

Cancer Detection in Full Field Optical Coherence Tomography Images

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December 7th, 2022

A Multidisciplinary Project

Cancer Diagnosis

rapid tissue analysis

Label-free Imaging

- Full-Field Optical Coherence Tomography (*FFOCT*)
- Dynamic Cell Imaging (*DCI*)



Image Analysis

- exploratory data analysis
- aid-to-diagnosis

Enable use of novel imaging technique for cancer diagnosis via data analysis.

Clinical Context

- **Cancer** – one of the leading cause of death worldwide
- Gold standard for diagnosis is **tissue analysis / histopathology**
- Standard histopathology is **time consuming, labor intensive**
- A need for rapid diagnosis in **interventional** settings
- Pathologists **shortage**

Fix

Embed

Slice

Stain

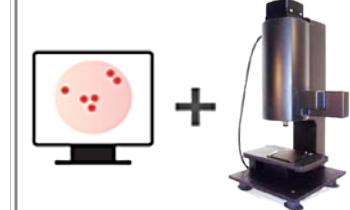
Visualize

Diagnose

Fresh
Tissue

Optical
Slicing

Endogenous
Contrast



novel technique

special training

Gold standard histology



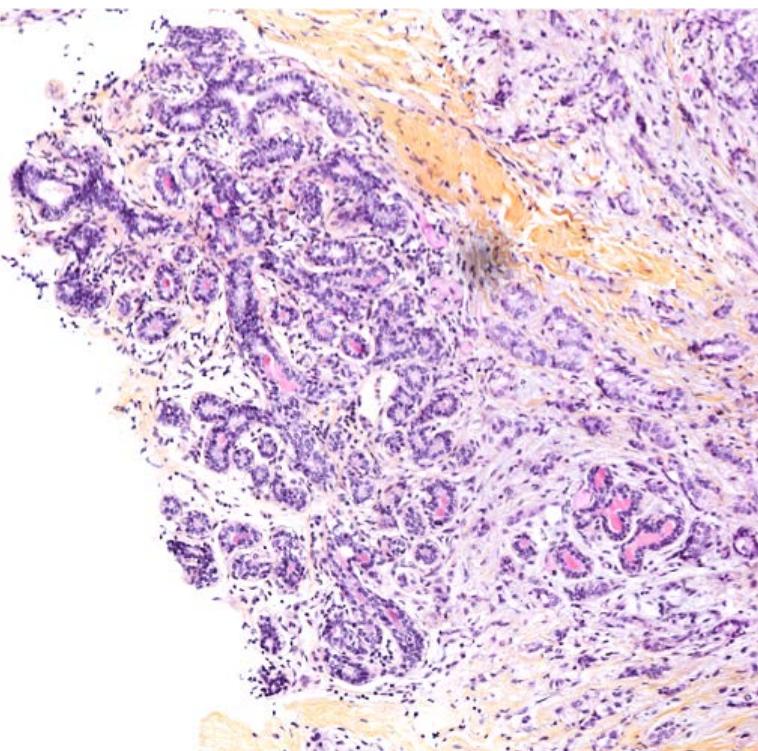
Label-free imaging



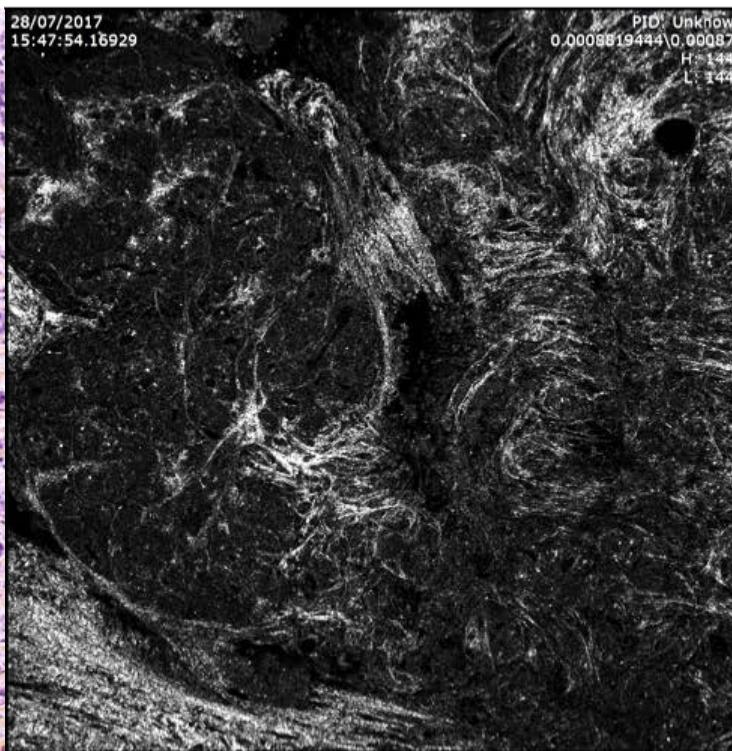
Medical personnel needs training to interpret new contrast.

Imaging Context

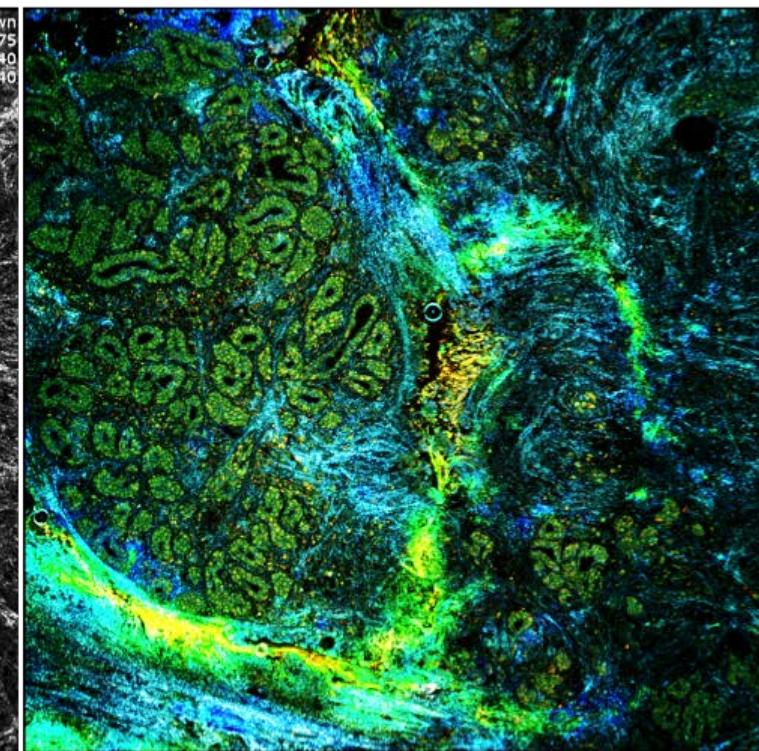
H&E Histology



Full-Field Optical Coherence
Tomography **FFOCT**



Dynamic Cell Imaging **DCI**



normal breast lobule

Full-Field Optical Coherence Tomography FFOCT

FFOCT = *en face* OCT

Optical setup : Michelson interferometer

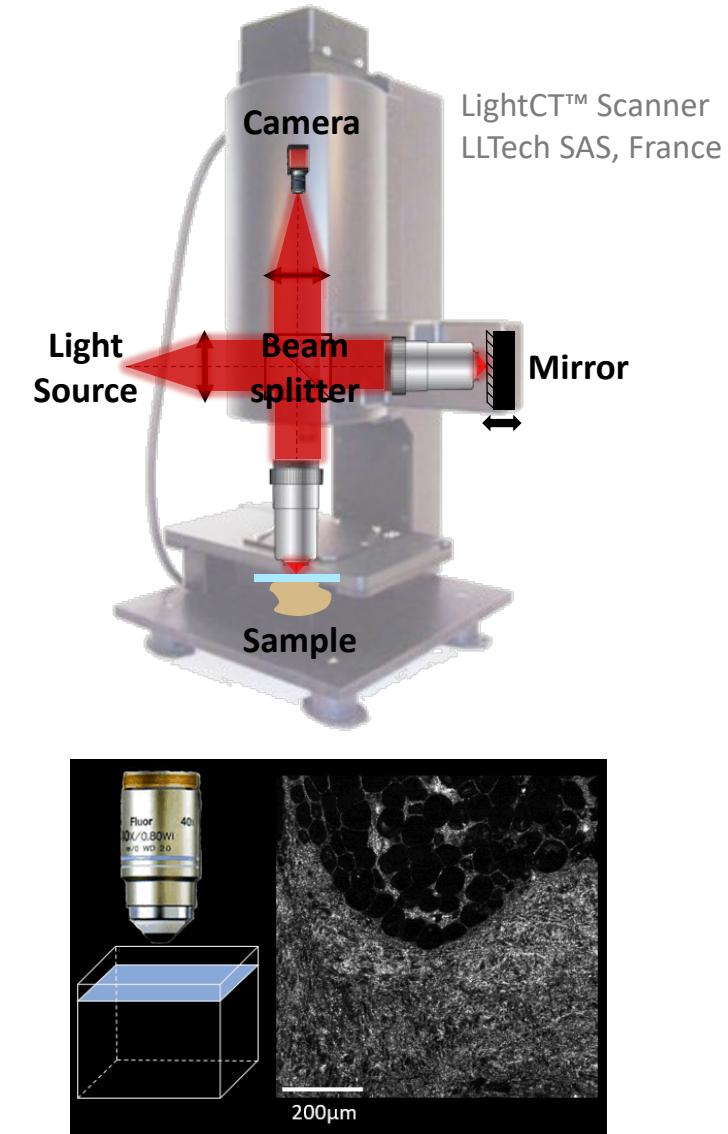
Light interferometry principle :

identical waves amplify when in phase, cancel when not

Low coherence interferometry:

large bandwidth = short coherence length \propto Z resolution

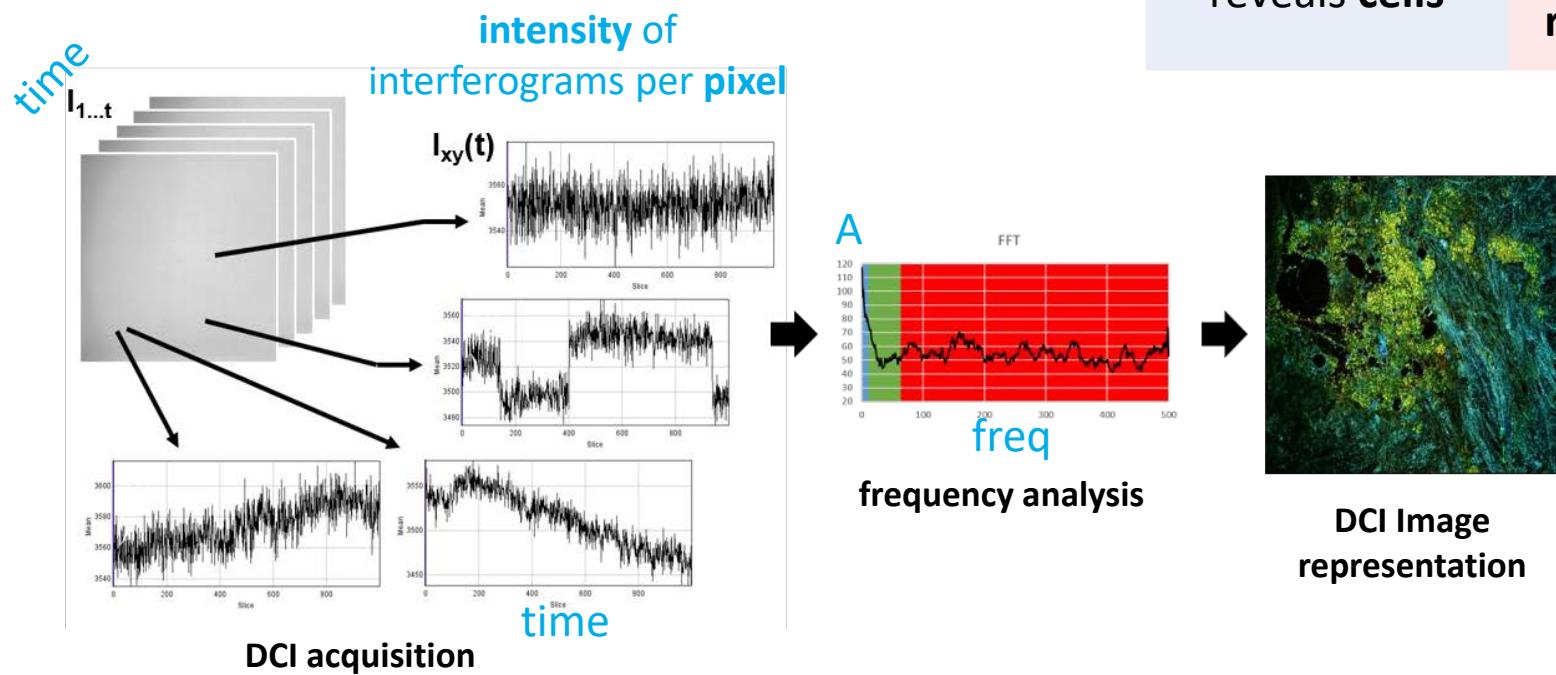
PROS	CONS
good resolution (1μm)	no cell information
fast (seconds)	
reveals fibers	



Dynamic Cell Imaging DCI

- overcomes **strong** signal from *fibers* and reveals **active** intra-cellular structures
- captures confined micro-displacements of scatterers
- from *10ms Brownian* to *6s migration*
- origin of signal presumably *glycolysis* → live tissue

PROS	CONS
good resolution ($1\mu\text{m}$)	motion artefacts
fast (minutes)	variable fiber contrast
reveals cells	image representation



Methodology Outline

Can we **extract** more info from DCI signal ?

What can we learn from DCI images ?

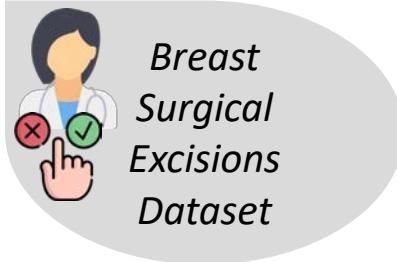
Can we learn fiber representation in DCI from FFOCT ?

Can DCI be **routinely** used in **clinical** applications ?

Data Exploration

DCI Signal

- Source separation



DCI Images

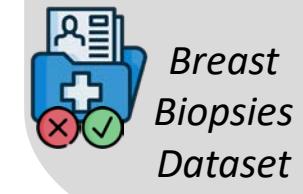
- Fully-supervised classification

Multi-modality

- FFOCT/DCI cross-modal representation learning

Clinical application

- Multiple Instance Learning classification



Breast Surgical Excisions Dataset

Goal : feasibility study to discern **pathological** from **healthy** tissue in DCI

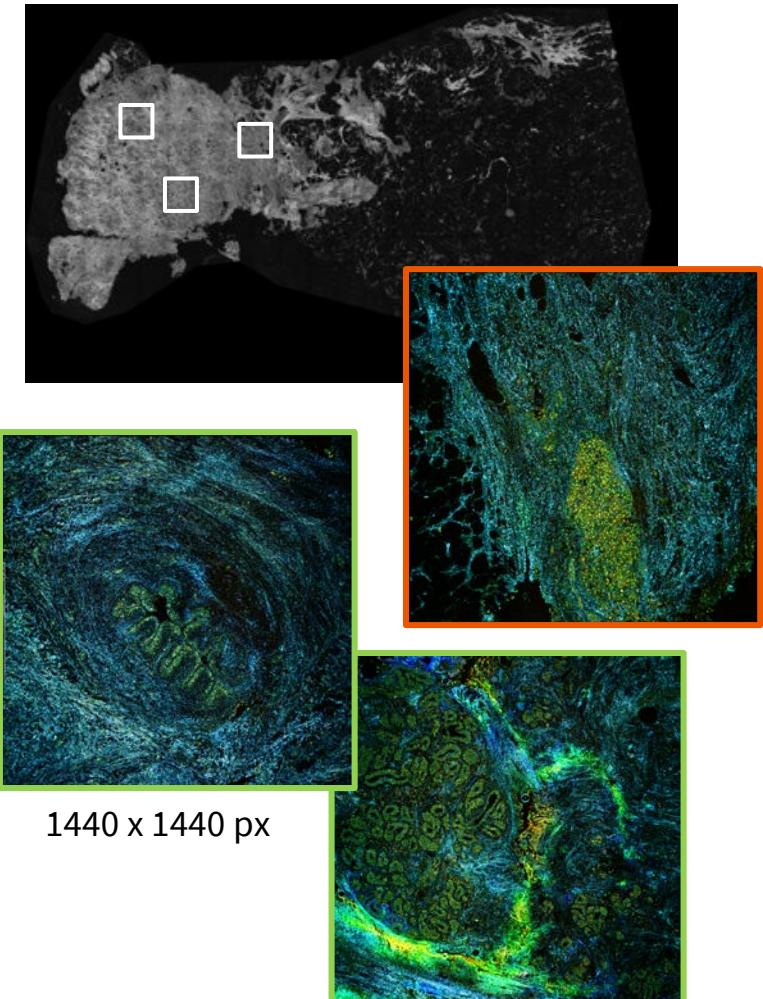
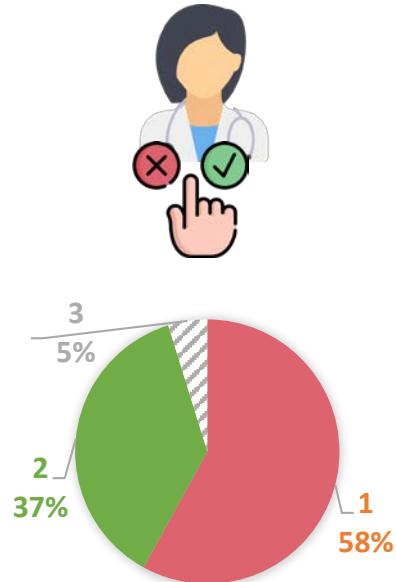
Cohort :

- 33 patients, **mastectomies**
- 47 samples, 11 **healthy** and 36 **tumoral**
- several ROIs per sample ~10 (3 to 16) ROIs / sample

Diagnostic : per ROI with H&E correlations, by pathologist

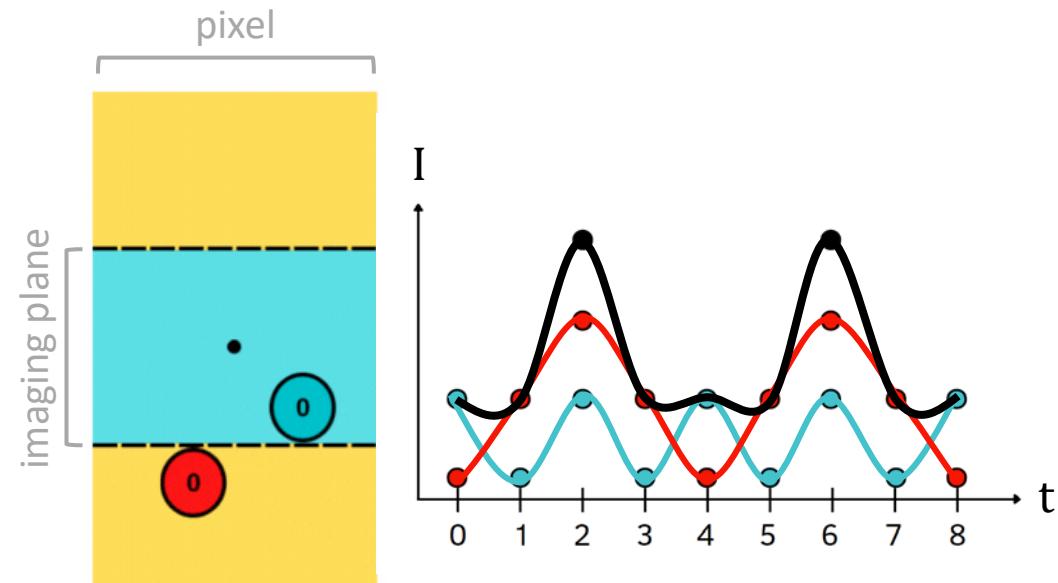
Dataset :

- ROIs:
 - 279 cancer
 - 179 normal
 - 23 uncertain



1 Exploring DCI Signal

- Hypothesis**
- multiple **oscillatory behaviors** present
 - **overlapping** scatterers per pixel
- Strategy**
- signal separation



Two scatterers moving inside a pixel relative to the focal plane & the acquired pixel intensity

$$I(t) = I_1(t) + I_2(t)$$

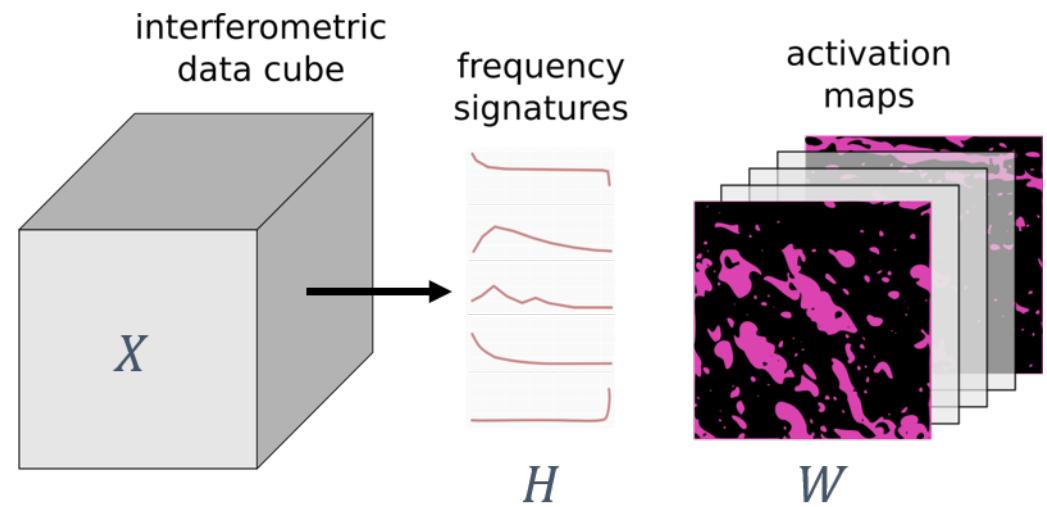
1 Exploring DCI Signal

Signal Separation

- recover the **independent** component signals from a **mixture** signal
- non-negative matrix factorization (**NMF**)

$$\min_{W \in \mathbb{R}^{n \times k}, H \in \mathbb{R}^{k \times f}} \|X - WH\|_F^2 \text{ s.t. } W \geq 0, H \geq 0$$

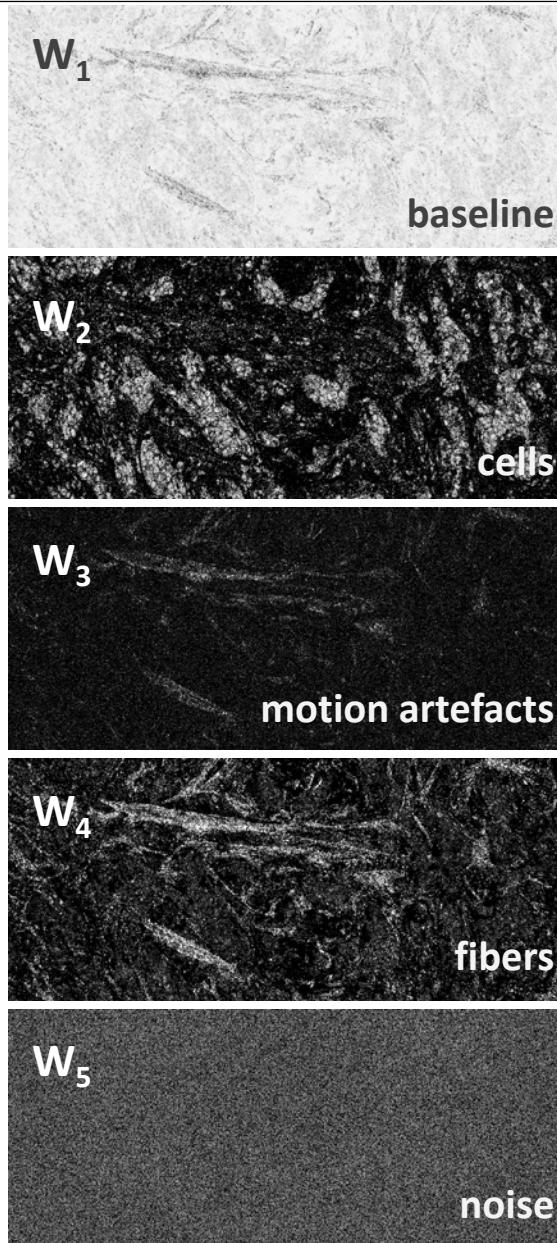
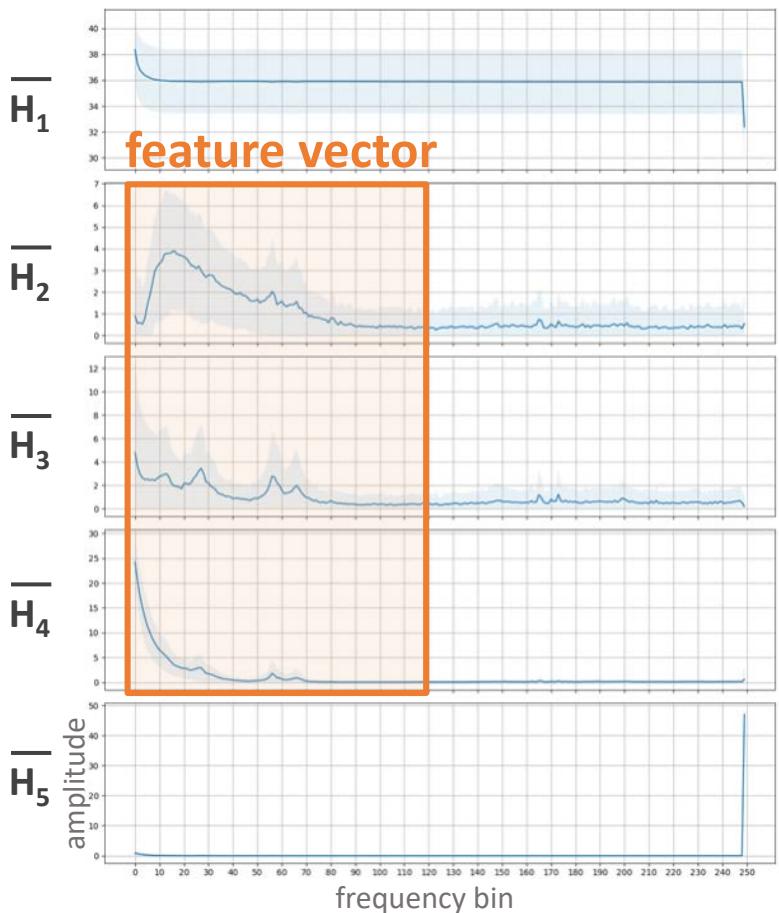
- positive **part-based** decomposition
- **dynamic** and **spatial** components
- empiric choice or rank $k = 5$



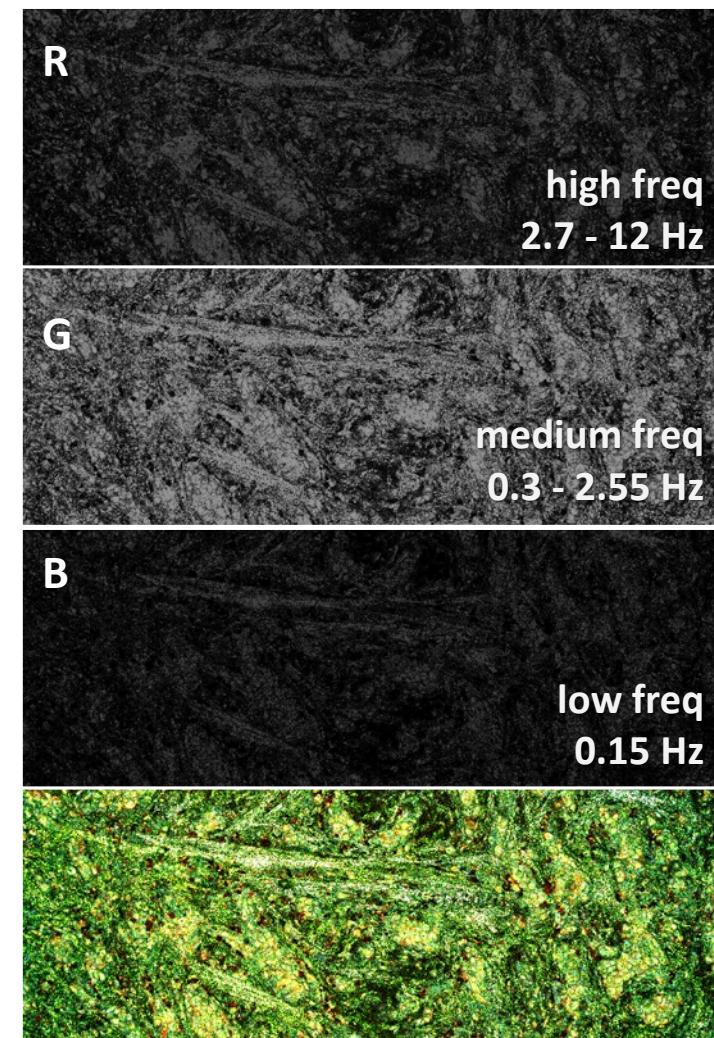
1 Exploring DCI Signal NMF Decomposition Results

$$X \approx WH$$

NMF dynamic and spatial components



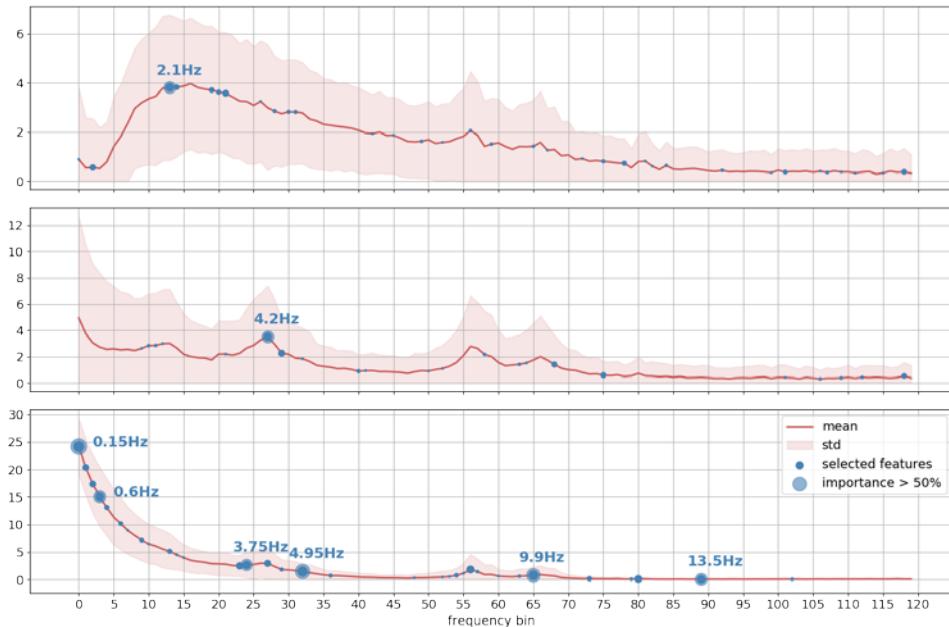
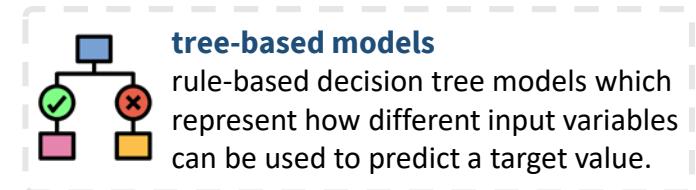
DCI processed image and RGB channels



1 Exploring DCI Signal A Promising Direction

Diagnosis

- train tree-based classifiers (eg. *XGBoost*, *AdaBoost*) on dynamic components only
- normal vs cancer discrimination accuracy $\leq 70\%$
- reveal feature importance



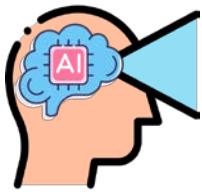
Conclusion

- a **framework** for quantitative analysis of oscillatory behaviors in DCI

What information can be learned from spatial DCI data ?

2 Normal vs Breast Cancer in DCI Images

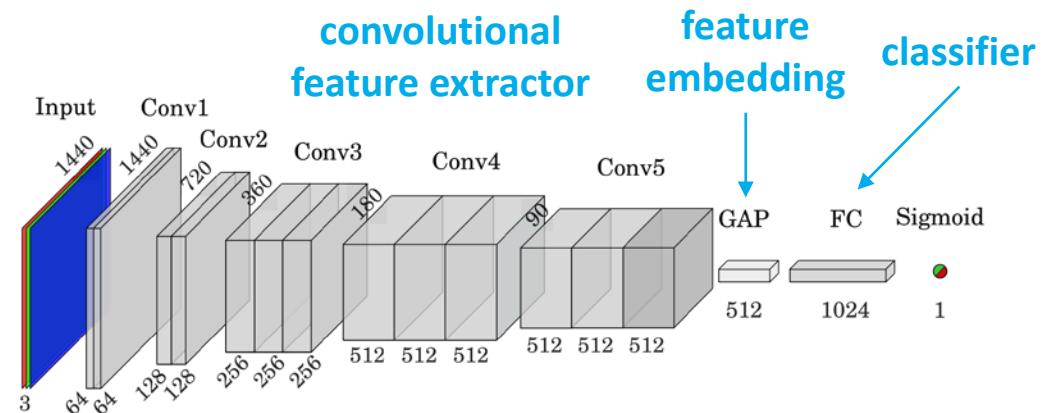
Goal: predict pathologist diagnosis from DCI images.



Convolutional Neural Networks (CNN)

ML models inspired by the human vision mechanism

- Learn **patterns** from image examples
- Input image > feature extractor > embedding > classifier > output prediction

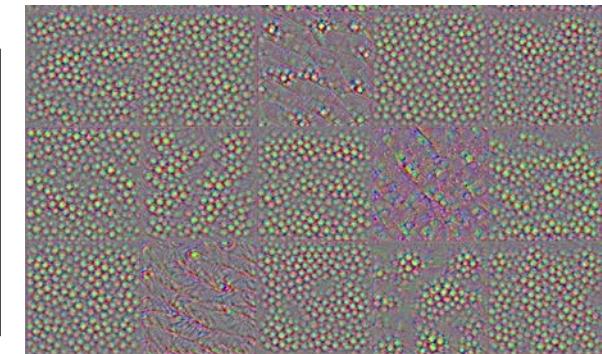


Our Training Strategy:

- ensure **convergence** : limited data → transfer learning, VGG16 / ImageNet
- ensure **generalization** → narrow bottleneck, GAP embedding, dictionary-like



low-level features
(e.g. edges, colors)

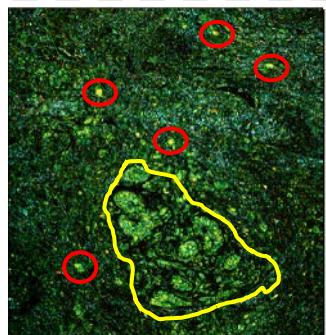


high-level features
(e.g. cell organization)

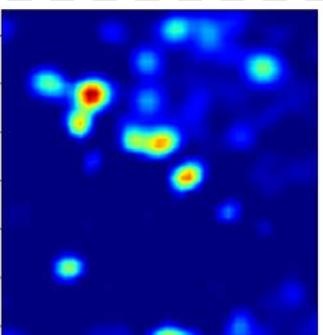
2 An interpretable diagnosis

localization maps - *GradCAM*

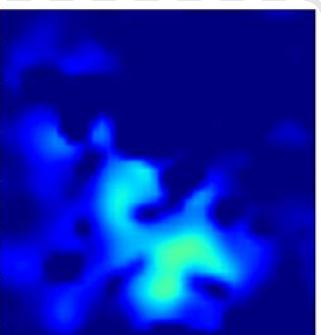
learned patterns - *synthetic input, gradient ascent*



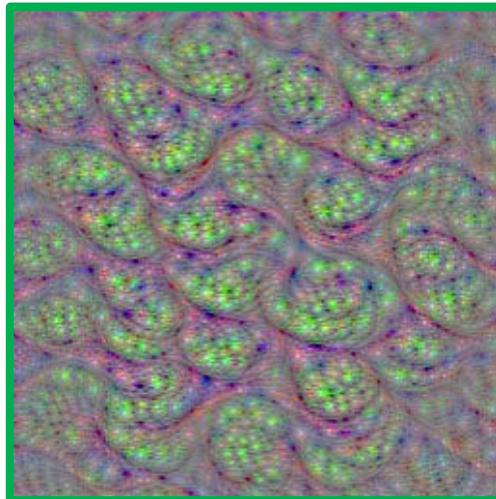
DCI crop of FOV
correctly classified as
tumoral



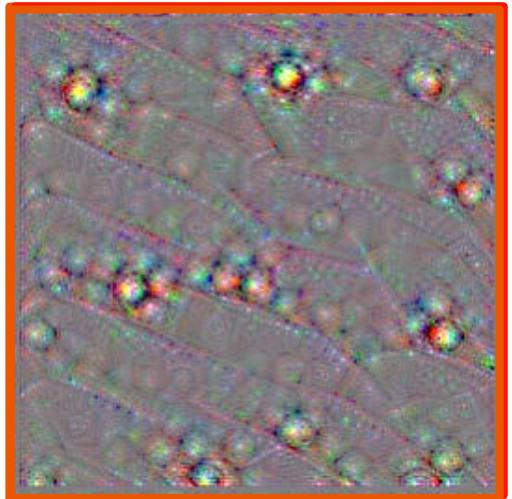
Tumor-positive
localization map
isolated cancer cells



Tumor-negative
localization map
healthy breast lobule

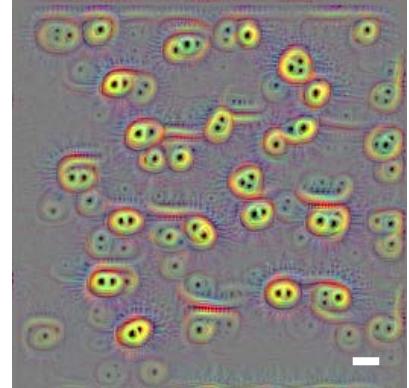
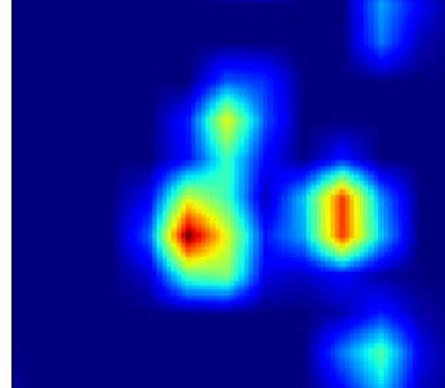
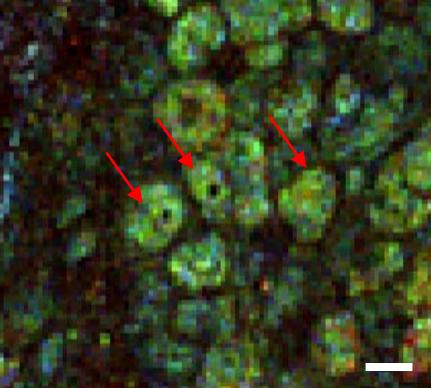
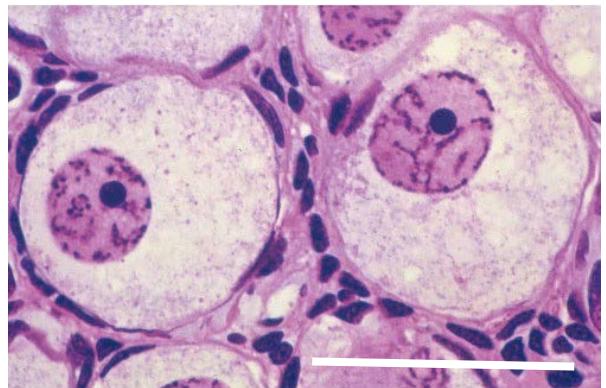


negative evidence



positive evidence

Example of learned **filters** in the last convolutional layer
showing different **cell sizes, shapes and organization**, proper to each **class**



Enlarged **nucleoli** as **biomarker** in DCI: appearance in H&E and DCI, qualitative evidence

2 Fully-supervised Classification Results

Quantitative Results

- Algorithm **surpasses** pathologist performance
 - Possible explanation:
 - ↗ **Sensitivity** : pathologist missed *low contrast isolated* invasive cancer cells
 - ↘ **Specificity** : normal vs in-situ cancer
- Error agreement between algorithm (3) and pathologists (6)
 - Model *appropriates medical reasoning*.
 - Model *overcomes human limitations*.
- Performance is robust to adding images with **uncertain** diagnosis
 - Model is *robust to ambiguity*.

	Accuracy	Sensitivity	Specificity
pathologist P1	91 %	91 %	92 %
pathologist P2	89 %	94 %	75 %
avg(pathologists)	90 %	93 %	83 %
algorithm ⁽¹⁾	94 %	97 %	85 %

⁽¹⁾ aggregated 5-fold CV test pred

+ 4%

+ 4%

+ 2%

Fully-supervised learning is powerful for diagnosis and cell feature extraction.

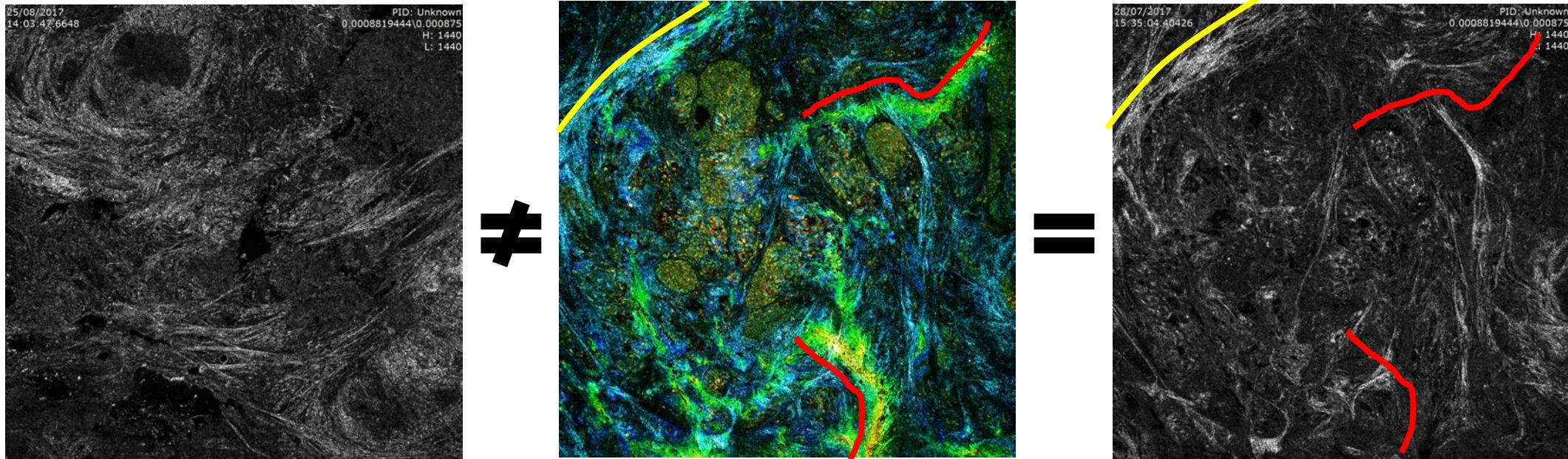
3 FFOCT/DCI Cross-Modal Representation

Goal : better characterize **fiber orientation** from DCI

Strategy

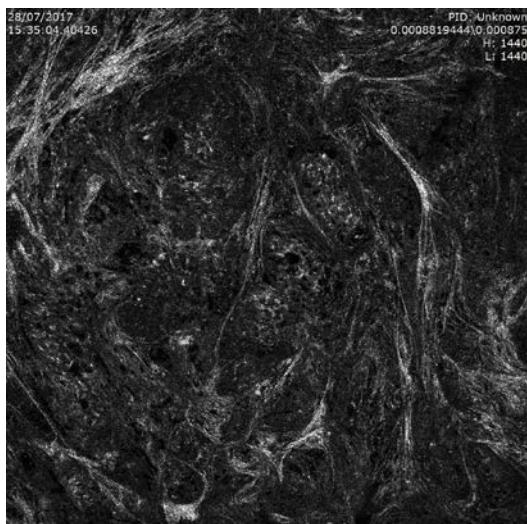
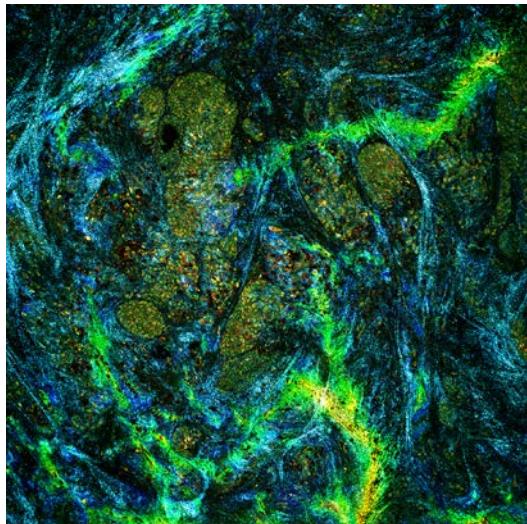
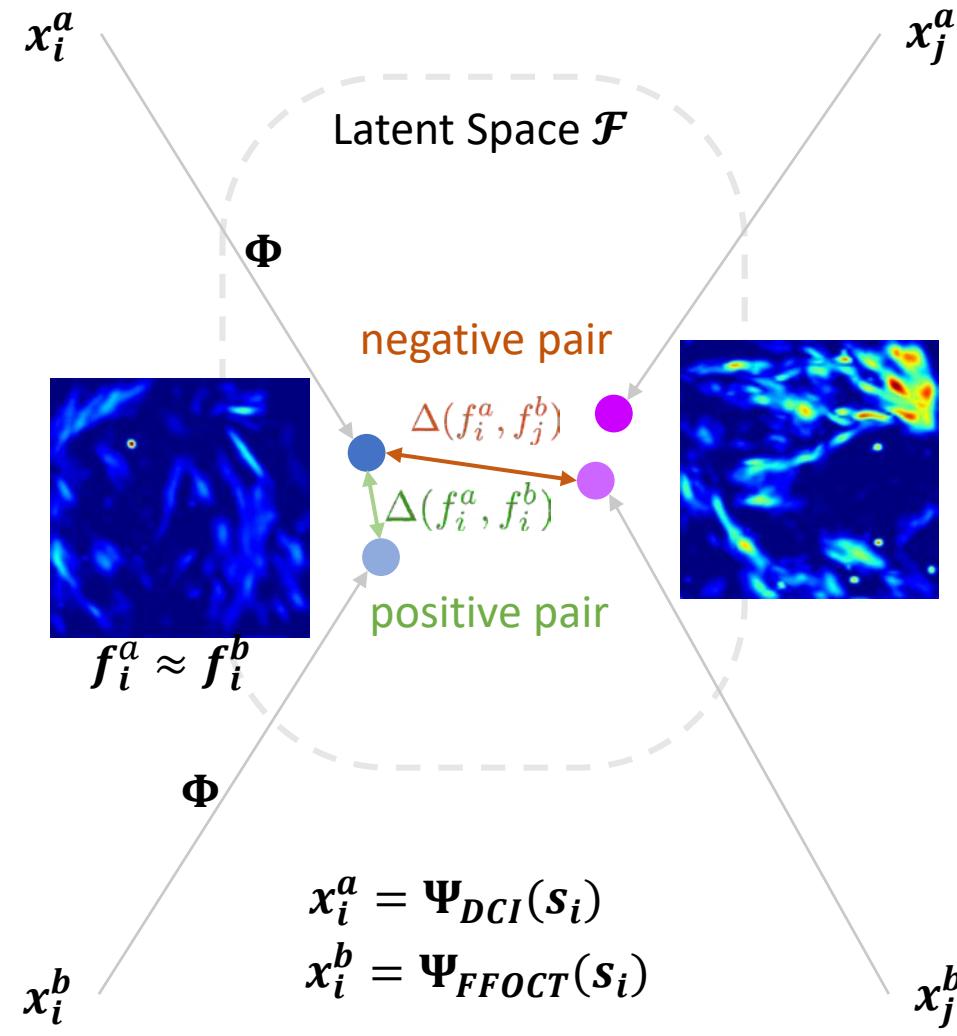
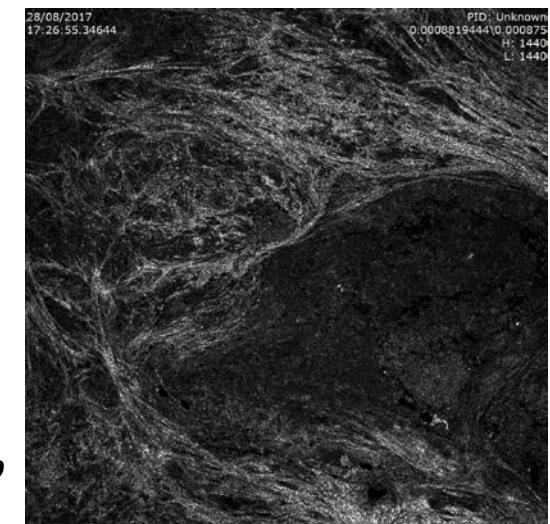
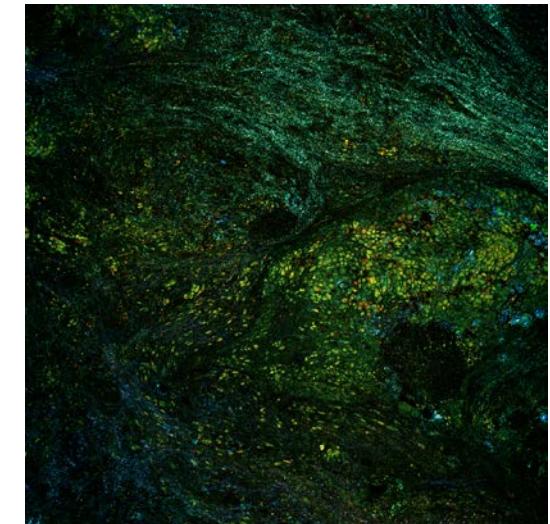
- akin to human agent, learn by **contrast** FFOCT / DCI
- train model to **match** corresponding images –
contrastive learning

contrastive representation learning
ML paradigm for building an embedding space in which similar sample pairs stay close to each other while dissimilar ones are far apart.



Cross-modal matching = pretext task for robust fiber representation in DCI.

3 Concept

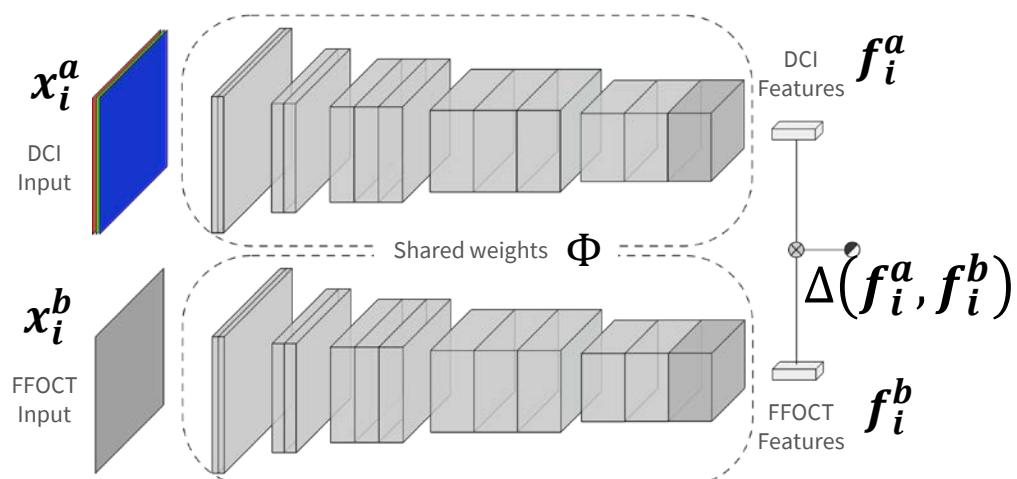
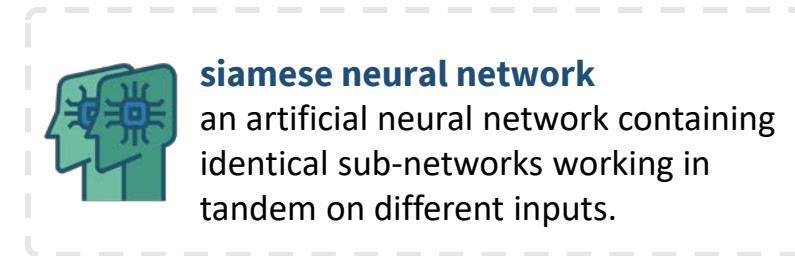
Sample s_i Sample s_j 

3 Implementation

- Siamese CNN encodes Φ embedding function
- Δ function is **cosine distance** :
 - not sensitive to amount of activation
 - bounded [0,1] → binary formulation:

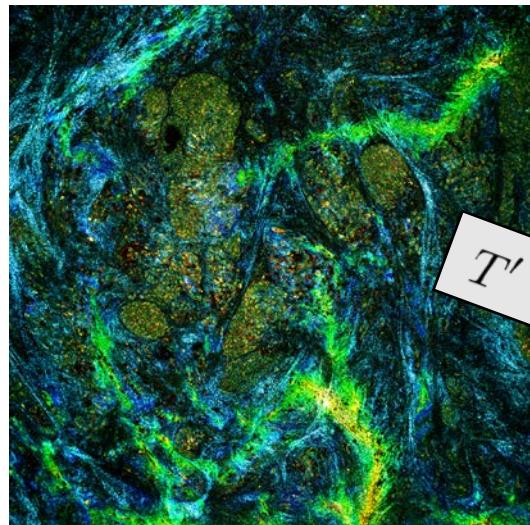
$$L(\theta, \hat{\theta}) = \begin{cases} -\log(\cos(\hat{\theta})) & \text{if } \theta = 0 \\ -\log(1 - \cos(\hat{\theta})) & \text{if } \theta > 0 \end{cases}$$

- “Infinite” dataset generation
 - exploit **registered** images
 - artificially **augment** dataset by extracting corresponding sub-images (480px patches)
 - **online** batch generation (new data every epoch)



$$\Delta(f_i^a, f_i^b) = 1 - \cos\Theta(f_i^a, f_i^b)$$

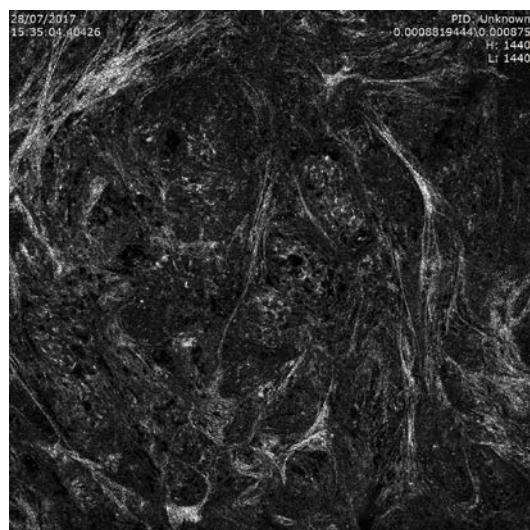
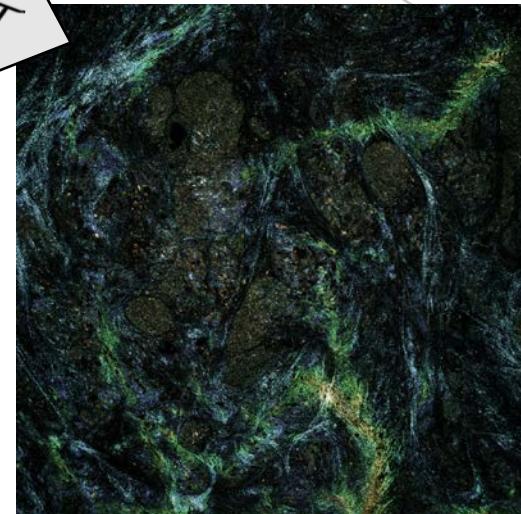
3 Validation Identity Error

Sample s_i  x_i^a $T' \in \mathcal{T}$

$$\varepsilon_{ii'} = \frac{1}{\text{card}(\mathcal{T})} \sum_{i'} |\Delta(f_{i'}^a, f_i^b) - \overline{\Delta(f_{i'}^a, f_i^b)}|$$

where $x_{i'}^a = T'(x_i^a)$ and $T' \in \mathcal{T}$

$$\overline{\varepsilon_{ii'}} = 0.004 \pm 0.008$$

 x_i^b  $x_{i'}^a$ Latent Space \mathcal{F}

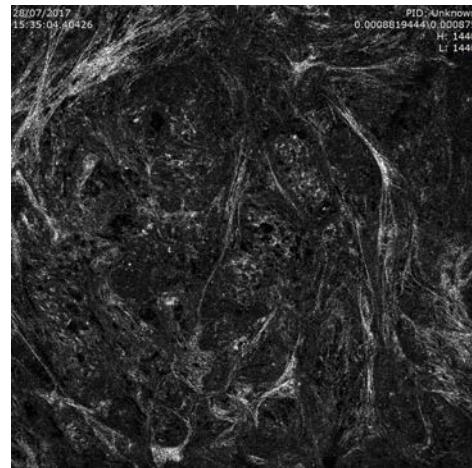
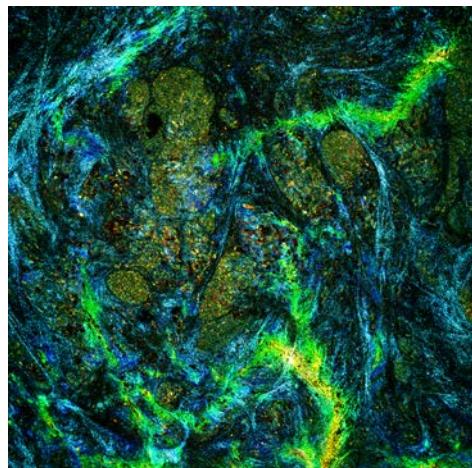
$$\Delta(f_{i'}^a, f_i^b)$$

$$\Delta(f_i^a, f_i^b)$$

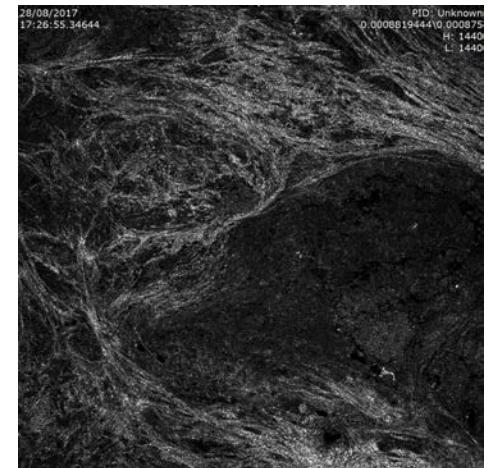
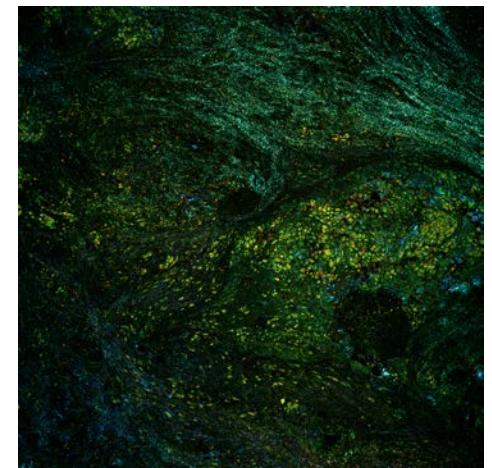
Measure metric robustness to slight transforms.

3 Validation Symmetry Error

$$\varepsilon_{ij} = |\Delta(f_i^a, f_j^b) - \Delta(f_j^a, f_i^b)| \text{ where } i \neq j$$

Sample s_i  x_i^a Latent Space \mathcal{F}

$$\overline{\varepsilon_{ij}} = 0.009 \pm 0.012$$

 x_j^a Sample s_j  x_i^b

**Measure metric robustness
to modality choice.**

 x_j^b

3 Cross-Modal Representation Results

Robust fiber characterization

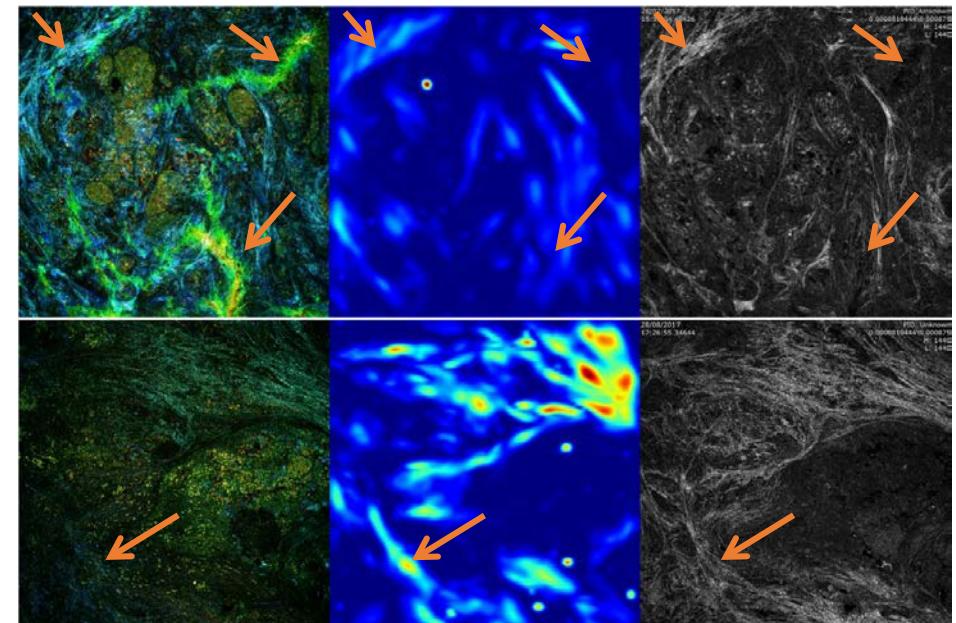
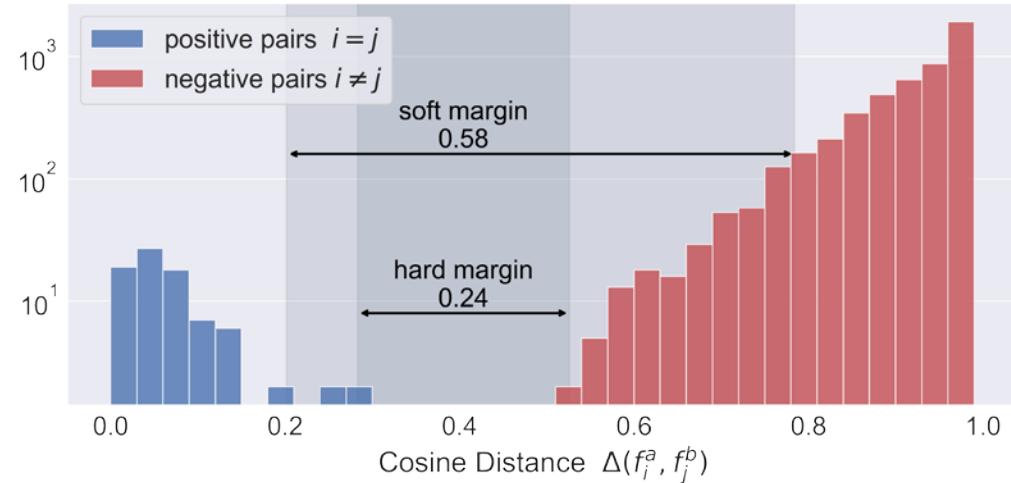
- **Quantitative :**

- *identity & symmetry errors* <1%
- implicit **margin** learned

- **Qualitative :**

- imaging **artifacts** are understood by the network and discounted
- **low contrast fibers** are captured by the network

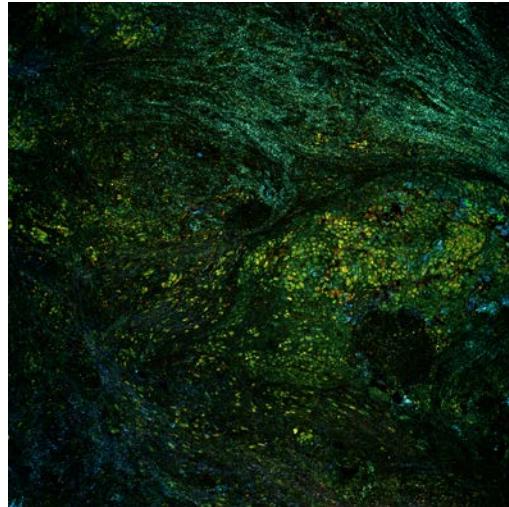
Universality : agnostic to dataset → build **general** fiber representation in DCI



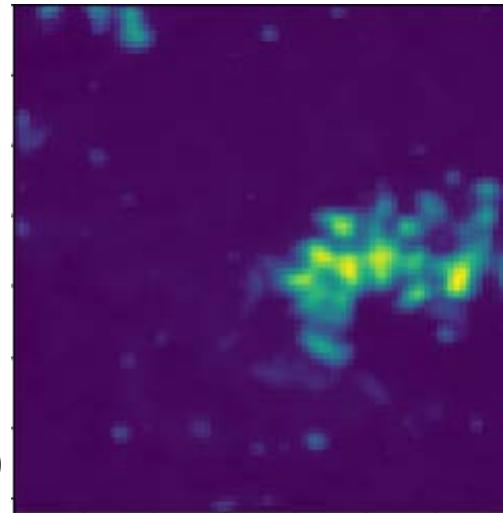
A Complete Characterization of DCI Images

tumor classification model
+
cross-modal matching model
=

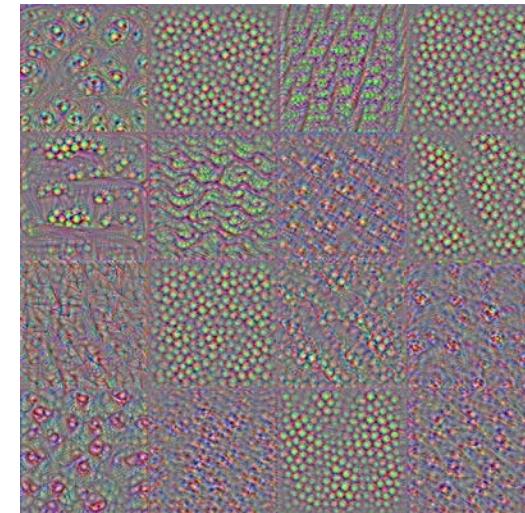
full (*cells + fibers*) image **representation**
↓
serve **downstream** tasks
(image coding, signal analysis, diagnosis...)



DCI image

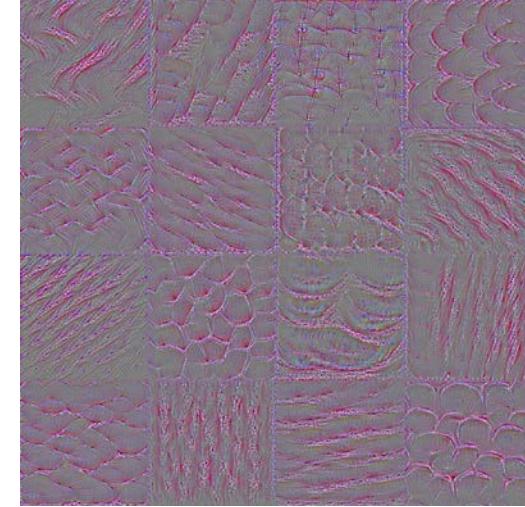


localization maps



learned filters

tumor
classification
model
(cell features)



cross-modal
matching
model
(fibers features)

Methodology Outline

Can we extract more from DCI signal ?

What can we learn from DCI images ?

Can we learn fiber representation in DCI from FFOCT ?

Can DCI be **routinely** used in **clinical** applications ?

Data Exploration

DCI Signal

- Source separation



DCI Images

- Fully-supervised classification

Multi-modality

- FFOCT/DCI cross-modal representation learning

Clinical application

- Multiple Instance Learning classification



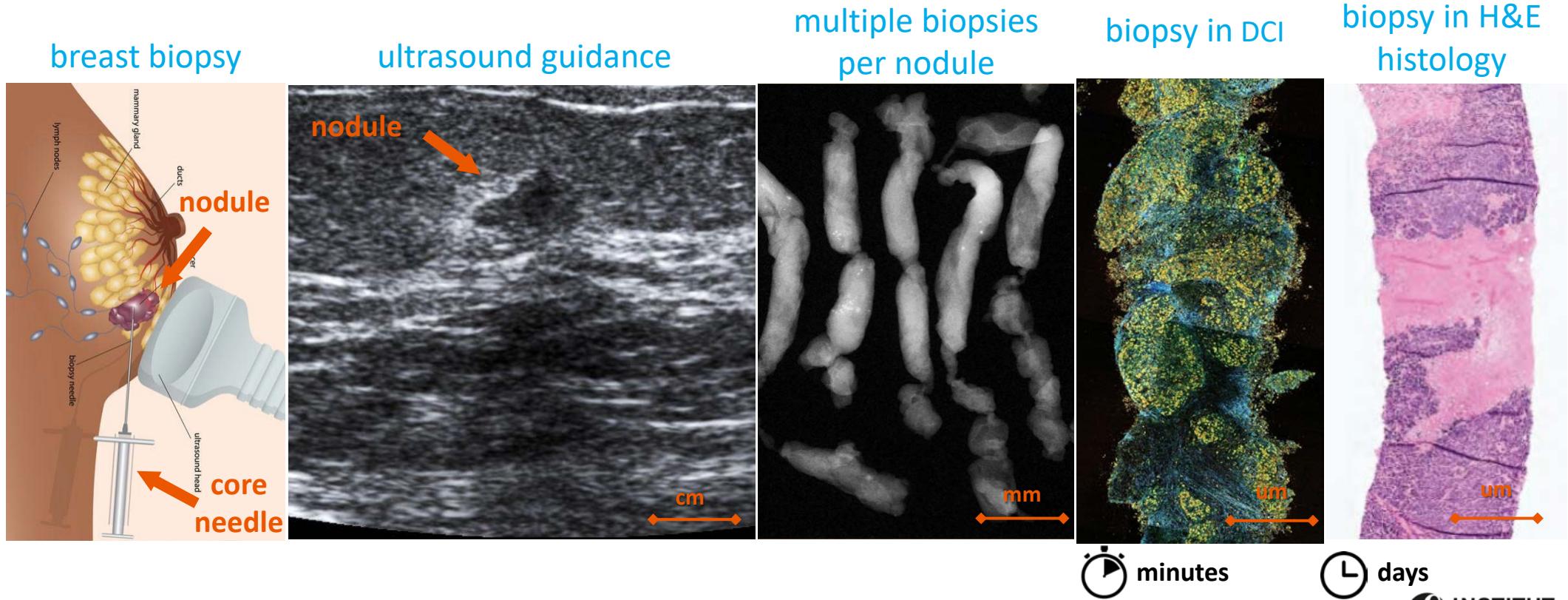
Breast
Biopsies
Dataset

Breast Biopsy Procedure

biopsy = sample tissue from suspect nodule to diagnose malignancy

DCI use-cases :

- biopsy **quality assessment** → **minimize** number of biopsies excised
- **rapid diagnosis** → **comfort** patient (80% biopsies not malignant)



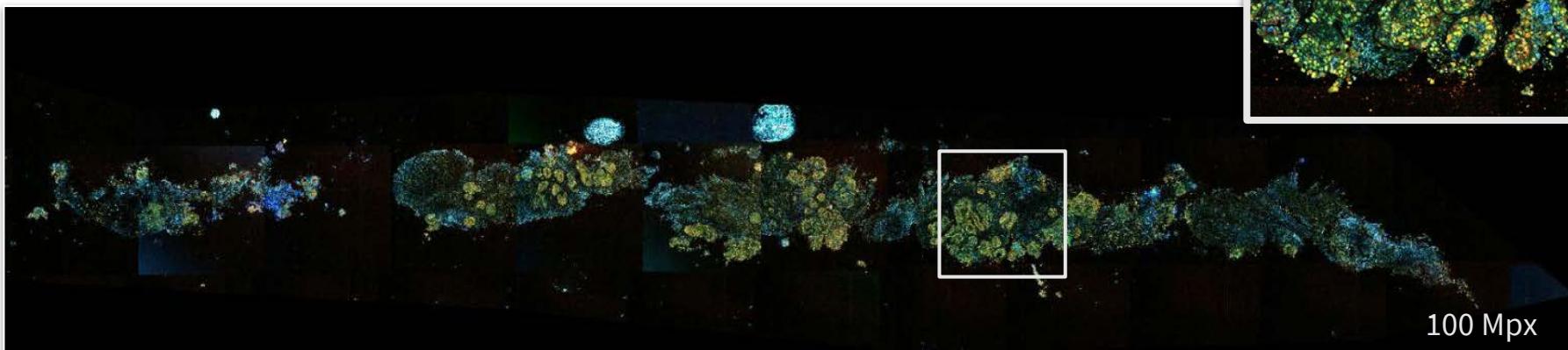
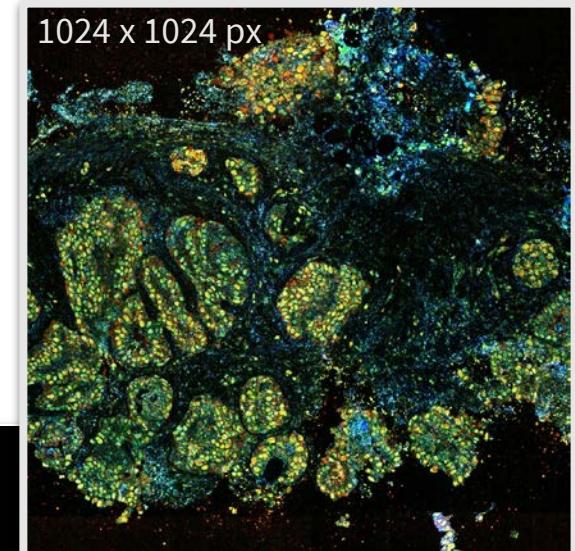
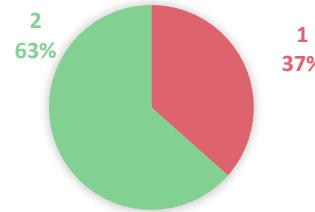
Breast Biopsies Dataset

Cohort : 71 breast nodules

Diagnostic : a histopathology report per nodule, based on H&E

Dataset :

- 71 breast nodules + pathology reports
 - 27 malignant
 - 44 benign
- 145 biopsies in DCI
 - 53 from malignant
 - 92 from benign



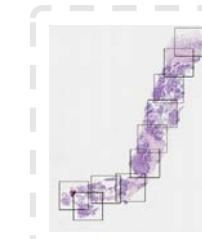
Breast Biopsies Dataset Image Sampling



- sub-sample image optimally :
 - minimal **fragmentation**
 - avoid splitting **homogenous** structures
- *SoSleek* - context-aware sampling with SLIC superpixel segmentation
⇒ 2K patches of 1024 x 1024 px / 145 biopsies

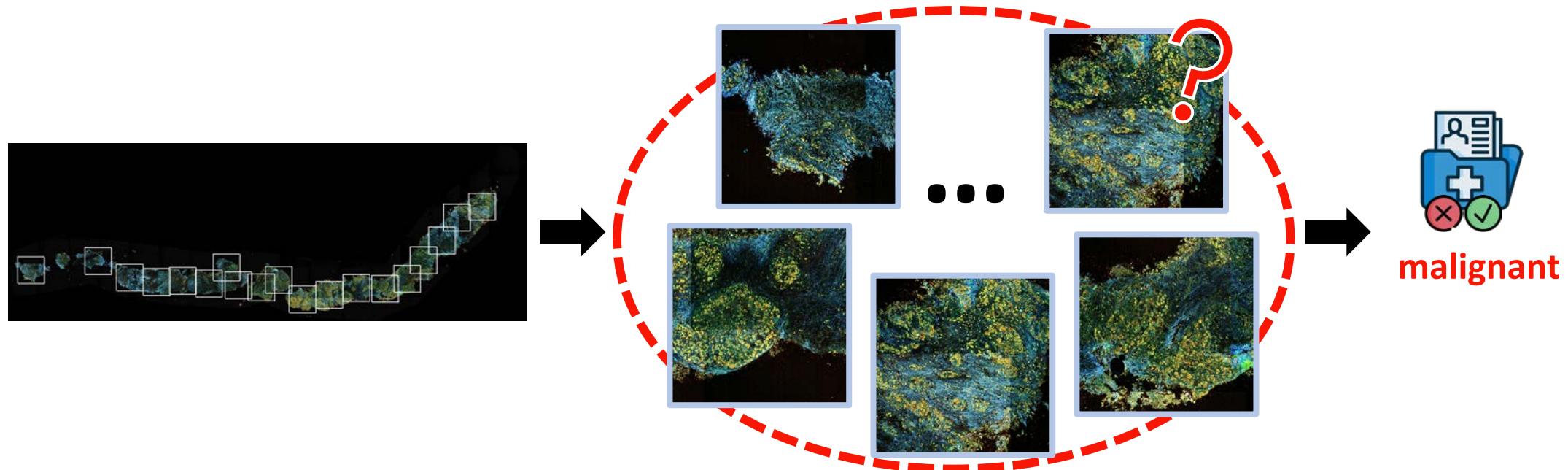


Simple Linear Iterative Clustering (SLIC)
image segmentation method that groups pixels according to their spatial and color proximity.



Sample Optimally with SLIC (SoSleek)
Python package for optimally sampling big images with texture awareness, based on SLIC superpixels.
github.com/dmandache/sleek-patch

Cancer Detection via Multiple Instance Learning



one diagnostic per **group** of patches → MIL training paradigm

MIL Assumptions:

- A malignant biopsy contains at least **one** malignant instance.
- A benign biopsy does not contain **any** malignant instances.



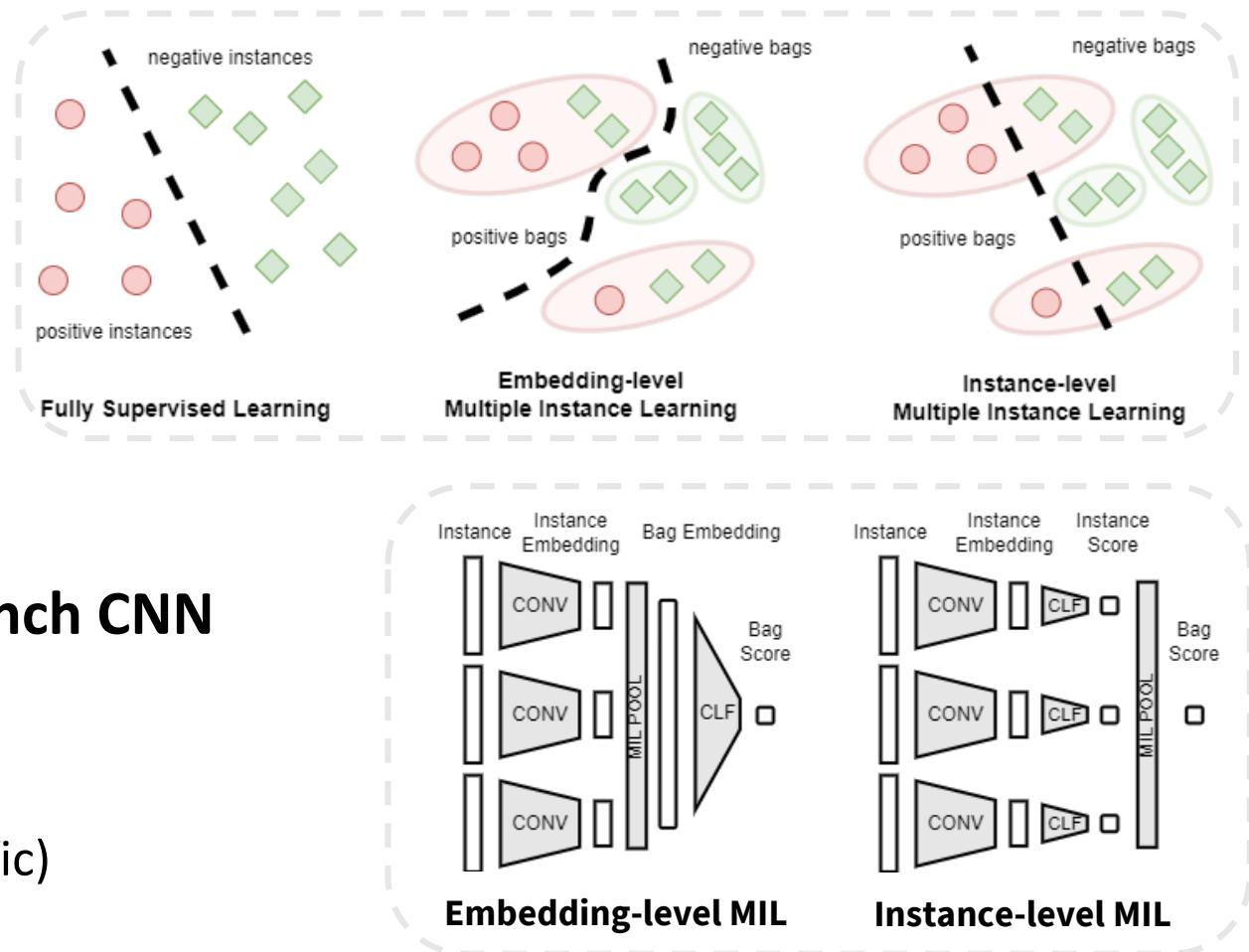
Multiple Instance Learning (MIL)
supervised method for learning from
labeled groups (bags) of instances and
the individual labels are unknown.

Goal: predict **global** (biopsies) and **local** (patches) diagnosis

Multiple Instance Learning

MIL formulations

- Embedding-level MIL
 - global embedding
- Instance-level MIL
 - local scores



Implementation = multi-branch CNN

- computationally heavy
- cannot train end-to-end
- transfer weights (not task-specific)

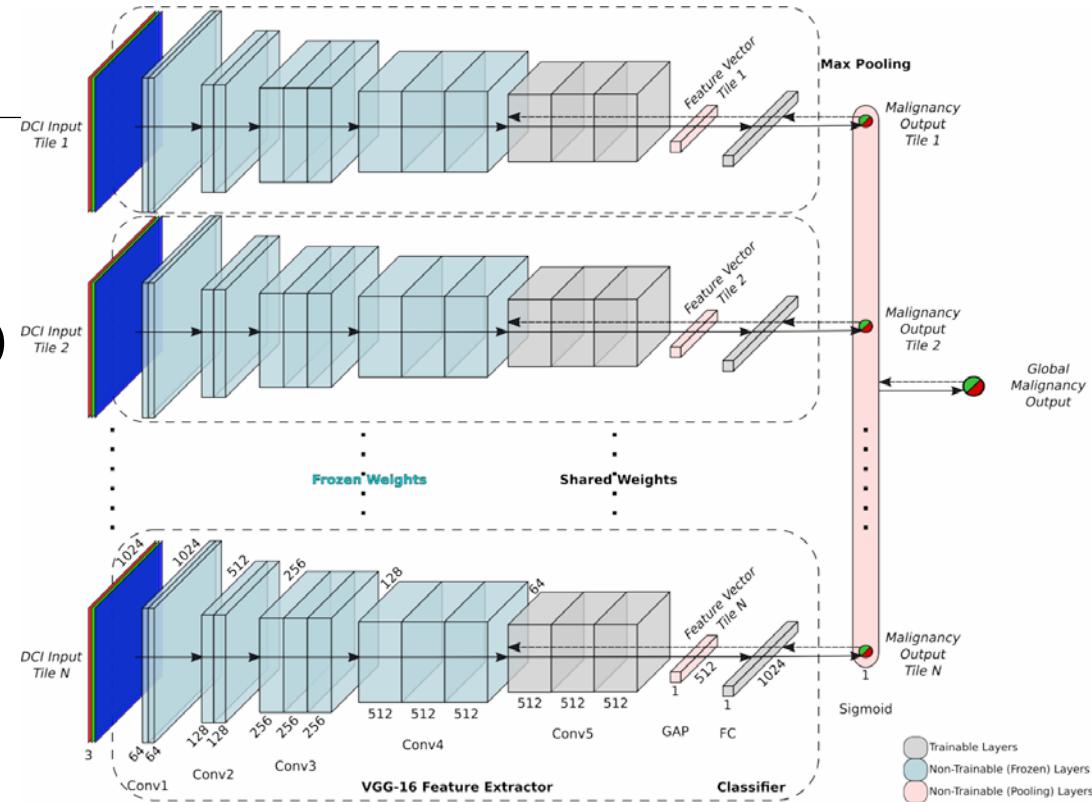
Most MIL applications are embedding-level with transferred feature extractors.

Favor interpretability and task-specific knowledge encoding in MIL.

Implementation

Architecture

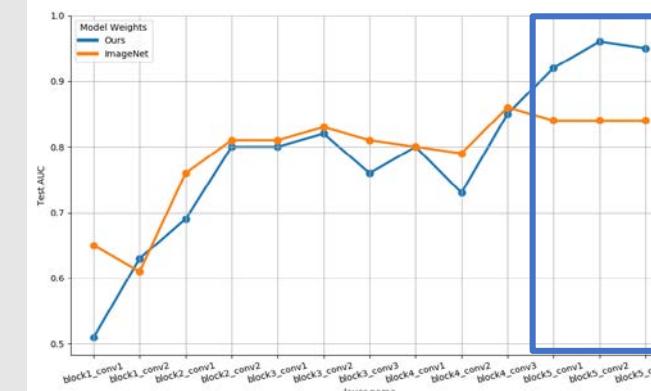
- instance-level MIL with max aggregation
implements MIL assumptions $\hat{Y} = \max_i(\hat{y}_i)$
- **main branch transferred from** our prior diagnostic task
- **freeze domain specific feature extractors**
- **fine-tune task specialized** feature extractors + classifier



Training

- $\mathcal{L}(\hat{Y}, Y) = \mathcal{L}(\max_i(\hat{y}_i), Y)$
- Focal Loss
 - focus on hard examples $FL = -(1 - P)^\gamma \log(P)$
 - 8% accuracy gain vs CE $CE = -\log(P)$

Which layers to freeze ?



task-specialized layers

Results

- intra-domain pre-training allows **convergence**

- relevant metric assessment:

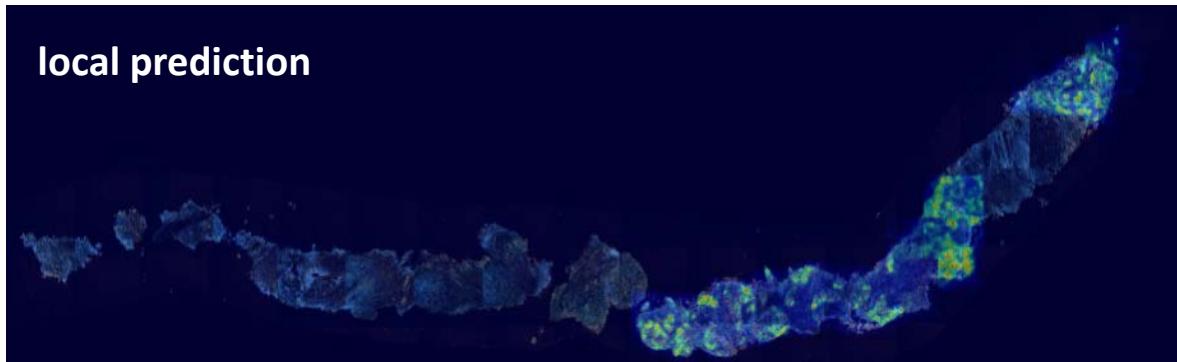
Not all biopsies of same nodule might be malignant.

- specificity at **biopsy** level **90 %**
- sensitivity at **nodule** level **89 %**

- **clinical acceptability criteria:**

- specificity > **90%**
- sensitivity > **80%**

- improve with local ground truth *OR* embedding-level MIL



Intra-domain vs Extra-domain pre-training

Datasets	Test Metrics		
	Accuracy	Sensitivity	Specificity
<i>ImageNet + BiopsyData</i>	72 %	57 %	82 %
	+ 14 %	+ 32 %	+ 2 %
<i>SurgeryData + BiopsyData</i>	86 %	89 %	84 %

Test Metrics

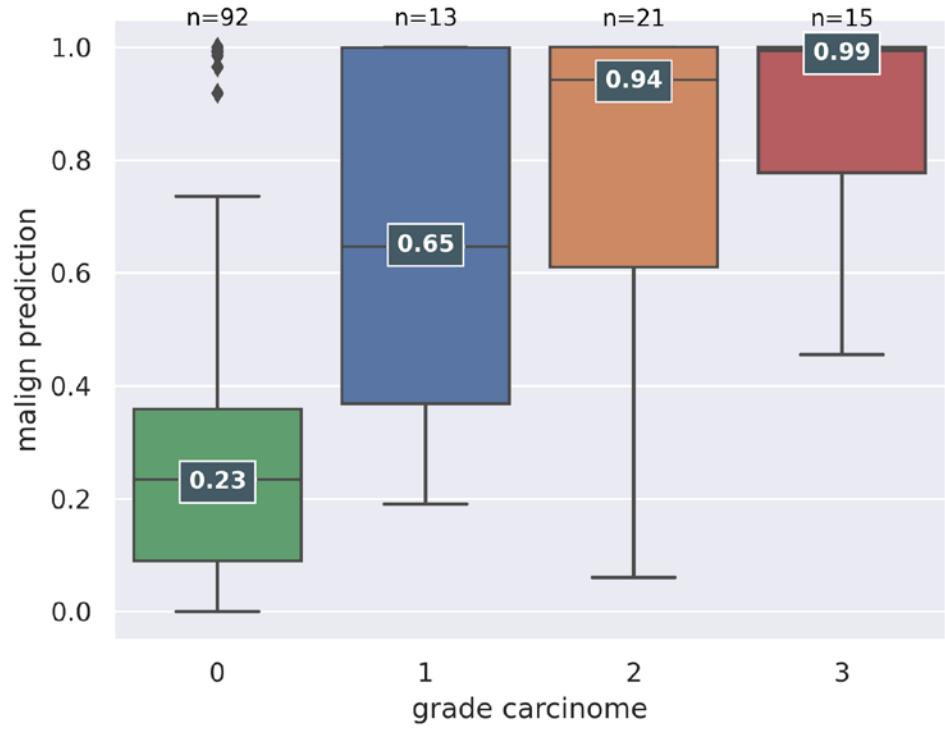
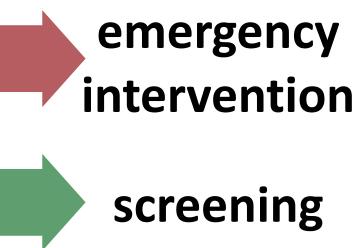
	Accuracy	Sensitivity	Specificity
biopsy	85 %	76 %	90 %
	86 %	89 %	84 %

Prediction Analysis

Benign tumors and high grade cancers have more chance to be identified.

Malignancy Grade	True Prediction
1	70 %
2	76 %
3	87 %
1+2+3	75 %
0	90 %

prediction accuracy according to malignancy grade

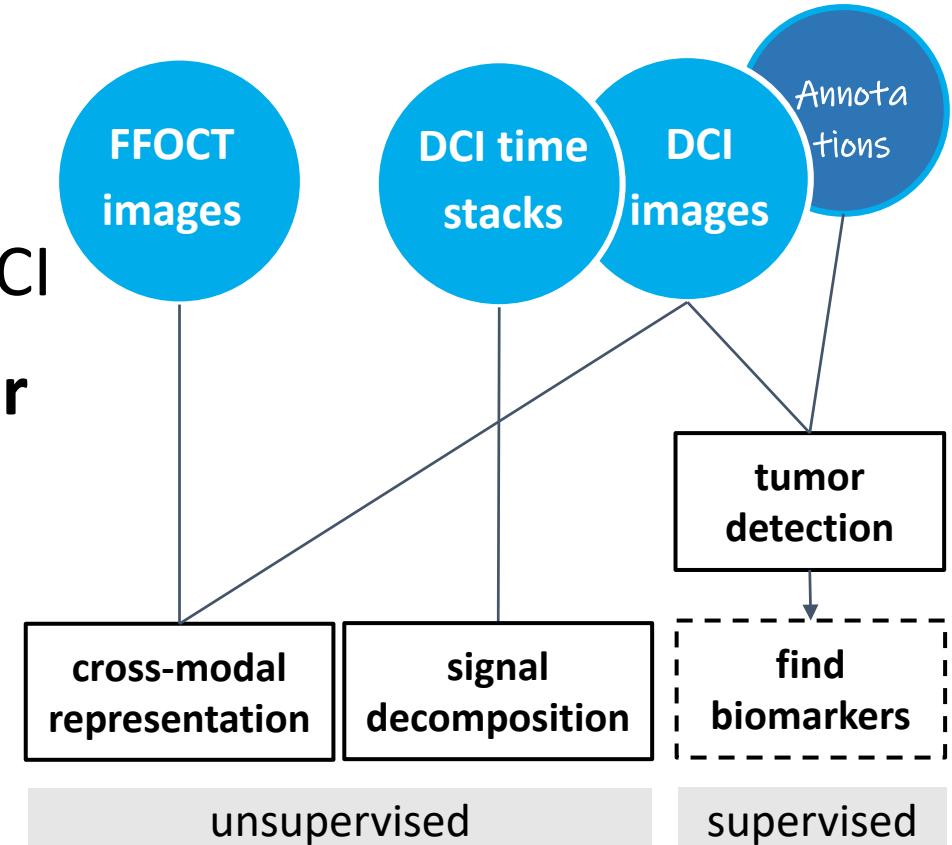


sample prediction according to malignancy grade

Find best use-case for DCI: screening, emergency intervention.

Conclusions Data Exploration

- ✓ framework for extracting oscillatory signatures
- ✓ *robust fiber characterization* in DCI
- ✓ *interpretable CNN tumor classifier* which *surpasses* pathologist performance
- ✓ *evidence* towards considering enlarged **nucleoli** as cancer **biomarker** in DCI



Better characterization of DCI data.

Conclusions Clinical Application

diagnosis method for real-world **clinical** application :

- ✓ *remove expert annotation bottleneck*
- ✓ *predict local diagnosis without explicit training*
 - interpretability
- ✓ *facilitate datasets and aid-to-diagnosis model development*

Efficient aid-to-diagnosis model development without disturbing clinical protocol.

Speed-up the adoption of DCI.

Perspectives

- ❑ **dynamic signal analysis + cell/fiber localization maps as ground truth**
 - supervised source separation
- ❑ include corresponding **histology images**
 - preparation protocol correlated with DCI acquisition
 - multi-modal contrastive learning
- ❑ **metabolic analysis + dynamic signal analysis**
 - 10x glycolysis rate in cancer cells (Warburg effect)

Efforts towards better image representation and biological understanding.

Thank you ! Merci ! Mulțumesc !



Bioimage Analysis Unit



LLTech

LIGHT FOR LIFE TECHNOLOGIES



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Timeline

