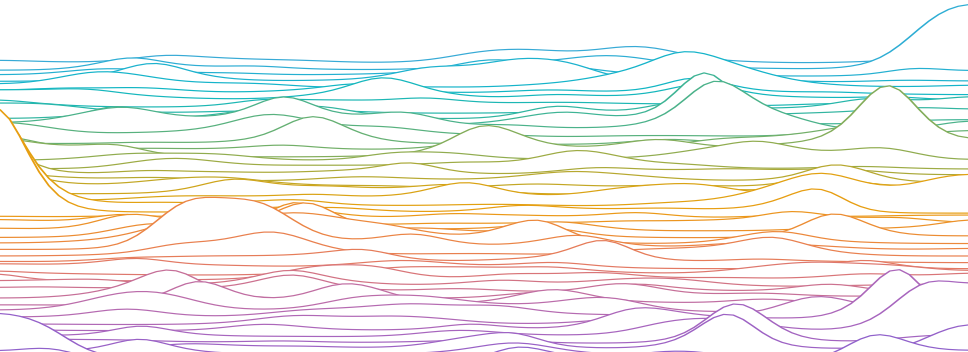


Leaky Integrate-and-Fire, Rate Neurons

SEMT30003/4



This lecture covers:

- ▶ Leaky Integrate and Fire (LIF)
- ▶ Rate Neurons

Learning goals:

- 1 What simplifications does the Leaky Integrate and Fire (LIF) model make?
- 2 How to solve for the firing rate of a model LIF neuron given constant current?
- 3 Connect the f - I curve to the idea of a rate neuron (rate coding)

Building on:

First-order ordinary differential equations

Membrane voltage dynamics

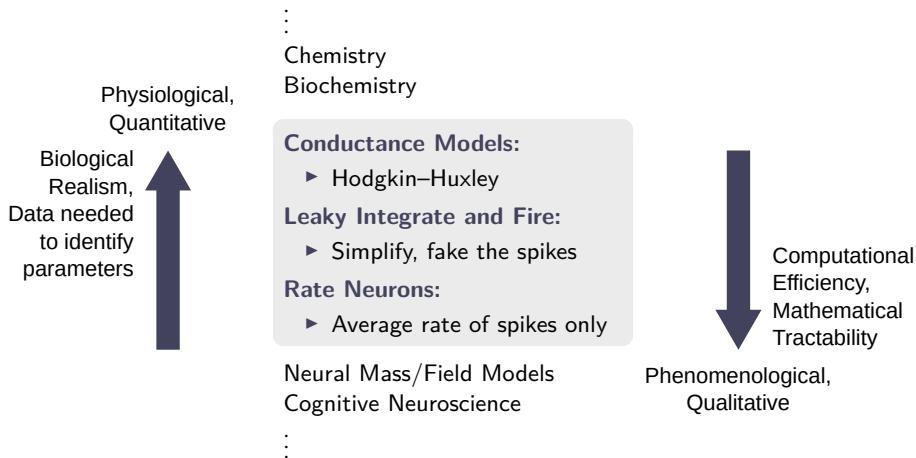
Building up to:

Visual system (+ rate neuron models)

Hodgkin Huxley model of the action potential

Topics in Computer Science Final exam question

Modelling Scales

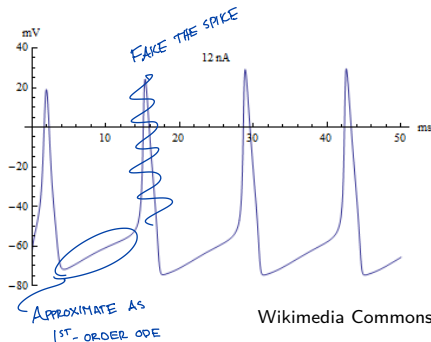


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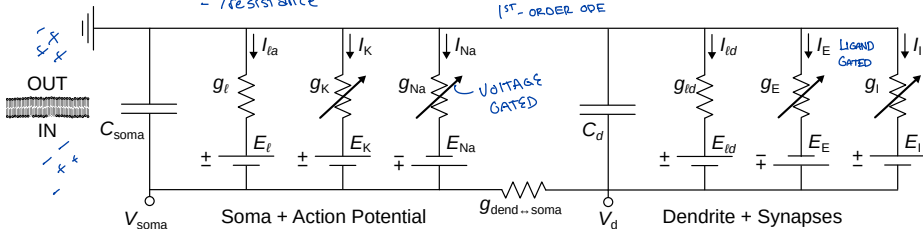
Full Conductance Model e.g. Hodgkin-Huxley

Nonlinear, action potential
costly to simulate

Study role of ion channels,
conductances, dendritic
morphology (shape), etc.



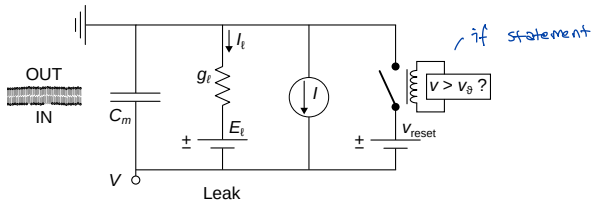
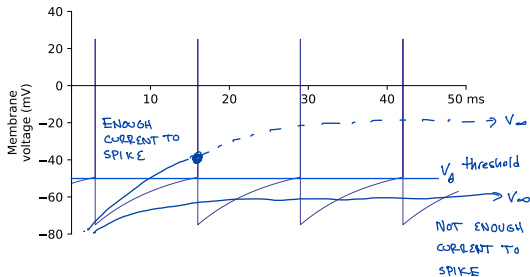
g = conductance
= $1/\text{resistance}$



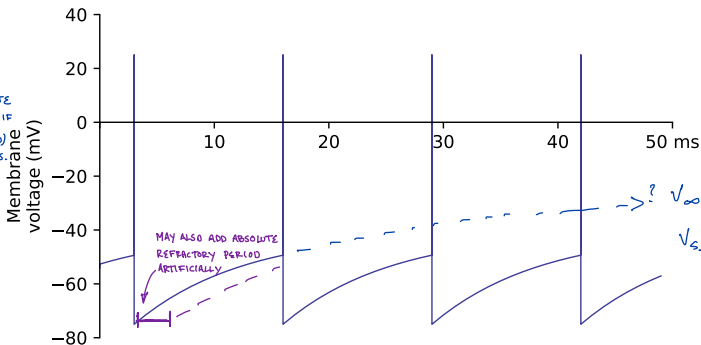
Leaky Integrate-and-Fire (LIF)

Departs from
physiology, but
sufficient to build
intuition

Easy to integrate



Leaky Integrate-and-Fire (LIF)



LIF model:

$$C\dot{v} = \frac{1}{R}(v_r - v) + I$$

if $v(t) > v_\theta$ then

$$v(t) \leftarrow v_r$$

Emit a spike <

MISTAKE:

EQUILIBRIUM (RESTING)

POTENTIAL NEED NOT BE
SAME AS RESET v_r ,

BUT IS SOMETIMES SET THE
SAME FOR SIMPLICITY. SHOULD
READ " E_A ".

$v(t)$: membrane voltage

v_θ : Threshold (spike when $v(t) > v_\theta$)

v_r : Reset voltage ($v(t) \leftarrow v_r$ after spike)

R : Membrane resistance

C : Membrane capacitance

I : Current through the membrane

ASIDE (NOT IN COURSE NOTES)

- there are many models that simplify voltage dynamics & "fake" the spike
- LIF not necessarily always "most" natural
- Exponential Integrate & Fire
- Izhikovich Neuron
- Quadratic Integrate & Fire
- Multi - (timescale) - Quadratic Integrate & Fire

QIF

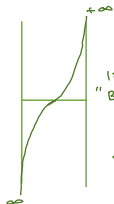
STATE ABSTRACT, NOT QUITE VOLTAGE

$$\dot{x} = x^2 + I$$

$$x(t) = \sqrt{I} \cdot \tan(C_0 + \sqrt{I} \cdot t)$$

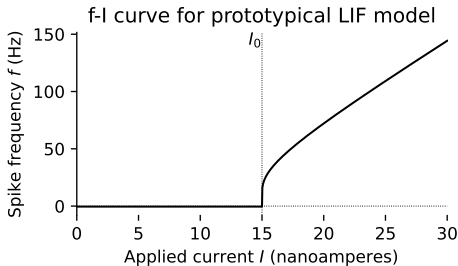
constant from initial condition

IF SPIKES, "BLOWS UP" IN FINITE TIME



CHANGE COORDINATES & JOIN AT $\pm \infty$ TO GET THETA NEURON

“f–I” curve



- ▶ F–I curve maps applied current “ I ” \rightarrow spiking frequency “ F ”
- ▶ Shown today in the case of the Leaky Integrate-and-Fire (LIF) neuron

$$C\dot{v} = \frac{1}{R}(v_r - v) + I$$

if $v(t) > v_g$ then $v(t) \leftarrow v_r$ and emit a spike

Q: Solve for the spiking frequency f as a function of applied current I in the LIF model

$$C\dot{v} = \frac{1}{R}(v_r - v) + I$$

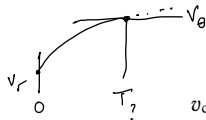
if $v(t) > v_g$ then $v(t) \leftarrow v_r$ and emit a spike

Membrane voltage ODE:

$$C\dot{v} = \frac{1}{R}(v_r - v) + I \quad \text{KNOWN \& CONSTANT}$$

$$\underbrace{RC}_{\tau} \dot{v} = \underbrace{v_r + IR}_{v_{\infty}} - v$$

$$\tau \dot{v} = v_{\infty} - v$$



Find time T where voltage reaches threshold v_g

$$v_g = v_{\infty} + e^{-T/\tau} [v_r - (v_r + IR)]$$

$$v_g = v_{\infty} - e^{-T/\tau} IR$$

Spikes if $v_{\infty} \geq v_g$

$$v_{\infty} - v_g = e^{-T/\tau} IR$$

$$e^{-T/\tau} S = \frac{v_{\infty} - v_g}{IR}$$

you can add fixed absolute refractory time here if you like

First-order ODE solution:

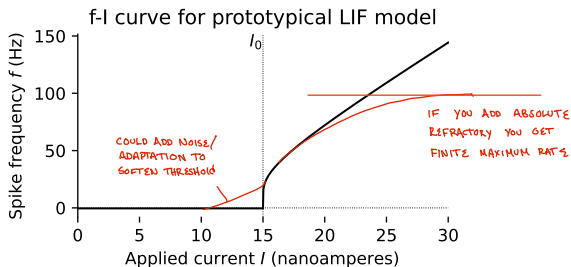
$$\underbrace{v(T)}_{v_g} = v_{\infty} + e^{-T/\tau} (\underbrace{v(0)}_{v_r} - v_{\infty})$$

$$T = \tau \ln \left(\frac{IR}{v_{\infty} - v_g} \right) + T_{\text{ABS. REFRACT}}$$

period ↑

Frequency is reciprocal of period $f = \frac{1}{T}$

What if we only care about the average number of spikes per unit time?
Do we need to model spikes at all?



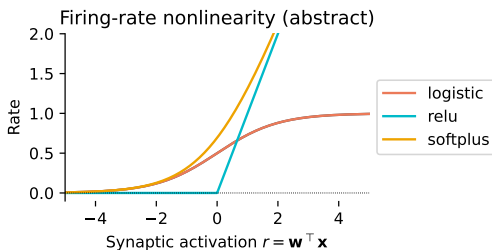
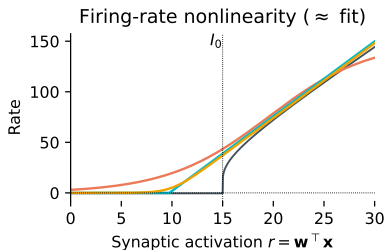
Rate Coding

- ▶ Only average # of spikes matters (over time **and/or** population).
- ▶ Exact timing of each spike is not used to encode information.

OK \approx for signals that **change slowly** (e.g. musculoskeletal dynamics low-pass filter spikes from α -motor neurons) or information represented in **average population activity of many neurons**.

Nice math: Continuously varying rates are differentiable: Calculus, ODEs, etc.

Nice machine learning: Differentiable nonlinearity emits “rate” rather than $\{0, 1\}$



Rate Coding

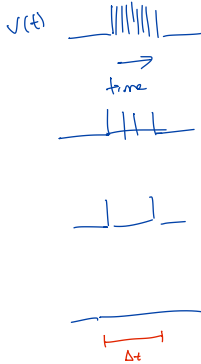
- ▶ Only average # of spikes matters (over time **and/or** population).
- ▶ Exact timing of each spike is not used to encode information.

NOT rate coding:

- ▶ Phase code: Spike time relative to rhythmic activity carries information
- ▶ Timing code: Medial superior olive (or in owls: “nucleus laminaris”) detects 10–700 μs Δt in sound arrival at left/right ears.
- ▶ Anything that models single spikes or restricts neuronal outputs to $\{0, 1\}$

SPIKES PER UNIT TIME

more applied current \uparrow



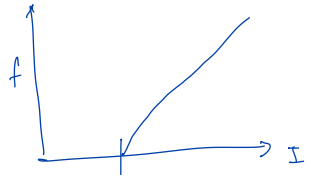
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0

IF ONLY SPIKE RATE MATTERS
SIMPLER TO TREAT NEURON AS
BLACK BOX FUNCTION FROM
ACTIVATION \rightarrow RATE (FREQUENCY)



Exam

Leaky Integrate and Fire (LIF)

What physical phenomena do R , C , $v(t)$, I , τ , $v_{\text{threshold}}$, v_{reset} approximate?

Determine whether neuron will cross threshold for a given input —

What is the minimum current I_0 to elicit a spike? —

Solve the voltage equation forward in time from some initial condition —

F-I Curve

Solve for the spiking frequency f as a function of applied current I —

What current I elicits spiking frequency f ? —

How does the F-I curve change when R , C , I , v_{θ} , v_r increase/decrease? —

Rate coding

What is rate coding; its pros/cons; what information does it capture/ignore?

Are models that average over *populations* of neurons still rate coding?

State example (from biology) where rate coding is a good/bad approximation.

