

## TD 1 – Models of Neurons I

### 1 Mathematical tools for Differential Equations

#### 1.1 Analytical solutions

① *Independent term only* – Solving  $\frac{dy}{dt} = \frac{1}{\tau}c(t)$ .

Any primitive of this function verifies the differential equation, and all those primitives differ only by a constant. The primitive which cancels at the initial time can be obtained by integrating up to time  $t : t \mapsto \int_0^t \frac{1}{\tau}c(t)dt$ .

The primitive which satisfies the initial condition is the one which takes the value  $y_0$  at time  $t = 0$ , which is the constant to add :  $y(t) = y_0 + \frac{1}{\tau} \int_0^t c(t)dt$ .

② *No independent term* – Solving  $\frac{dy}{dt} = -\frac{1}{\tau}y(t)$ .

⊞ Method 1 : Directly exhibiting a solution.

The exponential function has the property of being equal to its derivative. Therefore, any function  $t \mapsto \lambda e^{-\frac{t}{\tau}}$ ,  $\lambda \in \mathbb{R}$  verifies the differential equation, since its derivative is  $t \mapsto -\frac{1}{\tau} \lambda e^{-\frac{t}{\tau}}$  with  $\lambda \in \mathbb{R}$  a constant.

To further verify the initial condition, the constant  $\lambda$  should be set such as  $y(0) = y_0$ , i.e.  $y_0 = \lambda e^0 = \lambda$ .

⊞ Method 2 : Separation of variables.

The equation rewrites :  $\frac{dy}{y(t)} = -\frac{1}{\tau} dt$ . Integrating leads to :  $\int_0^t \frac{1}{y(t)} dy = -\frac{1}{\tau} \int_0^t dt \implies \ln\left(\frac{y(t)}{y_0}\right) = -\frac{1}{\tau}t$ .

Exponentiating to express the solution :  $\frac{y(t)}{y_0} = e^{-\frac{t}{\tau}} \implies y(t) = y_0 e^{-\frac{t}{\tau}}$ .

**Conclusion** Both methods lead to the unique solution  $y(t) = y_0 e^{-\frac{t}{\tau}}$

③ *Constant independent term* – Solving  $\frac{dy}{dt} = -\frac{1}{\tau}(y(t) - c_0)$

⊞ Method 1 : Separation of variables.

The equation  $\frac{dy}{y(t) - c_0} = -\frac{1}{\tau} dt$  can be integrated by linear change of variable ( $z(t) = y(t) - c_0$ ) :

$\ln\left(\frac{y(t) - c_0}{y_0 - c_0}\right) = -\frac{1}{\tau}t \implies y(t) = c_0 + (y_0 - c_0)e^{-\frac{t}{\tau}}$ .

⊞ Method 2 : Sum of particular solution and homogeneous solution.

This method proceeds in two steps, which can be interpreted by a physical meaning :

① Investigating if there exists a *particular solution*  $y_p(t)$  which is *constant*, thereby constituting an *equilibrium* of the system.

Such a constant solution does not evolve in time by definition :  $\frac{dy_p}{dt} = 0 \implies -y_p(t) + c_0 = 0 \implies y_p(t) = c_0$ .

② Finding the *transient dynamics* by which the system converges towards the equilibrium.

This involves finding the dynamics of the difference  $y(t) - y_p(t) = y(t) - c_0$ , which verifies a differential equation without independent term (as in ②) :  $\frac{d(y(t) - c_0)}{dt} = \frac{dy(t)}{dt} = -\frac{1}{\tau}(y(t) - c_0)$ . Therefore,  $(y(t) - c_0) = (y(t) - c_0)(0) \times e^{-\frac{t}{\tau}} = (y_0 - c_0) \times e^{-\frac{t}{\tau}}$ .

③ Summing both solutions lead to the unique solution :  $y(t) = c_0 + (y_0 - c_0)e^{-\frac{t}{\tau}}$ .

**Conclusion** Both methods lead to the unique solution  $y(t) = c_0 + (y_0 - c_0)e^{-\frac{t}{\tau}}$ .

④ *Arbitrary independent term* – Solving  $\frac{dy}{dt} = -\frac{1}{\tau}(y(t) - c(t))$

⊞ Method : 'Variation of the constant'.

The associated homogeneous equation  $\frac{dy_h}{dt} = -\frac{1}{\tau}y_h(t)$  (as in ②) is verified by functions of the form  $y_h(t) = \lambda e^{-\frac{t}{\tau}}$  with  $\lambda \in \mathbb{R}$ . Therefore, an ansatz is to look for the solution of the equation with time-varying independent term under the form  $t \mapsto \lambda(t)e^{-\frac{t}{\tau}}$ , with  $t \mapsto \lambda(t)$  a differentiable function to be determined (without loss of generality). This form is indeed convenient, since its derivative matches the form of the differential equation :

- On the one hand,  $\frac{dy_p}{dt} = \lambda'(t)e^{-\frac{t}{\tau}} - \frac{1}{\tau}\lambda(t)e^{-\frac{t}{\tau}} = \lambda'(t)e^{-\frac{t}{\tau}} - \frac{1}{\tau}y_p(t)$ , by the product expression of a derivative,
- On the other hand,  $\frac{dy_p}{dt} = -\frac{1}{\tau}(y_p(t) - c(t))$ , to satisfy the differential equation.

Equating both expressions leads to a simplification which allows to express the derivative of the function looked for :

$$\lambda'(t)e^{-\frac{t}{\tau}} - \cancel{\frac{1}{\tau}y_p(t)} = -\cancel{\frac{1}{\tau}y_p(t)} + \frac{1}{\tau}c(t) \implies \lambda'(t) = \frac{1}{\tau}e^{\frac{t}{\tau}}c(t) \implies \lambda(t) = \frac{1}{\tau} \int_0^t e^{\frac{s}{\tau}}c(s)ds + \alpha, \text{ with } \alpha \in \mathbb{R} \text{ a constant.}$$

Thus, a solution is given by :  $t \mapsto e^{-\frac{t}{\tau}} \left[ \frac{1}{\tau} \int_0^t e^{\frac{s}{\tau}} c(s) ds + \alpha \right]$ .

To satisfy the initial condition, the constant must verify  $1 \times (0 + \alpha) = y_0 \implies \alpha = y_0$ .

## 1.2 Numerical approximation with Euler Method

⑤ *Taylor expansion* The value of a function  $y$  in the neighborhood of a point  $t$  can be expressed by its Taylor expansion, provided the function  $y$  is infinitely differentiable :

$$y(t + \Delta_t) = y(t) + \sum_{n=0}^{\infty} \frac{y^{(n)}(t)}{n!} \Delta_t^n$$

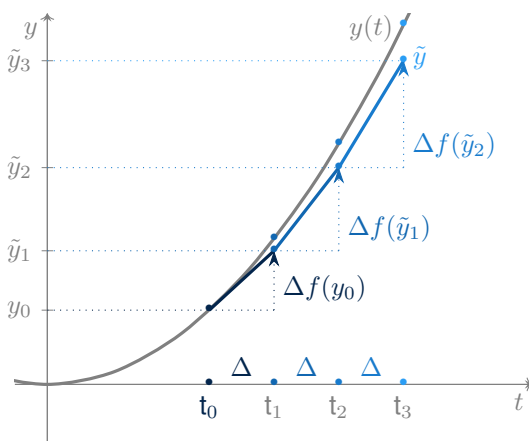
with  $y^{(n)}(t)$  the  $n^{\text{th}}$  derivative of  $y(t)$ .

Truncating at the first order :

$$y(t + \Delta_t) = y(t) + y'(t) \Delta_t + \mathcal{O}(\Delta_t^2)$$

The Euler method builds up an approximation by adding an increment proportional to the tangent at a given point :

$$\tilde{y}_{k+1} \approx \tilde{y}_k + \Delta_t f(\tilde{y}_k)$$



⑥ <sup>num</sup> *Implementation of the algorithm*



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### ⑦ Analytical solution

The solution is  $y(t) = y_0 e^{-kt}$  (question ②), which tends towards 0 when times grows (as  $k > 0$ ).

### ⑧ *Recurrence*

The approximated solution is obtained from the previous time step by (question ⑤) :  $\tilde{y}_{n+1} = y_n - k y_n \Delta t = y_n (1 - k \Delta t)$ .  
By an immediate recurrence (geometric sequence) :  $\tilde{y}_n = y_0 (1 - k \Delta t)^n$ .

This sequence tends to 0 if and only if  $|1 - k\Delta_t| < 1$ , i.e.  $-1 < 1 - k\Delta_t < 1$  which is satisfied provided  $\Delta_t < \frac{2}{k}$ .

### First order method

The error inherent to the Euler's method can be estimated more precisely. Pushing the Taylor expansion one order further :

$$f(t + \Delta t) = f(t) + f'(t)\Delta t + \frac{1}{2}f''(t)\Delta t^2 + \mathcal{O}(\Delta t^3)$$

Therefore, the error made by the Euler scheme at each step is of the order  $\epsilon = \Delta t^2$ . At time  $t$ , the approximation requires  $\approx t/\Delta t$  steps, such that the cumulative effect of the errors is expected to be of order  $\frac{t}{\Delta t} \times \Delta t^2 = t\Delta t$ .

### ⑨ num Failures of the Euler's method



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With  $k = 10$ , the numerical approximation is stable for  $\Delta t \in [0; 1/5]$ . Otherwise, oscillations and divergence can be observed.

## 2 Models of Point Neurons

### 2.1 Leaky Neuron

#### ⑩ Differential equation for the membrane potential

The membrane potential is related to the instantaneous charge of the membrane by :  $V_m = \frac{1}{C_m}Q$ , and deriving this expression gives  $\frac{dV_m}{dt} = \frac{1}{C_m} \frac{dQ}{dt} = I$ , since the current  $I$  is defined as the flow of charges.

Replacing  $I$  by its expression yields :

$$C_m \frac{dV_m}{dt} = -g_l(V_m - E_l)$$

#### ⑪ Solution of the membrane potential's dynamics

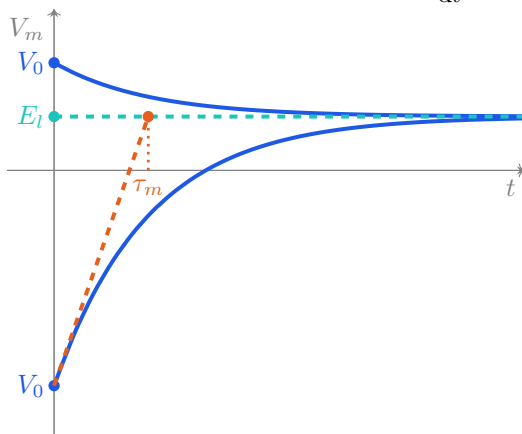
The equation rewrites :  $\frac{C_m}{g_l} \frac{dV_m}{dt} = -V_m + E_l$ .

A characteristic time constant of the system can be defined as  $\tau_m = \frac{C_m}{g_l}$  (it has a dimension of time to comply with the equation homogeneity).

Thus, the membrane potential relaxes exponentially from an initial condition  $V_0$  to its equilibrium  $E_l$  (question ③) :

$$V_m(t) = E_l + (V_0 - E_l) e^{-\frac{t}{\tau_m}}$$

The time constant represents the time at which the membrane potential has relaxed to  $\approx 36\%$  from its deviation from the equilibrium :  $t = \tau_m \implies e^{-\frac{t}{\tau_m}} = e^{-1} \approx 0.36$ . Alternatively, it can be seen as the time at which the tangent at the initial point crosses the abscisses :  $\frac{dV_m}{dt}(t=0) = -\frac{V_0 - E_l}{\tau_m}$



#### ⑫ Distinct behaviors

- $V_0 < E_l \implies V_m$  grows towards  $E_l$ .
- $V_0 > E_l \implies V_m$  decreases towards  $E_l$ .
- $V_0 = E_l \implies V_m$  is fixed.

## 2.2 Leaky Integrate-and-Fire model (LIF)

### (13) Threshold current

The membrane potential dynamics still follows the same differential equation, but with a modified equilibrium, which is switched from  $E_l$  to  $V_\infty = E_l + \frac{I_{app}}{g_l}$  by the additional input current.

Thus, starting from the reset potential, the membrane potential evolves as :


$$V_m(t) = V_\infty + (V_0 - V_\infty) e^{-\frac{t}{\tau_m}}$$

A spike can be emitted only if the membrane potential can reach the threshold  $V_{th}$ , which depends on the position of the equilibrium relative to the threshold. The spiking condition therefore is :

$$V_\infty > V_{th} \implies E_l + \frac{I_{app}}{g_l} > V_{th}$$

The threshold current required for this condition to be met is :

$$I_{th} = g_l(V_{th} - E_l)$$

 Numerical application : With the parameters given in the table,  $I_{th} = 200 \text{ pA}$ .

### (14) num Simulation with the reset mechanism



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With the reset mechanism, the membrane potential evolves periodically from the reset potential to the spiking threshold. This allows to define a firing rate as the inverse of the inter-spike interval, that is the time between two consecutive spikes.

### (15) Firing rate as a function of current

The time  $T_{ISI}$  between two spikes corresponds to the time required to reach the threshold from the reset potential :

$$V_m(T_{ISI}) = V_{th} \implies V_\infty + (V_r - V_\infty) e^{-\frac{T_{ISI}}{\tau_m}} = V_{th} \implies \exp\left(-\frac{T_{ISI}}{\tau_m}\right) = \frac{V_\infty - V_{th}}{V_\infty - V_r}$$

Solutions exist for  $V_\infty > V_{th}$ , which ensures a positive quotient (by assumption  $V_{th} > V_r$ , which implies  $V_\infty > V_{th}$ ). In this case :

$$T_{ISI} = \tau_m \ln\left(\frac{V_\infty - V_r}{V_\infty - V_{th}}\right) = \tau_m \ln\left(\frac{E_l + \frac{I_{app}}{g_l} - V_r}{E_l + \frac{I_{app}}{g_l} - V_{th}}\right)$$

The corresponding firing rate is :

$$f = \frac{1}{T_{ISI}}$$

### (16) Study the function $f(I)$

- Domain of validity : solutions exist for  $V_\infty > V_{th} \implies I_{app} > I_{th}$  (questions (13)).
- Limits of extreme values of the input current :

$$\bullet I_{app} \rightarrow +\infty \implies V_\infty \rightarrow +\infty \implies \frac{V_\infty - V_r}{V_\infty - V_{th}} = \frac{1 - \frac{V_r}{V_\infty}}{1 - \frac{V_{th}}{V_\infty}} \rightarrow 1 \implies T_{ISI} \rightarrow 0 \implies f \rightarrow +\infty$$

$$\bullet I_{app} \rightarrow I_{th}^+ \implies V_\infty \rightarrow V_{th} \implies \frac{V_\infty - V_r}{V_\infty - V_{th}} \rightarrow 0 \implies T_{ISI} \rightarrow +\infty \implies f \rightarrow 0$$

- Asymptotic behavior for  $I_{app} \rightarrow +\infty$  :

An equivalent of the quotient can be obtained by a limited development of logarithms :

$$T_{ISI} = \tau_m \ln\left(\frac{1 - \frac{V_r}{V_\infty}}{1 - \frac{V_{th}}{V_\infty}}\right) = \tau_m \left(\ln\left(1 - \frac{V_r}{V_\infty}\right) - \ln\left(1 - \frac{V_{th}}{V_\infty}\right)\right) \sim \tau_m \left(-\frac{V_r}{V_\infty} + \frac{V_{th}}{V_\infty}\right) = \tau_m \frac{V_{th} - V_r}{V_\infty}$$

Therefore, the firing rate is asymptotically linear in  $I_{app}$  :  $f \sim \frac{1}{\tau_m} \frac{V_\infty}{V_{th} - V_r}$ .

- Slope at the threshold current :

By the chain rule for derivatives :  $\frac{df}{dI_{app}} = \frac{df}{dT_{ISI}} \frac{dT_{ISI}}{dQ} \frac{dQ}{dV_\infty} \frac{dV_\infty}{dI_{app}}$ , with  $Q = \frac{V_\infty - V_r}{V_\infty - V_{th}}$  the quotient.

- $\frac{df}{dT_{ISI}} = -\frac{1}{T_{ISI}^2} = -\frac{1}{\left[\tau_m \ln\left(\frac{V_\infty - V_r}{V_\infty - V_{th}}\right)\right]^2}$
- $\frac{dT_{ISI}}{dQ} = \tau_m \frac{1}{Q} = \frac{V_\infty - V_{th}}{V_\infty - V_r}$
- $\frac{dV_\infty}{dI_{app}} = \frac{1 \times (V_\infty - V_{th}) - 1 \times (V_\infty - V_r)}{(V_\infty - V_{th})^2} = \frac{V_r - V_{th}}{(V_\infty - V_{th})^2}$
- $\frac{dQ}{dV_\infty} = \frac{1}{g_l}$

Altogether :  $\frac{df}{dI_{app}} = -\frac{1}{\tau_m^2 g_l} \frac{1}{\left[\ln\left(\frac{V_\infty - V_r}{V_\infty - V_{th}}\right)\right]^2} \frac{V_\infty - V_{th}}{V_\infty - V_r} \frac{V_r - V_{th}}{(V_\infty - V_{th})^2}$

$$= -\frac{1}{\tau_m^2 g_l} \frac{1}{\left[\ln\left(\frac{V_\infty - V_r}{V_\infty - V_{th}}\right) (V_\infty - V_{th})\right]^2} \frac{(V_\infty - V_{th})(V_r - V_{th})}{V_\infty - V_r}$$

Finding the limit when  $I_{app} \rightarrow I_{th}$  is equivalent to find the limit when  $V_\infty \rightarrow V_{th}$ .

Introducing  $(V_\infty - V_r)^2$  at numerator and denominator :

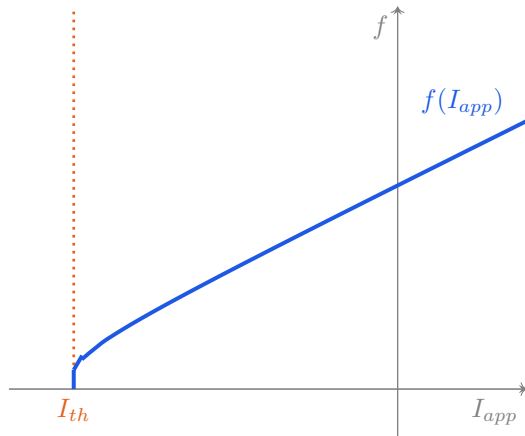
$$= -\frac{1}{\tau_m^2 g_l} \frac{1}{\left[\ln\left(\frac{V_\infty - V_r}{V_\infty - V_{th}}\right) (V_\infty - V_{th})\right]^2} \frac{(V_\infty - V_{th})(V_r - V_{th})}{V_\infty - V_r} \times \frac{(V_\infty - V_r)^2}{(V_\infty - V_r)^2}$$

$$= -\frac{1}{\tau_m^2 g_l} \left[ \frac{\frac{V_\infty - V_r}{V_\infty - V_{th}}}{\ln\left(\frac{V_\infty - V_r}{V_\infty - V_{th}}\right)} \right]^2 \frac{V_r - V_{th}}{V_\infty - V_r} \times \frac{V_\infty - V_{th}}{(V_\infty - V_r)^2}$$

- The squared term contains a limit of the form  $\frac{z}{\ln(z)} \xrightarrow{z \rightarrow +\infty} 0$  with  $z = \frac{V_\infty - V_r}{V_\infty - V_{th}} \xrightarrow{V_\infty \rightarrow V_{th}} +\infty$ .
- The middle term tends to a constant when  $V_\infty \rightarrow V_{th}$ .
- The last term rewrites :  $\frac{V_\infty - V_{th}}{(V_\infty - V_r)^2} = \frac{1}{V_\infty} \frac{1 - \frac{V_{th}}{V_\infty}}{\left(1 - \frac{V_r}{V_\infty}\right)^2} \xrightarrow{V_\infty \rightarrow V_{th}} +\infty$ .

Conclusion : The slope of the f-I curve is vertical when the current tends to its threshold value.

### 17 f-I curve



According to this model, the firing rate is not bounded when the input current increases ( $\lim_{I \rightarrow \infty} f = +\infty$ ), which is not biologically plausible. In real neurons, spikes are not points in time but last for a few milliseconds, and they moreover induce a refractory period during which the neuron is prevented to spike immediately afterwards.

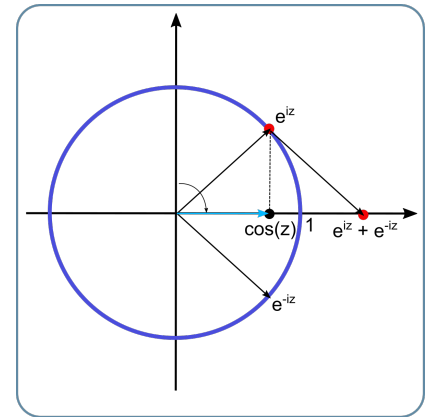
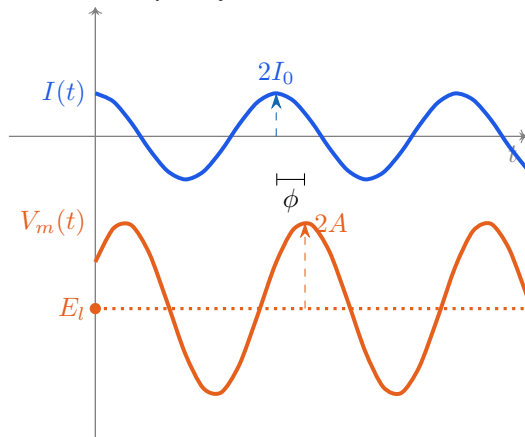
## 2.3 Response to an oscillating input current

### 18 Oscillatory functions

Interpretation of the parameters :

- $2I_0$  and  $2A$  : amplitudes of the oscillations.
- $\phi$  : phase shift (or time delay) of the response of  $V_m$  to the input  $I_{app}$ .

- $\omega$  : frequency of the oscillations.



### (19) Expressions with complex numbers

The cosinus can be expressed of two manners :  $\cos(\theta) = \frac{e^{i\theta} + e^{-i\theta}}{2} = \Re(e^{i\theta})$ .

With this formalism :

$$I(t) = I_0(e^{i\omega t} + e^{-i\omega t})$$

$$V_m(t) = E_l + A(e^{i(\omega t + \phi)} + e^{-i(\omega t + \phi)}).$$

(20) The expressions found in question (19) can be plugged into the differential equation :

$$C_m \frac{dV_m}{dt} = -g_l(V_m(t) - E_l) + I_{app}(t)$$

$$C_m A (i\omega e^{i(\omega t + \phi)} - i\omega e^{-i(\omega t + \phi)}) = -g_l([E_l + A(e^{i(\omega t + \phi)} + e^{-i(\omega t + \phi)})] - E_l) + I_0(e^{i\omega t} + e^{-i\omega t})$$

Factorizing by the independent functions  $t \mapsto e^{i\omega t}$  and  $t \mapsto e^{-i\omega t}$  :

$$(C_m A i\omega e^{i\phi} + g_l A e^{i\phi} - I_0)e^{i\omega t} + (-C_m A i\omega e^{-i\phi} + g_l A e^{-i\phi} - I_0)e^{-i\omega t} = 0$$

$$(A e^{i\phi}(C_m i\omega + g_l) - I_0)e^{i\omega t} + (A e^{-i\phi}(-C_m i\omega + g_l) - I_0)e^{-i\omega t} = 0$$

Multiplying by  $e^{-i\omega t}$  :

$$(A e^{i\phi}(C_m i\omega + g_l) - I_0) \times 1 + (A e^{-i\phi}(-C_m i\omega + g_l) - I_0)e^{-2i\omega t} = 0$$

For this equation to hold for all times  $t$ , both terms should cancel. For instance  $t = \frac{\pi}{4\omega} \Rightarrow e^{-2i\omega t} = e^{-i\frac{\pi}{2}} = -i$ , which imposes in particular for the first term :  $A e^{i\phi}(C_m i\omega + g_l) - I_0 = 0$ .

Simplifying leads to :

$$A \exp(i\phi) = \frac{I_0}{g_l + iC_m\omega}$$

Note : Using the real part expression of the cosinus, the same reasoning could have been carried out by taking a complex oscillating current  $I_{app}(t) = I_0 \cdot e^{i\omega t}$  (which has no physical meaning) and then focusing on the real part of the equations.

### (21) Amplitude and Phase of the response

Any complex number  $z$  can be written either in a Cartesian representation  $z = x + iy$  or polar representation  $z = |z|e^{i\phi_z}$ . From Cartesian to polar coordinates, its module and phase are given by :

$$|z| = \sqrt{x^2 + y^2} \quad \phi_z = \arctan(y/x) + 1_{\{x < 0\}} \cdot \text{sgn}(y) \cdot \pi$$

Applied to the complex number  $A \exp(i\phi)$ ,  $A$  corresponds to the amplitude and  $\phi$  to the phase. On the other hand, the expression found above can be rewritten so that imaginary parts appear only at the numerator :

$$\frac{I_0}{g_l + iC_m\omega} \times \frac{g_l - iC_m\omega}{g_l - iC_m\omega} = \frac{I_0}{g_l^2 + C_m^2\omega^2} \cdot (g_l - iC_m\omega)$$

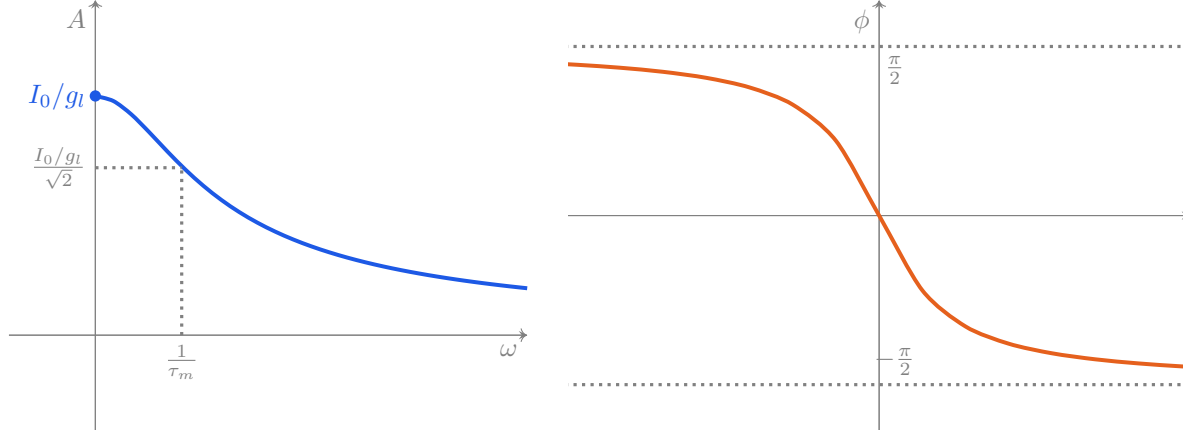
By identification :

$$A = \frac{I_0}{g_l^2 + C_m^2 \omega^2} \times \sqrt{g_l^2 + (C_m \omega)^2} = \frac{I_0}{g_l \sqrt{1 + \left(\frac{C_m}{g_l}\right)^2 \omega^2}} \quad \phi = \arctan\left(-\frac{C_m \omega}{g_l}\right) = -\arctan\left(\frac{C_m}{g_l} \omega\right)$$

Introducing the characteristic time constant  $\tau_m = \frac{C_m}{g_l}$  :

$$A = \frac{I_0/g_l}{\sqrt{1 + \tau_m^2 \omega^2}} \quad \phi = -\arctan(\tau_m \omega)$$

## 22 Behaviors at high and low frequencies



- At low frequency ( $\omega \ll 1/\tau_m$ ), the membrane response can perfectly follow the sinusoidal input since the phase tends to 0, and in this case the amplitude tends to its maximum  $A = I_0/g_l$ . For small oscillation frequencies  $\omega$ , the phase can be approximated  $\arctan(\tau_m \omega) \approx \tau_m \omega$  such that :

$$V_m(t) \approx E_l + 2I_0/g_l \cos(\omega(t - \tau_m))$$

Thus, the difference in phase just corresponds to the time for the membrane to relax (with the characteristic time scale  $\tau_m$ ).

- At high frequency ( $\omega \gg 1/\tau_m$ ), the input current oscillates too quickly for the membrane to have the time to integrate the signal (which requires an time scale of order  $\tau_m$ ). In that case, the amplitude cannot develop and remains close to 0, while the phase to  $-\pi/2$ .

For small oscillation frequencies  $\omega$ , the amplitude becomes equivalent to  $A \sim \frac{I_0/g_l}{\sqrt{\tau_m^2 \omega^2}} = \frac{I_0/g_l}{\tau_m \omega} = \frac{I_0}{C_m \omega}$ , such that :

$$V_m(t) \approx E_l + 2\frac{I_0}{C_m \omega} \cos(\omega t - \pi/2)$$

- Conclusion : The membrane acts as such as a first-order low-pass filter. No resonance phenomenon is observed (as there is no peak in the frequency) as can be seen with higher order integrators.