# Modeling native phonology and non-native speech perception using EEG signals





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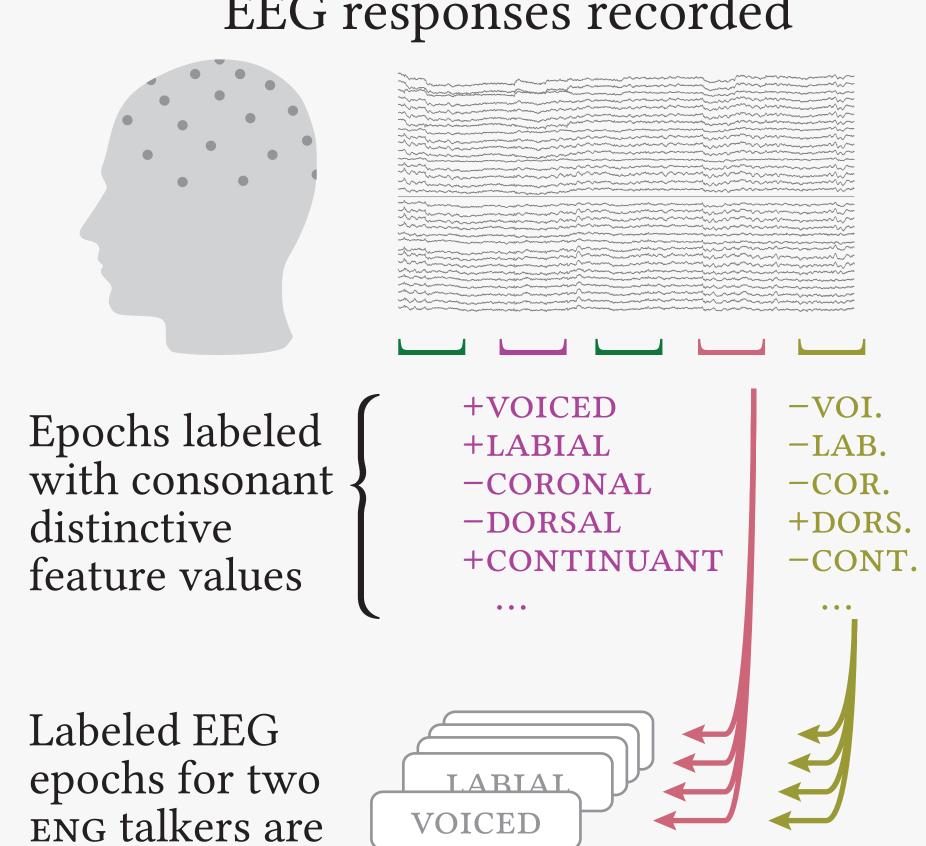


## Overview

Listener hears stream of CV syllables

HUNQ HINO HUNQ ENGO ENGQ ... dza va na sa ka...]

#### EEG responses recorded



training data for classifiers (1 classifier per distinctive feature)



Trained classifiers are given EEG epochs corresponding to foreign talkers and 2 new ENG talkers;

this yields guesses about which features the heard consonant had, and error rates for each classifier.

For each heard consonant type, use error rates to compute joint probability across classifier outputs; do this for different combinations of feature values to get a confusion matrix (see key).

# Acknowledgments

NIH T32 DC005361 (Auditory Neuroscience Training Program); NSF Jelenik Speech and Language Technology Workshop 2015 Probabilistic Transcription Team; Mark Hasegawa-Johnson; Preethi Jyothi; Majid Mirbagheri; Nick Foti; Eric Larson.

#### References

- [1] J. Särelä and H. Valpola, "Denoising source separation," J. Mach. Learn. Res., vol. 6, pp. 233-272, 2005.
- [2] A. de Cheveigné and J. Z. Simon, "Denoising based on spatial filtering," J. Neurosci. Methods, vol. 171, no. 2, pp. 331–339, 2008.
- [3] S. Moran, D. McCloy, and R. Wright (eds). PHOIBLE: Phonetics Information Base and Lexicon Online. Munich: Max Planck Digital Library, 2013.

# Background

 Studying phoneme confusion normally requires stimulus degradation or synthetic intermediate tokens (i.e., "ba - wa" continuum) to pull listener performance away from ceiling

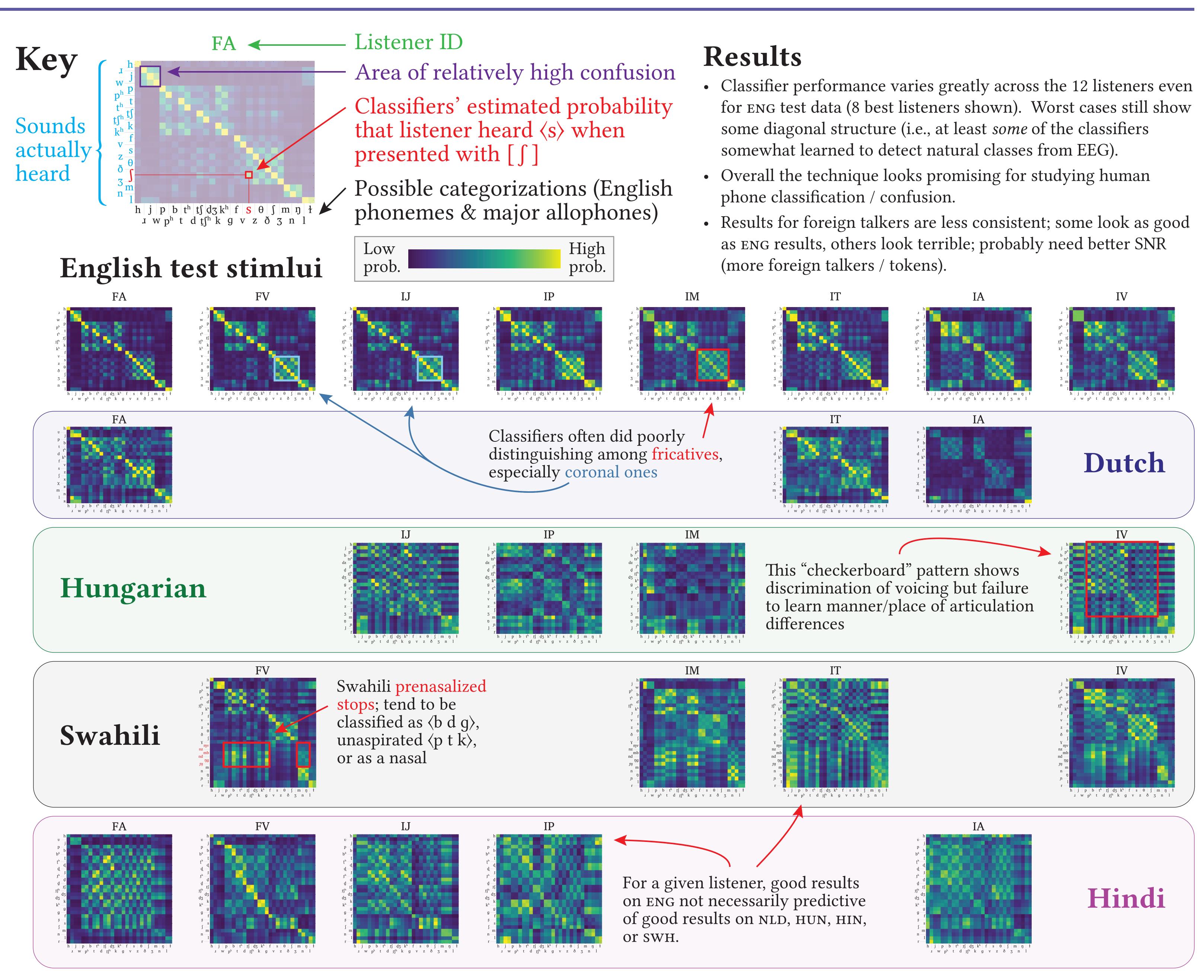
# Research Questions

- Can we estimate consonant confusions by observing neural responses to speech sounds?
- Does this method reveal something about the structure of mental representations of phones/ phonemes?

## Methods

- **STIMULI**: English & foreign consonant-vowel (cv) syllables; variable consonant, vowel always [a]
- TRAINING SET (ENGLISH): 2 talkers  $(\eth, \wp) \times 3$  recordings  $\times 23$  consonants  $\times 20$ presentations = 2760 trials
- TEST SET (ENGLISH): 2 new talkers  $(\mathcal{O}, \mathcal{P}) \times 1$  recording  $\times 23$  consonants  $\times 20$ presentations = 920 trials
- TEST SETS {DUTCH/HUNGARIAN/HINDI/SWAHILI}: 1 talker  $\{9/9/3/3\} \times \{18/25/30/30\}$  consonants × 20 presentations =  $\{360/500/600/600\}$  trials
- **RECORDING**: 32-channel BrainVision EEG, left earlobe reference, 1000 Hz sampling rate
- **PREPROCESSING**: bandpass 1-40 Hz, downsample to 100 Hz, align epochs on boundary between c and v, apply denoising source separation<sup>[1,2]</sup> (DSS), remove time domain autocorrelation with PCA (retains ~20 "time samples"), use only first 4 DSS components
- **SUPERVISED LEARNING**: label each epoch with consonant's distinctive feature values from PHOIBLE<sup>[3]</sup> database (16 feats. used), train binary classifier (support vector machine with radial basis function) for each distinctive feature (5-fold cross-validation + grid search), set threshold to equalize error rate (false positive rate = false negative rate) to handle class imbalance
- EVALUATION: apply classifiers to test data, estimate "probability that listener heard  $\langle \cdot \rangle$ " as joint probability of classifier outputs being consistent with the feature values of  $\langle \cdot \rangle$ , i.e.:

 $P(\langle \eth \rangle) = P(+\text{voi.}) \times P(-\text{son.}) \times P(+\text{cor.}) \times ... \times P(+\text{cont.})$ 



## Future directions

- Vary both consonants and vowels
- More languages / speech sound types (airstream and phonation contrasts, tone)
- Increase SNR: more talkers/tokens, different classifier strategies
- Unsupervised learning: derive optimal, perceptually based distinctive features
- Simultaneous MEG + EEG experiments to connect confusion patterns to cortico-spatial patterns
- Other applications of this method: diagnostic use for hearing / language impairments?