

# Uncertainty in multitask learning: joint representations for probabilistic MR-only radiotherapy treatment planning

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## Motivation and Overview

- **Multi-task learning** is dependent on the relative weighting of task losses and the mechanism for sharing network weights.
- Task loss weightings are generally hyper-parameters or learned [1]
- We propose a **probabilistic multi-task network** (Fig. 1) that:
  - a) estimates **heteroscedastic uncertainty** for spatially adaptive task loss weighting
  - b) captures **model uncertainty** through approximate Bayesian inference
- We apply our model to **MR-only radiotherapy treatment planning**,
- **Results** show:
  1. heteroscedastic uncertainty **improves** multi-task learning over learned task loss weights
  2. the estimated uncertainty can be exploited for **quality assurance and control** of the network

## MR-only radiotherapy treatment planning

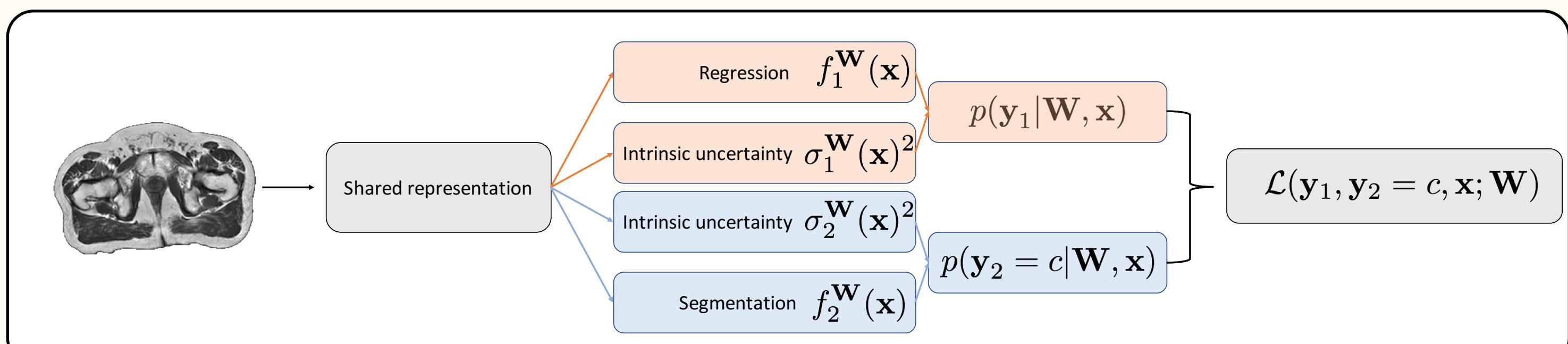
- Joint synthesis of a CT scan (synCT) - **regression** - and localisation of organs at risk (OAR) - **segmentation** - from an input MRI scan
- Input MR

Regression

Segmentation
- Fig 2.** MR-only radiotherapy treatment planning.
- Previous synthesis methods [2, 3] do not jointly segment OARs
  - CT synthesis methods are generally fully deterministic
  - A system that can sample both synCT and OAR segmentations will enable end-to-end uncertainty aware probabilistic planning

## Probabilistic dual-task neural network

- Probabilistic multi-task learning with hard-parameter sharing: representation network + task-specific networks



**Fig 1.** A representation network learns an invariant feature space for the anatomy. A task-specific network then learns the non-linear mapping between the input and the various output tasks. The task-specific likelihoods  $p(y_i|W, x)$  are combined to yield the multi-task likelihood.

## Task weighting with heteroscedastic uncertainty

- Heteroscedastic uncertainty represents inherent ambiguity present in the MR-CT intensity mapping and in obtaining voxel-wise class memberships
- Uncertainty is spatially varying and task dependent – this is exploited as a mechanism for task loss weighting

### □ Regression noise model

$$\text{Likelihood function} \\ p(y_1|W, x) = \mathcal{N}(f_1^W(x), \sigma_1^W(x)^2)$$

### □ Segmentation noise model

$$\text{Likelihood function} \\ p(y_2|W, x) = \text{Softmax}(f_2^W(x)/2\sigma_2^W(x)^2)$$

### □ Multi-task heteroscedastic likelihood

$$\mathcal{L}(y_1, y_2 = c, x; W) = \frac{\|y_1 - f_1^W(x)\|^2}{2\sigma_1^W(x)^2} + \frac{\text{CE}(f_2^W(x), y_2 = c)}{2\sigma_2^W(x)^2} + \log(\sigma_1^W(x)^2 \sigma_2^W(x)^2)$$

## Model uncertainty

- We account for parameter uncertainty through an approximation of the posterior distribution over the weights
- The posterior distribution is approximated through Bernoulli binary dropout [4]

### Posterior distribution approximation

$$q(W) \approx p(W|X, Y_1, Y_2)$$

### Sampling posterior during training

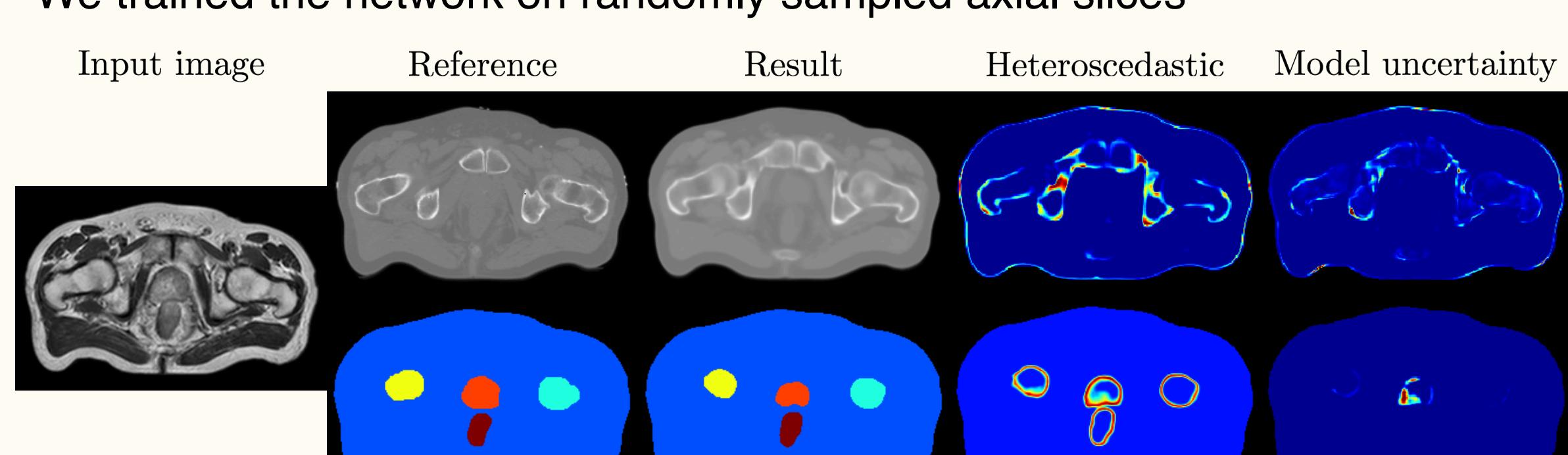
$$w' \sim q(W) \quad f^{w'}(x) := [f_1^{w'}(x), f_2^{w'}(x), \sigma_1^{w'}(x)^2, \sigma_2^{w'}(x)^2]$$

## Quantifying total uncertainty over predictions

- At test time, for each input patch  $x$ , output samples  $\{f^{w(t)}(x)\}_{t=1}^T$  are obtained by performing  $T$  stochastic passes through the network such that  $\{w^{(t)}\}_{t=1}^T \sim q(W)$
- The variance of the predictive distribution quantifies the **predictive uncertainty**
- We use the **predictive mean** as final estimates for  $f^w(x)$  whilst the **total uncertainty** is the sum of the predictive uncertainty and modelled heteroscedastic noise.

## Model performance

- We tested on 15 prostate scans using 3-fold cross-validation
- We trained the network on randomly sampled axial slices



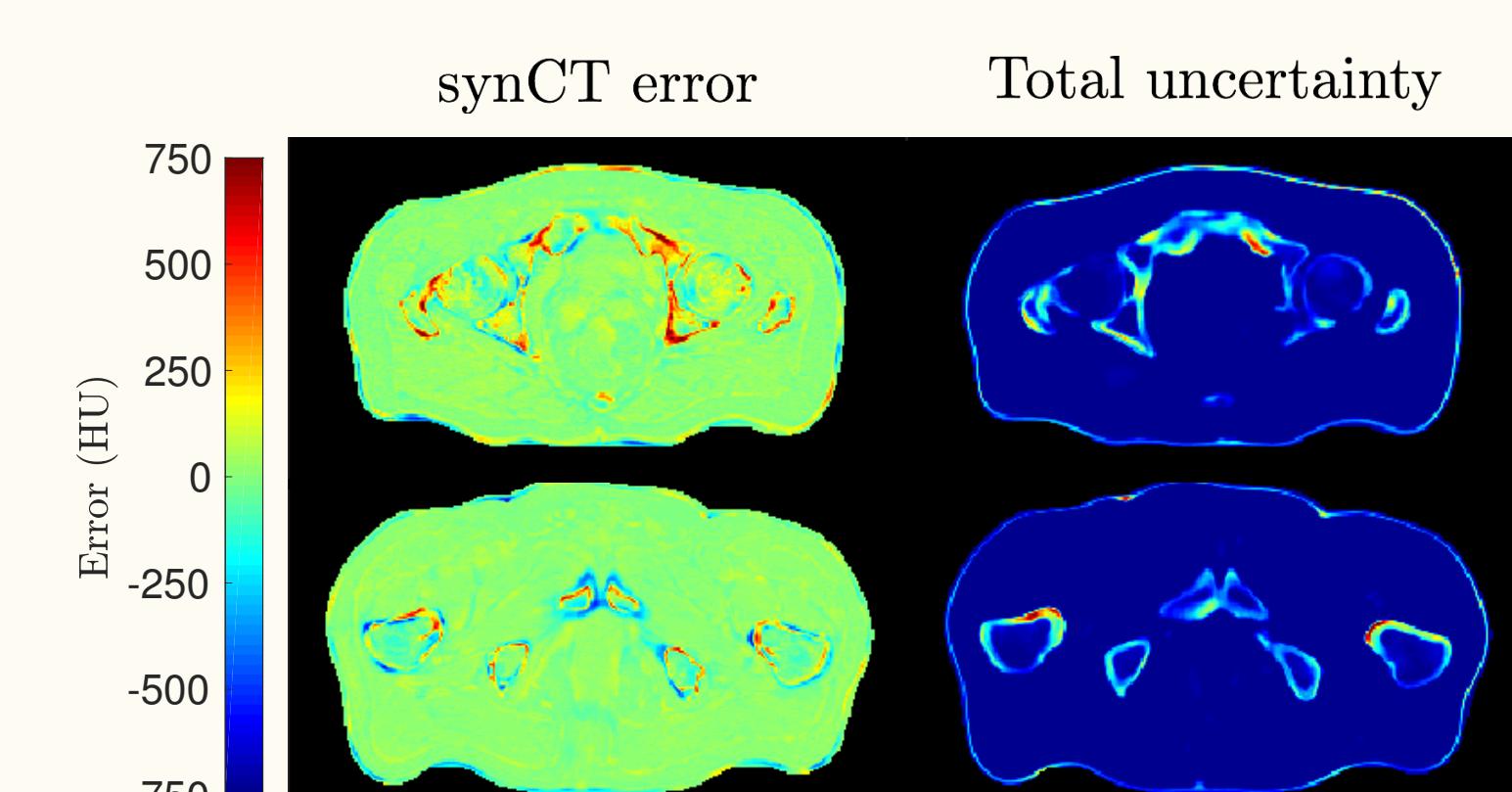
**Fig 3.** Example of the model output. For each new subject, we obtain: 1) a synCT, 2) segmentation of the organs, 3) the uncertainty across both predictions.

- Joint modelling of heteroscedastic and parameter uncertainty **achieves best performance** on synCT regression and **outperforms** homoscedastic task weighting
- Equivalent results in segmentation with the state of the art in pelvic segmentation [5]

Models	All	Bone	L femur	R femur	Prostate	Rectum	Bladder
Regression - synCT - Mean Absolute Error (HU)							
HighResNet [7]	48.1(4.2)	131(14.0)	78.6(19.2)	80.1(19.6)	37.1(10.4)	63.3(47.3)	24.3(5.2)
HighResNet + dropout	47.4(3.9)	130(12.1)	78.0(14.8)	77.0(13.0)	36.5(7.8)	67(44.6)	24.1(7.5)
HighResNet + dropout + hetero [6]	44.5(3.6)	128(17.1)	75.8(20.1)	74.2(17.4)	31.2(7.0)	56.1(45.5)	17.8(4.7)
Multi-task + homo noise weighting [1]	44.3(3.1)	126(14.4)	74.0(19.5)	73.7(17.1)	29.4(4.7)	58.4(48.0)	18.2(3.5)
Multi-atlas propagation [5]	45.7(4.6)	125(10.3)	-	-	-	-	-
Multi-task + dropout + hetero	43.3(2.9)	121(12.6)	69.7(13.7)	67.8(13.2)	28.9(2.9)	55.1(48.1)	18.3(6.1)
Segmentation - OAR - Fuzzy DICE score							
HighResNet [7]	-	-	0.91(0.02)	0.90(0.04)	0.67(0.12)	0.70(0.15)	0.92(0.05)
HighResNet + dropout	-	-	0.85(0.03)	0.90(0.04)	0.66(0.12)	0.69(0.13)	0.90(0.07)
HighResNet + dropout + hetero [6]	-	-	0.92(0.02)	0.92(0.01)	0.77(0.07)	0.74(0.13)	0.92(0.03)
Multi-task + homo noise weighting [1]	-	-	0.92(0.02)	0.92(0.02)	0.73(0.07)	0.76(0.10)	0.93(0.02)
Multi-atlas propagation [5]	-	-	0.89(0.02)	0.90(0.01)	0.73(0.06)	0.77(0.06)	0.90(0.03)
Multi-task + dropout + hetero	-	-	0.91(0.02)	0.91(0.02)	0.70(0.06)	0.74(0.12)	0.93(0.04)

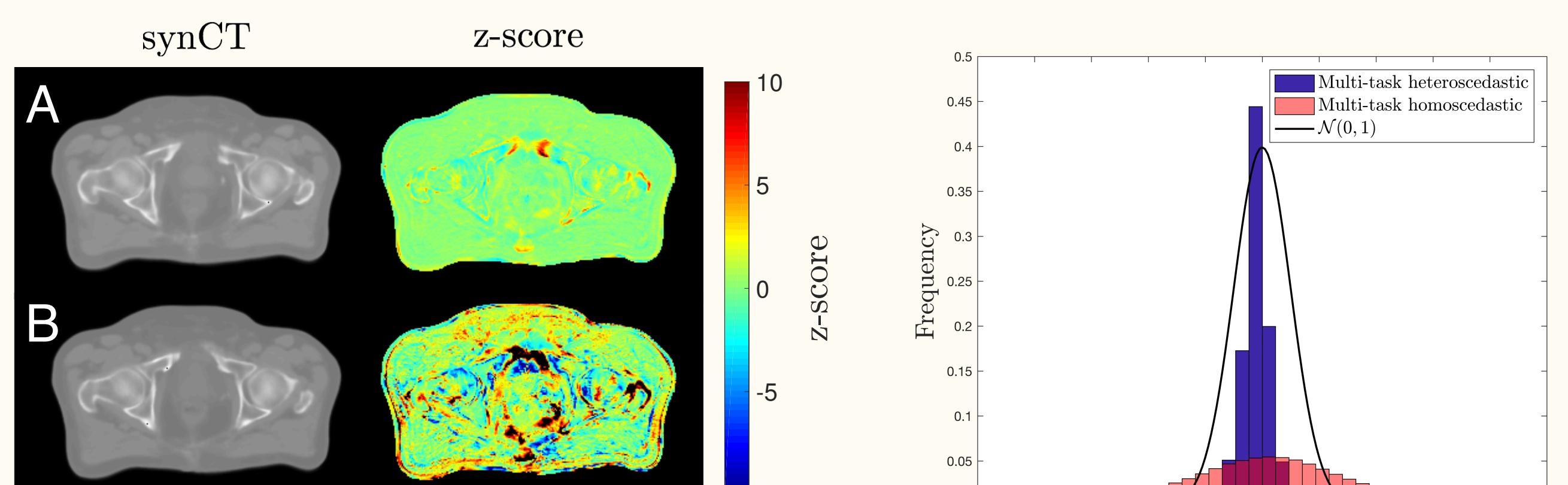
## Uncertainty as a quality control mechanism

- Total uncertainty correlates with regression errors in the synCT



**Fig 4.** Correlation between total uncertainty and regression error.

- Our method produces well calibrated uncertainty measures



**Fig 5.** We calculated the z-score using the total uncertainty estimated in a) our model and b) with homoscedastic task weighting.

## References

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