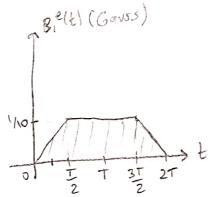
$$B_{1}^{e}(t) = \begin{cases} t & \frac{2}{10T}, & 0 \le t \le \frac{T}{2} \\ \frac{1}{10}, & \frac{T}{2} \le t \le \frac{3T}{2} \\ \frac{4}{10}, & \frac{2}{10T} t, & \frac{3T}{2} \le t \le 2T \end{cases}$$



$$\frac{|x+z|^{2}}{|oT|} \times |o^{-4}|, \quad 0 \le t \le \frac{\pi}{2}$$

$$\times |x|^{2} + |x|^{2} \times |x|^{2} + |x|^{2} \times |x|^{2} + |x|^{2} \times |$$

b)
$$\frac{\pi}{2} = 2\pi + \frac{3\pi}{20} \times 10^{-4}$$

$$T = \frac{5}{3\pi} \times 10^{4} = \frac{5}{3(42.58 \times 10^{6})} \times 10^{4} \Rightarrow T = 0.39142 \text{m/s}$$

DZ

E fe Even Cayon! 2 1903359

M2(t1= Mo(1-e^{-t/1}) + M2(0+)e^{-t/T}

Mxy (t1= Mosmx e⁵⁰ e^{-t/T2} > Rotating frame

TR>>>T2

Mz is defined at the steady state valve. So, if we try to calculate Mz after n repetitions, instead of Mo, we must use Mz of for the initial magnetization, s.t.

M2^(t|= M0(1-e-t/T1) + M25005de-t/T1 (1)

Thus $M_{\tilde{z}}^{\Lambda + 1}(0) = M_{\tilde{z}}^{\Lambda}(TR) = M_{\tilde{z}}^{SS}(2)$ (Pulses are separated)

50, if we plug (2) in (1):

M2"(TR)= M.(1-e-TR) + M250 cosx e-TR
11 (TR)= M.(1-e-TR) + M250 cosx e-TR
11 (TR)= M.(1-e-TR)

 $M_{2}^{55}(1-\cos\alpha e^{-\frac{TR}{T_{1}}}) = M_{0}(1-e^{-\frac{TR}{T_{1}}})$ $M_{2}^{55}=M_{0}\frac{1-e^{-\frac{TR}{T_{1}}}}{1-\cos\alpha e^{-\frac{TR}{T_{1}}}}$

Since M2 55 replaces Mo for initial valves,

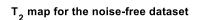
 $M_{xy}(t) = M(0^{\dagger}) \sin \alpha e^{i\beta t} e^{-t/T_2}$ $M_{xy}(t) = M_z^{55} \sin \alpha e^{i\beta t} e^{-t/T_2}$

Efe Eren Ceyani 2 (903355 Gx=Gy=Gz=+16/cm Perred Z=10cm DZ=5mm a) DV = DZ &6Z = (5x10 cm) (42.58 MHZ) (10-4 Tm) = 2.129 KHZ $FWHM_{\lambda} = \frac{1}{K_{\lambda}e^{\lambda}e^{\lambda}} = (MM) = K_{\lambda}e^{\lambda}e^{\lambda}e^{\lambda} = (MM) = (MM)$ b) Dx=1mm, Dy-2mm FWHMy = 1 = 2 mm = Ky, extent = 0.5 mm' = (b=0.25 mm') c) fovy= 10cm => [\(\text{Ley= 0.1cm-1} = 0.01mm-1 \) Ky, extent = [50 lines] $ty = \frac{\Delta ky}{fGy} = \frac{10^{-1}}{(c/m)(\frac{10^{2.58}\times10^{6}Hz}{10^{4}g})(\frac{16}{c/m})}$ d) for = 66x FOVx = 412.58x106Hz 10cm = [42.58kHz] e) Assuming we do not read data during moving to (a,b). All amplitudes are ± 1 G/cm. 0.0235 MS ADC 0.0235ms Total (2.35ms)(3)+(0.0235ms)(2) Time to go to Time to cover them = 2x1.17ms = 2.35m APC time ta: 5. 117m = 7.097ms

Efe Fren Ceyoni

a)
$$IMG_1(x,y) = AM_0(x,y) sind e^{-\frac{TE_1}{T_2(x,y)}}$$
 $IMG_2(x,y) = AM_0(x,y) sind e^{-\frac{TE_2}{T_2(x,y)}}$
 $\frac{IMG_2(x,y)}{IMG_2(x,y)} = e^{-\left(\frac{TE_1 - TE_2}{T_2(x,y)}\right)}$

(b)



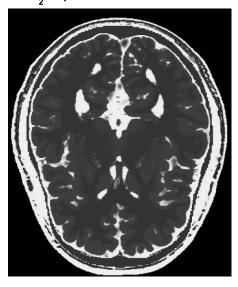


Figure 1.1.1 T₂ map for the noise-free dataset using the derived equation

(c)

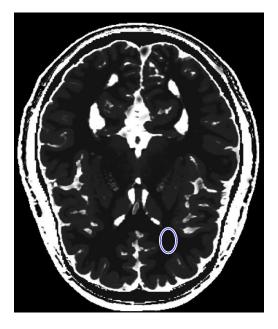


Figure 1.2.1 ROI ellipse for white matter, noise-free image. Estimated T_2 value for white matter is $70.05 \, \text{ms}$.

(d)

I used the same mask as in part (c), so there was no need to plot anything. Estimated T_2 value for white matter in the noisy T_2 map is 71.26ms. Percentage-wise deviation from the noise-free dataset is 1.74%.

(e)

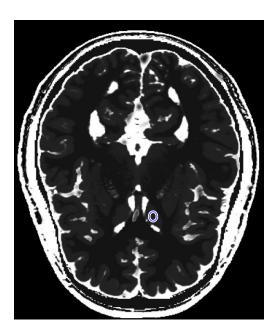


Figure 1.3.1 ROI ellipse for gray matter, noise-free image. Estimated T_2 value for gray matter is 83.97 ms.

Estimated T_2 value for gray matter in the noisy T_2 map is 84.50ms. Percentage-wise deviation from the noise-free dataset is 0.63%.

(f)

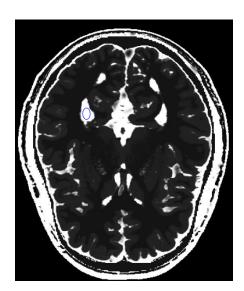


Figure 1.4.1 ROI ellipse for cerebrospinal fluid (CSF), noise-free image. Estimated T_2 value for CSF is 327.02ms.

Estimated T_2 value for CSF in the noisy T_2 map is 348.74ms. Percentage-wise deviation from the noise-free dataset is 6.64%.

(g)

The largest deviation in T_2 estimation was seen in CSF. Between the three tissues, CSF has the T_2 value, so in T_2 weighted contrast images, CSF is the brightest between the tissues. Hence, even a small noise in the scan will be strengthened drastically.

Code

```
%Homework 4 - Q4
dataset = load("brainT2 mri.mat");
TE = dataset.TE;
image1 = dataset.image1;
image2 = dataset.image2;
TR = dataset.TR;
flip degree = dataset.flip degree;
image1_noisy = dataset.image1 noisy;
image2 noisy = dataset.image2 noisy;
응응 b
T2map = (TE(1)-TE(2))./(log(image2)-log(image1));
figure;
imshow(abs(T2map),[0 350]);
title("T 2 map for the noise-free dataset");
응응 C
figure;
imshow(T2map, []);
mask wm = roiellipse;
T2 est wm = mean(T2map(mask wm));
%T2 \text{ est wm} = 70.0480 \text{ ms}
응응 d
T2map noisy = (TE(1)-TE(2))./(log(image2 noisy)-
log(image1 noisy));
T2 est wm noisy = mean(T2map noisy(mask wm));
%T2 est wm noisy = 71.2636 ms
deviation wm = (abs(T2 est wm -
T2 est wm noisy)/T2 est wm)*100;
deviation wm = 1.7355
응응 e
figure;
imshow(T2map, []);
mask gm = roiellipse;
T2 est gm = mean(T2map(mask gm));
%T2 \text{ est gm} = 83.9685 \text{ ms}
```

```
T2 est gm noisy = mean(T2map noisy(mask gm));
T2 est gm noisy = 84.5014 ms
deviation gm = (abs(T2 est gm -
T2 est gm noisy)/T2 est gm) *100;
deviation gm = 0.6347%
%% f
figure;
imshow(T2map, []);
mask csf = roiellipse;
T2 est csf = mean(T2map(mask csf));
%T2 \text{ est gm} = 327.0154 \text{ ms}
T2 est csf noisy = mean(T2map noisy(mask csf));
T2 est csf noisy = 348.7403 ms
deviation csf = (abs(T2 est csf -
T2 est csf noisy)/T2 est csf)*100;
%deviation csf = 6.6434%
```