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Predicting Clinical ICU-related Outcomes from Electronic Health Records: a Two-Stage Deep Learning Approach combining Transformers and Graph Neural Networks

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Abstract

Early detection of clinical decline enables for timely admission to the Intensive Care Unit (ICU) and saves lives. In this work, I present a two-stage Deep Learning pipeline designed to predict several clinical outcomes from the MIMIC-IV electronic health records (EHR) database. This approach first aggregates and pre-processes patient admission data, covering demographic and administrative details, early laboratory flags, ICU vital signs, and ICU timing intervals into a unified tabular representation. Then, a Transformer-based 'Clinical State Estimator' is used to produce an embedding for categorical features and to learn both ICU-transfer risk and time-to-ICU predictions. In the second stage, each hospital admission is represented as a node in a heterogeneous admission-centric hypergraph, with edges that capture three complementary relationships: early-stage similarity (K-Nearest-Neighbors in feature space), predicted ICU transfers (connections to a dummy ICU node, weighted by probabilities produced by the first stage), and temporal links between multiple admissions of the same patient. Finally, a multilayer Graph Neural Network (combining GCN/R-GCN, GATv2 and GraphSAGE with JumpingKnowledge concatenation) processes this graph to jointly predict in-hospital mortality, length of stay in the ICU, and discharge location. Experiments on MIMIC-IV show state of the art results for mortality risk prediction (AUC 0.909, Accuracy 0.963), ICU-duration regression (RMSE 54-55 h, MAE 35-36 h), and discharge-location accuracy (0.742). An ablation study confirmed that both the multi-edge graph design and the multitask supervision yield significant gains. This method relies exclusively on standard hospital data, is end-to-end differentiable, and runs

in real time on a single GPU, making it suitable for prospective deployment and a promising direction for graph-aware clinical decision support.

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Chapter 1

Introduction

Unrecognized deterioration in hospital wards often results in emergent transfers to the Intensive Care Unit (ICU), a scenario repeatedly associated with higher mortality and longer stays. Multiple studies report that every hour of delay in admission to the ICU increases the odds of death for critically ill adults. Mixed evidence on whether operational delays alone explain outcomes further underscores the value of earlier detection and proactive triage (Cardoso et al. 2011; Churpek et al. 2016; Kiekkas et al. 2022).

Hospitals commonly deploy early warning scores (EWS) that compare the values of a small set of vital signs and lab tests against fixed thresholds. Although simple, inexpensive, and broadly adopted, the clinical benefit of these metrics remains debated. Several articles show that EWS are validated with widely differing datasets, endpoints, time windows, and evaluation metrics, and are often digitized without being fully integrated into clinical decision workflows (Bedoya et al. 2019; Fang, Lim, and Balakrishnan 2020; Nagarajah, Krzyzanowska, and Murphy 2022; Wong et

al. 2024). Additionally, EWS can miss complex temporal patterns that are instead embedded in broader electronic health record (EHR) data.

In recent years, there has been a move towards the adoption of digital health record systems in hospitals: in 2015, in the United States, nearly 96% of hospitals had a digital EHR system. Retrospectively collected medical data has increasingly been used for epidemiology and predictive modeling, mainly due to the effectiveness of modeling approaches on large datasets. Despite these advances, access to medical data to improve patient care remains a significant challenge: while the reasons for limited sharing of medical data are multifaceted, concerns about patient privacy are highlighted as one of the most significant issues. Uniquely, the Medical Information Mart for Intensive Care (MIMIC, Goldberger et al. 2000) database adopted a permissive access scheme which allowed for broad reuse of the data, becoming the backbone in a variety of studies ranging from assessment of treatment efficacy in well defined cohorts to prediction of key patient outcomes such as mortality, while maintaining reproducibility.

However, this type of data is heterogeneous (categorical, binary, continuous), irregularly sampled, and frequently with missing information (Singh, Sato, and Ohkuma 2021; Ren et al. 2024). This structure poses modeling challenges for most of the classic machine learning approaches, such as Logistic Regression or Random Forests, that may struggle with complex temporal and cross-modal dependencies. To alleviate the need for feature engineering, which is currently a key aspect in tabular data learning methods, and, perhaps most importantly, to allow representation and multitask learning, which enables many valuable application scenarios, Deep Learning methods, such as Recurrent Neural Networks (RNNs), Long Short Term

Memory (LSTMs) and Attention-based Transformers, have improved data modeling in the EHR; however, they still treat each hospital encounter in isolation, overlooking cohort-level and longitudinal dependencies (Siebra, Kurpicz-Briki, and Wac 2024).

A solution to this problem is offered by Graph Neural Networks (GNNs) that are capable of encoding relations among admissions, patients, and clinical concepts by representing each admission as a node and encoding clinically meaningful relationships as edges. Early works built homogeneous patient-centric graphs via simple similarity metrics, while recent efforts have introduced heterogeneous graphs incorporating diagnoses, medications and procedures as separate node types.

Additionally, a recurring pattern in the latest works is the use of a two-stage pipeline, where an upstream sequence or tabular model (e.g., LSTM for vital data or a Transformer for admission features) estimates intermediate clinical states or latent embeddings. Then, these outputs are used to construct downstream the graph inputs (nodes, node attributes, or edge weights), effectively denoising raw EHR features and injecting domain structure into the graph (Tong et al. 2021). However, existing methods generally do not fully exploit these intermediate embeddings directly as node features or utilize multiple edge relationships within the same patient graph.

In this work, these gaps are addressed by introducing a novel and optimized two-stage architecture (see Fig. 1.1). This approach uses a Transformer-based Clinical State Estimator to predict from admission features (gender, age, admission type, admission location, and six laboratory test results obtained in the first 24 hours since admission) both the probability of an ICU transfer and the expected delay until that transfer, but also to provide the latent embeddings that directly feed into the nodes of a heterogeneous admission-centric graph. Each node represents a different hospital

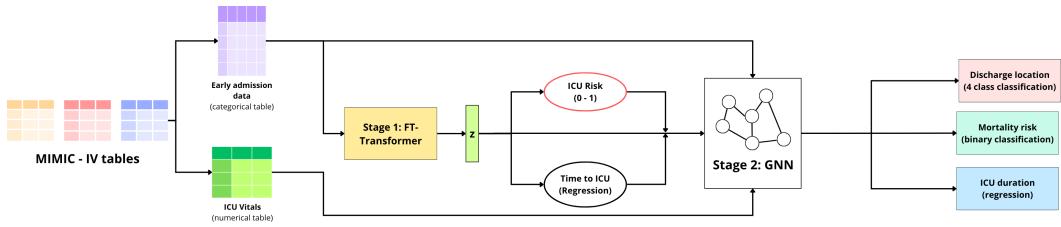


Figure 1.1. Pipeline Architecture: admission and vitals dataset aggregation; admission features are tokenized and fed to the Transformer to produce a latent representation (z) and to output ICU risk and delay; these (plus the Vitals for ICU patients) are used to enrich the graph that is processed by the GNN to predict mortality risk, ICU duration and discharge location.

admission, enriched with clinical predictions and, when available and applicable, the ICU vital signs. The nodes are connected through three complementary edge families: feature-space proximity, prospective transfer risk, and temporal continuity across a patient’s multiple admissions. Finally, a hybrid GCN (Kipf et al. 2016) / R-GCN (Schlichtkrull et al. 2018) + GATv2 (Velickovic et al. 2017) + GraphSAGE (Hamilton, Ying, and Leskovec 2017) model with Jumping Knowledge (Xu et al. 2018) aggregation performs mortality risk, ICU length-of-stay, and discharge location prediction in a single forward pass.

By combining tabular transformer embeddings with a relational graph model, this pipeline aims to capture both low-level feature interactions (e.g., between gender, age, and lab tests) and high-level cohort relationships (e.g., patients with similar early states, those at risk of ICU transfer, and a patient’s own longitudinal history). Together, these components demonstrate a modular and extensible framework for using tabular and graph deep learning techniques on real-world EHR data to improve clinical outcome predictions. This framework is evaluated against robust baseline

models from recent literature on the MIMIC-IV (Johnson et al. 2023) database, achieving state of the art predictive performance while operating in real time on a single GPU. The results obtained demonstrate that combining Transformer embeddings directly with heterogeneous GNNs provides an effective, efficient, and clinically actionable solution for early detection of clinical deterioration and more timely ICU transfers, with significant potential to improve patient outcomes.

1.1 Thesis Structure

This thesis is structured to progressively introduce the problem context, the methodological foundations, and the experimental validation of the proposed approach. The first chapter provides an overview of the clinical and technical motivations underlying the work, highlighting the challenges of predicting ICU-related outcomes from the EHR and describing the research questions addressed in this study. The second chapter reviews the relevant literature, discussing existing Machine Learning and Deep Learning approaches for clinical outcome prediction, with particular emphasis on Transformer-based models for tabular EHR data, Graph Neural Networks applied to healthcare, and two-stage and multi-task learning paradigms. The dataset and the preprocessing pipeline are presented in the third chapter, which describes the MIMIC-IV database, the data extraction process, feature engineering choices, and the strategies adopted to ensure temporal consistency and to mitigate data leakage. The fourth chapter details the proposed methodology, introducing the two-stage learning framework and providing an in-depth description of both the Transformer-based clinical state estimation module and the Graph Neural Network

used to model inter-patient relationships, together with the associated design choices and implementation details. Experimental results are reported in the fifth chapter, where the evaluation protocol, baseline comparisons and ablation studies are presented and discussed in order to assess the effectiveness of the proposed approach across multiple clinical prediction tasks; in this chapter, model interpretability and explainability are discussed, presenting post-hoc analysis techniques applied to the framework and discussing their relevance, limitations, and implications in a clinical decision-support setting. Finally, the sixth chapter concludes the thesis by summarizing the main findings, discussing the limitations of the proposed methodology, and outlining potential directions for future research.

Chapter 2

State of the Art

Predictive modeling in healthcare has gradually evolved from early rule-based and purely statistical approaches, such as Logistic Regression or Random Forests, to advanced Deep Learning architectures, which are capable of extracting meaningful representations from heterogeneous data sources. In addition, advances in model design have recently focused on addressing two challenges related to clinical prediction: the need to effectively capture relational dependencies among admissions and clinical events and the need of producing reliable and interpretable predictions that can be safely and meaningfully integrated into real-time clinical decision support systems.

2.1 Transformer Models on Tabular EHR

Attention mechanisms have proven particularly suitable for clinical data due to their ability to dynamically weight heterogeneous input features according to task relevance. Unlike traditional feed-forward architectures, attention allows the model to focus selectively on subsets of clinical variables, enabling context-dependent

feature interaction modeling. This property is especially important in EHR data, where the predictive relevance of a variable often depends on the presence or absence of other conditions, laboratory abnormalities, or demographic factors.

Attention-based architectures, such as FT-Transformer (Feature Tokenizer + Transformer, Gorishniy et al. 2022), a simple adaptation of the Transformer architecture for the tabular domain, and TabNet (Arik et al 2021), that uses sequential attention mechanisms to choose which features to reason from at each decision step, learn efficiently feature interactions, without extensive pre-processing, as the learning capacity is used for the most relevant features.

In the healthcare domain, Transformers have been successfully applied to a wide range of predictive tasks, including the forecasting of vital signs and the estimation of clinical risk scores for outcomes for ICU transfer or in-hospital mortality.

An et al. (2022) presented a time-aware Transformer-based Hierarchical Attention Network designed to model the irregular timing of multivariate ICU data (e.g. lab tests and vital signs) and to fuse heterogeneous modalities through a two-stage attention scheme. The Transformer learns personalized temporal decay functions for each event, while the hierarchical attention mechanism aggregates interactions into a unified patient representation.

Similarly, Darabi et al. (2020) introduced TAPER, a time-aware patient EHR representation framework that first uses a Transformer encoder (with causal masking and sinusoidal positional encodings) to embed structured codes and then a BioBERT (initialized BERT plus bidirectional GRU autoencoder) to summarize clinical text into unified visit vectors.

Such works demonstrate that Transformers can effectively handle structured and

unstructured EHR data, producing semantically rich patient-level representations that serve as ideal inputs for downstream predictors.

Despite their expressive power, Transformer-based models inherently operate on independent samples and therefore lack mechanisms to explicitly encode relationships between different patients or admissions, treating them as isolated instances. As a consequence, clinically meaningful similarities across individuals, such as shared comorbidity patterns, disease progression trajectories, or treatment responses, remain unexploited. Moreover, Transformers typically require substantial amounts of data to generalize well and may exhibit reduced robustness when deployed in highly heterogeneous cohorts. These limitations motivate the integration of relational inductive biases through graph-based modeling.

2.2 GNNs in Clinical Predictions

GNNs have recently emerged as a powerful tool for clinical prediction tasks by explicitly modeling the relational structure inherent to medical data. Instead of relying solely on independent feature vectors, GNNs propagate information along edges that encode domain-specific relationships. This property is particularly attractive for clinical applications, where patient similarity, comorbidity co-occurrence, and treatment pathways form complex, interconnected structures.

Early works adapted Graph Convolutional Networks to homogeneous patient similarity graphs, where nodes represent individual patients and edges encode similarity in demographics, comorbidity profiles or treatment histories (Boll et al. 2023; Maroudis et al. 2024; Rocheteau et al. 2021). These approaches demonstrated

that the message-passing mechanism between similar patients could improve stability and predictive accuracy, especially in data-sparse regions of the feature space.

Subsequent works introduced heterogeneous graphs and more sophisticated architectures, characterized by multiple node and edge types, such as patients, lab tests, medications and diagnoses, linked by different relations, allowing models to jointly learn across modalities and relation semantics and to produce robust early warning systems for conditions such as sepsis and acute kidney injury (Wang and Li 2025; Daphne et al. 2025; Liu et al. 2022).

In all these studies, the main advantage of GNNs lies in their ability to learn from both individual features and their complex inter-dependencies, which is crucial for accurate and clinically actionable predictions.

However, their application in clinical settings introduces some challenges: graph construction often relies on heuristic similarity measures or static thresholds, which may not generalize across cohorts or institutions; additionally, full-graph training can be computationally expensive and prone to oversmoothing, particularly in large and densely connected graphs. These factors require careful design choices with respect to edge definition, training strategy, and scalability.

2.3 Two-Stage Pipelines

Two-stage architectures decompose complex prediction tasks into a coarse 'proposal' or representation phase, followed by a finer-grained refinement and decision phase, and have proven effective in many domains, separating broad, information-rich but computationally inexpensive feature extraction from more targeted, high-capacity

inference. This separation also improves robustness, since errors in early-stage predictions do not necessarily propagate deterministically to final outcomes, especially when downstream models incorporate relational smoothing.

Applied first to recommender systems, retrieval-then-ranking pipelines (e.g., Covington et al. 2016) use a lightweight, approximate Nearest-Neighbor model to shortlist items before a more expressive deep ranking model refines the final recommendations.

Two-stage frameworks have also been adapted for tabular and clinical settings: for example, an autoencoder or feature-tokenizer backbone produces low-dimensional patient embeddings, which are then passed to a specialized sequence model or GNN for the final predictions (Wu et al. 2020; Li et al. 2021). Across these contexts, the two-stage paradigm balances efficiency and expressivity by allocating computational resources where they are most needed: broad-scope candidate identification followed by targeted high-capacity inference.

This modularity also enhances interpretability and facilitates transfer learning, since the intermediate embeddings can be reused or analyzed independently.

2.4 Multi-task Pipelines

Another major trend in the literature is the use of multi-task learning, where related prediction objectives are trained jointly within a shared representation space.

Joint multi-task learning frameworks in clinical prediction use shared representations to improve performance and regularize learning across related outcomes, such as in-hospital mortality, ICU length of stay, and readmission risk, which are often

correlated.

However, despite their benefits, multi-task learning frameworks must carefully balance shared and task-specific representations. Improper task weighting or overly constrained shared layers may lead to negative transfer, where optimization for one outcome degrades performance on others. Recent approaches therefore emphasize selective parameter sharing, auxiliary task supervision, and task-aware regularization strategies to maximize synergy while preserving task-specific discriminative capacity.

Harutyunyan et al. (2017) first demonstrated on the MIMIC-III benchmark that RNN-based multitask models with deep supervision outperform single-task baselines on mortality, length-of-stay forecasting, physiologic decline detection, and phenotype classification.

Rajkomar et al. (2018) followed this approach by training deep sequence models on raw EHR data to simultaneously predict in-hospital mortality, 30-day readmission, prolonged length-of-stay and final discharge diagnoses.

More recently, Shickel et al. (2021) introduced a Flexible Multimodal Transformer that jointly predicts several ICU outcomes, including various readmission windows and mortality horizons, within one end-to-end architecture, showcasing state of the art accuracy and the ability to incorporate diverse data modalities.

By exploiting common signals across tasks, these joint multi-task pipelines yield more robust, data-efficient, and interpretable clinical decision support systems.

2.5 Discussion and Positioning

Taken together, these research directions reflect a converging trend toward modular, relational, and semantically structured architectures for clinical predictive modeling. Nevertheless, the majority of existing approaches address these challenges in isolation rather than within a unified framework: Transformer-based models are effective at capturing intra-admission dependencies but ignore inter-patient similarity, while GNN-based approaches model population-level structure but often rely on precomputed or static node features; multi-task learning frameworks enhance performance but typically operate within homogeneous architectures.

The approach proposed in this thesis integrates these advances into a unified framework. In the first stage, a Transformer-based model generates informative latent representations and outcome probabilities at the admission level, which are then aggregated to form the node features. In the second stage, a heterogeneous graph model explicitly captures the relational structure among patients, enabling information sharing across clinically similar cases. Finally, a multi-task objective jointly predicts mortality, ICU length of stay and discharge location, encouraging the learning of robust and generalizable representations. This combination situates the proposed approach at the intersection of the most promising directions in clinical machine learning within a computationally efficient two-stage design which is not only accurate, but also scalable, interpretable, and adaptable to different healthcare environments.

Chapter 3

Dataset

3.1 MIMIC-IV

The MIMIC-IV (Medical Information Mart for Intensive Care) is one of the largest and most widely used publicly available databases for clinical research. It was developed and maintained by the Laboratory for Computational Physiology at the Massachusetts Institute of Technology (MIT) in collaboration with the Beth Israel Deaconess Medical Center in Boston, collecting patients admitted to the emergency department or an Intensive Care Unit at the Beth Israel Deaconess Medical Center. It contains data from 2008 to 2022 for more than 65,000 patients admitted to an ICU and over 200,000 patients admitted to the emergency department, reflecting present-day clinical practice with ICD-10 diagnosis codes, electronically charted medication administration, and other contemporary workflows.

Patient identifiers, as stipulated by the Health Insurance Portability and Accountability Act (HIPAA), have been removed and replaced using a random cipher, resulting in de-identified integer identifiers for patients, hospitalizations, and ICU

stays and ensuring that no protected health information is included.

The database is organized into modular components to facilitate targeted analysis and efficient data access. In detail, it is divided into two modules, 'hosp' and 'icu': data in the 'hosp' module is sourced from the hospital wide EHR, while data in the 'icu' module is sourced from the in-ICU clinical information system; the first one includes demographic information, admission and discharge details, diagnosis and procedure codes, laboratory results, microbiology tests, medication prescriptions, and other administrative or clinical events recorded during hospitalization, while the second contains continuously monitored vital signs, detailed nurse charting, fluid balance, ventilator settings, and hourly laboratory measurements.

This modular approach to data organization highlights data provenance and facilitates both individual and combined use of disparate data sources (Fig. 3.1).

3.2 Data Aggregation and Preprocessing

For preprocessing the data, specific columns were extracted and their values were aggregated to better fit into a Neural Network.

3.2.1 Administrative and Demographic Table

A first table is built from both the 'hosp' and 'icu' modules to capture the demographic and administrative details of each admission: hospital admission ID, patient ID, gender, age, admission logistics (specifying the admission type: elective, emergency or observation), source location (where the patient came from), discharge disposition (where the patient was sent after leaving the hospital: home, deceased,

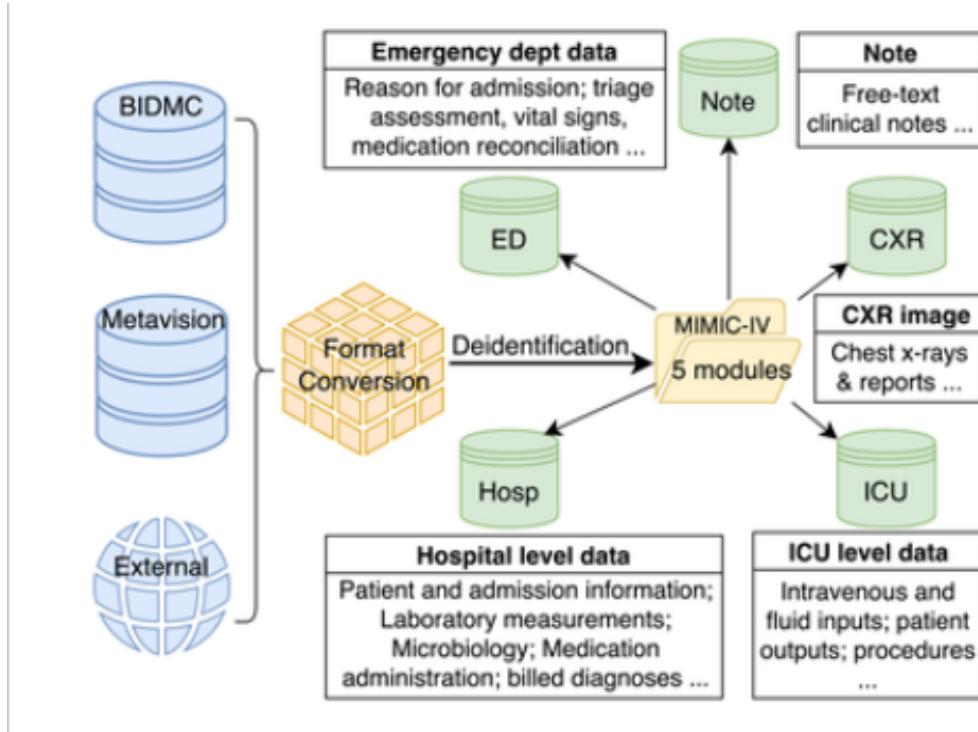


Figure 3.1. MIMIC-IV built by merging the various data sources and structured in five different modules, each with its own specific tables.

transfer, other). These variables provide essential contextual information that is routinely available at or shortly after admission and play a central role in early risk stratification and resource allocation. To improve robustness, the age of the patients was discretized into 8 ordered age groups (0-20, 21-30, 31-40, 41-50, 51-60, 61-70, 71-80, 81-99), reducing sensitivity to noise in exact age values, and facilitating downstream modeling with categorical feature encodings.

Next, a variable is added to identify whether the patient, during that specific admission, went to an ICU or not. This variable serves both as a primary target for ICU risk prediction and as a stratifying factor for the construction of ICU-specific features in subsequent tables.

Finally, for each admission, the time from hospital admission to the first ICU entry (in hours) and the duration of the ICU stay (in hours) were computed: these two values are used as model target data and have been min-max normalized to stabilize training and improve convergence.

3.2.2 Early Laboratory Results in the First 24 Hours

Laboratory measurements collected during the first 24 hours after hospital admission provide an early and clinically meaningful snapshot of a patient's physiological state. Abnormalities observed in this initial time window often reflect acute organ dysfunction, metabolic imbalance, or underlying disease severity, and are therefore highly informative for downstream outcomes such as ICU transfer, mortality, and length of stay.

For each lab test (bicarbonate, creatinine, glucose, ast, bilirubin, hematocrit), a categorical flag was introduced: if *any* measurement of that test in the first 24 hours after admission was marked as 'abnormal', the flag was set to 'abnormal'; otherwise, if there were all 'normal' or missing values, the flag was set to 'normal'. This aggregation strategy follows a clinically conservative assumption, whereby the presence of at least one abnormal value is considered sufficient to signal potential physiological instability, while the absence of measurements for a specific test is considered equivalent to a normal value for that test.

The resulting categorical variables were subsequently encoded as binary indicators, enabling seamless integration into the tabular feature set used by the first-stage Transformer model, reducing sensitivity to irregular sampling frequencies and missingness, which are common in real-world EHR data and may vary substantially

across patients and tests.

By focusing on early laboratory abnormalities, this design aligns with the objective of early risk stratification at admission time, providing informative yet compact signals that complement demographic and admission-level features in the overall modeling pipeline.

3.2.3 Vital Signs (for ICU-admissions only)

In addition, to incorporate physiological data, a separate table was created to summarize the vital signs measurements recorded for each admission during stays in the ICU. They represent continuous, high-frequency indicators of patient status and are particularly informative for characterizing disease severity and short-term clinical trajectories in critically ill patients.

Given the high temporal resolution and irregular sampling of these statistics, raw time series were aggregated at the admission level. Specifically, for each ICU-admission ID, the average, the minimum, and the maximum values were calculated for all available ICU chart events (Systolic Blood Pressure, Heart Rate, Respiratory Rate, Body Temperature, Peripheral Oxygen Saturation (SpO_2), Point-of-Care Glucose) and z-score normalized, resulting in a distribution with average 0 and standard deviation 1, to balance the absence of some or all of these statistics for many admissions.

The purpose of this table was to condense hundreds of individual measurements into a few clinically meaningful metrics for each admission, capturing both central tendency and extreme physiological deviations, without requiring explicit temporal modeling at this stage, and also balancing predictive accuracy, interpretability, and

computational and runtime costs.

3.3 Dataset Balancing

Real-world clinical datasets are often characterized by substantial class imbalance, reflecting the natural prevalence of clinical events rather than modeling convenience. In the context of this study, ICU admissions represent a minority of hospital encounters, which poses a significant challenge for supervised learning models. When trained on highly imbalanced data, predictive models tend to be biased toward the majority class, resulting in suboptimal discrimination performance and poorly calibrated risk estimates for clinically critical but less frequent outcomes. Addressing this imbalance is therefore a necessary preprocessing step to ensure reliable learning dynamics and meaningful evaluation.

To mitigate the class imbalance associated with the `was_in_icu` label, a targeted resampling strategy was applied to the original cohort. Starting from the full dataset of 546 028 hospital admissions, all ICU admissions were retained (85 242 rows), while 127 863 non-ICU admissions were randomly sampled and concatenated to form a balanced subset of 213 105 admissions. This procedure results in ICU cases representing 40% of the final dataset, a proportion that remains clinically realistic while substantially reducing the imbalance observed in the original distribution.

Such re-balancing was necessary to ensure stable model training and to avoid bias toward the majority non-ICU class in both classification and regression tasks. Compared to more aggressive balancing strategies (e.g., full undersampling or synthetic oversampling), this approach preserves a large and diverse set of non-ICU

Table 3.1. Summary of Dataset Balancing and Outliers Removal

Total admissions	546 028
ICU admissions (<code>was_in_icu = 1</code>)	85 242 (15.6%)
ICU ratio after balancing	40%
Dataset size after balancing	213 105
Rows removed (top 1% <code>icu_duration</code>)	2 131
Mean <code>icu_duration</code> before removal	84.20
Max <code>icu_duration</code> before removal	3 832.00
Mean <code>icu_duration</code> after removal	69.45
Max <code>icu_duration</code> after removal	421.66
ICU ratio after outlier removal	39.39%

cases while improving class balance.

In addition to class imbalance, clinical outcomes related to ICU stay duration are affected by extreme values, often corresponding to rare complications, prolonged recovery, or external organizational factors that are difficult to model reliably. To prevent such outliers from disproportionately influencing the optimization process, a final outlier removal step was performed. Specifically, admissions whose `icu_duration` fell within the top 1% of the distribution (from longest to shortest) were flagged as extreme outliers and removed. This choice reflects a conservative trimming strategy aimed at reducing variance without discarding clinically representative cases.

After these steps, the `ICU_duration` shows a mean of 69.5 hours and a standard deviation of 70.1 hours, with a maximum value of 421.6 hours, while the time from

hospital admission to ICU transfer (`hosp_to_icu`) has a mean of 34.5 hours with a standard deviation of 101.3 hours. These distributions indicate a residual but manageable degree of variability, consistent with the heterogeneous nature of critical care trajectories. Table 3.1 summarizes the effects of the balancing and outlier removal procedures on the dataset composition and key statistics.

After the preprocessing procedure, each row in the final dataset corresponds to a single hospital admission and integrates demographic and admission information, laboratory indicators, aggregated ICU vital signs, and outcome variables. This structured representation is specifically designed to support both stages of the proposed modeling pipeline: admission-level prediction in the Transformer-based first stage and relational reasoning in the graph-based second stage. A detailed summary of the variables and their distributions is reported in Tables 3.2 and 3.3.

Table 3.2. Dataset Columns: Attributes, Data Types and MIMIC-IV Sources

Attribute	Data Type	Source MIMIC-IV Table
hadm_id	Identifier (integer)	admissions
subject_id	Identifier (integer)	patients
gender	Binary (M/F)	patients
age_group	Categorical (8 bins)	patients (anchor_age)
year	Integer (admission year)	patients (anchor_year_group)
hosp_mortality	Binary (0/1)	admissions (deathtime)
adm_type	Multiclass (4 categories)	admissions
adm_loc	Multiclass (4 categories)	admissions
disc_loc	Multiclass (4 categories)	admissions
bicarbonate_test	Binary (normal/abnormal)	labevents (itemid=50868)
creatinine_test	Binary (normal/abnormal)	labevents (itemid=50882,50912)
glucose_test	Binary (normal/abnormal)	labevents (itemid=50931,50893)
ast_test	Binary (normal/abnormal)	labevents (itemid=50862)
bilirubin_test	Binary (normal/abnormal)	labevents (itemid=50878,50885)
hematocrit_test	Binary (normal/abnormal)	labevents (itemid=50822,50810)
was_in_icu	Binary (0/1)	icustays
mean_sysbp	Continuous (mmHg)	chartevents (itemid=220045)
min_sysbp	Continuous (mmHg)	chartevents (itemid=220045)
max_sysbp	Continuous (mmHg)	chartevents (itemid=220045)
mean_hr	Continuous (beats/min)	chartevents (itemid=220179)
min_hr	Continuous (beats/min)	chartevents (itemid=220179)
max_hr	Continuous (beats/min)	chartevents (itemid=220179)
mean_rr	Continuous (breaths/min)	chartevents (itemid=220180)
min_rr	Continuous (breaths/min)	chartevents (itemid=220180)
max_rr	Continuous (breaths/min)	chartevents (itemid=220180)
mean_temp	Continuous (°C)	chartevents (itemid=220210)
min_temp	Continuous (°C)	chartevents (itemid=220210)
max_temp	Continuous (°C)	chartevents (itemid=220210)
mean_spo2	Continuous (%)	chartevents (itemid=220277)
min_spo2	Continuous (%)	chartevents (itemid=220277)
max_spo2	Continuous (%)	chartevents (itemid=220277)
mean_glucose	Continuous (mg/dL)	chartevents (itemid=223761)
min_glucose	Continuous (mg/dL)	chartevents (itemid=223761)
max_glucose	Continuous (mg/dL)	chartevents (itemid=223761)
hosp_to_icu_1	Continuous (hours)	icustays & admissions
icu_duration_1	Continuous (hours)	icustays

Table 3.3. Distribution of the categorical attributes of the dataset

Attribute	Label	Count	%
Gender	0	106,413	50.4%
	1	104,561	49.6%
In-hospital mortality	0	199,753	94.7%
	1	11,221	5.3%
Admission type	0	29,488	14.0%
	1	138,289	65.6%
	2	43,197	20.5%
Admission location	0	85,277	40.4%
	1	2,456	1.2%
	2	83,728	39.7%
	3	39,513	18.7%
Discharge location	0	14,521	6.9%
	1	145,706	69.1%
	2	1,644	0.8%
	3	49,103	23.3%
Was in ICU	0	127,863	60.6%
	1	83,111	39.4%
Bicarbonate test	0	23,668	11.2%
	1	187,306	88.8%
Creatinine test	0	79,595	37.7%
	1	131,379	62.3%
Glucose test	0	133,936	63.5%
	1	77,038	36.5%
AST test	0	23,745	11.3%
	1	187,229	88.7%
Bilirubin test	0	31,344	14.9%
	1	179,630	85.1%
Hematocrit test	0	8,429	4.0%
	1	202,545	96.0%
Age group	0	2,695	1.3%
	1	15,727	7.5%
	2	18,335	8.7%
	3	24,254	11.5%
	4	39,162	18.6%
	5	45,090	21.4%
	6	36,549	17.3%
	7	29,162	13.8%

Chapter 4

Methodology

4.1 Stage 1

In recent years, many different approaches have been adopted to handle EHR data, which commonly include many discrete low-cardinality variables (e.g., gender, age group, admission type, location codes, binary lab flags). In particular, in this work the performances of Logistic Regression (for ICU risk classification only), Linear Regression (for time to ICU regression only), Random Forests, Multi-Layer Perceptron (MLP) and Feature-Tokenizer-Transformer (FT-Transformer) are compared. Tables 5.1 and 5.2 (shown in Chapter 5) summarize the results obtained in the experiments: the transition from linear to nonlinear and then to DL approaches produced incremental gains, the addition of multitask supervision consistently improved both classification and regression and, finally, the FT-Transformer (Figure 4.1) produced the greatest benefits, allowing also multi-task learning and the encoding of a latent representation.

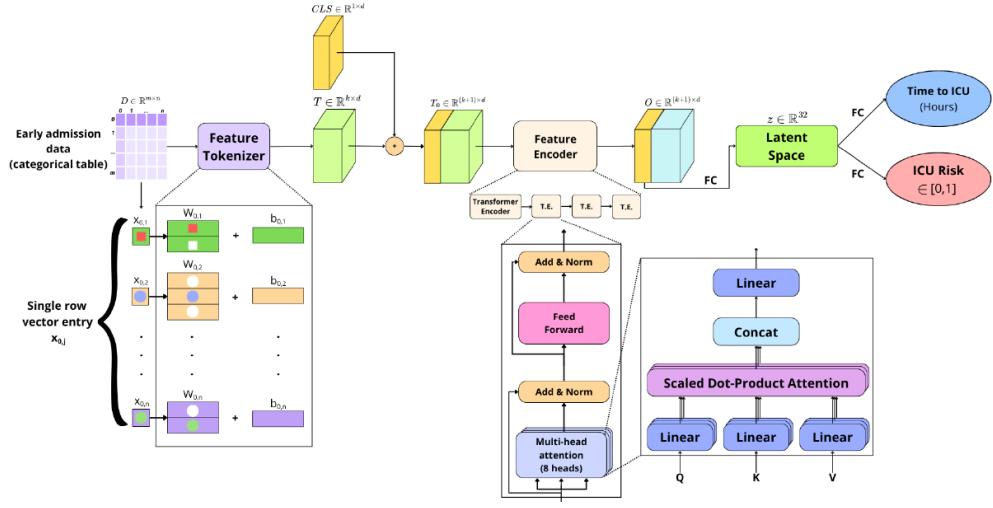


Figure 4.1. Feature-Tokenizer Transformer Architecture: admission features are tokenized and fed to the Transformer; it produces a latent representation (z) and outputs ICU risk and delay through its Multi-Head Attention mechanism and a final Fully Connected (FC) block.

4.1.1 Baseline Models

Before introducing the proposed Transformer-based clinical state estimator, several baseline models were implemented and evaluated, spanning different levels of model complexity and representational capacity. These models serve both as reference points for performance comparison and as methodological baselines to assess the contribution of nonlinear modeling, feature interaction learning, and multi-task optimization.

Logistic Regression

Logistic Regression was adopted as a baseline for the binary classification task of ICU admission risk prediction. Given an input feature vector $\mathbf{x} \in \mathbb{R}^d$, the model

estimates the probability of ICU admission as

$$p(y = 1 \mid \mathbf{x}) = \sigma(\mathbf{w}^\top \mathbf{x} + b), \quad (4.1)$$

where $\sigma(\cdot)$ denotes the sigmoid function, \mathbf{w} is the weight vector, and b is a bias term. Model parameters were optimized by minimizing the binary cross-entropy loss. Due to its linear decision boundary and high interpretability, Logistic Regression represents a widely used baseline in clinical risk stratification, although its inability to model nonlinear feature interactions limits its expressive power in complex EHR settings.

Linear Regression

For the regression task of predicting time-to-ICU transfer, a standard Linear Regression model was employed. The predicted outcome \hat{y} is given by

$$\hat{y} = \mathbf{w}^\top \mathbf{x} + b, \quad (4.2)$$

with parameters estimated by minimizing the mean squared error loss. While linear regression provides a simple and interpretable baseline, it assumes a linear relationship between clinical variables and the target outcome, an assumption that is often violated in heterogeneous and noisy healthcare data.

Random Forests

Random Forests were included as a nonlinear ensemble-based baseline capable of modeling higher-order feature interactions. A Random Forest consists of an ensemble of decision trees trained on bootstrap samples of the data, where predictions are obtained by aggregating the outputs of individual trees. For classification, majority

voting is used, while regression predictions are averaged across trees. Although Random Forests are robust to noise and do not require feature scaling, they rely on fixed, handcrafted feature representations and do not naturally support multi-task learning, limiting their suitability for jointly modeling correlated clinical outcomes.

Multi-Layer Perceptron

As a fully differentiable nonlinear baseline, a Multi-Layer Perceptron (MLP) was implemented to assess the benefits of end-to-end neural modeling. The MLP consists of multiple fully connected layers with nonlinear activation functions, computing a sequence of transformations of the form

$$\mathbf{h}^{(l+1)} = \phi(\mathbf{W}^{(l)}\mathbf{h}^{(l)} + \mathbf{b}^{(l)}), \quad (4.3)$$

where $\phi(\cdot)$ denotes a nonlinear activation function, and $\mathbf{W}^{(l)}$, $\mathbf{b}^{(l)}$ are the weights and biases of the l -th layer. Separate output heads were used for classification and regression tasks in the multi-task configuration. Despite their expressive capacity, MLPs process input features as an unstructured vector and do not explicitly model feature-wise semantics, which can limit their effectiveness when handling heterogeneous clinical variables with diverse statistical properties.

Model Selection Considerations

The progressive evaluation of linear, ensemble-based, and neural baselines highlights the trade-offs between interpretability, expressive power, and scalability. While simpler models provide transparent decision boundaries, they fail to capture the complex interactions and shared structure inherent in EHR data. These limitations

motivated the adoption of a Transformer-based architecture, which enables structured feature tokenization, flexible representation learning, and principled multi-task optimization within a unified framework.

4.1.2 Multi-task Transformer-Based Clinical State Estimator

Building upon the insights obtained from the comparative analysis of baseline models, a more expressive architecture is required to effectively model the heterogeneous and structured nature of EHR data. In particular, clinical variables differ substantially in scale, statistical properties, and semantic meaning, and their interactions are often nonlinear and task-dependent. To address these challenges, this work adopts a Transformer-based architecture specifically designed for tabular clinical data, which enables feature-wise representation learning while naturally supporting multi-task optimization. By leveraging self-attention mechanisms and structured tokenization, the proposed model is able to capture complex dependencies among input features and to produce informative latent representations that can be shared across multiple prediction objectives.

The Feature Tokenizer module learns to project the categorical features in input \mathbf{x} into embeddings $\mathbf{T} \in R^{k \times d}$, where k is the number of features and d their dimensionality. The embedding for a given feature x_j is computed as follows:

$$\mathbf{T}_j = \mathbf{b}_j + f_j(x_j), \quad f_j : \mathcal{X}_j \rightarrow R^d \quad (4.4)$$

For categorical features, $f_j^{(\text{cat})}$ is implemented as a lookup table $\mathbf{W}_j^{(\text{cat})} \in R^{S_j \times d}$:

$$\mathbf{T}_j^{(\text{cat})} = \mathbf{b}_j^{(\text{cat})} + \mathbf{e}_j^\top \mathbf{W}_j^{(\text{cat})} \in R^d \quad (4.5)$$

where \mathbf{e}_j is a one-hot vector for the corresponding categorical feature. The complete

embedding \mathbf{T} is constructed as:

$$\mathbf{T} = \text{stack} \left[\mathbf{T}_1^{(\text{cat})}, \dots, \mathbf{T}_{k_{\text{cat}}}^{(\text{cat})} \right] \in R^{k \times d} \quad (4.6)$$

Subsequently, a learnable classification token [CLS] (Devlin et al. 2019) is concatenated to the input embeddings \mathbf{T} ; the model uses it during training, to optimize how to summarize the feature embeddings into a single vector. This has proven effective in NLP and, more recently, in tabular tasks (Gorishniy et al. 2022).

$$\mathbf{T}_0 = \text{stack} [[\text{CLS}], \mathbf{T}], \quad \mathbf{T}_i = F_i(\mathbf{T}_{i-1}) \quad (4.7)$$

By stacking a small Transformer encoder (four layers, eight heads), the network can learn higher-order interactions among all categorical tokens. The intuition is that certain combinations of discrete attributes can jointly signal ICU-risk in ways that linear or shallow MLPs cannot easily capture: for example, specific combinations of age groups and abnormal laboratory results may signal early organ impairment or increased physiological stress. The Transformer attention mechanism can flexibly model interactions between all categorical features without explicitly hand-crafting cross-features. Attention layers can attend globally and thus adapt better to heterogeneous categories compared to a standard MLP on concatenated one-hot inputs.

$$\text{MultiHead}(\mathbf{Q}, \mathbf{K}, \mathbf{V}) = \text{Concat} (\text{head}_1, \dots, \text{head}_h) \mathbf{W}^O, \quad (4.8)$$

$$\text{head}_i = \text{Attn} \left(\mathbf{Q}\mathbf{W}_i^Q, \mathbf{K}\mathbf{W}_i^K, \mathbf{V}\mathbf{W}_i^V \right), \quad (4.9)$$

$$\text{Attn}(\mathbf{Q}, \mathbf{K}, \mathbf{V}) = \text{softmax} \left(\frac{\mathbf{Q}\mathbf{K}^\top}{\sqrt{d_e}} \right) \mathbf{V}, \quad (4.10)$$

In this formulation, \mathbf{Q} , \mathbf{K} , and \mathbf{V} denote the query, key, and value matrices obtained through learned linear projections of the input feature embeddings, while d_e denotes the dimensionality of the feature embedding space used throughout the Transformer encoder. Each attention head i applies an independent projection using parameter matrices \mathbf{W}_i^Q , \mathbf{W}_i^K , and \mathbf{W}_i^V , allowing the model to attend to different representation subspaces in parallel. The scaled dot-product attention computes pairwise similarity scores between queries and keys, normalizes them via a softmax function, and uses the resulting weights to aggregate the value vectors. The outputs of all h attention heads are then concatenated and linearly transformed by \mathbf{W}^O to produce the final attention representation.

Finally, the [CLS] token is passed to an MLP block, followed by Layer Normalization and Dropout (0.3), which help mitigate overfitting (particularly important when many categories are imbalanced, such as certain admission types or rare lab flags). This MLP simultaneously outputs a logit for ICU-risk (binary classification) and a scalar prediction of “delay until ICU transfer” (regression). This multi-task formulation encourages the shared latent representation ($z \in \mathbb{R}^{32}$), used as node feature in the second stage, to encode both information. In healthcare settings, predicting both “if” and “when” a patient deteriorates can provide more helpful clinical decision support than a single binary risk score. The loss used to train this network is the sum of the two individual ones:

$$\hat{y}_i^{(\text{Risk})} = \sigma(\mathbf{w}_{\text{Risk}}^\top \mathbf{h}_i + b_{\text{Risk}}) \quad (4.11)$$

$$\hat{y}_i^{(\text{Time})} = \mathbf{w}_{\text{Time}}^\top \mathbf{h}_i + b_{\text{Time}} \quad (4.12)$$

$$\mathcal{L}_{\text{Risk}} = -[y_i \log \hat{y}_i^{(\text{Risk})} + (1 - y_i) \log(1 - \hat{y}_i^{(\text{Risk})})] \quad (4.13)$$

$$\mathcal{L}_{\text{Time}} = \frac{1}{N} \sum_i (\hat{y}_i^{(\text{Time})} - y_i^{(\text{Time})})^2 \quad (4.14)$$

The overall loss is defined as the sum of the two components:

$$\mathcal{L} = \mathcal{L}_{\text{Risk}} + \mathcal{L}_{\text{Time}}. \quad (4.15)$$

The learning process adopts Adam as optimizer, with a learning rate of 10^{-4} , and a mechanism of early stopping based on the validation loss. In practice, this results in models that converge reliably and produce embeddings that reflect clinically meaningful patterns associated with elevated risk. From a clinical perspective, the Stage 1 embedding can be interpreted as a compact representation of the admission's initial severity. It synthesizes heterogeneous information sources into a format that is both machine-readable and clinically informative. From a modeling perspective, it provides a stable foundation for the construction of patient histories and relational structures, which are essential components of the graph-based modeling pipeline developed in the subsequent sections.

4.2 Stage 2

4.2.1 Multi-edge Graph Construction

A graph is a fundamental mathematical structure that models relationships between entities. Formally, a graph is defined as an ordered pair $G = (V, E)$, where $V = \{v_1, v_2, \dots, v_N\}$ is a finite set of nodes (or vertices) representing entities and $E \subseteq V \times V$ is a set of edges that represent pairwise relationships or interactions between them. An edge $e_{ij} = (v_i, v_j) \in E$ indicates a connection between nodes v_i and v_j . Graphs can be undirected, where $(v_i, v_j) = (v_j, v_i)$, or directed, where edges have an orientation. In weighted graphs, a function $w : E \rightarrow \mathbb{R}$ assigns a weight to each edge, encoding the strength or importance of the connection. A graph can also be represented algebraically through an adjacency matrix $A \in \mathbb{R}^{N \times N}$, where each entry A_{ij} denotes the weight of the edge between v_i and v_j (or 0 if no edge exists). This formalism provides the foundation for many algorithms and models in network analysis and Graph Neural Networks (GNNs).

In this work, a multi-edge admission-centric graph (Figure 4.2) is built to represent each hospital admission as a node, whose features are composed of admission data, latent representation (z) extracted from Stage-1, ICU Risk, Time to ICU, and Vitals (if the admission was in ICU). Nodes are connected through three edge families: clinical similarity, ICU transfer risk, temporal links among different admissions of the same patient.

The feature-space similarity edges are designed according to the K-Nearest Neighbors algorithm applied to the joint space of the node features and connect the admission nodes between each other, enforcing the idea that patients with similar

early-stage features share important information. Among the values tested ($k = 5$, $k = 15$, $k = 30$), the most consistent improvements were obtained with $k = 5$, which encouraged more diverse local structures and resulted in a more effective learning process.

The ICU transfer risk edges connect each admission node to a single Dummy Node and are weighted by the ICU Risk, calculated from Stage, implementing a star topology that aggregates global ICU knowledge. The purpose of the dummy node is to pool information about all admissions, handling scalability and oversmoothing issues in graph structure learning (Liu et al. 2022).

Finally, the temporal edges link all admissions of the same patient during the years, capturing longitudinal progression. In detail, a temporal link starting in node_i and arriving in node_j is weighted by the following formula:

$$w_{ij} = \frac{1}{1 + |\text{year}_i - \text{year}_j|} \quad (4.16)$$

where $\text{year}_i < \text{year}_j$. By doing so, the Stage 2 network can use the past history when predicting current outcomes (Gupta et al. 2025).

4.2.2 Multi-layer GNN

The generated graph is then processed by a GNN pipeline that consists of a GCN / R-GCN, a GATv2, and a GraphSAGE, followed by separated linear heads for each task. This multi-layer architecture combines different aggregation and message-passing mechanisms to capture complementary relational patterns across hospital stays.

A first GCNConv layer incorporates the local neighborhood structure and projects

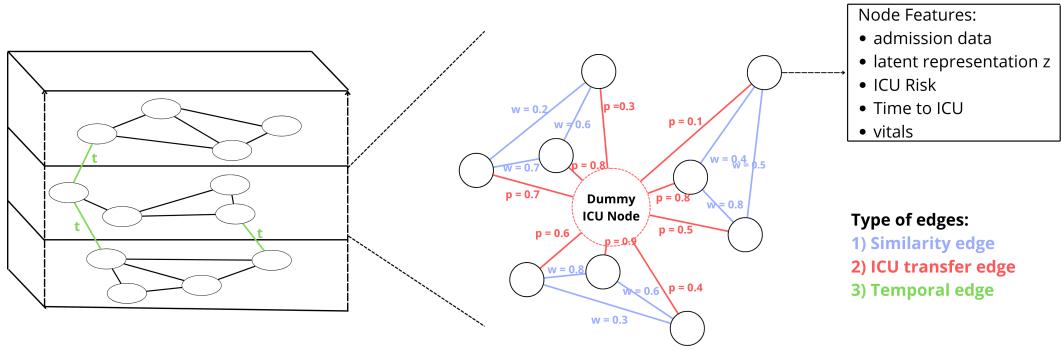


Figure 4.2. Admission-centric graph construction: each node represents an admission, characterized by admission data, latent representation, ICU risk, time to ICU and ICU Vitals; nodes are linked to each other through weighted similarity edges, ICU transfer edges (to a dummy node) and within-subject edges.

the raw node features into a hidden representation. Let $H^{(0)} \in R^{N \times d_0}$ be the matrix of initial node features, where N is the number of nodes and d_0 their dimensionality, and $A \in R^{N \times N}$ the weighted adjacency matrix; this layer applies:

$$H^{(1)} = \sigma(\tilde{D}^{-1/2} \tilde{A} \tilde{D}^{-1/2} H^{(0)} W^{(0)}) \quad (4.17)$$

where $\tilde{A} = A + I$, $\tilde{D}_{ii} = \sum_j \tilde{A}_{ij}$, $\sigma(\cdot)$ is the ReLU activation function, and $W^{(0)} \in R^{d_0 \times d_1}$. This architecture is simple and deterministic, accounts for edge weights during aggregation and is efficient on CPU with sparse matrices, but it does; however, it does not capture edge heterogeneity.

To address this problem, an alternative design uses an R-GCNConv (Schlichtkrull et al. 2018) as first layer, to model heterogeneous edge relations explicitly. It uses relation-specific transformation matrices $\{W_r\}$ and aggregates messages across different edge types as:

$$h_i^{(1_r)} = \sigma \left(\sum_{r \in \mathcal{R}} \sum_{j \in \mathcal{N}_i^r} \frac{1}{c_{i,r}} W_r h_j^{(1)} + W_0 h_i^{(1)} \right) \quad (4.18)$$

where \mathcal{R} denotes the set of relations and $c_{i,r}$ is a normalization constant. This allows the network to learn different propagation patterns for different clinical interactions while controlling parameter growth through basis decomposition.

Subsequently, a second **GATv2Conv** layer (Brody et al. 2022) applies adaptive multi-head attention to dynamically weigh the relative importance of neighboring nodes. For each node, attention coefficients are computed between neighbors and aggregated through a weighted average; for each edge (i, j) :

$$e_{ij} = \text{LeakyReLU}\left(\mathbf{a}^\top [\mathbf{W}^{(1)}\mathbf{h}_i^{(1)} \parallel \mathbf{W}^{(1)}\mathbf{h}_j^{(1)}]\right), \quad (4.19a)$$

$$\alpha_{ij} = \frac{\exp(e_{ij})}{\sum_{k \in \mathcal{N}(i)} \exp(e_{ik})}, \quad (4.19b)$$

$$\mathbf{h}_i^{(2)} = \sigma\left(\sum_{j \in \mathcal{N}(i)} \alpha_{ij} \mathbf{W}^{(1)}\mathbf{h}_j^{(1)}\right). \quad (4.19c)$$

In this way, this layer learns a different importance for each neighbor, improving expressiveness compared to a GCN at the cost of a bit higher computational consumption (attention on each edge).

Then, a third and last **SAGEConv** layer aggregates information from multi-hop neighbors and learns node-specific aggregation functions (e.g. *mean*, *max-pooling*, *LSTM*), enriching the contextual representation over neighbors for each node.

$$\mathbf{m}_i = \text{AGG}(\{\mathbf{h}_j^{(2)} : j \in \mathcal{N}(i)\}) \quad (4.20a)$$

$$\mathbf{h}_i^{(3)} = \sigma(\mathbf{W}^{(2)} [\mathbf{h}_i^{(2)} \parallel \mathbf{m}_i]) \quad (4.20b)$$

It is *inductive*, generating embeddings for new nodes using only their features, without requiring a global re-computation (scalable on large graphs through neighbor sampling). The complexity per layer is $\mathcal{O}(|E|)$, but is still efficient.

Finally, the embeddings from all layers $h_i^{(j)} \in R^{d_j}$ are concatenated using the Jumping Knowledge mechanism (mode=`cat`) to balance early and late feature contributions:

$$\mathbf{h}_i^{\text{JK}} = [\mathbf{h}_i^{(0)} \| \mathbf{h}_i^{(1)} \| \dots \| \mathbf{h}_i^{(3)}] \quad (4.21)$$

This “skip connection” style aggregation was introduced by Xu et al. (2018), finding that combining multiple types of layer (in particular GCN, GAT and SAGE) leads to a more stable training and improves accuracy on sparse or relational healthcare graphs.

Then, the resulting embedding is fed to three separate linear heads: **Mortality Risk, Length of ICU Stay, and Discharge Location.**

$$\hat{y}_i^{(\text{mort})} = \sigma(\mathbf{w}_{\text{mort}}^\top \mathbf{h}_i^{\text{JK}} + b_{\text{mort}}), \quad (4.22a)$$

$$\hat{y}_i^{(\text{hours})} = \mathbf{w}_{\text{hours}}^\top \mathbf{h}_i^{\text{JK}} + b_{\text{hours}}, \quad (4.22b)$$

$$\hat{y}_i^{(\text{disc})} = \text{softmax}(\mathbf{W}_{\text{disc}} \mathbf{h}_i^{\text{JK}} + \mathbf{b}_{\text{disc}}), \quad (4.22c)$$

$$\mathcal{L}_{\text{mort}} = -[y_i \log \hat{y}_i^{(\text{mort})} + (1 - y_i) \log(1 - \hat{y}_i^{(\text{mort})})], \quad (4.22d)$$

$$\mathcal{L}_{\text{hours}} = \frac{1}{N} \sum_i (\hat{y}_i^{(\text{hours})} - y_i^{(\text{hours})})^2, \quad (4.22e)$$

$$\mathcal{L}_{\text{disc}} = - \sum_{c=1}^4 y_{i,c}^{(\text{disc})} \log \hat{y}_{i,c}^{(\text{disc})}. \quad (4.22f)$$

The overall loss is a (weighted) sum of the three individual ones:

$$\mathcal{L} = \lambda_{\text{mort}} \mathcal{L}_{\text{mort}} + \lambda_{\text{hours}} \mathcal{L}_{\text{hours}} + \lambda_{\text{disc}} \mathcal{L}_{\text{disc}}. \quad (4.23)$$

This joint training strategy encourages the network to produce useful embeddings for all relevant clinical tasks at once, allowing to learn common representations useful for multiple tasks and to reduce the total number of parameters.

Furthermore, during training, Dynamic Edge Weighting via MLP is applied to recalculate weights based on the concatenated hidden states of source/destination nodes and the previous edge weight: in practice, the GNN learns to emphasize or de-emphasize certain connections dynamically.

$$\mathbf{e}_{ij} = [\mathbf{h}_i^{(l)} \parallel \mathbf{h}_j^{(l)} \parallel w_{ij}^{(0)}], \quad (4.24a)$$

$$w_{ij}^{(l)} = \text{MLP}_{\text{edge}}(\mathbf{e}_{ij}), \quad (4.24b)$$

$$\mathbf{m}_i^{(l+1)} = \sum_{j \in \mathcal{N}(i)} w_{ij}^{(l)} \cdot \mathbf{h}_j^{(l)}. \quad (4.24c)$$

Edges are also randomly dropped during training (with `dropedge_rate`= 0.2), to avoid over-reliance on a few strong connections and to reduce overfitting. DropEdge Regularization was introduced by Rong et al. (2020) and has since become a common practice in graph learning.

The last methodological choice encountered in training the graph concerns the trade-off between full-graph optimization and mini-batch graph training. In a full-graph setting, all admissions are represented as nodes within a single global graph whose structure is precomputed and remains fixed throughout the entire optimization process, while mini-batch training constructs a local graph at each iteration, induced exclusively by the subset of admissions in the current batch, resulting in adjacency structures that vary across training steps.

Full-graph optimization may appear more powerful due to its ability to preserve a coherent global relational structure, but requires the complete graph to be pre-computed, stored in memory, and repeatedly processed during training, leading to substantial memory consumption and limited scalability as size grows. In contrast, mini-batch training avoids these constraints by operating on smaller, dynamically

constructed subgraphs, resulting in reduced memory overhead and lower computational cost per iteration. Furthermore, gradients computed over smaller and more diverse subgraphs tend to explore the loss landscape more effectively, leading to better optimization, faster convergence, and improved predictive performance. Training a fixed global graph repeatedly propagates information through the same neighborhood, which may not be representative of the entire population: this static structure promotes oversmoothing, reducing the model’s ability to discriminate small but clinically significant differences. Mini-batch graph training, on the other hand, introduces a controlled and beneficial form of stochasticity, reconstructing the graph at each iteration and continuously exposing the model to diverse local neighborhoods. This variability mitigates overfitting to specific connections and improves generalization. For this reason and considering the significant computational advantages, the mini-batch configuration (with batch-size = 32, chosen against 64 and 256) was adopted as the definitive training strategy for Stage 2.

Chapter 5

Results

This chapter presents the evaluation of the proposed two-stage predictive framework. The experimental analysis is structured to assess both the individual contributions of each stage and their combined effect on clinical outcome prediction. In particular, the first part of the chapter focuses on the comparison of alternative modeling approaches for ICU risk estimation and time-to-ICU prediction, while the second part evaluates the graph-based model through ablation studies and comparative benchmarks. Beyond raw performance scores, the analysis aims to highlight the impact of architectural choices, training strategies, and data preprocessing steps on model stability and generalization. The results are reported using clinically meaningful metrics and are discussed in relation to prior work on MIMIC to contextualize the effectiveness of the proposed approach.

5.1 Metrics

Model performance is evaluated using a comprehensive set of metrics selected to capture both statistical reliability and clinical relevance across classification and regression tasks. Given the heterogeneous nature of the prediction objectives, different evaluation criteria are adopted for binary outcomes, including ICU risk and in-hospital mortality prediction, and continuous targets, such as time-to-ICU and ICU length-of-stay prediction, ensuring that each task is assessed using metrics aligned with its clinical interpretation and practical use.

Additionally, for prolonged ICU stays, binary AUC metrics at clinically meaningful thresholds (e.g., greater than 3 or 7 days) are included to evaluate the model's ability to identify patients at risk of extended critical care. Together, these metrics provide a balanced and task-appropriate evaluation of predictive accuracy, robustness, and clinical utility.

Binary Classification Metrics For binary classification tasks, including ICU admission risk and in-hospital mortality prediction, model discrimination is primarily assessed using the Area Under the Receiver Operating Characteristic Curve (AUC). The AUC measures the probability that the model assigns a higher risk score to a randomly selected positive case than to a randomly selected negative one, and is independent of any fixed classification threshold. Formally, the AUC can be expressed as:

$$\text{AUC} = \mathbb{P}(\hat{y}^+ > \hat{y}^-), \quad (5.1)$$

where \hat{y}^+ and \hat{y}^- denote the predicted scores for positive and negative samples, respectively. This property makes AUC particularly suitable for imbalanced clinical datasets, where the choice of a single operating threshold may be arbitrary or task-dependent.

In addition to AUC, accuracy is reported as an intuitive measure of overall correctness:

$$\text{Accuracy} = \frac{TP + TN}{TP + TN + FP + FN}, \quad (5.2)$$

where TP , TN , FP , and FN represent the number of true positives, true negatives, false positives, and false negatives, respectively. While accuracy provides an easily interpretable summary statistic, it is interpreted with caution due to its sensitivity to class imbalance, which is common in clinical prediction settings.

Regression Metrics For regression tasks, such as predicting the time to ICU admission and the duration of ICU stay, performance is evaluated using the Mean Absolute Error (MAE) and the Root Mean Squared Error (RMSE). The MAE quantifies the average magnitude of prediction errors in the same units as the target variable, providing a direct and clinically interpretable measure:

$$\text{MAE} = \frac{1}{N} \sum_{i=1}^N |y_i - \hat{y}_i|, \quad (5.3)$$

where y_i and \hat{y}_i denote the true and predicted values for sample i , respectively, and N is the number of observations.

The RMSE is defined as:

$$\text{RMSE} = \sqrt{\frac{1}{N} \sum_{i=1}^N (y_i - \hat{y}_i)^2}, \quad (5.4)$$

and places greater emphasis on large deviations by squaring the error term. This makes RMSE particularly sensitive to extreme prediction errors, which are clinically relevant in the context of prolonged ICU stays or delayed ICU transfers.

Threshold-Based Risk Evaluation. To further assess clinical utility in the context of prolonged critical care, additional binary classification metrics are computed by thresholding continuous ICU length-of-stay predictions at clinically meaningful cutoffs (e.g., ICU stay longer than 3 or 7 days). The resulting binary outcomes are evaluated using AUC, allowing the assessment of the model’s ability to identify patients at risk of extended ICU utilization. This analysis bridges continuous prediction accuracy and operational decision-making, where binary risk stratification is often required.

Overall, the combination of threshold-independent discrimination metrics, error-based regression measures, and clinically grounded binary evaluations provides a balanced and task-appropriate assessment of predictive performance, robustness, and potential clinical impact.

5.2 Stage 1 Results Comparison

Tables 5.1 and 5.2 summarize the performance of the five different modeling approaches implemented for the two ICU-prediction tasks. Overall, we can see that traditional methods, such as LogReg and Random Forests, yield reasonable performances on ICU risk prediction (AUC 0.75, Acc 0.70) and timing errors around 45 h (MAE); we can also notice that the usage of an MLP, in particular with the addition of multi-task learning, provides modest gains (AUC 0.76, Acc 0.71,

Table 5.1. ICU Risk prediction: Performance Summary across various classical ML and DL approaches

Model	AUC	Accuracy
Logistic Regression	0.751	0.701
Random Forest	0.756	0.707
MLP (single-task)	0.757	0.707
MLP (multi-task)	0.762	0.710
FT-Transformer (multi-task)	0.770	0.710

MAE 40 h). Finally, the Transformer-based multi-task model further improves discrimination (AUC 0.77, confusion matrix in Table 5.3) and timing accuracy (MAE 35 h), suggesting that its richer feature interactions can better capture both the classification and temporal aspects of ICU risk .

Compared to recent studies performed on the MIMIC-IV dataset, there are no benchmarks on ICU risk and delay, but previous and similar works on different datasets reported an ICU-risk AUC of around 0.75-0.80 using LSTM-based estimators or models using embeddings of categorical features with attention.

5.3 Stage 2 Layer Ablation Study

Table 5.4 summarizes the impact of different GNN configurations in the Stage 2 architecture. The baseline combination GCN + GAT + SAGE already achieves strong overall performance in both classification and regression tasks. The replacement of the GCN layer with a Relational Graph Convolution further improves the results in

Table 5.2. Time to ICU Regression: Performance Summary across various classical ML and DL approaches

Model	RMSE [h]	MAE [h]
Linear Regression	90	45
Random Forest	92	45
MLP (single-task)	92	45
MLP (multi-task)	90	40
FT-Transformer (multi-task)	92	35

Table 5.3. Confusion Matrix for ICU Risk Prediction (threshold = 0.5): true positives (TP), false positives (FP), false negatives (FN), and true negatives (TN) are reported.

Actual / Predicted	ICU	Not ICU
ICU	3 730 (TP)	4 564 (FN)
Not ICU	1 584 (FP)	11 220 (TN)

all metrics, with the entire R-GCN + GAT + SAGE model achieving the best overall performance (AUC 0.909, RMSE 54.6). This indicates that explicitly modeling edge types and relational dependencies enhances representation learning and stability during message passing.

Monolayer variants show slightly degraded results, confirming that multi-layer aggregation provides complementary information. In particular, the R-GCN variants produce better discrimination in long ICU-stays (AUC 0.86 for ICU duration > 3 days), suggesting improved temporal and relational reasoning across patient

Table 5.4. Ablation study on different GNN configurations for Stage 2. Metrics include AUC and Accuracy for Mortality Risk, RMSE and MAE for ICU Duration, Accuracy for Discharge Location, and AUC for ICU duration > 3 days and > 7 days.

Model	AUC(Mort)	Acc(Mort)	RMSE(h)	MAE(h)	Acc(DiscLoc)	AUC(>3d)	AUC(>7d)
Monolayer GCN	0.894	0.961	57.5	37.6	0.740	0.841	0.876
Monolayer GAT	0.902	0.962	55.7	37.0	0.741	0.848	0.888
Monolayer SAGE	0.904	0.961	57.0	37.1	0.739	0.843	0.875
Monolayer R-GCN	0.907	0.962	54.7	35.6	0.741	0.859	0.898
GCN + GAT	0.896	0.961	56.9	37.9	0.739	0.842	0.883
GCN + SAGE	0.898	0.962	56.4	35.5	0.742	0.848	0.883
GAT + SAGE	0.905	0.961	56.7	36.6	0.738	0.845	0.879
GCN + GAT + SAGE	0.903	0.962	55.6	36.7	0.740	0.850	0.890
R-GCN + GAT + SAGE	0.909	0.963	54.6	35.4	0.740	0.856	0.900

trajectories.

5.4 Stage 2 Results Comparison

Table 5.5 summarizes performance across three different configurations using the R-GCN + GAT + SAGE architecture. The first two columns from the left are the results obtained with/without outliers in the case in which the ICU Vitals are assigned with an ICU Risk > 0.5 from Stage 1; the third column from the left contains the results obtained when Vitals are assigned to all ICU admissions using the Ground Truth (GT) of the label 'was in ICU', removing the potential noise from Stage 1: this can be considered reasonable, knowing that vitals are available only if a patient has been in an ICU department and this fact, in a real-word scenario, may depend just in a first instance on the prediction from Stage 1 and more likely on the actual clinical condition of the patient. We can consider this solution, and the

Table 5.5. Performance Summary Across Experimental Conditions: before and after outliers removal and with the assignment of ICU Vitals using the ground truth of 'was in ICU'.

Metric	Outliers	No Outliers	GT Vitals
Mortality AUC	0.854	0.840	0.909
Mortality Acc	0.956	0.957	0.963
ICU RMSE (h)	120	63	55
ICU MAE (h)	72	42	35
Discharge Acc	0.722	0.722	0.740

corresponding results, as an "upper bound" for Stage 2.

Compared to the performance without outliers removal (AUC 0.8541, Accuracy 0.9562), after this cleaning step, the AUC decreased slightly (0.840), while the accuracy remained unchanged or slightly improved (0.9575). Since approximately 2100 admissions were removed (some of which probably included patients with extremely long ICU stays and atypical clinical profiles), this slight drop in AUC is expected: the model now mostly encounters admissions with more typical outcomes. However, the accuracy remains high, as the removal of outliers has little effect on the many "easy" cases of survival or non-survival. The impact of outlier removal is most evident in the ICU-Duration regression: RMSE was halved (from 120 to 63 hours) and MAE significantly decreased (from 72 to 42 hours).

In the last case, the graph-based mortality risk predictor achieved an AUC of 0.909 and an Accuracy of 0.963, surpassing the best publicly reported MIMIC-IV benchmarks (Table 5.6): mortality risk AUC around 0.90, obtained using a Bert

Table 5.6. Performance comparison with related works on MIMIC-III/IV for mortality risk prediction

Work	Model	AUC
Rocheteau et al. (2021)	LSTM	0.83
	LSTM+GNN	0.86
Bui et al. (2024)	XGBoost	0.87
	LSTM	0.83
van de Water et al. (2025)	GRU	0.87
Daphne et al. (2025)	Transformer+GNN	0.90
This Work	Transformer+GNN	0.91

Transformer for textual embeddings followed by a GNN (Daphne et al. 2025). Instead, the performance for the ICU-duration regression (MAE 35 h, RMSE 54 h) is slightly higher than the 37-40 h RMSE range reported by Rocheteau et al. (2021), using an LSTM + GNN. Finally, when considering the AUC for ICU duration > 3 days and > 7 days (respectively 0.84 and 0.90 with the LSTM + GNN by Maroudis et al. 2024), it achieves an AUC of 0.86 and 0.90, respectively. This indicates broadly comparable performance and demonstrates that, once true ICU admissions are known, the GNN can achieve nearly optimal predictive performance.

Figure 5.1 and tables 5.7 and 5.8 report some interesting and promising results obtained during the experiments.

The first provides insight into the optimization behavior of the graph-based



Figure 5.1. Training and validation loss across epochs for the GNN (in this case, in particular, R-GCN+GAT+SAGE). The validation loss stabilizes around epoch 40, where early stopping is applied.

Table 5.7. Confusion Matrix for In-Hospital Mortality Prediction (threshold = 0.5)

Actual / Predicted	Dead	Not Dead
Dead	498 (TP)	627 (FN)
Not Dead	170 (FP)	19 803 (TN)

model (R-GCN+GAT+SAGE): the training and validation loss curves show a stable and well-aligned trajectory, indicating convergence without overfitting. In particular, the validation loss encounters a plateau around epoch 40, at which point early stopping is triggered, suggesting that the model reaches its optimal generalization regime within a limited number of training iterations (50).

Then, the confusion matrix is provided for in-hospital mortality prediction using a decision threshold of 0.5. The model correctly identifies a substantial proportion

Table 5.8. ICU-Duration Prediction Error

Error Interval	Count	% of ICU	Cumulative %
≤ 6 h	1,234	14.88%	14.88%
6–12 h	1,175	14.17%	29.05%
12–24 h	1,801	21.71%	50.76%
24–36 h	1,206	14.54%	65.30%
36–48 h	868	10.47%	75.77%
48–72 h	876	10.56%	86.33%
72–96 h	446	5.38%	91.71%
96–120 h	260	3.13%	94.84%
≥ 120 h	428	5.16%	100.00%
Total	8,294	100.00%	100.00%

of non-survivor cases, achieving a true positive count of 498, while maintaining a relatively low number of false positives (170) among the much larger population of surviving patients. The resulting high true negative count reflects strong specificity, which is particularly important in clinical settings to avoid unnecessary alarms or interventions. At the same time, the presence of false negatives highlights the intrinsic difficulty of mortality prediction in heterogeneous patient populations and motivates the use of threshold-independent metrics, such as AUC, for a more comprehensive assessment of discriminative performance.

Finally, the error distribution for ICU length-of-stay prediction is reported to illustrate the practical reliability of the proposed framework: approximately half of the ICU stays are predicted within a 24-hour error margin, and over 75% fall within a 48-hour window. This concentration of errors in lower ranges indicates that the model is generally able to capture the temporal dynamics governing ICU utilization.

Larger errors are primarily associated with prolonged and atypical ICU trajectories, which are inherently harder to predict due to exogenous clinical events and evolving patient conditions.

5.5 Discussion

Overall, these experimental results demonstrate the effectiveness of the proposed architecture in capturing both admission-level risk signals and population-level relational patterns. The progression from classical linear and ensemble baselines to deep multi-task and Transformer-based models in Stage 1 highlights the importance of modeling feature interactions and shared representations in heterogeneous EHR data. The gains achieved by the FT-Transformer confirm its ability to leverage structured categorical inputs while producing informative latent representations for downstream tasks.

In Stage 2, the incorporation of graph-based reasoning further improves predictive performance, particularly when relational information is explicitly modeled through heterogeneous edges and relational convolutions. Ablation studies confirm that combining different GNN layers enhances stability and expressiveness, while mini-batch graph training provides both regularization benefits and improved computational scalability. When evaluated against existing benchmarks, the proposed approach achieves competitive or superior performance across mortality risk, ICU duration, and discharge prediction tasks.

5.6 Interpretability

Interpretability is fundamental in clinical decision support systems to ensure that model predictions can be trusted and validated by healthcare professionals. In this two-stage pipeline, the output of the GNN combines complex interactions across categorical embeddings, latent clinical state, and relational edges (similarity, ICU transfers, temporal history). To shed light on “why” the model predicts a high mortality risk or a long ICU-stay for a specific patient, two different approaches are implemented.

The first is based on a simple feature perturbation mechanism (for each input dimension of the selected admission node, the features are zeroed-out, observing how much the mortality risk or the ICU-duration changes; the resulting importance scores identify which inputs drive the final prediction (Table 5.9)). This straightforward perturbation technique provides an intuitive and model-agnostic way to rank features by their influence, enabling clinicians to verify that critical variables (e.g. age group, specific lab flags or prior ICU risk) align with medical knowledge when the model classifies a patient as high-risk.

The second and more advanced method is based on the GNNExplainer (Ying et al., NeurIPS 2019): it identifies the most influential subgraph structure and node features that contribute to a given prediction by optimizing a mutual information objective between the full model prediction and the explanation subgraph. Specifically, it learns a soft mask over edges and features to highlight the minimal subset that preserves the model’s output for a target node or graph. In addition to the previous and simpler approach, this allows visualization of clinically relevant relations, such as which node

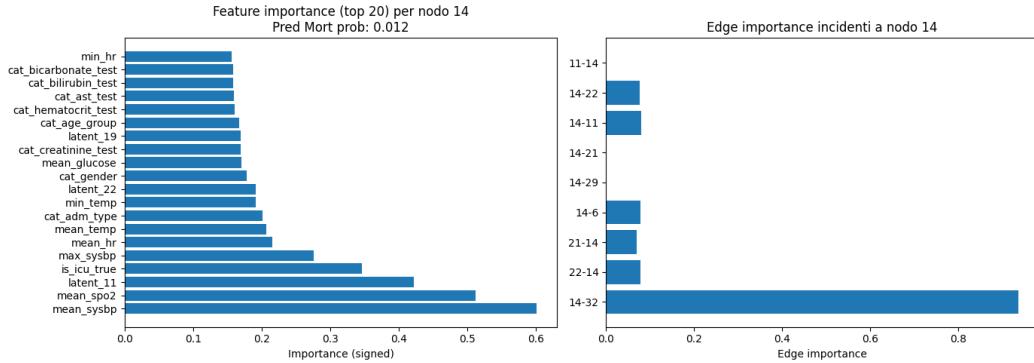


Figure 5.2. Example of Feature and Edge Importance produced by Explainer (GNNExplainerAlgo by torch geometric).

connections drive a particular risk prediction, thus improving transparency and trust in the model's decisions (Fig. 5.2).

Overall, the results obtained during this interpretability analysis confirm that mortality prediction is driven by a combination of physiologically meaningful signals (dominated by vital signs), latent representations of admission-related information, and a contribution of the most similar neighbors in the graph. This provides an intuitive and clinically meaningful explanation of the behavior of the model, strengthening the reliability of the predictions for downstream decision-support applications in real word scenarios.

Table 5.9. Feature Importance, ordered by magnitude, for Mortality Prediction Task (True Mortality, Predicted Probability = 0.873).

Feature	Importance	Feature	Importance
min_sysbp	0.789883	max_temp	0.001556
latent_25	0.752459	max_sysbp	0.001142
age_group	0.429172	max_glucose	-0.001022
latent_10	0.396917	max_spo2	-0.000947
adm_type	0.208608	max_hr	-0.000278
mean_temp	0.116018	gender	0.000000
mean_sysbp	0.114884	adm_loc	0.000000
latent_6	-0.087140	bicarbonate_test	0.000000
min_rr	0.086561	creatinine_test	0.000000
mean_hr	-0.064819	glucose_test	0.000000
latent_28	0.060689	ast_test	0.000000
min_temp	-0.043527	bilirubin_test	0.000000
latent_23	0.042981	hematocrit_test	0.000000
time_to_icu	0.041880	latent_0	0.000000
mean_rr	-0.040183	latent_2	0.000000
min_spo2	-0.038642	latent_4	0.000000
is_icu_pred	-0.037838	latent_5	0.000000
latent_29	0.037322	latent_7	0.000000
latent_21	-0.026424	latent_9	0.000000
min_hr	0.024553	latent_11	0.000000
mean_glucose	-0.019785	latent_13	0.000000
latent_1	0.018036	latent_14	0.000000
latent_12	-0.017621	latent_15	0.000000
latent_3	0.010438	latent_16	0.000000
latent_31	0.009088	latent_17	0.000000
latent_30	0.007445	latent_18	0.000000
latent_20	-0.006707	latent_19	0.000000
latent_8	-0.006500	latent_22	0.000000
max_rr	-0.004530	latent_24	0.000000
mean_spo2	0.004234	latent_26	0.000000
min_glucose	-0.003295	latent_27	0.000000

Chapter 6

Conclusions

This thesis presented a modular two-stage deep learning framework designed to address the challenges of predictive modeling from structured EHR, with a particular focus on capturing both admission-level characteristics and population-level relational patterns. By combining Transformer-based representation learning with GNN reasoning, the proposed approach integrates complementary modeling paradigms within a unified and extensible pipeline, evaluated on the large-scale MIMIC-IV clinical database.

In the first stage, a Transformer-based encoder processes raw admission-level features and produces compact latent embeddings while jointly estimating ICU transfer risk and time to ICU. Through a comparison with classical linear, ensemble-based, and shallow neural baselines, this stage demonstrated the benefits of structured feature tokenization and multi-task supervision, achieving consistent performance improvements while maintaining computational efficiency. Although the numerical gains over strong baselines are moderate, the resulting latent representations proved

to be highly informative for downstream relational modeling.

The second stage leverages these embeddings within a heterogeneous admission-centric hypergraph that explicitly models relationships through similarity, ICU-transfer, and temporal edges. By combining multiple graph convolutional operators in this multi-edge setting, the model captures complementary relational signals and enables joint prediction of in-hospital mortality, ICU length of stay, and discharge destination. Empirical evaluation demonstrates competitive state-of-the-art performance on MIMIC-IV, achieving an AUC of 0.91 for mortality prediction, a MAE of 35 hours for ICU length-of-stay estimation, and an accuracy of 0.74 for discharge location classification.

From a practical perspective, the proposed architecture exhibits favorable computational characteristics: inference requires approximately 1 second for the Transformer-based first stage and 3 seconds for the graph-based second stage when executed on a standard AMD Ryzen 5 7600X CPU, while achieving real-time performance on standard GPUs. This efficiency, combined with the modular design of the pipeline, supports the potential deployment in near-real-time clinical decision support systems without imposing excessive computational overhead.

Beyond predictive accuracy, the framework incorporates an explicit interpretability component through feature importance analysis. This mechanism enables clinicians to identify which clinical variables most strongly influence individual predictions, improving transparency in model outputs, essential for clinical adoption into existing hospital workflows.

Despite these strengths, some limitations remain. The current implementation relies primarily on structured tabular data and does not fully exploit unstructured

clinical information. In real-world settings, free-text diagnoses, clinical notes, and symptom descriptions provide valuable contextual information that is not available in MIMIC-IV or is only sparsely represented. Future extensions could integrate additional modalities, for instance by incorporating Bert Transformer for NLP to encode clinical text and either enriching node features or introducing dedicated node types within a fully heterogeneous graph formulation.

Additional research directions include refining edge construction strategies to better capture dynamic clinical trajectories, exploring temporal or evolving graph architectures, and scaling the framework to larger and more diverse healthcare datasets.

In conclusion, the proposed two-stage multi-edge graph neural network framework offers a flexible and extensible solution for modeling complex clinical data by jointly leveraging intra-admission features and inter-admission relationships. By integrating temporal modeling, relational reasoning, and multi-task learning within a computationally efficient architecture, this work contributes a promising foundation for future research and practical applications in clinical decision support and healthcare analytics.

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