

# Histogram of Gradient Orientations of Signal Plots applied to P300 Detection

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## 2 ABSTRACT

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4 The analysis of Electroencephalographic (EEG) signals is of ulterior importance to aid in the  
5 diagnosis of mental disease and to increase our understanding of the brain. Traditionally, clinical  
6 EEG has been analyzed in terms of temporal waveforms, looking at rhythms in spontaneous  
7 activity, subjectively identifying troughs and peaks in Event-Related Potentials (ERP), or by  
8 studying graphoelements in pathological sleep stages. Additionally, the discipline of Brain  
9 Computer Interfaces requires new methods to decode patterns from non-invasive EEG signals.  
10 This field is developing alternative communication pathways to transmit volitional information  
11 from the Central Nervous System. The technology could potentially enhance the quality of life  
12 of patients affected by neurodegenerative disorders and other mental illness. This work mimics  
13 what electroencephalographers have been doing clinically, visually inspecting and categorizing  
14 phenomena within the EEG by the extraction of features from images of signal plots. These  
15 features are constructed based on the calculation of histograms of oriented gradients from pixels  
16 around the signal plot. It aims to provide a new objective framework to analyze, characterize and  
17 classify EEG signal waveforms. The feasibility of the method is outlined by detecting the P300, an  
18 ERP elicited by the oddball paradigm of rare events, and implementing an offline P300-based BCI  
19 Speller. The validity of the proposal is shown by offline processing a public dataset of Amyotrophic  
20 Lateral Sclerosis (ALS) patients and an own dataset of healthy subjects.

21 **Keywords:** **electroencephalography, histogram of gradient orientations, brain-computer interfaces, P300, SIFT, amyotrophic lateral**  
22 **sclerosis, naive-bayes near neighbours, waveforms**

## 1 INTRODUCTION

23 Although recent advances in neuroimaging techniques, particularly radio-nuclear and radiological  
24 scanning methods (Schomer and Silva, 2010), have diminished the prospects of the traditional  
25 Electroencephalography (EEG), the advent and development of digitized devices has impelled for a  
26 revamping of this hundred years old technology. Their versatility, ease of use, temporal resolution, ease of  
27 development and production, and its proliferation as consumer devices, are pushing EEG to become the  
28 de-facto non invasive portable or ambulatory method to access and harness brain information (De Vos and  
29 Debener, 2014).

30 A key contribution to this expansion has been the field of Brain Computer Interfaces (BCI) (Wolpaw and  
31 E., 2012) which is the pursuit of the development of a new channel of communication particularly aimed to  
32 persons affected by neurodegenerative diseases.

33 One noteworthy aspect of this novel communication channel is the ability to transmit information from  
34 the Central Nervous System (CNS) to a computer device and from there use that information to control a  
35 wheelchair (Carlson and del R. Millan, 2013), as input to a speller application (Guger et al., 2009), in a  
36 Virtual Reality environment (Lotte et al., 2013) or as aiding tool in a rehabilitation procedure (Jure et al.,  
37 2016). The holly grail of BCI is to implement a new complete and alternative pathway to restore lost  
38 locomotion (Wolpaw and E., 2012).

39 EEG signals are remarkably complex and have been characterized as a multichannel non-stationary  
40 stochastic process. Additionally, they have high variability between different subjects and even between  
41 different moments for the same subject, requiring adaptive and co-adaptive calibration and learning  
42 procedures (Clerc et al., 2016). Hence, this imposes an outstanding challenge that is necessary to overcome  
43 in order to extract information from raw EEG signals.

44 BCI has gained mainstream public awareness with worldwide challenge competitions like  
45 Cybathlon (Riener and Seward, 2014; Novak et al., 2018) and even been broadcasted during the inauguration  
46 ceremony of the 2014 Soccer World Cup. New developments have overcome the out-of-the-lab high-bar  
47 and they are starting to be used in real world environments (Guger et al., 2017; Huggins et al., 2016).  
48 However, they still lack the necessary robustness, and its performance is well behind any other method of  
49 human computer interaction, including any kind of detection of residual muscular movement (Clerc et al.,  
50 2016).

51 A few works have explored the idea of exploiting the signal waveform to analyze the EEG signal.  
52 In (Alvarado-González et al., 2016) an approach based on Slope Horizontal Chain Code is presented,  
53 whereas in (Yamaguchi et al., 2009) a similar procedure was implemented based on Mathematical  
54 Morphological Analysis. The seminal work of Bandt-Pompe Permutation Entropy (Berger et al., 2017) also  
55 explores succinctly this idea as a basis to establish the time series ordinal patterns. In the article (Ramele  
56 et al., 2016), the authors introduce a method for classification of rhythmic EEG events like Visual Occipital  
57 Alpha Waves and Motor Imagery Rolandic Central  $\mu$  Rhythms using the Histogram of Gradient Orientations  
58 of signal plots. Inspired in that work, we propose a novel application of the developed method to classify  
59 and describe transient events, particularly the P300 Event Related Potential. The proposed approach is  
60 based on the waveform analysis of the shape of the EEG signal. The signal is drawn on a bidimensional  
61 image plot, vector gradients of pixels around the plot are obtained, and with them, the histogram of their  
62 orientations is calculated. This histogram is a direct representation of the waveform of the signal. The  
63 method is built by mimicking what regularly electroencephalographers have been performing for almost a  
64 century as it is described in (Hartman, 2005): visually inspecting raw signal plots.

65 This paper reports a method to, (1) describe a procedure to capture the shape of a waveform of an ERP  
66 component, the P300, using histograms of gradient orientations extracted from images of signal plots,  
67 and (2) outline the way in which this procedure can be used to implement an P300-Based BCI Speller  
68 application. Its validity is verified by offline processing two datasets, one of data from ALS patients and  
69 another one from data of healthy subjects.

70 This article unfolds as follows: Section 2.1 is dedicated to explain the Feature Extraction method based  
71 on Histogram of Gradient Orientations of the Signal Plot: Section 2.1.1 shows the preprocessing pipeline,  
72 Section 2.1.2 describes the image generation of the signal plot, Section 2.1.3 presents the feature extraction

73 procedure while Section 2.1.4 introduces the Speller Matrix Letter Identification procedure. In Section 2.2,  
74 the experimental protocol is expounded. Section 3 shows the results of applying the proposed technique. In  
75 the final Section 4 we expose our remarks, conclusions and future work.

## 2 MATERIALS AND METHODS

76 The P300 (Farwell and Donchin, 1988; Knuth et al., 2006) is a positive deflection of the EEG signal which  
77 occurs around 300 ms after the onset of a rare and deviant stimulus that the subject is expected to attend. It  
78 is produced under the oddball paradigm (Wolpaw and E., 2012) and it is consistent across different subjects.  
79 It has a lower amplitude ( $\pm 5\mu V$ ) compared to basal EEG activity, reaching a Signal to Noise Ratio (SNR)  
80 of around  $-15$  db estimated based on the amplitude of the P300 response signal divided by the standard  
81 deviation of the background EEG activity (Hu et al., 2010). This signal can be used to implement a speller  
82 application by means of a Speller Matrix (Farwell and Donchin, 1988). This matrix is composed of 6 rows  
83 and 6 columns of numbers and letters. The subject can focus on one character of the matrix. Figure 1 shows  
84 an example of the Speller Matrix used in the OpenVibe open source software (Renard et al., 2010), where  
85 the flashes of rows and columns provide the deviant stimulus required to elicit this physiological response.  
86 Each time a row or a column that contains the desired letter flashes, the corresponding synchronized EEG  
87 signal should also contain the P300 signature and by detecting it, the selected letter can be identified.

### 88 2.1 Feature Extraction from Signal Plots

89 In this section, the signal preprocessing, the method for generating images from signal plots, the feature  
90 extraction procedure and the Speller Matrix identification are described. Figure 2 shows a scheme of the  
91 entire process.

#### 92 2.1.1 Preprocessing Pipeline

93 The data obtained by the capturing device is digitalized and a multichannel EEG signal is constructed.  
94 The 6 rows and 6 columns of the Speller Matrix are intensified providing the visual stimulus. The  
95 number of a row or column is a location. A sequence of twelve randomly permuted locations  $l$  conform an  
96 intensification sequence. The whole set of twelve intensifications is repeated  $k_a$  times.

- 97 • **Signal Enhancement:** This stage consists of the enhancement of the SNR of the P300 pattern above  
98 the level of basal EEG. The pipeline starts by applying a notch filter to the raw digital signal, a 4th  
99 degree 10 Hz lowpass Butterworth filter and finally a decimation with a Finite Impulse Response (FIR)  
100 filter of order 30 from the original sampling frequency down to 16 Hz (Krusienski et al., 2006).
- 101 • **Artifact Removal:** For every complete sequence of 12 intensifications of 6 rows and 6 columns, a  
102 basic artifact elimination procedure is implemented by removing the entire sequence when any signal  
103 deviates above/below  $\pm 70\mu V$ .
- 104 • **Segmentation:** For each of the 12 intensifications of one intensification sequence, a segment  $S_i^l$   
105 of a window of  $t_{max}$  seconds of the multichannel signal is extracted, starting from the stimulus  
106 onset, corresponding to each row/column intensification  $l$  and to the intensification sequence  $i$ . As  
107 intensifications are permuted in a random order, the segments are rearranged corresponding to row  
108 flickering, labeled 1-6, whereas those corresponding to column flickering are labeled 7-12. Two of  
109 these segments should contain the P300 ERP signature time-locked to the flashing stimulus, one for  
110 the row, and one for the column.

111 • **Signal Averaging:** The P300 ERP is deeply buried under basal EEG so the standard approach to  
 112 identify it is by point-to-point averaging the time-locked stacked signal segments. Hence the values  
 113 which are not related to, and not time-locked to the onset of the stimulus are canceled out (Liang and  
 114 Bougrain, 2008).

115 This last step determines the operation of any P300 Speller. In order to obtain an improved signal  
 116 in terms of its SNR, repetitions of the sequence of row/column intensification are necessary. And,  
 117 at the same time, as long as more repetitions are needed, the ability to transfer information faster is  
 118 diminished, so there is a trade-off that must be acutely determined.

119 The procedure to obtain the point-to-point averaged signal goes as follows:

- 120 1. Highlight randomly the rows and columns from the matrix. There is one row and one column that  
 121 should match the letter selected by the subject.
- 122 2. Repeat step 1  $k_a$  times, obtaining the  $1 \leq l \leq 12$  segments  $S_1^l(n, c), \dots, S_{k_a}^l(n, c)$ , of the EEG  
 123 signal where the variables  $1 \leq n \leq n_{max}$  and  $1 \leq c \leq C$  correspond to sample points and channel,  
 124 respectively. The parameter  $C$  is the number of available EEG channels whereas  $n_{max} = F_s t_{max}$   
 125 is the segment length and  $F_s$  is the sampling frequency. The parameter  $k_a$  is the number of  
 126 repetitions of intensifications and it is an input parameter of the algorithm.
- 127 3. Compute the Ensemble Average by

$$x^l(n, c) = \frac{1}{k_a} \sum_{i=1}^{k_a} S_i^l(n, c) \quad (1)$$

128 for  $1 \leq n \leq n_{max}$  and for the channels  $1 \leq c \leq C$ . This provide an averaged signal  $x^l(n, c)$  for  
 129 the twelve locations  $1 \leq l \leq 12$ .

### 130 2.1.2 Signal Plotting

131 Averaged signal segments are standardized and scaled for  $1 \leq n \leq n_{max}$  and  $1 \leq c \leq C$  by

$$\tilde{x}^l(n, c) = \left\lfloor \gamma \frac{(x^l(n, c) - \bar{x}^l(c))}{\hat{\sigma}^l(c)} \right\rfloor \quad (2)$$

where  $\gamma > 0$  is an input parameter of the algorithm and it is related to the image scale. In addition,  $x^l(n, c)$  is the point-to-point averaged multichannel EEG signal for the sample point  $n$  and for channel  $c$ . Lastly,

$$\bar{x}^l(c) = \frac{1}{n_{max}} \sum_{n=1}^{n_{max}} x^l(n, c)$$

and

$$\hat{\sigma}^l(c) = \left\{ \frac{1}{n_{max} - 1} \sum_{n=1}^{n_{max}} [x^l(n, c) - \bar{x}^l(c)]^2 \right\}^{\frac{1}{2}}$$

132 are the mean and estimated standard deviation of  $x^l(n, c)$ ,  $1 \leq n \leq n_{max}$ , for each channel  $c$ .

133 Consequently, a binary image  $I^{(l,c)}$  is constructed according to

$$I^{(l,c)}(z_1, z_2) = \begin{cases} 255 & \text{if } z_1 = \gamma n \quad \text{and} \quad z_2 = \tilde{x}^l(n, c) + z^l(c) \\ 0 & \text{otherwise} \end{cases} \quad (3)$$

134 with 255 being white and representing the signal's value location and 0 for black which is the background  
 135 contrast, conforming a black-and-white plot of the signal. Pixel arguments  $(z_1, z_2) \in \mathbb{N} \times \mathbb{N}$  iterate over  
 136 the width (based on the length of the signal segment) and height (based on the peak-to-peak amplitude) of  
 137 the newly created image with  $1 \leq n \leq n_{max}$  and  $1 \leq c \leq C$ . The value  $z^l(c)$  is the image vertical position  
 138 where the signal's zero value has to be situated in order to fit the entire signal within the image for each  
 139 channel c:

$$z^l(c) = \left\lfloor \frac{\max_n \tilde{x}^l(n, c) - \min_n \tilde{x}^l(n, c)}{2} \right\rfloor - \left\lfloor \frac{\max_n \tilde{x}^l(n, c) + \min_n \tilde{x}^l(n, c)}{2} \right\rfloor \quad (4)$$

140 where the minimization and maximization are carried out for  $n$  varying between  $1 \leq n \leq n_{max}$ , and  $\lfloor \cdot \rfloor$   
 141 denote the rounding to the smaller nearest integer of the number.

142 In order to complete the plot  $I^{(l,c)}$  from the pixels, the Bresenham (Bresenham, 1965; Ramele et al.,  
 143 2016) algorithm is used to interpolate straight lines between each pair of consecutive pixels.

#### 144 2.1.3 Feature Extraction: Histogram of Gradient Orientations

145 The work of Edelman, Intrator and Poggio (Edelman et al., 1997) on how the visual cortex sense features  
 146 was the inspiration to the development of an algorithm to identify and decode salient local information  
 147 from image regions. The Scale Invariant Feature Transform (SIFT) is a Computer Vision method proposed  
 148 by Lowe (2004) which is composed of two parts, the SIFT Detector and the SIFT Descriptor. The former  
 149 is the procedure to identify relevant areas of an image whereas the latter is the procedure to describe and  
 150 characterize a region of an image (i.e. patch) calculating an histogram of the gradient orientations. In  
 151 order to characterize EEG signal waveforms, this work proposes an alternative to the SIFT Descriptor, the  
 152 Histogram of Gradient Orientations algorithm. We stripped away all the details which are not used and  
 153 refined the procedure to enable the effective capturing of the waveform shape.

154 For each generated image  $I^{(l,c)}$ , a keypoint  $p_k$  is placed on a pixel  $(x_{p_k}, y_{p_k})$  over the image plot and a  
 155 window around the keypoint is considered. A local image patch of size  $X_p \times X_p$  pixels is constructed by  
 156 dividing the window in 16 blocks of size  $3s$  each one, where  $s$  is the scale of the local patch and it is an  
 157 input parameter of the algorithm. It is arranged in a  $4 \times 4$  grid and the pixel  $p_k$  is the patch center, thus  
 158  $X_p = 12s$  pixels.

159 A local representation of the signal shape within the patch can be described by obtaining the gradient  
 160 orientations on each of the 16 blocks  $B_{i,j}$  with  $0 \leq i, j \leq 3$  and creating a histogram of gradients. In  
 161 order to calculate the histogram, the interval  $[0, 360]$  of possible angles is divided in 8 bins, each one of 45  
 162 degrees.

163 Hence, for each spatial bin  $0 \leq i, j \leq 3$ , corresponding to the indexes of each block  $B_{i,j}$ , the orientations  
 164 are accumulated in a 3-dimensional histogram  $h$  through the following equation:

$$h(\theta, i, j) = 3s \sum_{\mathbf{p} \in I^{(l,c)}} w_{ang}(\angle J(\mathbf{p}) - \theta) w_{ij} \left( \frac{\mathbf{p} - \mathbf{p}_k}{3s} \right) \|J(\mathbf{p})\| \quad (5)$$

165 where  $\mathbf{p}$  is a pixel from the image  $I^{(l,c)}$ ,  $\theta$  is the angle bin with  $\theta \in \{0, 45, 90, 135, 180, 225, 270, 315\}$ ,  
 166  $\|J(\mathbf{p})\|$  is the norm of the gradient vector in the pixel  $\mathbf{p}$  and it is computed using finite differences and  
 167  $\angle J(\mathbf{p})$  is the angle of the gradient vector.

168 The contribution of each gradient vector to the histogram calculated by Equation 5 is balanced by a  
 169 trilinear interpolation. The scalar  $w_{ang}(\cdot)$  and vector  $w_{ij}(\cdot)$  functions are linear interpolations used by Lowe  
 170 (2004) and Vedaldi and Fulkerson (2010) to provide a weighting contribution to the eight adjacent bins in  
 171 the tridimensional histogram. They are calculated as

$$w_{ij}(\mathbf{v}) = w(v_x - x_i)w(v_y - y_j) \quad (6)$$

172 with  $0 \leq i, j \leq 3$  and

$$w_{ang}(\alpha) = \sum_{r=-1}^1 w\left(\frac{8\alpha}{2\pi} + 8r\right) \quad (7)$$

173 where  $x_i$  and  $y_i$  are the spatial bin centers located in  $x_i, y_i \in \{-\frac{3}{2}, -\frac{1}{2}, \frac{1}{2}, \frac{3}{2}\}$  and the interpolating function  
 174  $w(\cdot)$  is defined as  $w(z) = \max(0, |z| - 1)$ . The function parameter  $\mathbf{v} = (v_x, v_y)$  is a vector variable and  $\alpha$   
 175 a scalar variable. Vector  $\mathbf{v}$  holds pixel coordinates  $(v_x, v_y)$  normalized between  $-2$  and  $2$  and combined  
 176 with the function  $w(z)$  it produces zero for every combination of  $(i, j)$  except for the 4 adjacent spatial  
 177 bins. On the other hand,  $r$  is an integer that can vary freely in the set  $\{-1, 0, 1\}$  and  $\alpha$  is the difference  
 178 between the gradient orientation angle and the angle bin center in radians. By following this procedure,  
 179 summands on Equation 7 are nullified except for the 2 adjacent angular bins.

180 These binning functions conform the trilinear interpolation that has a combined effect of sharing the  
 181 contribution of each oriented gradient between their eight adjacent bins in a tridimensional cube in the  
 182 histogram space, and zero everywhere else (Mortensen et al., 2005).

183 Lastly, the fixed value of 3 is a magnification factor which corresponds to the number of pixels per each  
 184 block when  $s = 1$ . As the patch has 16 blocks and 8 bin angles are considered, for each location  $l$  and  
 185 channel  $c$  a feature called *descriptor*  $\mathbf{d}^{(l,c)}$  of 128 dimension is obtained.

186 Figure 3 shows an example of a patch and a scheme of the histogram computation. In (A) a plot of the  
 187 signal and the patch centered around the keypoint is shown. In (B) the possible orientations on each patch  
 188 are illustrated. Only the upper-left four blocks are visible. The first eight orientations of the first block, are  
 189 labeled from 1 to 8 clockwise. The orientations of the second block  $B_{1,2}$  are labeled from 9 to 16. This  
 190 labeling continues left-to-right, up-down until the eight orientations for all the sixteen blocks are assigned.  
 191 They form the corresponding descriptor  $\mathbf{d}$  of 128 coordinates. Finally, in (C) an enlarged image plot is  
 192 shown where the oriented gradient vector for each pixel can be seen.

### 193 2.1.4 Speller Matrix letter Identification

#### 194 2.1.4.1 P300 ERP Extraction

195 Segments corresponding to row flickering are labeled 1-6, whereas those corresponding to column  
 196 flickering are labeled 7-12. The extraction process has the following steps:

- 197 • **Step A:** First highlight rows and columns from the matrix in a random permutation order and obtain  
 198 the Ensemble Average as detailed in steps 1, 2 and 3 in Section 2.1.1.

- 199 • **Step B:** Plot the signals  $\tilde{x}^l(n, c)$ ,  $1 \leq n \leq n_{max}$ ,  $1 \leq c \leq C$ , according Section 2.1.2 in order to  
200 generate the images  $I^{(l,c)}$  for rows and columns  $1 \leq l \leq 12$ .  
201 • **Step C:** Obtain the descriptors  $\mathbf{d}^{(l,c)}$  for rows and columns from  $I^{(l,c)}$  in accordance to the method  
202 described in Section 2.1.3.

203 **2.1.4.2 Calibration**

204 A trial, as defined by the BCI2000 platform (Schalk et al., 2004), is every attempt to select just one letter  
205 from the speller. A set of trials is used for calibration and once the calibration is complete it can be used to  
206 identify new letters from new trials.

207 During the calibration phase, two descriptors  $\mathbf{d}^{(l,c)}$  are extracted for each available channel, corresponding  
208 to the locations  $l$  of a selection of one previously instructed letter from the set of calibration trials. These  
209 descriptors are the P300 templates, grouped together in a template set called  $T^c$ . The set is constructed  
210 using the steps described in Section 2.1.1 and the steps A, B and C of the P300 ERP extraction process.

211 Additionally, the best performing channel,  $bpc$  is identified based on the the channel where the best  
212 Character Recognition Rate is obtained.

213 **2.1.4.3 Letter identification**

214 In order to identify the selected letter, the template set  $T^{bpc}$  is used as a database. Thus, new unclassified  
215 descriptors  $\mathbf{q}^{(l,bpc)}$  are computed and they are compared against the descriptors belonging to the calibration  
216 template set  $T^{bpc}$ .

217 The Naive Bayes Nearest Neighbor (k-NBNN) (Boiman et al., 2008) is a discriminative (Wolpaw and E.,  
218 2012) semi-supervised classification algorithm that allows the categorization of an image to one class by  
219 comparing the set of extracted descriptors to those which are more similar from template dictionaries. This  
220 work proposes an adapted version to obtain a unary classification scheme to identify the selected letter in  
221 the P300-Based BCI Speller, based on the features provided by the calculated descriptors.

222 • **Step D:** Match to the calibration template  $T^{bpc}$  by computing

$$\hat{row} = \arg \min_{l \in \{1, \dots, 6\}} \sum_{h=1}^k \left\| \mathbf{q}^{(l,bpc)} - \mathbf{d}_h^{(bpc)} \right\|^2 \quad (8)$$

223 and

$$\hat{col} = \arg \min_{l \in \{7, \dots, 12\}} \sum_{h=1}^k \left\| \mathbf{q}^{(l,bpc)} - \mathbf{d}_h^{(bpc)} \right\|^2 \quad (9)$$

224 with  $\mathbf{d}_h^{(bpc)}$  belonging to the set  $N_T(\mathbf{q}^{(l,bpc)})$ , which is defined, for the best performing channel, as  
225  $N_T(\mathbf{q}^{(l,bpc)}) = \{\mathbf{d}_h^{(bpc)} \in T^{bpc} / \mathbf{d}_h^{(bpc)} \text{ is the } k\text{-nearest neighbor of } \mathbf{q}^{(l,bpc)}\}$ . This set is obtained by  
226 sorting all the elements in  $T^{bpc}$  based on distances between them and  $\mathbf{q}^{(l,bpc)}$ , choosing the  $k$  with  
227 smaller values, with  $k$  a parameter of the algorithm.

228 By computing the aforementioned equations, the letter of the matrix can be determined from the intersection  
229 of the row  $\hat{row}$  and column  $\hat{col}$ . Figure 2 shows a scheme of this process.

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**230 2.2 Experimental Protocol**

231 To verify the validity of the proposed framework and method, the public dataset 008-2014 (Riccio et al.,  
232 2013) published on the BNCI-Horizon website (Brunner et al., 2014) by IRCCS Fondazione Santa Lucia,  
233 is used. Additionally, an own dataset with the same experimental conditions is generated. Both of them are  
234 utilized to perform an offline BCI Simulation to decode the spelled words from the provided signals.

235 The algorithm is implemented on MATLAB V2017a (Mathworks Inc., Natick, MA, USA). The algorithm  
236 described in 2.1.3 is implemented on a modified version of the VLFeat (Vedaldi and Fulkerson, 2010)  
237 Computer Vision library. Furthermore, in order to enhance the impact of this paper and for a sake of  
238 reproducibility, the code of the entire algorithm, including the modified VLFeat library, has been made  
239 available at: <https://bitbucket.org/itba/hist>.

240 In the following sections the characteristics of the datasets and parameters of the identification algorithm  
241 are described.

**242 2.2.1 P300 ALS Public Dataset**

243 The experimental protocol used to generate this dataset is explained in (Riccio et al., 2013) but can  
244 be summarized as follows: 8 subjects with confirmed diagnoses but on different stages of ALS disease,  
245 were recruited and accepted to perform the experiments. The Visual P300 detection task designed for this  
246 experiment consisted of spelling 7 words of 5 letters each, using the traditional P300 Speller Matrix (Farwell  
247 and Donchin, 1988). The flashing of rows and columns provide the deviant stimulus required to elicit this  
248 physiological response. The first 3 words are used for calibration and the remaining 4 words, for testing  
249 with visual feedback. A trial is every attempt to select a letter from the speller. It is composed of signal  
250 segments corresponding to  $k_a = 10$  repetitions of flashes of 6 rows and  $k_a = 10$  repetitions of flashes of 6  
251 columns of the matrix, yielding 120 repetitions. Flashing of a row or a column is performed for 0.125s,  
252 following by a resting period (i.e. inter-stimulus interval) of the same length. After 120 repetitions an  
253 inter-trial pause is included before resuming with the following letter.

254 The recorded dataset was sampled at 256 Hz and it consisted of a scalp multichannel EEG signal for  
255 electrode channels Fz, Cz, Pz, Oz, P3, P4, PO7 and PO8, identified according to the 10-20 International  
256 System, for each one of the 8 subjects. The recording device was a research-oriented digital EEG device  
257 (g.Mobilab, g.Tec, Austria) and the data acquisition and stimuli delivery were handled by the BCI2000  
258 open source software (Schalk et al., 2004).

259 In order to assess and verify the identification of the P300 response, subjects are instructed to perform a  
260 copy-spelling task. They have to fix their attention to successive letters for copying a previously determined  
261 set of words, in contrast to a free-running operation of the speller where each user decides on its own what  
262 letter to choose.

**263 2.2.2 P300 for healthy subjects**

264 We replicate the same experiment on healthy subjects using a wireless digital EEG device (g.Nautilus,  
265 g.Tec, Austria). The experimental conditions are the same as those used for the previous dataset, as detailed  
266 in section 2.2.1. The produced dataset is available in a public online repository (Ramele et al., 2017).

267 Participants are recruited voluntarily and the experiment is conducted anonymously in accordance with  
268 the Declaration of Helsinki published by the World Health Organization. No monetary compensation  
269 is handed out and all participants agree and sign a written informed consent. This study is approved  
270 by the *Departamento de Investigación y Doctorado, Instituto Tecnológico de Buenos Aires (ITBA)*. All

271 healthy subjects have normal or corrected-to-normal vision and no history of neurological disorders. The  
 272 experiment is performed with 8 subjects, 6 males, 2 females, 6 right-handed, 2 left-handed, average age  
 273 29.00 years, standard deviation 11.56 years, range 20-56 years.

274 EEG data is collected in a single recording session. Participants are seated in a comfortable chair, with  
 275 their vision aligned to a computer screen located one meter in front of them. The handling and processing  
 276 of the data and stimuli is conducted by the OpenVibe platform (Renard et al., 2010).

277 Gel-based active electrodes (g.LADYbird, g.Tec, Austria) are used on the same positions Fz, Cz, Pz,  
 278 Oz, P3,P4, PO7 and PO8. Reference is set to the right ear lobe and ground is preset as the AFz position.  
 279 Sampling frequency is slightly different, and is set to 250 Hz, which is the closest possible to the one used  
 280 with the other dataset.

### 281 2.2.3 Parameters

282 The patch size is  $X_P = 12s \times 12s$  pixels, where  $s$  is the scale of the local patch and it is an input parameter  
 283 of the algorithm. The P300 event can have a span of 400 ms and its amplitude can reach  $10\mu V$  (Rao, 2013).  
 284 Hence it is necessary to utilize a signal segment of size  $t_{max} = 1$  second and a size patch  $X_P$  that could  
 285 capture an entire transient event. With this purpose in consideration, the  $s$  value election is essential.

286 We propose the Equations 10 and 11 to compute the scale value in horizontal and vertical directions,  
 287 respectively.

$$s_x = \frac{\gamma \lambda F_s}{12} \quad (10)$$

$$s_y = \frac{\gamma \Delta\mu V}{12} \quad (11)$$

288 where  $\lambda$  is the length in seconds covered by the patch,  $F_s$  is the sampling frequency of the EEG signal  
 289 (downsampled to 16 Hz) and  $\Delta\mu V$  corresponds to the amplitude in microvolts that can be covered by the  
 290 height of the patch. The geometric structure of the patch forces a squared configuration, then we discerned  
 291 that by using  $s = s_x = s_y = 3$  and  $\gamma = 4$ , the local patch and the descriptor can identify events of  $9\mu V$   
 292 of amplitude, with a span of  $\lambda = 0.56$  seconds. This also determines that 1 pixel represents  $\frac{1}{\gamma} = \frac{1}{4}\mu V$  on  
 293 the vertical direction and  $\frac{1}{F_s \gamma} = \frac{1}{64}$  seconds on the horizontal direction. The keypoints  $p_k$  are located at  
 294  $(x_{p_k}, y_{p_k}) = (0.55F_s \gamma, z^l(c)) = (35, z^l(c))$  for the corresponding channel  $c$  and location  $l$  (see Equation 4).  
 295 In this way the whole transient event is captured. Figure 4 shows a patch of a signal plot covering the  
 296 complete amplitude (vertical direction) and the complete span of the signal event (horizontal direction).

297 Moreover, the number of channels  $C$  is equal to 8 for both datasets, and the number of intensification  
 298 sequences  $k_a$  is fixed to 10. The parameter  $k$  used to construct the set  $N_T(\mathbf{d}^{(l,c)})$  is assigned to  $k = 7$ ,  
 299 which was found empirically to achieve better results. In addition, the norm used on Equations 8 and 9 is  
 300 the cosine norm, and descriptors are normalized to  $[-1, 1]$ .

301 Lastly, in order to assess the validity of the Histogram of Gradient Orientations (HIST) method, the  
 302 character recognition rate for both datasets is evaluated replicating the methodology proposed by the  
 303 ALS dataset's publisher, since authors Riccio et al. (2013) did not report the Character Recognition  
 304 Rate obtained for this dataset. Frequency filtering, data segmentation and artifact rejection is conducted  
 305 according to Section 2.1.1 yielding 16 x 8 samples per epoch. A multichannel feature consists of time  
 306 points vector (Lotte et al., 2018), formed by concatenating all the channels (Krusienski et al., 2006). A  
 307 single-channel variant consists of using time points from a single electrode and performing the analysis on

308 a channel-by-channel basis. Three classification schemes are considered as well. A multichannel version of  
309 the Stepwise Linear Discriminant Analysis (SWLDA) classification algorithm. SWLDA is the methodology  
310 proposed by the ALS dataset's publisher. Additionally, a single-channel and a multichannel variant of a  
311 linear kernel Support Vector Machine (SVM) (Scholkopf and Smola, 2001) classifier are utilized. SVM has  
312 been successfully used in several BCI Competitions (Rakotomamonjy and Guigue, 2008).

### 3 RESULTS

313 Table 1 shows the results of applying the HIST algorithm to the subjects of the public dataset of ALS  
314 patients. The percentage of correctly spelled letters is calculated while performing an offline BCI Simulation.  
315 From the seven words for each subject, the first three are used for calibration, and the remaining four are  
316 used for testing. The best performing channel *bpc* is informed as well. The target ratio is 1 : 36; hence  
317 theoretical chance level is 2.8%. It can be observed that the best performance of the letter identification  
318 method is reached in a dissimilar channel depending on the subject being studied. Table 1 and 2 show for  
319 comparison the obtained performance rates using single-channel signals with the SVM classifier. The best  
320 performing channel, where the best letter identification rate was achieved, is also depicted.

321 The Information Transfer Rate (ITR), or Bit Transfer Rate (BTR), in the case of reactive BCIs (Wolpaw  
322 and E., 2012) depends on the amount of signal averaging required to transmit a valid and robust selection.  
323 Figure 5 shows the performance curves for varying intensification sequences for the subjects included in  
324 the dataset of ALS patients. It can be noticed that the percentage of correctly identified letters depends  
325 on the number of intensification sequences that are used to obtain the averaged signal. Moreover, when  
326 the number of intensification sequences tend to 1, which corresponds to single-intensification character  
327 recognition, the performance is reduced. As mentioned before, the SNR of the P300 obtained from only  
328 one segment of the intensification sequence is very low and the shape of its P300 component is not very  
329 well defined.

330 In Table 2 the results obtained for 8 healthy subjects are shown. It can be observed that the performance  
331 is above chance level. It is verified that HIST method has an improved performance at letter identification  
332 than SVM that process the signals on a channel by channel strategy (Wilcoxon signed-rank test,  $p = 0.004$   
333 for both datasets).

334 Tables 3 and 4 are presented in order to compare the performance of the HIST method versus multichannel  
335 SWLDA and SVM classification algorithms for both datasets. It is verified for the dataset of ALS patients  
336 that it has similar performance against other methods like SWLDA or SVM, which use a multichannel  
337 feature (Quade test with  $p = 0.55$ ) whereas for the dataset of healthy subjects significant differences are  
338 found (Quade test with  $p = 0.02$ ) where only the HIST method achieves a different performance than SVM  
339 (with multiple comparisons, significant difference of level 0.05).

340 The P300 ERP consists of two overlapping components: the P3a and P3b, the former with frontocentral  
341 distribution while the later stronger on centroparietal region (Polich, 2007). Hence, the standard practice is  
342 to find the stronger response on the central channel Cz (Riccio et al., 2013). However, Krusienski et al.  
343 (2006) show that the response may also arise in occipital regions. We found that by analyzing only the  
344 waveforms, occipital channels PO8 and PO7 show higher performances for some subjects.

345 As subjects have varying *latencies* and *amplitudes* of their P300 components, they also have a varying  
346 stability of the *shape* of the generated ERP (Nam et al., 2010). Figure 6 shows 10 sample P300 templates  
347 patches for patients 8 and 3 from the dataset of ALS patients. It can be discerned that in coincidence with

348 the performance results, the P300 signature is more clear and consistent for subject 8 (A) while for subject  
349 3 (B) the characteristic pattern is more difficult to perceive.

350 Additionally, the stability of the P300 component waveform has been extensively studied in patients  
351 with ALS (Sellers et al., 2006; Madarame et al., 2008; Nijboer and Broermann, 2009; Mak et al., 2012;  
352 McCane et al., 2015) where it was found that these patients have a stable P300 component, which were  
353 also sustained across different sessions. In line with these results we do not find evidence of a difference in  
354 terms of the performance obtained by analyzing the waveforms (HIST) for the group of patients with ALS  
355 and the healthy group of volunteers (Mann-Whitney U Test,  $p = 0.46$ ). Particularly, the best performance  
356 is obtained for a subject from the ALS dataset for which, based on visual observation, the shape of they  
357 P300 component is consistently identified.

358 It is important to remark that when applied to binary images obtained from signal plots, the feature  
359 extraction method described in Section 2.1.3 generates sparse descriptors. Under this subspace we found  
360 that using the cosine metric yielded a significant performance improvement. On the other hand, the unary  
361 classification scheme based on the NBNN algorithm proved very beneficial for the P300 Speller Matrix.  
362 This is due to the fact that this approach solves the unbalance dataset problem which is inherent to the  
363 oddball paradigm (Tibon and Levy, 2015).

## 4 DISCUSSION

364 Among other applications of Brain Computer Interfaces, the goal of the discipline is to provide  
365 communication assistance to people affected by neuro-degenerative diseases, who are the most likely  
366 population to benefit from BCI systems and EEG processing and analysis.

367 In this work, a method to extract an objective metric from the waveform of the plots of EEG signals is  
368 presented. Its usage to implement a valid P300-Based BCI Speller application is expounded. Additionally,  
369 its validity is evaluated using a public dataset of ALS patients and an own dataset of healthy subjects.

370 It was verified that this method has an improved performance at letter identification than other methods  
371 that process the signals on a channel by channel strategy, and it even has a comparable performance against  
372 other methods like SWLDA or SVM, which uses a multichannel feature. Furthermore, this method has the  
373 advantage that shapes of waveforms can be analyzed in an objective way. We observed that the shape of  
374 the P300 component is more stable in occipital channels, where the performance for identifying letters  
375 is higher. We additionally verified that ALS P300 signatures are stable in comparison to those of healthy  
376 subjects.

377 We believe that the use of descriptors based on histogram of gradient orientation, presented in this work,  
378 can also be utilized for deriving a shape metric in the space of the P300 signals which can complement  
379 other metrics based on time-domain as those defined by Mak et al. (2012). It is important to notice  
380 that the analysis of waveform shapes is usually performed in a qualitative approach based on visual  
381 inspection (Sellers et al., 2006), and a complementary methodology which offer a quantitative metric will  
382 be beneficial to these routinely analysis of the waveform of ERPs.

383 The goal of this work is to answer the question if a P300 component could be solely determined by  
384 inspecting automatically their waveforms. We conclude affirmatively, though two very important issues  
385 still remain:

386 First, the stability of the P300 in terms of its shape is crucial: the averaging procedure, montages, the  
387 signal to noise ratio and spatial filters all of them are non-physiological factors that affect the stability of

388 the shape of the P300 ERP. We tested a preliminary approach to assess if the morphological shape of the  
389 P300 of the averaged signal can be stabilized by applying different alignments of the stacked segments (see  
390 Figure 2) and we verified that there is a better performance when a correct segment alignment is applied.  
391 We applied Dynamic Time Warping (DTW) (Casarotto et al., 2005) to automate the alignment procedure  
392 but we were unable to find a substantial improvement. Further work to study the stability of the shape of  
393 the P300 signature component needs to be addressed.

394 The second problem is the amplitude variation of the P300. We propose a solution by standardizing the  
395 signal, shown in Equation 2. It has the effect of normalizing the peak-to-peak amplitude, moderating its  
396 variation. It has also the advantage of reducing noise that was not reduced by the averaging procedure. It is  
397 important to remark that the averaged signal variance depends on the number of segments used to compute  
398 it (Van Drongelen, 2006). The standardizing process converts the signal to unit signal variance which  
399 makes it independent of the number  $k_a$  of signals averaged. Although this is initially an advantageous  
400 approach, the standardizing process reduces the amplitude of any significant P300 complex diminishing its  
401 automatic interpretation capability.

402 To further extend the capabilities of this method, it would be desirable to implement a multichannel  
403 version. The straightforward extension of concatenating the obtained descriptors results in high dimensional  
404 feature vector, while other variants that merge descriptors per channel may diminish the mutual information  
405 between different channels. Hitherto variants using color versions of SIFT (Van De Sande et al., 2010),  
406 where different color bands are mapped to electrode channels, have been explored without substantial  
407 success.

408 In our opinion, the best benefit of the presented method is that a closer collaboration of the field of BCI  
409 with physicians can be fostered (Chavarriaga et al., 2017), since this procedure intent to imitate human  
410 visual observation. Automatic classification of patterns in EEG that are specifically identified by their  
411 shapes like K-Complex, Vertex Waves, Positive Occipital Sharp Transient (Hartman, 2005) are a prospect  
412 future work to be considered. We are currently working in unpublished material analyzing K-Complex  
413 components that could eventually provide assistance to physicians to locate these EEG patterns, specially in  
414 long recording periods, frequent in sleep research (Michel and Murray, 2012). Additionally, it can be used  
415 for artifact removal which is performed on many occasions by visually inspecting signals. This is due to  
416 the fact that the descriptors are a direct representation of the shape of signal waveforms. In line with these  
417 applications, it can be used to build a database (Chavarriaga et al., 2017) of quantitative representations of  
418 waveforms and improve atlases (Hartman, 2005), which are currently based on qualitative descriptions of  
419 signal shapes.

## CONFLICT OF INTEREST STATEMENT

420 The authors declare that the research was conducted in the absence of any commercial or financial  
421 relationships that could be construed as a potential conflict of interest.

## AUTHOR CONTRIBUTIONS

422 This work is part of the PhD thesis of RR which is directed by JS and codirected by AV.

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## REFERENCES

- 425 Alvarado-González, M., Garduño, E., Bribiesca, E., Yáñez-Suárez, O., and Medina-Bañuelos, V. (2016).  
426 P300 Detection Based on EEG Shape Features. *Computational and Mathematical Methods in Medicine*,  
427 1–14doi:10.1155/2016/2029791
- 428 Berger, S., Schneider, G., Kochs, E., and Jordan, D. (2017). Permutation Entropy: Too Complex a Measure  
429 for EEG Time Series? *Entropy 2017, Vol. 19, Page 692* 19, 692. doi:10.3390/E19120692
- 430 Boiman, O., Shechtman, E., and Irani, M. (2008). In defense of nearest-neighbor based image classification.  
431 *26th IEEE Conference on Computer Vision and Pattern Recognition, CVPR* doi:10.1109/CVPR.2008.  
432 4587598
- 433 Bresenham, J. E. (1965). Algorithm for computer control of a digital plotter. *IBM Systems Journal* 4,  
434 25–30
- 435 Brunner, C., Blankertz, B., Cincotti, F., Kübler, A., Mattia, D., Miralles, F., et al. (2014). BNCI Horizon  
436 2020 – Towards a Roadmap for Brain / Neural Computer Interaction. *Lecture Notes in Computer Science*  
437 8513, 475–486
- 438 Carlson, T. and del R. Millan, J. (2013). Brain-controlled wheelchairs: A robotic architecture. *IEEE  
439 Robotics & Automation Magazine* 20, 65–73. doi:10.1109/MRA.2012.2229936
- 440 Casarotto, S., Bianchi, A., Cerutti, S., and Chiarenza, G. (2005). Dynamic time warping in the analysis of  
441 event-related potentials. *IEEE Engineering in Medicine and Biology Magazine* 24, 68–77. doi:10.1109/  
442 MEMB.2005.1384103
- 443 Chavarriaga, R., Fried-Oken, M., Kleih, S., Lotte, F., and Scherer, R. (2017). Heading for new shores!  
444 Overcoming pitfalls in BCI design. *Brain-Computer Interfaces* 4, 60–73. doi:10.1080/2326263X.2016.  
445 1263916
- 446 Clerc, M., Bougrain, L., and Lotte, F. (2016). *Brain-computer interfaces, Technology and applications*  
447 2(Cognitive Science) (ISTE Ltd. and Wiley)
- 448 De Vos, M. and Debener, S. (2014). Mobile EEG: Towards brain activity monitoring during natural action  
449 and cognition. *International Journal of Psychophysiology* 91, 1–2. doi:10.1016/j.ijpsycho.2013.10.008
- 450 Edelman, S., Intrator, N., and Poggio, T. (1997). Complex cells and object recognition
- 451 Farwell, L. A. and Donchin, E. (1988). Talking off the top of your head: toward a mental prosthesis utilizing  
452 event-related brain potentials. *Electroencephalography and clinical neurophysiology* 70, 510–23
- 453 Guger, C., Allison, B. Z., and Lebedev, M. A. (2017). Introduction. In *Brain Computer Interface Research:  
454 A State of the Art Summary* 6 (Springer, Cham). 1–8. doi:10.1007/978-3-319-64373-1\_1
- 455 Guger, C., Daban, S., Sellers, E., Holzner, C., Krausz, G., Carabalona, R., et al. (2009). How many people  
456 are able to control a P300-based brain-computer interface (BCI)? *Neuroscience Letters* 462, 94–98.  
457 doi:10.1016/j.neulet.2009.06.045
- 458 Hartman, a. L. (2005). *Atlas of EEG Patterns*, vol. 65 (Lippincott Williams & Wilkins). doi:10.1212/01.  
459 wnl.0000174180.41994.39
- 460 Hu, L., Mouraux, A., Hu, Y., and Iannetti, G. D. (2010). A novel approach for enhancing the signal-to-noise  
461 ratio and detecting automatically event-related potentials (ERPs) in single trials. *NeuroImage* 50, 99–111.  
462 doi:10.1016/j.neuroimage.2009.12.010

- 463 Huggins, J. E., Alcaide-Aguirre, R. E., and Hill, K. (2016). Effects of text generation on P300 brain-  
464 computer interface performance. *Brain-Computer Interfaces* 3, 112–120. doi:10.1080/2326263X.2016.  
465 1203629
- 466 Jure, F., Carrere, L., Gentiletti, G., and Tabernig, C. (2016). BCI-FES system for neuro-rehabilitation of  
467 stroke patients. *Journal of Physics: Conference Series* 705, 1–8. doi:10.1088/1742-6596/705/1/012058
- 468 Knuth, K. H., Shah, A. S., Truccolo, W. A., Ding, M., Bressler, S. L., and Schroeder, C. E. (2006).  
469 Differentially variable component analysis: Identifying multiple evoked components using trial-to-trial  
470 variability. *Journal of Neurophysiology* 95, 3257–3276. doi:10.1152/jn.00663.2005
- 471 Krusienski, D. J., Sellers, E. W., Cabestaing, F., Bayoudh, S., McFarland, D. J., Vaughan, T. M., et al.  
472 (2006). A comparison of classification techniques for the P300 Speller. *Journal of Neural Engineering*  
473 3, 299–305. doi:10.1088/1741-2560/3/4/007
- 474 Liang, N. and Bougrain, L. (2008). Averaging techniques for single-trial analysis of oddball event-related  
475 potentials. *4th International Brain-Computer*, 1–6
- 476 Lotte, F., Bougrain, L., Cichocki, A., Clerc, M., Congedo, M., Rakotomamonjy, A., et al. (2018). A review  
477 of classification algorithms for EEG-based brain–computer interfaces: a 10 year update. *Journal of*  
478 *Neural Engineering* 15, 031005. doi:10.1088/1741-2552/aab2f2
- 479 Lotte, F., Faller, J., Guger, C., Renard, Y., Pfurtscheller, G., Lécuyer, A., et al. (2013). *Combining BCI*  
480 *with Virtual Reality: Towards New Applications and Improved BCI* (Berlin, Heidelberg: Springer Berlin  
481 Heidelberg). 197–220. doi:10.1007/978-3-642-29746-5\_10
- 482 Lowe, G. (2004). SIFT - The Scale Invariant Feature Transform. *International Journal* 2, 91–110
- 483 Madarame, T., Tanaka, H., Inoue, T., Kamata, M., and Shino, M. (2008). The development of a brain  
484 computer interface device for amyotrophic lateral sclerosis patients. In *Conference Proceedings - IEEE*  
485 *International Conference on Systems, Man and Cybernetics* (IEEE), 2401–2406. doi:10.1109/ICSMC.  
486 2008.4811654
- 487 Mak, J. N., McFarland, D. J., Vaughan, T. M., McCane, L. M., Tsui, P. Z., Zeitlin, D. J., et al. (2012). EEG  
488 correlates of P300-based brain-computer interface (BCI) performance in people with amyotrophic lateral  
489 sclerosis. *Journal of Neural Engineering* 9. doi:10.1088/1741-2560/9/2/026014
- 490 McCane, L. M., Heckman, S. M., McFarland, D. J., Townsend, G., Mak, J. N., Sellers, E. W., et al.  
491 (2015). P300-based brain-computer interface (BCI) event-related potentials (ERPs): People with  
492 amyotrophic lateral sclerosis (ALS) vs. age-matched controls. *Clinical Neurophysiology* 126, 2124–2131.  
493 doi:10.1016/j.clinph.2015.01.013
- 494 Michel, C. M. and Murray, M. M. (2012). Towards the utilization of EEG as a brain imaging tool.  
495 *NeuroImage* 61, 371–385. doi:10.1016/j.neuroimage.2011.12.039
- 496 Mortensen, E. N., , and Shapiro, L. (2005). A sift descriptor with global context. In *2005 IEEE*  
497 *Computer Society Conference on Computer Vision and Pattern Recognition (CVPR'05)*. vol. 1, 184–190.  
498 doi:10.1109/CVPR.2005.45
- 499 Nam, C. S., Li, Y., and Johnson, S. (2010). Evaluation of P300-based brain-computer interface in real-  
500 world contexts. *International Journal of Human-Computer Interaction* 26, 621–637. doi:10.1080/  
501 10447311003781326
- 502 Nijboer, F. and Broermann, U. (2009). Brain Computer Interfaces for Communication and Control in  
503 Locked-in Patients. In *Graimann B., Pfurtscheller G., Allison B. (eds) Brain-Computer Interfaces. The*  
504 *Frontiers Collection*. (Springer Berlin Heidelberg). 185–201. doi:10.1007/978-3-642-02091-9\_11
- 505 Novak, D., Sigrist, R., Gerig, N. J., Wyss, D., Bauer, R., Gotz, U., et al. (2018). Benchmarking brain-  
506 computer interfaces outside the laboratory: The cybathlon 2016. *Frontiers in Neuroscience* 11, 756.  
507 doi:10.3389/fnins.2017.00756

- 508 Polich, J. (2007). Updating P300: An integrative theory of P3a and P3b. *Clinical Neurophysiology* 118,  
509 2128–2148. doi:10.1016/j.clinph.2007.04.019
- 510 Rakotomamonjy, A. and Guigue, V. (2008). BCI Competition III: Dataset II- Ensemble of SVMs for BCI  
511 P300 Speller. *IEEE Transactions on Biomedical Engineering* 55, 1147–1154. doi:10.1109/TBME.2008.  
512 915728
- 513 Ramele, R., Villar, A. J., and Santos, J. M. (2016). BCI classification based on signal plots and SIFT  
514 descriptors. In *4th International Winter Conference on Brain-Computer Interface, BCI 2016* (Yongpyong:  
515 IEEE), 1–4. doi:10.1109/IWW-BCI.2016.7457454
- 516 [Dataset] Ramele, R., Villar, A. J., and Santos, J. M. (2017). P300-dataset rrid scr\_015977.  
517 <https://www.kaggle.com/rramele/p300samplingdataset>
- 518 Rao, R. P. N. (2013). *Brain-Computer Interfacing: An Introduction* (New York, NY, USA: Cambridge  
519 University Press)
- 520 Renard, Y., Lotte, F., Gibert, G., Congedo, M., Maby, E., Delannoy, V., et al. (2010). OpenViBE: An  
521 Open-Source Software Platform to Design, Test, and Use Brain-Computer Interfaces in Real and Virtual  
522 Environments. *Presence: Teleoperators and Virtual Environments* 19, 35–53. doi:10.1162/pres.19.1.35
- 523 Riccio, A., Simione, L., Schettini, F., Pizzimenti, A., Inghilleri, M., Belardinelli, M. O., et al. (2013).  
524 Attention and P300-based BCI performance in people with amyotrophic lateral sclerosis. *Frontiers in  
525 Human Neuroscience* 7, 732. doi:10.3389/fnhum.2013.00732
- 526 Riener, R. and Seward, L. J. (2014). Cybathlon 2016. *2014 IEEE International Conference on Systems,  
527 Man, and Cybernetics (SMC)*, 2792–2794doi:10.1109/SMC.2014.6974351
- 528 Schalk, G., McFarland, D. J., Hinterberger, T., Birbaumer, N., and Wolpaw, J. R. (2004). BCI2000: a  
529 general-purpose brain-computer interface (BCI) system. *IEEE transactions on bio-medical engineering*  
530 51, 1034–43. doi:10.1109/TBME.2004.827072
- 531 Scholkopf, B. and Smola, A. J. (2001). *Learning with kernels: support vector machines, regularization,  
532 optimization, and beyond* (MIT press)
- 533 Schomer, D. L. and Silva, F. L. D. (2010). *Niedermeyer's Electroencephalography: Basic Principles,  
534 Clinical Applications, and Related Fields* (Walters Klutter -Lippincott Williams & Wilkins)
- 535 Sellers, E. W., Kübler, A., and Donchin, E. (2006). Brain-computer interface research at the University of  
536 South Florida cognitive psychophysiology laboratory: The P300 speller. *IEEE Transactions on Neural  
537 Systems and Rehabilitation Engineering* 14, 221–224. doi:10.1109/TNSRE.2006.875580
- 538 Tibon, R. and Levy, D. A. (2015). Striking a balance: analyzing unbalanced event-related potential data.  
539 *Frontiers in psychology* 6, 555. doi:10.3389/fpsyg.2015.00555
- 540 Van De Sande, K., Gevers, T., and Snoek, C. (2010). Evaluating color descriptors for object and  
541 scene recognition. *IEEE Transactions on Pattern Analysis and Machine Intelligence* 32, 1582–1596.  
542 doi:10.1109/TPAMI.2009.154
- 543 Van Drongelen, W. (2006). *Signal processing for neuroscientists: an introduction to the analysis of  
544 physiological signals* (Academic press)
- 545 Vedaldi, A. and Fulkerson, B. (2010). VLFeat - An open and portable library of computer vision algorithms.  
546 *Design* 3, 1–4. doi:10.1145/1873951.1874249
- 547 Wolpaw, J. and E., W. (2012). *Brain-Computer Interfaces: Principles and Practice* (Oxford University  
548 Press)
- 549 Yamaguchi, T., Fujio, M., Inoue, K., and Pfurtscheller, G. (2009). Design method of morphological  
550 structural function for pattern recognition of EEG signals during motor imagery and cognition. In *Fourth  
551 International Conference on Innovative Computing, Information and Control (ICICIC)*. 1558–1561.  
552 doi:10.1109/ICICIC.2009.161

**Table 1.** Character recognition rates for the public dataset of ALS patients using the Histogram of Gradient (HIST) calculated from single-channel plots. Performance rates using single-channel signals with the SVM classifier are shown for comparison. The best performing channel *bpc* for each method is visualized

Participant	<i>bpc</i>	HIST	<i>bpc</i>	Single Channel SVM
1	Cz	35%	Cz	15%
2	Fz	85%	PO8	25%
3	Cz	25%	Fz	5%
4	PO8	55%	Oz	5%
5	PO7	40%	P3	25%
6	PO7	60%	PO8	20%
7	PO8	80%	Fz	30%
8	PO7	95%	PO7	85%

**Table 2.** Character recognition rates for the own dataset of healthy subjects using the Histogram of Gradient (HIST) calculated from single-channel plots. Performance rates using single-channel signals with the SVM classifier are shown for comparison. The best performing channel *bpc* for each method is visualized.

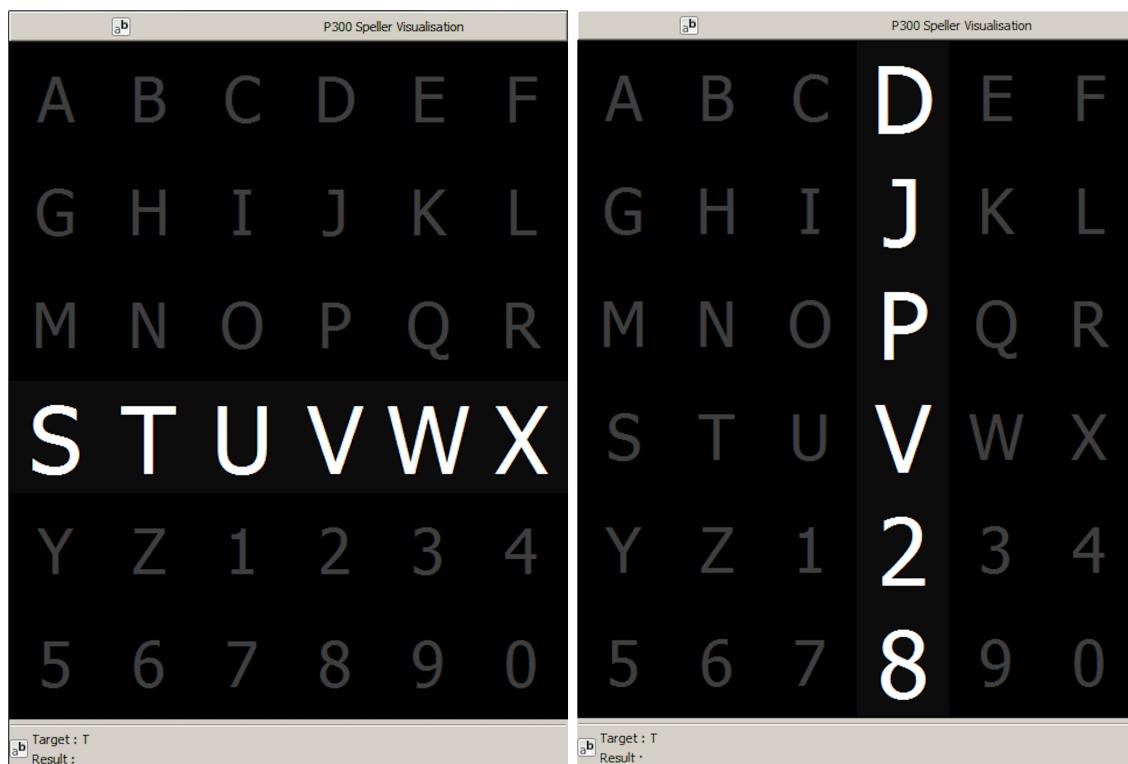
Participant	<i>bpc</i>	HIST	<i>bpc</i>	Single Channel SVM
1	Oz	40%	Cz	10%
2	PO7	30%	Cz	5%
3	P4	40%	P3	10%
4	P4	45%	P4	35%
5	P4	60%	P3	10%
6	Pz	50%	P4	25%
7	PO7	70%	P3	30%
8	P4	50%	PO7	10%

**Table 3.** Character recognition rates and the best performing channel *bpc* for the public dataset of ALS patients using the Histogram of Gradient (HIST) (repeated here for comparison purposes). Performance rates obtained by SWLDA and SVM classification algorithms with a multichannel concatenated feature.

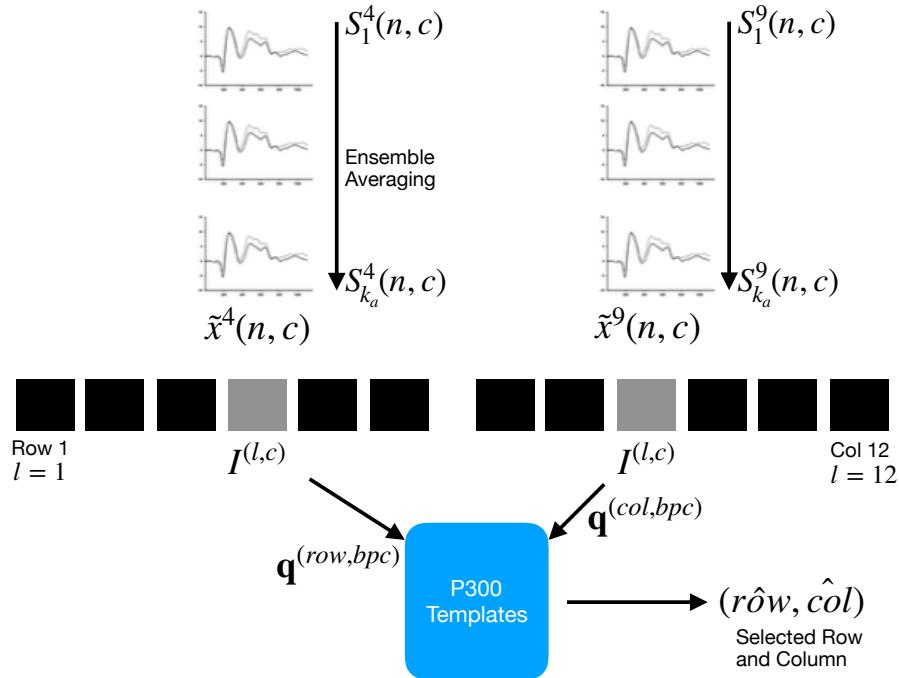
Participant	<i>bpc</i> for HIST	HIST	Multichannel SWLDA	Multichannel SVM
1	Cz	35%	45%	40%
2	Fz	85%	30%	50%
3	Cz	25%	65%	55%
4	PO8	55%	40%	50%
5	PO7	40%	35%	45%
6	PO7	60%	35%	70%
7	PO8	80%	60%	35%
8	PO7	95%	90%	95%

**Table 4.** Character recognition rates and the best performing channel *bpc* for the own dataset of healthy subjects using the Histogram of Gradient (HIST) (repeated here for comparison purposes). Performance rates obtained by SWLDA and SVM classification algorithms with a multichannel concatenated feature.

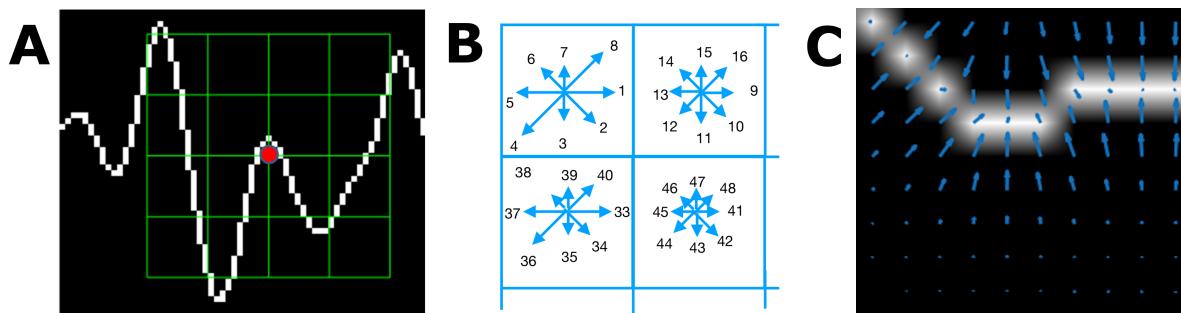
Participant	<i>bpc</i> for HIST	HIST	Multichannel SWLDA	Multichannel SVM
1	Oz	40%	65%	40%
2	PO7	30%	15%	10%
3	P4	40%	50%	25%
4	P4	45%	40%	20%
5	P4	60%	30%	20%
6	Pz	50%	35%	30%
7	PO7	70%	25%	30%
8	P4	50%	35%	20%



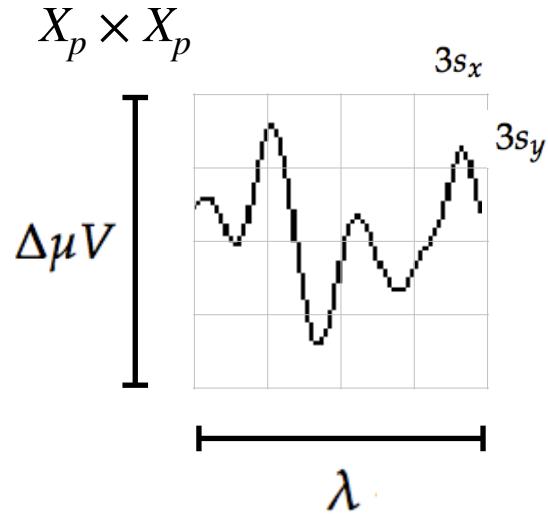
**Figure 1.** Example of the  $6 \times 6$  Speller Matrix used in the study obtained from the OpenVibe software. Rows and columns flash in random permutations.



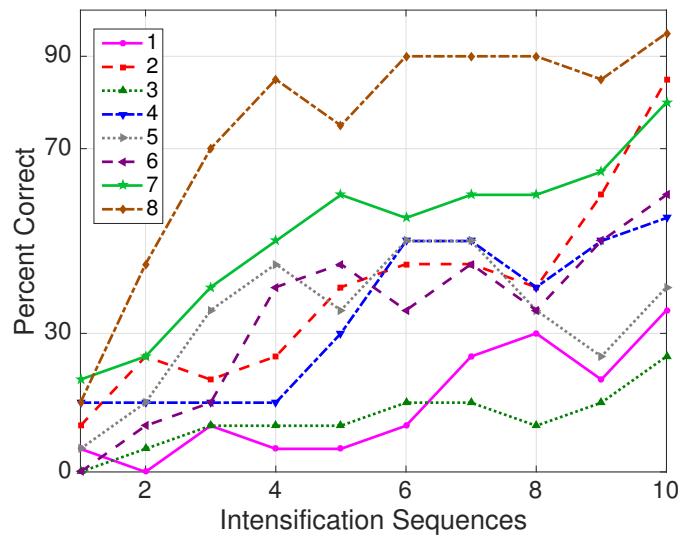
**Figure 2.** For each column and row, an averaged, standardized and scaled signal  $\tilde{x}^l(n, c)$  is obtained from the segments  $S_i^l$  corresponding to the  $k_a$  intensification sequences with  $1 \leq i \leq k_a$  and location  $l$  varying between 1 and 12. From the averaged signal, the image  $I^{(l,c)}$  of the signal plot is generated and each descriptor is computed. By comparing each descriptor against the set of templates, the P300 ERP can be detected, and finally the desired letter from the matrix can be inferred.



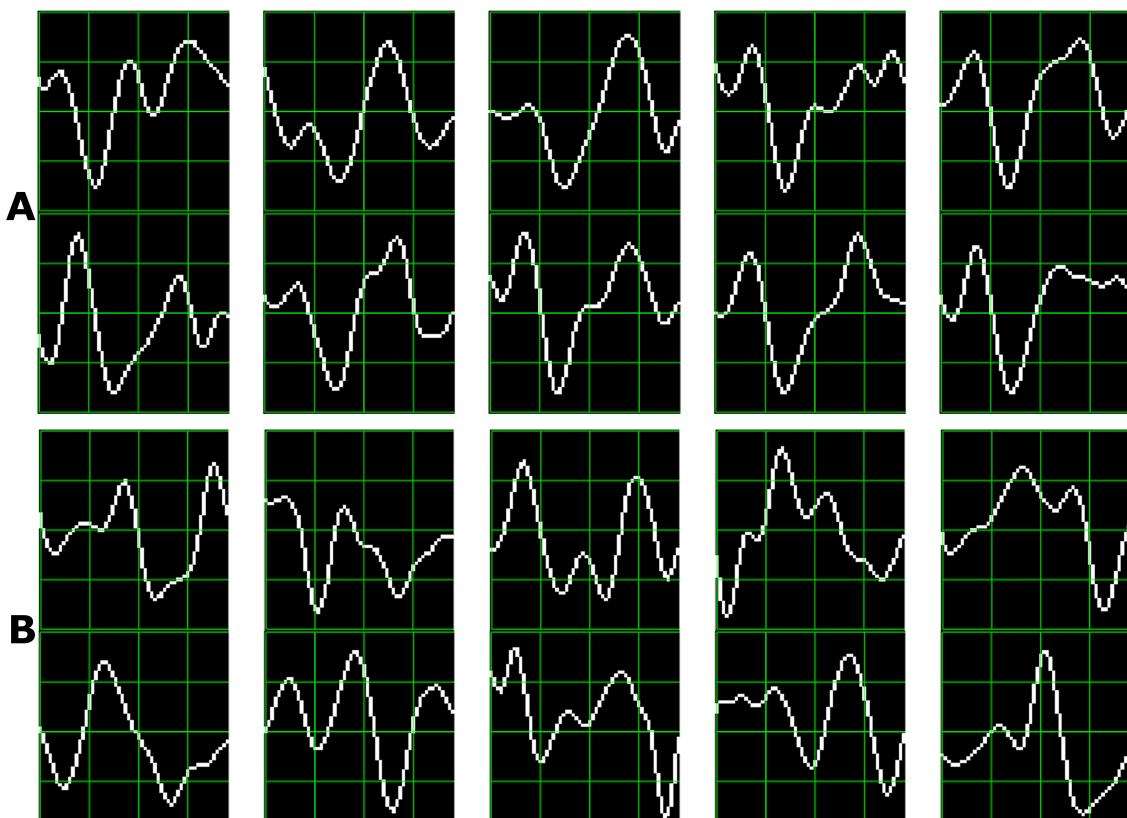
**Figure 3.** (A) Example of a plot of the signal, a keypoint and the corresponding patch. (B) A scheme of the orientation's histogram computation. Only the upper-left four blocks are visible. The first eight orientations of the first block, are labeled from 1 to 8 clockwise. The orientation of the second block  $B_{1,2}$  is labeled from 9 to 16. This labeling continues left-to-right, up-down until the eight orientations for all the sixteen blocks are assigned. They form the corresponding descriptor of 128 coordinates. The length of each arrow represent the value of the histogram on each direction for each block. (C) Vector field of oriented gradients. Each pixel is assigned an orientation and magnitude calculated using finite differences.



**Figure 4.** The scale of local patch is selected in order to capture the whole transient event. The size of the patch is  $X_p \times X_p$  pixels. The vertical size consists of 4 blocks of size  $3s_y$  pixels which is high enough as to contain the signal  $\Delta\mu V$ , the peak-to-peak amplitude of the transient event. The horizontal size includes 4 blocks of  $3s_x$  and covers the entire duration in seconds of the transient signal event,  $\lambda$ .



**Figure 5.** Performance curves for the eight subjects included in the dataset of ALS patients. Three out of eight subjects achieved the necessary performance to implement a valid P300 speller.



**Figure 6.** Ten sample P300 template patches for subjects 8 (A) and 3 (B) of the ALS Dataset. Downward deflection is positive polarity.