

AN INNOVATIVE ENERGY METHOD TO INFORM SURGICAL PLANNING OF ADOLESCENT IDIOPATHIC SCOLIOSIS



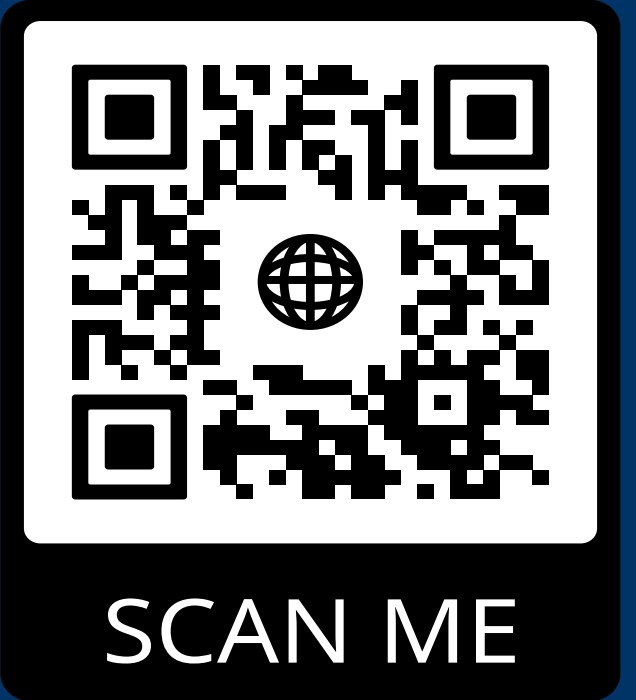
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Context

- **Adolescent Idiopathic Scoliosis (AIS)** requires surgery in severe cases yet choosing the right **instrumented levels** and ensuring proper **sagittal balance** remain **clinical challenges** [1].
- To **reduce empiricism** in surgical planning, we developed an **image-driven, in silico energetic model**, implemented in our in-house simulation tool, **Spinergy®**, to **simulate post-surgery spinal alignment** from **pre-operative effective properties** [2], Fig. 1.

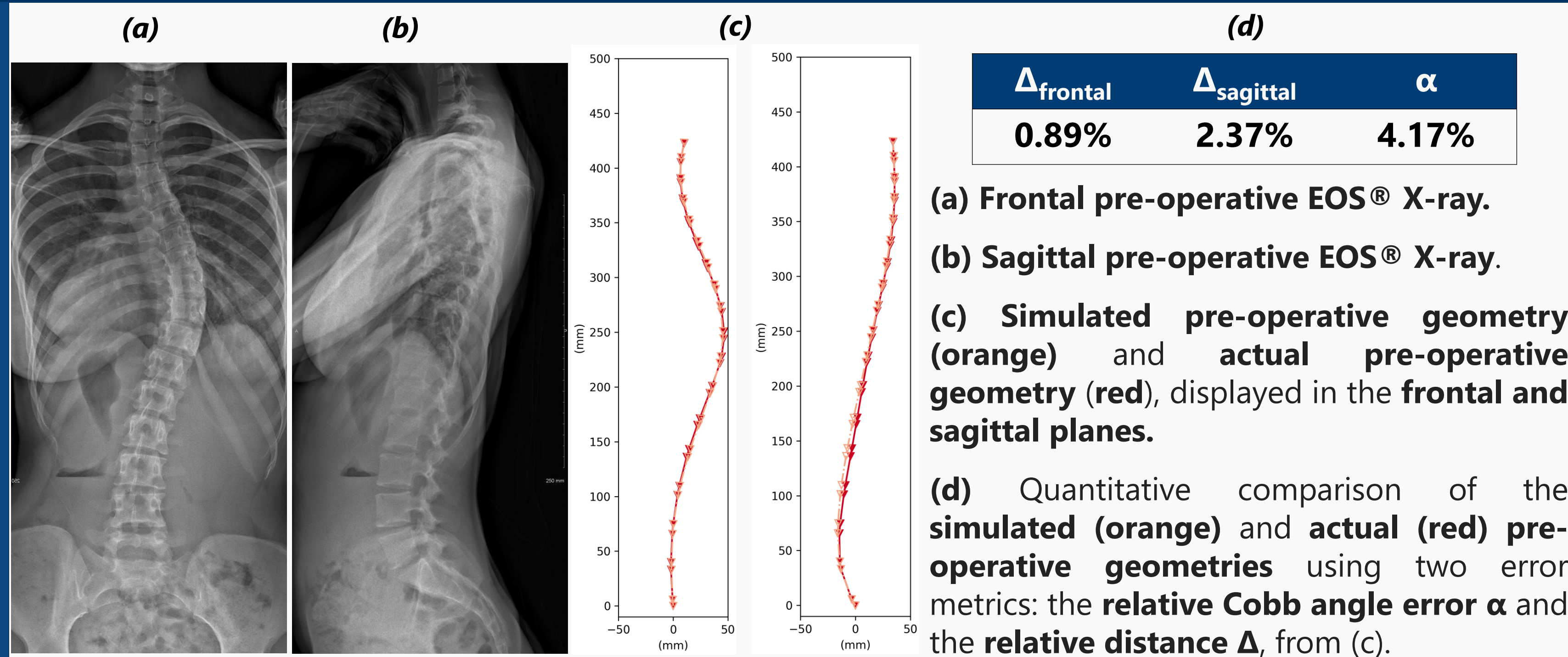


Figure 1 – Biplanar radiographs and pre-operative Spinergy® simulation

Objectives

Simulate the impact of the instrumentation length, ie. the choice of lower and upper instrumented vertebrae (LIV and UIV), on post-operative spinal alignment.

Mechanical Model Equation [2]

$$V(\mathbf{u}, \mathbf{p}) = \frac{1}{2} \sum_i \mathbf{q}_{i/\mathcal{R}_i}^\top \cdot \mathbf{K}_i \cdot \mathbf{q}_{i/\mathcal{R}_i} + \frac{1}{2} \sum_i \mathbf{q}_{i/\mathcal{R}_A}^\top \cdot \mathbf{B}_i \cdot \mathbf{q}_{i/\mathcal{R}_A} - \sum_i \mathbf{G}_i \cdot \mathbf{q}_{i/\mathcal{R}_A}$$

The **local elastic (strain) energy** on vertebral segments

The **global elastic (strain) energy** on vertebral segments

Gravitational potential energy

Methodology

- **3D wire-frame model** of the spine
 - Based on **pre-operative biplanar EOS® X-rays**, Fig.1a,b
 - **Inverse algorithm based on mechanical energy minimization** (Fig.1c)
-> Energy and effective tensors
- **Clinical balance** defined as:
 - Alignment of vertebral bodies along the **vertical axis** in the **frontal plane**
- **Surgery simulation inputs**, Fig.2a,c:
 - Pre-operative **effective parameters**
 - **Instrumented length** (range of UIV to LIV)
 - **Sagittal curvature**
 - **Spine curve reduction**
- **Surgery simulations**, Fig.2e-h:
 - **Residual area A**: between non-instrumented vertebrae and the T1-S1 axis
 - **Z_{max}**: **absolute distance** between the **vertical axis** and the **apex of free (non-instrumented) vertebral segments**

Discussion

- **Spinergy®** enables **fast** and **efficient** simulations:
 - ~1 hour to compute inputs on 10 CPU cores
 - Simulation of **multiple instrumentation lengths** in a few seconds
- **Fig. 2e–h** illustrates the impact of **varying instrumentation levels** (n–2 to n+1) **compared to the actual case** (n = T3–L3):
 $\downarrow L_{\text{instrumentation}} \Rightarrow \uparrow A_{\text{residual}} \text{ and } \equiv Z_{\text{max}}$

UIV-LIV	A_{residual} (mm ²)	Z_{max} (mm)
T3-L4 (n+1)	34	<0.5
T3-L3 (n)	78	1
T3-L2 (n-1)	153	3
T3-L1 (n-2)	467	3

- In Fig.2b,d: **simulated (blue)** and **post-operative (dark blue)** distributions based on Fig.2a,c show a **good agreement on the actual T3–L3** thoracic-lumbar instrumentation.

Conclusion

- **Spinergy®** provides **efficient patient-specific simulations** that **enhance** and **personalize AIS surgical planning**. Expert-reviewed results suggest that, in the illustrative case, a **shorter instrumentation could have been appropriate**.
- This project contributes to the development of **Spinergy®** as a **decision-support tool** to:
 - Help surgeons choose **optimal** instrumentation levels
 - Improve **surgical outcomes** and **patient well-being**

Results

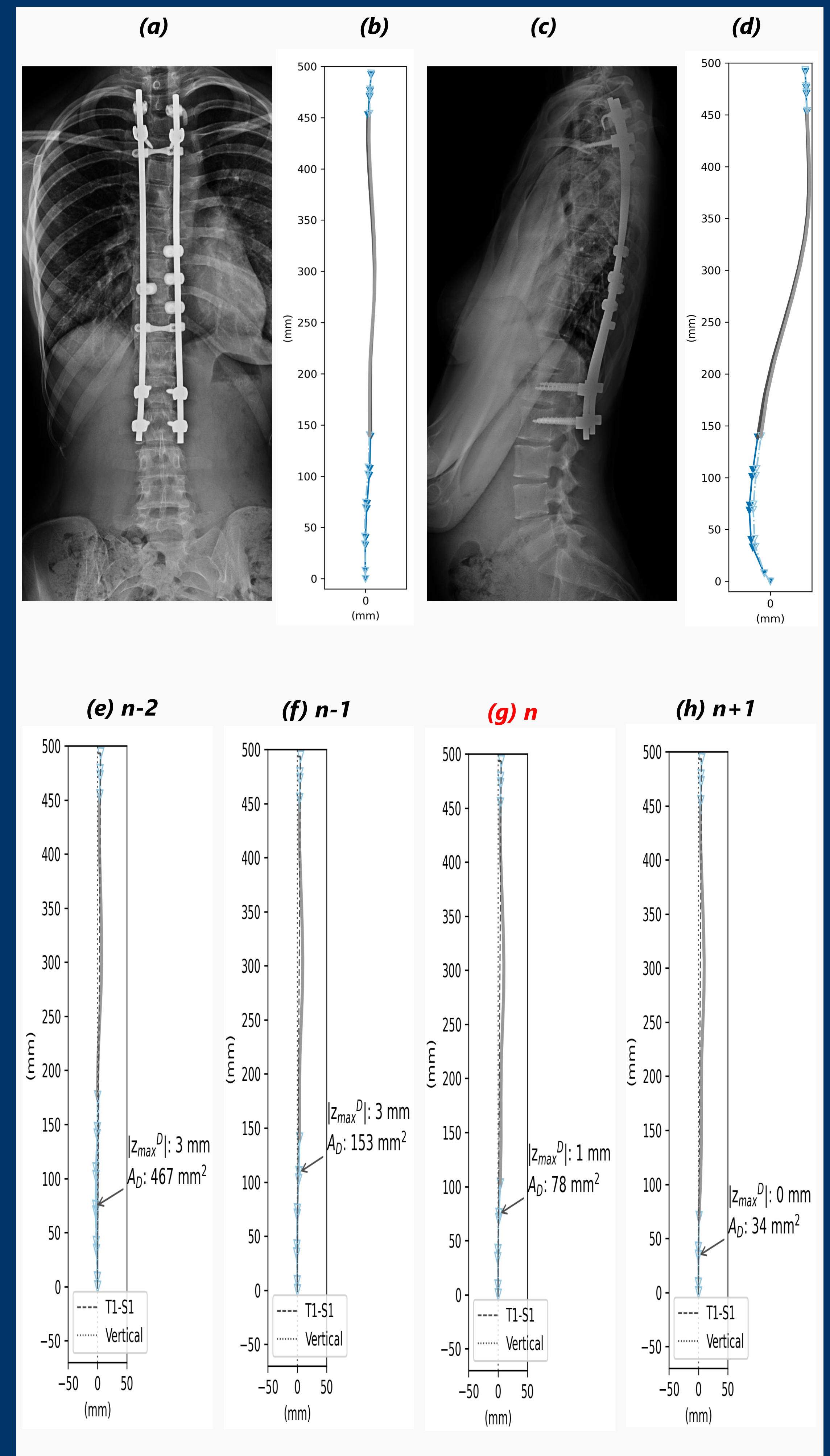


Figure 2 - Post-operative results and Spinergy® simulations

References

- [1] Compagnon, R. et al., Orthopaedics & Traumatology: Surgery & Research, Volume 108, Issue 6, 2022.
- [2] Brun-Cottan, B. et al., Biomechanic and modeling in mecanobiology. 20, 359–370, 2021.