

Histogram of Gradient Orientations of EEG Signal Plots for Brain Computer Interfaces

Dissertation Defense

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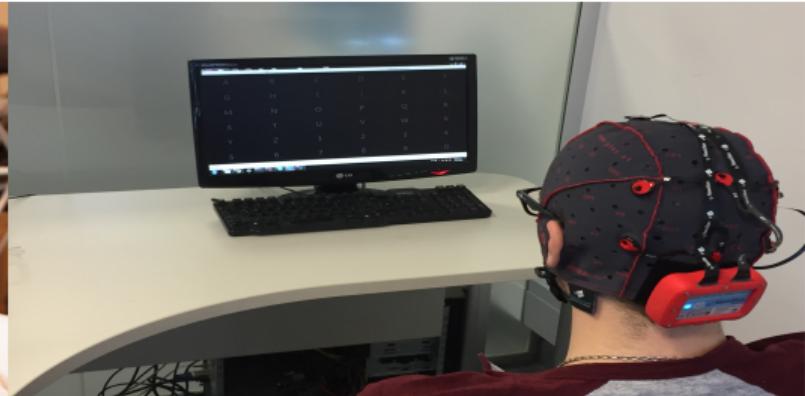
Doctorado en Ingeniería en Informática
Instituto Tecnológico de Buenos Aires

Noviembre 29 2018

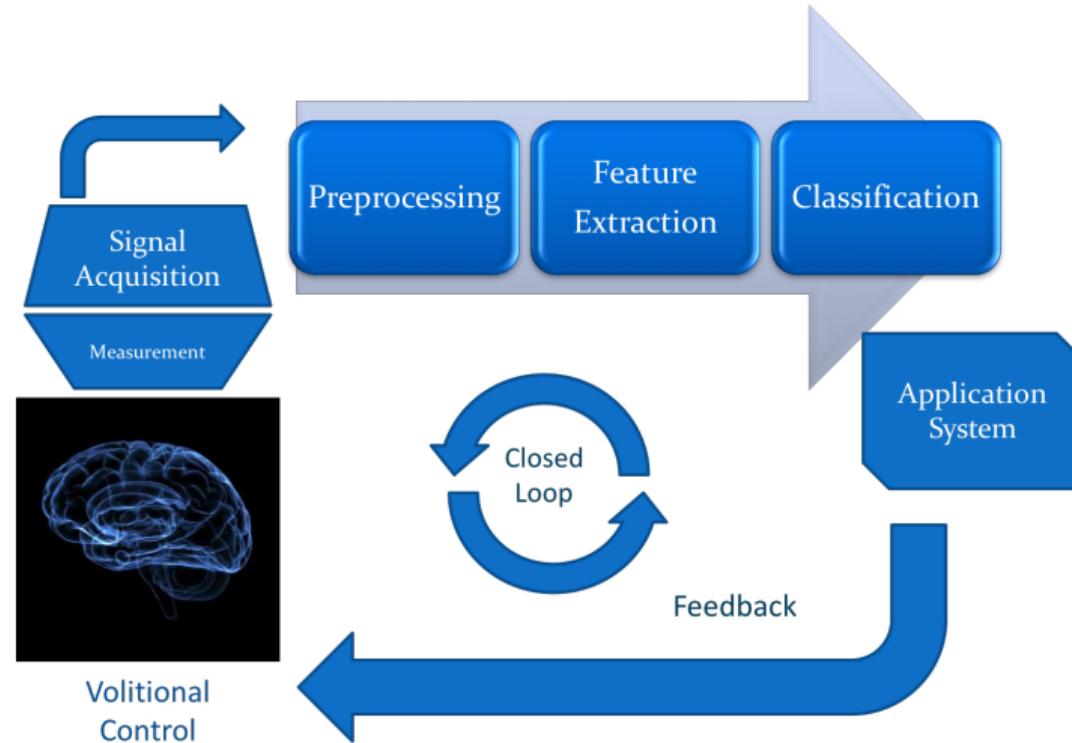
Outline

- 1 Introduction
- 2 Motivation
- 3 The Histogram of Gradient Orientations
- 4 Experimental Validation
- 5 Conclusion
- 6 Questions

Brain Computer Interfaces - Current trends



Brain Computer Interfaces - System Components



Brain Computer Interfaces - BCI Paradigms

Evoked Potential

Steady State Visual Evoked Potential

SSVEP
SSAEP
SSSEP

Visual Spatial Covert Attention

Motor Imagery: ERD/ERS: Event Related De/Synchronization

Wadsworth BCI
Graz BCI

Bereitschaftspotentials

Selective Attention

P300,N400

Tübingen BCI

Mental Tasks

Operant Conditioning:

Slow Cortical Potentials
ErrP

Berlin BCI

Brain Computer Interfaces - Problem Statement

- Clinical and Physician involvement¹

¹**Yuste2017.**

²**Perdikis2014.**

Brain Computer Interfaces - Problem Statement

- Clinical and Physician involvement¹
- Practical, relevant, and invariant features that convey good-enough information².

¹**Yuste2017.**

²**Perdikis2014.**

Is it possible to analyze and discriminate
electroencephalographic signals by automatic processing the
shape of the waveforms using the
Histogram of Gradient Orientations ?

What we aim to do

- ➊ Construct analyzable 2D-image plots.

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- ① Construct analyzable 2D-image plots.
- ② Adaptation of the SIFT method to EEG time-series

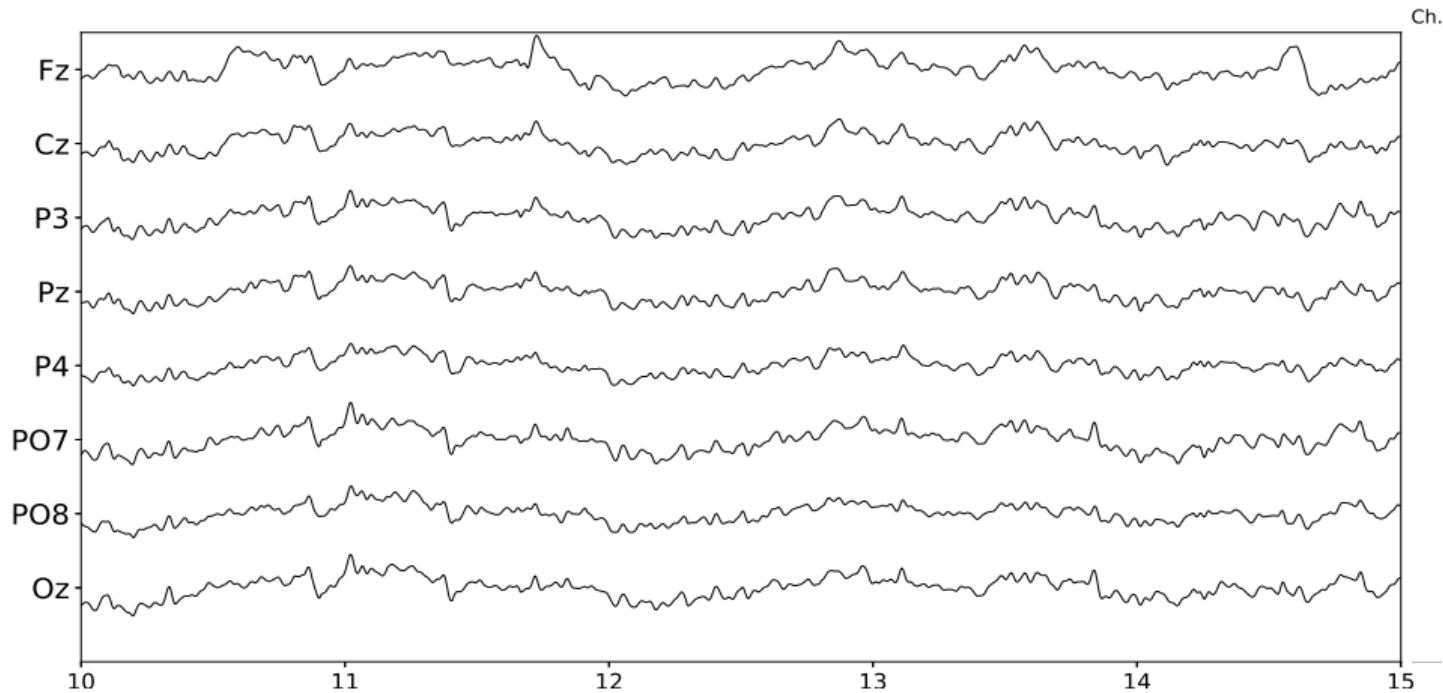
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- ① Construct analyzable 2D-image plots.
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- ③ Feature extraction procedure

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- ① Construct analyzable 2D-image plots.
- ② Adaptation of the SIFT method to EEG time-series
- ③ Feature extraction procedure
- ④ Classification algorithm

Electroencephalography



Sample 8-channel EEG signal obtained from (g.Nautilus, g.Tec, Austria). Voltage in μ V vs time in seconds. Five seconds are displayed.

Waveform-Based Algorithms

- Peak Picking/aEEG/PAA

Waveform-Based Algorithms

- Peak Picking/aEEG/PAA
- Merge of Increasing and Decreasing Sequences

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- Permutation Entropy - PE

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- Permutation Entropy - PE
- Matching Pursuit - MP
- Slope Horizontal Chain Code - SHCC

Proposal

The Histogram of Gradient Orientation

① Signal Preprocessing

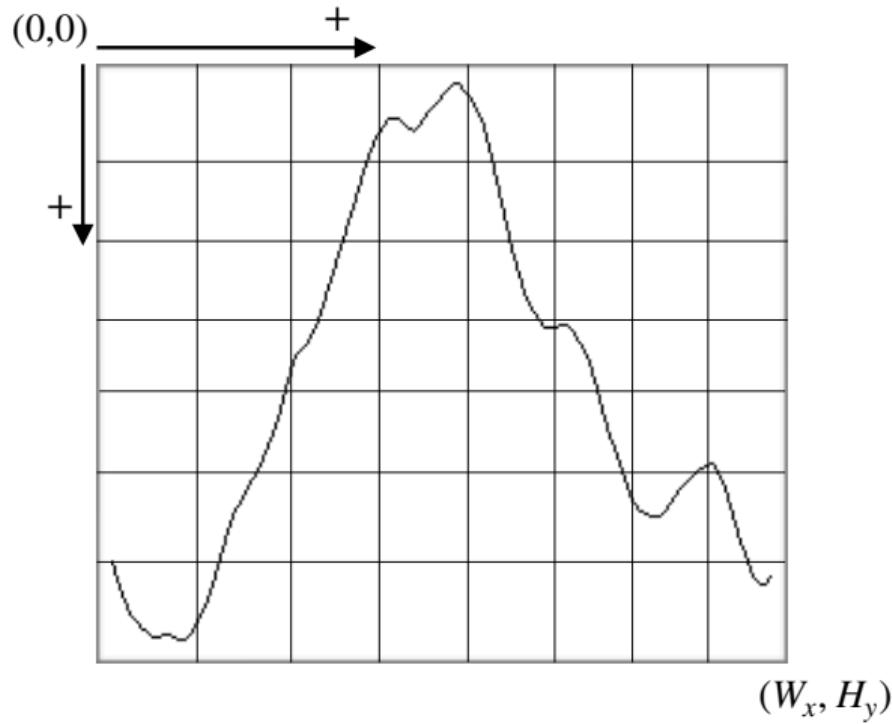
- ① Signal Preprocessing
- ② Signal Segmentation

- ① Signal Preprocessing
- ② Signal Segmentation
- ③ Signal Plotting

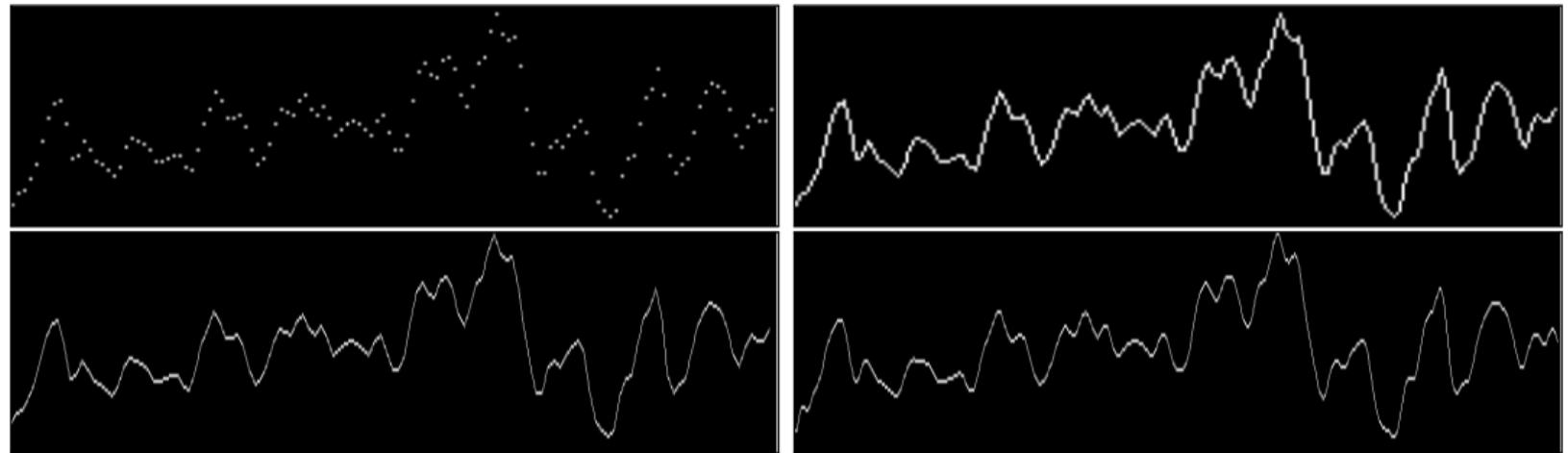
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- ④ Keypoint Localization

- ① Signal Preprocessing
- ② Signal Segmentation
- ③ Signal Plotting
- ④ Keypoint Localization
- ⑤ Calculation of the Histogram of Gradient Orientation

Image Coordinate System

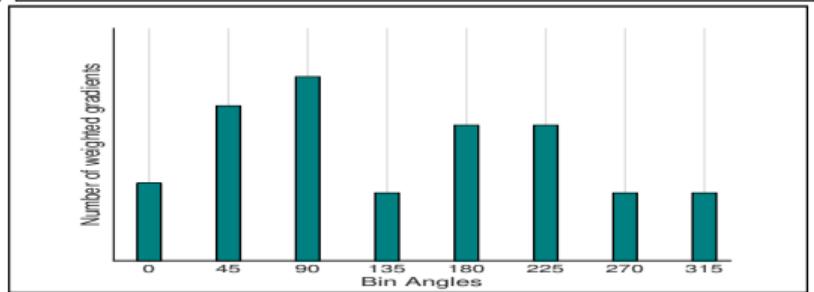
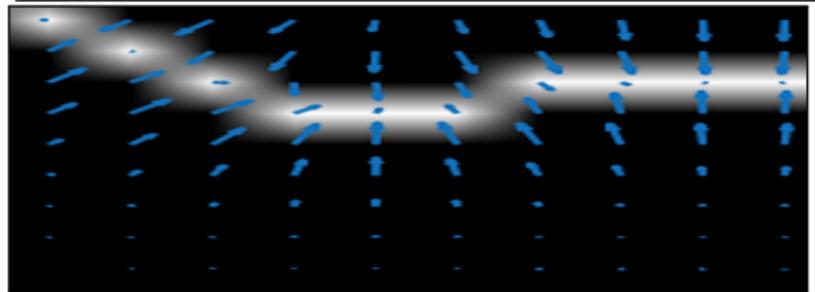
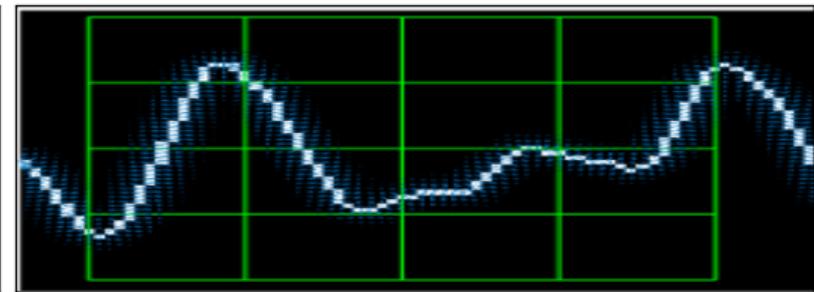
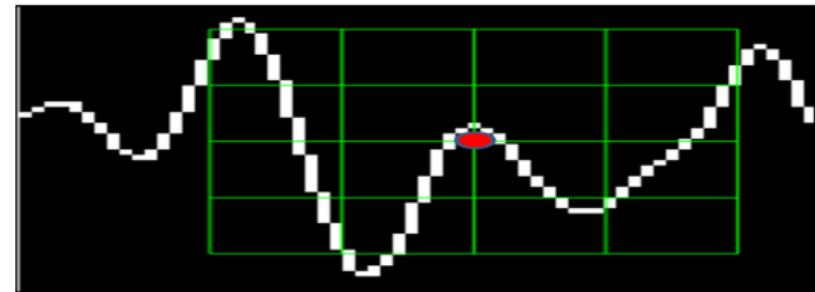


Signal Plotting

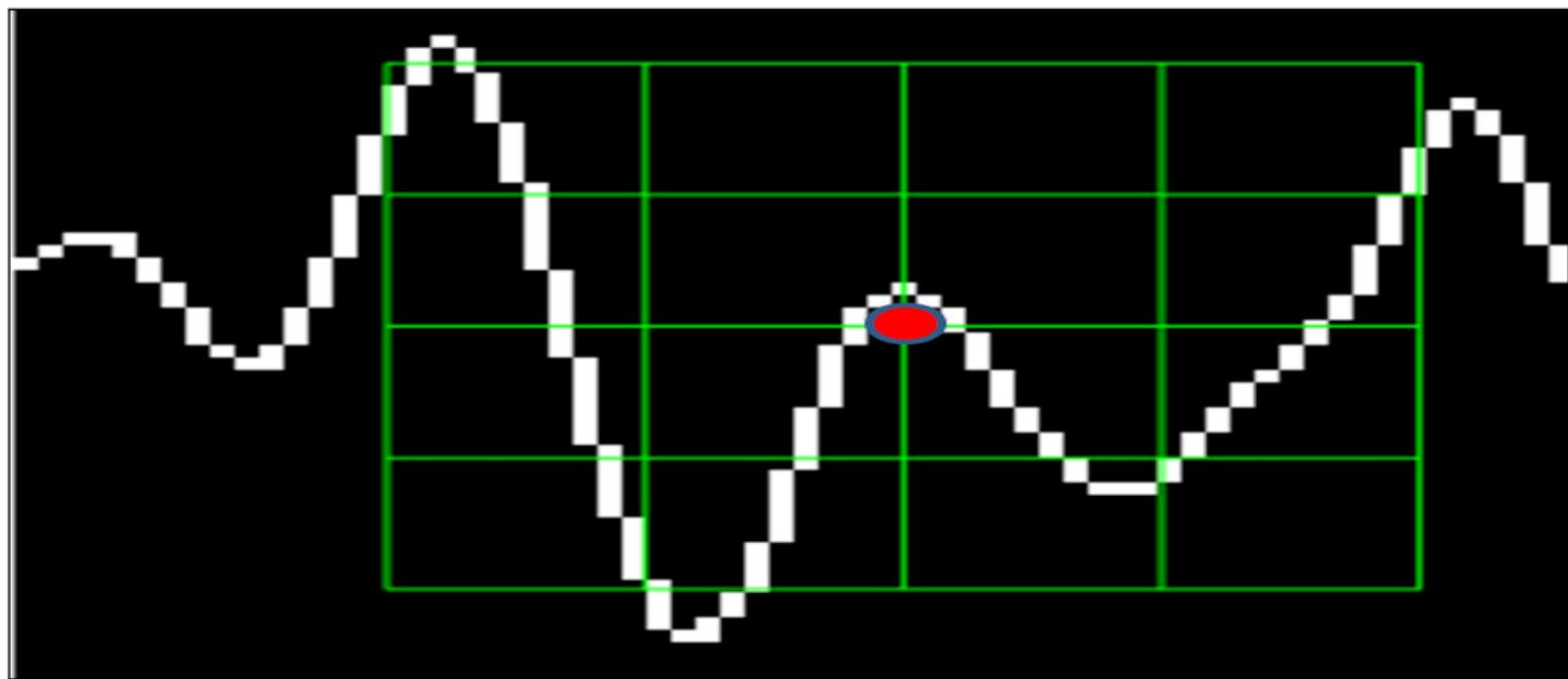


Generated images based on different interpolation schemes.

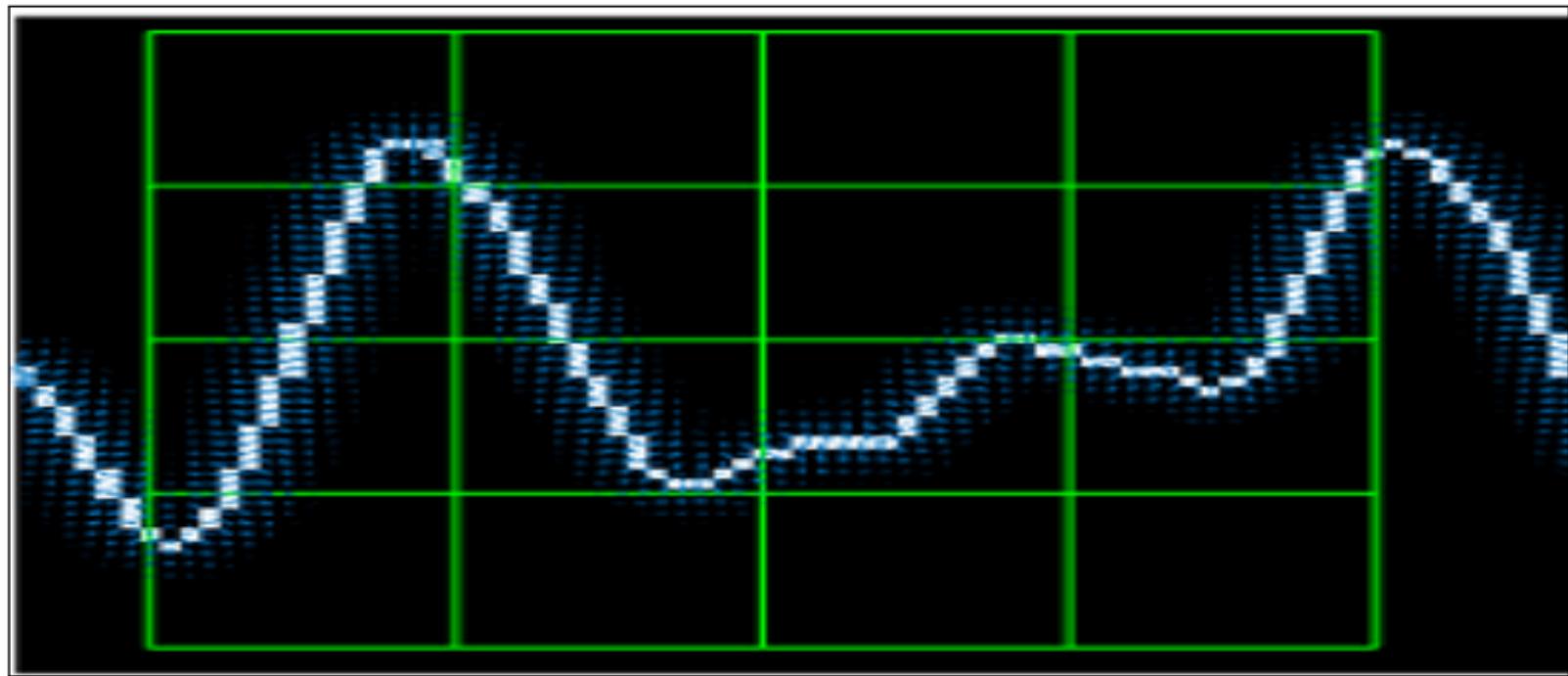
The Histogram of Gradient Orientations



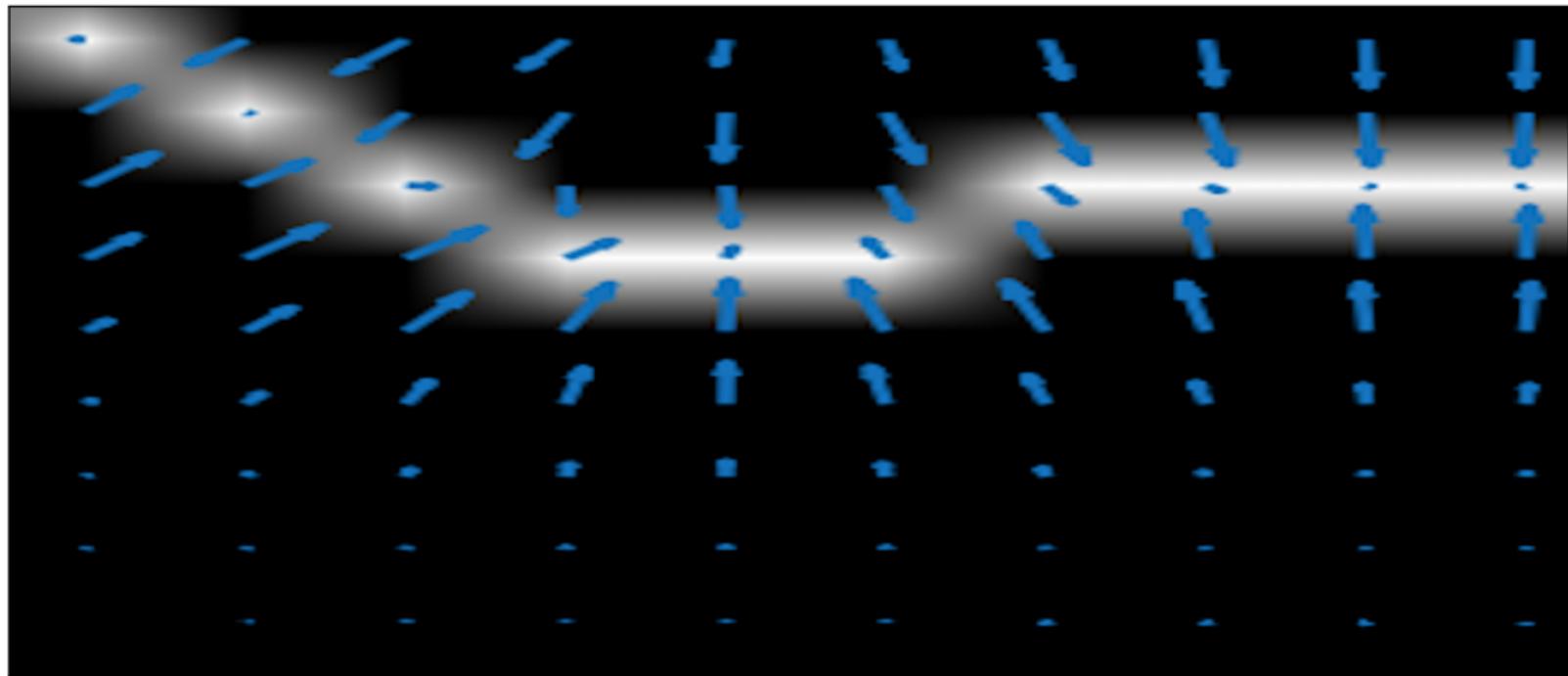
Keypoint Localization



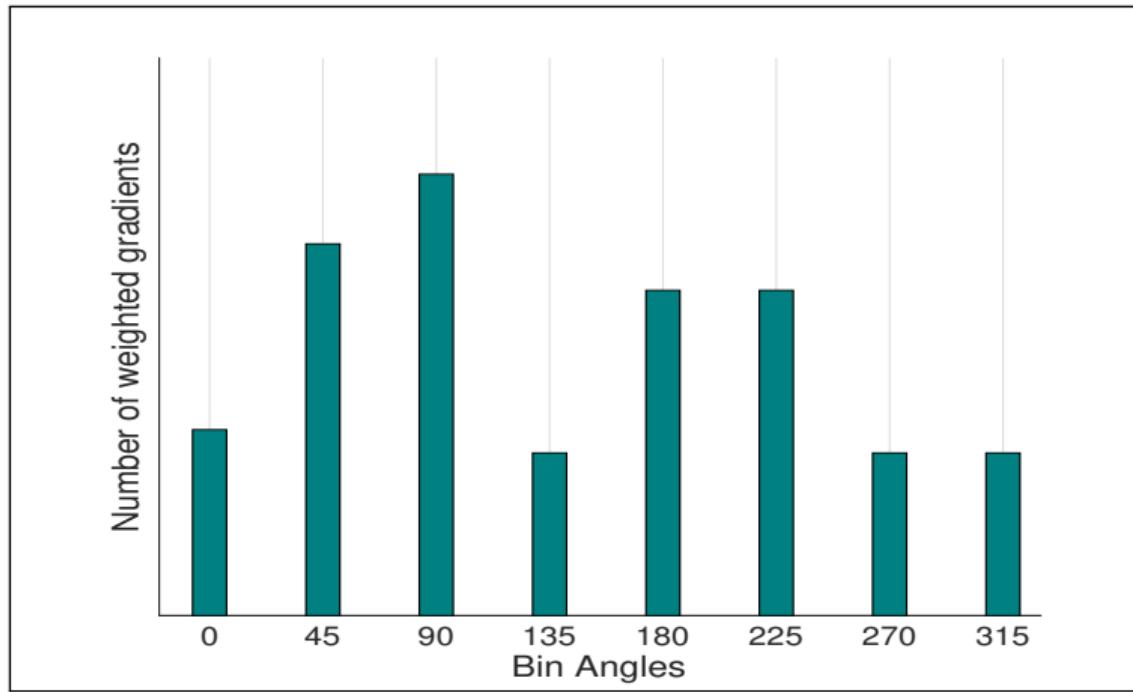
Pixel Gradient Vector Field



Pixel Gradient Vector Field



Orientation histogram



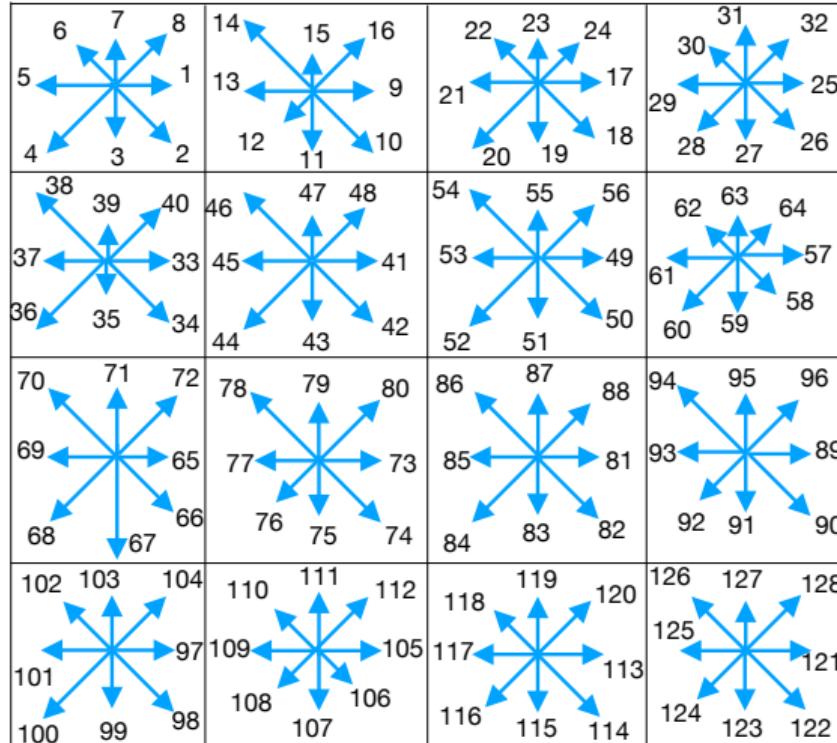
Histogram Calculation

$$h(\theta, i, j) = \sum_{\mathbf{p}} \omega_{\text{ang}}(\angle J(\mathbf{p}) - \theta) \omega_{ij} (\mathbf{p} - \mathbf{kp}) \|J(\mathbf{p})\| \quad (1)$$

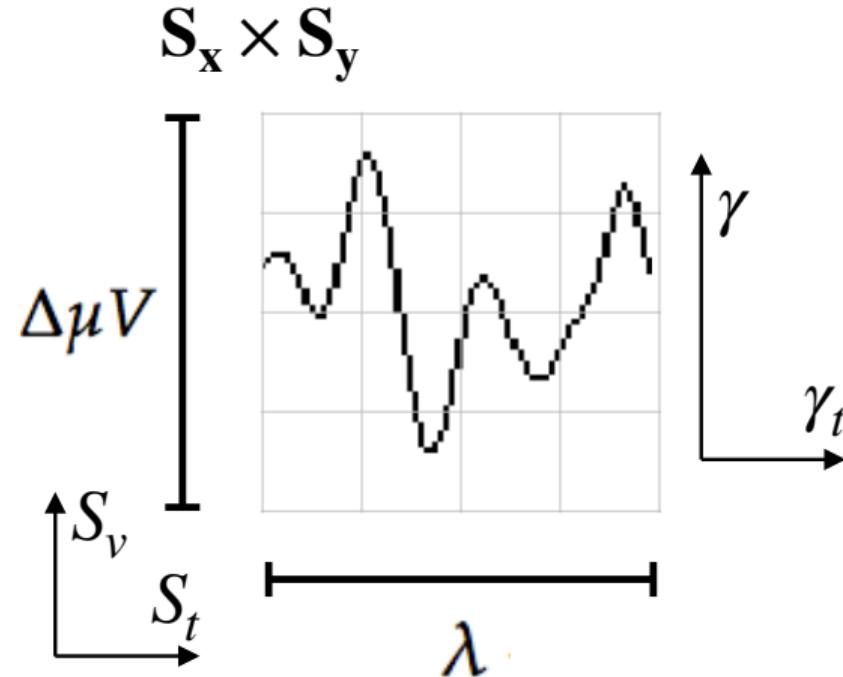
- θ is the angle bin with $\theta \in \{0, 45, 90, 135, 180, 225, 270, 315\}$.
- $i, j = \{0, 1, 2, 3\}$ indexes of the 16 grid blocks.
- \mathbf{kp} is the keypoint center location.
- \mathbf{p} is a pixel from within the patch, centered around \mathbf{kp} .
- $\angle J(\mathbf{p})$ is the angle of the gradient vector.
- $\|J(\mathbf{p})\|$ is the norm of the gradient vector in the pixel \mathbf{p} .
- $\omega_{\text{ang}}(\cdot)$ scalar and $\omega_{ij}(\cdot)$ vector linear interpolation functions³.

³Lowe2004, Vedaldi2010.

Descriptor



Patch Geometry



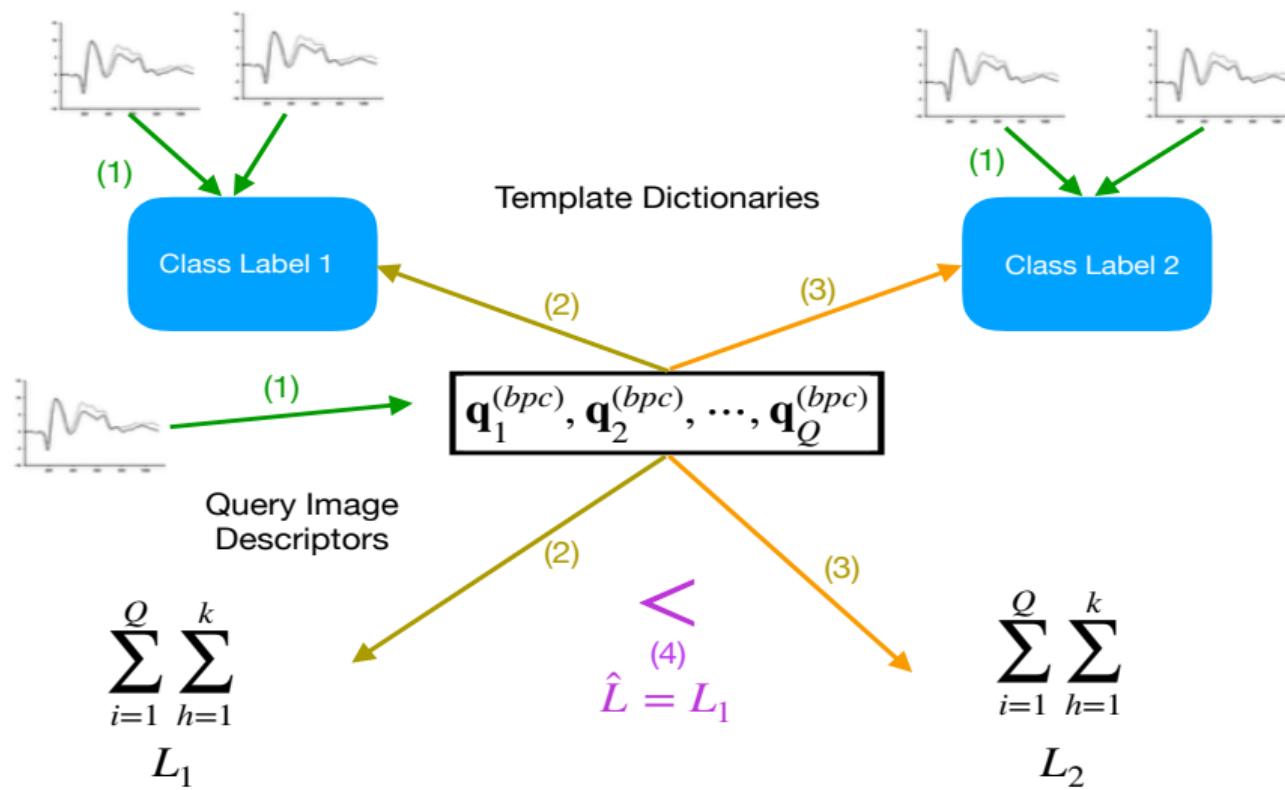
Proposed Classification Method

$$\hat{L} = \arg \min_L \sum_{i=1}^Q \sum_{h=1}^k \left\| \mathbf{q}_i^{(bpc)} - \mathbf{d}_h^{(L,bpc)} \right\|^2 \quad (2)$$

- L class label.
- Q number of descriptors extracted from the query image.
- $\mathbf{q}_i^{(bpc)}$ query descriptors.
- $\mathbf{d}_h^{(L,bpc)}$ neighbors descriptors from template dictionary of class L .
- $\mathbf{d}_h^{(L,bpc)} \in N_T(\mathbf{q}_i^{(bpc)})$.
- $N_T(\mathbf{q}_i^{(bpc)}) = \{\mathbf{d}_h^{(bpc)} \in T_L^{bpc} / \mathbf{d} \text{ is the } k\text{-nearest neighbor of } \mathbf{q}_i^{(bpc)}\}$.
- \hat{L} predicted class label.
- k the number of neighbors to pick from the template⁴.

⁴Boiman2008.

Classification Algorithm



Experimental Validation

Experimental Validation

- Alpha Waves Wiggles

Experimental Validation

- Alpha Waves Wiggles
- μ Rhythm

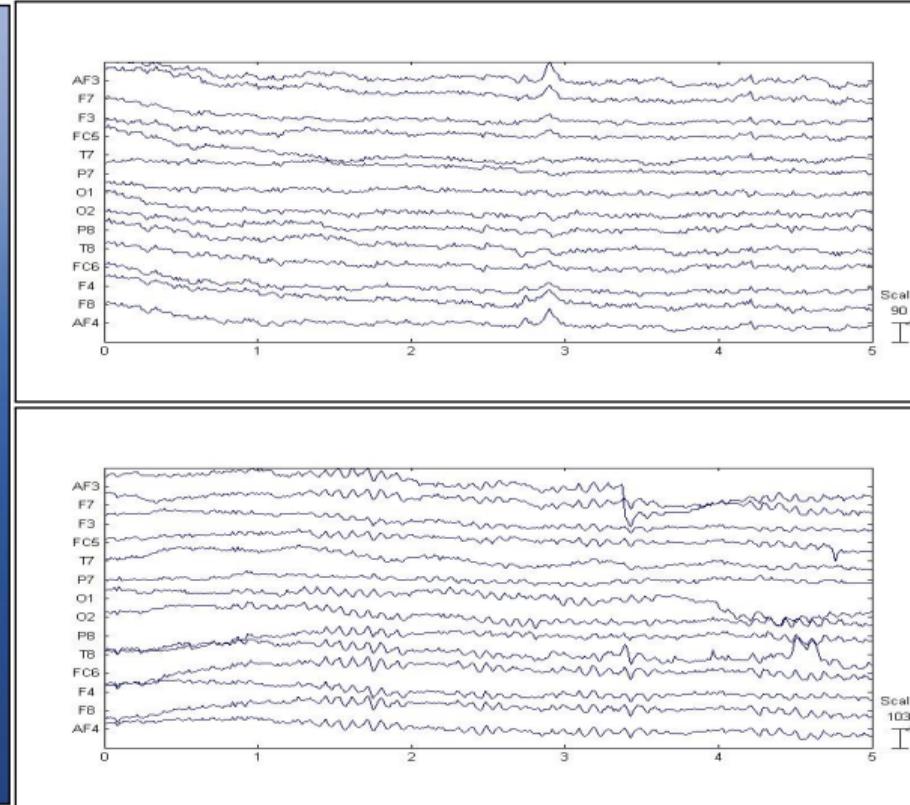
Experimental Validation

- Alpha Waves Wiggles
- μ Rhythm
- The P300 Waveform

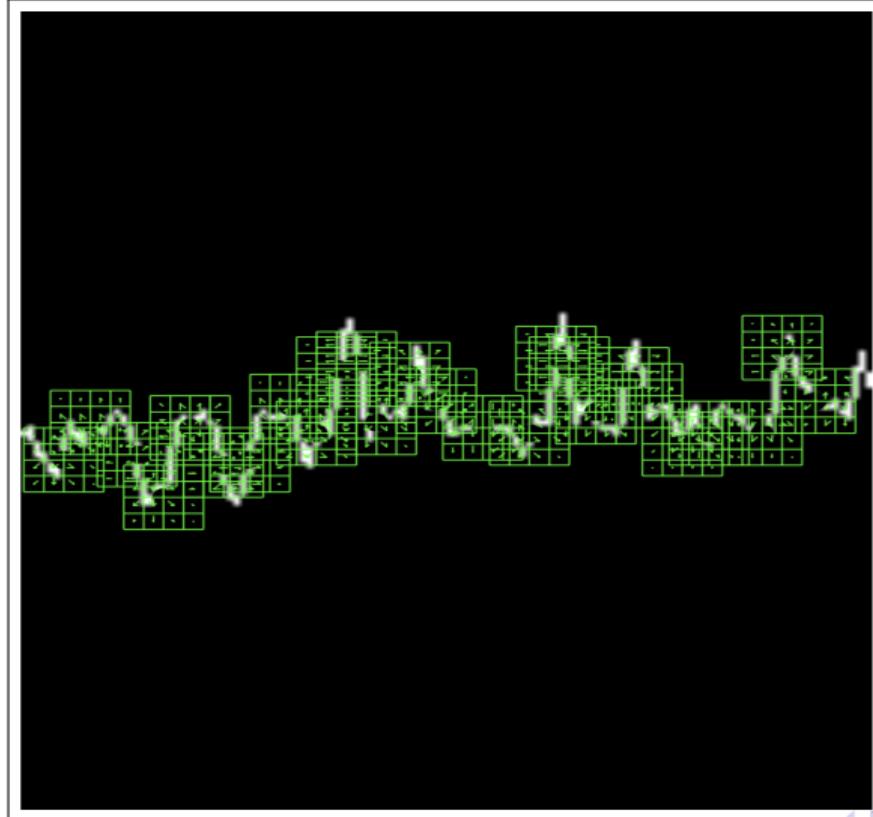
Alpha Waves wiggles

- Dataset I: EPOC Emotiv Consumer Grade EEG Device
 - 128 Hz, 14 channels, 10 subjects, 10 class 1 vs 10 class 2.
- Dataset II: EEG MI NHS PhysioNet
 - 160 Hz, 64 channels, 25 subjects, Run 1 vs Run 2, 60 vs 60.

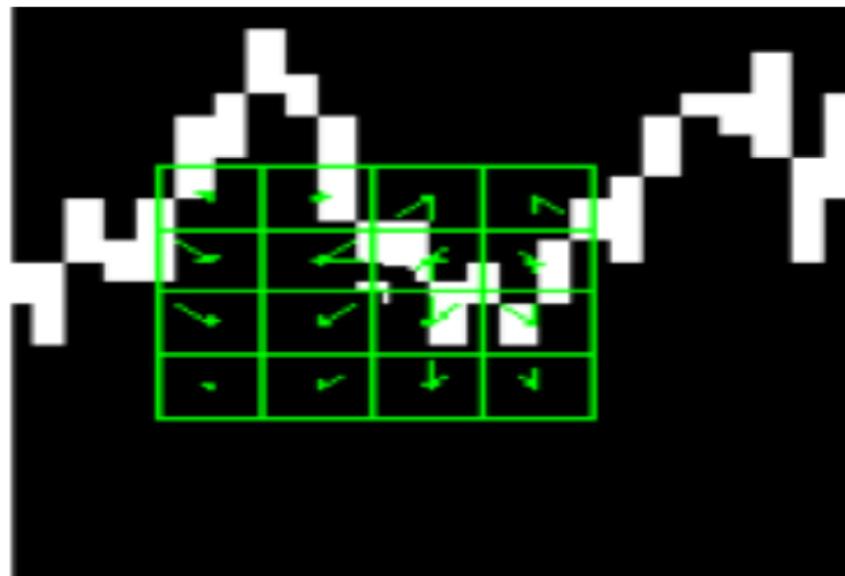
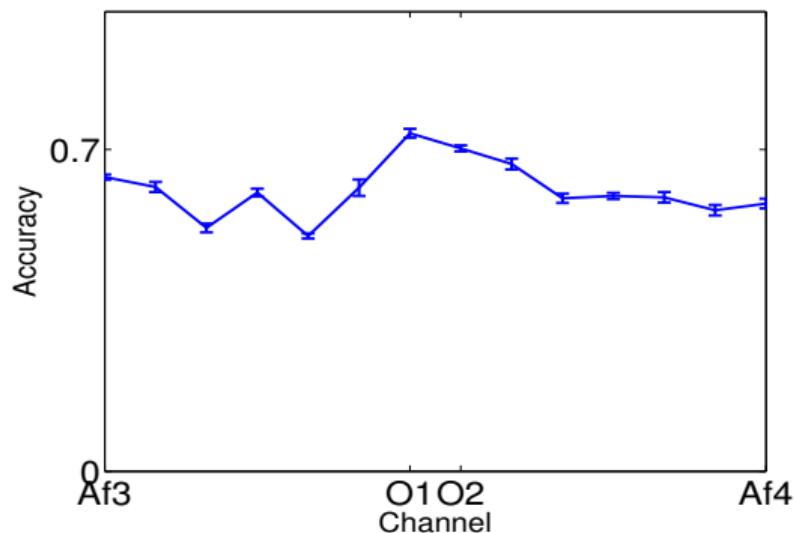
EEG Consumer Grade Digital Device and EEG Signals



Keypoint populations

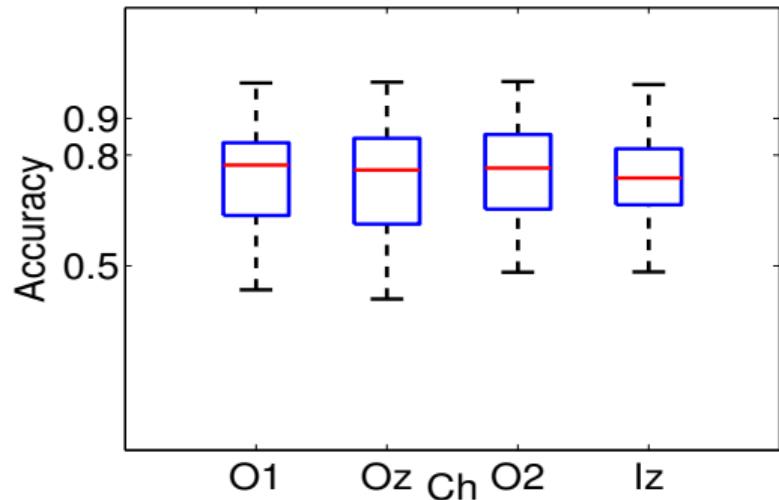
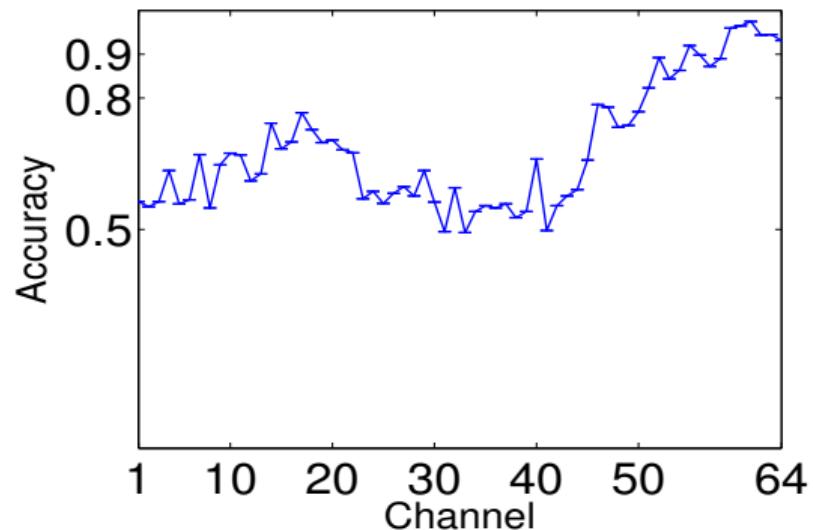


10-Fold Cross Validated Binary Classification Accuracy - Dataset I



The horizontal patch scale S_t and the vertical patch scale S_v are set to 1, whereas γ and γ_t are set to 2, which corresponds to a variation of $\Delta\mu V = 10$ microvolts in the signal amplitude during $\lambda = 0.08$ seconds.

10-Fold Cross Validated Binary Classification Accuracy - Dataset II

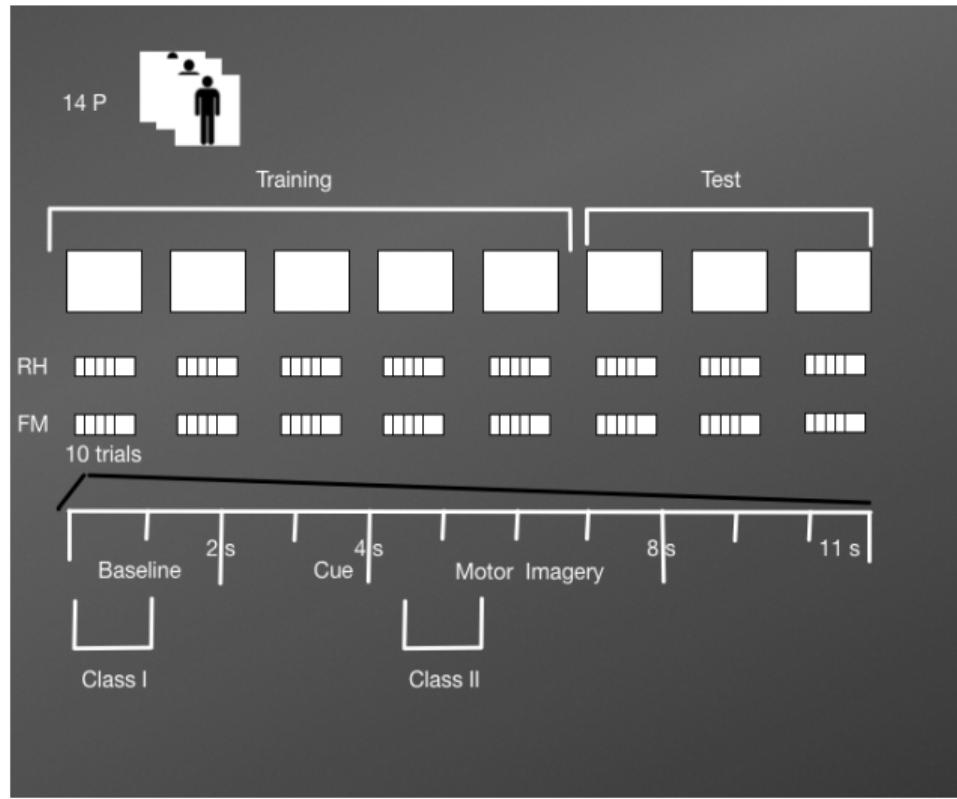


Binary classification accuracy for subject 25 and boxplots obtained for the 25 subjects on 4 occipital channels

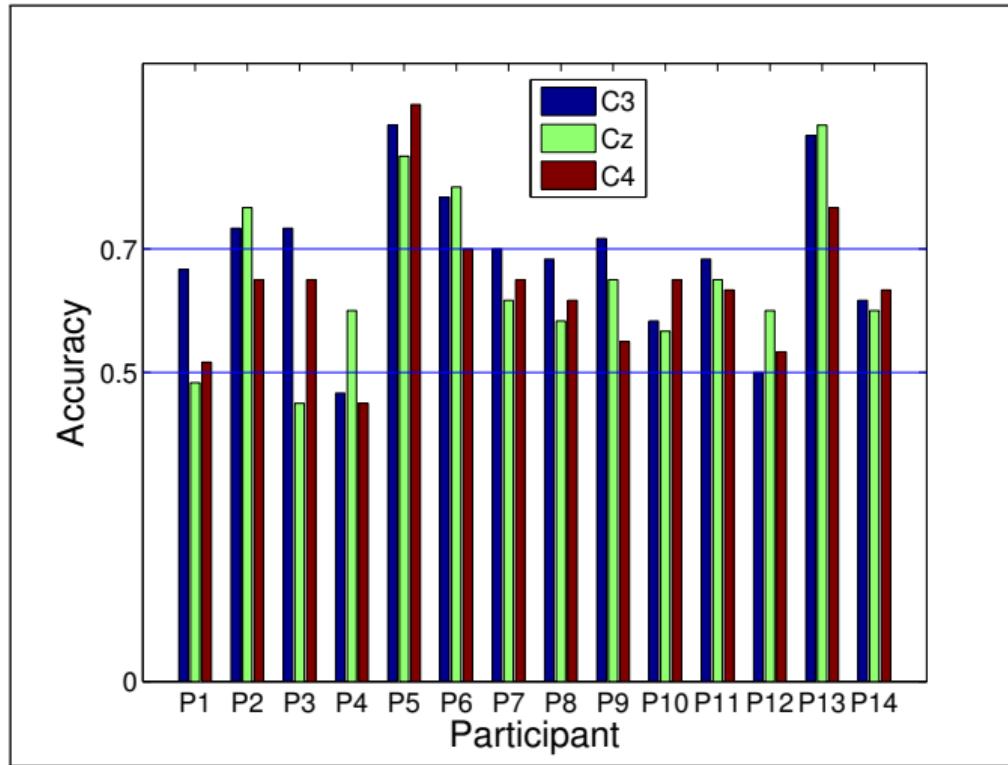
Experimental Validation

μ Rhythm

Dataset 002-2014 BNCI-Horizon 2020 (Steyrl, Scherer et al 2015)

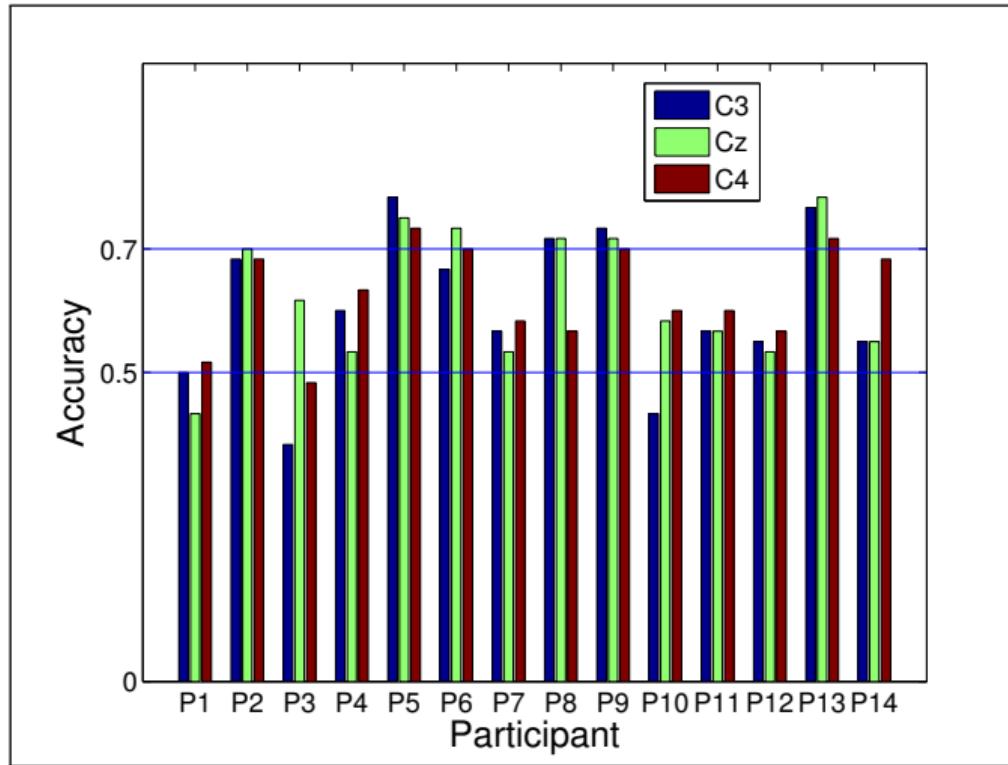


μ Rhythm



Accuracy for the BCI Simulation classifying Baseline vs. RH (Right Hand) motor imagery.

μ Rhythm



Accuracy for the BCI Simulation classifying Baseline vs. FM (Feet Movement) motor imagery.



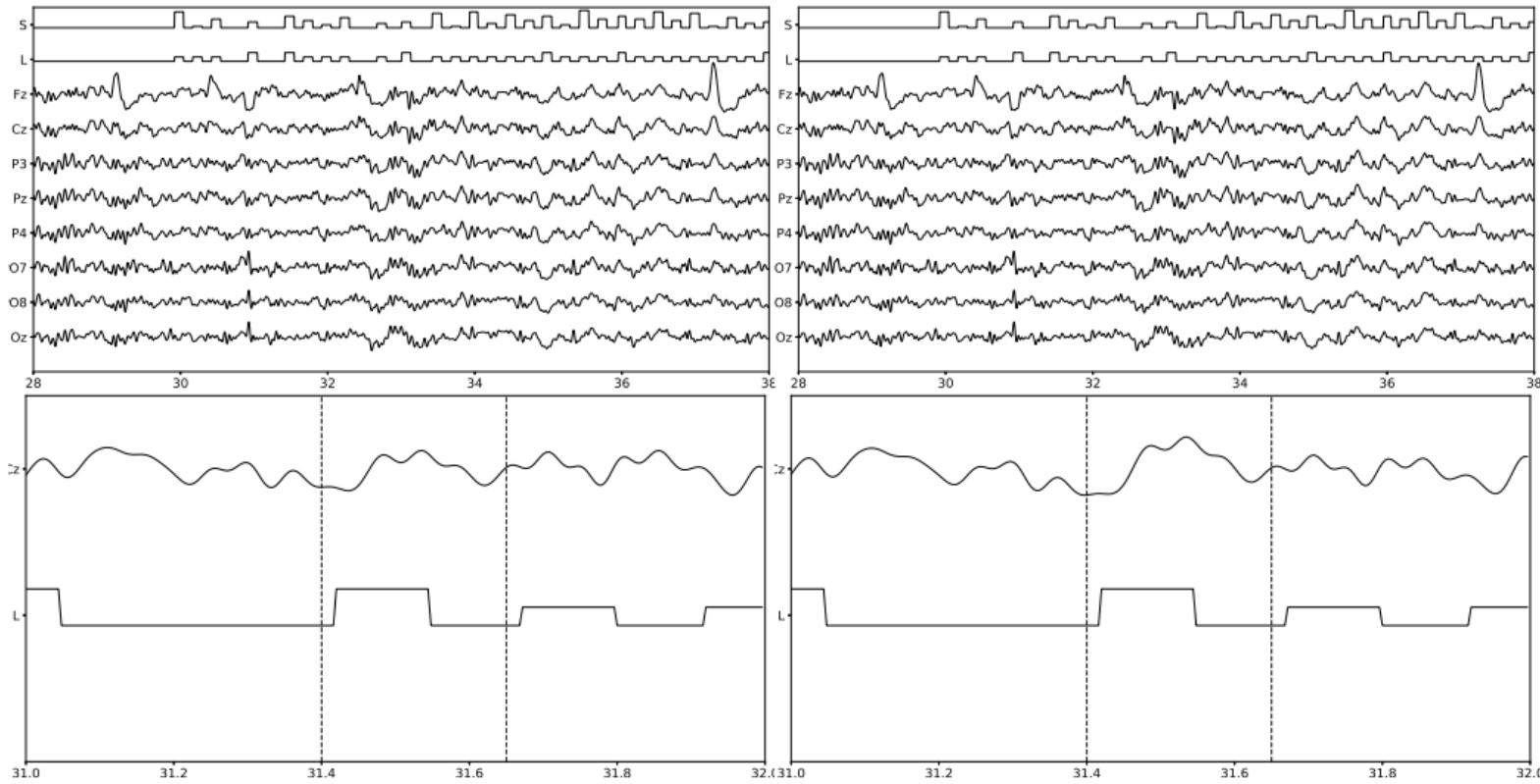
The P300 Waveform

P300-Based Speller Matrix

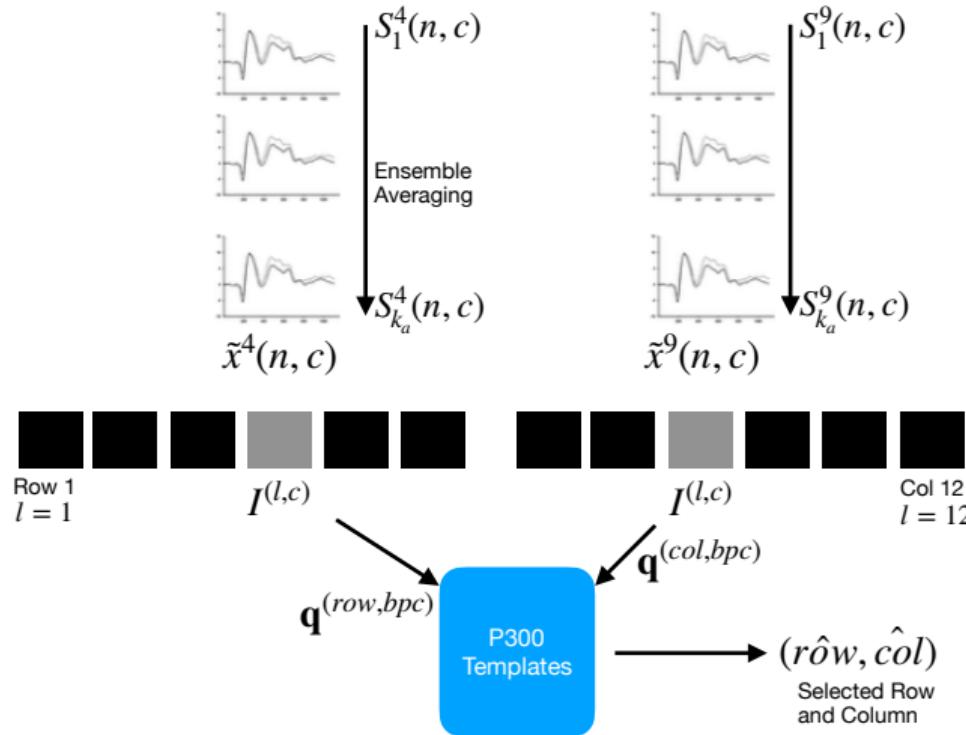


OpenVibe software 6×6 Speller Matrix. Rows and columns flash in random permutations.

The P300 Waveform - Signal Preprocessing



Signal Averaging



P300-Based BCI Speller - Letter Identification

$$\hat{row} = \arg \min_{l \in \{1, \dots, 6\}} \sum_{h=1}^k \left\| \mathbf{q}^{(l, bpc)} - \mathbf{d}_h^{(bpc)} \right\|^2 \quad (3)$$

$$\hat{col} = \arg \min_{l \in \{7, \dots, 12\}} \sum_{h=1}^k \left\| \mathbf{q}^{(l, bpc)} - \mathbf{d}_h^{(bpc)} \right\|^2 \quad (4)$$

- $l \in \{1, \dots, 12\}$ speller matrix row/col index.
- \hat{row} and \hat{col} predicted row and col of the speller matrix.
- $\mathbf{q}^{(l, bpc)}$ query descriptor of matrix index l .
- $\mathbf{d}_h^{(bpc)}$ neighbors descriptors from the template.
- $\mathbf{d}_h^{(bpc)} \in N_T(\mathbf{q}^{(l, bpc)})$.
- \hat{L} predicted class label.
- k the number of neighbors to pick from the template⁵.

⁵Boiman2008.

- Dataset I - P300 ALS Public Dataset

- 8 subjects, 8 channels, $F_s=256$ Hz, 7 words, 5 letters, $ISI=0.125$ s, 10 epochs

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 - 1 subject, null-signals

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- Dataset III - P300 Pseudo-Real Dataset
 - 1 subject, null-signals
- Dataset IV - P300 Dataset IIb BCI Competition II (2003)
 - 1 subject, 64 channels, $F_s=240$ Hz, 73 trials, 42 train and 31 test, $ISI=0.25$ s, 15 epochs

Alternative Methods used for comparison

- Support Vector Machine SVM

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- Matching Pursuit 2 MP-2

Alternative Methods used for comparison

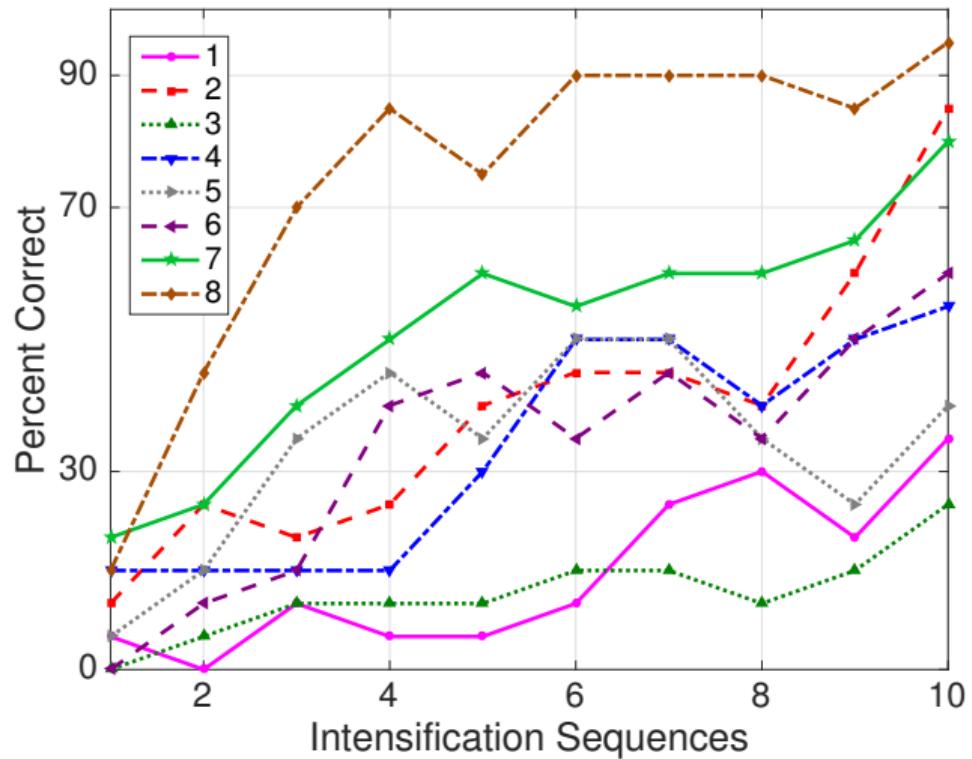
- Support Vector Machine SVM
- Stepwise Linear Discriminant Analysis SWLDA.
- Permutation Entropy
- Matching Pursuit 1 MP-1
- Matching Pursuit 2 MP-2
- Slope Horizontal Chain Code SHCC.

P300 Waveform - Dataset I

Table: Character recognition rates public dataset of ALS patients.

| Participant | bpc | HIST | bpc | Single Channel SVM |
|-------------|-----|------|-----|--------------------|
| 1 | Cz | 35% | Cz | 15% |
| 2 | Fz | 85% | PO8 | 25% |
| 3 | Cz | 25% | Fz | 5% |
| 4 | PO8 | 55% | Oz | 5% |
| 5 | PO7 | 40% | P3 | 25% |
| 6 | PO7 | 60% | PO8 | 20% |
| 7 | PO8 | 80% | Fz | 30% |
| 8 | PO7 | 95% | PO7 | 85% |

Character Identification Rates - Dataset I



The P300 Waveform - Dataset II

Table: Character recognition rates for the Dataset of Healthy volunteers.

| Participant | bpc | HIST | bpc | Single Channel SVM |
|-------------|-----|------|-----|--------------------|
| 1 | Oz | 40% | Cz | 10% |
| 2 | PO7 | 30% | Cz | 5% |
| 3 | P4 | 40% | P3 | 10% |
| 4 | P4 | 45% | P4 | 35% |
| 5 | P4 | 60% | P3 | 10% |
| 6 | Pz | 50% | P4 | 25% |
| 7 | PO7 | 70% | P3 | 30% |
| 8 | P4 | 50% | PO7 | 10% |

Dataset I Multichannel comparison

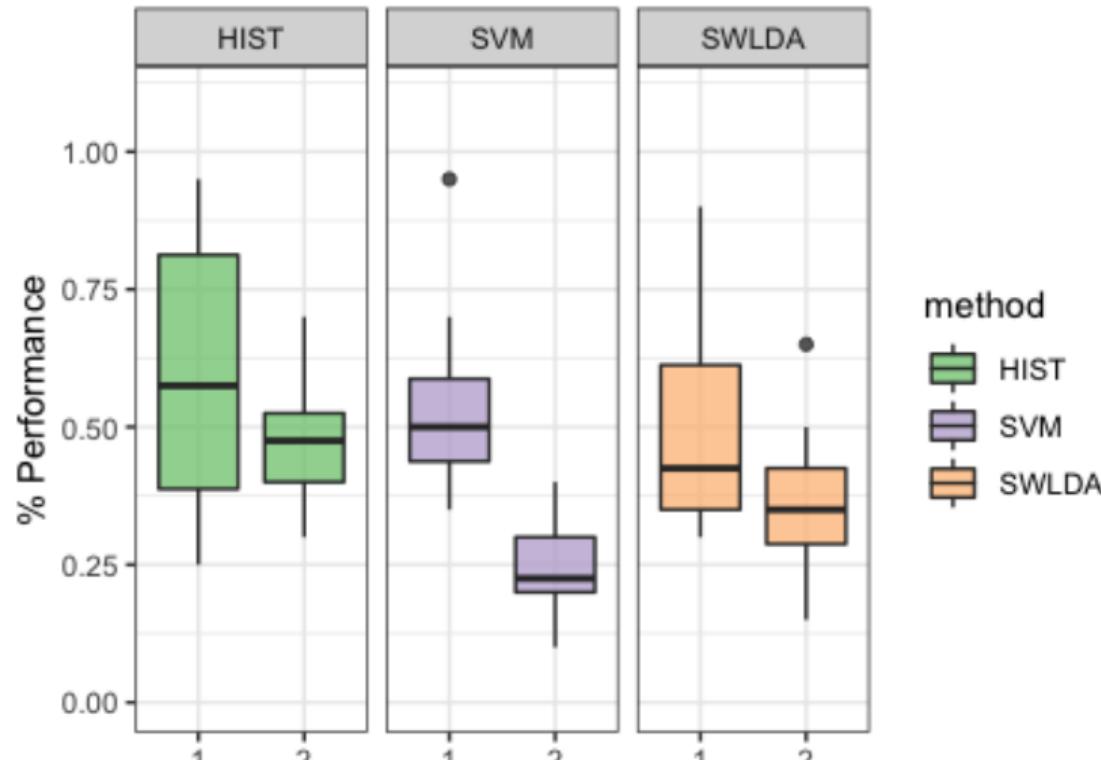
| Participant | <i>bpc</i> for HIST | HIST | Multichannel SWLDA | Multichannel SVM |
|-------------|------------------------|------|--------------------|------------------|
| 1 | Cz | 35% | 45% | 40% |
| 2 | Fz | 85% | 30% | 50% |
| 3 | Cz | 25% | 65% | 55% |
| 4 | PO8 | 55% | 40% | 50% |
| 5 | PO7 | 40% | 35% | 45% |
| 6 | PO7 | 60% | 35% | 70% |
| 7 | PO8 | 80% | 60% | 35% |
| 8 | PO7 | 95% | 90% | 95% |

Dataset II Multichannel Comparison

| Participant | <i>bpc</i> for HIST | HIST | Multichannel SWLDA | Multichannel SVM |
|-------------|------------------------|------|--------------------|------------------|
| 1 | Oz | 40% | 65% | 40% |
| 2 | PO7 | 30% | 15% | 10% |
| 3 | P4 | 40% | 50% | 25% |
| 4 | P4 | 45% | 40% | 20% |
| 5 | P4 | 60% | 30% | 20% |
| 6 | Pz | 50% | 35% | 30% |
| 7 | PO7 | 70% | 25% | 30% |
| 8 | P4 | 50% | 35% | 20% |

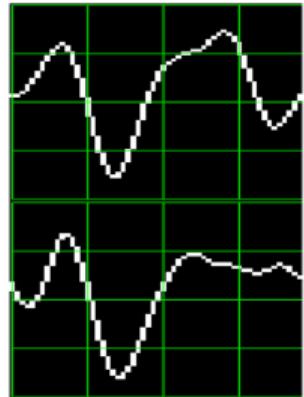
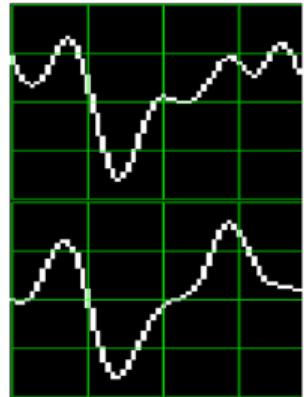
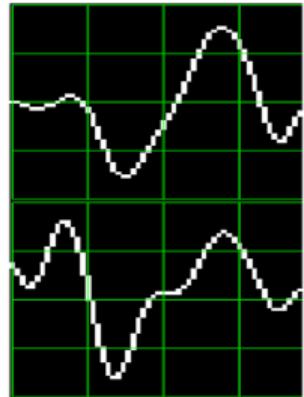
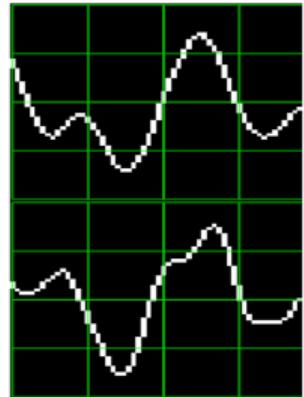
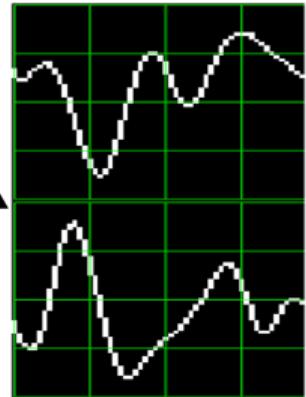
Character Identification Rates for Dataset I and II

Performance by Dataset and Method

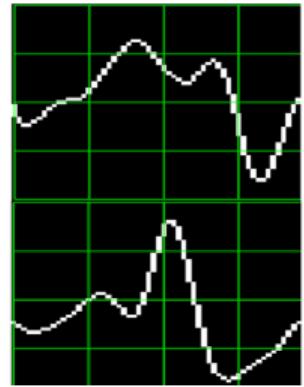
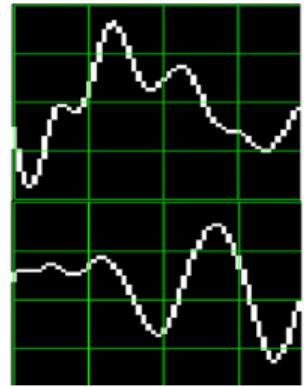
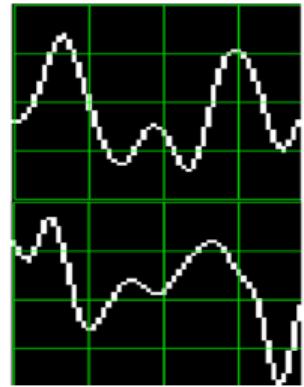
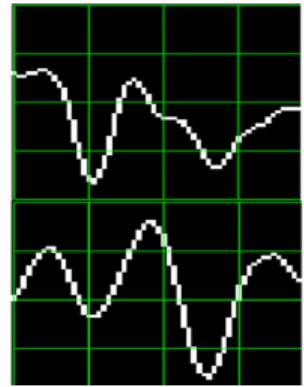
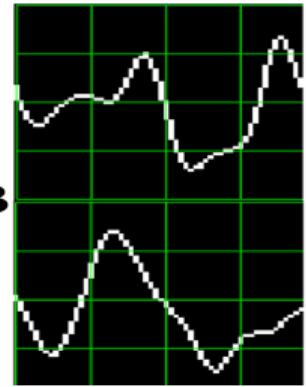


P300 Waveforms for Subject 8 (A) and 3 (B)

A



B



P300 Pseudo-Real Dataset III Performance Results

| Method | <i>bpc</i> | Performance | | |
|--------|------------|--------------|--------------|--------------|
| | | Experiment 1 | Experiment 2 | Experiment 3 |
| MP 1 | PO8 | 67% | 15% | 50% |
| MP 2 | PO7 | 24% | 6% | 10% |
| HIST | PO8 | 91% | 18% | 66% |
| PE | Cz | 61% | 9% | 32% |
| SHCC | P4 | 98% | 31% | 80% |
| SVM | PO8 | 78% | 7% | 53% |

The P300 Wave - Dataset IV BCI Competition 2003

| Method | <i>bpc</i> | Performance |
|---------------|------------|--------------------|
| MP 1 | FC2 | 50% |
| MP 2 | CPz | 22% |
| HIST | Cz | 67% |
| PE | PO8 | 22% |
| SHCC | Cz | 61% |
| SVM | C1 | 32% |

Conclusion

- α and μ waves can be identified by their waveforms.
- Occipital regions more prominent P300 waveforms.
- The stability of ERP transient components in ALS patients
 - Mann-Whitney U Test, $p = 0.46$
- Latency jitter
 - Wilcoxon rank sum test, one tail, $p = 0.0022$
- Amplitude resistance
 - Wilcoxon rank sum test, two tails, $p = 0.17$

Thesis Contributions

- Method to construct analyzable image plots.
- EEG Waveform Feature Extraction Procedure
- SIFT extension and modification: HIST
- Classification algorithm

Practical Contributions

- P300-Dataset on Kaggle
- Registered as EEGWave Code Ocean Reproducible Research Online Platform
- Online Application based on OpenVibe and LSL.
- BCI Online Blog
- Matlab toolbox for Computer Vision EEG Analysis.

- EEG Waveforms can be objectively analyzed.
- Inherent Intelligible System may foster clinical collaboration.

Future Work

- BCI Paradigms Potential Universal Applicability
- Multichannel extension.
- Keypoint localization.
- Neuroimaging.

Questions?

Thank you very much

Preprocessing steps

- Notch filter:
- Band-pass filter
- Decimation or Downsizing:
- Segmentation
- Baseline Removal
- Artifact Rejection
- Spatial Filter

An excellent review can be found here⁶.

⁶Simons2016.

Histogram of Gradient Orientation - Trilinear Interpolation

$$\omega_{ij}(\mathbf{v}) = \omega\left(\frac{5 v_x}{\Delta_s S_t} - x_i\right) \omega\left(\frac{5 v_y}{\Delta_s S_v} - y_i\right) \quad (5)$$

$$\omega_{ang}(\alpha) = \sum_{r=-1}^1 \omega\left(\frac{8\alpha}{2\pi} + 8r\right) \quad (6)$$

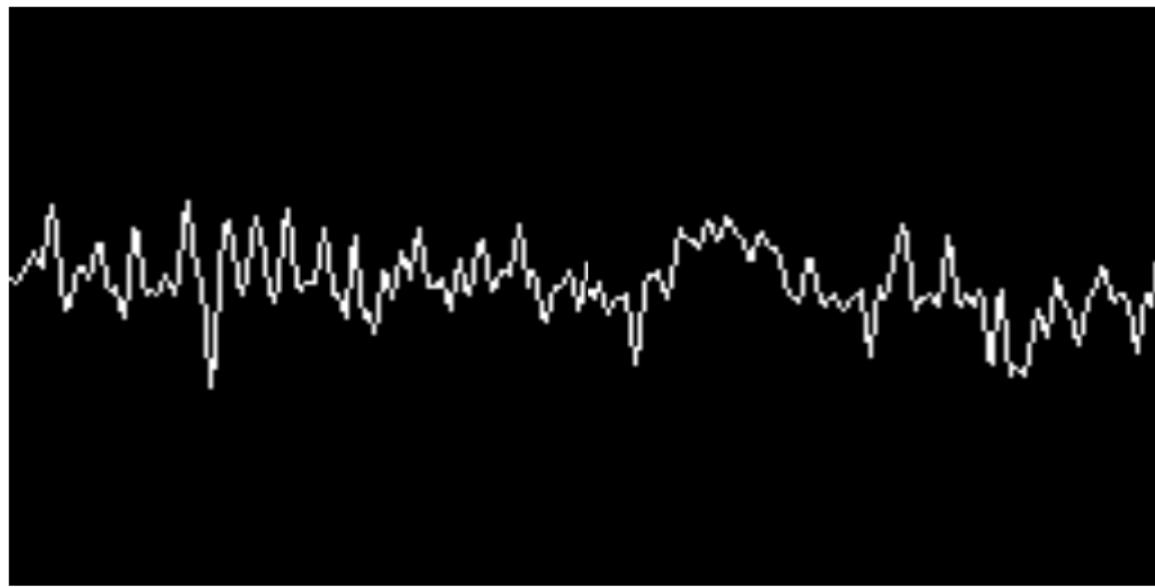
EEG Signal Plot - Zero Level and Standardization

$$\tilde{x}(n, c) = \frac{x(n, c) - \bar{x}(c)}{\hat{\sigma}(c)} \quad (7)$$

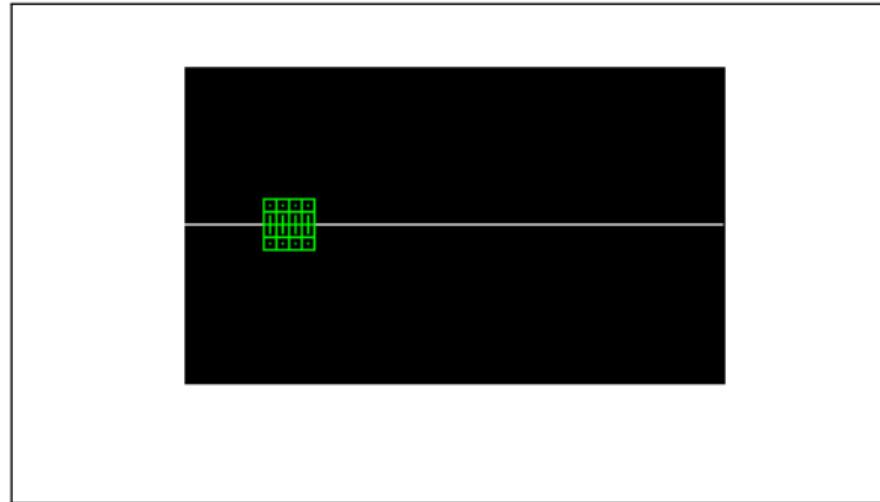
$$z(c) = \left\lfloor \frac{\max_n \tilde{x}(n, c) - \min_n \tilde{x}(n, c)}{2} \right\rfloor - \left\lfloor \frac{\max_n \tilde{x}(n, c) + \min_n \tilde{x}(n, c)}{2} \right\rfloor \quad (8)$$

EEG Signal Plot

$$\mathcal{I}^{(c)}(z_1, z_2) = \begin{cases} 255 & \text{if } z_1 = \gamma_t \text{ and } z_2 = \lfloor \gamma \tilde{x}(n, c) \rceil + z(c) \\ 0 & \text{otherwise} \end{cases} \quad (9)$$

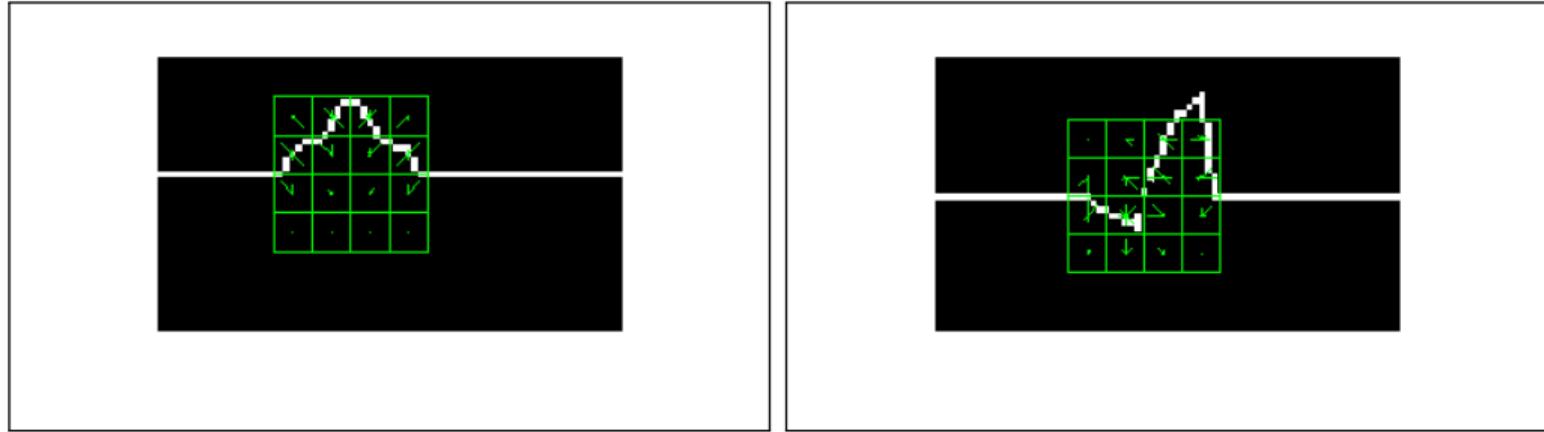


SIFT Descriptors



SIFT Descriptor $[z_1, z_2, \theta, \sigma]$ where (z_1, z_2) are the 2D coordinates where the *Keypoint* is located, θ is the descriptor general orientation and σ is the descriptor size.

SIFT Descriptors



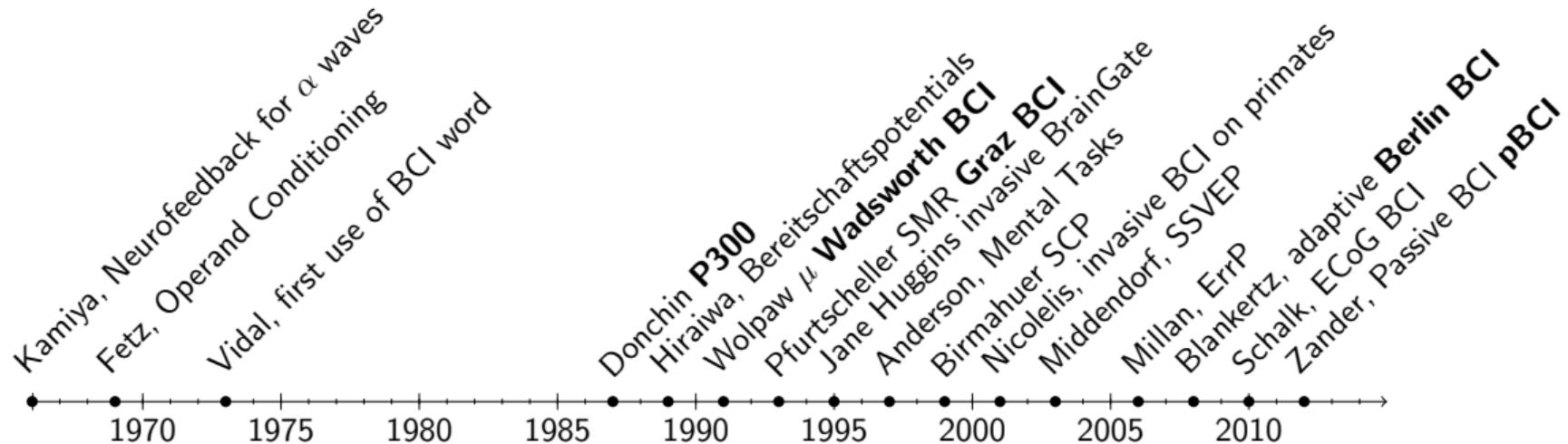
Sample Descriptors from artificial signals.

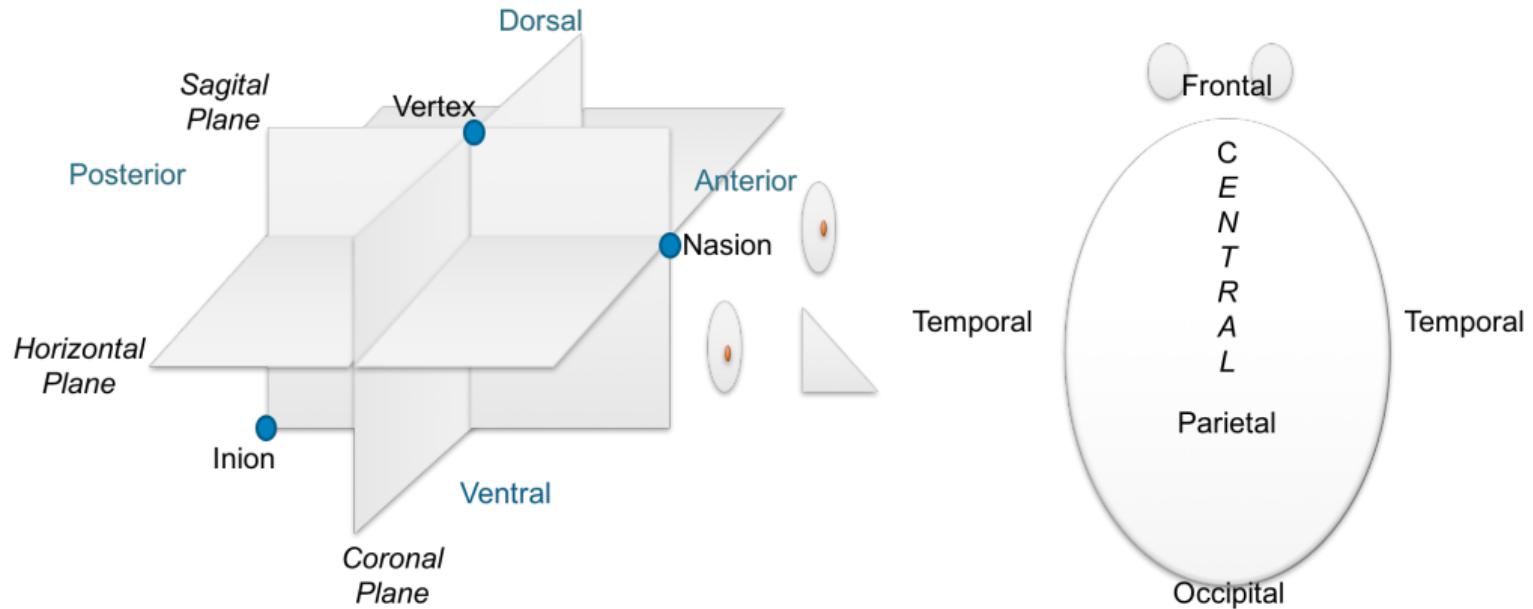
SIFT Descriptors

| | | | | | | | | | | | | | | | | | | | |
|----|----|----|----|-----|-----|-----|-----|-----|-----|-----|-----|----|----|----|----|----|---|---|---|
| 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 |
| 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 |
| 17 | 22 | 22 | 17 | 173 | 173 | 173 | 173 | 40 | 51 | 51 | 40 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 |
| 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 |
| 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 |
| 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 |
| 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 |
| 0 | 0 | 0 | 0 | 40 | 51 | 51 | 40 | 173 | 173 | 173 | 173 | 17 | 22 | 22 | 22 | 17 | 0 | 0 | 0 |
| 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 |

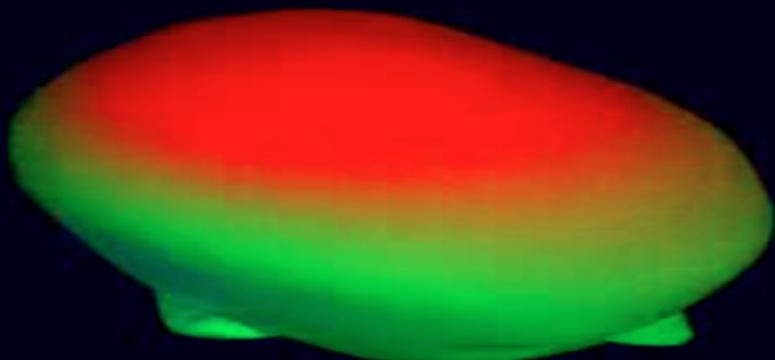
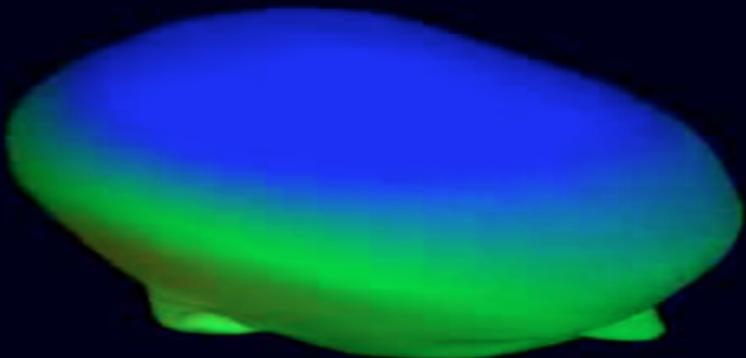
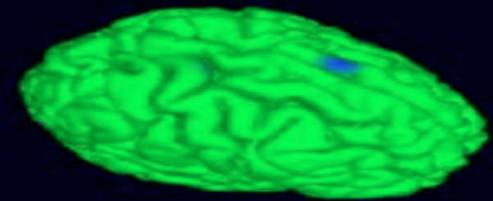
Sample descriptor values of the given patch.

Brain Computer Interfaces - Chronology



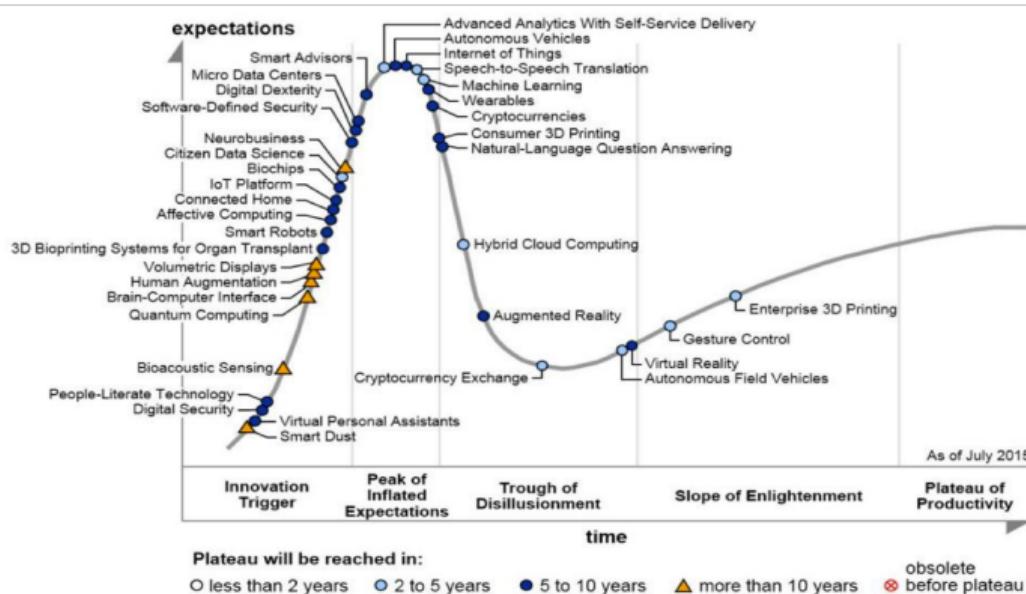


Neuronal Planes regularly used in neuroscience research. In BCI they are used to understand electrode location and spatial filters.





Digital and wearable electroencephalographs.



<http://www.gartner.com/newsroom/id/3412017>

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► Human Augmentation: Cyborgs

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Exoskeletons
Assistive Devices

► BioChips

Cochlear Implant

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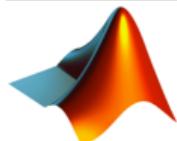
NeuroSky



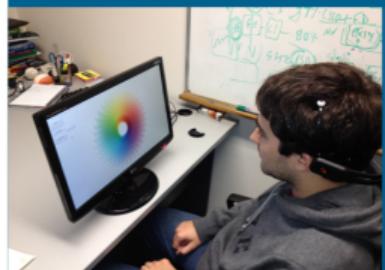
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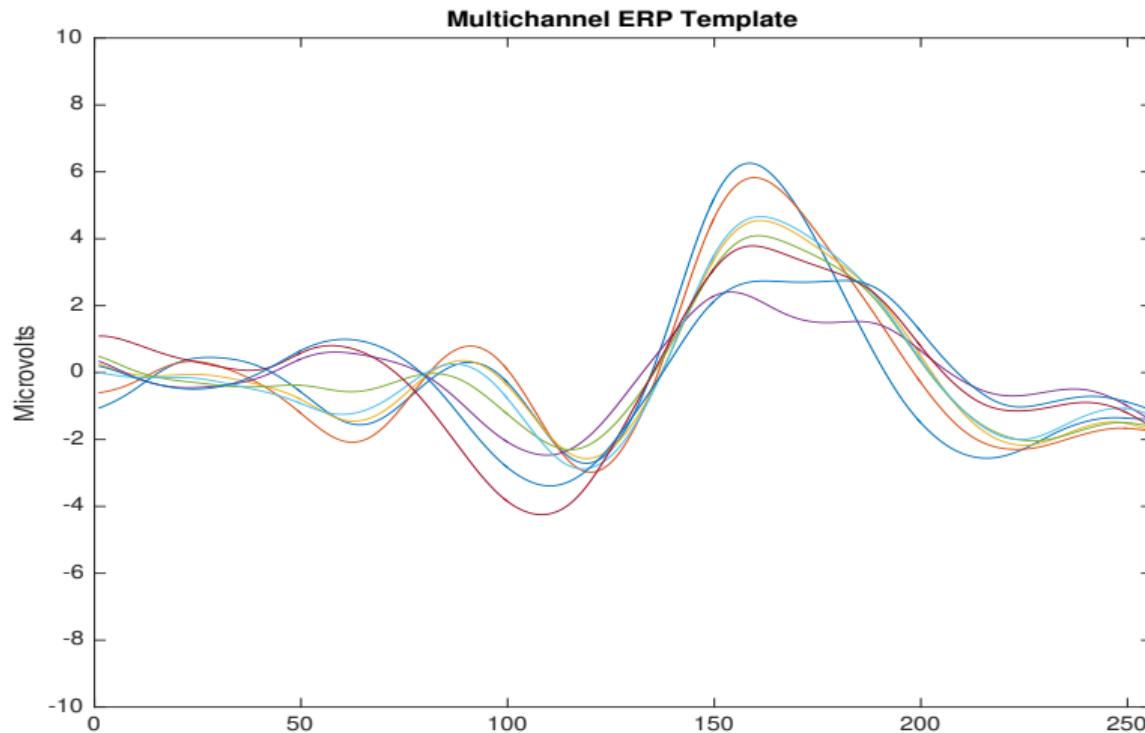
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29, 30 & 31 October

The P300 Wave

Additionally, the stability of the P300 component waveform has been extensively studied in patients with ALS⁷ where it was found that these patients have a stable P300 component, which were also sustained across different sessions. In line with these results we do not find evidence of a difference in terms of the performance obtained by analyzing the waveforms, by using the HIST method, for the group of patients with ALS and the healthy group of volunteers (Mann-Whitney U Test, $p = 0.46$). Particularly, the best performance is obtained for a subject from the ALS dataset for which, based on visual observation, the shape of they P300 component is consistently identified.

⁷Sellers and Emanuel Donchin 2006, Tomohiro Madarame 2008, Nijboer 2009, Mak 2012, McCane 2015.

P300 ERP Template for Dataset III



Performance Curves for Dataset IV (Dataset IIb BCI Competition II 2003)

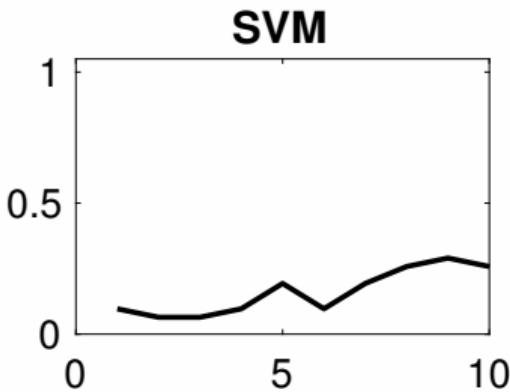
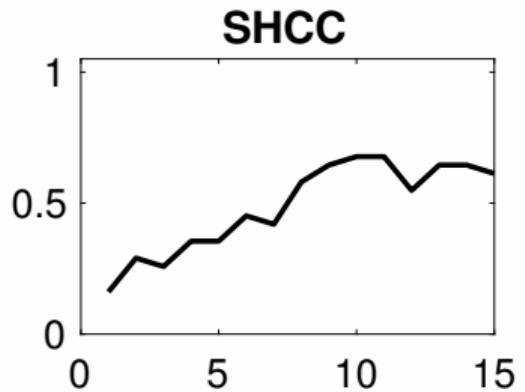
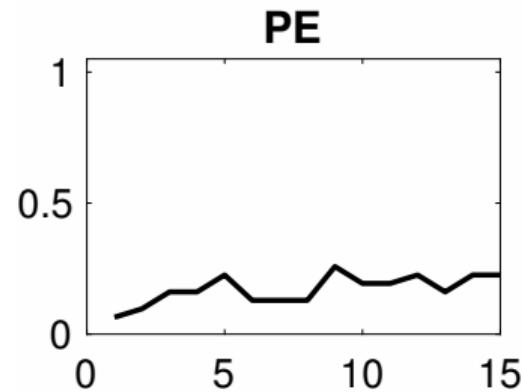
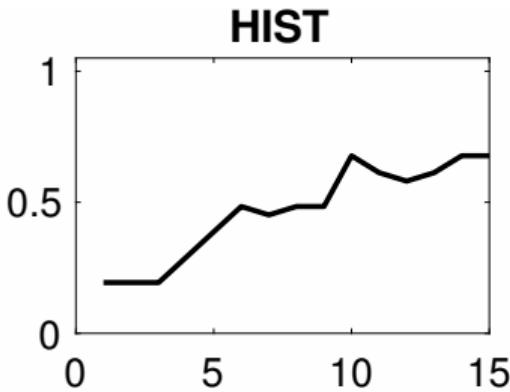
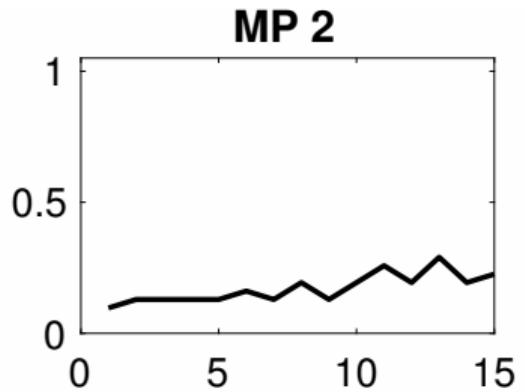
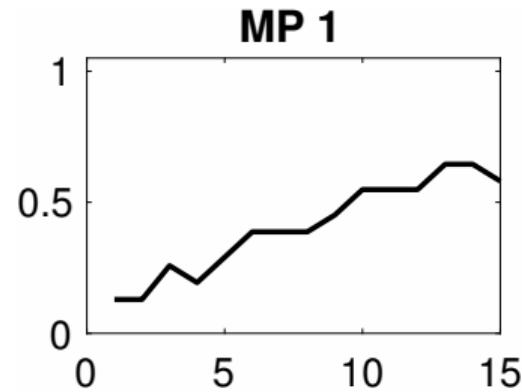


Table: EEG waveforms descriptions found in the surveyed literature.

| Method | Phenomena |
|---------------------------------------|---------------------------|
| Positive Rounded Component | α -Waves, Epilepsy |
| Rising and Falling Phase | Epilepsy |
| Terminal plateau | Epilepsy |
| Ripples and Wiggles | Epilepsy, ERP |
| Sinusoidal Shape | Epilepsy |
| Sawtooth | Motor Imagery, Sleep |
| Sharpness or Spike-like | Epilepsy |
| Rectangular | Epilepsy |
| Line length | Anomaly Detection |
| Root Mean Square | Anomaly Detection |
| Wicket Shape | Epilepsy |
| Peak and Trough Sharpness Ratio | Epilepsy |
| Symmetry between rise and decay phase | Epilepsy |
| Slope Ratio | Sleep |

Table: EEG waveforms descriptions found in the surveyed literature.

| Method | Phenomena |
|---|----------------------|
| Positive/Negative Peak Amplitude | ERP |
| Positive vs Negative Ratio | Sleep K-Complex |
| Base-to-Peak Amplitude | ERP |
| Peak-to-Peak Amplitude | ERP |
| Positive/Negative Peak Latency | ERP |
| Integrated Activity | ERP, Epilepsy, ICU |
| Cross-Correlation | ERP, Epilepsy, Sleep |
| Coupling | |
| Cross Frequency, Phase-Amplitude, Phase-Phase | Sleep |
| Period Amplitude Analysis | ERP, Epilepsy |