

Histogram of Gradient Orientations of Signal Plots applied to P300 Detection

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2 ABSTRACT

3 Word Count: 5132

4 The analysis of Electroencephalographic (EEG) signals is of ulterior importance to aid in the
5 diagnosis of mental disease and to increase our understanding of the brain. Traditionally, clinical
6 EEG has been analyzed in terms of temporal waveforms, looking at rhythms in spontaneous
7 activity, subjectively identifying troughs and peaks in Event-Related Potentials (ERP), or by
8 studying graphoelements in pathological sleep stages. Additionally, the discipline of Brain
9 Computer Interfaces requires new methods to decode patterns from non-invasive EEG signals.
10 This field is developing alternative communication pathways to transmit volitional information
11 from the Central Nervous System. The technology could potentially enhance the quality of life
12 of patients affected by neurodegenerative disorders and other mental illness. This work mimics
13 what electroencephalographers have been doing clinically, visually inspecting and categorizing
14 phenomena within the EEG by the extraction of features from images of signal plots. These
15 features are constructed based on the calculation of histograms of oriented gradients from pixels
16 around the signal plot. It aims to provide a new objective framework to analyze, characterize and
17 classify EEG signal waveforms. The feasibility of the method is outlined by detecting the P300, an
18 ERP elicited by the oddball paradigm of rare events, and implementing an offline P300-based BCI
19 Speller. The validity of the proposal is shown by offline processing a public dataset of Amyotrophic
20 Lateral Sclerosis (ALS) patients and an own dataset of healthy subjects.

21 **Keywords:** **electroencephalography, histogram of gradient orientations, brain-computer interfaces, P300, SIFT, amyotrophic lateral**
22 **sclerosis, naive-bayes near neighbours, waveforms**

1 INTRODUCTION

23 Although recent advances in neuroimaging techniques, particularly radio-nuclear and radiological
24 scanning methods (Schomer and Silva, 2010), have diminished the prospects of the traditional
25 Electroencephalography (EEG), the advent and development of digitized devices has impelled for a
26 revamping of this hundred years old technology. Their versatility, ease of use, temporal resolution, ease of
27 development and production, and its proliferation as consumer devices, are pushing EEG to become the
28 de-facto non invasive portable or ambulatory method to access and harness brain information (De Vos and
29 Debener, 2014).

30 A key contribution to this expansion has been the field of Brain Computer Interfaces (BCI) (Wolpaw and
31 E., 2012) which is the pursuit of the development of a new channel of communication particularly aimed to
32 persons affected by neurodegenerative diseases.

33 One noteworthy aspect of this novel communication channel is the ability to transmit information from
34 the Central Nervous System (CNS) to a computer device and from there use that information to control a
35 wheelchair (Carlson and del R. Millan, 2013), as input to a speller application (Guger et al., 2009), in a
36 Virtual Reality environment (Lotte et al., 2013) or as aiding tool in a rehabilitation procedure (Jure et al.,
37 2016). The holly grail of BCI is to implement a new complete and alternative pathway to restore lost
38 locomotion (Wolpaw and E., 2012).

39 EEG signals are remarkably complex and have been characterized as a multichannel non-stationary
40 stochastic process. Additionally, they have high variability between different subjects and even between
41 different moments for the same subject, requiring adaptive and co-adaptive calibration and learning
42 procedures (Clerc et al., 2016). Hence, this imposes an outstanding challenge that is necessary to overcome
43 in order to extract information from raw EEG signals.

44 BCI has gained mainstream public awareness with worldwide challenge competitions like
45 Cybathlon (Riener and Seward, 2014; Novak et al., 2018) and even been broadcasted during the inauguration
46 ceremony of the 2014 Soccer World Cup. New developments have overcome the out-of-the-lab high-bar
47 and they are starting to be used in real world environments (Guger et al., 2017; Huggins et al., 2016).
48 However, they still lack the necessary robustness, and its performance is well behind any other method of
49 human computer interaction, including any kind of detection of residual muscular movement (Clerc et al.,
50 2016).

51 A few works have explored the idea of exploiting the signal waveform to analyze the EEG signal.
52 In (Alvarado-González et al., 2016) an approach based on Slope Horizontal Chain Code is presented,
53 whereas in (Yamaguchi et al., 2009) a similar procedure was implemented based on Mathematical
54 Morphological Analysis. The seminal work of Bandt-Pompe Permutation Entropy (Berger et al., 2017) also
55 explores succinctly this idea as a basis to establish the time series ordinal patterns. In the article (Ramele
56 et al., 2016), the authors introduce a method for classification of rhythmic EEG events like Visual Occipital
57 Alpha Waves and Motor Imagery Rolandic Central μ Rhythms using the Histogram of Gradient Orientations
58 of signal plots. Inspired in that work, we propose a novel application of the developed method to classify
59 and describe transient events, particularly the P300 Event Related Potential. The proposed approach is
60 based on the waveform analysis of the shape of the EEG signal. The signal is drawn on a bidimensional
61 image plot, vector gradients of pixels around the plot are obtained, and with them, the histogram of their
62 orientations is calculated. This histogram is a direct representation of the waveform of the signal. The
63 method is built by mimicking what regularly electroencephalographers have been performing for almost a
64 century as it is described in (Hartman, 2005): visually inspecting raw signal plots.

65 This paper reports a method to, (1) describe a procedure to capture the shape of a waveform of an ERP
66 component, the P300, using histograms of gradient orientations extracted from images of signal plots,
67 and (2) outline the way in which this procedure can be used to implement an P300-Based BCI Speller
68 application. Its validity is verified by offline processing two datasets, one of data from ALS patients and
69 another one from data of healthy subjects.

70 This article unfolds as follows: Section 2.1 is dedicated to explain the Feature Extraction method based
71 on Histogram of Gradient Orientations of the Signal Plot: Section 2.1.1 shows the preprocessing pipeline,
72 Section 2.1.2 describes the image generation of the signal plot, Section 2.1.3 presents the feature extraction

73 procedure while Section 2.1.4 introduces the Speller Matrix Letter Identification procedure. In Section 2.2,
74 the experimental protocol is expounded. Section 3 shows the results of applying the proposed technique. In
75 the final Section 4 we expose our remarks, conclusions and future work.

2 MATERIALS AND METHODS

76 The P300 (Farwell and Donchin, 1988; Knuth et al., 2006) is a positive deflection of the EEG signal which
77 occurs around 300 ms after the onset of a rare and deviant stimulus that the subject is expected to attend. It
78 is produced under the oddball paradigm (Wolpaw and E., 2012) and it is consistent across different subjects.
79 It has a lower amplitude ($\pm 5\mu V$) compared to basal EEG activity, reaching a Signal to Noise Ratio (SNR)
80 of around -15 db estimated based on the amplitude of the P300 response signal divided by the standard
81 deviation of the background EEG activity (Hu et al., 2010). This signal can be used to implement a speller
82 application by means of a Speller Matrix (Farwell and Donchin, 1988). This matrix is composed of 6 rows
83 and 6 columns of numbers and letters. The subject can focus on one character of the matrix. Figure 1 shows
84 an example of the Speller Matrix used in the OpenVibe open source software (Renard et al., 2010), where
85 the flashes of rows and columns provide the deviant stimulus required to elicit this physiological response.
86 Each time a row or a column that contains the desired letter flashes, the corresponding synchronized EEG
87 signal should also contain the P300 signature and by detecting it, the selected letter can be identified.

88 2.1 Feature Extraction from Signal Plots

89 In this section, the signal preprocessing, the method for generating images from signal plots, the feature
90 extraction procedure and the Speller Matrix identification are described. Figure 2 shows a scheme of the
91 entire process.

92 2.1.1 Preprocessing Pipeline

93 The data obtained by the capturing device is digitalized and a multichannel EEG signal is constructed.
94 The 6 rows and 6 columns of the Speller Matrix are intensified providing the visual stimulus. The
95 number of a row or column is a location. A sequence of twelve randomly permuted locations l conform an
96 intensification sequence. The whole set of twelve intensifications is repeated k_a times.

- 97 • **Signal Enhancement:** This stage consists of the enhancement of the SNR of the P300 pattern above
98 the level of basal EEG. The pipeline starts by applying a notch filter to the raw digital signal, a 4th
99 degree 10 Hz lowpass Butterworth filter and finally a decimation with a Finite Impulse Response (FIR)
100 filter of order 30 from the original sampling frequency down to 16 Hz (Krusienski et al., 2006).
- 101 • **Artifact Removal:** For every complete sequence of 12 intensifications of 6 rows and 6 columns, a
102 basic artifact elimination procedure is implemented by removing the entire sequence when any signal
103 deviates above/below $\pm 70\mu V$.
- 104 • **Segmentation:** For each of the 12 intensifications of one intensification sequence, a segment S_i^l
105 of a window of t_{max} seconds of the multichannel signal is extracted, starting from the stimulus
106 onset, corresponding to each row/column intensification l and to the intensification sequence i . As
107 intensifications are permuted in a random order, the segments are rearranged corresponding to row
108 flickering, labeled 1-6, whereas those corresponding to column flickering are labeled 7-12. Two of
109 these segments should contain the P300 ERP signature time-locked to the flashing stimulus, one for
110 the row, and one for the column.

111 • **Signal Averaging:** The P300 ERP is deeply buried under basal EEG so the standard approach to
 112 identify it is by point-to-point averaging the time-locked stacked signal segments. Hence the values
 113 which are not related to, and not time-locked to the onset of the stimulus are canceled out (Liang and
 114 Bougrain, 2008).

115 This last step determines the operation of any P300 Speller. In order to obtain an improved signal
 116 in terms of its SNR, repetitions of the sequence of row/column intensification are necessary. And,
 117 at the same time, as long as more repetitions are needed, the ability to transfer information faster is
 118 diminished, so there is a trade-off that must be acutely determined.

119 The procedure to obtain the point-to-point averaged signal goes as follows:

- 120 1. Highlight randomly the rows and columns from the matrix. There is one row and one column that
 121 should match the letter selected by the subject.
- 122 2. Repeat step 1 k_a times, obtaining the $1 \leq l \leq 12$ segments $S_1^l(n, c), \dots, S_{k_a}^l(n, c)$, of the EEG
 123 signal where the variables $1 \leq n \leq n_{max}$ and $1 \leq c \leq C$ correspond to sample points and channel,
 124 respectively. The parameter C is the number of available EEG channels whereas $n_{max} = F_s t_{max}$
 125 is the segment length and F_s is the sampling frequency. The parameter k_a is the number of
 126 repetitions of intensifications and it is an input parameter of the algorithm.
- 127 3. Compute the Ensemble Average by

$$x^l(n, c) = \frac{1}{k_a} \sum_{i=1}^{k_a} S_i^l(n, c) \quad (1)$$

128 for $1 \leq n \leq n_{max}$ and for the channels $1 \leq c \leq C$. This provide an averaged signal $x^l(n, c)$ for
 129 the twelve locations $1 \leq l \leq 12$.

130 2.1.2 Signal Plotting

131 Averaged signal segments are standardized and scaled for $1 \leq n \leq n_{max}$ and $1 \leq c \leq C$ by

$$\tilde{x}^l(n, c) = \left[\gamma \frac{(x^l(n, c) - \bar{x}^l(c))}{\hat{\sigma}^l(c)} \right] \quad (2)$$

where $\gamma > 0$ is an input parameter of the algorithm and it is related to the image scale. In addition, $x^l(n, c)$ is the point-to-point averaged multichannel EEG signal for the sample point n and for channel c . Lastly,

$$\bar{x}^l(c) = \frac{1}{n_{max}} \sum_{n=1}^{n_{max}} x^l(n, c)$$

and

$$\hat{\sigma}^l(c) = \left(\frac{1}{n_{max} - 1} \sum_{n=1}^{n_{max}} (x^l(n, c) - \bar{x}^l(c))^2 \right)^{\frac{1}{2}}$$

132 are the mean and estimated standard deviation of $x^l(n, c)$, $1 \leq n \leq n_{max}$, for each channel c .

133 Consequently, a binary image $I^{(l,c)}$ is constructed according to

$$I^{(l,c)}(z_1, z_2) = \begin{cases} 255 & \text{if } z_1 = \gamma n; z_2 = \tilde{x}^l(n, c) + z^l(c) \\ 0 & \text{otherwise} \end{cases} \quad (3)$$

134 with 255 being white and representing the signal's value location and 0 for black which is the background
 135 contrast, conforming a black-and-white plot of the signal. Pixel arguments $(z_1, z_2) \in \mathbb{N} \times \mathbb{N}$ iterate over
 136 the width (based on the length of the signal segment) and height (based on the peak-to-peak amplitude) of
 137 the newly created image with $1 \leq n \leq n_{max}$ and $1 \leq c \leq C$. The value $z^l(c)$ is the image vertical position
 138 where the signal's zero value has to be situated in order to fit the entire signal within the image for each
 139 channel c :

$$z^l(c) = \left\lfloor \frac{\max_n \tilde{x}^l(n, c) - \min_n \tilde{x}^l(n, c)}{2} \right\rfloor - \left\lfloor \frac{\max_n \tilde{x}^l(n, c) + \min_n \tilde{x}^l(n, c)}{2} \right\rfloor \quad (4)$$

140 where the minimization and maximization are carried out for n varying between $1 \leq n \leq n_{max}$, and $\lfloor \cdot \rfloor$
 141 denote the rounding to the smaller nearest integer of the number.

142 In order to complete the plot $I^{(l,c)}$ from the pixels, the Bresenham (Bresenham, 1965; Ramele et al.,
 143 2016) algorithm is used to interpolate straight lines between each pair of consecutive pixels.

144 2.1.3 Feature Extraction: Histogram of Gradient Orientations

145 The work of Edelman, Intrator and Poggio (Edelman et al., 1997) on how the visual cortex sense features
 146 was the inspiration to the development of an algorithm to identify and decode salient local information
 147 from image regions. The Scale Invariant Feature Transform (SIFT) is a Computer Vision method proposed
 148 by Lowe (2004) which is composed of two parts, the SIFT Detector and the SIFT Descriptor. The former
 149 is the procedure to identify relevant areas of an image whereas the latter is the procedure to describe and
 150 characterize a region of an image (i.e. patch) calculating an histogram of the gradient orientations. In
 151 order to characterize EEG signal waveforms, this work proposes an alternative Histogram of Gradient
 152 Orientations algorithm. We stripped away all the details which are not used and refined the procedure to
 153 enable the effective capturing of the waveform shape.

154 For each generated image $I^{(l,c)}$, a keypoint p_k is placed on a pixel (x_{p_k}, y_{p_k}) over the image plot and a
 155 window around the keypoint is considered. A local image patch of size $X_p \times X_p$ pixels is constructed by
 156 dividing the window in 16 blocks of size $3s$ each one, where s is the scale of the local patch and it is an
 157 input parameter of the algorithm. It is arranged in a 4×4 grid and the pixel p_k is the patch center, thus
 158 $X_p = 12s$ pixels.

159 A local representation of the signal shape within the patch can be described by obtaining the gradient
 160 orientations on each of the 16 blocks $B_{i,j}$ with $0 \leq i, j \leq 3$ and creating a histogram of gradients. In
 161 order to calculate the histogram, the interval $[0, 360]$ of possible angles is divided in 8 bins, each one of 45
 162 degrees.

163 Hence, for each spatial bin $0 \leq i, j \leq 3$, corresponding to the indexes of each block $B_{i,j}$, the orientations
 164 are accumulated in a 3-dimensional histogram h through the following equation:

$$h(\theta, i, j) = 3s \sum_{\mathbf{p} \in I^{(l,c)}} w_{ang}(\angle J(\mathbf{p}) - \theta) w_{ij} \left(\frac{\mathbf{p} - \mathbf{p}_k}{3s} \right) \|J(\mathbf{p})\| \quad (5)$$

165 where \mathbf{p} is a pixel from the image $I^{(l,c)}$, θ is the angle bin with $\theta \in \{0, 45, 90, 135, 180, 225, 270, 315\}$,
 166 $\|J(\mathbf{p})\|$ is the norm of the gradient vector in the pixel \mathbf{p} and it is computed using finite differences and
 167 $\angle J(\mathbf{p})$ is the angle of the gradient vector.

168 The contribution of each gradient vector to the histogram calculated by equation 5 is balanced by a
 169 trilinear interpolation. The scalar $w_{\text{ang}}(\cdot)$ and vector $w_{ij}(\cdot)$ functions are linear interpolations used by Lowe
 170 (2004) and Vedaldi and Fulkerson (2010) to provide a weighting contribution to the eight adjacent bins in
 171 the tridimensional histogram. They are calculated as

$$w_{ij}(\mathbf{v}) = w(v_x - x_i)w(v_y - y_j) \quad (6)$$

172 with $0 \leq i, j \leq 3$ and

$$w_{\text{ang}}(\alpha) = \sum_{r=-1}^1 w\left(\frac{8\alpha}{2\pi} + 8r\right) \quad (7)$$

173 where x_i and y_i are the spatial bin centers located in $x_i, y_j \in \{-\frac{3}{2}, -\frac{1}{2}, \frac{1}{2}, \frac{3}{2}\}$. The function parameter
 174 $\mathbf{v} = (v_x, v_y)$ is a vector variable and α a scalar variable. Vector \mathbf{v} holds pixel \mathbf{p} coordinates on the image
 175 in normalized bin units. On the other hand, r is an integer that can vary freely in the set $\{-1, 0, 1\}$ and
 176 allows the argument α to be unconstrained in terms of its values in radians. The interpolating function $w(\cdot)$
 177 is defined as $w(z) = \max(0, |z| - 1)$.

178 These binning functions conform the trilinear interpolation that has a combined effect of sharing the
 179 contribution of each oriented gradient between their eight adjacent bins in a tridimensional cube in the
 180 histogram space, and zero everywhere else (Mortensen et al., 2005).

181 Lastly, the fixed value of 3 is a magnification factor which corresponds to the number of pixels per each
 182 block when $s = 1$. As the patch has 16 blocks and 8 bin angles are considered, for each location l and
 183 channel c a feature called *descriptor* $\mathbf{d}^{(l,c)}$ of 128 dimension is obtained.

184 Figure 3 shows an example of a patch and a scheme of the histogram computation. In (A) a plot of the
 185 signal and the patch centered around the keypoint is shown. In (B) the possible orientations on each patch
 186 are illustrated. Only the upper-left four blocks are visible. The first eight orientations of the first block, are
 187 labeled from 1 to 8 clockwise. The orientations of the second block $B_{1,2}$ are labeled from 9 to 16. This
 188 labeling continues left-to-right, up-down until the eight orientations for all the sixteen blocks are assigned.
 189 They form the corresponding descriptor \mathbf{d} of 128 coordinates. Finally, in (C) an enlarged image plot is
 190 shown where the oriented gradient vector for each pixel can be seen.

191 2.1.4 Speller Matrix letter Identification

192 2.1.4.1 P300 ERP Extraction

193 Segments corresponding to row flickering are labeled 1-6, whereas those corresponding to column
 194 flickering are labeled 7-12. The extraction process has the following steps:

- 195 • **Step A:** First highlight rows and columns from the matrix in a random permutation order and obtain
 196 the Ensemble Average as detailed in steps 1, 2 and 3 in Section 2.1.1.
- 197 • **Step B:** Plot the signals $\tilde{x}^l(n, c)$, $1 \leq n \leq n_{\text{max}}$, $1 \leq c \leq C$, according Section 2.1.2 in order to
 198 generate the images $I^{(l,c)}$ for rows and columns $1 \leq l \leq 12$.
- 199 • **Step C:** Obtain the descriptors $\mathbf{d}^{(l,c)}$ for rows and columns from $I^{(l,c)}$ in accordance to the method
 200 described in Section 2.1.3.

201 **2.1.4.2 Calibration**

202 A trial, as defined by the BCI2000 platform (Schalk et al., 2004), is every attempt to select just one letter
 203 from the speller. A set of trials is used for calibration and once the calibration is complete it can be used to
 204 identify new letters from new trials.

205 During the calibration phase, two descriptors $\mathbf{d}^{(l,c)}$ are extracted for each available channel, corresponding
 206 to the locations l of a selection of one previously instructed letter from the set of calibration trials. These
 207 descriptors are the P300 templates, grouped together in a template set called T^c . The set is constructed
 208 using the steps described in Section 2.1.1 and the steps A, B and C of the P300 ERP extraction process.

209 Additionally, the best performing channel, bpc is identified based on the the channel where the best
 210 Character Recognition Rate is obtained.

211 **2.1.4.3 Letter identification**

212 In order to identify the selected letter, the template set T^{bpc} is used as a database. Thus, new unclassified
 213 descriptors $\mathbf{q}^{(l,bpc)}$ are computed and they are compared against the descriptors belonging to the calibration
 214 template set T^{bpc} .

215 The Naive Bayes Nearest Neighbor (k-NBNN) (Boiman et al., 2008) is a classification algorithm that
 216 allows the categorization of an image to one class by comparing the set of extracted descriptors to those
 217 which are more similar from template dictionaries. This work propose an adapted discriminative (Wolpaw
 218 and E., 2012) semi-supervised unary classification scheme to identify the selected letter in the P300-Based
 219 BCI Speller, based on the features provided by the calculated descriptors.

220 • **Step D:** Match to the calibration template T^{bpc} by computing

$$r\hat{o}w = \arg \min_{l \in \{1, \dots, 6\}} \sum_{h=1}^k \left\| \mathbf{q}^{(l,bpc)} - \mathbf{d}_h^{(bpc)} \right\|^2 \quad (8)$$

221 and

$$\hat{c}ol = \arg \min_{l \in \{7, \dots, 12\}} \sum_{h=1}^k \left\| \mathbf{q}^{(l,bpc)} - \mathbf{d}_h^{(bpc)} \right\|^2 \quad (9)$$

222 with $\mathbf{d}_h^{(bpc)}$ belonging to the set $N_T(\mathbf{q}^{(l,bpc)})$, which is defined, for the best performing channel, as
 223 $N_T(\mathbf{q}^{(l,bpc)}) = \{\mathbf{d}_h^{(bpc)} \in T^{bpc} / \mathbf{d}_h^{(bpc)} \text{ is the } k\text{-nearest neighbor of } \mathbf{q}^{(l,bpc)}\}$. This set is obtained by
 224 sorting all the elements in T^{bpc} based on distances between them and $\mathbf{q}^{(l,bpc)}$, choosing the k with
 225 smaller values, with k a parameter of the algorithm.

226 By computing the aforementioned equations, the letter of the matrix can be determined from the intersection
 227 of the row $r\hat{o}w$ and column $\hat{c}ol$. Figure 2 shows a scheme of this process.

228 **2.2 Experimental Protocol**

229 To verify the validity of the proposed framework and method, the public dataset 008-2014 (Riccio et al.,
 230 2013) published on the BNCI-Horizon website (Brunner et al., 2014) by IRCCS Fondazione Santa Lucia,
 231 is used. Additionally, an own dataset with the same experimental conditions is generated. Both of them are
 232 utilized to perform an offline BCI Simulation to decode the spelled words from the provided signals.

233 The algorithm is implemented on MATLAB V2017a (Mathworks Inc., Natick, MA, USA). The algorithm
234 described in 2.1.3 is written on a modified version of the VLFeat (Vedaldi and Fulkerson, 2010) Computer
235 Vision library. Furthermore, in order to enhance the impact of this paper and for a sake of reproducibility,
236 the code of the entire algorithm, including the modified VLFeat library, has been made available at:
237 <https://bitbucket.org/itba/hist>.

238 In the following sections the characteristics of the datasets and parameters of the identification algorithm
239 are described.

240 2.2.1 P300 ALS Public Dataset

241 The experimental protocol used to generate this dataset is explained in (Riccio et al., 2013) but can
242 be summarized as follows: 8 subjects with confirmed diagnoses but on different stages of ALS disease,
243 were recruited and accepted to perform the experiments. The Visual P300 detection task designed for this
244 experiment consisted of spelling 7 words of 5 letters each, using the traditional P300 Speller Matrix (Farwell
245 and Donchin, 1988). The flashing of rows and columns provide the deviant stimulus required to elicit this
246 physiological response. The first 3 words are used for calibration and the remaining 4 words, for testing
247 with visual feedback. A trial is every attempt to select a letter from the speller. It is composed of signal
248 segments corresponding to $k_a = 10$ repetitions of flashes of 6 rows and $k_a = 10$ repetitions of flashes of
249 6 columns of the matrix, yielding 120 repetitions. Flashing of a row or a column is performed for 0.125
250 s, following by a resting period (i.e. inter-stimulus interval) of the same length. After 120 repetitions an
251 inter-trial pause is included before resuming with the following letter.

252 The recorded dataset was sampled at 256 Hz and it consisted of a scalp multichannel EEG signal for
253 electrode channels Fz, Cz, Pz, Oz, P3, P4, PO7 and PO8, identified according to the 10-20 International
254 System, for each one of the 8 subjects. The recording device was a research-oriented digital EEG device
255 (g.Mobilab, g.Tec, Austria) and the data acquisition and stimuli delivery were handled by the BCI2000
256 open source software (Schalk et al., 2004).

257 In order to assess and verify the identification of the P300 response, subjects are instructed to perform a
258 copy-spelling task. They have to fix their attention to successive letters for copying a previously determined
259 set of words, in contrast to a free-running operation of the speller where each user decides on its own what
260 letter to choose.

261 2.2.2 P300 for healthy subjects

262 We replicate the same experiment on healthy subjects using a wireless digital EEG device (g.Nautilus,
263 g.Tec, Austria). The experimental conditions are the same as those used for the previous dataset, as detailed
264 in section 2.2.1. The produced dataset is available in a public online repository (Ramele et al., 2017).

265 Participants are recruited voluntarily and the experiment is conducted anonymously in accordance with
266 the Declaration of Helsinki published by the World Health Organization. No monetary compensation
267 is handed out and all participants agree and sign a written informed consent. This study is approved
268 by the *Departamento de Investigación y Doctorado, Instituto Tecnológico de Buenos Aires (ITBA)*. All
269 healthy subjects have normal or corrected-to-normal vision and no history of neurological disorders. The
270 experiment is performed with 8 subjects, 6 males, 2 females, 6 right-handed, 2 left-handed, average age
271 29.00 years, standard deviation 11.56 years, range 20-56 years.

272 EEG data is collected in a single recording session. Participants are seated in a comfortable chair, with
 273 their vision aligned to a computer screen located one meter in front of them. The handling and processing
 274 of the data and stimuli is conducted by the OpenVibe platform (Renard et al., 2010).

275 Gel-based active electrodes (g.LADYbird, g.Tec, Austria) are used on the same positions Fz, Cz, Pz,
 276 Oz, P3,P4, PO7 and PO8. Reference is set to the right ear lobe and ground is preset as the AFz position.
 277 Sampling frequency is slightly different, and is set to 250 Hz, which is the closest possible to the one used
 278 with the other dataset.

279 **2.2.3 Parameters**

280 The patch size is $X_P = 12s \times 12s$ pixels, where s is the scale of the local patch and it is an input parameter
 281 of the algorithm. The P300 event can have a span of 400 ms and its amplitude can reach $10\mu V$ (Rao, 2013).
 282 Hence it is necessary to utilize a signal segment of size $t_{max} = 1$ second and a size patch X_P that could
 283 capture an entire transient event. With this purpose in consideration, the s value election is essential.

284 We propose the Equations 10 and 11 to compute the scale value in horizontal and vertical directions,
 285 respectively.

$$s_x = \frac{\gamma \lambda F_s}{12} \quad (10)$$

$$s_y = \frac{\gamma \Delta\mu V}{12} \quad (11)$$

286 where λ is the length in seconds covered by the patch, F_s is the sampling frequency of the EEG signal
 287 (downsampled to 16 Hz) and $\Delta\mu V$ corresponds to the amplitude in microvolts that can be covered by the
 288 height of the patch. The geometric structure of the patch forces a squared configuration, then we discerned
 289 that by using $s = s_x = s_y = 3$ and $\gamma = 4$, the local patch and the descriptor can identify events of $9\mu V$
 290 of amplitude, with a span of $\lambda = 0.56$ seconds. This also determines that 1 pixel represents $\frac{1}{\gamma} = \frac{1}{4}\mu V$ on
 291 the vertical direction and $\frac{1}{F_s \gamma} = \frac{1}{64}$ seconds on the horizontal direction. The keypoints p_k are located at
 292 $(x_{p_k}, y_{p_k}) = (0.55F_s \gamma, z^l(c)) = (35, z^l(c))$ for the corresponding channel c and location l (see Equation 4).
 293 In this way the whole transient event is captured. Figure 4 shows a patch of a signal plot covering the
 294 complete amplitude (vertical direction) and the complete span of the signal event (horizontal direction).

295 Moreover, the number of channels C is equal to 8 for both datasets, and the number of intensification
 296 sequences k_a is fixed to 10. The parameter k used to construct the set $N_T(d^{(l,c)})$ is assigned to $k = 7$,
 297 which was found empirically to achieve better results. In addition, the norm used on Equations 8 and 9 is
 298 the cosine norm, and descriptors are normalized to $[-1, 1]$.

299 Lastly, in order to assess the validity of the Histogram of Gradient Orientations (HIST) method, the
 300 character recognition rate for both datasets is evaluated replicating the methodology proposed by the
 301 ALS dataset's publisher, since authors Riccio et al. (2013) did not report the Character Recognition
 302 Rate obtained for this dataset. Frequency filtering, data segmentation and artifact rejection is conducted
 303 according to Section 2.1.1 yielding 16×8 samples per epoch. A multichannel feature consists of time
 304 points vector (Lotte et al., 2018), formed by concatenating all the channels (Krusienski et al., 2006). A
 305 single-channel variant consists of using time points from a single electrode and performing the analysis on
 306 a channel-by-channel basis. Three classification schemes are considered as well. A multichannel version of
 307 the Stepwise Linear Discriminant Analysis (SWLDA) classification algorithm. SWLDA is the methodology
 308 proposed by the ALS dataset's publisher. Additionally, a single-channel and a multichannel variant of a

309 linear kernel Support Vector Machine (SVM) (Scholkopf and Smola, 2001) classifier are utilized. SVM has
310 been successfully used in several BCI Competitions (Rakotomamonjy and Guigue, 2008).

3 RESULTS

311 Table 1 shows the results of applying the HIST algorithm to the subjects of the public dataset of ALS
312 patients. The percentage of correctly spelled letters is calculated while performing an offline BCI Simulation.
313 From the seven words for each subject, the first three are used for calibration, and the remaining four are
314 used for testing. The best performing channel *bpc* is informed as well. The target ratio is 1 : 36; hence
315 theoretical chance level is 2.8%. It can be observed that the best performance of the letter identification
316 method is reached in a dissimilar channel depending on the subject being studied. Table 1 and 2 show for
317 comparison the obtained performance rates using single-channel signals with the SVM classifier. The best
318 performing channel, where the best letter identification rate was achieved, is also depicted.

319 The Information Transfer Rate (ITR), or Bit Transfer Rate (BTR), in the case of reactive BCIs (Wolpaw
320 and E., 2012) depends on the amount of signal averaging required to transmit a valid and robust selection.
321 Figure 5 shows the performance curves for varying intensification sequences for the subjects included in
322 the dataset of ALS patients. It can be noticed that the percentage of correctly identified letters depends
323 on the number of intensification sequences that are used to obtain the averaged signal. Moreover, when
324 the number of intensification sequences tend to 1, which corresponds to single-intensification character
325 recognition, the performance is reduced. As mentioned before, the SNR of the P300 obtained from only
326 one segment of the intensification sequence is very low and the shape of its P300 component is not very
327 well defined.

328 In Table 2 the results obtained for 8 healthy subjects are shown. It can be observed that the performance
329 is above chance level. It is verified that HIST method has an improved performance at letter identification
330 than SVM that process the signals on a channel by channel strategy (Wilcoxon signed-rank test, $p = 0.004$
331 for both datasets).

332 Tables 3 and 4 are presented in order to compare the performance of the HIST method versus multichannel
333 SWLDA and SVM classification algorithms for both datasets. It is verified for the dataset of ALS patients
334 that it has similar performance against other methods like SWLDA or SVM, which use a multichannel
335 feature (Quade test with $p = 0.55$) whereas for the dataset of healthy subjects significant differences are
336 found (Quade test with $p = 0.02$) where only the HIST method achieves a different performance than SVM
337 (with multiple comparisons, significant difference of level 0.05).

338 The P300 ERP consists of two overlapping components: the P3a and P3b, the former with frontocentral
339 distribution while the later stronger on centroparietal region (Polich, 2007). Hence, the standard practice is
340 to find the stronger response on the central channel Cz (Riccio et al., 2013). However, Krusienski et al.
341 (2006) show that the response may also arise in occipital regions. We found that by analyzing only the
342 waveforms, occipital channels PO8 and PO7 show higher performances for some subjects.

343 As subjects have varying *latencies* and *amplitudes* of their P300 components, they also have a varying
344 stability of the *shape* of the generated ERP (Nam et al., 2010). Figure 6 shows 10 sample P300 templates
345 patches for patients 8 and 3 from the dataset of ALS patients. It can be discerned that in coincidence with
346 the performance results, the P300 signature is more clear and consistent for subject 8 (A) while for subject
347 3 (B) the characteristic pattern is more difficult to perceive.

348 Additionally, the stability of the P300 component waveform has been extensively studied in patients
349 with ALS (Sellers et al., 2006; Madarame et al., 2008; Nijboer and Broermann, 2009; Mak et al., 2012;
350 McCane et al., 2015) where it was found that these patients have a stable P300 component, which were
351 also sustained across different sessions. In line with these results we do not find evidence of a difference in
352 terms of the performance obtained by analyzing the waveforms (HIST) for the group of patients with ALS
353 and the healthy group of volunteers (Mann-Whitney U Test, $p = 0.46$). Particularly, the best performance
354 is obtained for a subject from the ALS dataset for which, based on visual observation, the shape of they
355 P300 component is consistently identified.

356 It is important to remark that when applied to binary images obtained from signal plots, the feature
357 extraction method described in Section 2.1.3 generates sparse descriptors. Under this subspace we found
358 that using the cosine metric yielded a significant performance improvement. On the other hand, the unary
359 classification scheme based on the NBNN algorithm proved very beneficial for the P300 Speller Matrix.
360 This is due to the fact that this approach solves the unbalance dataset problem which is inherent to the
361 oddball paradigm (Tibon and Levy, 2015).

4 DISCUSSION

362 Among other applications of Brain Computer Interfaces, the goal of the discipline is to provide
363 communication assistance to people affected by neuro-degenerative diseases, who are the most likely
364 population to benefit from BCI systems and EEG processing and analysis.

365 In this work, a method to extract an objective metric from the waveform of the plots of EEG signals is
366 presented. Its usage to implement a valid P300-Based BCI Speller application is expounded. Additionally,
367 its validity is evaluated using a public dataset of ALS patients and an own dataset of healthy subjects.

368 It was verified that this method has an improved performance at letter identification than other methods
369 that process the signals on a channel by channel strategy, and it even has a comparable performance against
370 other methods like SWLDA or SVM, which uses a multichannel feature. Furthermore, this method has the
371 advantage that shapes of waveforms can be analyzed in an objective way. We observed that the shape of
372 the P300 component is more stable in occipital channels, where the performance for identifying letters
373 is higher. We additionally verified that ALS P300 signatures are stable in comparison to those of healthy
374 subjects.

375 We believe that the use of descriptors based on histogram of gradient orientation, presented in this work,
376 can also be utilized for deriving a shape metric in the space of the P300 signals which can complement
377 other metrics based on time-domain as those defined by Mak et al. (2012). It is important to notice
378 that the analysis of waveform shapes is usually performed in a qualitative approach based on visual
379 inspection (Sellers et al., 2006), and a complementary methodology which offer a quantitative metric will
380 be beneficial to these routinely analysis of the waveform of ERPs.

381 The goal of this work is to answer the question if a P300 component could be solely determined by
382 inspecting automatically their waveforms. We conclude affirmatively, though two very important issues
383 still remain:

384 First, the stability of the P300 in terms of its shape is crucial: the averaging procedure, montages, the
385 signal to noise ratio and spatial filters all of them are non-physiological factors that affect the stability of
386 the shape of the P300 ERP. We tested a preliminary approach to assess if the morphological shape of the
387 P300 of the averaged signal can be stabilized by applying different alignments of the stacked segments (see

388 Figure 2) and we verified that there is a better performance when a correct segment alignment is applied.
389 We applied Dynamic Time Warping (DTW) (Casarotto et al., 2005) to automate the alignment procedure
390 but we were unable to find a substantial improvement. Further work to study the stability of the shape of
391 the P300 signature component needs to be addressed.

392 The second problem is the amplitude variation of the P300. We propose a solution by standardizing the
393 signal, shown in Equation 2. It has the effect of normalizing the peak-to-peak amplitude, moderating its
394 variation. It has also the advantage of reducing noise that was not reduced by the averaging procedure. It is
395 important to remark that the averaged signal variance depends on the number of segments used to compute
396 it (Van Drongelen, 2006). The standardizing process converts the signal to unit signal variance which
397 makes it independent of the number k_a of signals averaged. Although this is initially an advantageous
398 approach, the standardizing process reduces the amplitude of any significant P300 complex diminishing its
399 automatic interpretation capability.

400 In our opinion, the best benefit of the presented method is that a closer collaboration of the field of BCI
401 with physicians can be fostered (Chavarriaga et al., 2017), since this procedure intent to imitate human
402 visual observation. Automatic classification of patterns in EEG that are specifically identified by their
403 shapes like K-Complex, Vertex Waves, Positive Occipital Sharp Transient (Hartman, 2005) are a prospect
404 future work to be considered. We are currently working in unpublished material analyzing K-Complex
405 components that could eventually provide assistance to physicians to locate these EEG patterns, specially in
406 long recording periods, frequent in sleep research (Michel and Murray, 2012). Additionally, it can be used
407 for artifact removal which is performed on many occasions by visually inspecting signals. This is due to
408 the fact that the descriptors are a direct representation of the shape of signal waveforms. In line with these
409 applications, it can be used to build a database (Chavarriaga et al., 2017) of quantitative representations of
410 waveforms and improve atlases (Hartman, 2005), which are currently based on qualitative descriptions of
411 signal shapes.

CONFLICT OF INTEREST STATEMENT

412 The authors declare that the research was conducted in the absence of any commercial or financial
413 relationships that could be construed as a potential conflict of interest.

AUTHOR CONTRIBUTIONS

414 This work is part of the PhD thesis of RR which is directed by JS and codirected by AV.

FUNDING

415 This project was supported by the ITBACyT-15 funding program issued by ITBA University from Buenos
416 Aires, Argentina.

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Table 1. Character recognition rates for the public dataset of ALS patients using the Histogram of Gradient (HIST) calculated from single-channel plots. Performance rates using single-channel signals with the SVM classifier are shown for comparison. The best performing channel *bpc* for each method is visualized

Participant	<i>bpc</i>	HIST	<i>bpc</i>	Single Channel SVM
1	Cz	35%	Cz	15%
2	Fz	85%	PO8	25%
3	Cz	25%	Fz	5%
4	PO8	55%	Oz	5%
5	PO7	40%	P3	25%
6	PO7	60%	PO8	20%
7	PO8	80%	Fz	30%
8	PO7	95%	PO7	85%

Table 2. Character recognition rates for the own dataset of healthy subjects using the Histogram of Gradient (HIST) calculated from single-channel plots. Performance rates using single-channel signals with the SVM classifier are shown for comparison. The best performing channel *bpc* for each method is visualized.

Participant	<i>bpc</i>	HIST	<i>bpc</i>	Single Channel SVM
1	Oz	40%	Cz	10%
2	PO7	30%	Cz	5%
3	P4	40%	P3	10%
4	P4	45%	P4	35%
5	P4	60%	P3	10%
6	Pz	50%	P4	25%
7	PO7	70%	P3	30%
8	P4	50%	PO7	10%

Table 3. Character recognition rates and the best performing channel *bpc* for the public dataset of ALS patients using the Histogram of Gradient (HIST) (repeated here for comparison purposes). Performance rates obtained by SWLDA and SVM classification algorithms with a multichannel concatenated feature.

Participant	<i>bpc</i> for HIST	HIST	Multichannel SWLDA	Multichannel SVM
1	Cz	35%	45%	40%
2	Fz	85%	30%	50%
3	Cz	25%	65%	55%
4	PO8	55%	40%	50%
5	PO7	40%	35%	45%
6	PO7	60%	35%	70%
7	PO8	80%	60%	35%
8	PO7	95%	90%	95%

Table 4. Character recognition rates and the best performing channel *bpc* for the own dataset of healthy subjects using the Histogram of Gradient (HIST) (repeated here for comparison purposes). Performance rates obtained by SWLDA and SVM classification algorithms with a multichannel concatenated feature.

Participant	<i>bpc</i> for HIST	HIST	Multichannel SWLDA	Multichannel SVM
1	Oz	40%	65%	40%
2	PO7	30%	15%	10%
3	P4	40%	50%	25%
4	P4	45%	40%	20%
5	P4	60%	30%	20%
6	Pz	50%	35%	30%
7	PO7	70%	25%	30%
8	P4	50%	35%	20%

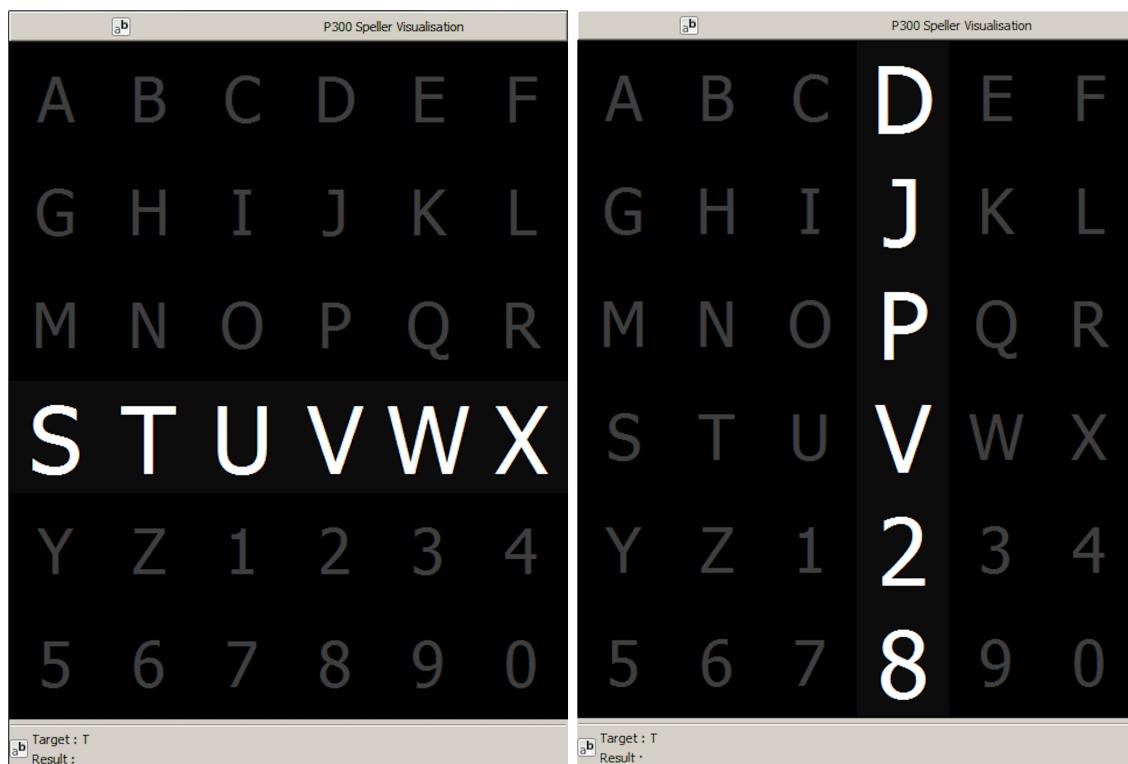


Figure 1. Example of the 6×6 Speller Matrix used in the study obtained from the OpenVibe software. Rows and columns flash in random permutations.

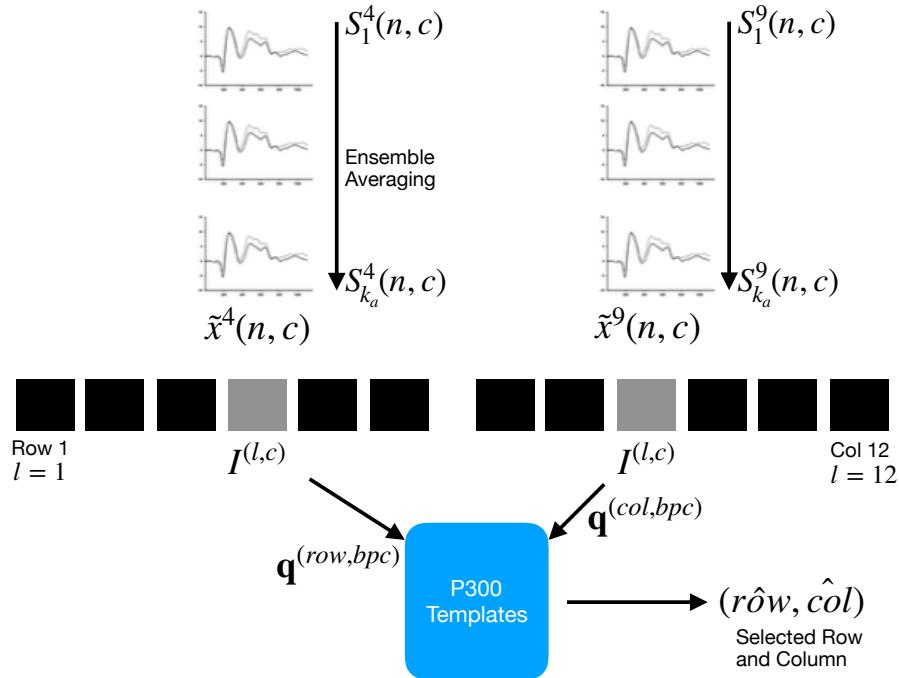


Figure 2. For each column and row, an averaged, standardized and scaled signal $\tilde{x}^l(n, c)$ is obtained from the segments S_i^l corresponding to the k_a intensification sequences with $1 \leq i \leq k_a$ and location l varying between 1 and 12. From the averaged signal, the image $I^{(l,c)}$ of the signal plot is generated and each descriptor is computed. By comparing each descriptor against the set of templates, the P300 ERP can be detected, and finally the desired letter from the matrix can be inferred.

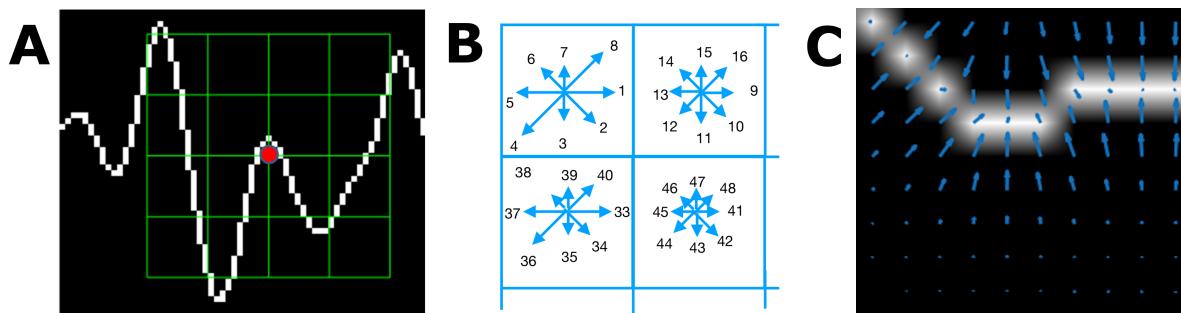


Figure 3. (A) Example of a plot of the signal, a keypoint and the corresponding patch. (B) A scheme of the orientation's histogram computation. Only the upper-left four blocks are visible. The first eight orientations of the first block, are labeled from 1 to 8 clockwise. The orientation of the second block $B_{1,2}$ is labeled from 9 to 16. This labeling continues left-to-right, up-down until the eight orientations for all the sixteen blocks are assigned. They form the corresponding descriptor of 128 coordinates. The length of each arrow represent the value of the histogram on each direction for each block. (C) Vector field of oriented gradients. Each pixel is assigned an orientation and magnitude calculated using finite differences.

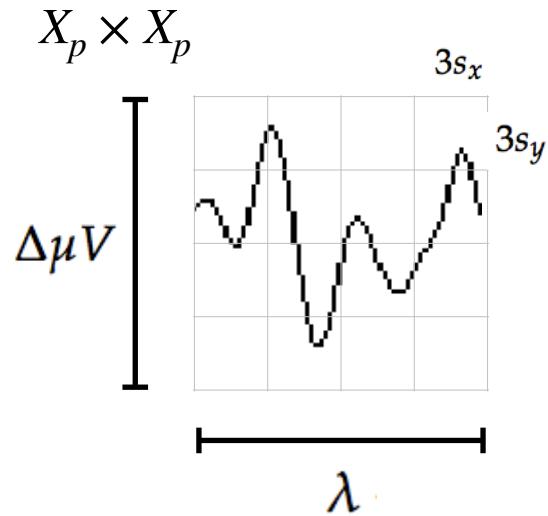


Figure 4. The scale of local patch is selected in order to capture the whole transient event. The size of the patch is $X_p \times X_p$ pixels. The vertical size consists of 4 blocks of size $3s_y$ pixels which is high enough as to contain the signal $\Delta\mu V$, the peak-to-peak amplitude of the transient event. The horizontal size includes 4 blocks of $3s_x$ and covers the entire duration in seconds of the transient signal event, λ .

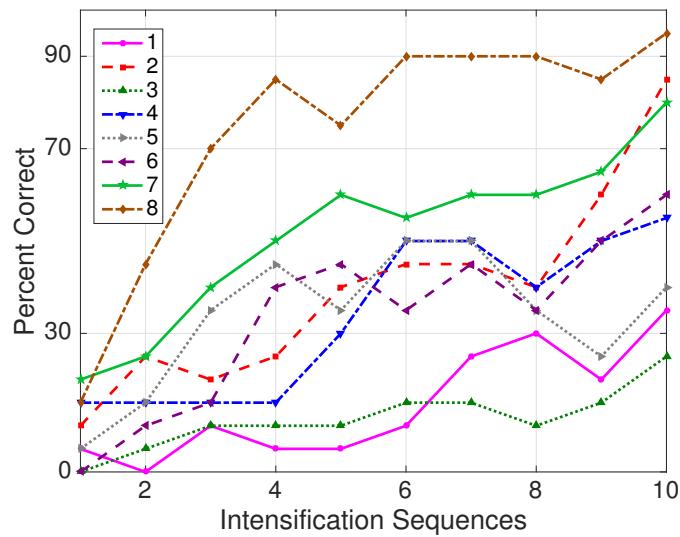


Figure 5. Performance curves for the eight subjects included in the dataset of ALS patients. Three out of eight subjects achieved the necessary performance to implement a valid P300 speller.

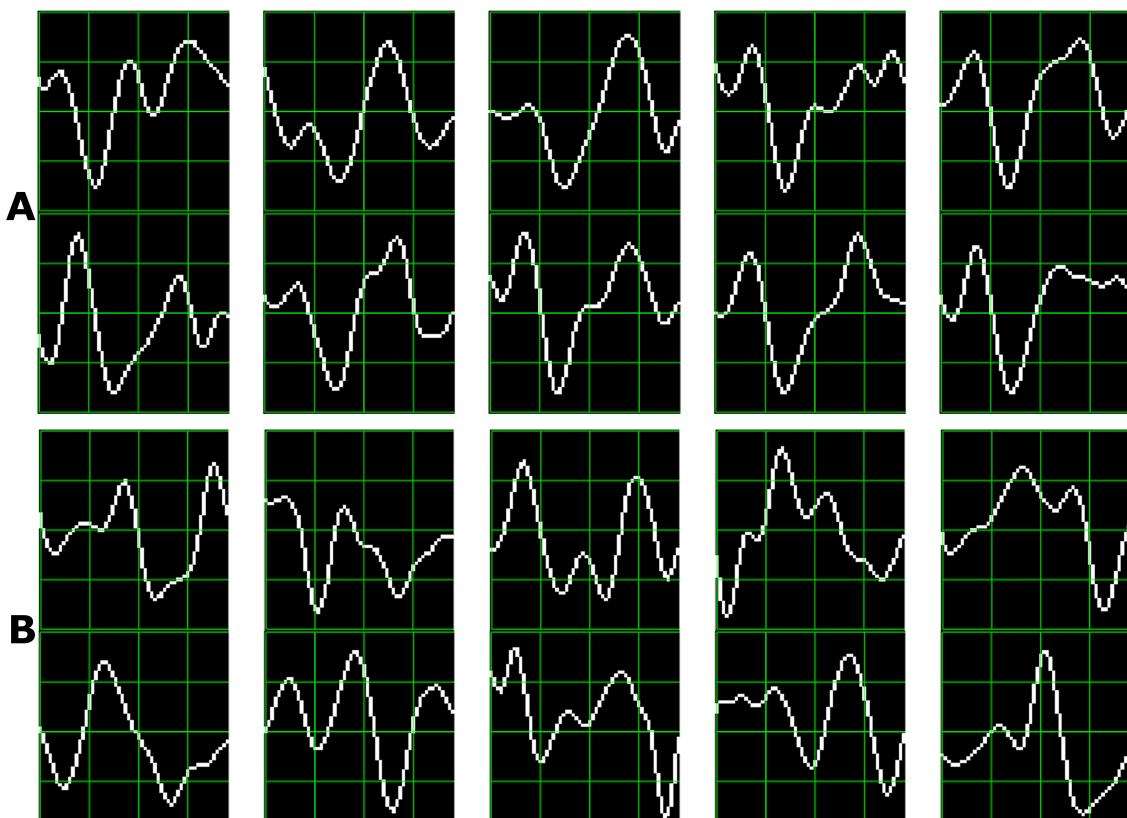


Figure 6. Ten sample P300 template patches for subjects 8 (A) and 3 (B) of the ALS Dataset. Downward deflection is positive polarity.