**Cognitive, Pathological and Prognostic Profiles of Different Brain Ages in the Early Alzheimer’s Disease Continuum**

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Brain aging is characterized by anatomical and molecular changes. Brain age can differ from chronological age (“brain age gap”, *BAG*); and this difference, typically estimated from structural MRI, is associated with various intracerebral abnormalities, such as e.g. observed in Alzheimer’s disease (AD). 18F-Fluorodeoxyglucose PET (FDG-PET) is considered to represent an earlier indicator of neurodegeneration compared to structural MRI. Possibly, processes associated with brain aging are captured by FDG-PET with greater sensitivity compared to structural MRI. Here, we compare the accuracy of brain age estimation from FDG-PET and structural MRI, and we associate BAG derived each modality with cognitive impairment and AD biomarkers. Furthermore, we present cutoffs for the prediction of cognitive outcome after two years. Analyses were conducted in individuals without (CN), with subjective cognitive decline (SCD) and with mild cognitive impairment (MCI).

**Methods**: Machine learning algorithms were trained to estimate brain age from 376 matched T1-weighted MRI or FDG-PET scans of CN+SCD from the Alzheimer’s Disease Neuroimaging Initiative and validated in internal and external test sets. BAG was correlated with measures of amyloid and tau pathology in CN+SCD and MCI (n=596). Finally, BAG was used to predict cognitive outcome after two years using logistic regression. Cutoffs for cognitive decline were estimated from the logistic regression output.

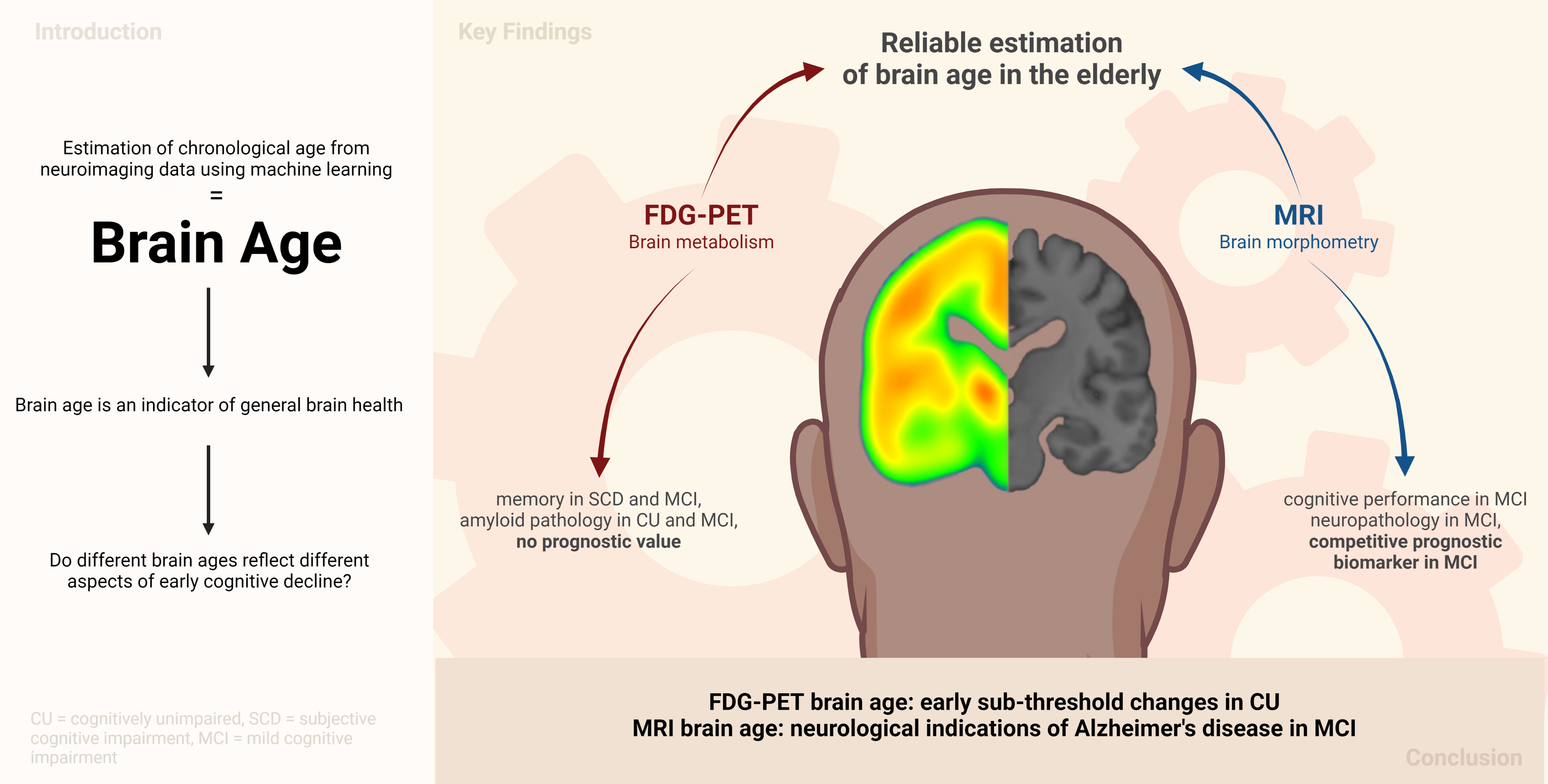
**Results**: FDG-PET (mean absolute error, *MAE*=2.46 years) and MRI (MAE=1.96 years) both estimated chronological age well. Both, FDG-PET- and MRI-derived BAG were correlated with amyloid load across groups and with cognitive performance in MCI. FDG-PET-derived BAG exceeding 0.85 years was indicative of pending cognitive impairment in CN+SCD, while an MRI-derived BAG beyond 2.23 years suggested development of dementia in MCI. BAG from the respective other modality was not/less indicative of cognitive outcome.

**Conclusion**:

Brain age is reliably estimated from FDG-PET or MRI. FDG-PET-derived BAG is more sensitive to early intracerebral changes related to cognitive deterioration in CN+SCD, while early features indicative of impending dementia in MCI are better reflected by MRI-derived BAG.

RUNNING TITLE: FDG-PET or MRI for Brain Age Estimation

**Graphical Abstract**



**1 Introduction**

Brain aging entails changes in cognitive performance, as well as brain function and structural parameters of brain integrity. Brain age can be modeled using machine learning algorithms by estimating a person’s chronological age from their neuroimaging data. Deviations of brain age from chronological age (the *brain age gap, “BAG”*) are associated with a variety of neurological conditions. Of special interest in this research field are neurodegenerative disease, including the Alzheimer’s disease (AD) continuum1–3. A recent study1 showed that BAG is associated with positron emission tomography (PET) AD biomarkers in patients with mild cognitive impairment (MCI), and that BAG is significantly elevated in individuals with impending cognitive deterioration/AD. These results motivate further research into the unique contribution of BAG as a marker of brain health and as a prognostic biomarker of cognitive impairment in the early stages of AD (MCI and subjective cognitive decline (SCD)).

Age-related changes in the brain are most evident in the brain’s anatomy, such as loss of brain volume (atrophy), and metabolism (neuronal dysfunction). Brain atrophy and metabolism can be quantified by T1-weighted magnetic resonance imaging (MRI) and 18F-Fluorodeoxyglucose-PET (FDG-PET), respectively. FDG-PET is considered to be an earlier indicator of neurodegeneration compared to structural MRI, as neuronal dysfunction precedes atrophy (i.e., neuronal loss) and regional proneness to the aging process is different when observed with FDG-PET or MRI4. It can therefore be assumed that different age- or disease-related processes are captured by the two modalities. To date, however, brain age estimation, in the vast majority of cases, is performed using MRI rather than FDG-PET. Only one recent study compared the two modalities and showed slightly better performance when using FDG-PET1. However, in this study, FDG-PET was not investigated independently of MRI, as FDG-PET was preprocessed using partial volume correction. This argues for further exploration of FDG-PET-derived BAG, and its potentially superior performance in delineating the earliest deviations from normal aging when cognitive impairment is not yet evident.

Here, we investigated the potential of FDG-PET and MRI separately as input for brain age estimation, with a particular focus on the early stages of the AD continuum. First, we estimated brain age in cohorts of individuals who were either cognitively normal (CN), had subjective cognitive decline (SCD), or mild cognitive impairment (MCI). Second, we calculated BAG and compared associations of FDG-PET- and MRI-derived BAG with cognitive performance and AD neuropathology in these cohorts. Finally, we evaluated the prognostic capacity of BAG for the prediction of cognitive outcome by using a logistic regression classifier to predict cognitive outcome from BAG and established risk factors of cognitive decline.

**2 Methods**

**2.1 Participants**

Baseline T1-weighted MRI and FDG-PET scans of 276 CN (*CNADNI*) whose MRI and FDG-PET scans were less than a year apart (mean = 30 days, SD = 23 days) were acquired from the Alzheimer's Disease Neuroimaging Initiative (ADNI) database ([adni.loni.usc.edu](https://ida.loni.usc.edu/collaboration/access/adni.loni.usc.edu)) to train our brain age estimation frameworks. The primary goal of the ADNI study has been to test whether biological markers and clinical and neuropsychological assessments can be combined to measure the progression of MCI and dementia. An additional 49 MRI and FDG-PET scans of CN were acquired from the Open Access of Imaging Studies-3 database5 (OASIS-3, https://www.oasis-brains.org/, *CNOASIS*) to validate the models in an external dataset (within-group, out-of-sample validation). Finally, we assessed brain age in SCD and MCI patient groups from the ADNI (out-of-group, within-sample), OASIS-3 and DZNE-Longitudinal Cognitive Impairment and Dementia Study6 (DELCODE) studies (out-of-group, out-of-sample) for an overview, see **Table 1**). To be included, participants in all samples had to be older than 60 years at the time of their scan. CN, SCD and MCI diagnoses from ADNI, OASIS, and DELCODE followed the current recommendations for the respective groups7,8 (details provided in the Supplementary Materials (SM) section 1a).

**2.2 Acquisition & Preprocessing of MRI and FDG-PET Scans**

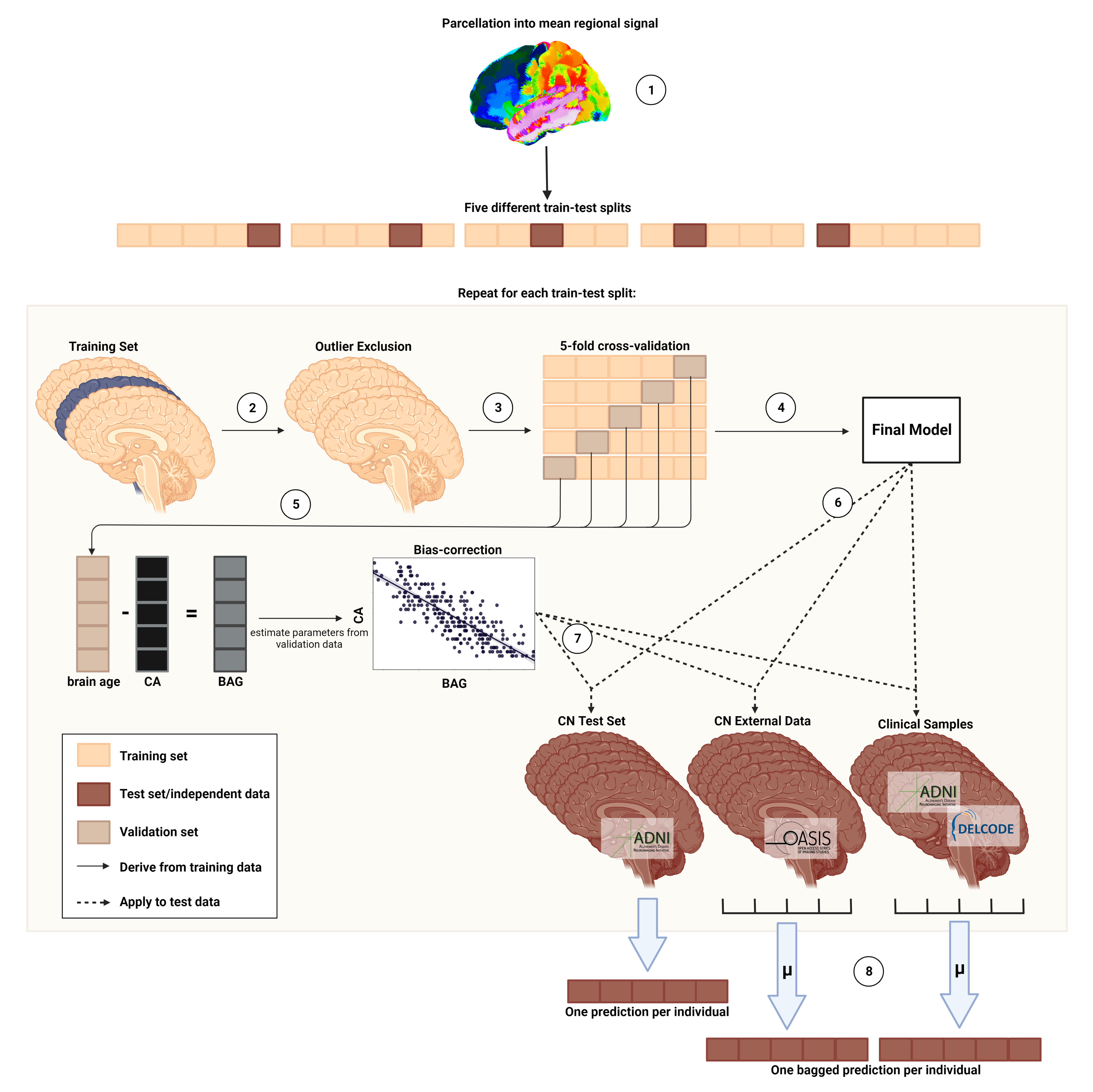
FDG-PET scans in ADNI and OASIS were acquired dynamically 30-60 minutes (6x5 min frames) after injection with an average dose of 185 MBq (5 mCi). The DELCODE FDG-PET data were acquired 40-60 minutes (4x5 min frames) after injection with an average dose of 170-180 MBq. T1-weighted MRI scans were acquired according to previously published MRI acquisition protocols5,6,9 and were preprocessed with the CAT toolbox (version 12.5) in SPM12 based on MATLAB (r2019b). After preprocessing, both FDG-PET and MRI images were in the standard MNI152 space (see details in the SM section 1b).

**2.3 Estimation of brain age**

To estimate brain age, we implemented a pipeline (**FIGURE 1)** in Python 3.8.5 using the Julearn library (<https://juaml.github.io/julearn/main/index.html>), which is based on scikit-learn10. The same pipeline was run independently for MRI and FDG-PET and was evaluated by means of the mean absolute error (MAE) between chronological and brain age. First, signal of 90 cortical and subcortical regions of interest was extracted for the respective modality (MRI: gray matter volume, FDG-PET: SUVR) using the automated anatomical labeling (AAL) atlas11. Next, we applied a five-fold nested cross-validation (CV) approach, wherein the CNADNI sample was split into five different training and test sets, stratified by age bin (<74, 75-84 and >85 years) for the outer CV, and each training set was again split into five different training and validation folds for the inner CV.

Linear-kernel support vector regression (SVR) and relevance vector regression (RVR) with were used to estimate brain age as they are recommended for brain age estimation with small sample sizes12. Prior to the inner CV loop, outlier exclusion was performed in the outer CV loop (SM section 1c). The inner CV loop was used to select optimal hyperparameters (SM section 1d) and the final model was selected across SVR and RVR based on the MAE before bias correction on the validation folds. Bias correction parameters were estimated based on predictions yielded from the validation folds13 (SM section 1e). Subsequently, the final model was used to estimate brain age in the test and clincal samples and bias correction was applied.

**FIGURE 1. Nested cross-validation approach for brain age prediction.** Five different train-test splits were used to train and test the models. (1) Region-of-interest parcellation. (2) Outlier exclusion. (3) Five-fold CV. (4) Selection of final model. (5) Bias correction. (6) Estimation of brain age in test sets. (7) Bias correction in test sets. (8) Bagging. BAG = brain age gap; CA = chronological age; CV = cross-validation. Created with BioRender.



As a result of the nested CV approach, we obtained five final models per modality. Thus, per modality, we obtained one brain age estimate per (non-outlier) subject in the CNADNI sample, and five estimates per subject in the OASIS and patient samples. In the OASIS and patient samples, the average of the five estimates was treated as the final brain age estimate (*bagging*). The feature importance (δ) of each brain region was assessed by considering the learned weights of the final models.

**2.4 Statistical analyses**

BAG was calculated for each individual as the difference between brain age and chronological age, such that higher bag reflected more advanced brain age. The accuracy of brain age estimation from MRI or FDG-PET was assessed by comparing the MAE of brain age estimations from the two modalities using a paired t-test in the CNADNI sample. To assess generalizability of our brain age frameworks, we compared the MAE between CNADNI and CNOASIS by means of a standard t-test, using either MRI or FDG-PET as input for brain age estimation. To assess advancement of brain age in the clinical samples, we compared the average BAG and MAE, respectively, between CNADNI and each clinical cohort.

To assess the independence of brain age models trained on MRI or FDG-PET, we correlated BAG and regional feature importance from the two modalities in CNADNI using Pearson correlation. Feature importance was assessed using permutation importance, which measures the impact of shuffling a feature's values on a model's performance, indicating the feature's importance to the model.

To assess whether BAG is associated with cognitive performance, we calculated partial correlations between BAG and composite scores of memory (ADNI-MEM14) and executive function (ADNI-EF15). In addition, partial correlations of BAG with PET amyloid load (AV45-PET), cerebrospinal fluid (CSF) markers of beta-amyloid1-42 (CSF Aβ1-42) and p-Tau181-to- Aβ1-42 ratio (p-Tau181/Aβ1-42) were calculated to assess whether BAG is associated with AD neuropathology. Correlations were computed for CNADNI, SCDADNI and MCIADNI individually, as well as for cognitively unimpaired individuals (CUADNI; CNADNI + SCDADNI). The method of correlation (Pearson or Spearman) was decided based upon normality assessment as per Shapiro-Wilk test and all partial correlations were corrected for age, sex, years of education and APOE-ε4 carriership. Correction for age was added despite successful bias correction given the age-associativity of the dependent variables. Significance levels were as follows: p < .1 = “trend significant”, p < .05 = “significant”, p < Bonferroni correction = “significant after Bonferroni correction” (cognitive performance: α = 0.05/2, AD neuropathology: α = 0.05/2). Descriptions of the variables assessed are provided in SM sections 1f and 1g.

Finally, we aimed to assess the prognostic value of the brain age gap for cognitive outcome in comparison to existing biomarkers. All BAG assessments took place at baseline. We differentiated between cognitively “stable” individuals, who maintained their baseline diagnosis until the two-year follow-up screening, and “decliners”, who received a diagnosis of (more severe) cognitive impairment within two years after baseline. First, we computed an analysis of covariance of BAG between individuals with and without impending cognitive impairment, while correcting for sex, years of education and APOE-ε4 carriership in CNADNI, SCDADNI and MCIADNI. Subsequently, we trained multiple single-feature logistic regression classifiers in a stratified ten-fold cross-validated manner to predict cognitive outcome in different cognitive groups from FDG-PET BAG, MRI BAG, hippocampal volume, global AV45-PET SUVr, FDG-PET SUVr in the precuneus, p-tau181/Aβ1-42 ratio, mini mental state exam score or chronological age (total models per group = 8). MRI and FDG-PET measures were derived from the AAL parcellation. Global AV45-PET was taken from publicly available prior analyses16. To correct for possible confound effects among the predictors, all predictor variables were transformed to standardized residuals using a linear model trained on the stable individuals in each training fold prior to training the classifier17. Due to the small number of decliners in the CNADNI (n=16≙10%) and SCDADNI samples (n=10≙12%), we combined the two groups to a cognitively unimpaired (CUADNI) cohort. We compared the mean area under the curve (AUC) obtained from the validation folds across all predictors. If BAG of one modality showed comparable performance to the best biomarkers, we derived a cut-off given the a priori probability of cognitive decline in each training fold, and we validated this cut-off in available external datasets.

**3 Results**

**3.1 Participants**

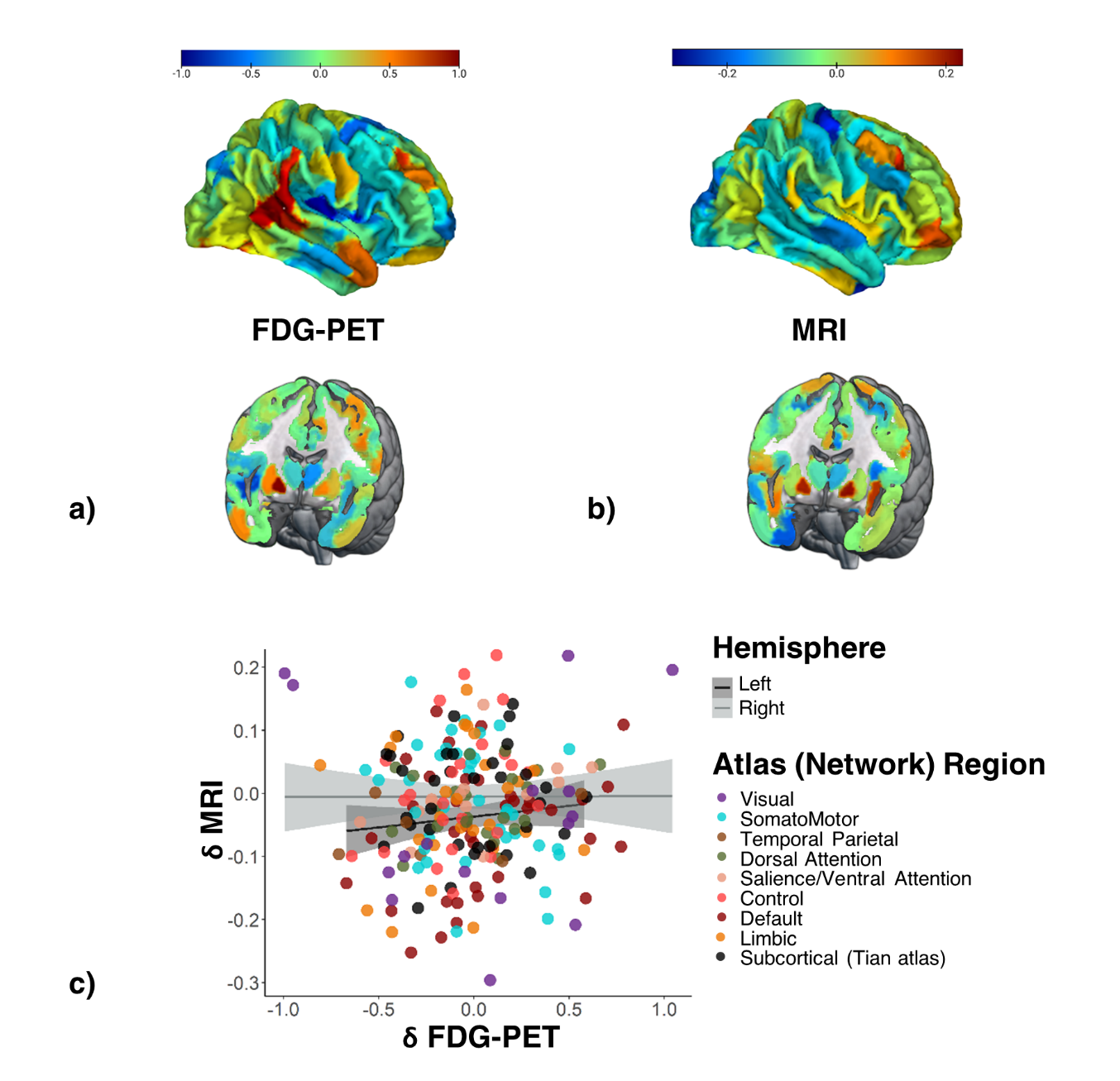
An overview of participant characteristics is shown in **Table 1**. CNOASIS, SCDADNI and SCDDELCODE subjects were significantly younger compared to the main CNADNI cohort. The SCD and MCI cohorts further differed from CNADNI in terms of cognitive performance (MCIADNI and MCIDELCODE), years of education (SCDADNI and MCIDELCODE), amyloid status (SCDDELCODE and MCIADNI) and APOE-ε4 carriership (MCIADNI and MCIDELCODE).

**3.2 Accuracy and demographic profile of estimated brain age**

MRI- and FDG-PET estimated brain age comparably well in CNADNI (MAEMRI = 2.49, MAEFDG-PET = 2.60), CNOASIS (MAEMRI = 2.92, MAEFDG-PET = 2.54) and SCDADNI (MAEMRI  = 2.50, MAEFDG-PET = 2.56), while the MAE of MRI-derived brain age (MAEMRI = 3.30) was significantly higher compared to FDG-PET (MAEFDG-PET = 2.59; **Table 2**). Within-modality comparison of MAE in CNOASIS and CNADNI yielded no significant differences, thus suggesting high generalization performance of our frameworks to external datasets comprising CN populations. However, the R² value of MRI-derived brain age was only 0.42 in CNOASIS compared to 0.74 in CNADNI and FDG-PET-derived brain age showed significantly higher BAG in CNOASIS compared to CNADNI. FDG-PET-, but not MRI-derived brain age was trend significantly advanced in SCDADNI (MEMRI = 0.11, MEFDG-PET = 0.64). In all other clinical cohorts brain age was significantly advanced compared to CNADNI (SCDDELCODE: MEFDG-PET = 2.77; MCIADNI: MEMRI = 2.16, MEFDG-PET = 0.55; MCIDELCODE: MEMRI = 2.89).

BAG was trend significantly correlated between MRI- and FDG-PET-based models (r = .128, *p* = .09, 95% CI [-0.02, 0.27]). Model selection returned different model types with mostly linear kernels (see Table SM1). Regional weight coefficients

Regional weight coefficients were strongly correlated across models of the same modality (MRI: r = [.79, 0.89], FDG-PET: r = [.74, .79]), but average weight coefficients were not correlated between the two modalities (r = .048, *p* = .48), i.e., the regions used for brain age estimation in the two modalities were substantially different (**FIGURE 3**). For FDG-PET, important regions (very low or very high weight coefficient) included parts of the temporal and pre-frontal cortex, as well as sub-cortical regions (globus pallidus, nucleus accumbens, and caudate nucleus). Notably, SUVR in the most important regions in FDG-PET was pre-dominantly right hemispheric, and consistently negatively correlated with chronological age after Bonferroni correction (α=.05/9). For MRI, important regions included parts of the parietal, pre-frontal and occipital cortex and sub-cortical regions (e.g., hippocampus, nucleus accumbens, globus pallidus, and caudate nucleus). The majority of most important regions for brain age estimation from MRI were negatively correlated with age after Bonferroni correction (α=.05/13) and spread across hemispheres. A full list of most important regions with correlation results is presented in SM section 2b.

**3.3 BAG and cognitive performance**

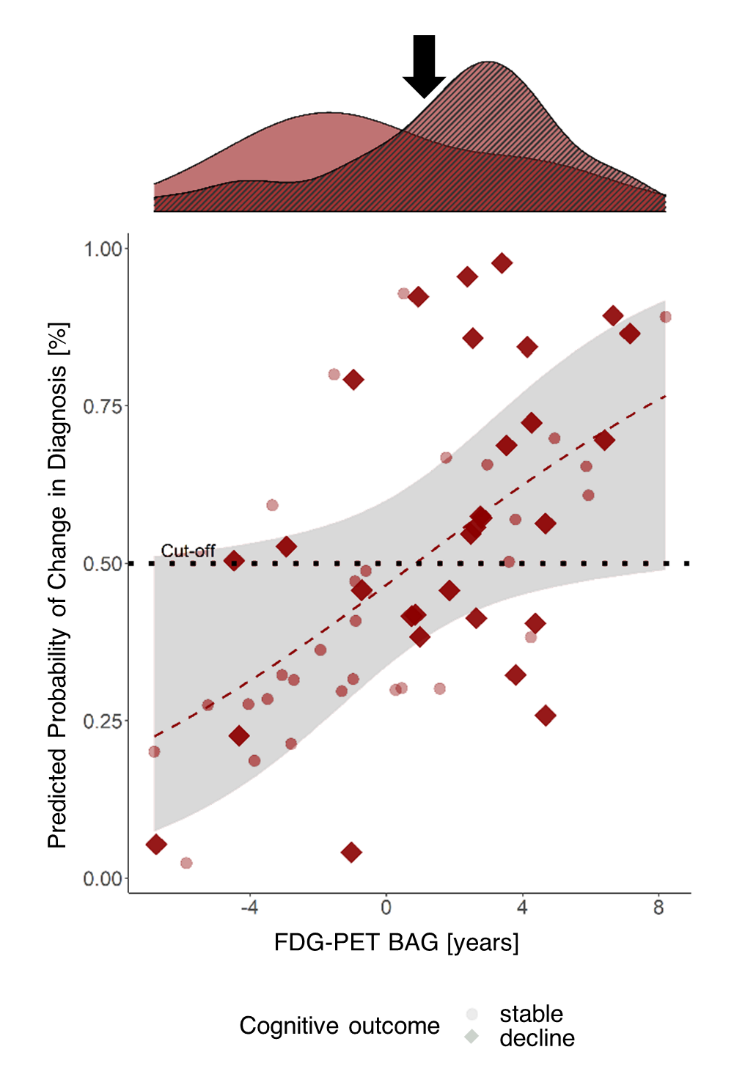
**FIGURE 3** **Feature importance for brain age prediction.** a) Average weights for brain age prediction using FDG-PET. b) Average weights for brain age prediction using MRI. More relevant weights are depicted in blue and red. c) Scatter plot of average feature importance in FDG-PET and MRI and regression lines (per hemisphere).

In CN+SCDADNI, MRI-derived BAG was associated with lower ADNI-EF scores (normally distributed; r =-.137, *p*=.01). A marginally significant correlation was observed between FDG-PET-derived BAG and ADNI-MEM scores (normally distributed; r =-.100, *p* =.06).

In MCIADNI, both, MRI- and FDG-PET-derived BAG were negatively correlated with ADNI-MEM (not normally distributed; rhoMRI =-.379, *pMRI <*.0001; rhoFDG-PET =-.237, *pFDG-PET* <.0001) and ADNI-EF (not normally distributed; rhoMRI =-.272, *pMRI <*.0001; rhoFDG-PET =-.243, *pFDG-PET*  <.0001).

**3.4 BAG and AD neuropathology**

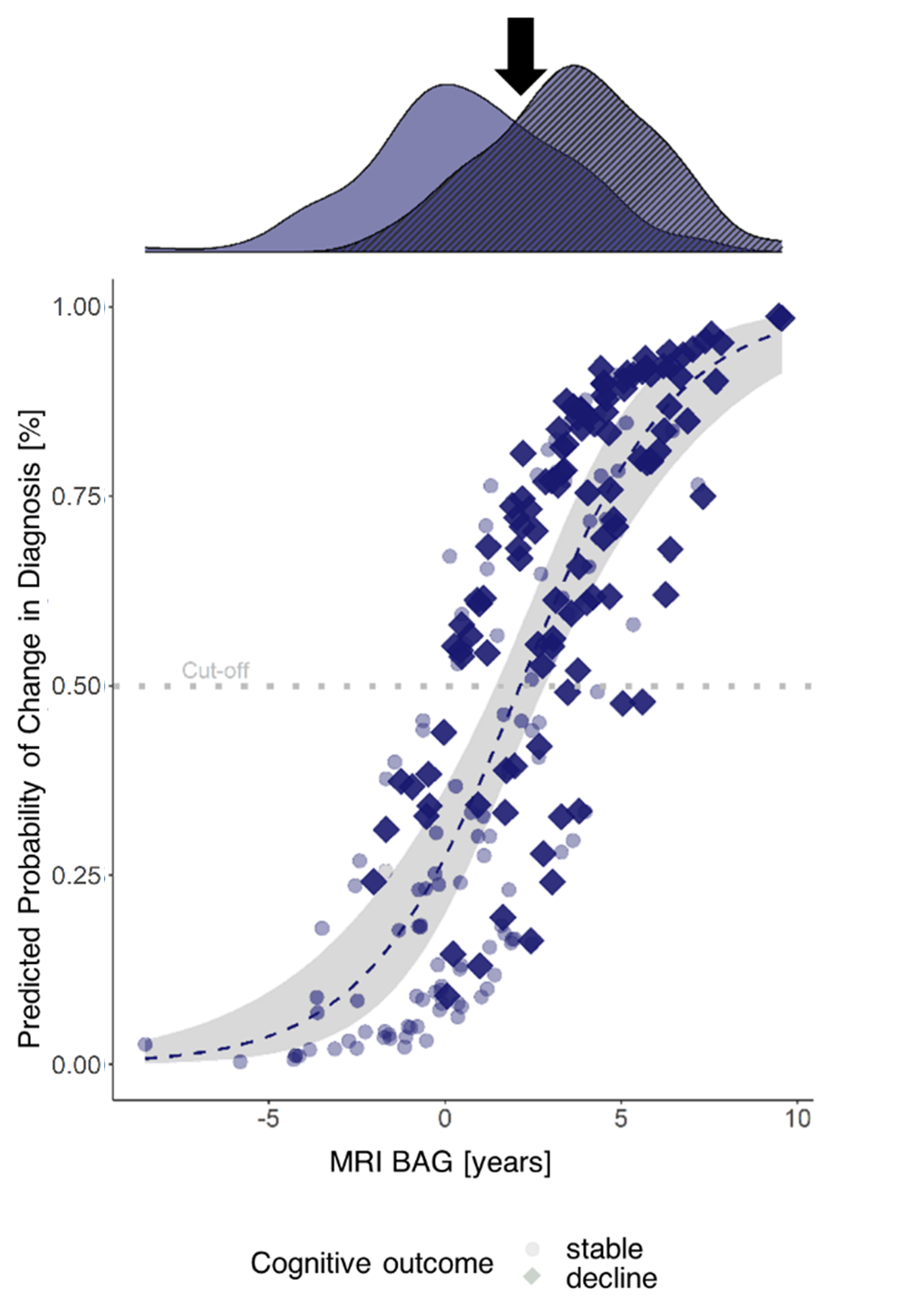
In CN+SCDADNI, higher MRI- and FDG-PET-derived BAG were both correlated with a decrease in CSF Aβ1-42 (not normally distributed; rhoMRI =-.152, *pMRI* =.012; rhoFDG-PET =-.152, *pFDG-PET* =.012), but none of the other neuropathological variables. In MCIADNI, higher MRI- and FDG-PET-derived BAG were associated with enhanced amyloid accumulation, as reflected by significant negative correlations with CSF Aβ1-42 (not normally distributed; rhoMRI = -.232, *pMRI <*.0001; rhoFDG-PET = -.144, *pFDG-PET* =.002) and (marginal) positive correlations with global AV45 (not normally distributed; rhoMRI =.144, *pMRI* =.004; rhoFDG-PET =.110, *pFDG-PET* =.026). Moreover, higher MRI-derived BAG was marginally associated with higher levels of CSF pTau181 (not normally distributed; rhoMRI =.093, *pMRI* =.048).

**3.5 BAG and Cognitive Outcome**

CN+SCDADNI sample 1 consisted of 30 decliners and 30 stables. Holding all other predictor variables constant, FDG-PET-derived BAG and APOE-ε4 carriership significantly predicted cognitive outcome at year two follow-up. The odds of a cognitive impairment diagnosis within two years were increased by 29% (95% CI [1.079, 1.604], *p* = .010) for every FDG-PET-derived BAG year and by eightfold with a positive APOE-ε4 carriership status (95% CI [1.496, 71.814], *p* = .028). To obtain a cutoff for prognoses of cognitive impairment, we fitted a logistic regression model on cognitive outcome by BAG on FDG-PET. The intersection of the curve with a 50% probability of receiving such a diagnosis was at 0.85 years FDG-PET BAG (**FIGURE 4**), i.e., cognitively unimpaired individuals with a brain age advanced by 0.85 years had an elevated risk of converting to cognitive impairment. Stratification by this cutoff in the current CN+SCDADNI sample 1 yielded a sensitivity of 70% and a specificity of 67% (positive predictive value *PPV* = 68%, negative predictive value *NPV* = 69%). We additionally applied the cutoff to the SCDDELCODE cohort (ndecliners= 8, nstables = 80), where we obtained a sensitivity of 88% and a specificity of 34% (PPV = 13%, NPV = 96%).

**FIGURE 4** **Cross-validated probability of a change in diagnosis from CN+SCD to MCI/dementia within two years by FDG-PET BAG.** The red line shows the logistic regression on cognitive outcome by FDG-PET BAG, with the shaded area representing standard error. The density plot above shows FDG-PET BAG distribution of stables (clear) and decliners (striped) in the subsample and the black error points to the cutoff.

MCIADNI sample 1 consisted of 113 decliners and 113 stables. Holding all other predictor variables constant, elevated MRI-derived BAG (OR=1.52, 95% CI [1.304, 1.788]), a positive amyloid status in CSF (OR=4.11, 95% CI [1.632, 11.255]) and APOE-ε4 carriership (OR=3.03, 95% CI [1.495, 6.254]) significantly predicted a dementia diagnosis at year-two follow up. The intersection of the curve with a 50% probability of receiving a diagnosis of dementia within two years was at 2.14 years of MRI BAG (**FIGURE 5**). Stratification by this cutoff in the current MCIADNI subsample yielded a sensitivity of 73% and a specificity of 72% (PPV = 72%, NPV = 73%). In the MCIDELCODE sample (nstables = 41, ndecliners = 28), the cutoff had a sensitivity of 68% and a specificity of 73% (PPV = 63%, NPV = 79%).



Analyses excluding subjects without information on amyloid status (sample 2) in both, CN+SCDADNI (n=48) and MCIADNI (n=186) yielded results consistent with those obtained with sample 1 (see SM section 2c). Finally, given the correlations observed between FDG-PET- and MRI BAG in CN+SCDADNI and MCIADNI (see Section 3.2), we assessed logistic regression models with unimodal BAG18. Considered in separate models, both MRI- and FDG-PET-BAG significantly predicted cognitive outcome in MCIADNI, while only FDG-PET predicted cognitive outcome in CN+SCDADNI (see Tables SM2-SM5 for estimates of logistic regression in sample 1 analyses using only one imaging modality).

**FIGURE 5 Cross-validated probability of cognitive decline within two years after a baseline diagnosis of MCI by MRI-BAG.** The blue line shows the logistic regression on cognitive outcome by MRI BAG, with the shaded area representing standard error. The blue line intersects 50% at 2.14 years BAG on MRI. The density plot above shows MRI BAG distribution of stables (clear) and decliners (striped) in the subsample and the black error points to the cutoff.

**4 Discussion**

Previous studies have mainly used MRI to estimate brain age. FDG-PET is an early indicator of neurodegeneration-related cerebral changes and a recent study showed for the first time that it could also be used successfully to estimate brain age1. Here, we compared the accuracy of FDG-PET and MRI-estimated brain age and provided a comprehensive overview of the cognitive and neuropathological profile of FDG-PET and MRI-derived BAG in different cognitive groups. We showed that 1) MRI and FDG-PET both accurately estimated brain age; 2) MRI and FDG-PET-derived BAG both reflect neuropathological abnormalities in CN/SCD and MCI, as well as cognitive dysfunction in MCI, and 3) BAG derived from FDG-PET, but not MRI, yields prognostic value for cognitive outcome in CN/SCD, while MRI yields better prognostic value in MCI. We also calculated and validated cutoffs for predicting cognitive outcome. Importantly, this study is the first to present modality-dependent BAG cutoffs, which can aid in the prognosis of cognitive outcome not only in MCI patients, but even patients without objective cognitive impairment.

Our findings suggest that BAG derived from FDG-PET captures greater and more consistent changes associated with early and subtle neurodegeneration as observed in cognitively unimpaired individuals. On the other hand, MRI-derived BAG was superior in delineating dementia-related changes in MCI4. While Lee and colleagues showed that both, MRI and FDG-PET BAG are significantly increased in CN converting to MCI or AD at baseline1, we demonstrated that prognostic value exists only for FDG-PET BAG. Among the CN population, our results are likely most relevant for individuals with SCD. Individuals with SCD are 1) assumed to recognize cognitive deficits before they become clinically measurable7, 2) more likely to develop MCI or AD compared to CN19, and 3) likely to be seen by a physician given their subjective symptoms. Prediction of cognitive outcome in our cohorts based on FDG-PET BAG was moderately to highly sensitive with moderately to very high NPV. Together, these findings provide strong evidence that FDG-PET BAG could complement the identification of at-risk individuals, as individuals with a BAG below our proposed cutoff are unlikely to develop cognitive impairment within two years.

Including BAG in AD clinical trials could have several advantages. Numerous anti-amyloid therapies are currently under assessment or have recently been approved for the treatment of MCI and early AD. Since cognitive decline is an important outcome factor of these trials, BAG could support the exclusion of individuals at lower risk of cognitive decline, thereby helping to reduce the number of participants and therefore the cost and time required for treatment trials. Moreover, BAG, which is a summary measure of overall brain health20 and reflects amyloid neuropathology even in cognitively unimpaired individuals, could potentially provide useful information on drug efficacy21.

Similar to previous studies1,4, we found differences in brain regions displaying aging as observed on FDG-PET and MRI. Thus, different aging processes may be observed depending on the modality, which underlines the importance of considering the appropriate modality for a research question. The regions deemed most important by our MRI and FDG-PET models have previously been described to be substrates heavily affected by aging4, and almost all regions we identified as ‘most important’ for brain age estimation were correlated strongly with age in our ADNI cohort. The greater left-hemisphere involvement in brain age estimation on MRI compared to FDG-PET could explain the better association of MRI-derived BAG with AD biomarkers and cognitive outcome in MCI, as the left hemisphere is known to be affected early on in AD aetiology22. Given the overall strong association of regions deemed important for brain age estimation with AD, our work further supports the claim that AD-related neurodegeneration, at least in part, resembles a form of advanced brain aging.

Some limitations should be acknowledged. First, due to data availability and increased risk of cognitive deficits being due to neurodegenerative processes23, we only included participants over the age of 60, however, accelerated aging starting before this age remained uninvestigated in our study. Moreover, there is a lack of publicly available big neuroimaging databases on SCD, enabling to disentangle early differences in brain health, possibly related to cognitive decline, between CN and SCD. The SCD label was only included in the second phase of the ADNI study – individuals recruited during ADNI-1 (~1/4 of our sample) may therefore have had SCD which was undetected at the time and which possibly caused the indifferent results of brain age between CN and SCD in the ADNI sample. However, exclusion of these individuals would have caused further shrinkage of our sample size, which would have been undesirable. Furthermore, the sensitivity and especially specificity values for prognoses of cognitive outcome are not high enough to use these measures as standalone biomarkers of cognitive outcome. Moreover, obtaining FDG-PET scans from a cognitively unimpaired population is not straightforward, as it requires logistical availability, high cost, and the injection of a radioactive tracer in the absence of evident cognitive impairment. However, accurate prognoses, particularly for cognitively unimpaired individuals, are difficult to establish and we believe that BAG assessment with a group-dependent choice of modality can aid this process by providing a first indicator of cognitive outcome. Future work should evaluate the combined potential of FDG-PET BAG and APOE-ε4 carriership as a prognostic biomarker of cognitive outcomes. Second, the different FDG-PET scanning protocol of DELCODE (acquisition time: 40-60 min post injection) compared to ADNI and OASIS (acquisition time: 30-60 min post injection) might have influenced generalization of our models to the DELCODE cohort. Yet, we believe that the difference would not be substantial, as we averaged time frames over the entire acquisition time. Moreover, the average BAG (ME) of SCDDELCODE exceeds the previously reported BAG on MRI (1.1 years24), and the MRI and FDG-PET BAG of MCI patients in our analyses. These differences may be driven by methodological differences, including substantially younger age compared to the study by Rockiki et al., which likely lowers the risk of these individuals to be incipient AD patients, and a different choice of modality (MRI instead of FDG-PET). Whether the FDG-PET BAG is abnormally high in our analyses, or whether higher FDG-PET BAG in SCD reflects very early neurological dysfunction needs further investigation.

In summary, we have shown that MRI and FDG-PET can both be used to estimate brain age and, with some respects, show different benefits depending on the group analyzed: While MRI- and FDG-PET BAG both accurately reflect neuropathological burden across groups and cognitive performance in MCI, only FDG-PET BAG can aid in the prognosis of cognitive outcome in cognitively unimpaired individuals. On the other hand, MRI-derived BAG demonstrates a better estimate for dementia risk in MCI. Estimating cognitive outcome using our BAG cutoffs could complement the identification of patients in need of frequent monitoring at an early time point of cognitive decline and could support clinical trials, both methodologically and financially.

**Author Contributions**

All authors contributed to the study conception and design. Material preparation, data collection and analysis were performed by ElD and GA, with support from KRP and MCH. KRP, TvE, SBE and AD jointly supervised this work. DELCODE data preparation was supervised by MD and HB (PET), EmD (MRI) and FJ (clinical data). The first draft of the manuscript was written by ED and all authors commented on previous versions of the manuscript. All authors read and approved the final manuscript.

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**Key Points**

**QUESTION:** What is the neuropathological and predictive profile of brain age gaps (BAGs) derived from structural MRI or FDG-PET?

**PERTINENT FINDINGS**: BAG was computed from structural MRI and FDG-PET and subsequently associated with neuropathological markers of Alzheimer’s disease, as well as risk of cognitive deterioration. While both, MRI- and FDG-PET-derived BAG were indicative of existing amyloid pathology already in individuals without cognitive impairment, the predictive capacity of BAG for cognitive outcome was group-dependent: FDG-PET-derived BAG predicted cognitive deterioration in cognitively unimpaired individuals and MRI-derived BAG predicted cognitive deterioration in patients with mild cognitive impairment.

**IMPLICATIONS FOR PATIENT CARE:** A group-dependent choice of modality for BAG assessment can complement care management plans of cognitively unimpaired and impaired individuals by providing estimates of cognitive outcomes.

**References**

1. Lee J, Burkett BJ, Min H-K, et al. Deep learning-based brain age prediction in normal aging and dementia. *Nat Aging*. 2022;2:412–424. doi:10.1038/s43587-022-00219-7

2. Löwe LC, Gaser C, Franke K. The effect of the APOE genotype on individual BrainAGE in normal aging, Mild cognitive impairment, and Alzheimer’s Disease. *PLoS One*. 2016;11(7):e0157514. doi:10.1371/journal.pone.0157514

3. Gaser C, Franke K, Klöppel S, Koutsouleris N, Sauer H. BrainAGE in Mild Cognitive Impaired Patients: Predicting the Conversion to Alzheimer’s Disease. *PLoS One*. 2013;8(6):e67346. doi:10.1371/journal.pone.0067346

4. Dukart J, Kherif F, Mueller K, et al. Generative FDG-PET and MRI Model of Aging and Disease Progression in Alzheimer’s Disease. *PLoS Comput Biol*. 2013;9(4):e1002987. doi:10.1371/journal.pcbi.1002987

5. LaMontagne PJ, Benzinger TLS, Morris JC, et al. OASIS-3: Longitudinal neuroimaging, clinical, and cognitive dataset for normal aging and Alzheimer disease. *medRxiv*. Published online 2019. doi:10.1101/2019.12.13.19014902

6. Jessen F, Spottke A, Boecker H, et al. Design and first baseline data of the DZNE multicenter observational study on predementia Alzheimer’s disease (DELCODE). *Alzheimer’s Res Ther*. 2018;10(1):15. doi:10.1186/s13195-017-0314-2

7. Jessen F, Amariglio RE, Van Boxtel M, et al. A conceptual framework for research on subjective cognitive decline in preclinical Alzheimer’s disease. *Alzheimer’s Dement*. 2014;10(6):844-852. doi:10.1016/j.jalz.2014.01.001

8. Albert MS, DeKosky ST, Dickson D, et al. The diagnosis of mild cognitive impairment due to Alzheimer’s disease: Recommendations from the National Institute on Aging-Alzheimer’s Association workgroups on diagnostic guidelines for Alzheimer’s disease. *Alzheimer’s Dement*. 2011;7(3):270-279. doi:10.1016/j.jalz.2011.03.008

9. Jack CR, Bernstein MA, Fox NC, et al. The Alzheimer’s Disease Neuroimaging Initiative (ADNI): MRI methods. *J Magn Reson Imaging*. 2008;27(4):685-691. doi:10.1002/jmri.21049

10. Pedregosa F, Varoquaux G, Gramfort A, et al. Scikit-learn: Machine learning in Python. *J Mach Learn Res*. 2011;12:2825-2830. Accessed April 20, 2021. http://scikit-learn.sourceforge.net.

11. Tzourio-Mazoyer N, Landeau B, Papathanassiou D, et al. Automated anatomical labeling of activations in SPM using a macroscopic anatomical parcellation of the MNI MRI single-subject brain. *Neuroimage*. 2002;15(1). doi:10.1006/nimg.2001.0978

12. Beheshti I, Ganaie MA, Paliwal V, Rastogi A, Razzak I, Tanveer M. Predicting Brain Age Using Machine Learning Algorithms: A Comprehensive Evaluation. *IEEE J Biomed Heal Informatics*. 2022;26(4):1432-1440. doi:10.1109/JBHI.2021.3083187

13. Beheshti I, Nugent S, Potvin O, Duchesne S. Bias-adjustment in neuroimaging-based brain age frameworks: A robust scheme. *NeuroImage Clin*. 2019;24:102063. doi:10.1016/j.nicl.2019.102063

14. Crane PK, Carle A, Gibbons LE, et al. Development and assessment of a composite score for memory in the Alzheimer’s Disease Neuroimaging Initiative (ADNI). *Brain Imaging Behav*. 2012;6(4):502-516. doi:10.1007/s11682-012-9186-z

15. Gibbons LE, Carle AC, Mackin RS, et al. A composite score for executive functioning, validated in Alzheimer’s Disease Neuroimaging Initiative (ADNI) participants with baseline mild cognitive impairment. *Brain Imaging Behav*. 2012;6(4):517-527. doi:10.1007/s11682-012-9176-1

16. Landau S, Jagust W. *Florbetapir Processing Methods*.; 2011.

17. Dukart J, Schroeter ML, Mueller K. Age correction in Dementia - Matching to a healthy brain. *PLoS One*. 2011;6(7). doi:10.1371/journal.pone.0022193

18. Ranganathan P, Pramesh C, Aggarwal R. Common pitfalls in statistical analysis: Logistic regression. *Perspect Clin Res*. 2017;8(3):148-151. doi:10.4103/picr.PICR\_87\_17

19. Parfenov VA, Zakharov VV, Kabaeva AR, Vakhnina NV. Subjective cognitive decline as a predictor of future cognitive decline a systematic review. *Dement e Neuropsychol*. 2020;14(3):248-257. doi:10.1590/1980-57642020dn14-030007

20. Cole JH, Marioni RE, Harris SE, Deary IJ. Brain age and other bodily ‘ages’: implications for neuropsychiatry. *Mol Psychiatry*. 2019;24(2):266-281. doi:10.1038/s41380-018-0098-1

21. Van Gestel H, Franke K, Petite J, et al. Brain age in bipolar disorders: Effects of lithium treatment. *Aust N Z J Psychiatry*. 2019;53(12):1179-1188. doi:10.1177/0004867419857814

22. Pfeil J, Hoenig MC, Doering E, van Eimeren T, Drzezga A, Bischof GN. Unique regional patterns of amyloid burden predict progression to prodromal and clinical stages of Alzheimer’s disease. *Neurobiol Aging*. 2021;106:119-129. doi:10.1016/j.neurobiolaging.2021.06.014

23. Jessen F, Amariglio RE, Buckley RF, et al. The characterisation of subjective cognitive decline. *Lancet Neurol*. 2020;19(3). doi:10.1016/S1474-4422(19)30368-0

24. Rokicki J, Wolfers T, Nordhøy W, et al. Multimodal imaging improves brain age prediction and reveals distinct abnormalities in patients with psychiatric and neurological disorders. *Hum Brain Mapp*. 2021;42(6):1714-1726. doi:10.1002/hbm.25323

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| --- | --- | --- | --- | --- | --- | --- |
| **Table 1.** Overview of samples | | | | | | |
|  | CNADNI | CNOASIS | SCDADNI | MCIADNI | SCDDELCODE | MCIDELCODE | |
| *n* total | 186 | 49 | 102 | 595 | 88 | 80 | |
| Age at PET scan [avg. years (SD)] | 73.8 (6.46) | 70.6 (5.07)+ | 72.3 (5.60)+ | 73.2 (6.93) | 70.9 (5.57)+ | NA | |
| Age at MRI scan [avg. years (SD)] | 73.8 (6.44) | 69.2 (4.98)+ | 72.3 (5.60)+ | 73.2 (6.92) | NA | 73.4 (5.87) | |
| Sex [%female (nNA)] | 53 (0) | 53 (0) | 59 (0) | 42 (2)+ | 36 (0)+ | 36 (0)+ | |
| MMSE [avg. score] | 29 (1.26) | 29 (0.78) | 29 (1.20) | 28 (1.75)+ | 29 (1.03) | 28 (1.67)+ | |
| Education [avg. years (SD)] | 16 (2.54) | 16 (2.51) | 17 (2.50)+ | 16 (2.67) | 16 (3.00) | 14 (3.06)+ | |
| CSFAβ1-42 Status [%positive (nNA)] | 41 (27) | NA | 35 (9) | 64 (126)+ | 22 (28)+ | 38 (38) | |
| APOE [% ε4-carriers (nNA)] | 29 (1) | NA | 31 (0) | 49 (4)+ | 38 (3) | 49 (0)+ | |
| Notes. Percentage of CSFAβ1-42 status indicates percentage of amyloid positive individuals among all who received lumbar puncture (excluding NA). Thresholds for amyloid positivity was 1100 pg/ml in ADNI and 496 pg/ml in DELCODE. +significantly different from CNADNI as assessed per t-test (age, MMSE, education) or χ² (sex, amyloid status, APOE status). | | | | | | | |

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| --- | --- | --- | --- | --- | --- | --- | --- | --- | --- | --- |
|  | | **Table 2.** Accuracy of estimating chronological age from FDG-PET and MRI scans using AAL atlas. | | | | | | | | |
|  | Modality | | *n* | MAE | Range | ME | R² | **Accuracy**  *paired t-test*  MAE MRI vs FDG-PET | **Generalizability**  *t-test*  MAE current vs CNADNI | **Brain age advancement**  *t-test*  MEcurrent vs CNADNI |
| **CNADNI** | MRI | | 175+ | 2.49 | [-9.4, 8.7] | 0.06 | 0.74 | t = 0.48  95% CI [-0.33, 0.55] | NA | NA |
| FDG-PET | | 175+ | 2.60 | [-10.1, 9.6] | -0.10 | 0.70 | NA |
| **CNOASIS** | MRI | | 49+ | 2.92 | [-7.1, 8.4] | 0.13 | 0.42 | t = - 0.94  95% CI [-1.20, 0.43] | t = 1.16  95% CI [-0.31, 1.18] | t = 0.12  95% CI [-1.12, 1.26] |
| FDG-PET | | 49+ | 2.54 | [-5.0, 6.8] | 0.89 | 0.63 | t = -0.18  95% CI [-0.64, 0.53] | t = 2.00\*  95% CI [0.01, 1.97] |
| **SCDADNI** | MRI | | 102 | 2.50 | [-6.6, 7.0] | 0.11 | 0.69 | t = 0.26 95% CI [-0.42, 0.54] | NA | t = 0.11  95% CI [-0.73, 0.82] |
| FDG-PET | | 102 | 2.56 | [-5.6, 9.8] | 0.64 | 0.69 | NA | t = 1.86+  95% CI [-0.05, 1.53] |
| **MCIADNI** | MRI | | 595 | 3.30 | [-10.5, 13.5] | 2.16 | 0.65 | t = -5.72\*\*  95% CI [-0.95, 0.46] | NA | t = 7.47\*\*  95% CI [1.55, 2.65] |
| FDG-PET | | 595 | 2.59 | [-10.0, 11.0] | 0.55 | 0.78 | NA | t=2.23\*  95% CI [0.08, 1.22] |
| **SCDDELCODE** | FDG-PET | | 88 | 3.16 | [-2.7, 9.3] | 2.77 | 0.52 | NA | NA | t = 7.45\*\*  95% CI [2.11, 3.63] |
| **MCIDELCODE** | MRI | | 80 | 3.69 | [-5.1, 11.6] | 2.89 | 0.38 | NA | NA | t = 6.04\*\*  95% CI [1.90, 3.75] |
|  | | *Notes.* +After outlier exclusion using CN train set (IQR > 6). +trend significant with α = 0.1, \* significant with α = 0.05, \*\* significant with α = 0.01 | | | | | | | | |

1. + both authors contributed equally

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