of the study population across all cohorts. Single
19 visits were included for each participant.

20 **Selection criterion** Participants were eligible for inclusion in the study if they had undergone at least one
21 A β PET scan and had clinical or neuroimaging visits within one year of the PET scan. For cohorts with
22 multiple eligible visits such as ADNI, HABS, NACC, OASIS, and AIBL, visits were selected to minimize
23 the time difference between PET scan and clinical or MRI visits. Because OASIS may share participants
24 with ADNI and NACC, we conducted pairwise comparisons between participants in OASIS and ADNI as
25 well as OASIS and NACC - we searched for similar characteristics across demographics, physical charac-
26 teristics, medical history and comorbidities, functional assessment scores, neuropsychiatric symptoms, and
27 cognitive statuses, with an error tolerance of 2 units in numerical features and excluded any such potentially
28 duplicated participants. All subjects in the A4 cohort with a A β PET scan were included. In the FHS co-
29 hort, participants with a A β PET scan performed within one year after a clinical visit were retained. To
30 ensure consistency across the diverse cohorts, all data were renamed according to the Uniform Data Set
31 Researchers Data Dictionary 3. Despite the unique sets of variables between cohorts, which did not always
32 overlap, no cases were excluded due to missing data. This was facilitated by our model training approach,
33 which incorporated random feature and label masking, as previously reported³⁴.

34 **PET image processing** Cortical amyloid positivity was quantified using various PET imaging agents in
35 the cohorts: Dynamic 11C-PiB for FHS, late-frame 18F-florbetapen and 18F-florbetapir for ADNI, 18F-
36 florbetapir for A4 and OASIS3, 18F-flutemetamol for AIBL, and 11C-PiB for AIBL, OASIS3, and HABS.
37 Centiloid (CL) values were provided directly by ADNI, A4, OASIS, and a subset of NACC ($n = 334$)
38 while for AIBL and HABS, an internal pipeline was used to process standard uptake value (SUV) images,
39 following the methodology established by Klunk and colleagues⁴⁸. Briefly, A β PET and T1 weighted (T1w)
40 images were automatically realigned to match the orientation of the MNI152 template. We then coregistered
41 the A β PET and T1w MRI images to the MNI152 template, normalized to standard space, and calculated
42 global cortical SUV ratios (SUVR) using the Global Alzheimer's Association Interactive Network (GAAIN)
43 masks. Our pipeline, which uses SPM12 for image realignment and normalization, differs slightly from

44 the standard Klunk method⁴⁸, which requires us to process GAAIN data and regress our calculated SUVrs
45 against Klunk's published values to derive a scaling equation to convert SUVrs to CL for each tracer. For
46 the FHS cohort, mean cortical ¹¹C-PiB distribution volume ratios (DVR) images were estimated using the
47 Logan method⁴⁹ and these were subsequently processed as described above to calculate global cortical DVR
48 values. DVR images and T1w scans were realigned to the MNI152 orientation, before being co-registered
49 and normalized to standard space. GAAIN masks were finally used to estimate the global cortical DVR. For
50 tau PET, standardized uptake value ratios (SUVr) in Freesurfer-defined regions were made available by the
51 A4, OASIS, FHS, ADNI, HABS and a subset of the NACC cohorts ($n = 344$).

52 **PET data harmonization** Tau PET data from the various cohorts were processed using different image
53 processing pipelines^{18,50–52}. Therefore, we employed the ComBat tool to harmonize tau PET SUVr values
54 to account for variation across cohorts⁵³. A batch variable for cohort and several covariates were used,
55 including age, sex, amyloid status and diagnosis. We used an analysis of covariance (ANCOVA) framework
56 to assess the main effects of cohorts on tau SUVr measurements across brain regions before and after Com-
57 Bat harmonization, adjusting for covariates age, sex, diagnosis, and amyloid status. Raw p-values from the
58 ANOVA results were adjusted using the Benjamini-Hochberg procedure to control for the false discovery
59 rate across multiple comparisons. ROIs with an adjusted p-value below 0.05 were considered significant.
60 For SUVr regions where the ANOVA indicated a significant cohort effect post harmonization, post hoc
61 pairwise comparisons were conducted using estimated marginal means. Pairwise contrasts between cohorts
62 were computed with Tukey's adjustment for multiple comparisons. Please refer to Extended Data Fig. 6 and
63 Supplementary Tables S20 and S21 for more detail on the effect of harmonization.

64 **PET positivity thresholding and tau profiling** For A β PET, a pre-established threshold of 24 CL¹⁴ was
65 applied to define positivity in A4, OASIS3, AIBL, HABS, ADNI and the subset of NACC with available CL
66 data. For FHS, a pre-established threshold of 1.2 DVR was used to define A β PET positivity¹⁴. Most of the
67 NACC subjects included in this study ($n = 4,006$) were assessed using a binary UDS variable indicating
68 A β positivity, and no information was available regarding site-specific thresholding. For tau PET, a meta-
69 temporal region of interest (ROI) was constructed following established standards³¹. A Gaussian mixture
70 model (GMM) with two components was run on the training dataset and tau PET positivity was defined as
71 SUVr values greater than 1.37. In addition to the meta-temporal ROI, we also defined tau ROIs associated
72 with various AD stages and subtypes: medial temporal, lateral temporal, medial parietal, lateral parietal,
73 frontal and occipital^{17,18}. GMM analyses set the positivity thresholds at 1.32, 1.33, 1.38, 1.29, 1.30 and
74 1.23, respectively. Table S9 provides an overview of the study population broken down by regional tau
75 positivity status.

76 **MRI processing** T1-weighted (T1w), FLAIR, and T2*-weighted (T2*w) MRI sequences were collected
77 from various cohorts. Table 1 details the MRI counts for each sequence across these cohorts. T1w images
78 were segmented with Fastsurfer⁵⁴, and regional volumes were estimated. A Swin UNETR architecture^{55,56}
79 was further leveraged to extract features from bias field corrected volumetric T1 scans, as well as FLAIR
80 and T2* images that were resampled to 1mm resolution. FLAIR and T2* images were additionally padded
81 to $256 \times 256 \times 256$ before being input to the Swin UNETR architecture. All resulting embeddings were of
82 length $768 \times 8 \times 8 \times 8$.

83 **Modeling framework** We utilized the framework detailed in Xue et. al.³⁴ to analyze 443 distinct clinical
84 features encompassing personal demographics, medical history, functional assessments, neuropsycholog-
85 ical test scores, neuroimaging data, and fluid biomarkers (Fig. 1). Each feature was first encoded into a

fixed length vector via a modality-specific embedding technique that served as input to the transformer. The transformer then integrated these inputs to generate predictions. A key feature of this model is the implementation of a feature masking mechanism within the transformer, which is designed to handle missing data effectively. The framework also incorporated a label masking strategy to leverage datasets with missing labels. The task was formulated as a multilabel classification problem, with separate binary heads assigned for predicting each label. To account for missing labels, the loss associated with samples lacking specific labels was masked before backpropagation. This approach significantly enhanced the model's robustness and accuracy in real-world scenarios with incomplete datasets. We fine-tuned this model, originally trained on a 13-label classification task³⁴, using a two-stage process. In the first stage, we trained the model to predict A β and meta- τ labels by transferring the weights of the transformer encoder module and the embedding modules corresponding to overlapping features. During the initial 15 epochs, only the newly initialized weights were trained, while the transferred weights remained frozen. Subsequently, we unfroze the transferred weights and included them in the training process. In the second stage, we further fine-tuned the model to predict regional τ labels. To prevent label leakage, we maintained the same training and testing splits for the NACC dataset as in the original transformer protocol³⁴, ensuring no subject overlap between the two sets.

Loss function Our model was trained by minimizing the “Focal Loss (FL)”⁵⁷ (\mathcal{L}), along with the standard L2 regularization term. FL is a variant of standard cross-entropy loss that addresses the issue of class imbalance. It assigns low weight to easy (well-classified) instances and high weight to hard-to-classify examples. This loss function was used for each of the biomarker categories. Therefore, our \mathcal{L}_{FL} term was:

$$\mathcal{L}_{\text{FL}} = \frac{1}{N} \sum_{k=1}^N \sum_{i=1}^M -y_{k,i} \alpha_i (1 - p_{k,i})^\gamma \log(p_{k,i}) - (1 - y_{k,i})(1 - \alpha_i)(p_{k,i})^\gamma \log(1 - p_{k,i}),$$

where N was the batch size and M was the number of biomarker categories (2 for the first stage and 6 for the second), and other parameters and variables were as defined. The focusing parameter γ was set to 2, which had been reported to work well in previous studies^{34,57}. Moreover, $\alpha_i \in [0, 1]$ was the balancing parameter that influenced the weights of positive and negative instances. It was set as the square of the complement of the fraction of samples labeled as 1, varying for each i due to the differing level of class imbalance across biomarker categories. After combining all terms, the overall loss function (\mathcal{L}) was:

$$\mathcal{L} = \mathcal{L}_{\text{FL}} + \beta \|\mathbf{w}\|^2,$$

where β controlled the importance of the L2 regularization term. For both stages of training, the maximum epochs was set to 128 epochs, with early stopping applied if no improvement was observed on the validation split for 15 epochs in the first stage and 30 epochs in the second. The L2 regularization parameter β was set to 0.01 for the first stage and 0.005 for the second. Mini-batch training was performed using the AdamW optimizer⁵⁸, with learning rates of 0.001 and 0.0001 for the respective stages. Additionally, a cosine scheduler was employed to dynamically adjust the learning rate during training.

Interpretability analysis To interpret the model predictions, we conducted Shapley analysis⁵⁹ on the outputs for A β , meta- τ , and regional τ models. Shapley values quantify the contribution of each feature to the model's predictions, effectively providing a measure of feature importance. We employed a permutation sampling strategy^{34,60} to efficiently estimate Shapley values across the high-dimensional feature space. This approach involves permuting feature values and measuring changes in the model's output to approximate each feature's impact. For each label prediction, Shapley values were calculated for all input features, including imaging-derived measures, whole brain image embeddings and clinical variables. Missing features

125 were assigned a Shapley value of zero, indicating no contribution to the prediction. The features were then
126 ranked by their mean Shapley values across true positive samples, identifying the most influential features
127 driving the model's decisions.

128 **Traditional machine learning model** We sought to compare the performance of our model with that of
129 a traditional machine learning framework, CatBoost⁶¹, to provide a benchmark for our approach. As a
130 tree-based classification framework, CatBoost effectively handles missing features by assigning designated
131 missing values when an input is absent at inference. However, CatBoost lacks support for incorporating
132 learned embeddings from imaging data, limiting its ability to leverage spatial patterns captured in MRI
133 scans. To address this, we used regional volumes derived from FastSurfer as the imaging-related inputs for
134 CatBoost. Additionally, unlike our transformer-based model, which performs multi-label classification in a
135 unified manner, CatBoost requires training separate models for each output variable. As a result, we trained
136 eight independent CatBoost models, one for each label, while our deep learning approach benefited from
137 joint optimization across multiple tasks.

138 **Model validation on biological outcomes** We sought to validate predicted probabilities of the model
139 against PET estimates of amyloid and tau burden, as well as evaluate its alignment with a common clinical
140 endpoint in AD clinical trials, the Alzheimer's Disease Assessment Scale-Cognitive Subscale (ADAS-
141 Cog₁₃). Importantly, ADAS-Cog₁₃ scores were not incorporated as input during the model's training, en-
142 suring independent validation of the model's predictive capabilities. Participants from the ADNI cohort
143 were selected for this analysis, as they both underwent amyloid and tau PET imaging and completed the
144 ADAS-Cog₁₃ assessment. To further evaluate our model performance in preclinical AD, we included a sub-
145 set of cases from the ADNI and HABS cohort who were cognitively unimpaired. We then compared model
146 predicted probabilities for amyloid, P(A β), between cases who were A β PET negative vs A β PET positive.
147 Finally, we aimed to validate our model predictions of regional tau positivity and investigate its potential
148 for disease staging. To derive a unified quantification of AD pathology, we employed principal component
149 analysis (PCA). This dimensionality reduction technique allowed us to capture the shared variance across
150 different regional tau and amyloid probabilities into a single composite score. We applied PCA and used the
151 first principal component (PC1), which explained 97.5% of the variance, as our composite measure of AD
152 pathology, termed the amyloid-tau (AT) score. Based on the PET binary labels, we classified participants
153 and compared the AT scores across four distinct disease stages. These included cases who are A β PET
154 negative and tau PET negative in all regions (A-T-), A β positive but tau negative in all regions (A+T-), A β
155 positive with tau PET positivity restricted to the medial temporal lobe (A+MTL+), and A β positive cases
156 with tau PET positivity in the medial temporal and neocortical regions (A+NEO+).

157 **Subgroup analysis on biomarker profiles** We selected a subset of cases from the testing set with PET-
158 confirmed A β positivity, mirroring the inclusion criteria for amyloid presence used in recent clinical trials
159 [REF]. Participants were then stratified into tertiles (low, medium, and high) based on their meta- τ SUV_r
160 values to evaluate the model's predictive accuracy across a spectrum of tau burdens. We further assessed
161 the relationship between tertile groups and centiloids to evaluate whether the model's output is consistent
162 with empirically measured amyloid levels. Similarly, we conducted an analysis of the model-predicted tau
163 probabilities, P(τ), in A β + cases, this time stratifying participants into tertiles based on their centiloid
164 values. Because the NACC* testing cohort did not have continuous PET data available, only ADNI and
165 HABS were included in these analyses. Finally, to further validate our model's ability to differentiate those
166 who are positive on both biomarkers from those who are negative on both, we compared the distributions of
167 P(A β) and P(τ) in the combined ADNI, HABS and NACC* test set between A β +, τ + and A β -, τ - cases.

168 **Spatial analysis** Cases with positive regional τ labels and predictions were selected for this data-driven
169 analysis. A fully-connected graph network was constructed with nodes representing individual brain re-
170 gions and edges connecting the nodes. Edge weights were determined by computing pairwise normalized
171 mutual information (NMI)^{62–64} on the Shapley values of T1-derived regional volumetric features. This
172 quantifies the mutual dependence between two brain regions in their contribution to the model. We identi-
173 fied non-overlapping communities of brain regions that the model deemed important for positive predictions
174 on each regional label using the Louvain method for community detection⁶⁵. We preset the number of com-
175 munities in each graph to five, corresponding to the established Braak staging of tau pathology progression,
176 combining regions from stages 1 and 2³³. To address the randomness inherent in the Louvain algorithm,
177 we employed consensus clustering with 100 draws⁶³. Using the same set of cases, we established another
178 graph network on the same brain regions, but with edges defined by the NMI of the tau PET SUVR values.
179 We identified communities of brain regions in this network using the same methodology as before. To com-
180 pare the T1-derived communities identified as important by the model against the communities identified
181 in the tau PET scan, we evaluated the similarity between these two clusterings using the adjusted mutual
182 information (AMI)⁶⁶. The AMI measures the level of agreement between two clusterings with correction
183 for random clustering agreement, and is preferred over adjusted Rand index (ARI) when the reference clus-
184 tering is unbalanced and there exist small clusters⁶⁷, which aligns well with our results (Table S22). A *t*-test
185 on 5,000 spatial permutation draws was conducted on AMI for assessing statistical significance^{68,69}. Spatial
186 permutations were applied to maintain the brain's contralateral symmetry through rotating spherically
187 projected brain region coordinates extracted from the Desikan-Killiany atlas by a random angle along each
188 of the x, y, and z axes. New labels were assigned by mapping the original region centroids to the closest
189 permuted region centroid based on Euclidean distance.

190 **Postmortem validation** To assess the alignment of our model with neuropathological evidence, we utilized
191 a subset of cases from the ADNI database ($n = 41$) for which postmortem evaluations were available. We
192 supplemented this sample with an additional subset of cases from the NACC database ($n = 147$) for which
193 neuropathological data was available, excluding these cases from the training set. Of note, this subset of
194 NACC cases was also in the testing set of the original transformer model³⁴ that we are finetuning in this
195 study, thus preventing potential label leakage. The average time lag between the visit selected for model
196 development and the time of death was 3 years on average. On these cases, we examined the Thal phase
197 for amyloid plaques (A score), Braak stage for neurofibrillary degeneration (B score), density of neocortical
198 neuritic plaques (CERAD score) (C score), density of diffuse plaques (CERAD semi-quantitative score),
199 and cerebral amyloid angiopathy, and investigated the correlation between the model-generated probability
200 scores of $A\beta$ and τ positivity and the grades of these neuropathological features.

201 **Statistical analyses** We conducted a series of statistical analyses to rigorously evaluate our AI model's
202 alignment with PET burden, biomarker profiles, and post-mortem neuropathological grades. A Shapiro-Wilk
203 test was performed prior to each analysis to assess normality. To evaluate the alignment between our model-
204 predicted probabilities and continuous PET values, we computed both the Spearman's ρ and Pearson's r
205 coefficients, log-transforming regional τ SUVR values to improve linearity. We then sought to validate our
206 model's predictive accuracy across quantiles of disease severity. We used a one-sided Mann-Whitney U test
207 to compare predicted probabilities ($P(A\beta)$ and $P(\tau)$) and PET measures (centiloids and meta-T SUVR) be-
208 tween cases with low/medium vs. high disease burden. Similarly, we applied a one-sided Mann-Whitney U
209 test to compare $P(A\beta)$ and $P(\tau)$ between cases who are PET-confirmed biomarker positive and negative. Ad-
210 ditionally, we evaluated the model's ability to detect preclinical AD by comparing amyloid probability out-
211 puts between $A\beta$ PET negative and positive cognitively unimpaired cases using a one-sided Mann-Whitney
212 U test. We then aimed to validate our model's ability to distinguish disease stages. A Kruskal-Wallis H

213 test, followed by post hoc Dunn's test with Holm-Bonferroni adjustments for multiple comparisons was
214 performed to assess the alignment of our model's AT score with PET-defined disease stages. To evaluate
215 differences in model probability outputs across various stages of neuropathological scores, we employed the
216 Kruskal-Wallis test, followed by post hoc Dunn's tests to conduct pairwise comparisons between groups,
217 with adjustments for multiple comparisons using the Holm-Bonferroni correction method. Additionally, to
218 assess the overall correlation between the model-generated probabilities and each neuropathological fea-
219 ture, we computed the Spearman correlation coefficient, assessing the strength and direction of association
220 between the ranked neuropathological grades and model probabilities.

221 **Performance metrics** Receiver operating characteristic (ROC) and precision-recall (PR) curves were cre-
222 ated based on the predictions on the combined ADNI and HABS external datasets, as well as on the NACC
223 test set. Additional performance metrics including balanced accuracy, sensitivity, specificity, precision (pos-
224 itive predictive value), F1 score, Matthews correlation coefficient, and negative predictive value (NPV) were
225 computed by determining the optimal threshold for each label using Youden's J statistic, based on the per-
226 formance of the validation split.

227 **Computational hardware and software** Our software development utilized Python (version 3.11.9) and
228 the models were developed using PyTorch (version 2.4.0). We used several other Python libraries to support
229 data analysis, including pandas (version 2.2.2), numpy (version 1.26.3), matplotlib (version 3.9.1), monai
230 (version 1.3.2), scipy (version 1.14.0), and scikit-learn (version 1.5.1). Several R packages were also used
231 for data analysis and visualization, including dplyr, emmeans, and ggseg3D. Training the model on a single
232 Tesla V100 GPU on a shared computing cluster had an average runtime of 2 minutes per epoch, while
233 the inference task took less than a minute per instance. All figures were prepared using Canva and Adobe
234 Illustrator.

235 **Data availability** Data from A4, AIBL and ADNI are available to download from the LONI website
236 at <https://ida.loni.usc.edu>. NACC and OASIS-3 data can be requested and downloaded at
237 <https://naccdata.org> and <https://sites.wustl.edu/oasisbrains/>, respectively. FHS
238 data (<https://www.framinghamheartstudy.org/fhs-for-researchers/data-available-overvie>)
239 can be requested by emailing fhs@bu.edu, and access conditions include completing the steps outlined at
240 <https://www.framinghamheartstudy.org/fhs-for-researchers/>, as well as approval
241 from the FHS Research Committee. HABS data can be requested at <https://habs.mgh.harvard.edu/researchers/request-data/>. All data used in this study should be available free of charge
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62 and LEARN Studies. ATRI coordinates these studies, and the data is accessible through the Laboratory for
63 Neuro Imaging at the University of Southern California.

64 The Harvard Aging Brain Study (HABS), initiated in 2010, provided data for this manuscript (P01AG036694;
65 <https://habs.mgh.harvard.edu>). The study, supported by the National Institute on Aging, is directed by prin-
66 cipal investigators R. A. Sperling and K. A. Johnson at the Massachusetts General Hospital/Harvard Medical
67 School in Boston.

68 Author contributions

69 V.H.J. and S.P. performed data collection. S.S.K. designed and developed the machine learning framework.
70 V.H.J., S.S.K., S.P., M.F.R. and L.X. performed model training and validation. V.H.J., S.P., and L.X. per-
71 formed statistical analysis. V.H.J., S.S.K., S.P., M.F.R. and L.X. generated figures and tables. R.A. provided
72 access to data. V.B.K. and V.H.J. wrote the manuscript. All authors reviewed, edited and approved the
73 manuscript. V.B.K. conceived, designed and directed the study.

74 Ethics declarations

75 V.B.K. is a co-founder and equity holder of deepPath Inc., and CogniScreen, Inc. He also serves on the
76 scientific advisory board of Altoida Inc. R.A. is a scientific advisor to Signant Health and NovoNordisk.
77 The remaining authors declare no competing interests.

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Dataset	Age (mean ± std)	Male gender (n, %)	Education in years (mean ± std)	Race (White; Black; Asian; American Indian; Pa- cific; Multi-race)	CDR (0.0, 0.5, 1.0, 2.0, 3.0)	MRIs available (T1, T2*, FLAIR)
Training						
NACC training [n = 4193]						
Amyloid-Negative [n=2311, 55.12%]	70.28±8.83	1073, 46.43%	16.21±2.85	1899; 237; 62; 22; 3; 65	1231; 788; 194; 64; 33	129, 0, 0
Amyloid-Positive [n=1882, 44.88%]	71.51±8.75	908, 48.25%	16.25±2.75	1723; 87; 27; 5; 0; 29	325; 884; 470; 147; 56	79, 0, 0
Tau-Negative [n=1090, 67.58%]	70.60±9.56	519, 47.61%	16.17±2.87	913; 96; 17; 18; 1; 34	560; 359; 103; 42; 26	0, 0, 0
Tau-Positive [n=523, 32.42%]	68.95±9.34	251, 47.99%	16.15±2.66	481; 20; 10; 3; 0; 7	46; 251; 158; 52; 16	0, 0, 0
p-values	1.26e-08	6.81e-01	8.26e-01	1.24e-16	5.03e-199	
OASIS [n = 962]						
Amyloid-Negative [n=631, 65.59%]	68.80±8.62	267, 42.31%	16.10±2.50	520; 104; 4; 1; 0; 2	591; 37; 3; 0; 0	629, 586, 398
Amyloid-Positive [n=331, 34.41%]	74.55±6.79	158, 47.73%	15.90±2.76	300; 28; 2; 0; 1	194; 96; 36; 4; 1	329, 304, 227
Tau-Negative [n=323, 86.83%]	68.94±8.39	140, 43.34%	16.43±2.29	282; 38; 2; 1; 0; 0	303; 19; 1; 0; 0	322, 320, 319
Tau-Positive [n=49, 13.17%]	74.19±6.51	19, 38.78%	15.55±2.53	43; 5; 0; 0; 1	15; 20; 12; 2; 0	49, 48, 49
p-values	1.96e-27	3.65e-01	1.79e-02	N.A.	2.12e-66	
A4 [n = 4475]						
Amyloid-Negative [n=3156, 70.53%]	70.89±4.49	1277, 40.46%	16.57±2.83	2846; 127; 136; 7; 21	3156; 0; 0; 0	623, 624, 104
Amyloid-Positive [n=1319, 29.47%]	72.23±4.94	544, 41.24%	16.62±2.85	1236; 32; 34; 2; 0; 6	1319; 0; 0; 0	1155, 1156, 280
Tau-Negative [n=357, 80.41%]	71.55±4.83	154, 43.14%	16.18±2.87	325; 6; 19; 1; 0; 4	357; 0; 0; 0	357, 357, 69
Tau-Positive [n=87, 19.59%]	73.05±4.76	36, 41.38%	16.43±2.69	82; 4; 1; 0; 0; 0	87; 0; 0; 0	87, 87, 11
p-values	1.87e-19	7.86e-01	6.79e-02	2.78e-02	N.A.	
AIBL [n = 467]						
Amyloid-Negative [n=235, 50.32%]	72.89±6.69	101, 42.98%	N.A.	N.A.	199; 34; 2; 0; 0	235, 0, 150
Amyloid-Positive [n=232, 49.68%]	75.62±6.77	112, 48.28%	N.A.	N.A.	95; 89; 40; 7; 1	232, 0, 103
p-values	1.52e-05	2.91e-01	N.A.	N.A.	4.01e-22	
Testing						
ADNI [n = 1404]						
Amyloid-Negative [n=726, 51.71%]	72.23±7.53	370, 50.96%	16.56±2.44	632; 56; 17; 3; 1; 11	399; 299; 27; 1; 0	726, 725, 350
Amyloid-Positive [n=678, 48.29%]	74.79±7.57	332, 48.97%	16.06±2.68	614; 39; 12; 0; 1; 10	178; 379; 112; 7; 1	678, 678, 330
Tau-Negative [n=499, 79.84%]	72.94±7.55	235, 47.09%	16.51±2.43	420; 54; 13; 2; 0; 7	333; 149; 16; 1; 0	499, 499, 268
Tau-Positive [n=126, 20.16%]	74.65±8.17	56, 44.44%	15.86±2.34	111; 8; 2; 0; 0; 3	20; 73; 28; 4; 1	126, 126, 58
p-values	1.08e-09	4.09e-01	1.16e-04	3.00e-01	1.48e-63	
HABS [n = 282]						
Amyloid-Negative [n=201, 71.28%]	75.92±6.51	82, 40.80%	15.72±3.16	159; 35; 5; 0; 0; 1	186; 12; 0; 0; 0	201, 0, 198
Amyloid-Positive [n=81, 28.72%]	77.56±5.89	32, 39.51%	16.11±2.91	70; 9; 1; 0; 0; 1	69; 12; 0; 0; 0	81, 0, 81
Tau-Negative [n=153, 88.44%]	77.55±6.05	61, 39.87%	16.04±3.02	135; 16; 1; 0; 0; 0	135; 15; 0; 0; 0	153, 0, 152
Tau-Positive [n=20, 11.56%]	80.89±5.89	9, 45.00%	16.45±3.41	15; 5; 0; 0; 0; 0	15; 5; 0; 0; 0	20, 0, 20
p-values	1.51e-03	9.72e-01	5.71e-01	N.A.	N.A.	
NACC testing [n = 147]						
Amyloid-Negative [n=60, 40.82%]	71.80±11.25	41, 68.33%	16.00±2.78	55; 4; 0; 0; 0; 1	10; 17; 19; 6; 8	2, 0, 0
Amyloid-Positive [n=87, 59.18%]	70.66±10.34	48, 55.17%	16.22±2.94	82; 5; 0; 0; 0	3; 28; 29; 22; 5	2, 0, 0
Tau-Negative [n=29, 64.44%]	73.07±13.19	20, 68.97%	15.59±3.26	26; 2; 0; 0; 1	3; 10; 9; 3; 4	1, 0, 0
Tau-Positive [n=16, 35.56%]	65.81±9.77	6, 37.50%	15.13±2.72	16; 0; 0; 0; 0	0; 4; 4; 8; 0	0, 0, 0
p-values	1.80e-01	7.45e-02	5.02e-01	N.A.	1.06e-02	

Table 1: Study population. Summary of demographic and clinical attributes for the training and testing cohorts used in the study. Each cohort section details the mean age (with standard deviation), male participant count (with percentage), average years of education (with standard deviation), racial demographics (with counts for each racial category), clinical dementia rating (CDR) breakdown (with counts for each category), and the availability of MRI types (T1, T2*, and FLAIR). Statistical significance for between-group comparisons was assessed using one-way ANOVA for continuous variables (age, education), and chi-squared tests for categorical variables (gender, race, CDR), with p-values reported in scientific notation for each comparison. Statistical comparisons were not concluded for differences in MRI availability. The N.A. entries in the table signify scenarios when statistical tests could not be concluded and when data were not available.

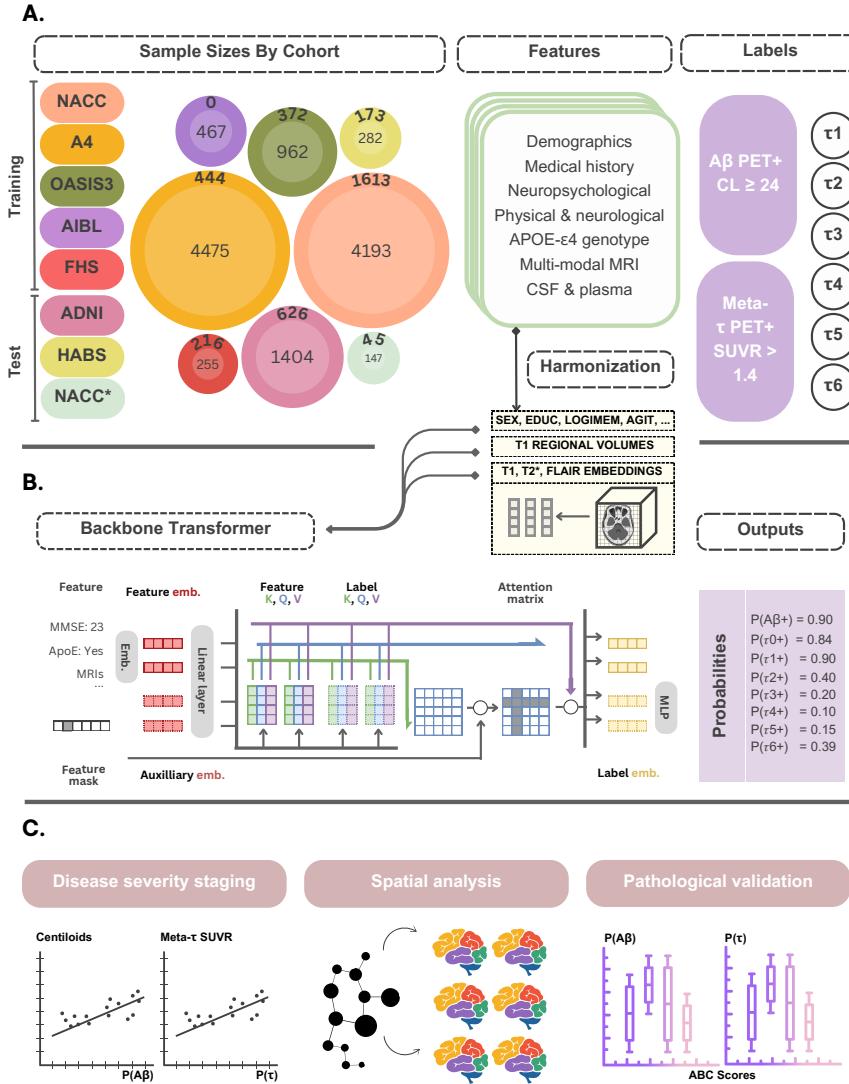


Figure 1: Data, model development and validation strategy. (a) Our model for assessing amyloid and tau status was developed using diverse data modalities, including individual-level demographics, health history, genetic information, neuropsychological testing, physical/neurological exams, and multi-sequence MRI scans. These data sources were aggregated from eight independent cohorts: NACC, A4, OASIS3, AIBL, FHS, ADNI and HABS. All features were harmonized to the UDS3 format and embeddings were extracted from multi-modal MRI scans. Inner concentric circles provide the sample size of the cases with $\text{A}\beta$ PET data and outer circles denote the sample size with τ PET data. (b) Each feature was transformed into a set length vector through a modality-specific embedding approach before being input into the main transformer. A linear layer then linked the transformer to the output prediction layer. (c) The external ADNI and HABS datasets, as well as a held-out set of NACC* data, were selected to compare pathology-specific model predicted probabilities with functional and biological outcomes, as well as alignment with neuropathology grades. Shapley analysis was run on the regional τ model, and a graphical network analysis was performed to detect clusters of important brain regions using the Shapley values of the T1-weighted derived volumes. A similar community detection algorithm was run on the raw regional tau PET SUVrs and we compared communities derived from Shapley values with those derived from the regional SUVrs with statistical testing. The model architecture schematic in (b) was reproduced from our previous work³⁴.

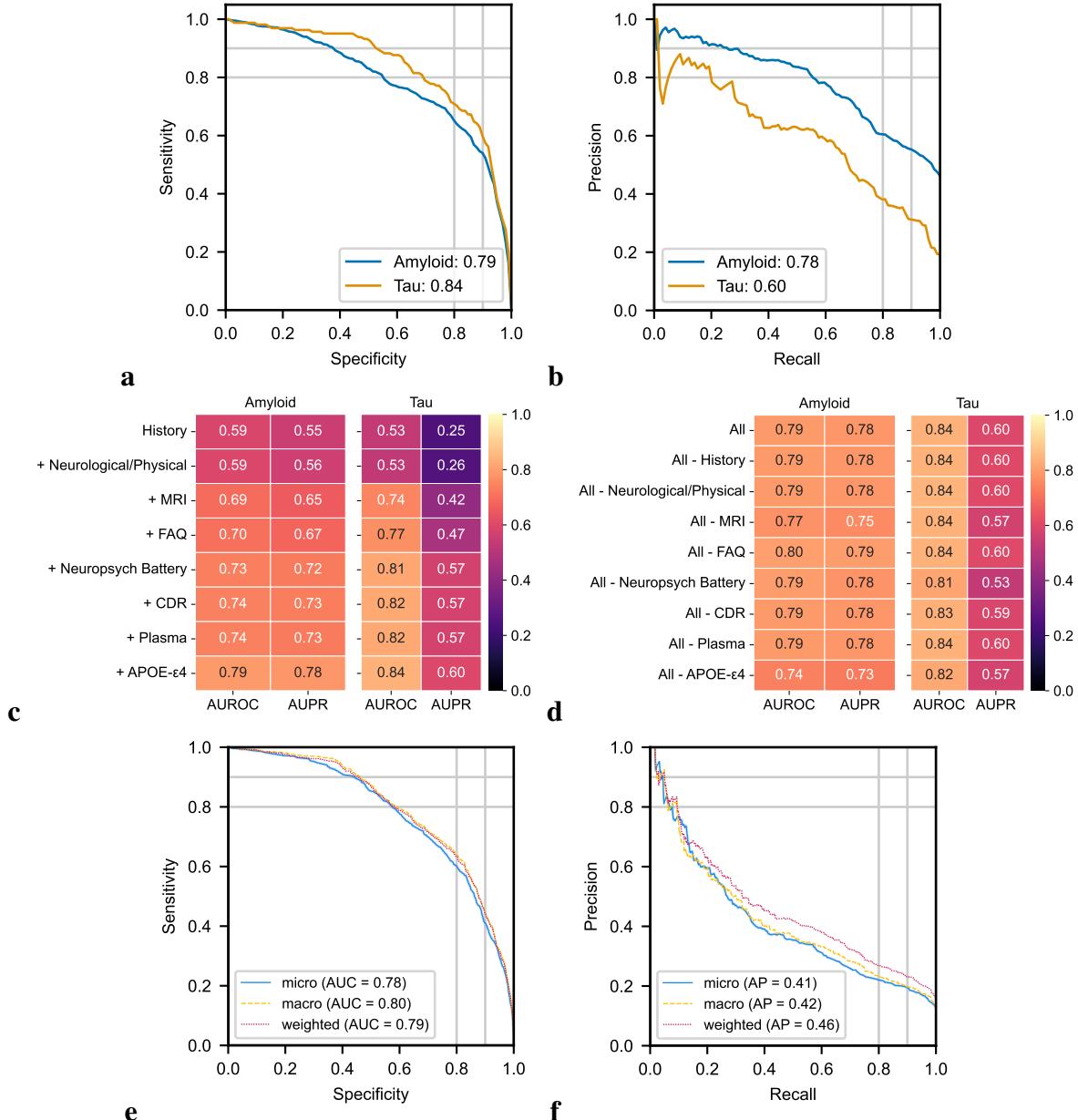


Figure 2: Model performance in predicting amyloid and tau positivity. (a, b) Receiver operating characteristic (ROC) and precision-recall (PR) curves for $A\beta$ and meta- τ predictions are shown. The area under the ROC curve (AUC) and the area under the PR curve (AUPR) values for $A\beta$ and meta- τ are displayed in the legends, respectively. (c) Heatmap presenting the ROC and PR values for $A\beta$ and meta- τ predictions using various combinations of clinical features, starting with person-level history alone and incrementally adding features such as MRI, neuropsychological battery, and plasma data. (d) Heatmap displaying the AUC and AUPR values for $A\beta$ and meta- τ predictions when specific feature sets are removed from the full model. Each row represents the model performance after excluding one feature set, showing how the absence of that data impacts prediction accuracy. (e, f) ROC and PR curves showing micro-average, macro-average, and weighted-average calculations based on the regional τ labels. A portion of the NACC dataset used for internal testing, along with data from the ADNI and HABS cohorts for external validation, contributed to generating these results.

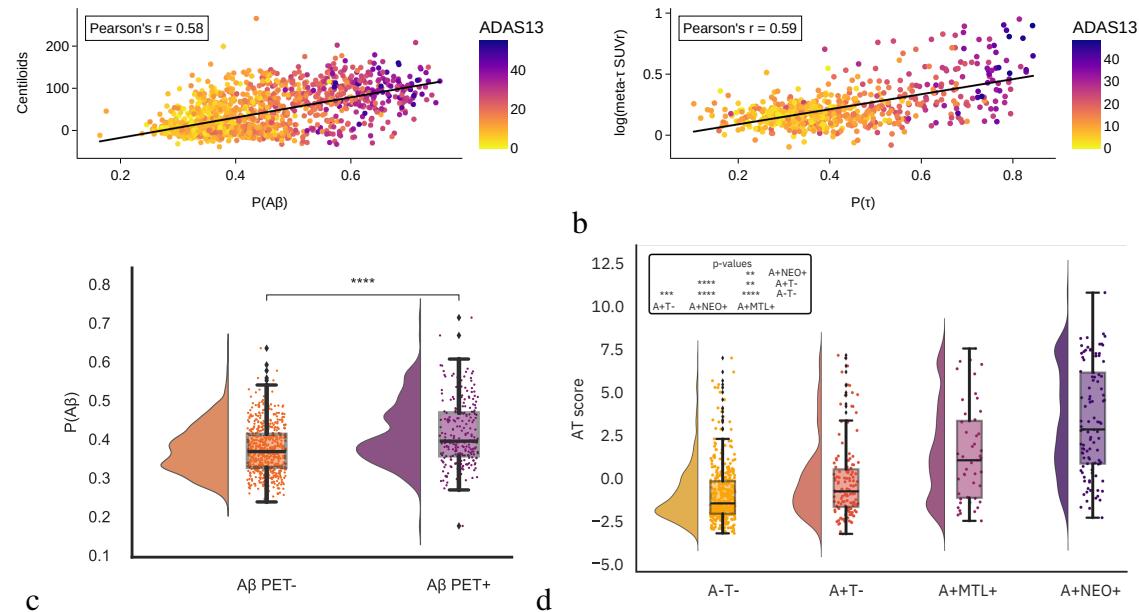


Figure 3: Model alignment with biological outcomes. (a) The bubble plot illustrates the model-predicted probabilities of amyloid PET positivity, $P(A\beta)$, over centiloid values. The Pearson's correlation coefficient was used to assess the strength of the relationship between the model's probabilities and centiloids ($n = 1392$, $r = 0.58$, $p = 4.04 \times 10^{-124}$). The color scale indicates participants' scores on the ADAS-Cog 13 task, a clinical tool for staging AD symptoms that was not provided as input to the model. (b) Model-predicted probabilities of tau PET positivity, $P(\tau)$, are shown over log-transformed SUVr values in the meta-temporal region. The Pearson's correlation test was used to assess the relationship between the model probabilities and the log of meta- τ SUVr values ($n = 619$, $r = 0.59$, $p = 2.35 \times 10^{-58}$). Similarly, each data point is colored by ADAS-Cog 13 scores. Detailed statistical results can be found in Tables S14. (c) In a subset of cognitively unimpaired cases, we compared $P(A\beta)$ between true $A\beta$ PET negative ($n = 590$) and $A\beta$ positive ($n = 245$) groups. A one-sided Mann-Whitney test indicated that model predicted probabilities were significantly lower for $A\beta$ PET negative cases ($U = 50727$, $p = 5.60 \times 10^{-12}$). (d) The rainclouds plot illustrates the relationship between a composite score of model-predicted probabilities for $A\beta$ and regional τ positivity against PET-defined disease stages. A Kruskal-Wallis H test, followed by post hoc Dunn's testing with the Holm-Bonferroni correction revealed significant differences among cases in the A-T- ($n = 411$), A+T- ($n = 139$), A+MTL+ ($n = 47$), and A+NEO+ ($n = 101$) groups ($H = 180.73$, $p = 6.15 \times 10^{-39}$). Pair-wise post hoc results are provided in Supplementary Table S16. Cases from the ADNI cohort were used to generate the results shown in panels a-b and cases from both ADNI and HABS were used to generate results in panels c-d.

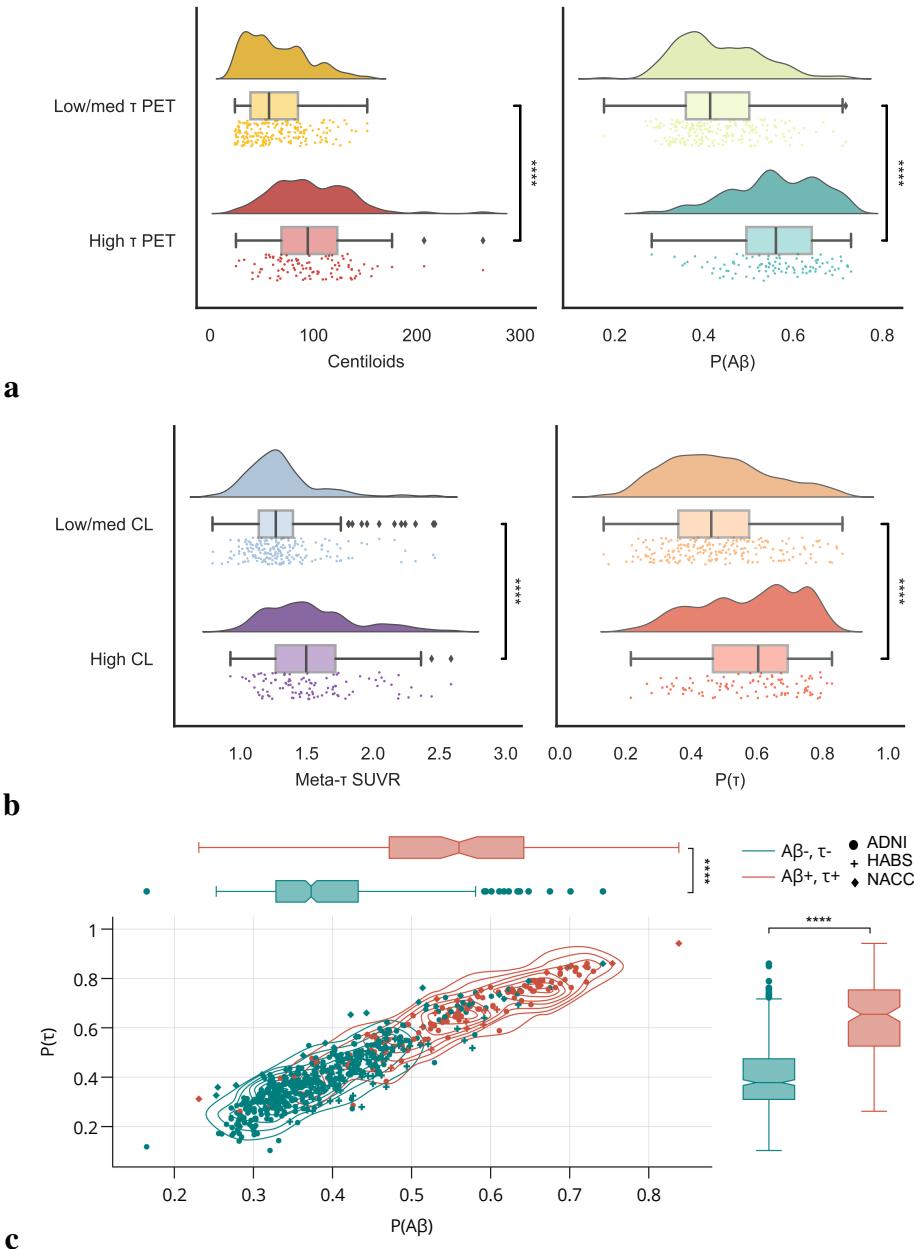


Figure 4: Model ability to capture the synergistic relationship between $A\beta$ and τ pathologies. (a) The panel on the left serves as a reference and shows the differences in centiloid distribution in PET-estimated $A\beta$ + individuals across low/medium ($n = 202$) and high ($n = 102$) τ PET groups, with the one-sided Mann-Whitney U test indicating significant differences across τ groups ($U = 5047, p = 1.92 \times 10^{-13}$). The panel on the right shows the comparisons of our model's predicted probabilities of $A\beta$ + cases across the same τ PET groups ($U = 3707, p = 4.01 \times 10^{-20}$). (b) The left panel shows the comparison of meta-temporal tau SUVR (meta- τ SUVR) across low/medium ($n = 203$) and high ($n = 101$) centiloid (CL) groups in $A\beta$ + cases, with the one-sided Mann-Whitney U test pointing to significant differences across CL groups ($U = 5876, p = 6.78 \times 10^{-10}$). The right panel illustrates the differences in model predicted probabilities across the same CL groups ($U = 6655.5, p = 3.17 \times 10^{-7}$). Cases from the ADNI ($n = 252$) and HABS ($n = 52$) test set were used for rainclouds plots a and b. Detailed statistical tests and results for the data presented in panels a and b can be found in Supplementary Table S17. (c) Kernel density plots comparing model-predicted probabilities of $A\beta$ and τ in two distinct A/T profiles ($A\beta +, \tau +$ and $A\beta -, \tau -$), are shown in cases from ADNI, denoted by circles, HABS, denoted by cross symbols, and the held-out NACC* set, denoted by diamond symbols. The color of the points, contour lines and boxplots indicates PET-estimated $A\beta +, \tau +$ (in red, $n = 139$) and $A\beta -, \tau -$ (in green, $n = 500$) groups. A one-sided Mann-Whitney U test indicated significant differences in $P(A\beta)$ between negative and positive groups ($n = 639, U = 61430, p = 5.71 \times 10^{-44}$) and similarly in $P(\tau)$ between negative and positive groups ($n = 639, U = 60963, p = 1.63 \times 10^{-42}$). All boxplots include a box presenting the median value and interquartile range (IQR), with whiskers extending from the box to the maxima and minima no further than a distance of 1.5 times the IQR. In all the panels, significance levels are denoted as ** for $p < 0.01$; *** for $p < 0.001$; and **** for $p < 0.0001$.

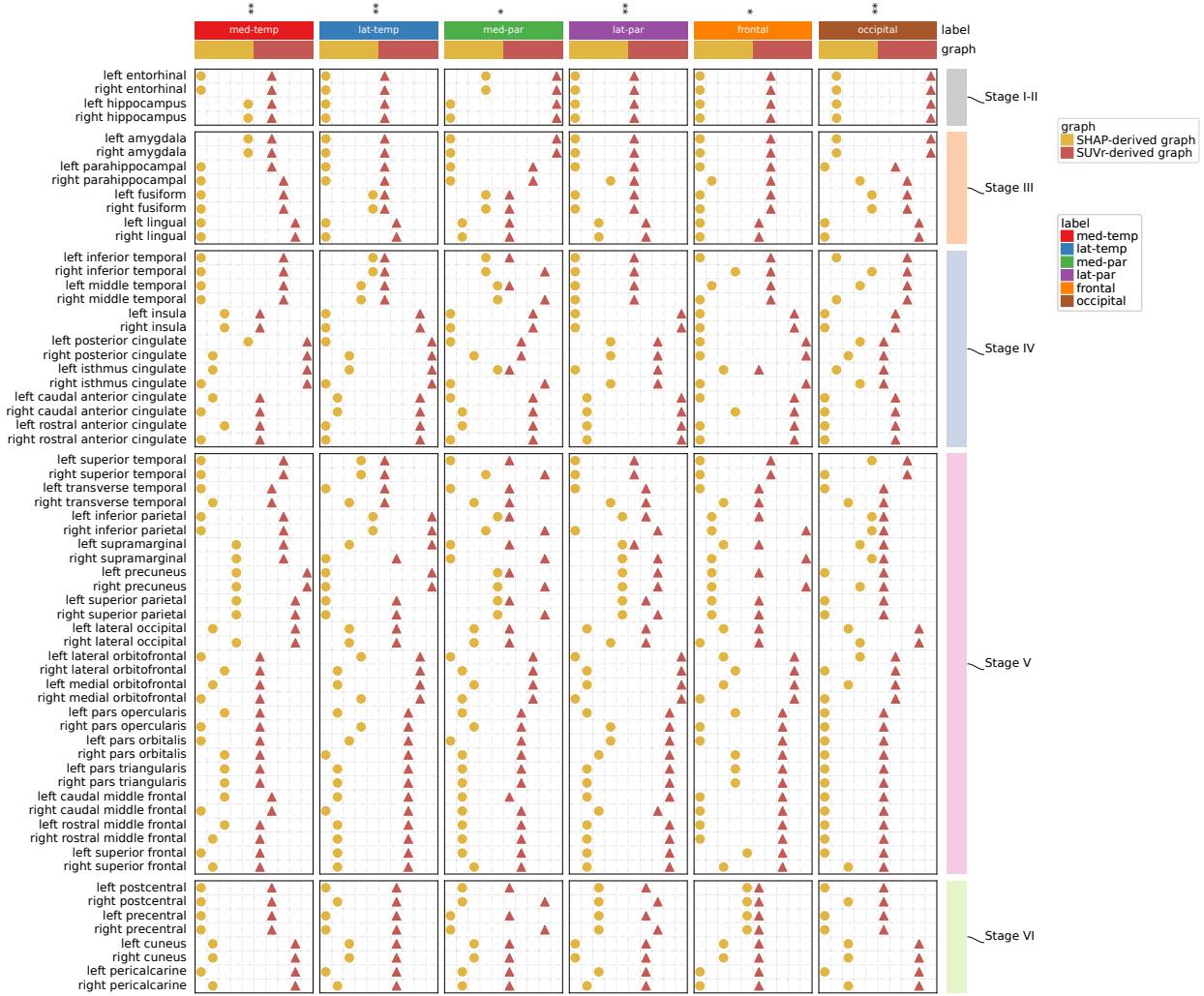


Figure 5: Communities detected from model predictions-driven and tau SUVR-derived graph networks. The dot heatmap visualizes the detected communities within the graph network constructed from normalized mutual information (NMI): one based on Shapley values of T1-weighted regional volumetric features, and the other based on tau PET SUVR within true positive cases. For each of the six regional labels (medial temporal (med-temp), lateral temporal (lat-temp), medial parietal (med-par), lateral parietal (lat-par), frontal, and occipital), communities derived from Shapley values of volumetric features are denoted by yellow dots, and communities derived from tau SUVR are denoted by red up-pointing triangles, with all dots or triangles in the same column as one detected community within the associated graph. Communities are order-invariant. Brain regions are grouped into pre-defined Braak stages (I-II, III, IV, V, and VI) shown on the right for visualization purposes. Statistical annotations denote the results of spatial permutation *t*-tests on the similarity between model-based and tau SUVR-derived communities evaluated by the adjusted mutual information (AMI). Significance levels are denoted as * for $p < 0.05$ and ** for $p < 0.01$.

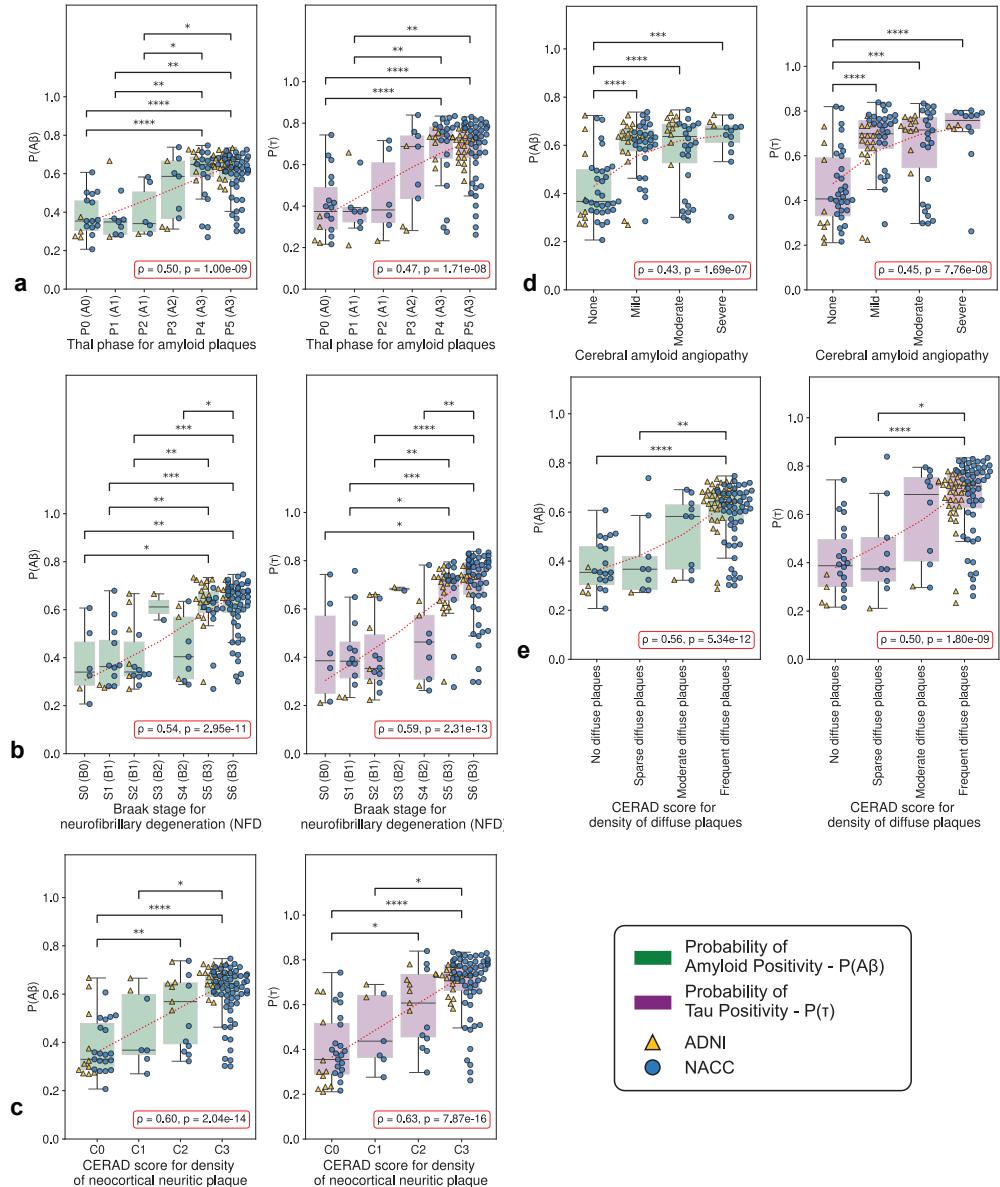


Figure 6: Model alignment with postmortem findings. The figure shows five panels (a-e) displaying predicted probabilities of amyloid-beta positivity ($P(A\beta)$) and tau positivity ($P(\tau)$) across various neuropathological grades. Panel (a) shows Thal phase for amyloid plaques, panel (b) shows Braak stage for neurofibrillary degeneration (NFD), panel (c) shows CERAD score for density of neocortical neuritic plaque, panel (d) shows cerebral amyloid angiopathy, and panel (e) shows CERAD score for density of diffuse plaques. Each panel includes a red box indicating the Spearman correlation coefficient ρ and associated p-value for the overall strength of the correlation between model probabilities and neuropathological grades. The figure legend specifies the magenta and green shades representing $P(A\beta)$ and $P(\tau)$, respectively, as well as the yellow triangle marker and blue circle marker indicating patients from the ADNI ($n = 41$) and NACC ($n = 147$) neuropathological validation cohorts, respectively. Each boxplot includes a box presenting the median value and interquartile range (IQR), with whiskers extending from the box to the maxima and minima no further than a distance of 1.5 times the IQR. Detailed statistics regarding median values and IQRs can be found in S18 and specific statistics and p-values for Spearman correlation and Kruskal-Wallis tests can be found in S19.

Extended data

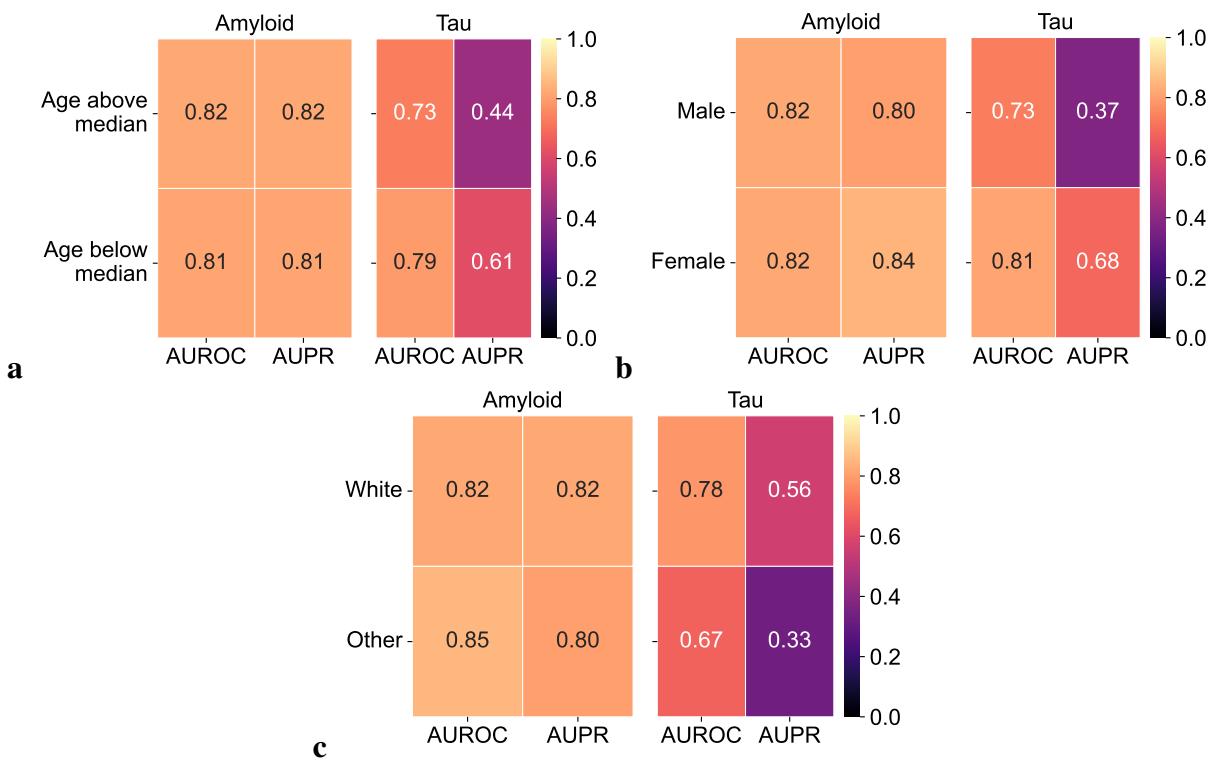
Metric	A β label	Meta- τ label
Accuracy	0.68	0.82
Balanced Accuracy	0.68	0.76
Precision	0.62	0.52
Sensitivity/Recall	0.77	0.67
Specificity	0.59	0.85
F1 score	0.69	0.59
MCC	0.37	0.48
AUC (ROC)	0.79	0.84
AUC (PR)	0.78	0.60
NPV	0.75	0.92

(a)

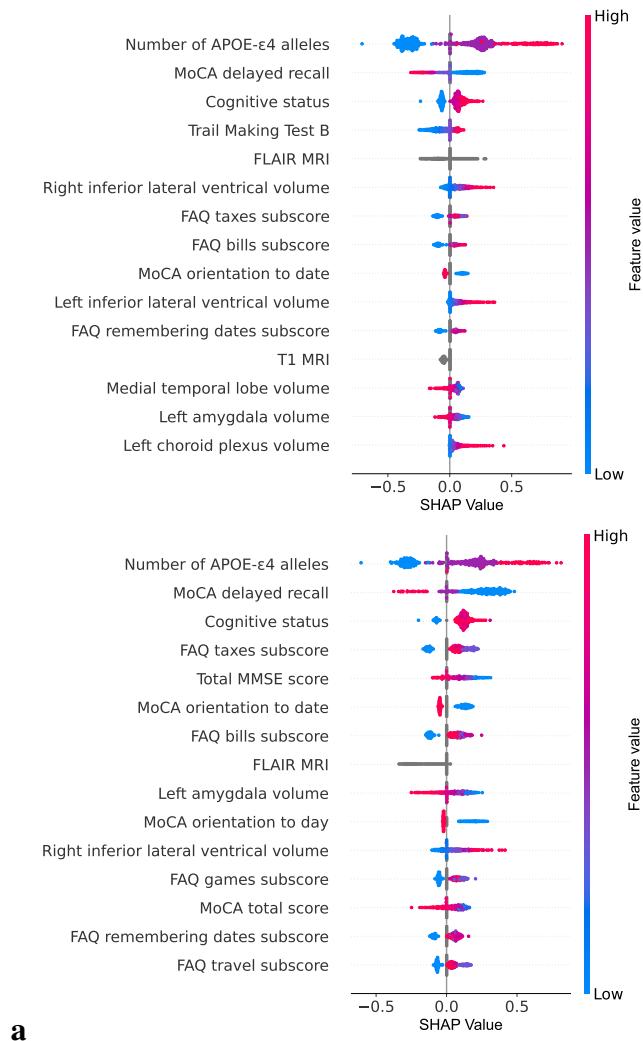
Metric	$\tau_{\text{med-temporal}}$	$\tau_{\text{lat-temporal}}$	$\tau_{\text{med-parietal}}$	$\tau_{\text{lat-parietal}}$	τ_{frontal}	$\tau_{\text{occipital}}$
Accuracy	0.68	0.75	0.84	0.82	0.76	0.80
Balanced Accuracy	0.71	0.74	0.72	0.72	0.61	0.78
Precision	0.43	0.33	0.27	0.31	0.24	0.23
Sensitivity/Recall	0.75	0.72	0.58	0.60	0.42	0.76
Specificity	0.66	0.76	0.87	0.84	0.81	0.80
F1 score	0.55	0.45	0.37	0.40	0.31	0.36
MCC	0.36	0.36	0.32	0.33	0.18	0.34
AUC (ROC)	0.79	0.83	0.82	0.79	0.71	0.84
AUC (PR)	0.60	0.50	0.37	0.39	0.30	0.37
NPV	0.89	0.94	0.96	0.95	0.90	0.98

(b)

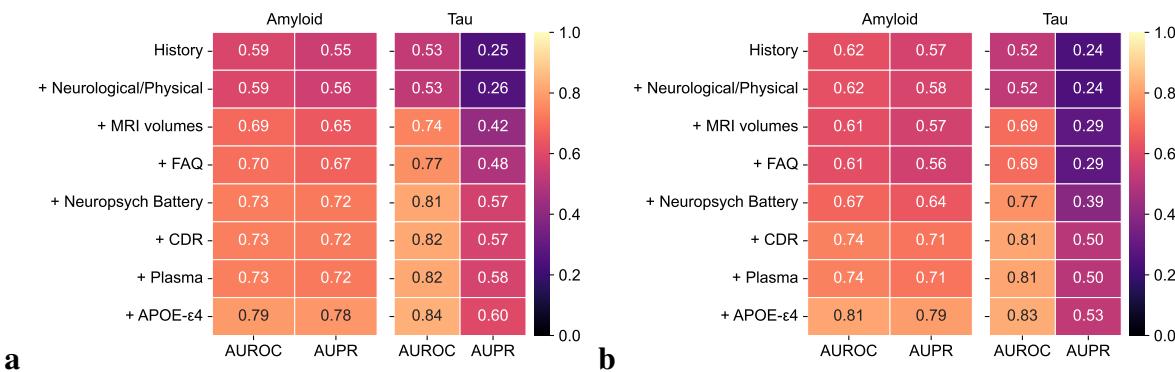
Extended Table 1: Model performance. Performance metrics for A β and τ labels on the combined ADNI (A β : $n = 1404$, τ : $n = 625$), HABS (A β : $n = 282$, τ : $n = 173$) and NACC* (A β : $n = 147$, τ : $n = 45$) cohorts are shown. Table (a) presents the performance metrics for A β and meta- τ labels, and table (b) presents the performance metrics for the regional τ labels. Note that all available data from ADNI and HABS, and a held-out set from NACC were used for model testing.



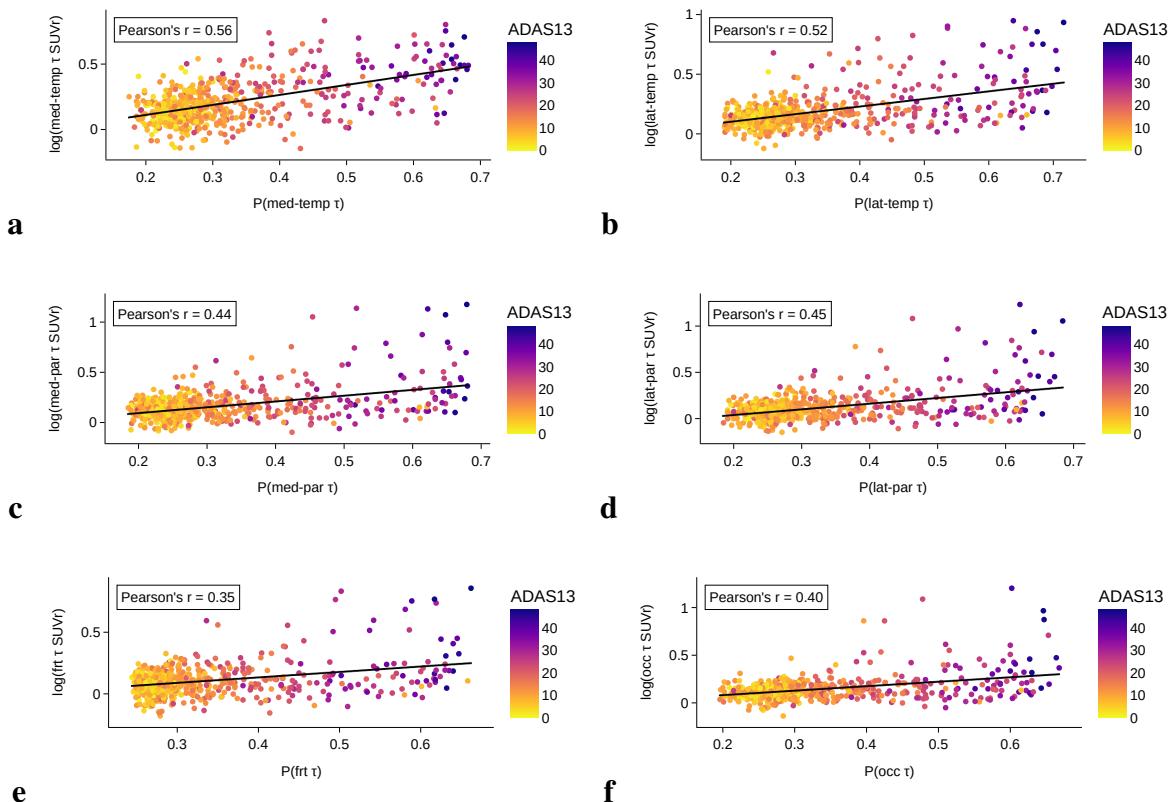
Extended Figure 1: Model performance across demographic subgroups. (a) Area under the receiver operating characteristic (ROC) and precision-recall (PR) curves for $\text{A}\beta$ and meta- τ predictions in individuals younger than 73 years ($\text{A}\beta: n = 917, \tau: n = 415$) and those aged 73 years and older ($\text{A}\beta: n = 916, \tau: n = 428$). The median age of the testing population is 73 years. (b) Area under the ROC and PR curves for $\text{A}\beta$ and meta- τ predictions stratified by age groups: individuals younger than 73 years ($\text{A}\beta: n = 917, \tau: n = 415$) and those aged 73 years and older ($\text{A}\beta: n = 916, \tau: n = 428$). The median age of the testing population is 73 years. (c) Area under the ROC and PR curves for $\text{A}\beta$ and meta- τ predictions stratified by sex: (a, b) individuals identified as male ($\text{A}\beta: n = 905, \tau: n = 387$) and (c, d) individuals identified as female ($\text{A}\beta: n = 928, \tau: n = 456$).



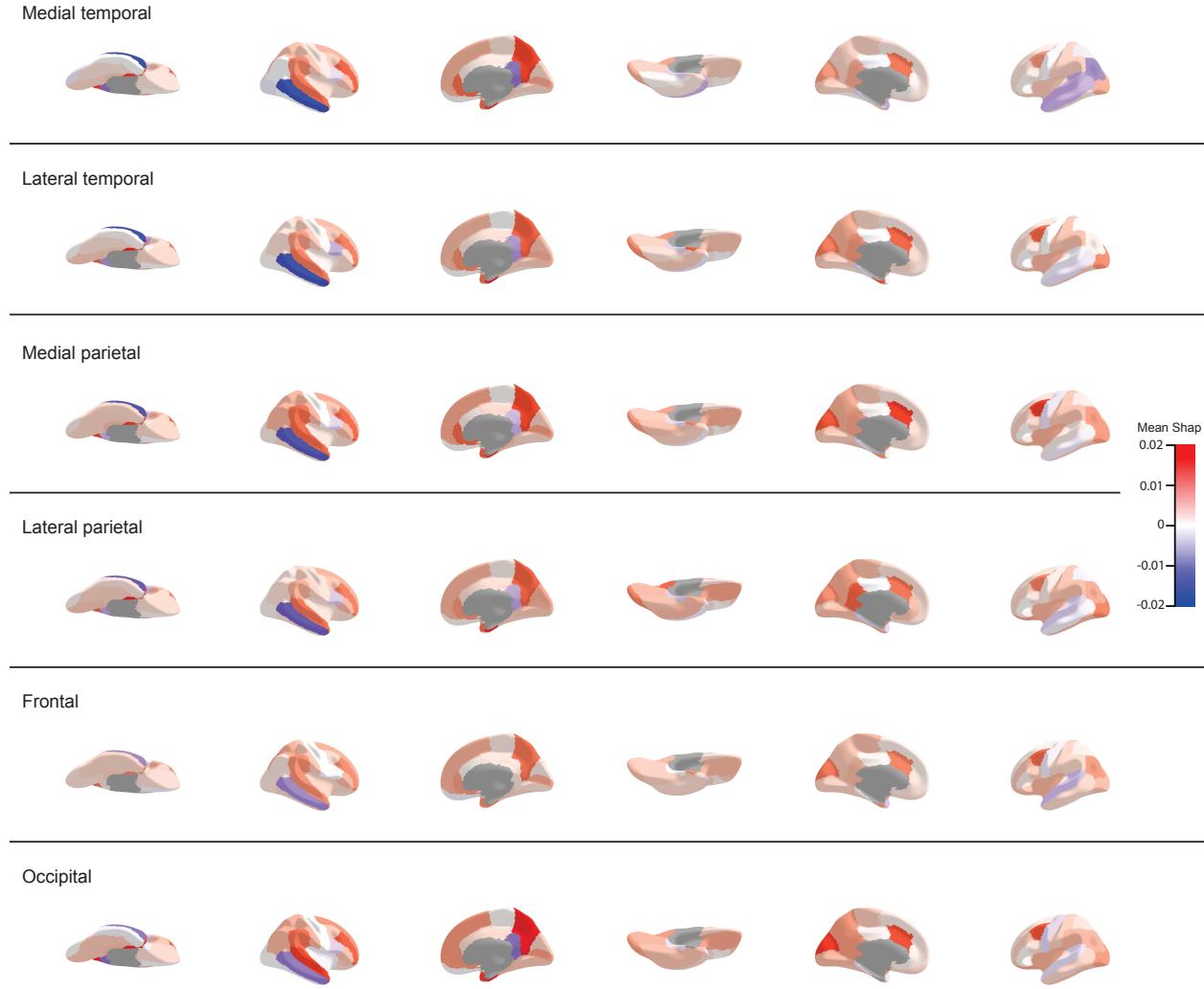
Extended Figure 2: Shapley analysis. The figure presents the top fifteen contributing features for the model's positive predictions of (a) A β and (b) τ labels, ranked by their mean Shapley values. These values, which represent the average contribution of each feature to the model's decision, were used to rank the features from highest to lowest impact.



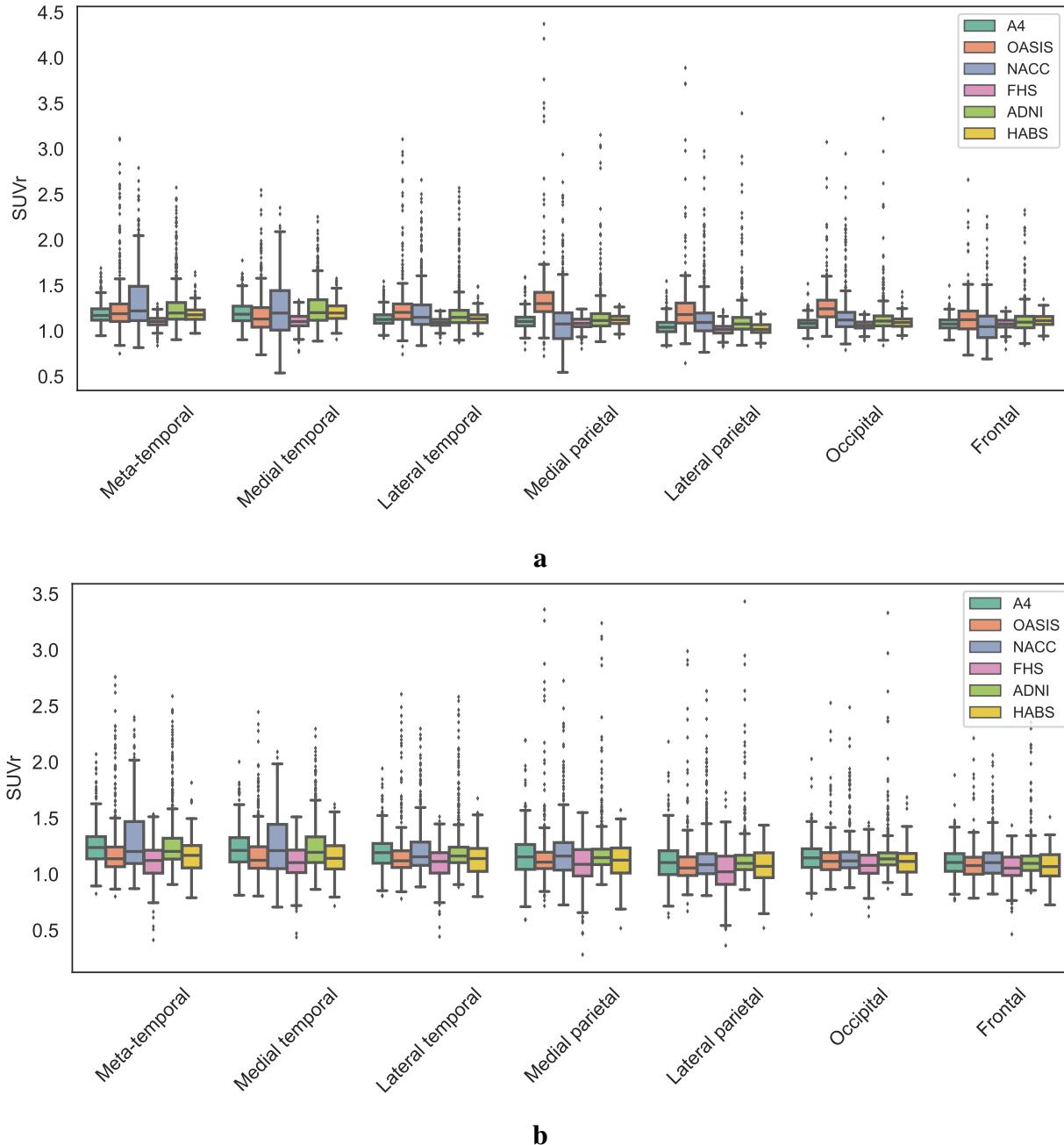
Extended Figure 3: AUROC and AUPR performance using incremental clinical features. Heatmap presenting the AUROC and AUPR values for A β and meta- τ predictions using various combinations of clinical features for (a) our model without image embeddings (b) CatBoost.



Extended Figure 4: Regional tau model's alignment with biological outcomes. The bubble plots illustrate model-predicted probabilities of regional τ positivity with the respective regional τ PET SUVR values. SUVR values were log transformed before computing Pearson's r correlations. Detailed statistics are reported in Table S15, including Pearson's and Spearman's correlation coefficients with p-values.



Extended Figure 5: Inflated cortical surfaces showing Shapley values of regional brain volumes for regional tau predictions. Shapley values are overlaid on the Desikan-Killiany-Tourville atlas to illustrate the relative importance of different cortical volumes in predicting regional tau positivity. The first panel displays the mean Shapley values for the medial temporal predictions and subsequent panels are ordered according to Braak stages.



Extended Figure 6: Impact of harmonization on SUVR distributions across cohorts. The top panel presents boxplots of unharmonized SUVR values for each τ PET ROI, while the bottom panel displays SUVR values after harmonization. Each box represents the distribution of SUVR within a cohort, with different colors indicating different cohorts. Harmonization reduced the batch effect of cohort-specific variability, while controlling for meaningful covariates. Detailed statistics are reported in Supplementary Tables S20 and S21.