



Functional Regression Models in Human Movement Biomechanics

Methodology and Applications

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Background

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“...the inter-discipline that describes, analyses, and assesses human movement”

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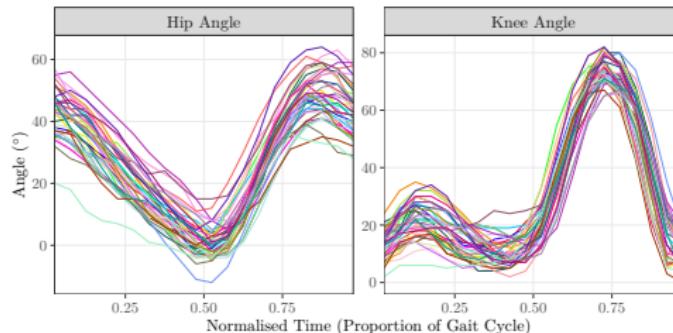


Figure: The childrens' gait dataset (Rice and Silverman, 1991).

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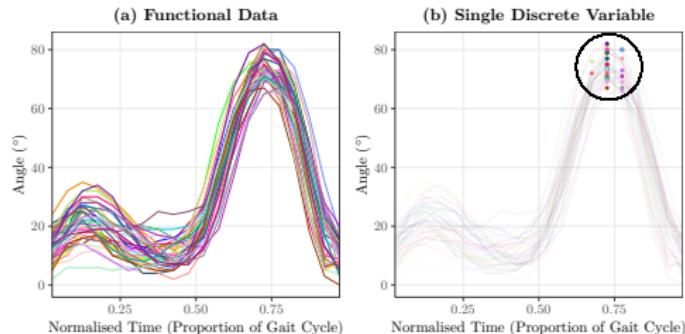


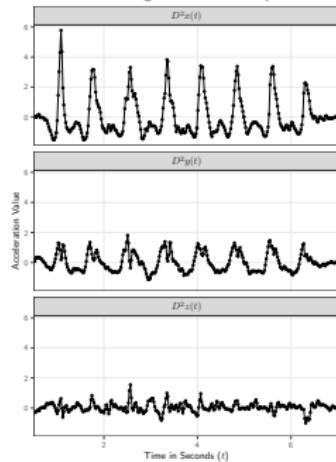
Figure: Data reduction of the knee angle curve to a single discrete variable (peak knee flexion).

Second-Generation Functional Data in Biomechanics

Volume



My Own Motion Data from Apple
Collected During a Short Warm-Up Exercise

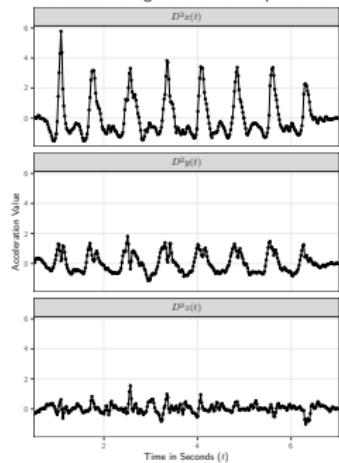


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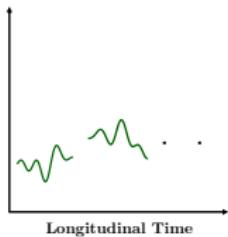
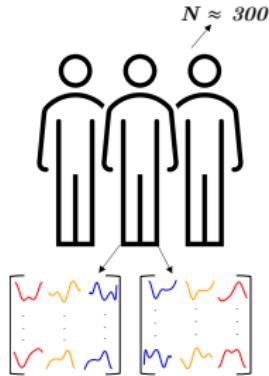
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Complexity

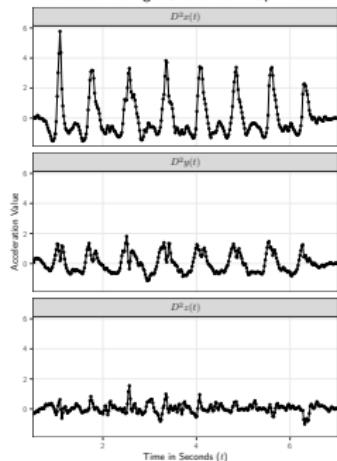


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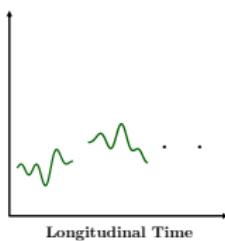
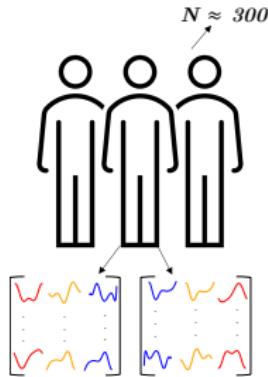
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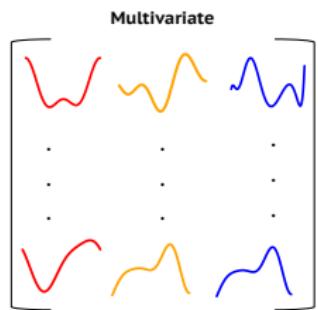
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Complexity



Variety



Human movement as a system of multiple related parts → **multivariate** and **dynamical systems** approaches to analysis.

Compare and Contrast

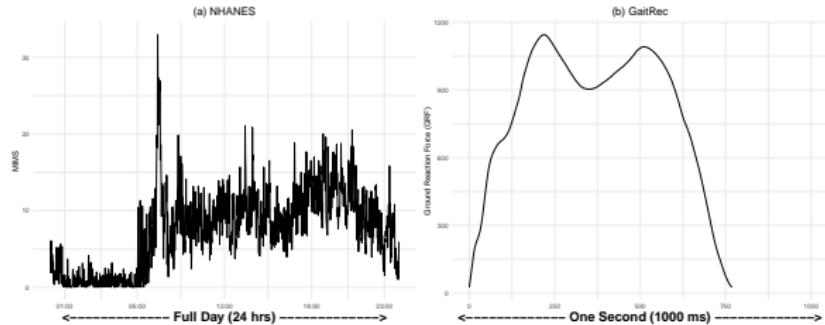


Figure: (a) NHANES (Crainiceanu, Goldsmith, et al., 2024); (b) GaitRec (Horsak et al., 2020).

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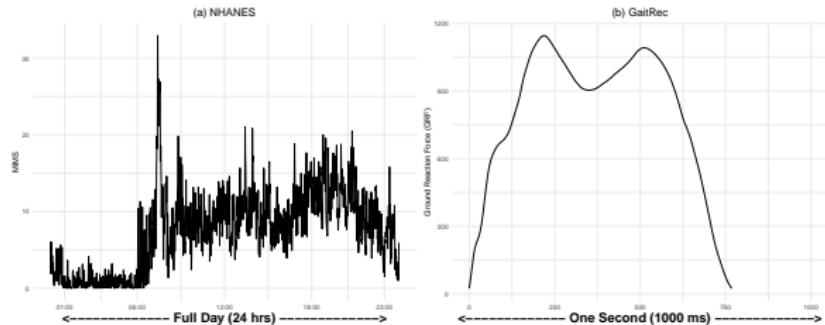


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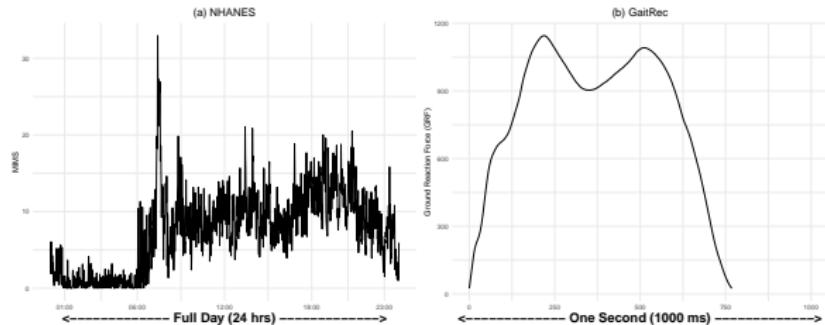


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- Movement on macro vs. micro scales.

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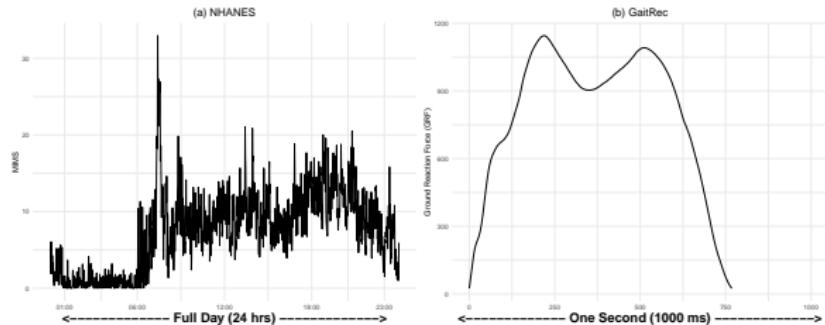


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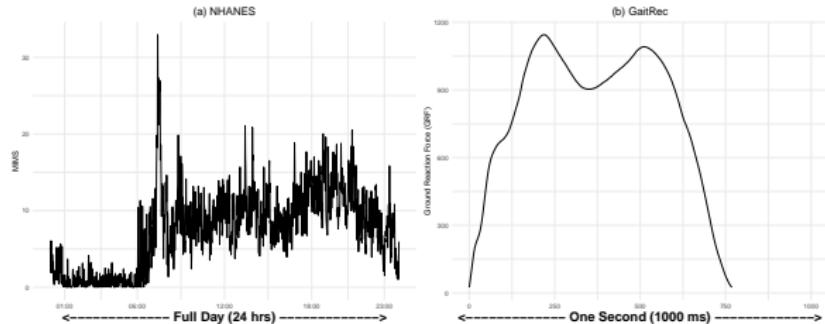


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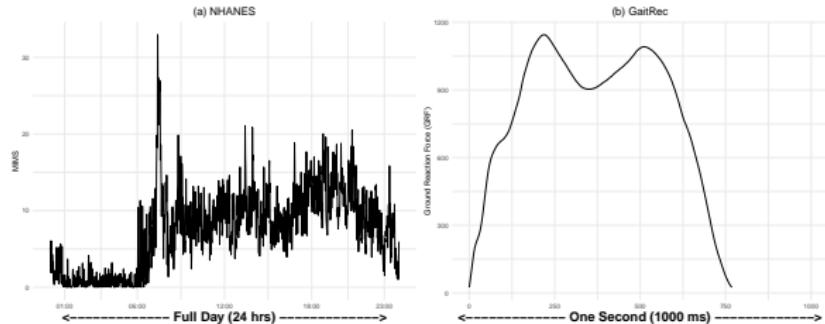


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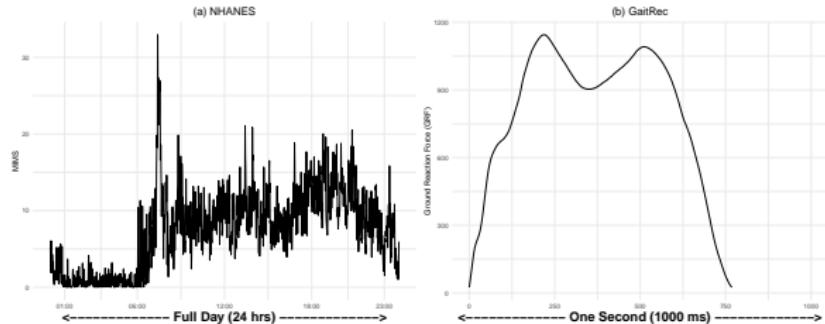


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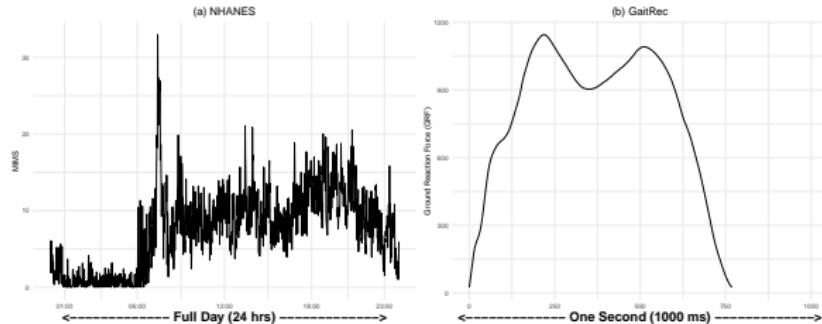


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→ We need principled and efficient statistical modelling approaches to extract information from rich, complex and structured functional data.

GaitRec (Horsak et al., 2020)

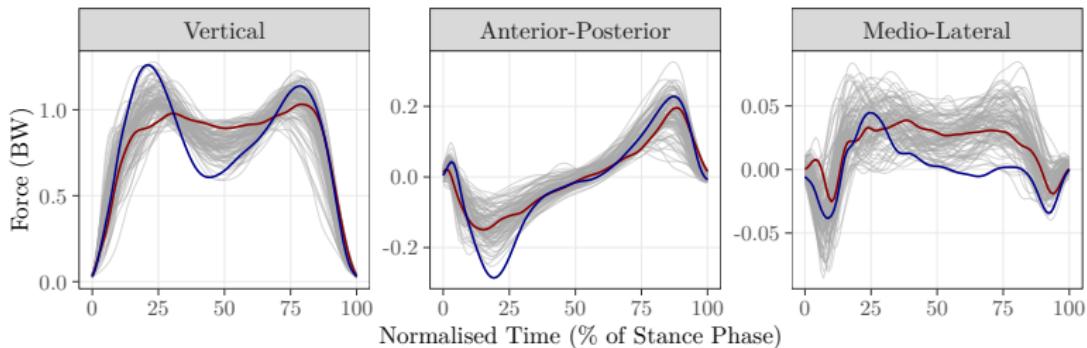


Figure: A sample of observations from the GaitRec dataset (Horsak et al., 2020).

GaitRec (Horsak et al., 2020)

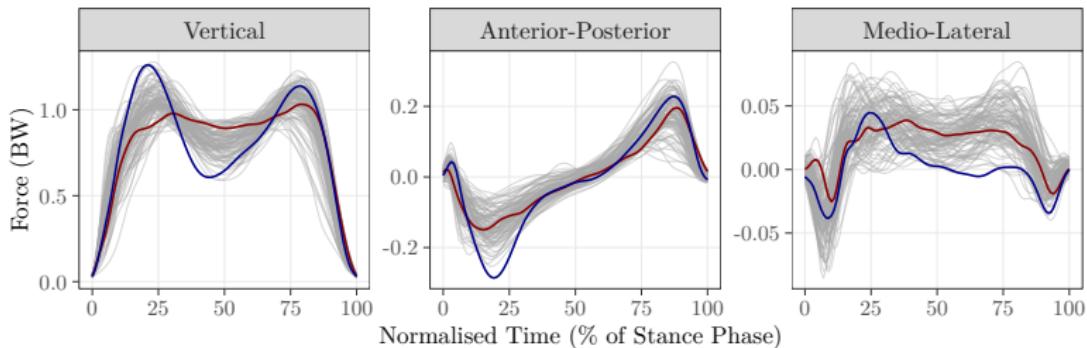


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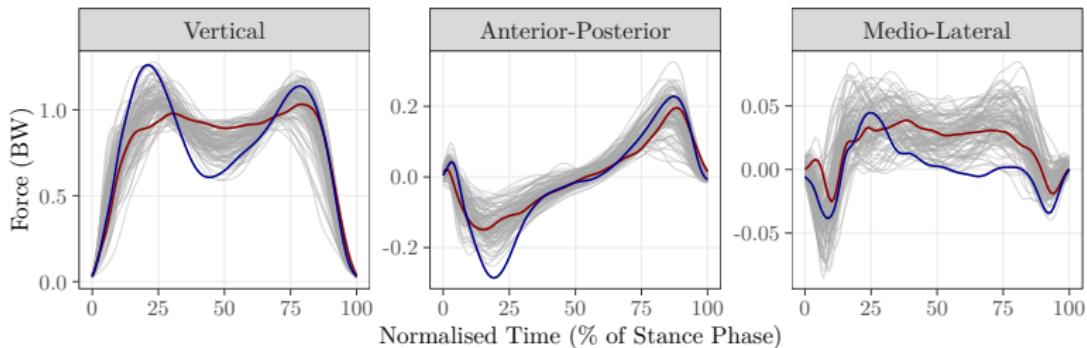


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- 2,295 individuals measured under different conditions (75,732 trials in total).

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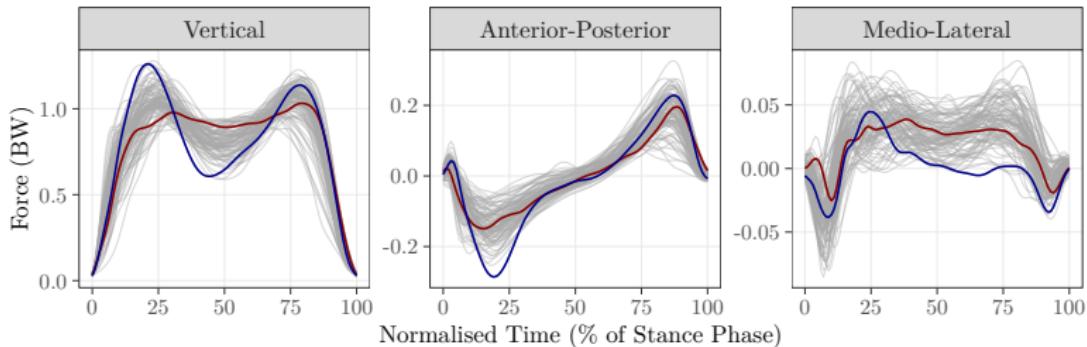
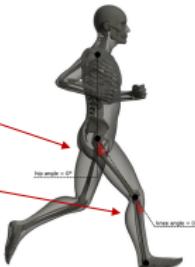
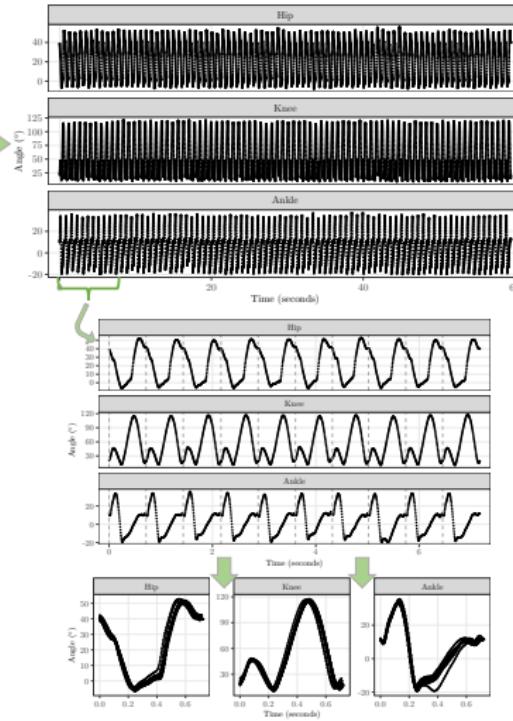


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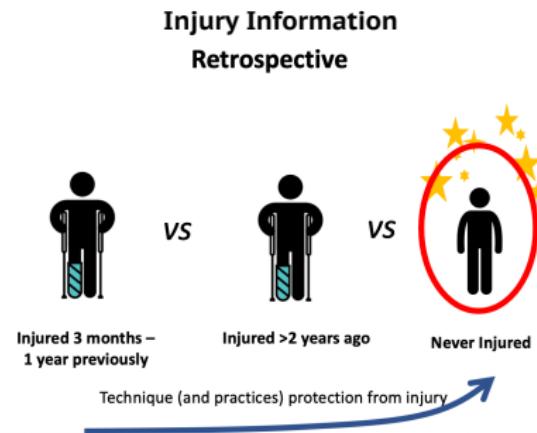
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- 2,295 individuals measured under different conditions (75,732 trials in total).
- Healthy controls and individuals with impairments in the hip, knee, ankle and calcaneus.

Motivating Dataset

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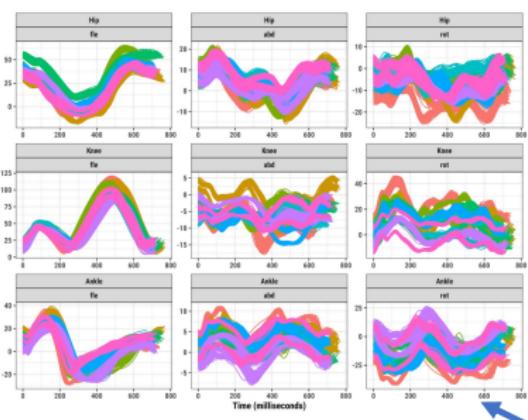


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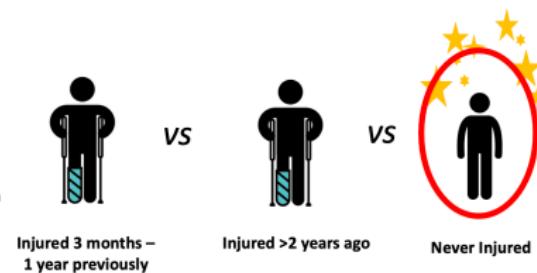


Motivating Dataset

Multivariate Functional Data



Injury Information
Retrospective



Covariates Affecting Running Technique



adjust for

Initial Approach (Gunning et al., 2024b)

- “Start simple” → focus on average bilateral hip and knee flexion angles.
- Regress the average bivariate functions on scalar covariates, e.g., injury status, sex, speed ...

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$$\begin{array}{c} \text{Y}(t) \\ \left[\begin{array}{cc} \text{green wavy line} & \text{green wavy line} \\ \text{green wavy line} & \text{green wavy line} \\ \vdots & \vdots \\ \vdots & \vdots \\ \text{blue wavy line} & \text{blue wavy line} \\ \text{blue wavy line} & \text{blue wavy line} \end{array} \right] \end{array} = \begin{array}{c} \text{X} \\ \left[\begin{array}{cc} 1 & \textcolor{red}{1.5} \\ 1 & 0 \\ \vdots & \vdots \\ \vdots & \vdots \\ 1 & \textcolor{red}{1.2} \\ 1 & 0 \end{array} \right] \end{array} + \begin{array}{c} \text{B}(t) \\ \left[\begin{array}{cc} \text{green wavy line} & \text{green wavy line} \\ \text{red wavy line} & \text{red wavy line} \end{array} \right] \end{array} + \begin{array}{c} \text{Z} \\ \left[\begin{array}{ccc} 1 & \cdots & 0 \\ 1 & \cdots & 0 \\ \vdots & \ddots & \vdots \\ \vdots & \ddots & \vdots \\ 0 & \cdots & 1 \\ 0 & \cdots & 1 \end{array} \right] \end{array} + \begin{array}{c} \text{U}(t) \\ \left[\begin{array}{cc} \text{green wavy line} & \text{green wavy line} \\ \vdots & \vdots \\ \text{blue wavy line} & \text{blue wavy line} \end{array} \right] \end{array} + \begin{array}{c} \text{E}(t) \\ \left[\begin{array}{cc} \text{green wavy line} & \text{green wavy line} \\ \text{blue wavy line} & \text{blue wavy line} \\ \vdots & \vdots \\ \vdots & \vdots \\ \text{blue wavy line} & \text{blue wavy line} \end{array} \right] \end{array}$$

Initial Approach (Gunning et al., 2024b)

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- Developed a simple, flexible and scalable multivariate functional mixed effects modelling approach based on the basis modelling approach of Morris and Carroll (2006).

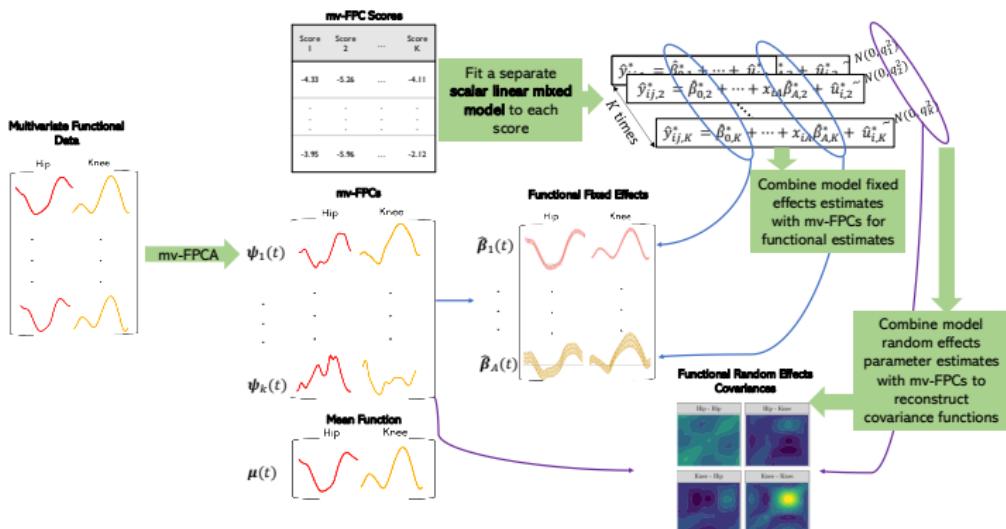
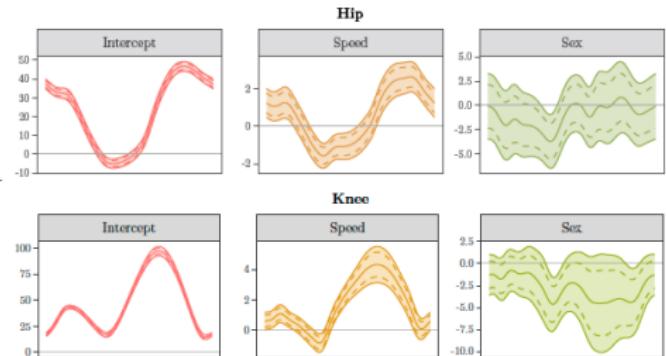


Figure: Flowchart of methodology.

Initial Approach (Gunning et al., 2024b)

Estimation and Inference

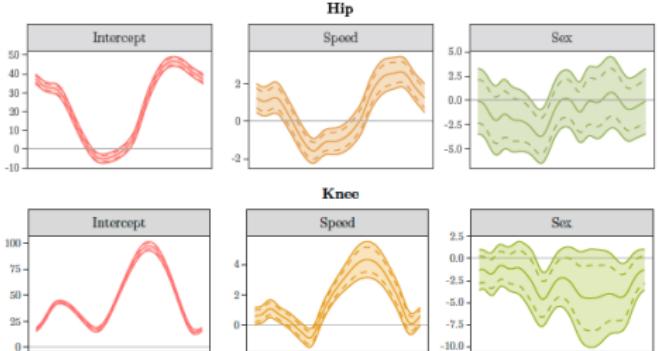
- Bayesian approach of Morris and Carroll (2006) uses MCMC for estimation and inference of functional parameters.
- We adapt resampling and simulation ideas from Crainiceanu, Staicu, et al. (2012) to implement in a frequentist setting using lme4.



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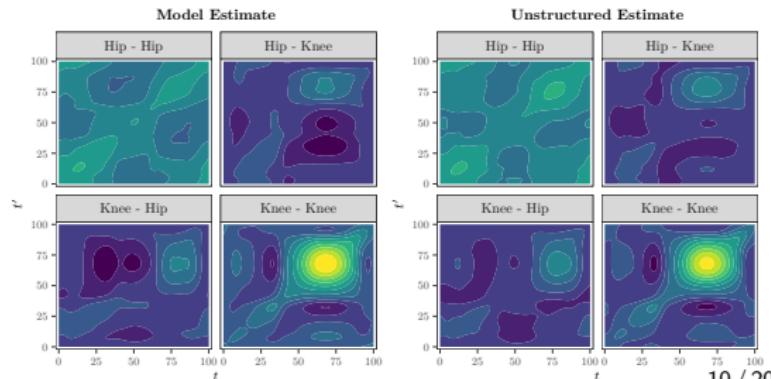
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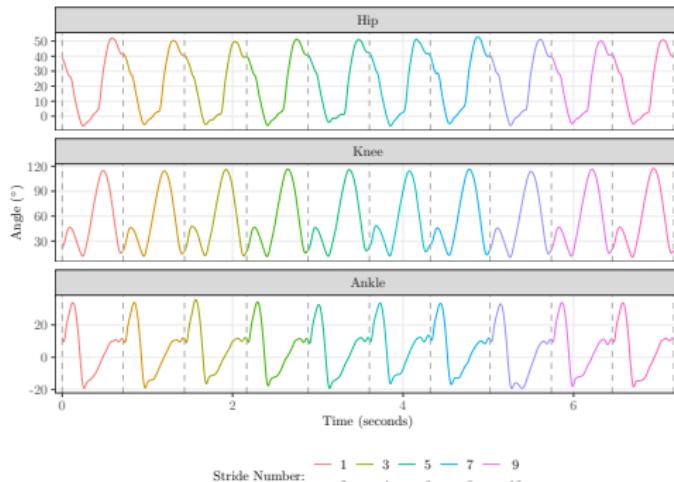
Covariance Analysis

- Modelling each basis coefficient separately makes potentially limiting assumptions on the form of the functional random effects and error covariances.
- We propose to check this by using an extension of multilevel FPCA (Di et al., 2009) to calculate unstructured estimates to compare with.



Summary and Limitations of Initial Approach

- Simple methodological approach combines existing methodologies, e.g., Morris and Carroll (2006), Di et al. (2009), and Crainiceanu, Staicu, et al. (2012).
- Scientific results consistent with and expand upon existing biomechanical literature (e.g., based on scalar values).
- **However, working with an average stride is potentially wasteful.** For just a one-minute run, this is a data reduction of almost 100 : 1.



Multivariate Multilevel Longitudinal Functional Model (Gunning et al., 2024a)

Solution: Develop a structured functional model for all of the strides:

- Hip, knee and ankle → **multivariate**.
- Multiple strides measured bilaterally for each subject → **multilevel**.
- Strides have a natural time ordering → **longitudinal**.

Multivariate Multilevel Longitudinal Functional Model (Gunning et al., 2024a)

Our multivariate multilevel longitudinal functional model is

$$\mathbf{y}_{ijl}(t) = \boldsymbol{\beta}_0(t, T_{ijl}) + \sum_{a=1}^A x_{ija} \boldsymbol{\beta}_a(t) + \mathbf{u}_i(t, T_{ijl}) + \mathbf{v}_{ij}(t, T_{ijl}) + \boldsymbol{\varepsilon}_{ijl}(t),$$

where

- $\mathbf{y}_{ijl}(t) = \left(y_{ijl}^{(\text{hip})}(t), y_{ijl}^{(\text{knee})}(t), y_{ijl}^{(\text{ankle})}(t) \right)^\top$,
- $t \in [0, 100]\text{(\%)}$ ("functional time") and $T \in [0, 1]$ ("longitudinal time"), and
- $l = 1, \dots, n_{ij}, j \in \{\text{left, right}\}$, and $i = 1, \dots, N$.

Multivariate Multilevel Longitudinal Functional Model (Gunning et al., 2024a)

Our multivariate multilevel longitudinal functional model is

$$\mathbf{y}_{ijl}(t) = \underbrace{\beta_0(t, T_{ijl})}_{\text{Intercept}} + \sum_{a=1}^A x_{ija}\beta_a(t) + \mathbf{u}_i(t, T_{ijl}) + \mathbf{v}_{ij}(t, T_{ijl}) + \varepsilon_{ijl}(t),$$

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$$\mathbf{y}_{ijl}(t) = \beta_0(t, T_{ijl}) + \underbrace{\sum_{a=1}^A x_{ija} \beta_a(t)}_{\text{Fixed Effects}} + \mathbf{u}_i(t, T_{ijl}) + \mathbf{v}_{ij}(t, T_{ijl}) + \varepsilon_{ijl}(t),$$

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Multivariate Multilevel Longitudinal Functional Model (Gunning et al., 2024a)

Again, take a basis modelling approach¹ by representing

$$\mathbf{y}_{ijl}(t) = \sum_{k=1}^K y_{ijl,k}^* \psi_k(t),$$

where $y_{ijl,k}^*$ are scalar basis coefficients and $\psi_k(t)$ are multivariate basis functions in the *functional direction* (we choose mv-FPCs).

Reduces the problem to fitting a series of K mixed models of the form:

$$y_{ijl,k}^* = \beta_{0,k}^*(T_{ijl}) + \sum_{a=1}^A x_{ia} \beta_{a,k}^* + u_{i,k}^*(T_{ijl}) + v_{ij,k}^*(T_{ijl}) + \varepsilon_{ijl,k}^*,$$

which is a standard multilevel functional model (Di et al., 2009) in the *longitudinal direction*.

¹ Similar idea proposed in univariate two-level case by Park and Staicu (2015).

Multivariate Multilevel Longitudinal Functional Model (Gunning et al., 2024a)

Again, we use basis expansions, this time in the longitudinal direction:

$$\beta_{0,k}^*(T) = \sum_{d=1}^D \beta_{0,k,d}^* \xi_d(T), \quad u_{i,k}^*(T) = \sum_{d=1}^D u_{i,k,d}^* \xi_d(T) \quad \text{and} \quad v_{ij,k}^*(T) = \sum_{d=1}^D v_{ij,k,d}^* \xi_d(T).$$

Question: Which basis functions should we use for $u_{i,k}^*(T)$ and $v_{ij,k}^*(T)$?

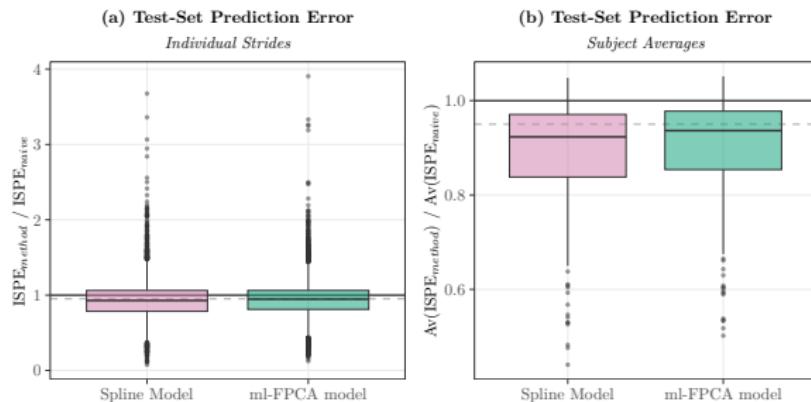


Figure: Representation using pre-specified spline (pink) and empirically-determined ml-FPCA basis (Cui et al., 2022, green) basis functions gives similar results.

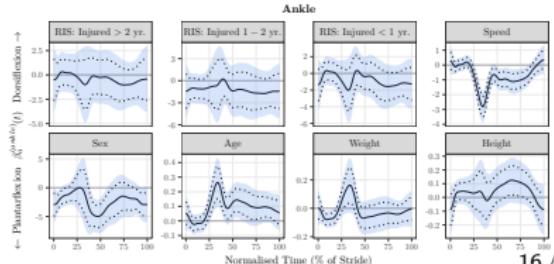
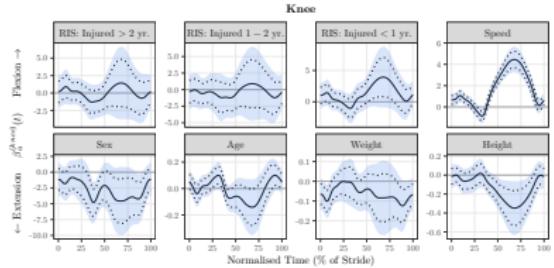
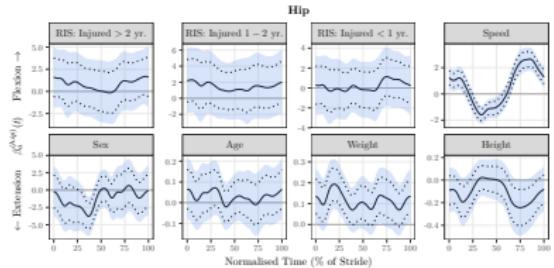
Results: Fixed Effects

- Fixed effects estimates

$$\hat{\beta}_a(t) = \sum_{k=1}^K \hat{\beta}_{a,k}^* \psi_k(t).$$

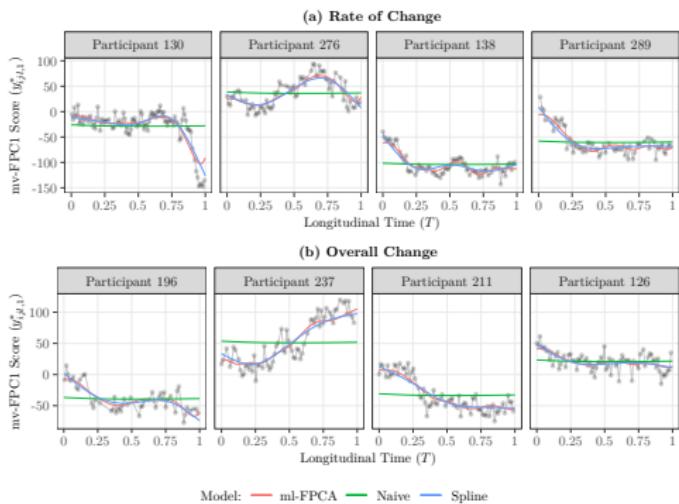
- Simultaneous bands account for multiple comparisons across t and the hip, knee and ankle. Obtained using bootstrap and simulation approaches^a.
- Scientific results consistent with existing biomechanical knowledge.

^aSee Faraway (1997), Ruppert, Wand, and Carroll (2003), Crainiceanu, Staicu, et al. (2012), and Cui et al. (2022).



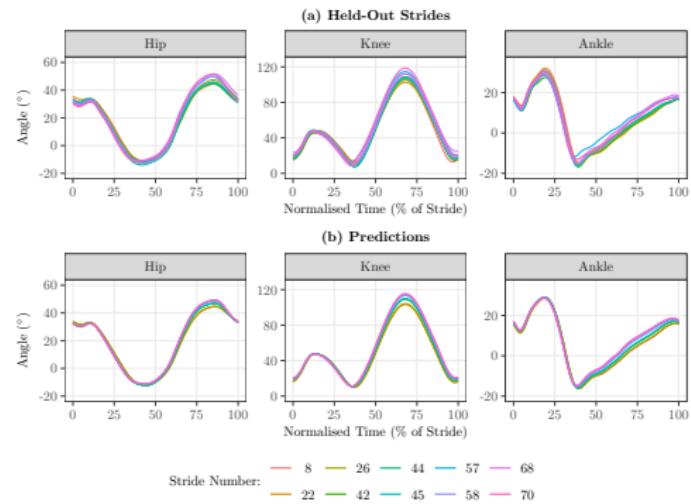
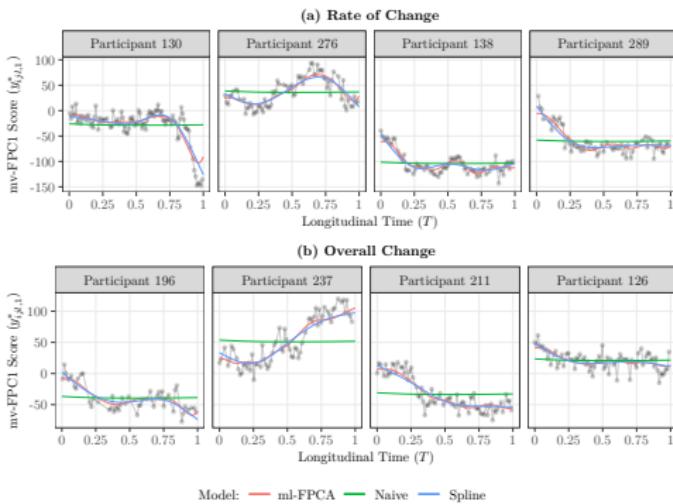
Results: Random Effects

Rates of change of $\hat{\mathbf{u}}_i(t, T)$ and $\hat{\mathbf{v}}_{ij}(t, T)$ w.r.t. T characterise changes over the course of the treadmill run.



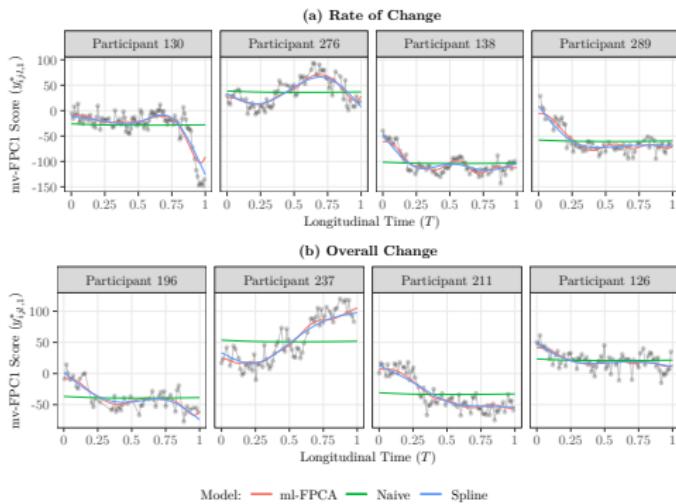
Results: Random Effects

Rates of change of $\hat{\mathbf{u}}_i(t, T)$ and $\hat{\mathbf{v}}_{ij}(t, T)$ w.r.t. T characterise changes over the course of the treadmill run.

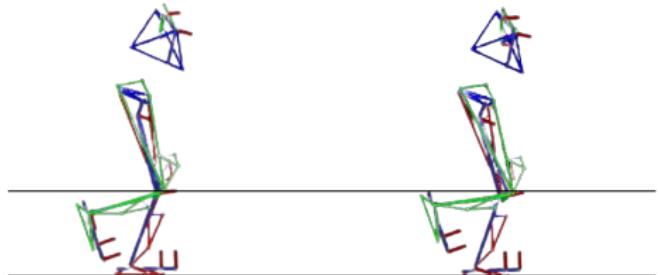


Results: Random Effects

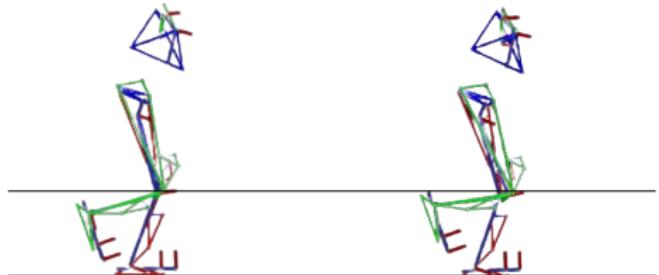
Rates of change of $\hat{\mathbf{u}}_i(t, T)$ and $\hat{\mathbf{v}}_{ij}(t, T)$ w.r.t. T characterise changes over the course of the treadmill run.



(c) Start of Treadmill Run



(d) End of Treadmill Run



Summary

- Simple and flexible approach for modelling streams of smooth multivariate functional data that arise in biomechanics.
- Characterise population-level fixed effects and intra-individual longitudinal changes during the treadmill run – practically meaningful insights.
- Potential to use the model in different contexts and extend it to more complex settings.

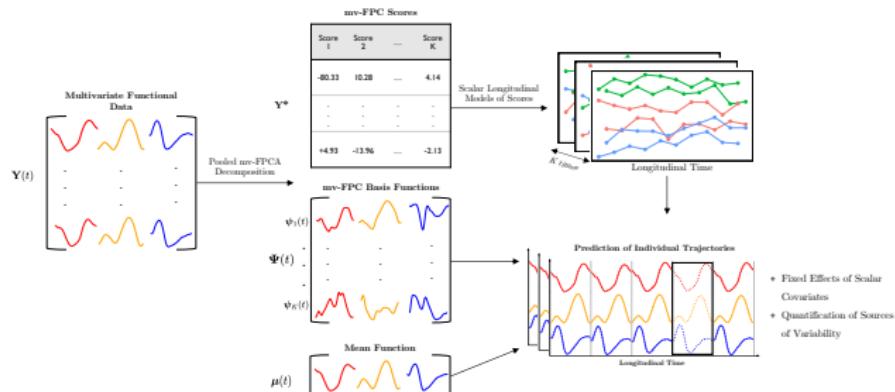


Figure: Summary of the modelling approach.

Thank you!

More Information

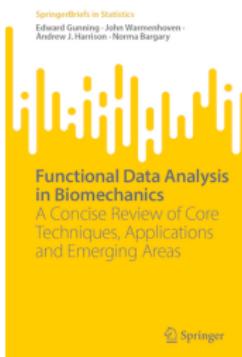
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- E Gunning et al. (2024b). *Analysing Kinematic Data from Recreational Runners using Functional Data Analysis*. arXiv:2408.08200 [stat]
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Upcoming Book:



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