

# Hand Orthosis for Living Activities

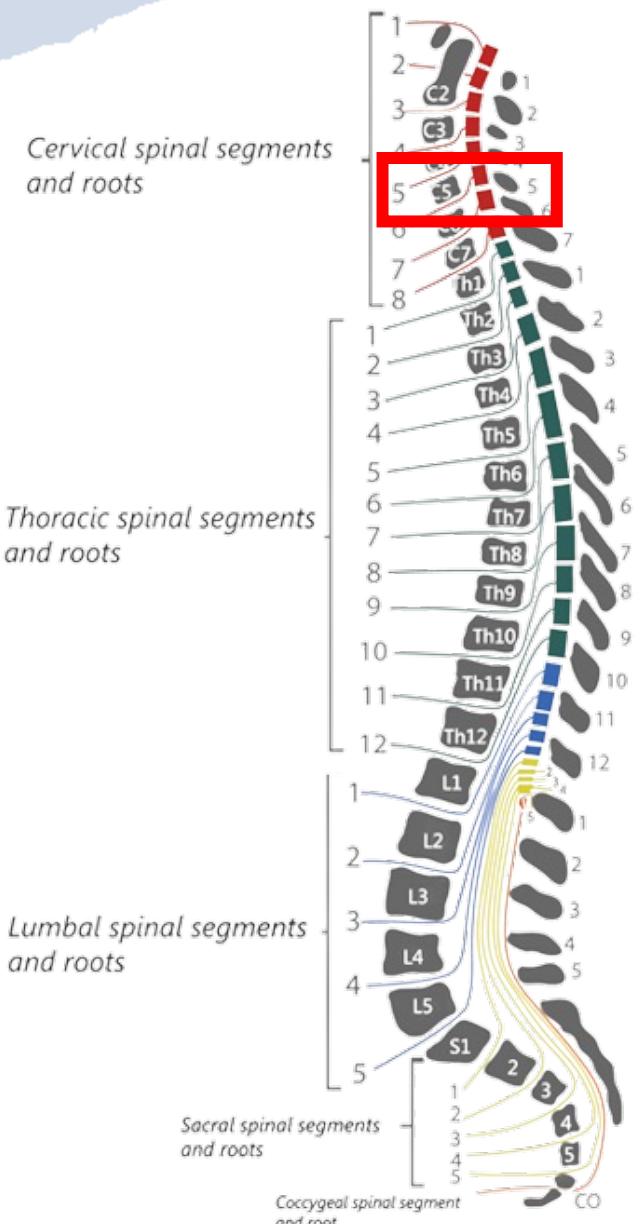
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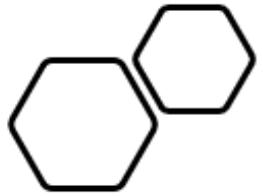
Group 5



# Problem Statement

- **Spinal Cord Injury (SCI)** causes profound life changes, especially at the **C5 level** [1]
  - Patients at an American Spinal Injury Association (ASIA) C level retain some functionality below the injury [2]
- Impairments in **upper limb functionality** cause difficulty in completing Activities of Daily Living (ADLs) [1,3]
  - This compromises patient independence





## The Market Gap

Current solutions offer effective movement,  
but **require assistance and are time-  
consuming to don/doff**



*"If there's a device I need a care attendant  
to put on, I don't ever foresee using it."*

- Andrew McPherson, C5/C6 Spinal Cord Injury Patient [6]

# Situation Impact Statement

Design a device, to be used at home by C5 SCI patients classified at a C level on the ASIA scale, that allows for **independent donning, doffing, and the performance of ADLs associated with transverse volar grips (TVGs) and lateral pinches (LPs)**.



2. Lateral Pinch



6. Transverse Volar Grip

*Targeted Grips [7]*

# Project Scope and Objectives



Create a **high-fidelity prototype** that supports user independence and safely allows for the user to complete the desired hand grasps

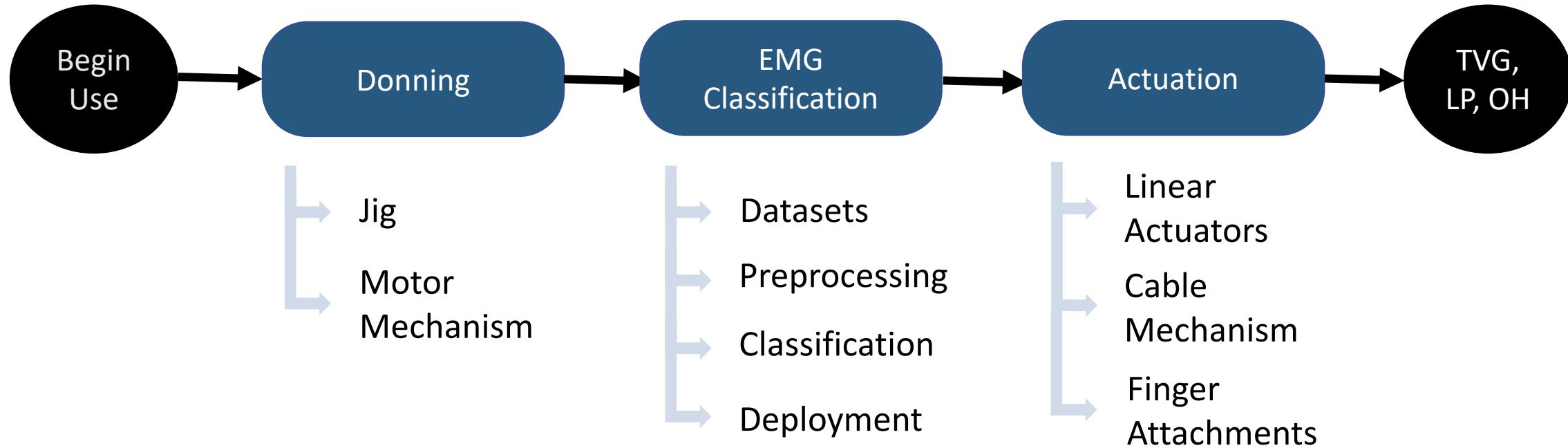


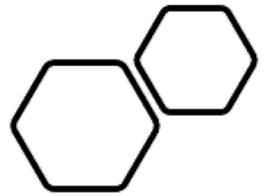
Develop a **highly specific classification algorithm** that leverages electromyography (EMG) signals to determine grasp intention



**Conduct user testing** with an SCI patient to assess the ease of donning/doffing and overall functionality

# High Level Overview

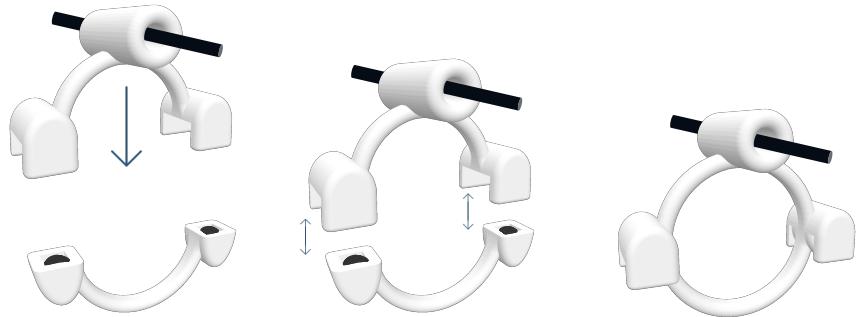


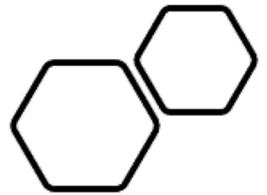


# Donning/Doffing – Jig

Goal: Open and position user's hand

- Curved edge and grooves facilitate opening and alignment
- Indents hold and position the bottom half of the finger attachments

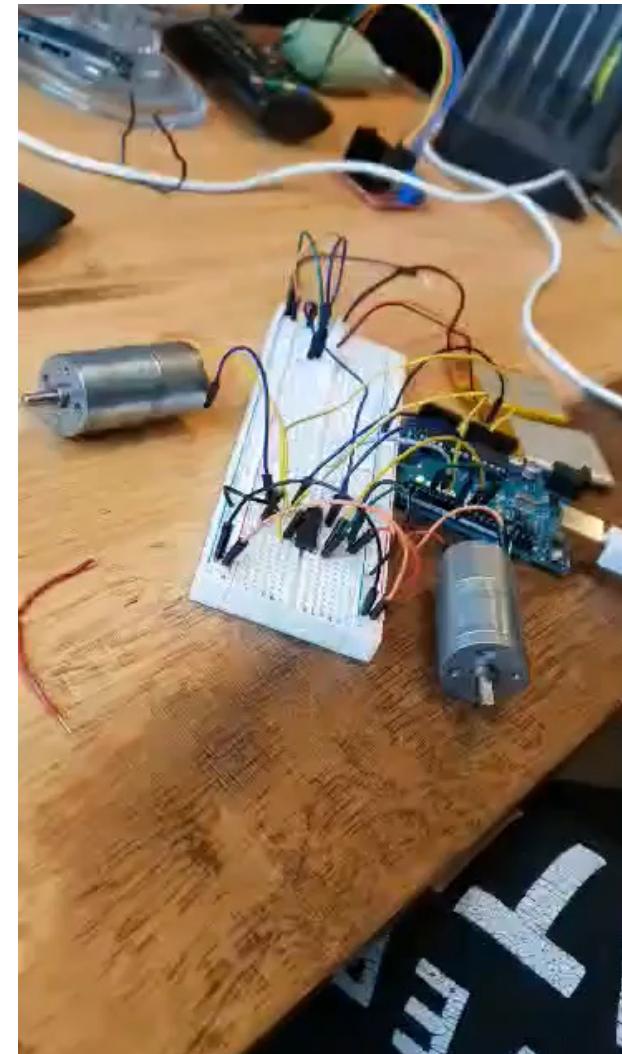
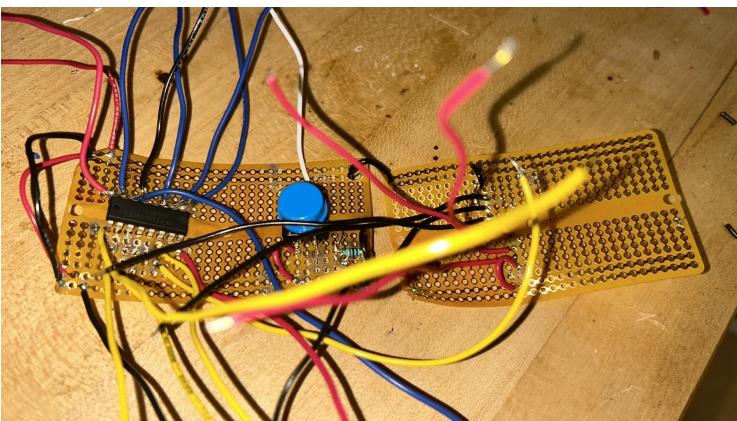


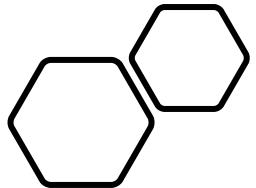


# Donning/Doffing – Motor Mechanism

Goal: Facilitate independent donning/doffing

- Initiate via push button
- Motors appropriately timed to lower/raise top half of device
  - Doffing → higher current to lift against gravity
- Maintain weight balance of components through specific positioning
- Worm gear motors and rod holders to strengthen the rods and resist torque

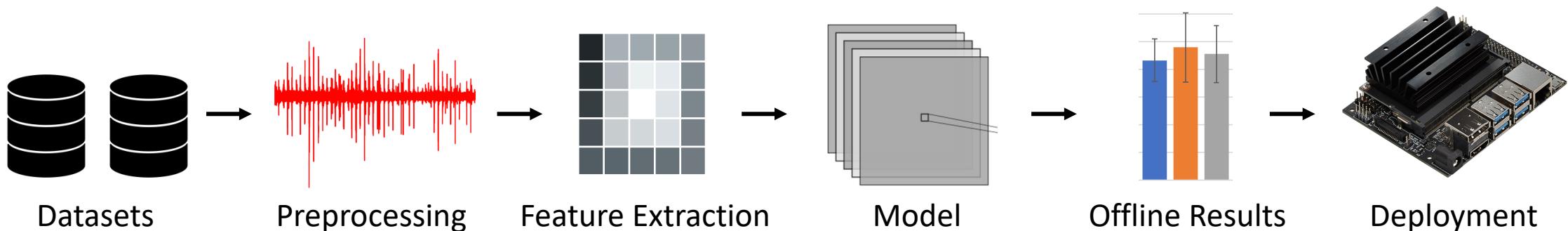


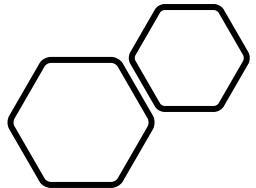


# EMG Trigger – Overview

Goal: Detect user intent

Electromyograph (EMG) shown to be effective for intent detection [8-10]

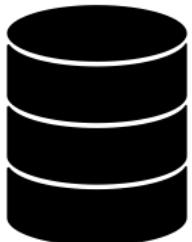




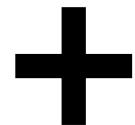
# EMG Trigger - Datasets

- Data requirements:
  - Max. 5 EMG channels
  - Specific placement of electrodes
  - Inclusion of Open Hand (OH) motion

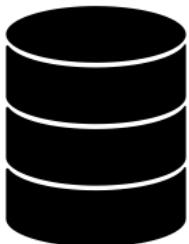
NinaPro DB 10 [11]



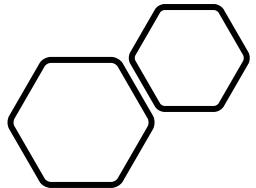
29 healthy, 7 amputees  
Transverse Volar Grip & Lateral Pinch Labels



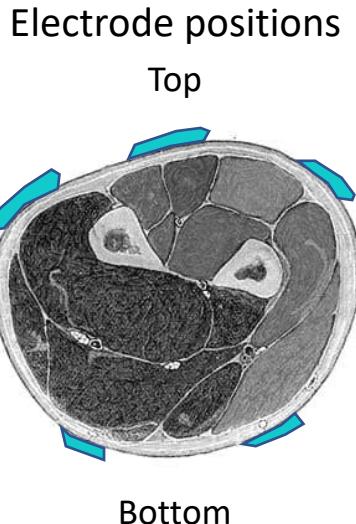
GrabMyo [12]



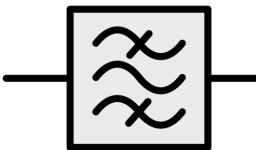
43 healthy  
Open Hand Labels



# EMG Trigger – Data Preprocessing



Removal of unusable subjects/data



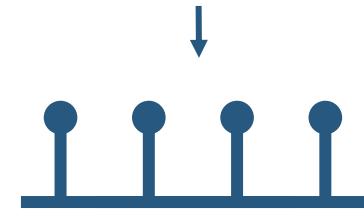
2<sup>nd</sup> Order Butterworth  
Band-Pass Filter  
10-125 Hz



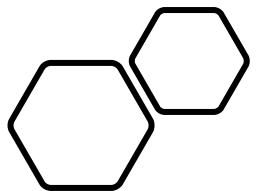
Notch Filter  
(QF = 30)  
60 Hz



NinaPro DB 10 @ 1926 Hz  
GrabMyo @ 2048 Hz

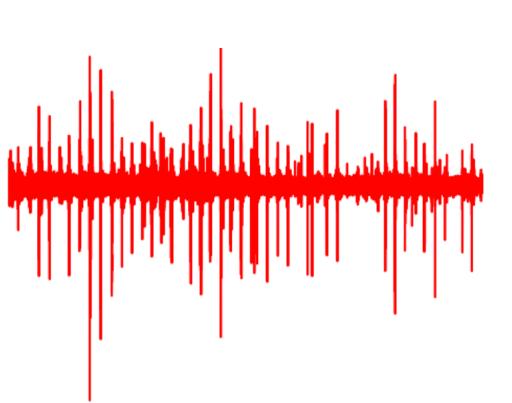


Resampled  
@ 250 Hz

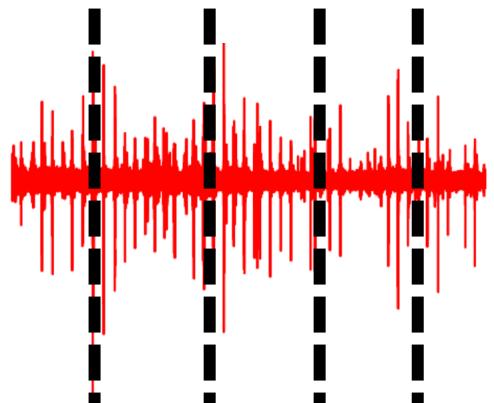


# EMG Trigger – Feature Extraction

Preprocessed Signal

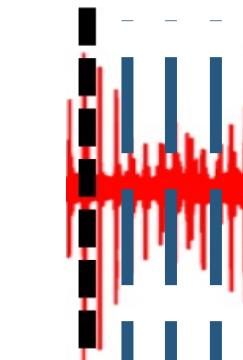


Windowing



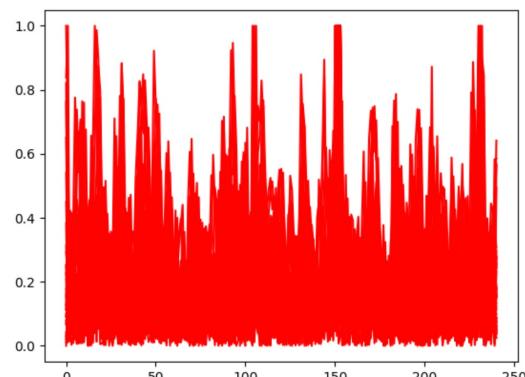
152 ms w/ 116ms overlap

Short Time Fourier Transform

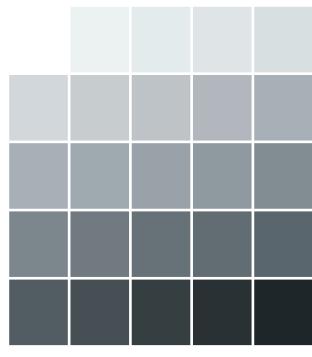


8 ms w/ 4.8 ms overlap

Min-Max Norm

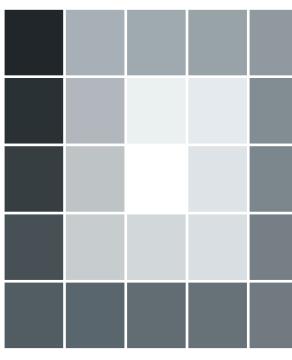


Principal Component Analysis

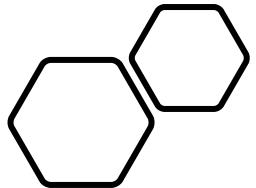


5

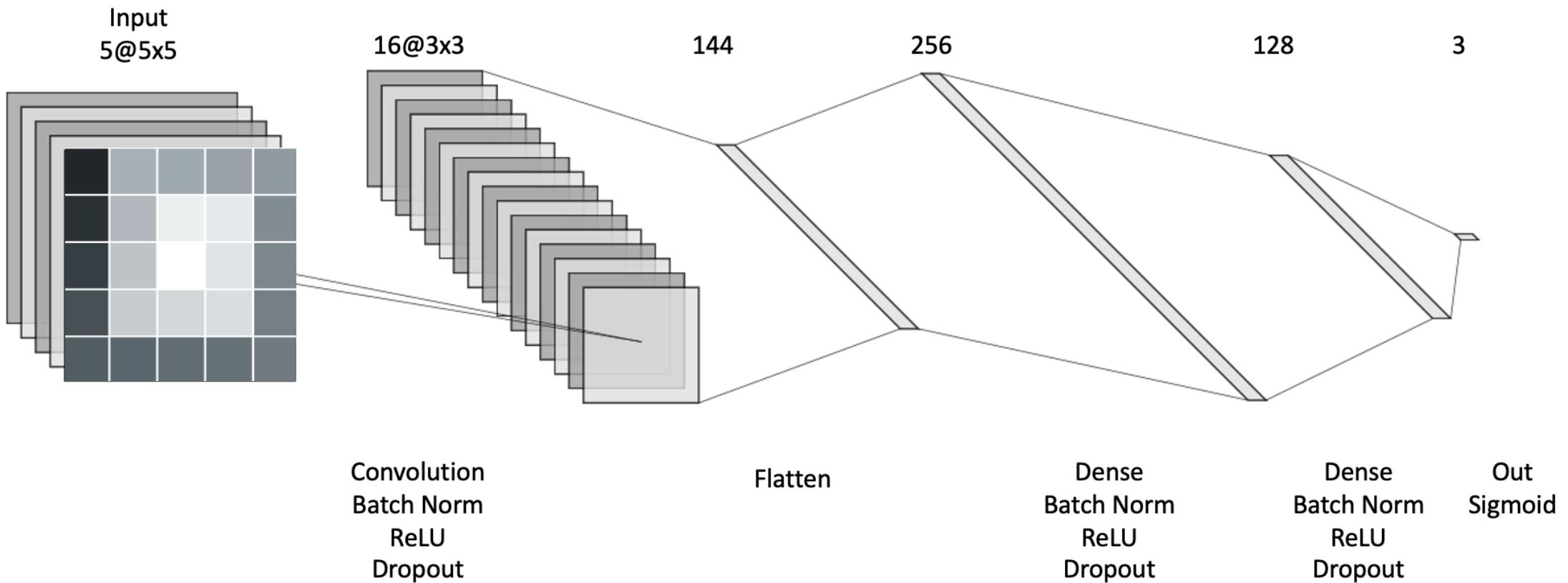
Spiral Reshape



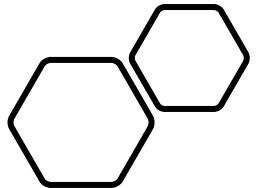
5



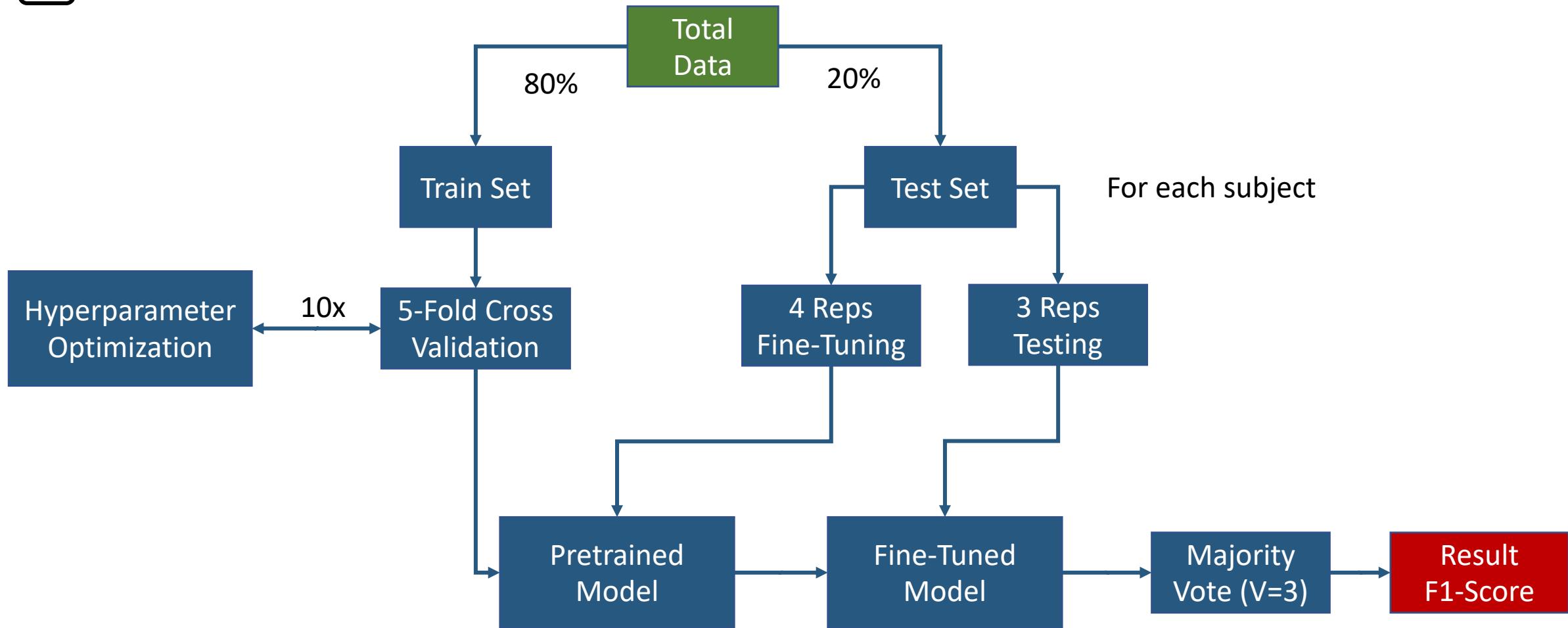
# EMG Trigger – CNN Model Architecture

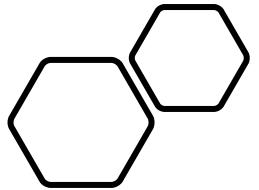


Minimizes cross-entropy loss function with class-specific weights



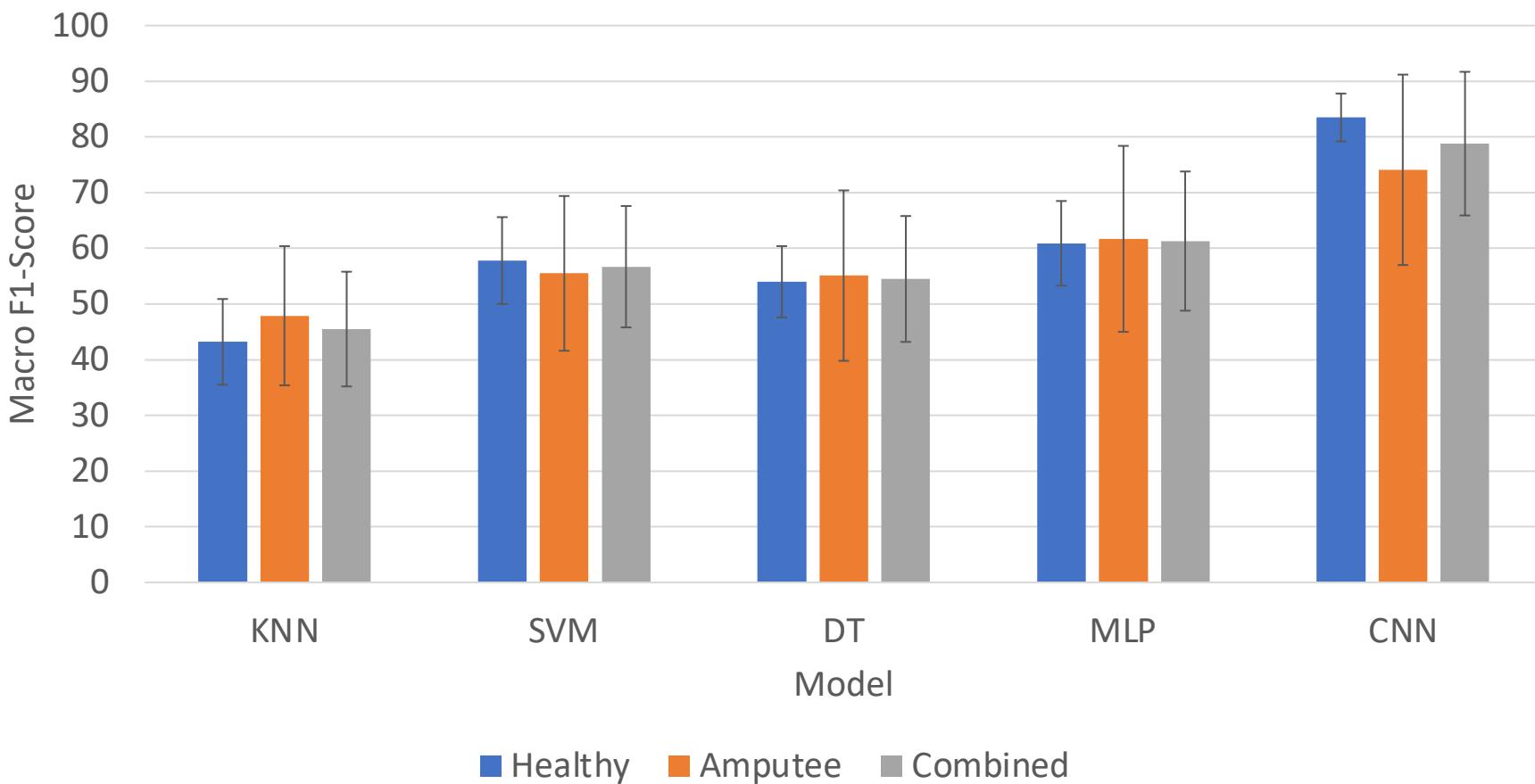
# EMG Trigger – Experimentation Scheme

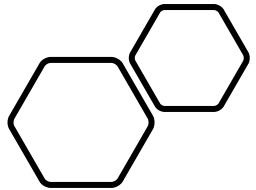




# EMG Trigger – Offline Results

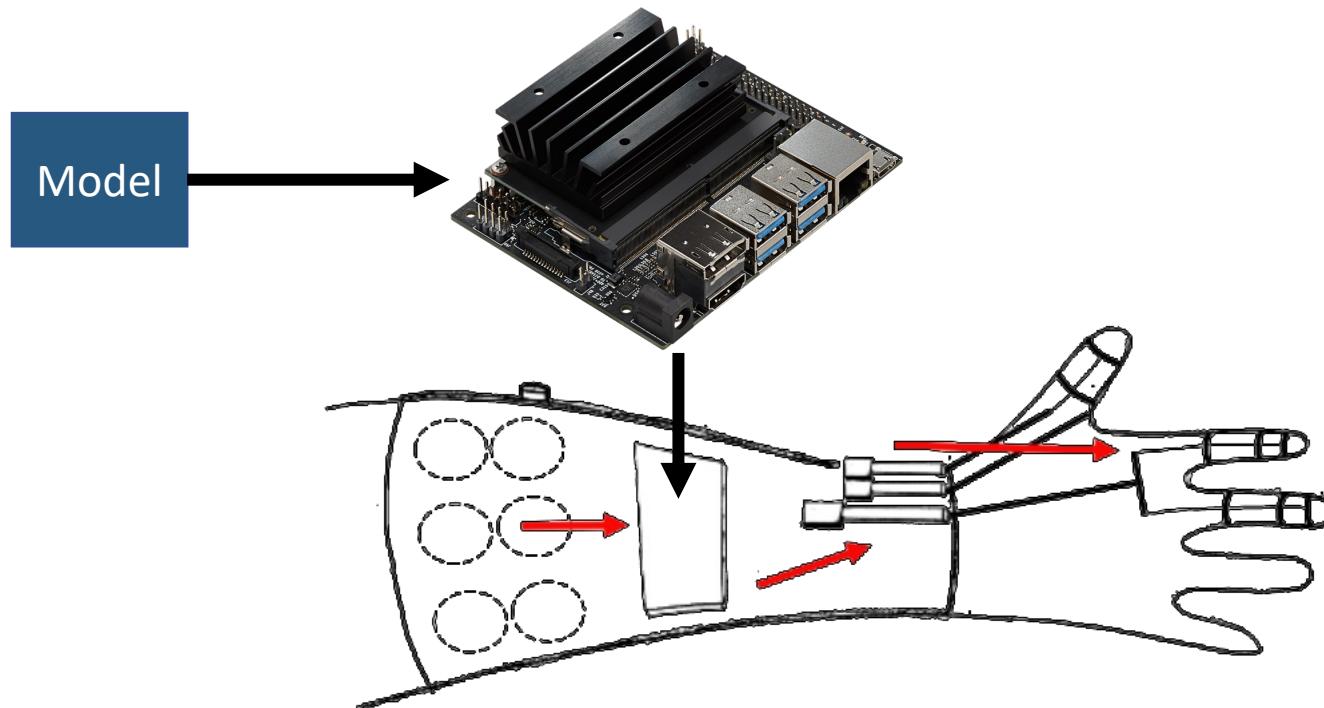
- Macro F1-Scores: 84% for Healthy, 74% for Amputees, 79% Combined

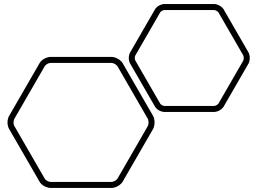




# EMG Trigger – Deployment

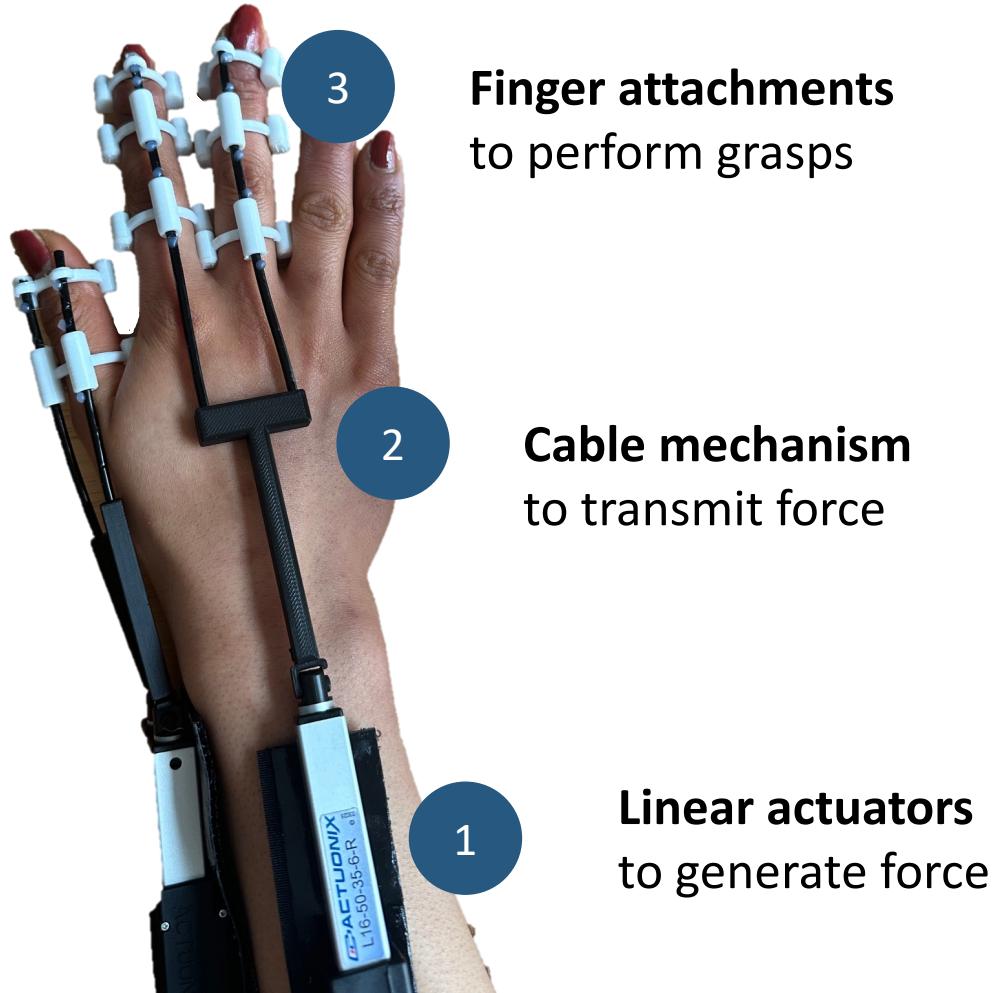
- Deployed CNN model onto Jetson Nano microcontroller for real-time intent detection

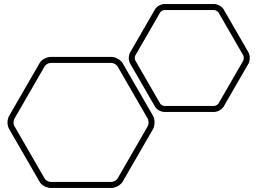




# Actuation – Overview

Goal: Facilitate desired grasps





# Actuation – Linear Actuators

Goal: Generate force using Actuonix Rapid Control (RC) linear servos

**Thumb:** L12-30-50-6-R

- 30mm stroke length
- 34g mass
- 22N max force
- 25mm/s max speed
- 12N backdrive force



Flexion  
Extension



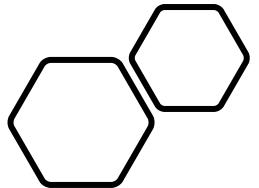
Abduction  
Adduction



Flexion  
Extension

**Middle/Index:** L16-50-35-6-R

- 50mm stroke length
- 56g mass
- 50N max force
- 32mm/s max speed
- 31N backdrive force



# Actuation – Linear Actuators

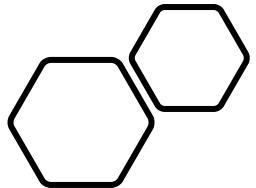
Goal: Control force using Servo library

Transverse Volar Grip

```
29 void TVG() {
30     // Abduct thumb
31     for (pos = 0; pos <= 120; pos += 1) {
32         thumb_abd.write(pos);
33         delay(15);
34     }
35
36     delay(1000);
37
38     // Flex index/middle
39     for (pos = 0; pos <= 100; pos += 1) {
40         index.write(pos);
41         delay(15);
42     }
43 }
```

Lateral Pinch

```
45 void LP(){
46     // Flex index/middle
47     for (pos = 0; pos <= 100; pos += 1) {
48         index.write(pos);
49         delay(15);
50     }
51
52     delay(2000);
53
54     // Abduct and flex thumb
55     for (pos = 0; pos <= 100; pos += 1) {
56         thumb_flex.write(pos);
57         thumb_abd.write(pos);
58         delay(15);
59     }
60 }
```



# Actuation – Cable Mechanism

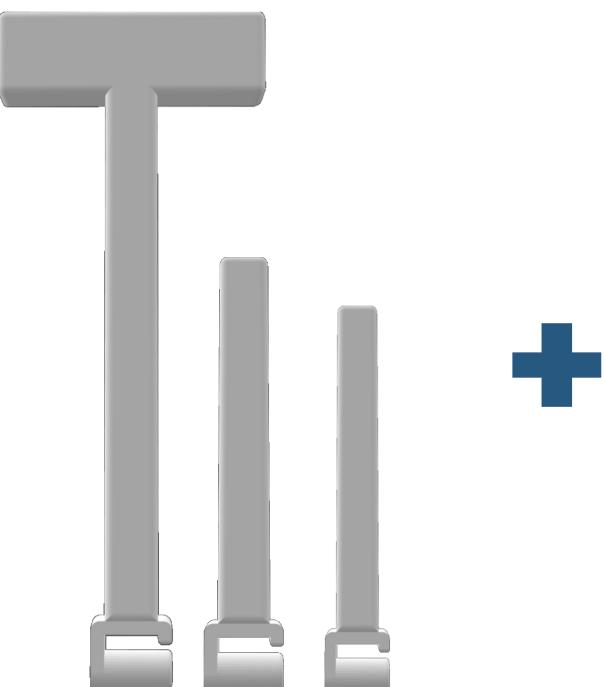
Goal: Transmit force from linear actuators

## Benefits:

- Low-profile & compact
- Lightweight
- Comfortable
- Compliant

## Challenges:

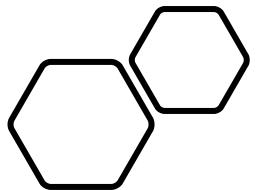
- Diminished strength
  - Friction
  - Buckling



3D printed  
connector



Inner: Teflon-coated cable  
Outer: Seal liner

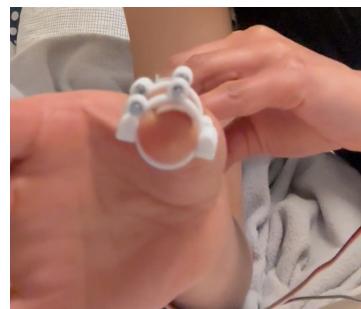
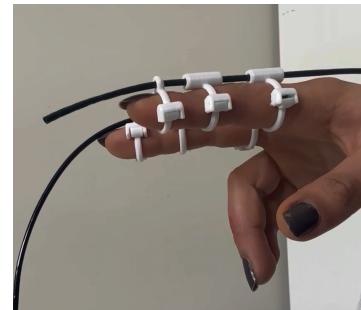
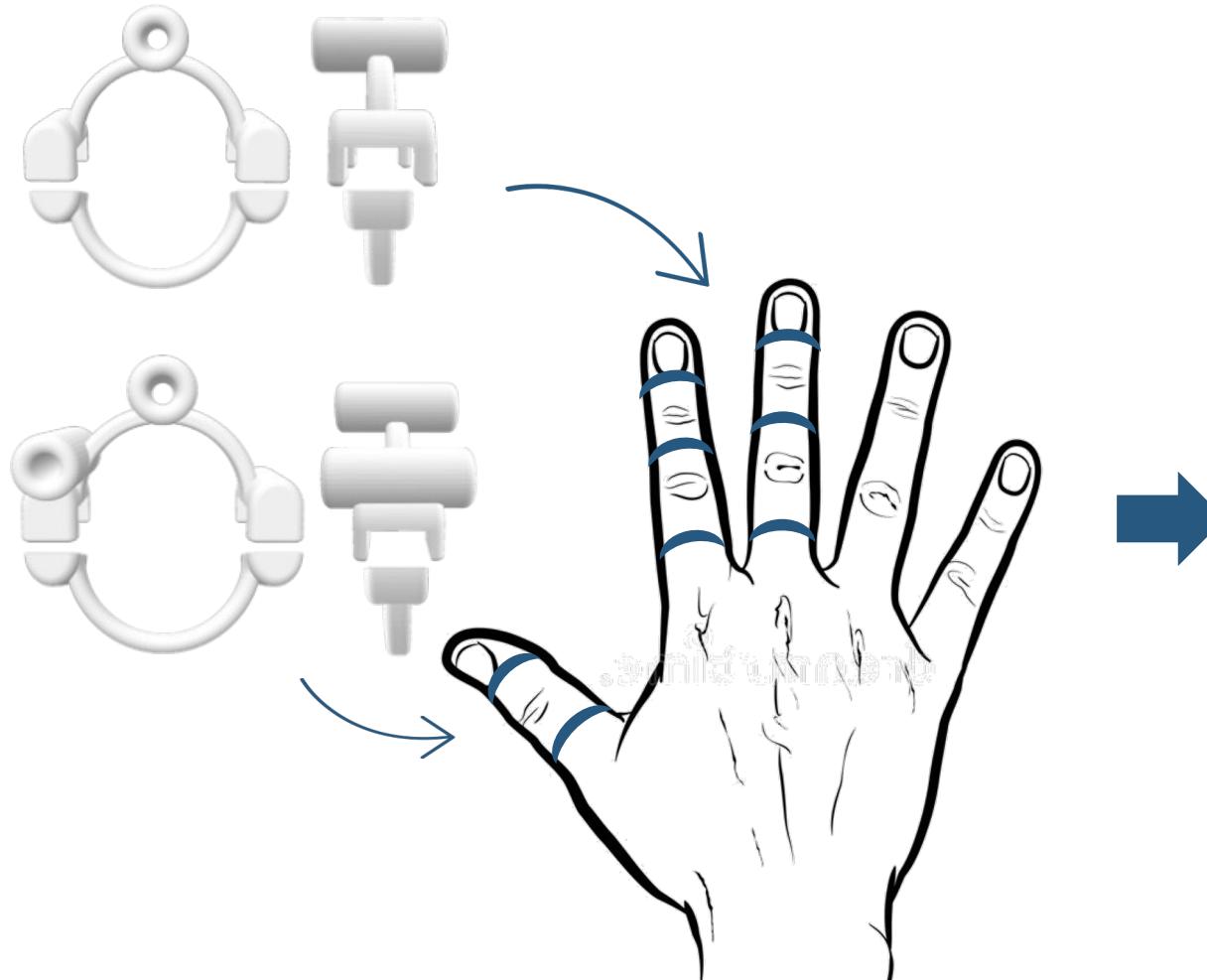


# Actuation – Finger Attachments

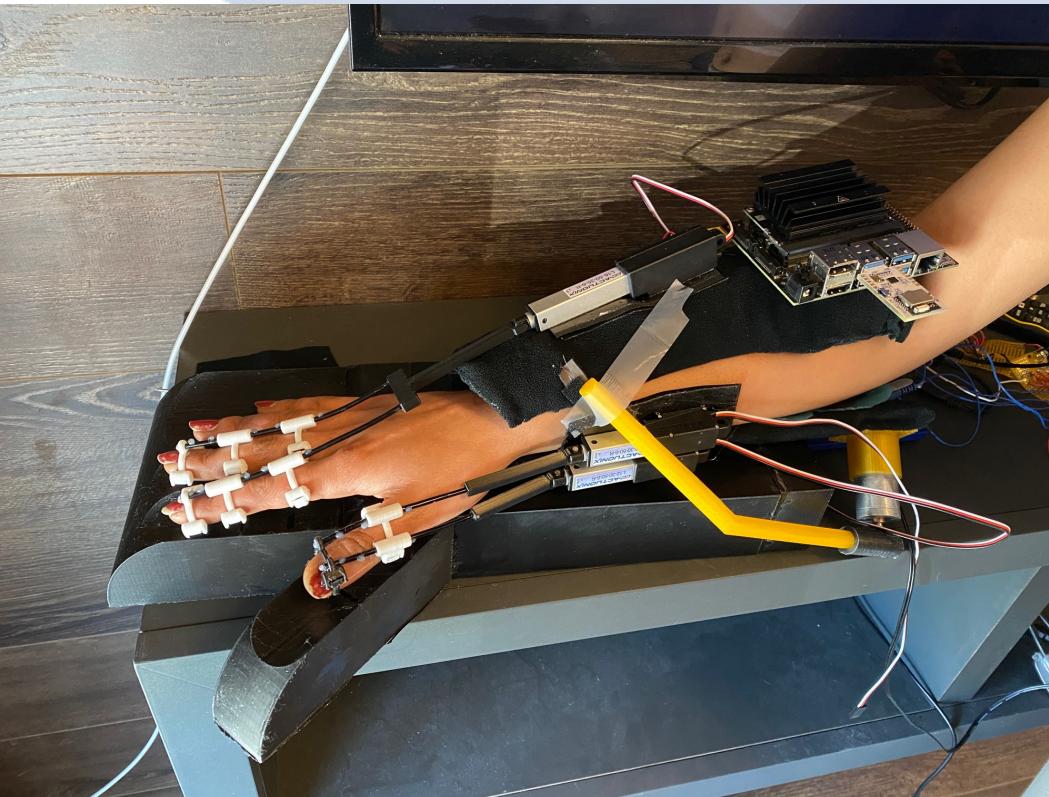
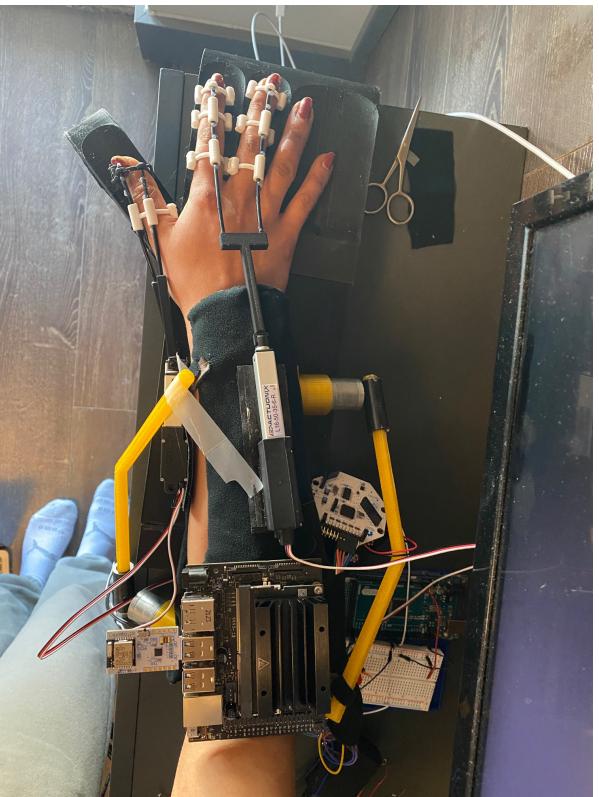
Goal: Deliver force to fingers

## Requirements:

- Bend at joints vs. allow force transmission
- Prevent buckling vs. maintain comfort
- Independent donning/doffing vs. secure attachment



# Designed Solution



# Designed Solution – Actuation

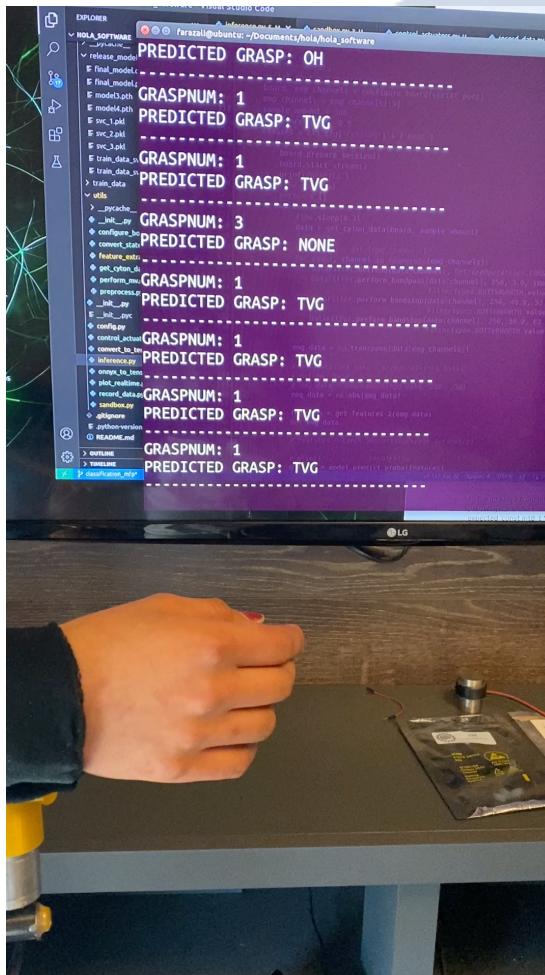
Transverse Volar Grip



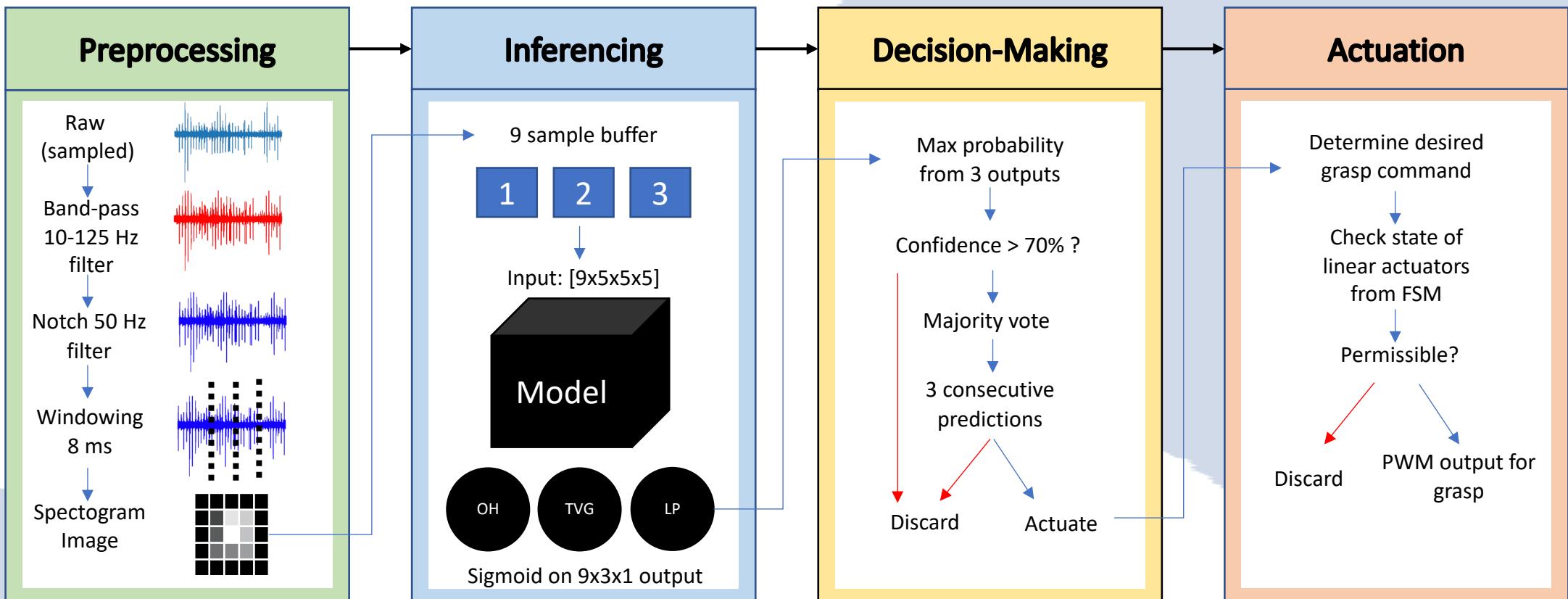
Lateral Pinch



# Designed Solution – Intent Detection



# Designed Solution – Control Flow



# Verification & Validation

Specification	Result
Device must provide a minimum output force of 45N and 25N during TVG and LP, respectively	Able to lift a 500g weight via TVG and LP; further testing required to get to specification weight
Device's trigger classification model must have at least 90% F1-score for all grasping motions	75.9% for SCI participant (offline) 70.1% for proxy healthy user (real-time)
Device must retain at least 80% of the user's natural ROM	42%
Device must not weight more than 550g	823g
Device must enable the user to perform TVGs and LPs	Grasp performance complete in isolation; unable to test in assembly

Other specifications required an SCI patient (e.g., Jebsen-Taylor Hand Function Test) or were not feasible given the single prototype (e.g., tensile testing)

# Limitations

Designed solution is bulky (273g over target weight)

Designed solution is highly specific to one user (component dimensions, jig alignment)

Discrepancy in EMG electrode placement (limited to top and bottom of forearm)

EMG classification data came from differing datasets, resulting in turbulent learning

# Safety & Regulations

## Regulation

- Device subject to FDA Class I regulation [18,19]

## Prevent Device Heating

- Motors contained in 3D printed housings
- Linear actuators and Jetson Nano separated from Fabrifoam layer

## Cable Management

- Limited wire exposure

## User Comfort

- Fabrifoam reduces skin irritation and supports long-term wearability
- Finger attachments feature a split design to mitigate pinching concerns

# Impacts

## Social

- Device supports user independence and autonomy in completing ADLs, restoring self-confidence and providing a sense of empowerment

## Economic

- Device is less expensive than competitors by >\$500 before streamlining manufacturing

## Environmental

- Dry electrodes are reusable for ~100 sessions
- Use of additive manufacturing reduces impact

# Challenges & Successes

## Challenges

- Individual components had their own unique technical challenges, resulting in delayed integration and testing
- Limited access to target user group impacted validation activities
- Scarcity/delay of required resources (e.g., microcontroller, batteries, motors)
- Inconsistencies with 3D printing technology

## Successes

- Executed several design loops to create and test individual components
  - Actuation workflow effectively transmitted force to perform the desired grasps
  - 5-channel EMG classification achieved comparable results to dense sampling approaches
  - Jig and motors facilitated the independent donning/doffing process

# Conclusion & Recommendations

## Conclusion

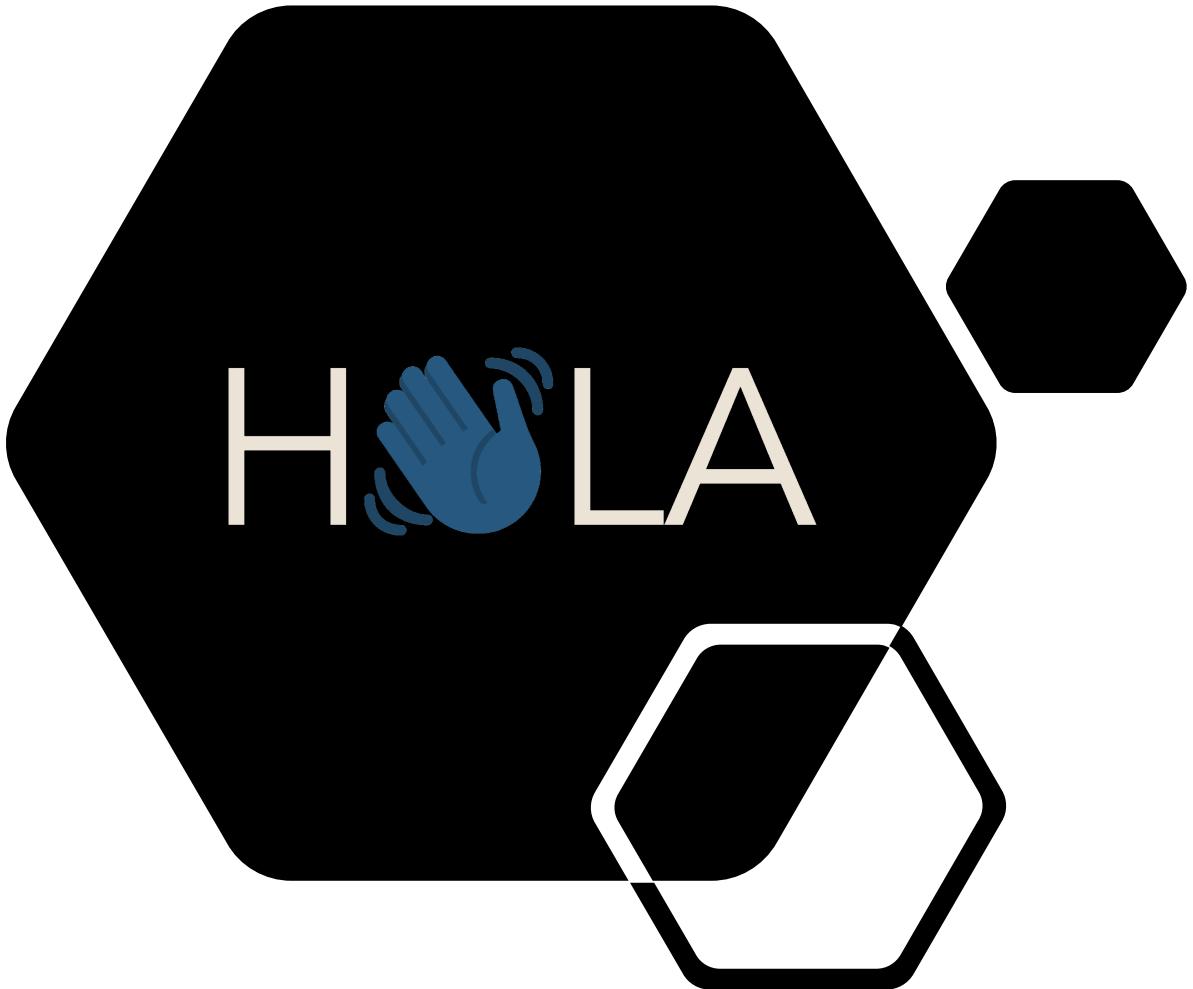
- Classification algorithm achieved a high level of accuracy, with only a small amount of data required for calibration
- Actuation mechanism successfully allowed for execution of TVG and LP grasps
- Device supported independent donning/doffing capability

## Recommendations

- Reduce device bulk to improve formfactor and comfort
- Further improve finger attachment design to facilitate gripping
- Implement closed-loop feedback to allow for automatic grip strength control
- Collect and aggregate EMG dataset with consistent electrode placement
- Conduct validation with SCI patient

# Thank you!

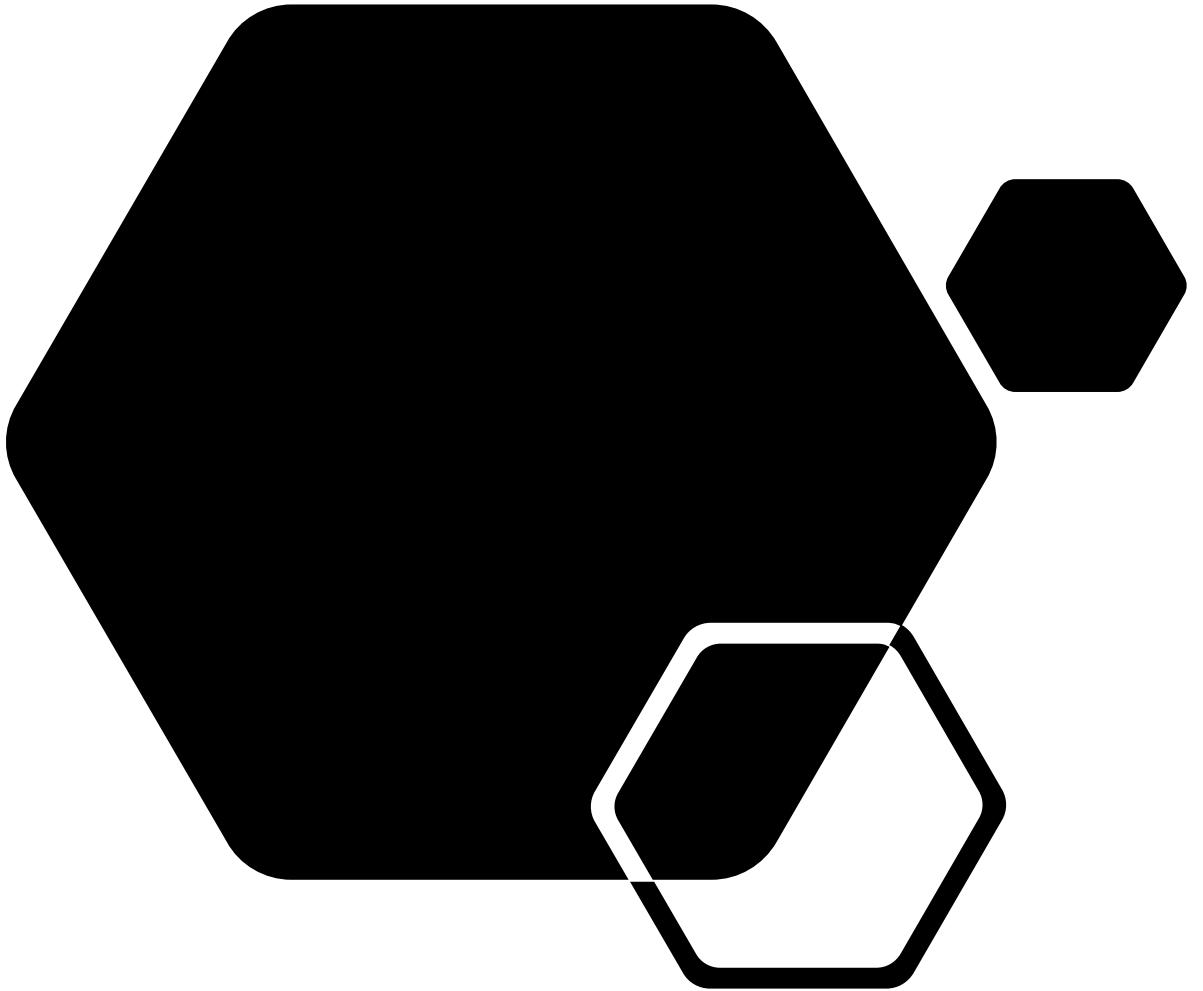
Questions?



# References

- [1] L. Simpson, J. Eng, J. Hsieh and D. Wolfe and the Spinal Cord Injury Research Institute, "The Health and Life Priorities of Individuals with Spinal Cord Injury: A Systematic Review", *Journal of Neurotrauma*, vol. 29, no. 8, pp. 1548-1555, 2012. Available: 10.1089/neu.2011.2226
- [2] "American Spinal Cord Injury Association (ASIA) Impairment Scale", Physiopedia, 2021. [Online]. Available: [https://www.physiopedia.com/American\\_Spinal\\_Cord\\_Injury\\_Association\\_\(ASIA\)\\_Impairment\\_Scale](https://www.physiopedia.com/American_Spinal_Cord_Injury_Association_(ASIA)_Impairment_Scale). [Accessed: 31- Oct- 2021].
- [3] D. Wolfe and D. Lala, "University of Waterloo Capstone Discussion", Microsoft Teams, 2021.
- [4] "Neofect Neomano," Neofect. [Online]. Available: <https://www.neofect.com/us/neomano>. [Accessed: 06-Dec-2022].
- [5] "Ness H200," Neurorehabdirectory.com, 10-Dec-2019. [Online]. Available: <https://www.neurorehabdirectory.com/rehab-products/ness-h200/>. [Accessed: 06-Dec-2022].
- [6] Laura Hallock. Drew McPherson - Building Effective Assistive Devices & Organizations as an Engineer, Leader, & User. (Sept. 26, 2022). Accessed: Sept. 30, 2022. [Online video]. Available: [https://www.youtube.com/watch?v=PpKjlOvSME&list=PL51-747gY2lx12n\\_HjmTpLB439tpO852D&index=4](https://www.youtube.com/watch?v=PpKjlOvSME&list=PL51-747gY2lx12n_HjmTpLB439tpO852D&index=4)
- [7] C. Sollerman and A. Ejeskär, "Sollerman Hand Function Test: A Standardised Method and its Use in Tetraplegic Patients", *Scandinavian Journal of Plastic and Reconstructive Surgery and Hand Surgery*, vol. 29, no. 2, pp. 167-176, 1995. Available: 10.3109/02844319509034334.
- [8] U. Cote-Allard et al., "Deep Learning for Electromyographic Hand Gesture Signal Classification Using Transfer Learning," *IEEE Transactions on Neural Systems and Rehabilitation Engineering*, vol. 27, no. 4, pp. 760–771, Apr. 2019, doi: <https://doi.org/10.1109/tnsre.2019.2896269>.
- [9] X. Zhai, B. Jelfs, R. H. M. Chan, and C. Tin, "Self-Recalibrating Surface EMG Pattern Recognition for Neuroprostheses Control Based on Convolutional Neural Network," *Frontiers in Neuroscience*, vol. 11, Jul. 2017, doi: <https://doi.org/10.3389/fnins.2017.00379>.
- [10] E. Campbell, A. Phinyomark, and E. Scheme, "Deep Cross-User Models Reduce the Training Burden in Myoelectric Control," *Frontiers in Neuroscience*, vol. 15, May 2021, doi: <https://doi.org/10.3389/fnins.2021.657958>.
- [11] M. Cognolato et al., "Gaze, visual, myoelectric, and inertial data of grasps for intelligent prosthetics," *Scientific Data*, vol. 7, no. 1, pp. 1–15, Feb. 2020, doi: <https://doi.org/10.1038/s41597-020-0380-3>.
- [12] A. Pradhan, J. He, and N. Jiang, "Multi-day dataset of forearm and wrist electromyogram for hand gesture recognition and biometrics," *Scientific Data*, vol. 9, no. 1, Nov. 2022, doi: <https://doi.org/10.1038/s41597-022-01836-y>.
- [13] "Actuonix L12-30-50-6-R," Actuonix Motion Devices. [Online]. Available: <https://www.actuonix.com/l12-30-50-6-r>. [Accessed: 12-Apr-2023].
- [14] "Actuonix L16-50-35-6-R," Actuonix Motion Devices. [Online]. Available: <https://www.actuonix.com/l16-50-35-6-r>. [Accessed: 12-Apr-2023].
- [15] J. Dittli, U. A. Hofmann, T. Bützer, G. Smit, O. Lambercy, and R. Gassert, "Remote Actuation Systems for Fully Wearable Assistive Devices," *Frontiers in Robotics and AI*, vol. 7, Jan. 2021.
- [16] R. Conti, B. Allotta, E. Meli, and A. Ridolfi, "Development, design and validation of an assistive device for hand disabilities based on an innovative mechanism," *Robotica*, vol. 35, no. 4, pp. 892–906, Nov. 2015.
- [17] "Jagwire Mountain Pro Shift Cable kit," Cyclesmith. [Online]. Available: <https://www.cyclesmith.ca/product/jagwire-mountain-pro-shift-cable-kit-187929-1.htm>. [Accessed: 12-Apr-2023].
- [18] "Code of Federal Regulations Title 21, Volume 8, 21CFR890.5410", accessdata.fda.gov. [Online]. Available: <https://www.accessdata.fda.gov/scripts/cdrh/cfdocs/cfcfr/CFRSearch.cfm?fr=890.5410>. [Accessed: 04-Dec-2022].
- [19] "CFR - Code of Federal Regulations Title 21, Volume 8, 21CFR890.3025," accessdata.fda.gov. [Online]. Available: <https://www.accessdata.fda.gov/scripts/cdrh/cfdocs/cfcfr/CFRSearch.cfm?fr=890.3025>. [Accessed: 04-Dec-2022].

# Supporting Content



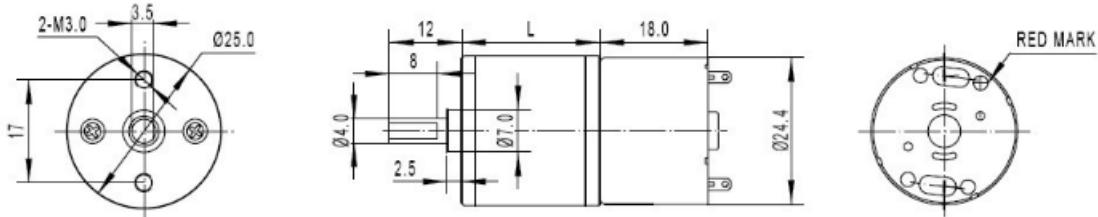
# Motor Specs

Metal DC Geared Motor - 6V 15RPM 10Kg.cm  
SKU:FIT0495-A



## INTRODUCTION

This is a metal DC geared motor, 478:1 metal reducer. It has a small size and large torque. The maximum torque could arrive 10 kg.cm. It is stable and durable!



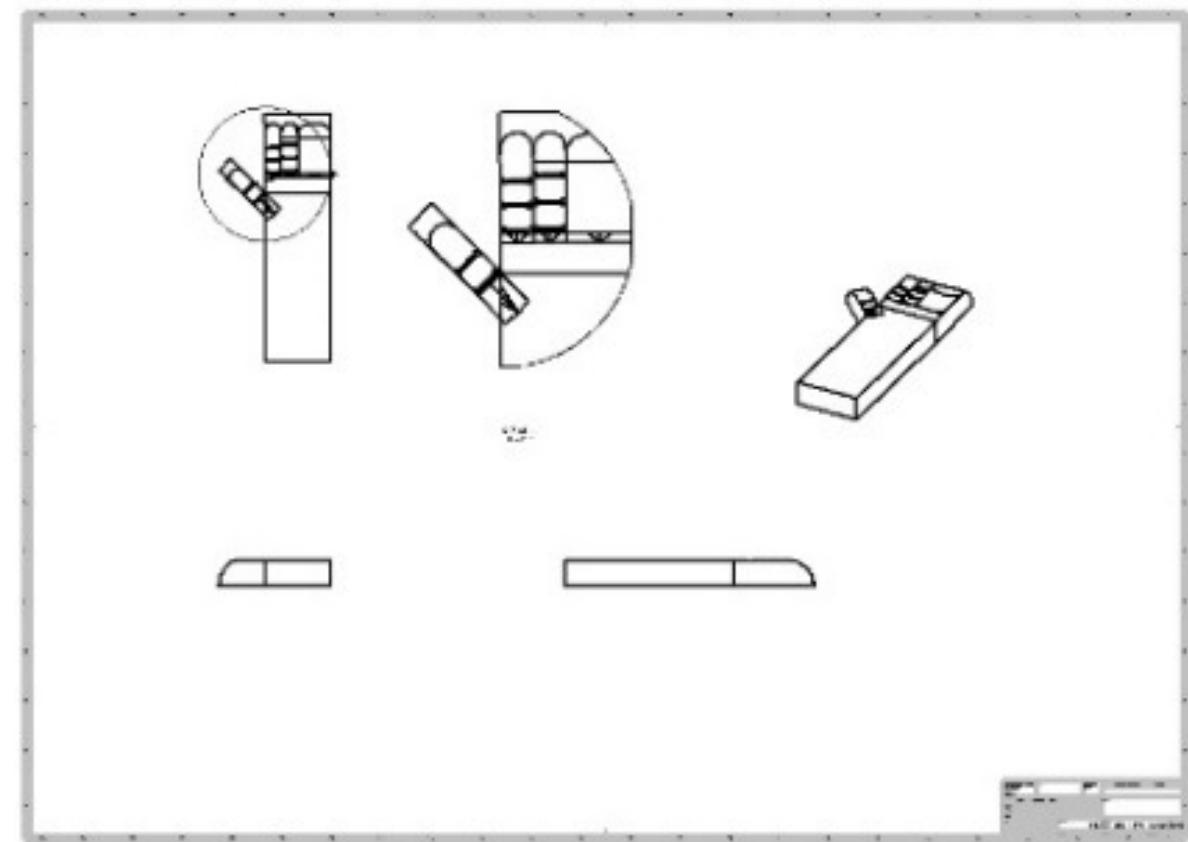
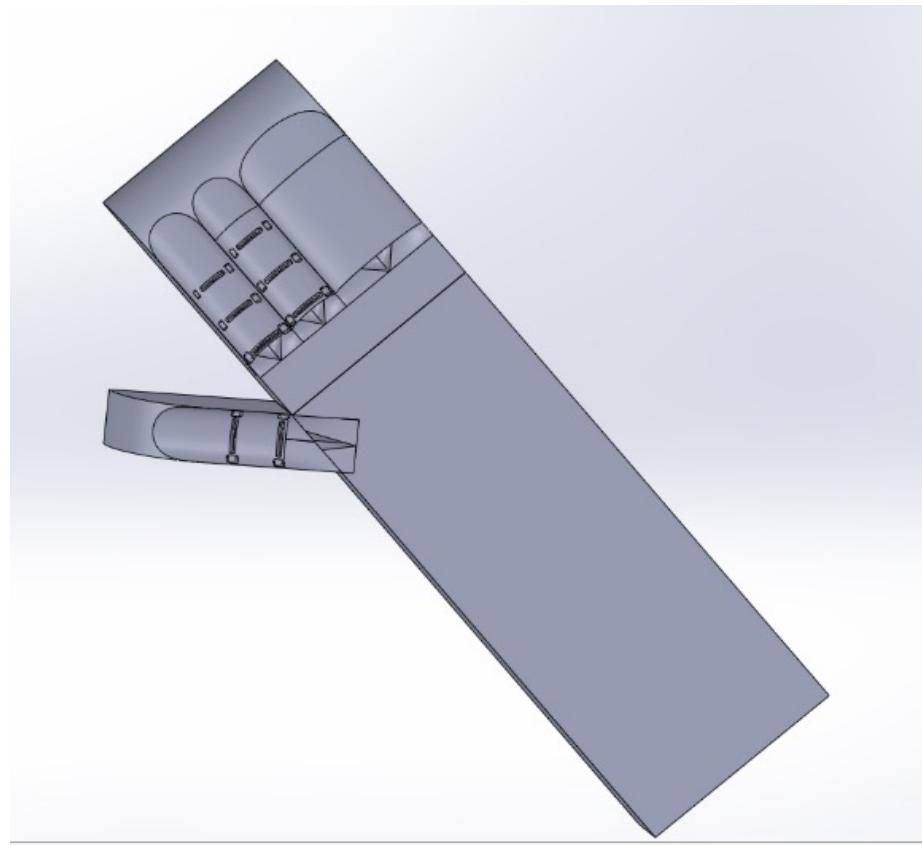
## SPECIFICATION

- Rated Voltage: 6 V
- Operating Voltage Range 2~7.5V
- Gear reduction ratio: 478:1:1
- Gearbox length: 27 mm
- "D" shape shaft diameter: 4 mm
- No-load speed: 15 RPM @ 6V
- No-load current: 50 mA
- Locked-rotor torque: 10 Kg.cm
- Locked-rotor current: 0.6 A
- Operating Temperature: -20~60°C
- Weight: 74g

## SHIPPING LIST

- Metal DC Geared Motor - 6V 15RPM 10Kg.cm x1

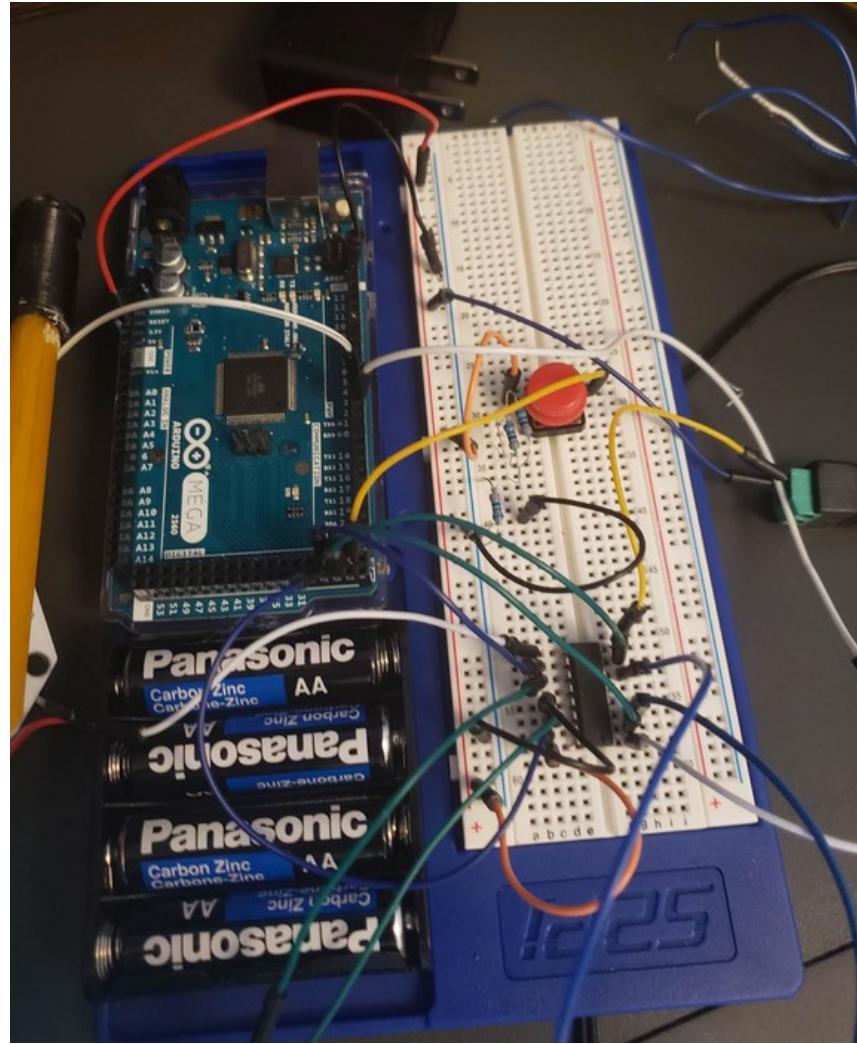
# Jig SolidWorks Design and Assembly Drawing



# Battery Specs



# Motor Setup



# Frame



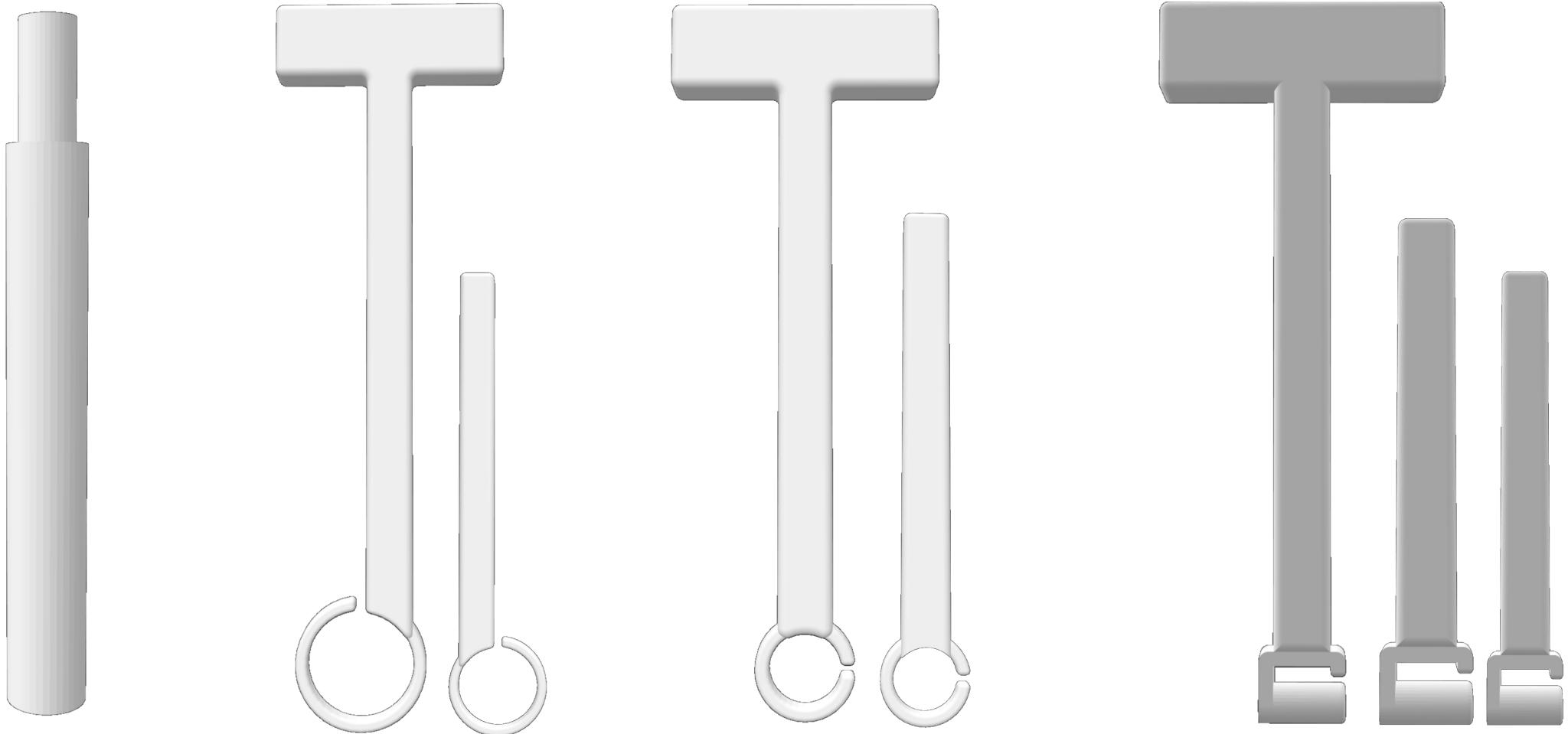
# Actuation – Thumb DoF



# Actuation – Cable/Connector Evolution



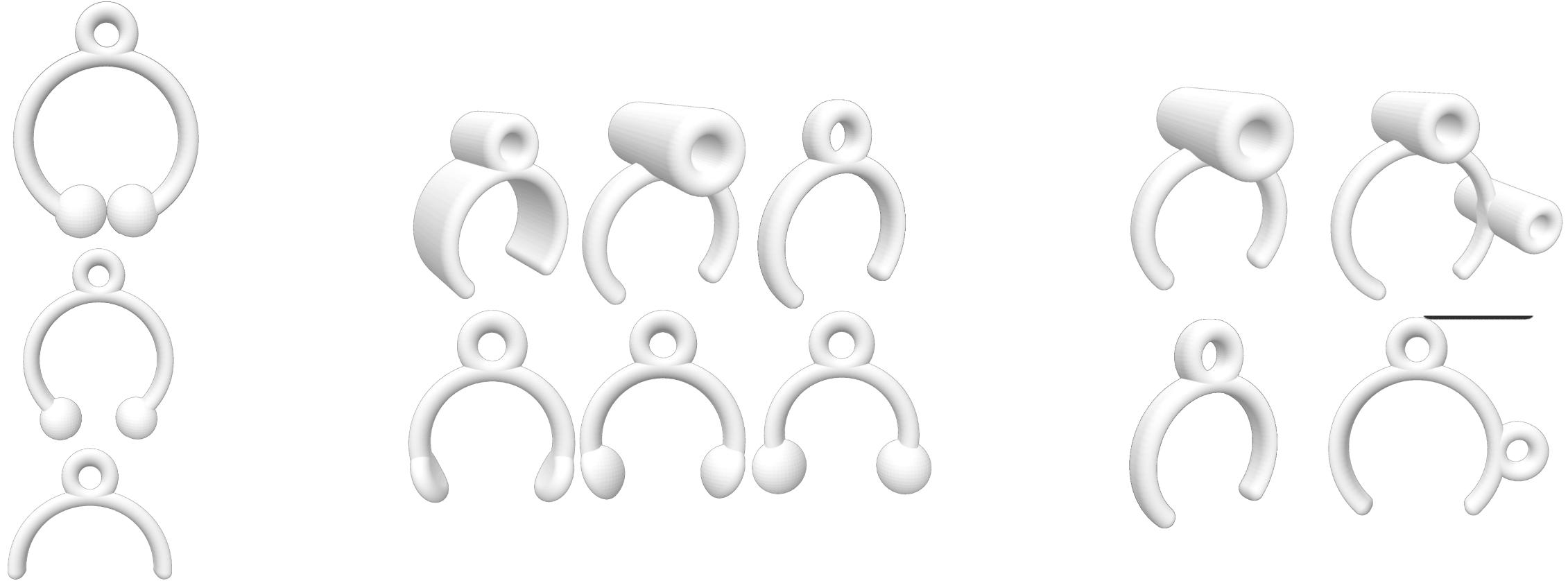
# Actuation – Cable/Connector Evolution



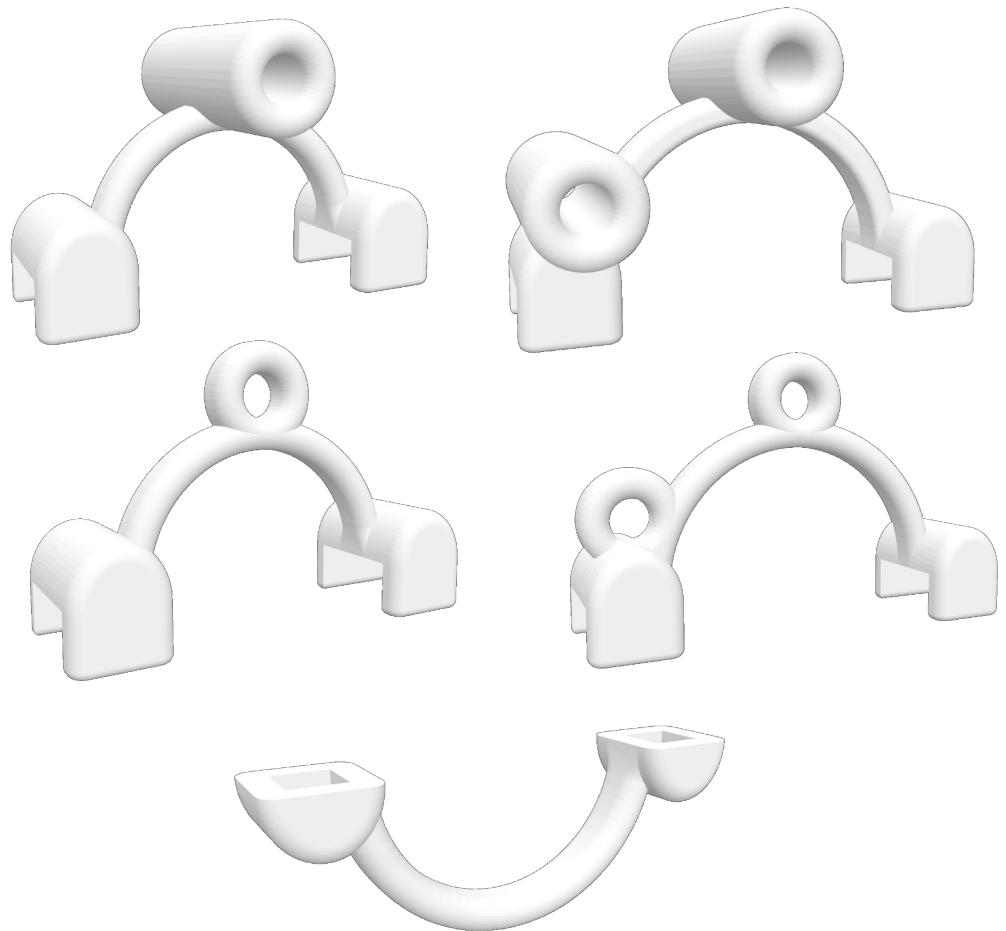
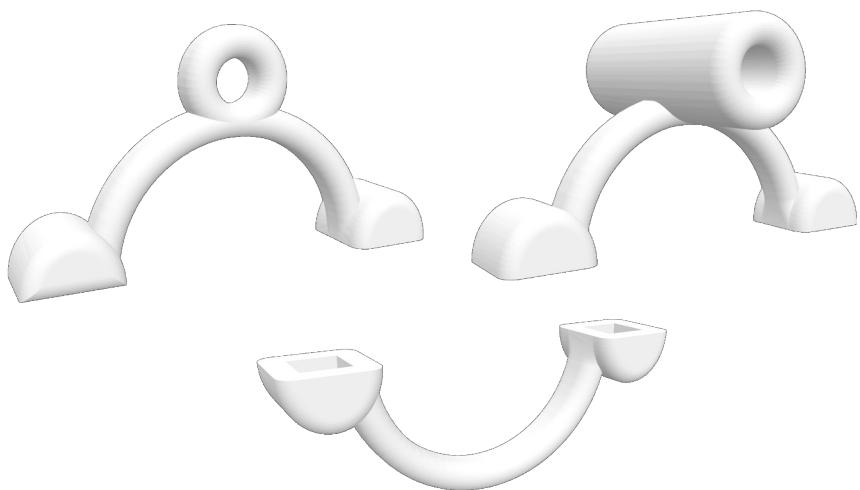
# Actuation – Finger Attachment Evolution



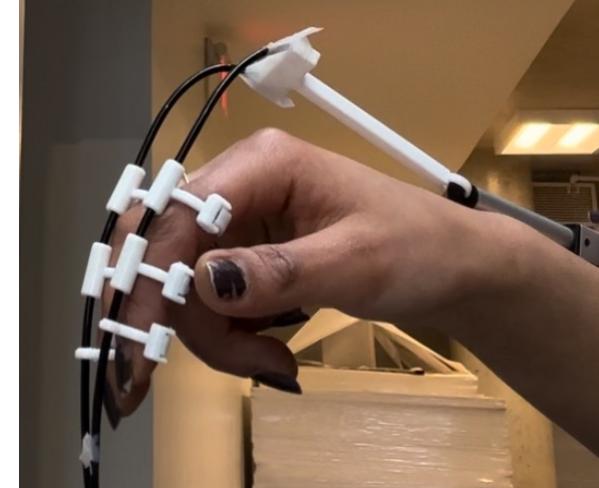
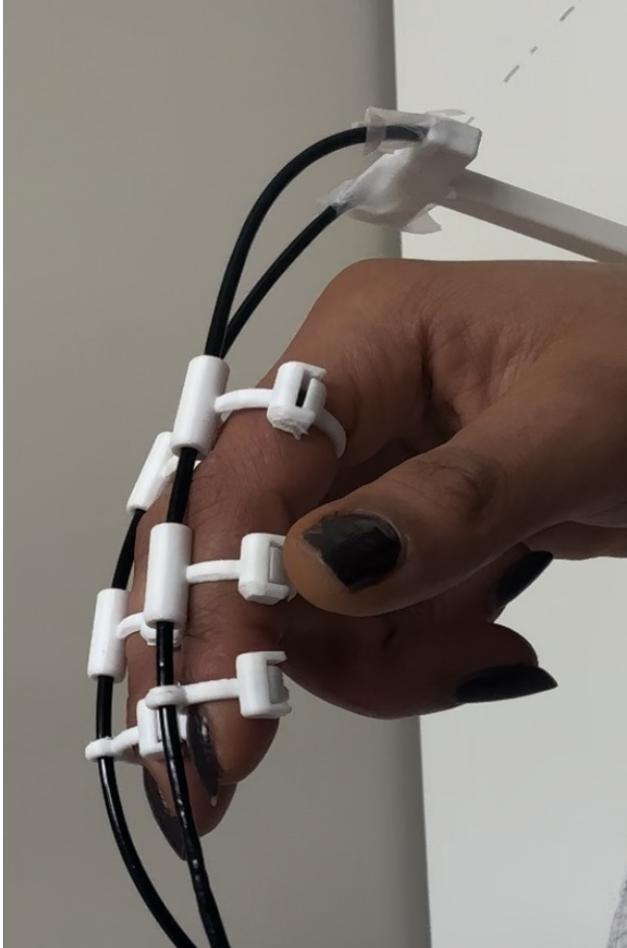
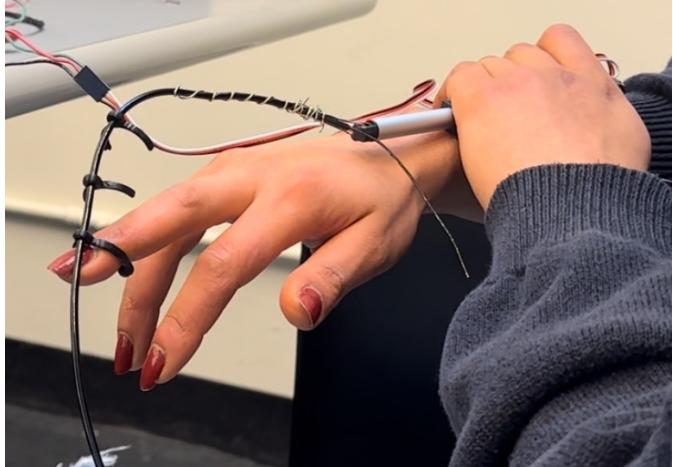
# Actuation – Finger Attachment Evolution



# Actuation – Finger Attachment Evolution



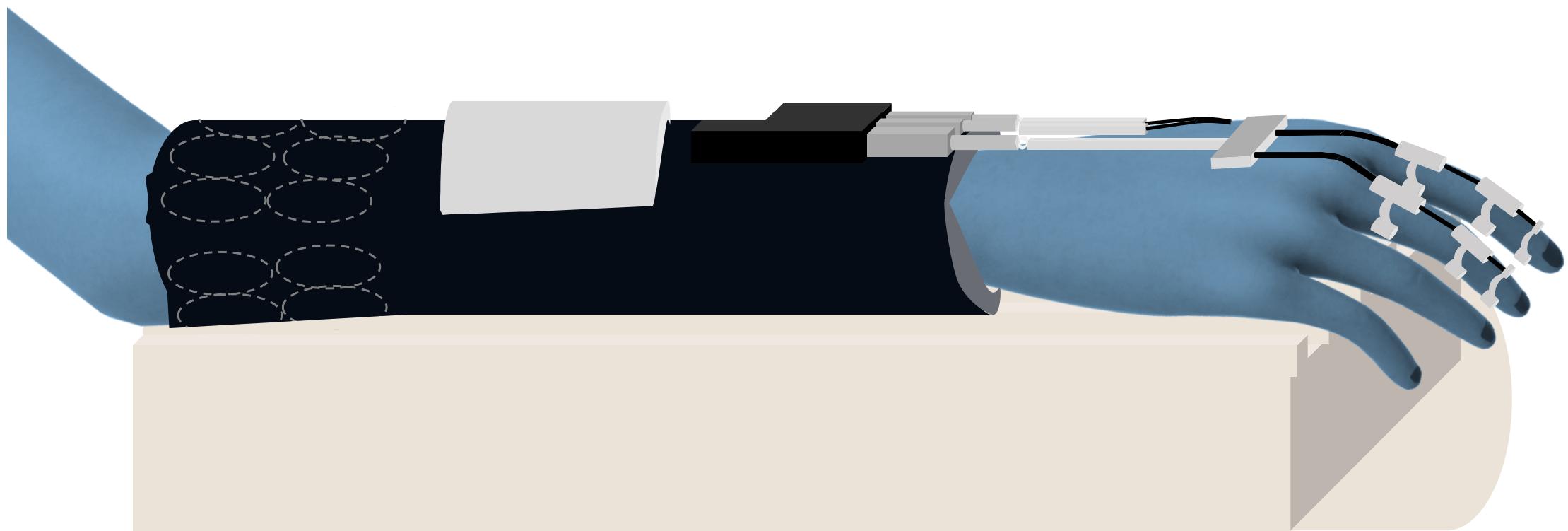
# Actuation – Challenges



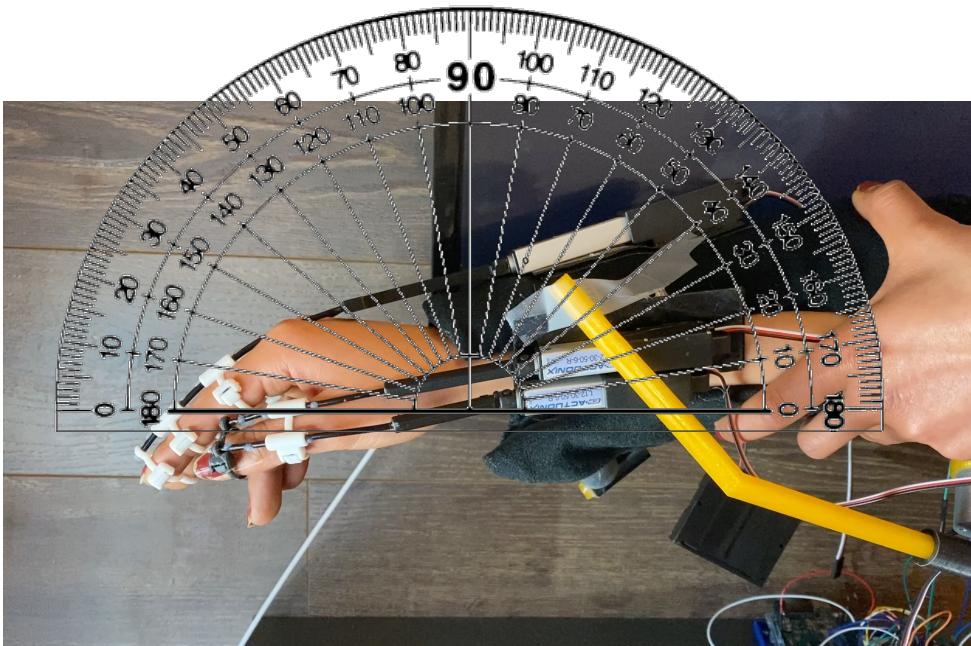
# Actuation – Final



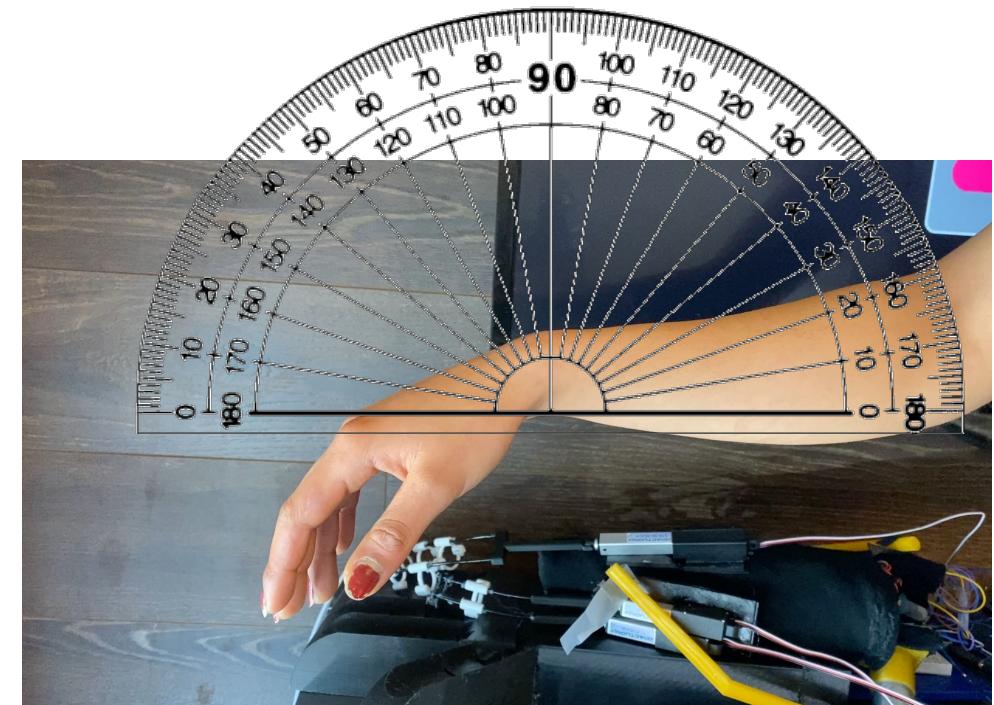
# Designed Solution Graphic



# Validation – Wrist ROM Videos



With ~ 25 degrees



Without ~ 60 degrees

# Trigger Component – Hyperparameter Results

Parameter	Range	Selected
Learning Rate	0.001-0.01	0.009
Dropout Rate	0.3-0.7	0.35
Conv Filters	[32, 64, 128, 256]	128

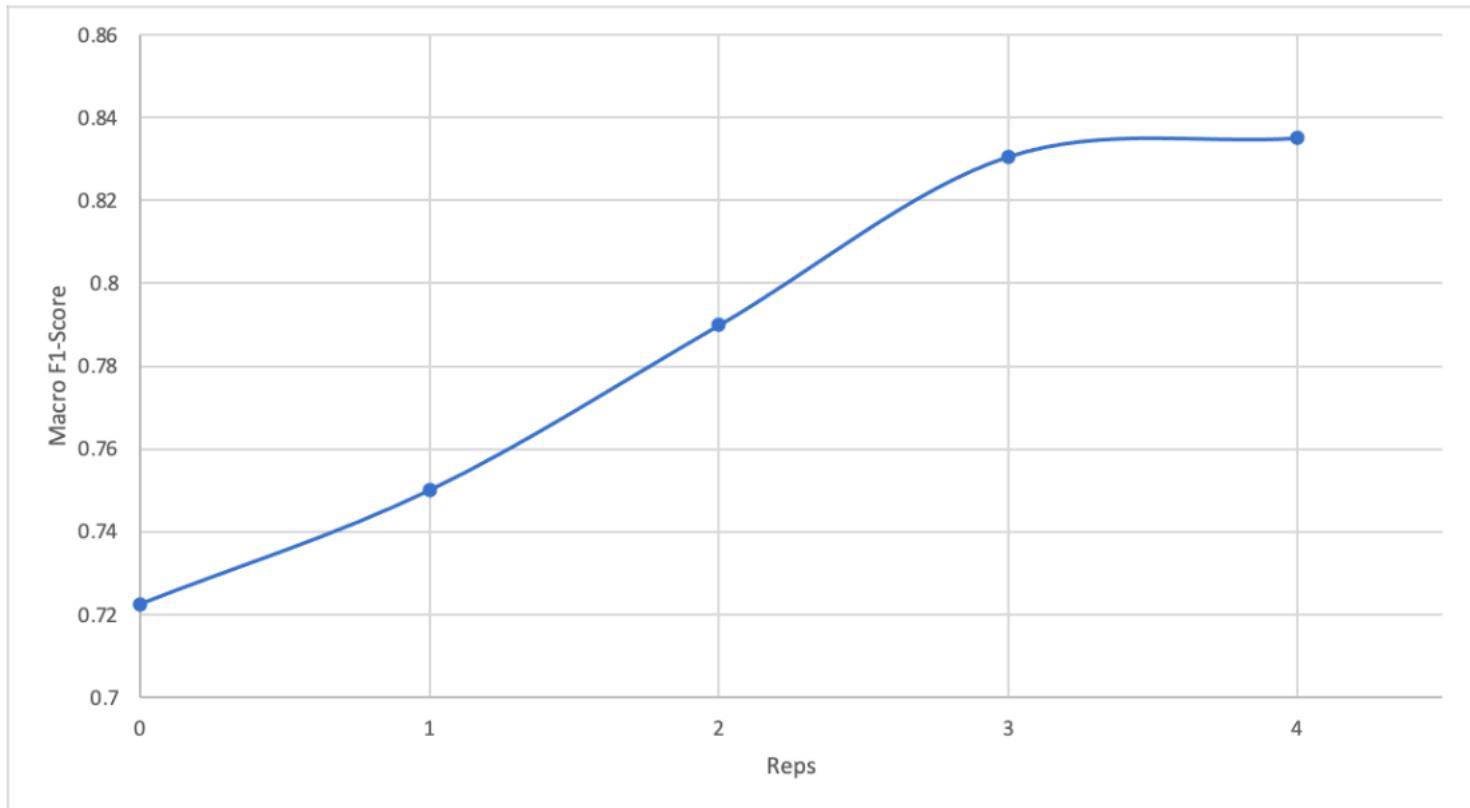
# Trigger Component – Objective Function

$$J = - \sum_{c=1}^M \alpha_c y_{i,c} \log(\hat{y}_{i,c})$$

Where:

- $i$  is the current input sample
- $c$  is the current class
- $M$  is the total number of classes
- $\alpha_c$  is class-specific weight that penalizes misclassifications based on proportion of the class in the dataset
  - $1 -$  proportion of that class in dataset
- $y_{i,c}$  is the ground-truth label for the class
- $\hat{y}_{i,c}$  is the predicted label for the class

# Trigger Component – Fine-Tuning Ablation



# OpenBCI Cyton Main Specs

## Cyton Board Technical Specifications

OpenBCI 32bit Board:

- 8 differential, high gain, low noise input channels
- Compatible with active and passive electrodes
- Texas Instruments ADS1299 ADC ([link to datasheet](#))
- PIC32MX250F128B microcontroller w/chipKIT™ bootloader (50MHz)
- RFduino™ Low Power Bluetooth™ radio ([Link to datasheet](#))
- 24-bit channel data resolution
- Programmable gain: 1, 2, 4, 6, 8, 12, 24
- 3.3V digital operating voltage
- +/-2.5V analog operating voltage
- ~3.3-12V input voltage
- LIS3DH accelerometer ([link to datasheet](#))
- Micro SD card slot
- 5 GPIO pins, 3 of which can be Analog

OpenBCI Dongle:

- [RFD22301 radio module](#) from RFdigital™
- FT231X USB-to-serial converter from FTDI
- Can upload code to the OpenBCI board or the dongle
- Fully broken out and pin-compatible w/ RFduino form factor

Note: If you want a back-up (optional) battery, we recommend this rechargeable [JST 2-pin Lithium Ion Polymer Battery - 3.7v](#). **and** its USB-battery [charger](#)

DO NOT EXCEED A 6V Battery