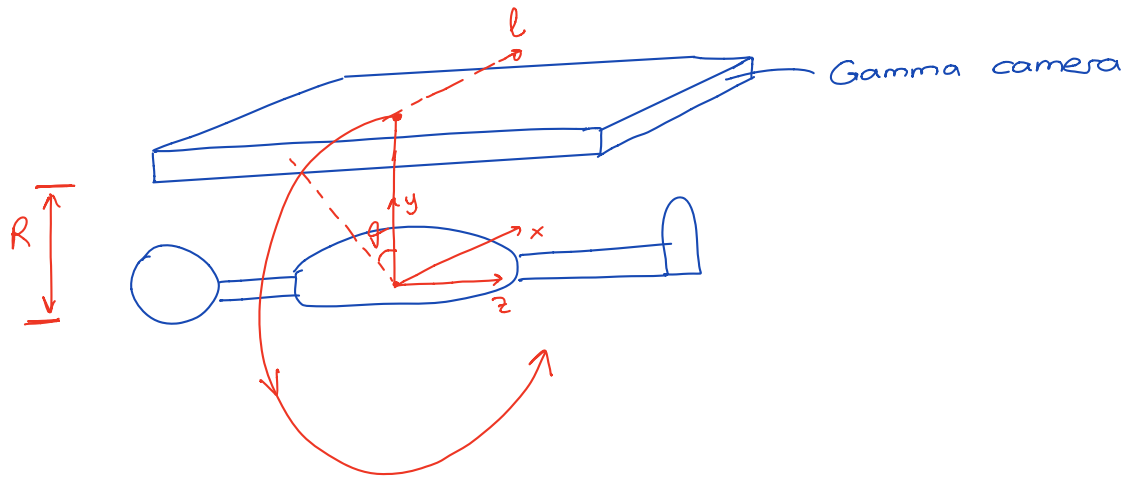
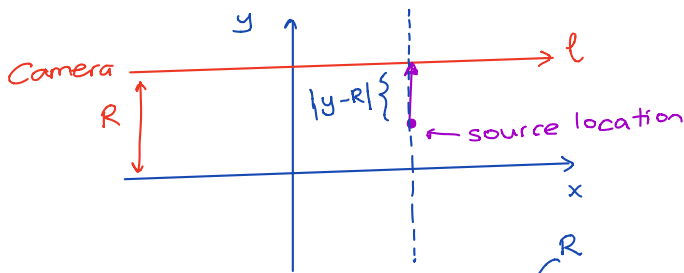


SPECT Image Formation: change coordinate system

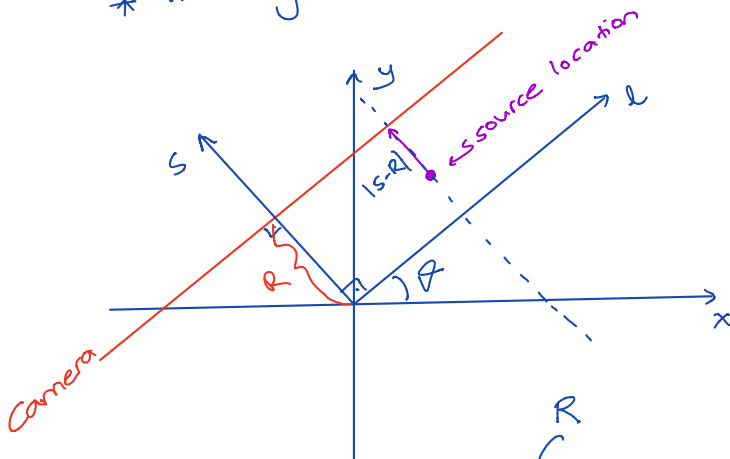


* when $\theta = 0$



$$\phi(z, l) = \int_{-\infty}^R \frac{A(x, y, z)}{4\pi (y-R)^2} \cdot \exp \left\{ - \int_y^R \mu(x, y', z; E) dy' \right\} dy$$

* In general



$$L(l, \theta) = \{ (x, y) | x \cos \theta + y \sin \theta = l \}$$

$$x(s) = l \cos \theta - s \sin \theta$$

$$y(s) = l \sin \theta + s \cos \theta$$

$$\phi(l, \theta) = \int_{-\infty}^R \frac{A(x(s), y(s))}{4\pi (s-R)^2} \exp \left\{ - \int_s^R \mu(x(s'), y(s'); E) ds' \right\} ds$$

Too complicated because of unknown μ in between (2)
the source and the camera, and also
inverse square law.

* Ignore inverse square law and attenuation.
→ works reasonably well in practice

Then,

$$\begin{aligned}\phi(l, \theta) &= \int_{-\infty}^{\infty} A(x(s), y(s)) ds \\ &= \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} A(x, y) \delta(x \cos \theta + y \sin \theta - l) dx dy\end{aligned}$$

⇒ same as CT imaging equation

* There is one difference: in CT, we first take
the logarithm of the data to arrive at the
necessary projections:

$$g(l, \theta) = -\ln\left(\frac{I_l}{I_0}\right)$$

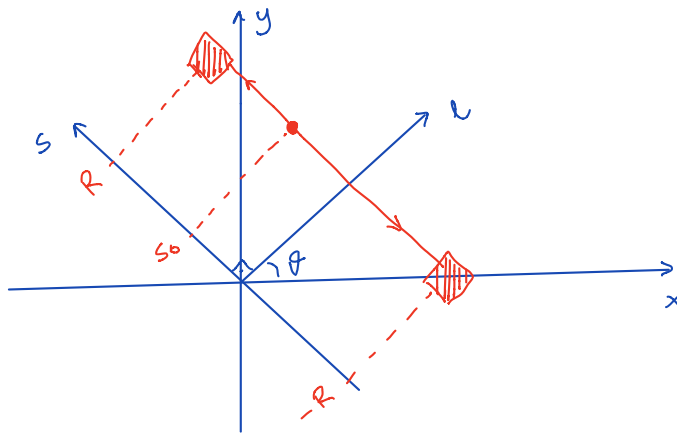
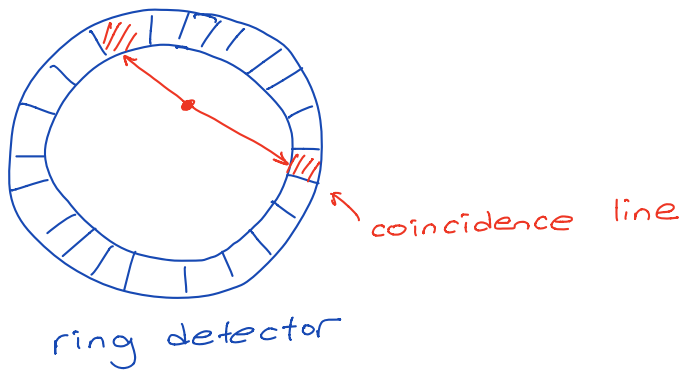
* In SPECT, recorded # of photons directly provides
the projection data.

Reconstruction: same as in CT ⇒ filtered backprojection

Iterative reconstruction: First ignore inverse square law
and attenuation and reconstruct.
Then incorporate attenuation
and depth dependency and
reconstruct again,

PET Image Formation :

3



line of response : the line joining two opposing detectors that identified an event.

\Rightarrow event must have happened along that line.

$$N_c(s_0) = N_0 \cdot \exp \left\{ - \int_{s_0}^R \mu(x(s'), y(s'); E) ds' \right\} \cdot \exp \left\{ - \int_{-R}^{s_0} \mu(x(s'), y(s'); E) ds' \right\}$$

\uparrow coincident photon count
 \uparrow # of annihilations
 $\underbrace{\hspace{10em}}$ % that survive and hit the upper detector
 $\underbrace{\hspace{10em}}$ % that survive and hit the lower detector
 $\underbrace{\hspace{15em}}$ % of coincident photons

$$= N_0 \cdot \exp \left\{ - \int_{-R}^R \mu(x(s'), y(s'); E) ds' \right\}$$

$\underbrace{\hspace{15em}}$ total attenuation along the line independent of source location.

* Over the whole line :

$$\begin{aligned} \phi(l, \theta) &= K \cdot \int_{-R}^R A(x(s), y(s)) \cdot \exp \left\{ - \int_{-R}^R \mu(x(s'), y(s'); E) ds' \right\} ds \\ &= K \cdot \underbrace{\int_{-R}^R A(x(s), y(s)) ds}_{\text{total events along the line}} \cdot \underbrace{\exp \left\{ - \int_{-R}^R \mu(x(s), y(s); E) ds \right\}}_{\text{attenuation along the line}} \end{aligned}$$

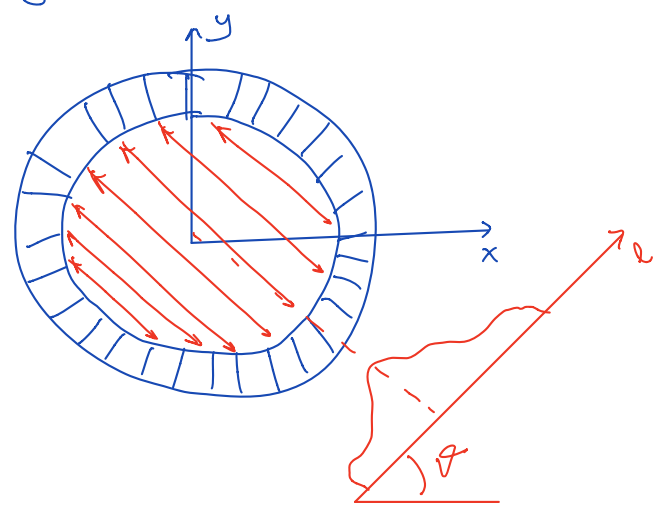
Some constant

* if we ignore attenuation:

$$\phi(l, \theta) = K \cdot \int_{-R}^R A(x(s), y(s)) ds$$

} projection of $A(x, y)$ along angle θ

* organize the response into parallel-ray projection



* Reconstruction : filtered backprojection

* Attenuation correction : if $\mu(x, y)$ were known

$$\phi_c(l, \theta) = \frac{\theta(l, \theta) \quad \text{actual measured activity}}{K \cdot \underbrace{\exp \left\{ - \int_{-R}^R \mu(x(s), y(s); E) ds \right\}}_{\text{attenuation}}} = \int_{-R}^R A(x(s), y(s)) ds$$

@511 keV in PET

$\mu(x,y)$ can be reconstructed from a CT scan.
 ↑
 @ 80-120 keV

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→ need to estimate μ @ 511 keV.

⇒ motivation for combined PET/CT scanner.