

# Connectivity measures in electrophysiology

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# Measuring brain activity

ECoG

invasive

fMRI

bad temporal resolution ( $\approx 1s$ )

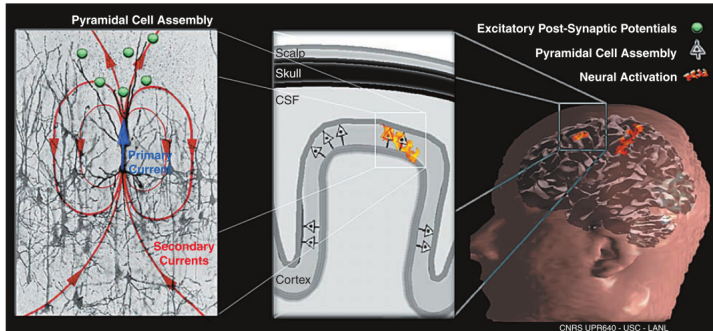
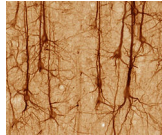
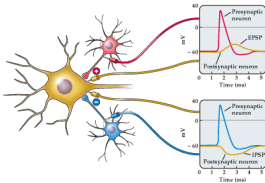
MEG

EEG



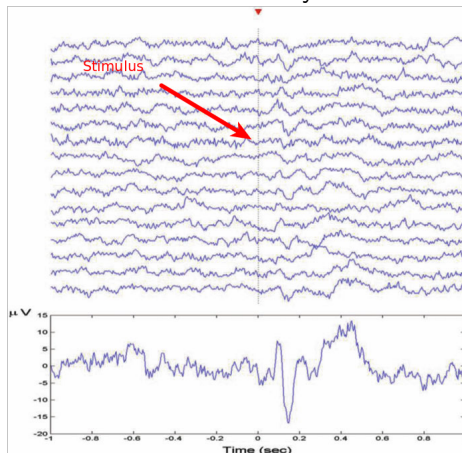
*EEG and MEG allow to measure electromagnetic brain activity directly, noninvasively and with good temporal resolution*

# Source of electrophysiological activity in MEG/EEG

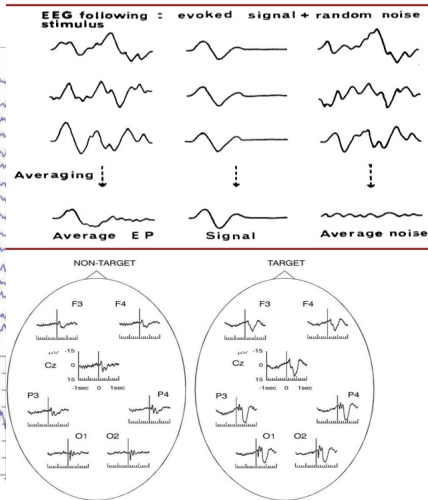


[Baillet et al., *Electromagnetic brain mapping*, 2001]

Subject is presented with stimulus repetitively while we measure his brain activity

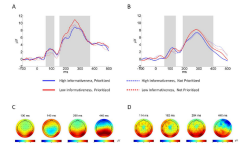
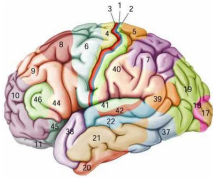


## Averaging



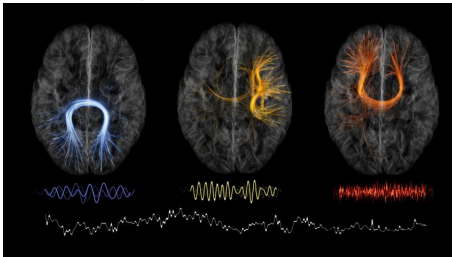
# Studying brain activity...

From evoked responses

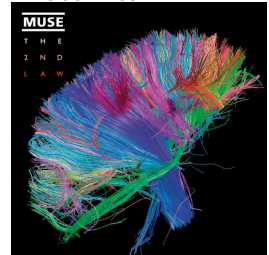


... to connectivity analysis

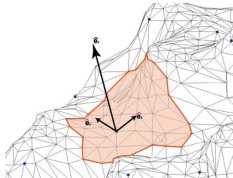
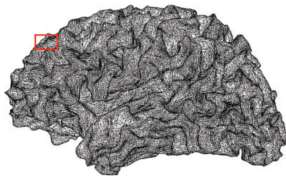
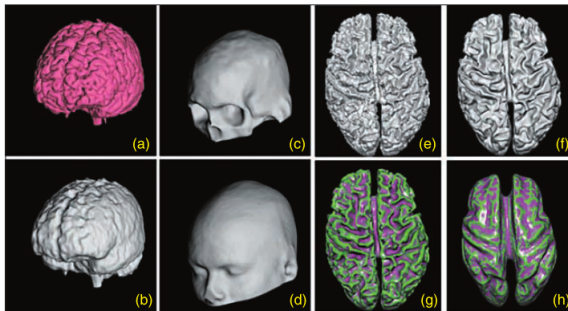
Functional / Effective



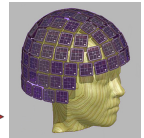
Anatomical



# Forward modeling

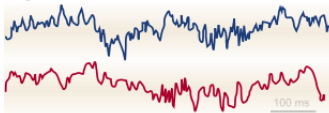


Forward  
operator:  $G$



# Studying phase synchrony

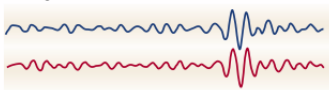
Raw signals



Band pass filter



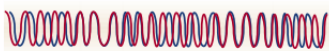
Filtered signals



Spectral analysis

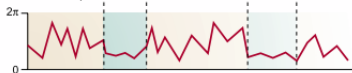


Instantaneous phase difference



Statistical identification of phase-locking synchrony

Stable phase-difference episodes

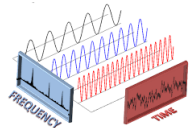


$$C_{xy}(\tau) = \int_u \hat{x}(u) \hat{y}(u - \tau) du \quad (1)$$

where  $\hat{x}$  is the zero-mean, normalized transform of  $x$  (EQN 2):

$$\hat{x}(u) = \frac{(x(u) - \langle x \rangle_{time})}{\sqrt{\int_{time} (x(u) - \langle x \rangle_{time})^2 dv}} \quad (2)$$

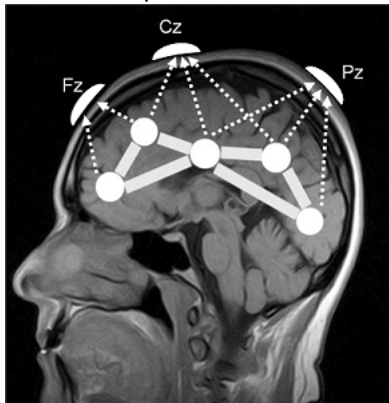
Time-frequency transform



$$\tilde{x}(f, t) = a(t) \exp(i(ft + \phi_x(t))) \quad (3)$$

$$\Phi_{xy}(t) = |n\phi_x(t) - m\phi_y(t)| \quad (4)$$

Simultaneous recording of the same brain activity on different electrodes leads to false positive detections of connectivity





## Generative model

$$\begin{aligned}\begin{pmatrix} m_1 \\ m_2 \end{pmatrix}(t) &= \begin{pmatrix} g_1^1 & g_2^1 \\ g_1^2 & g_2^2 \end{pmatrix} \begin{pmatrix} s_1 \\ s_2 \end{pmatrix}(t) = \\ &= \begin{pmatrix} g_1^1 \\ g_2^1 \end{pmatrix} s_1(t) + \begin{pmatrix} g_2^1 \\ g_2^2 \end{pmatrix} s_2(t) = \vec{g}_1 s_1(t) + \vec{g}_2 s_2(t) \quad (1)\end{aligned}$$

$m_{1,2}(t)$  - MEG/EEG measurements

$\{g_i^j\}$  - matrix of a forward model

$s_{1,2}(t)$  - unknown timeseries on cortex

## Time-frequency transformation

Apply time-frequency transform to (1)...

$$\begin{pmatrix} M_1 \\ M_2 \end{pmatrix} (f, t) = \vec{g}_1 S_1(f, t) + \vec{g}_2 S_2(f, t) \quad (2)$$

... and write cross-spectrum:

$$\mathbf{C}^{MM}(t, f) \stackrel{def}{=} \mathbf{E}\{\mathbf{M}(t, f)\mathbf{M}^H(t, f)\} \quad (3)$$

N.B.

$M_1, M_2, S_1, S_2$  after time-frequency transformation are complex

Let's substitute (2) into (3)

$$\mathbf{C}^{MM}(t, f) = \mathbf{E} \left\{ \begin{pmatrix} M_1 \bar{M}_1 & M_1 \bar{M}_2 \\ M_2 \bar{M}_1 & M_2 \bar{M}_2 \end{pmatrix} (f, t) \right\} =$$

$$\mathbf{E} \left\{ \left( \vec{g}_1 S_1(f, t) + \vec{g}_2 S_2(f, t) \right) \cdot \left( \vec{g}_1^T \bar{S}_1(f, t) + \vec{g}_2^T \bar{S}_2(f, t) \right) \right\} \quad (4)$$

Let's substitute (2) into (3)

$$\mathbf{C}^{MM}(t, f) = \mathbf{E} \left\{ \begin{pmatrix} M_1 \bar{M}_1 & M_1 \bar{M}_2 \\ M_2 \bar{M}_1 & M_2 \bar{M}_2 \end{pmatrix} (f, t) \right\} =$$

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**N.B.**

$\vec{g}_i$  are real  $\implies \vec{g}_i^H = \vec{g}_i^T$

Let's substitute (2) into (3)

$$\begin{aligned}
 \mathbf{C}^{MM}(t, f) &= \mathbf{E} \left\{ \begin{pmatrix} M_1 \bar{M}_1 & M_1 \bar{M}_2 \\ M_2 \bar{M}_1 & M_2 \bar{M}_2 \end{pmatrix} (f, t) \right\} = \\
 &\mathbf{E} \left\{ \left( \vec{g}_1 S_1(f, t) + \vec{g}_2 S_2(f, t) \right) \cdot \left( \vec{g}_1^T \bar{S}_1(f, t) + \vec{g}_2^T \bar{S}_2(f, t) \right) \right\} \\
 &= \vec{g}_1 \vec{g}_1^T \mathbf{E} \{ S_1(f, t) \bar{S}_1(f, t) \} + \vec{g}_1 \vec{g}_2^T \mathbf{E} \{ S_1(f, t) \bar{S}_2(f, t) \} + \\
 &\quad + \vec{g}_2 \vec{g}_1^T \mathbf{E} \{ S_2(f, t) \bar{S}_1(f, t) \} + \vec{g}_2 \vec{g}_2^T \mathbf{E} \{ S_2(f, t) \bar{S}_2(f, t) \} \quad (4)
 \end{aligned}$$

Let's substitute (2) into (3)

$$\begin{aligned}\mathbf{C}^{MM}(t, f) &= \\ &= \vec{g}_1 \vec{g}_1^T \mathbf{E}\{S_1(f, t) \bar{S}_1(f, t)\} + \vec{g}_1 \vec{g}_2^T \mathbf{E}\{S_1(f, t) \bar{S}_2(f, t)\} + \\ &\quad + \vec{g}_2 \vec{g}_1^T \mathbf{E}\{S_2(f, t) \bar{S}_1(f, t)\} + \vec{g}_2 \vec{g}_2^T \mathbf{E}\{S_2(f, t) \bar{S}_2(f, t)\} \quad (4)\end{aligned}$$

Finally, we've got

$$\begin{pmatrix} c_{11}^{MM} & c_{12}^{MM} \\ c_{21}^{MM} & c_{22}^{MM} \end{pmatrix} = \vec{g}_1 \vec{g}_1^T c_{11}^{SS} + \vec{g}_1 \vec{g}_2^T c_{12}^{SS} + \vec{g}_2 \vec{g}_1^T c_{21}^{SS} + \vec{g}_2 \vec{g}_2^T c_{22}^{SS} \quad (5)$$

Or in matrix form:

$$\begin{pmatrix} c_{11}^{MM} & c_{12}^{MM} \\ c_{21}^{MM} & c_{22}^{MM} \end{pmatrix} = \\
 = \begin{pmatrix} g_1^1 g_1^1 & g_1^1 g_1^2 \\ g_1^2 g_1^1 & g_1^2 g_1^2 \end{pmatrix} c_{11}^{SS} + \begin{pmatrix} g_1^1 g_2^1 & g_1^1 g_2^2 \\ g_1^2 g_2^1 & g_1^2 g_2^2 \end{pmatrix} c_{12}^{SS} + \\
 + \begin{pmatrix} g_2^1 g_1^1 & g_2^1 g_1^2 \\ g_2^2 g_1^1 & g_2^2 g_1^2 \end{pmatrix} c_{21}^{SS} + \begin{pmatrix} g_2^1 g_2^1 & g_2^1 g_2^2 \\ g_2^2 g_2^1 & g_2^2 g_2^2 \end{pmatrix} c_{22}^{SS} \quad (5)$$



Or in matrix form:

$$\begin{pmatrix} c_{11}^{MM} & c_{12}^{MM} \\ c_{21}^{MM} & c_{22}^{MM} \end{pmatrix} = \begin{pmatrix} g_1^1 g_1^1 & g_1^1 g_1^2 \\ g_1^2 g_1^1 & g_1^2 g_1^2 \end{pmatrix} c_{11}^{SS} + \begin{pmatrix} g_1^1 g_2^1 & g_1^1 g_2^2 \\ g_1^2 g_2^1 & g_1^2 g_2^2 \end{pmatrix} c_{12}^{SS} + \\ + \begin{pmatrix} g_2^1 g_1^1 & g_2^1 g_1^2 \\ g_2^2 g_1^1 & g_2^2 g_1^2 \end{pmatrix} c_{21}^{SS} + \begin{pmatrix} g_2^1 g_2^1 & g_2^1 g_2^2 \\ g_2^2 g_2^1 & g_2^2 g_2^2 \end{pmatrix} c_{22}^{SS} \quad (5)$$

## Signal leakage

Drop the real part of this equation away [Nolte et al., 2004] to deal with true connectivity only

Or in matrix form:

$$\begin{pmatrix} c_{11}^{MM} & c_{12}^{MM} \\ c_{21}^{MM} & c_{22}^{MM} \end{pmatrix} = \begin{pmatrix} g_1^1 g_1^1 & g_1^1 g_1^2 \\ g_1^2 g_1^1 & g_1^2 g_1^2 \end{pmatrix} c_{11}^{SS} + \begin{pmatrix} g_1^1 g_2^1 & g_1^1 g_2^2 \\ g_1^2 g_2^1 & g_1^2 g_2^2 \end{pmatrix} c_{12}^{SS} + \\ + \begin{pmatrix} g_2^1 g_1^1 & g_2^1 g_1^2 \\ g_2^2 g_1^1 & g_2^2 g_1^2 \end{pmatrix} c_{21}^{SS} + \begin{pmatrix} g_2^1 g_2^1 & g_2^1 g_2^2 \\ g_2^2 g_2^1 & g_2^2 g_2^2 \end{pmatrix} c_{22}^{SS} \quad (5)$$

## Signal leakage

Drop the real part of this equation away [Nolte et al., 2004] to deal with true connectivity only

# DICS algorithm [Gross et al., 2001]

We want to estimate coherence of two cortical sources:

$$\mathbf{M}_{i,j}(f) = \frac{|\mathbf{C}_{i,j}(f)|^2}{\mathbf{C}_{i,i}(f)\mathbf{C}_{j,j}(f)}. \quad [1]$$

Beamformer: construct a spatial filter which passes activity from source  $r$  with unit gain while suppressing activity coming from other sources

$$\min[\mathcal{E}\{\|\mathbf{AD}\|^2\} + \alpha\|\mathbf{A}\|^2] \quad \text{subject to } \mathbf{AL}(\mathbf{r}) = \mathbf{I}, \quad [2]$$

Where  $D$  - time-frequency-transformed data

$L(r)$  - forward problem solution for two orthogonal tangential dipoles at  $r$

$A$  - inverse operator (we want to find it)

Solve minimization problem:

$$\mathbf{A}(\mathbf{r},f) = (\mathbf{L}^T(\mathbf{r})\mathbf{C}_r(f)^{-1}\mathbf{L}(\mathbf{r}))^{-1}\mathbf{L}^T(\mathbf{r})\mathbf{C}_r(f)^{-1}, \quad [3]$$

with  $\mathbf{C}_r(f) = \mathbf{C}(f) + \alpha\mathbf{I}$ , where  $\mathbf{C}(f)$  is the cross spectral density matrix at frequency  $f$  or averaged across a frequency band centered at  $f$ , and superscript  $T$  indicates the matrix transpose.

$$\mathbf{C}_s(\mathbf{r}_1, \mathbf{r}_2, f) = \mathbf{A}(\mathbf{r}_1, f)\mathbf{C}(f)\mathbf{A}^{*T}(\mathbf{r}_2, f). \quad [4]$$

$$\mathbf{P}(\mathbf{r}, f) = \mathbf{C}_s(\mathbf{r}, \mathbf{r}, f). \quad [5]$$

$$c_s(\mathbf{r}_1, \mathbf{r}_2, f) = \lambda_1\{\mathbf{C}_s(\mathbf{r}_1, \mathbf{r}_2, f)\}, \quad [7]$$

where  $\lambda_1\{\}$  indicates the larger singular value of the expression in braces.

Analogously, the power in the dominant direction is

$$p(\mathbf{r}, f) = \lambda_1(\mathbf{P}(\mathbf{r}, f)), \quad [8]$$

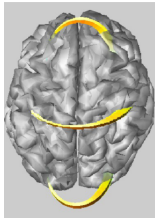
and we obtain the coherence from Eqs. 7 and 8 as

$$M(\mathbf{r}_1, \mathbf{r}_2, f) = \frac{|c_s(\mathbf{r}_1, \mathbf{r}_2, f)|^2}{p(\mathbf{r}_1, f)p(\mathbf{r}_2, f)}. \quad [9]$$

Apply the imaginary coherence idea to DICS:

$$C_s(r_1, r_2, f) = \text{Im}(A(r_1, f)C(f)A^{*T}(r_2, f))[4^*]$$

To evaluate algorithm performance we simulate MEG recordings with three networks active across trial



- 1 We add artificial brain noise
- 2 ... and sensor noise
- 3 Networks are active with different time profiles
- 4 Signal to noise ratio and phase lag are varied during the experiment