

International Conference on Computational Science and Engineering

# Assessment of regional myocardial work through adjoint-based data assimilation

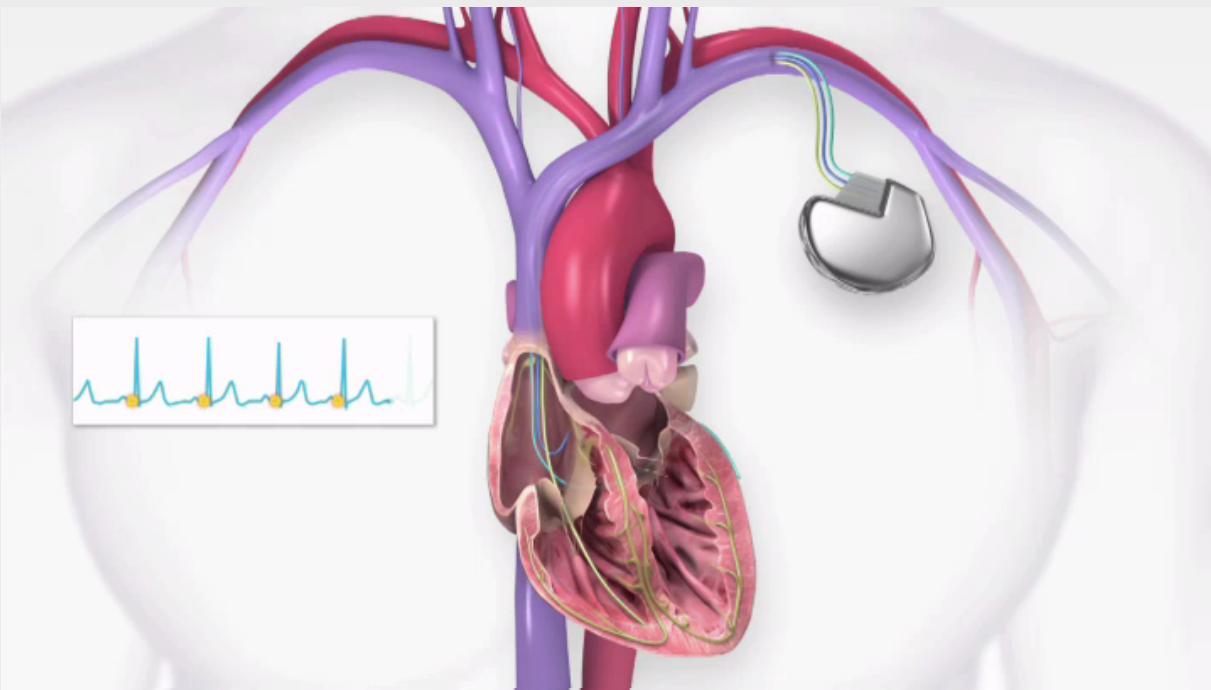
October 25<sup>th</sup> 2017

Henrik Finsberg



simula

# Clinicians need better biomarkers for identifying responders in heart failure treatment



Source: American Heart Association

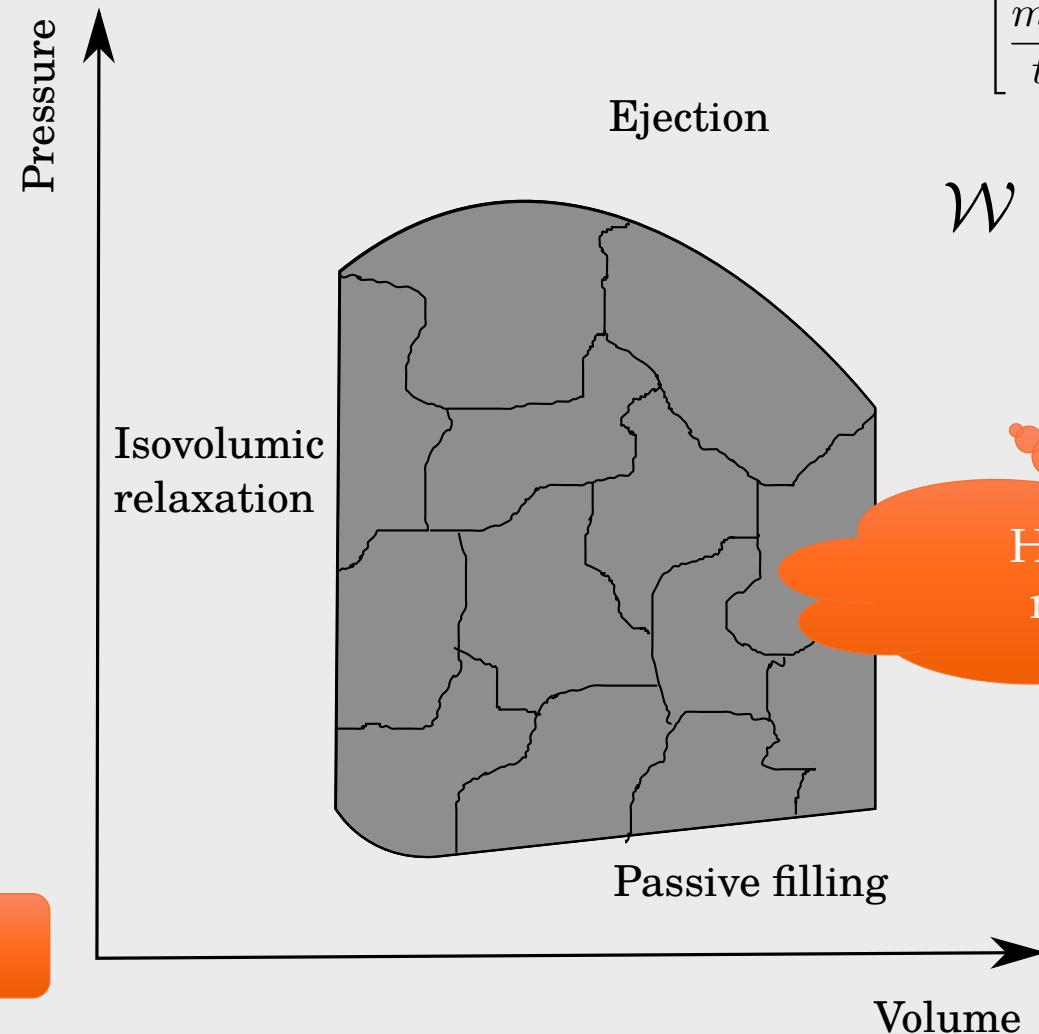
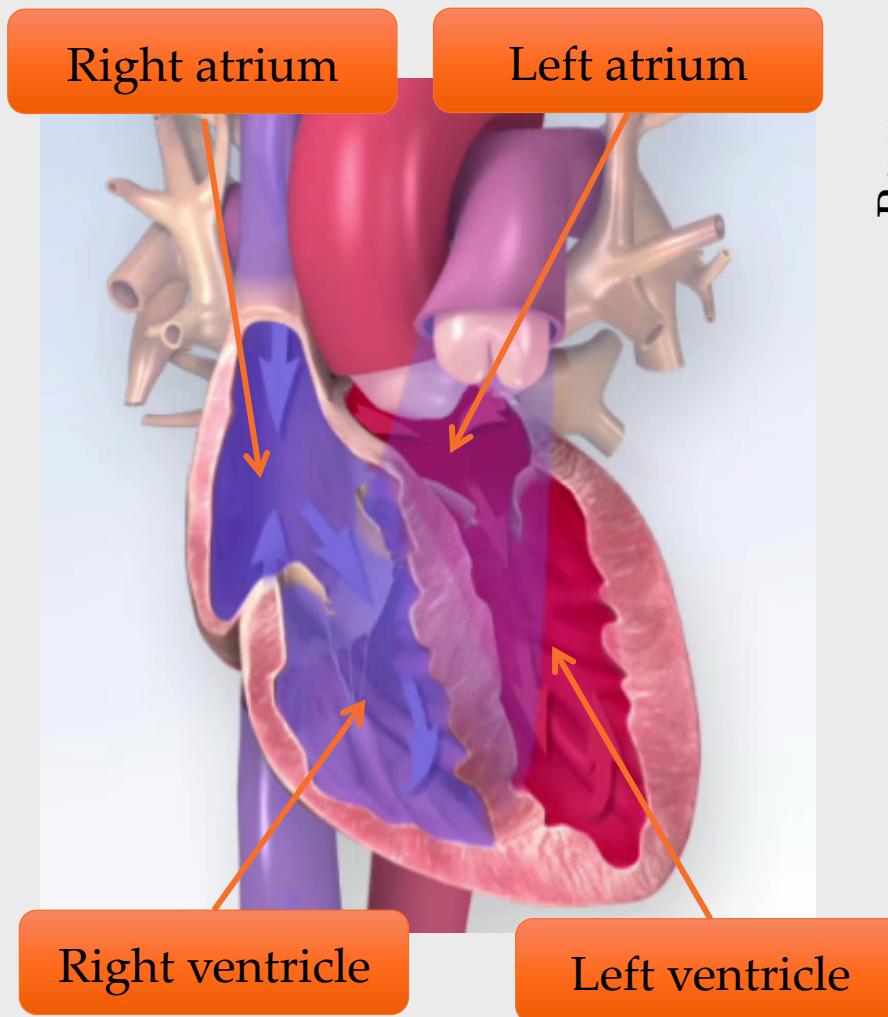


European Heart Journal – Cardiovascular Imaging (2016) **17**, 624–632  
doi:10.1093/ehjci/jew019

## Wasted septal work in left ventricular dyssynchrony: a novel principle to predict response to cardiac resynchronization therapy

J. Vecera<sup>1,2</sup>, M. Penicka<sup>2</sup>, M. Eriksen<sup>1</sup>, K. Russell<sup>1</sup>, J. Bartunek<sup>2</sup>, M. Vanderheyden<sup>2</sup>, and O.A. Smiseth<sup>1\*</sup>

Total myocardial work in the left ventricle can be estimated by the area of the pressure-volume loop

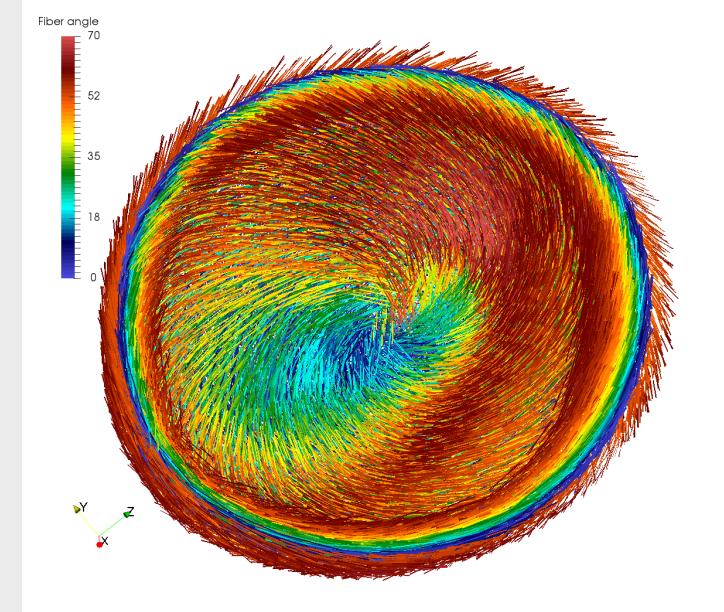
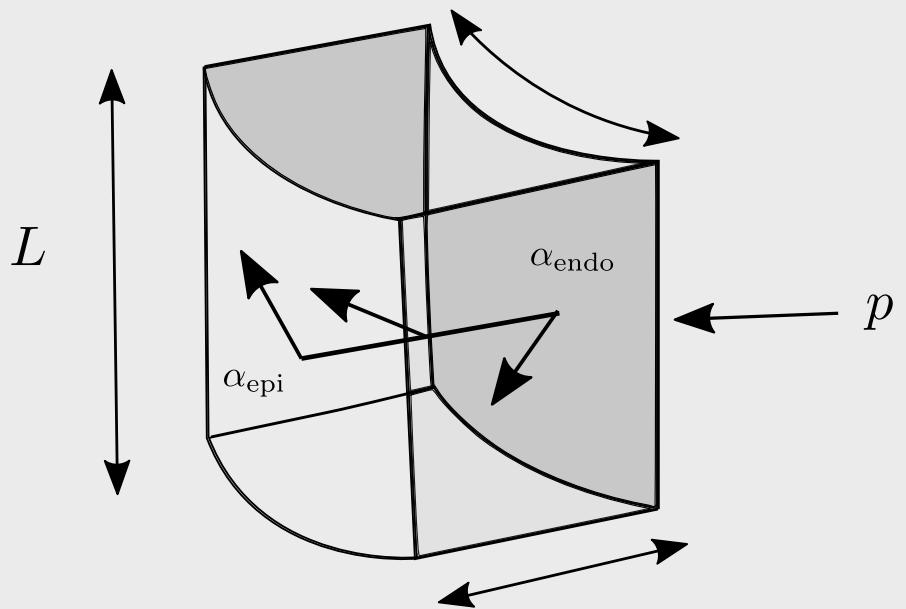
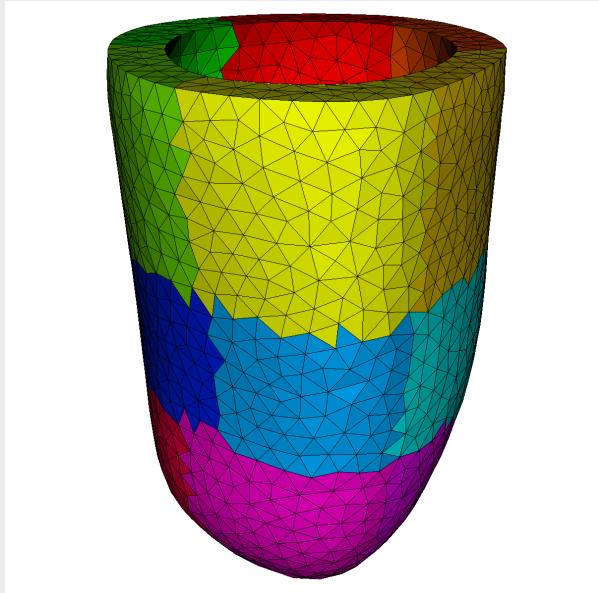


$$\left[ \frac{m^3}{t} \cdot Pa \cdot t \right] = [Pa \cdot m^3] = [\text{Joule}]$$

$$W = \int \frac{dV}{dt} P(t) dt$$

How to compute  
regional work?

Regional work is estimated in the clinic based on the area of pressure strain loops – reasonable assumption?

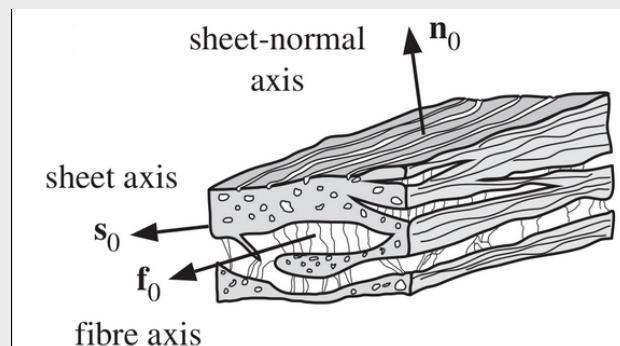


$$V \leftrightarrow \varepsilon = \frac{L - L_0}{L_0} \quad [\text{Pa} \cdot 1] = [\text{Joule}/m^3]$$

# Mathematical models of the heart allow for formulation of realistic constitutive equations in a continuum mechanics framework

## Model for the passive tissue

$$\Psi(\bar{\mathbf{C}}) = \frac{a}{2b} \left( e^{b(\bar{I}_1 - 3)} - 1 \right) + \frac{a_f}{2b_f} \left( e^{b_f(\bar{I}_{4\mathbf{f}_0} - 1)_+^2} - 1 \right)$$

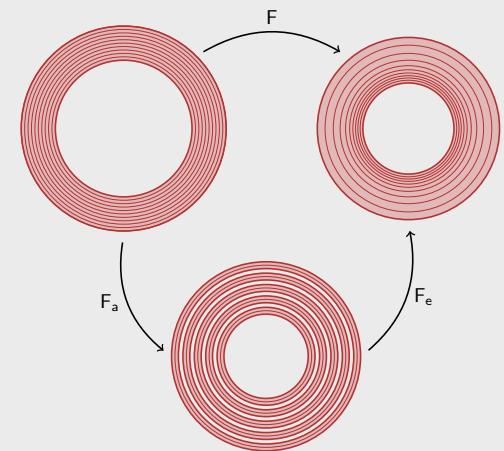


Holzapfel et al.

## Model for active contraction

$$\mathbf{F} = \mathbf{F}_e \mathbf{F}_a$$

Pezzuto et al.

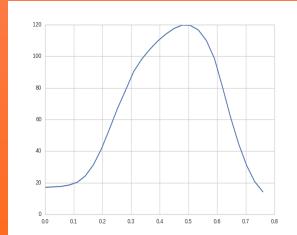


$$\mathbf{F}_a = (1 - \gamma) \mathbf{f}_0 \otimes \mathbf{f}_0 + \frac{1}{\sqrt{1 - \gamma}} (\mathbf{I} - \mathbf{f}_0 \otimes \mathbf{f}_0)$$

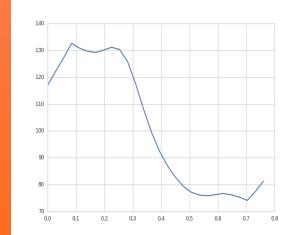
# Personalized mechanics models can be created through data assimilation

## Non-invasive data from 3D ultrasound

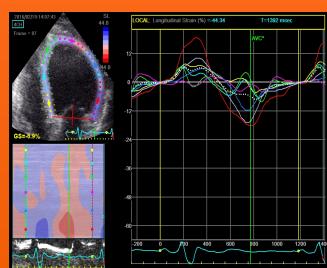
Estimated pressure



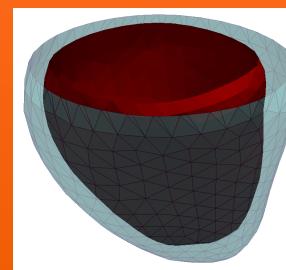
Measured volume



Longitudinal strain



Segmented surfaces



## Data assimilation

Minimize difference between model and observations by tuning parameters in the model

Mismatch functional

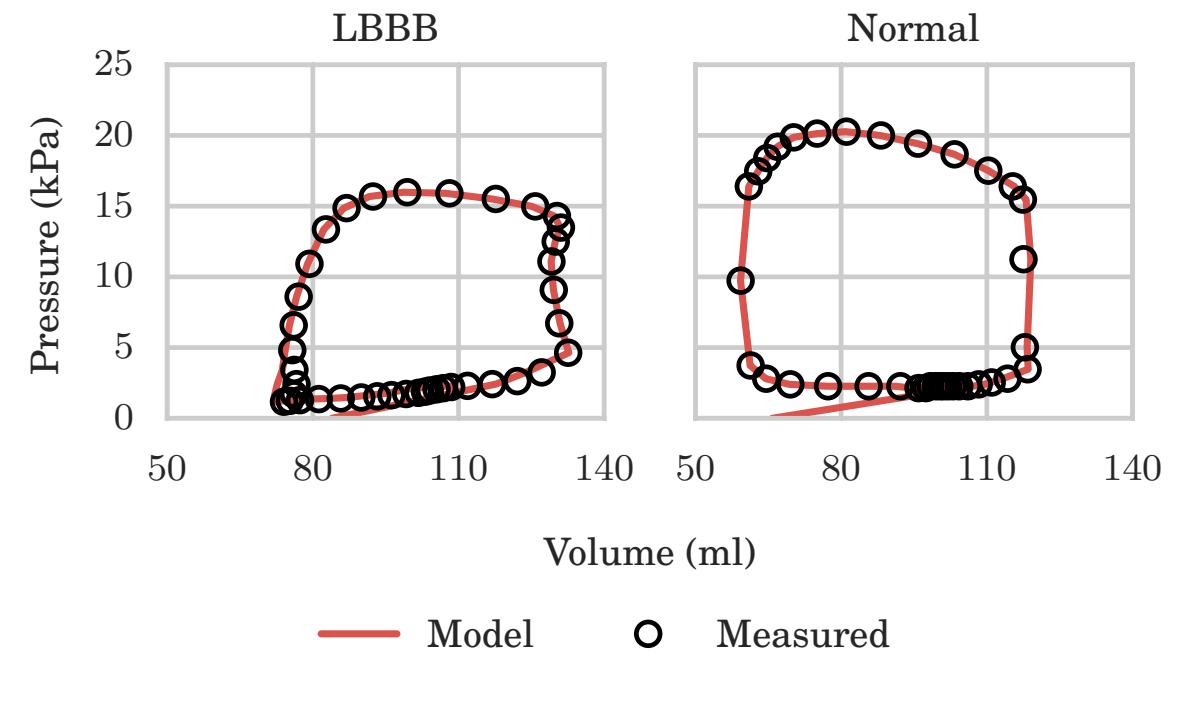
$$\underset{\mu}{\text{minimize}} \quad \mathcal{J}(\mathbf{w}(\mu), \mu)$$

$$\text{subject to} \quad F(\mathbf{w}, \mu) = 0,$$

Force balance equation

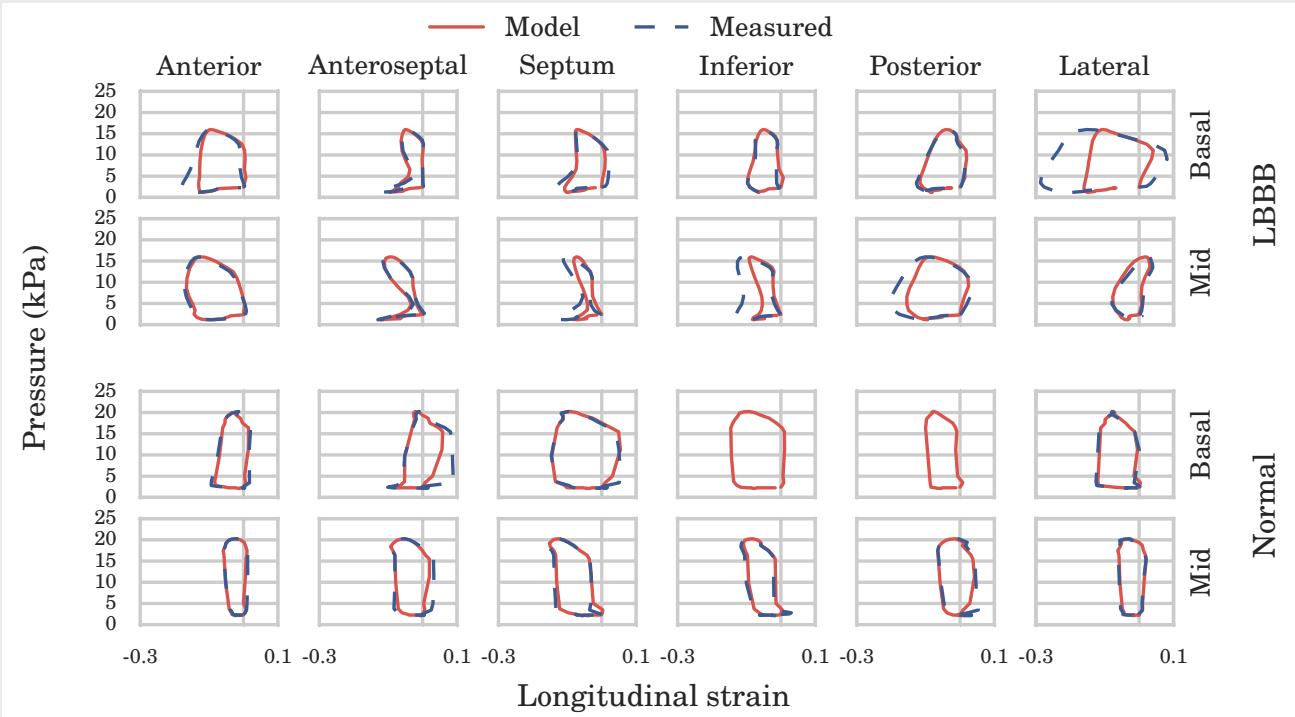
# Excellent fit between measured and simulated data is obtained

Pressure-Volume Loops

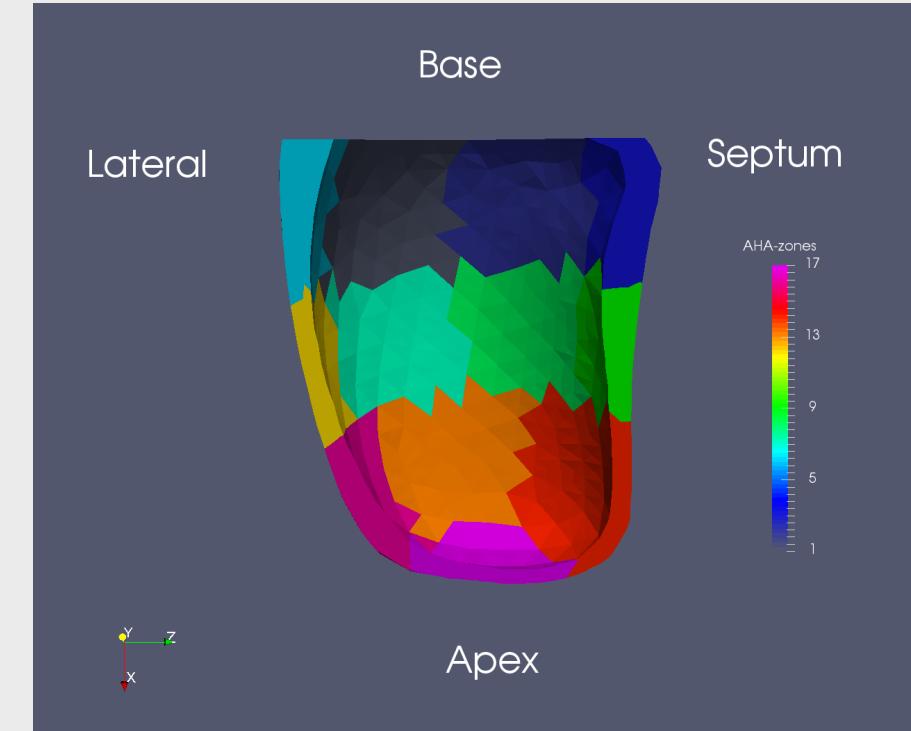
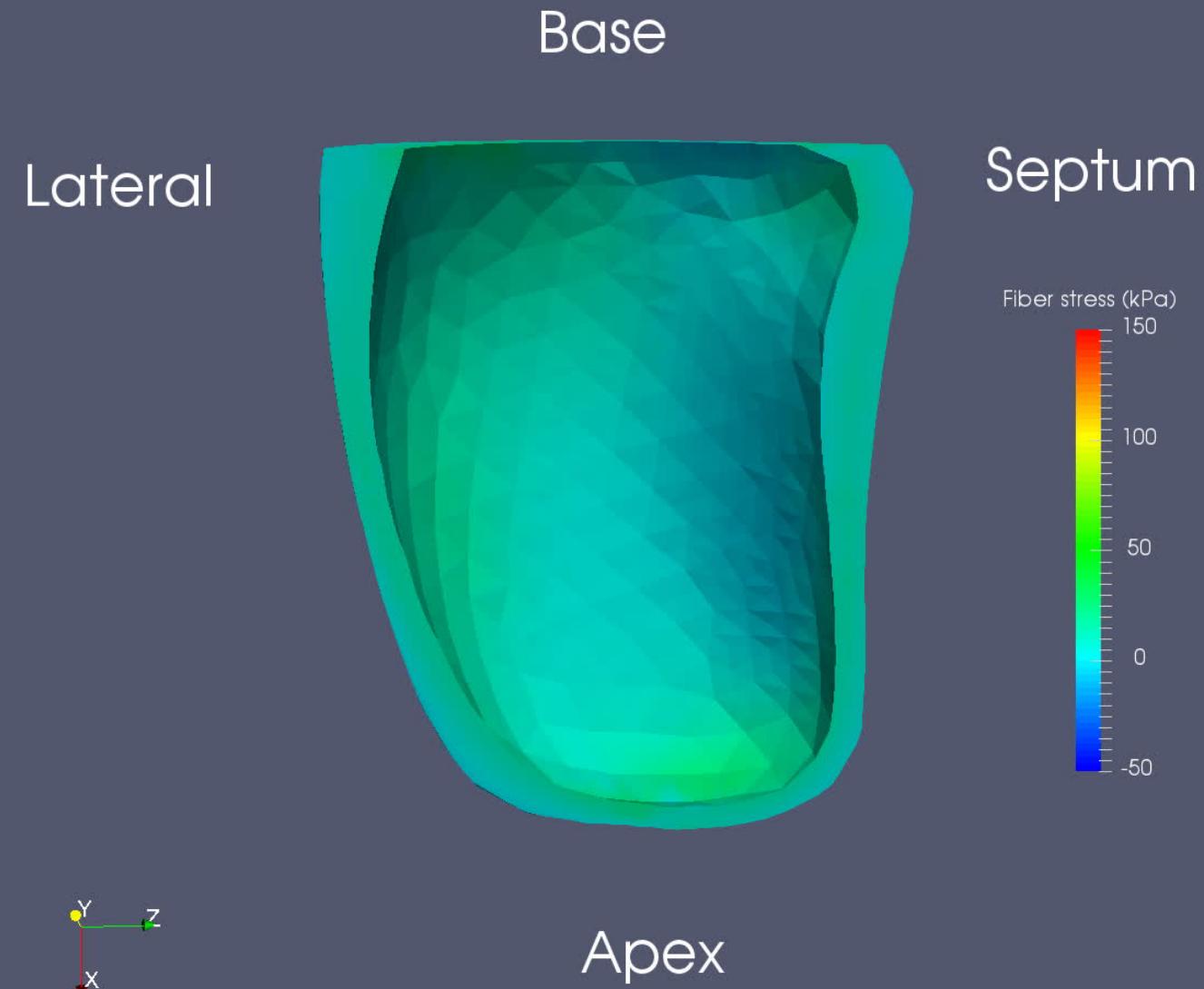


LBBB: patient with dyssynchrony

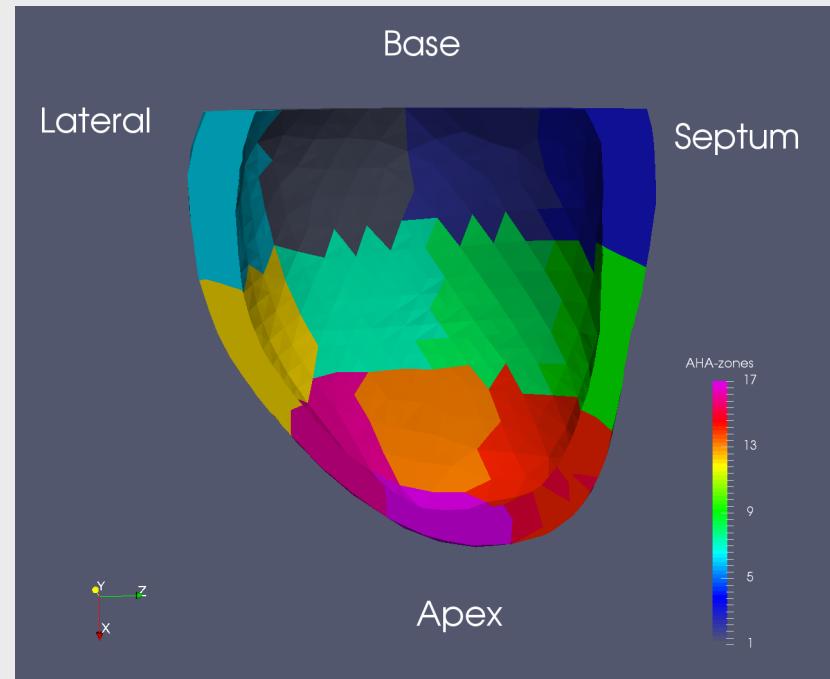
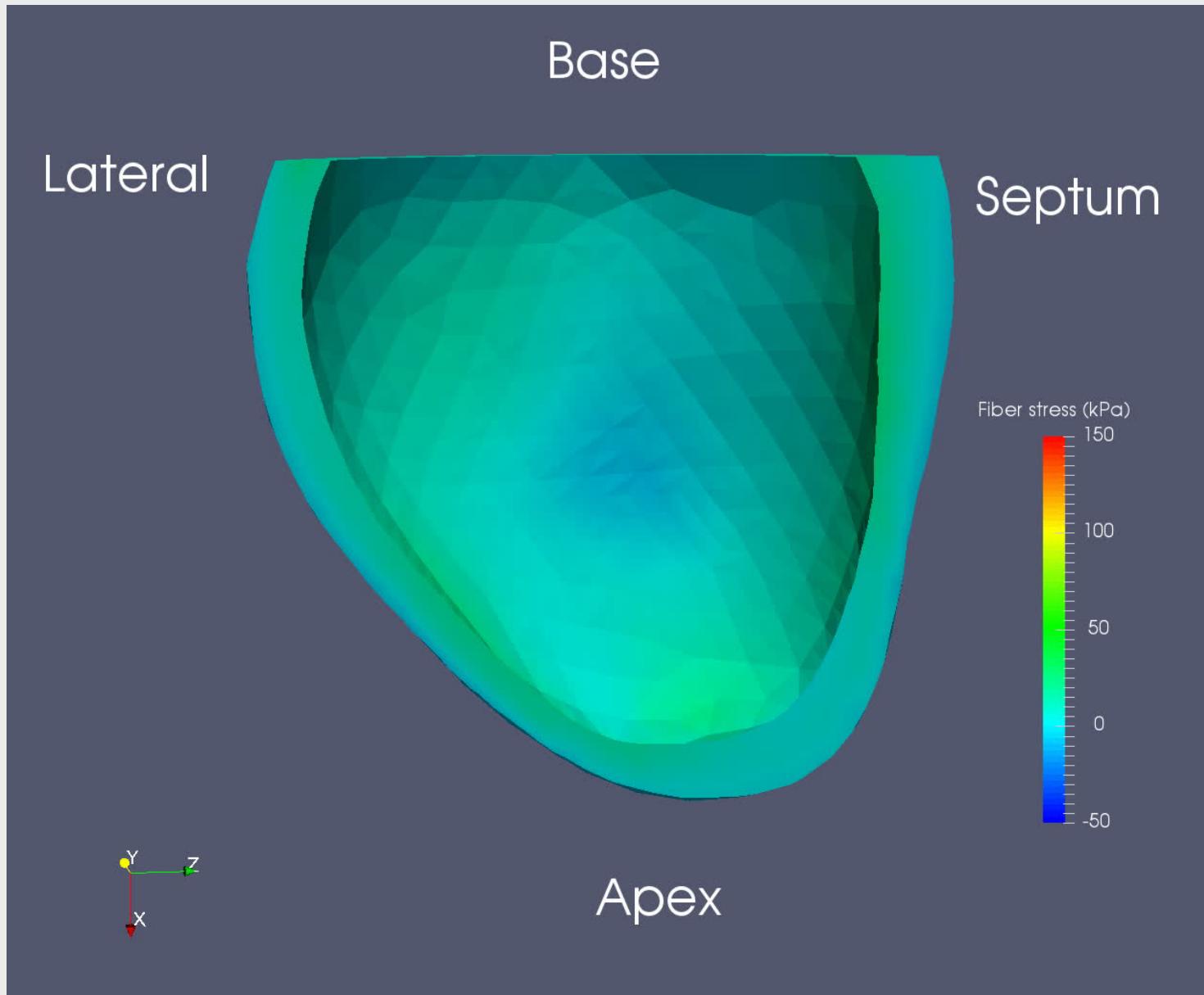
Pressure-Strain Loops



# Normal



# LBBB



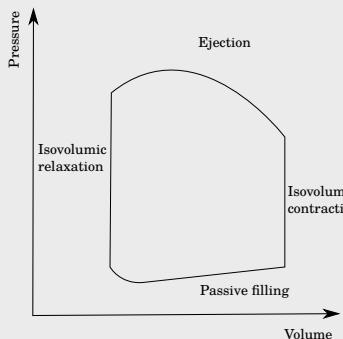
# The patient specific mechanical models can be used to estimate work

$$\mathcal{W}(t_1, t_2)[\Omega_j] = - \int_{t_1}^{t_2} \int_{\Omega_j} \mathbf{S}(t, \mathbf{X}) : \dot{\mathbf{E}}(t, \mathbf{X}) d\mathbf{X} dt$$

Second Piola-Kirchhoff stress tensor:  $\mathbf{S}(t, \mathbf{X})$   
 Green-Lagrange strain tensor:  $\mathbf{E}(t, \mathbf{X})$

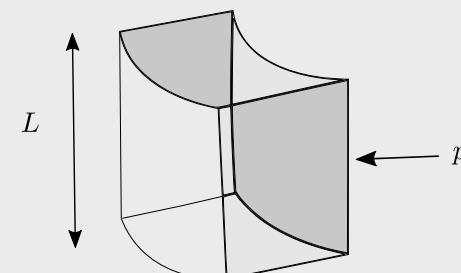
Case	PV area ( $\text{kW m}^{-3}$ )	Full ( $\text{kW m}^{-3}$ )	Fiber ( $\text{kW m}^{-3}$ )	Pressure-GLS ( $\text{kW m}^{-3}$ )
LBBB	8.41	10.60	6.42	1.02
Normal	15.79	16.35	9.59	1.59

$$\mathcal{W}(t_1, t_2)[\Omega_j]/|\Omega_j| \cdot (t_2 - t_1)$$

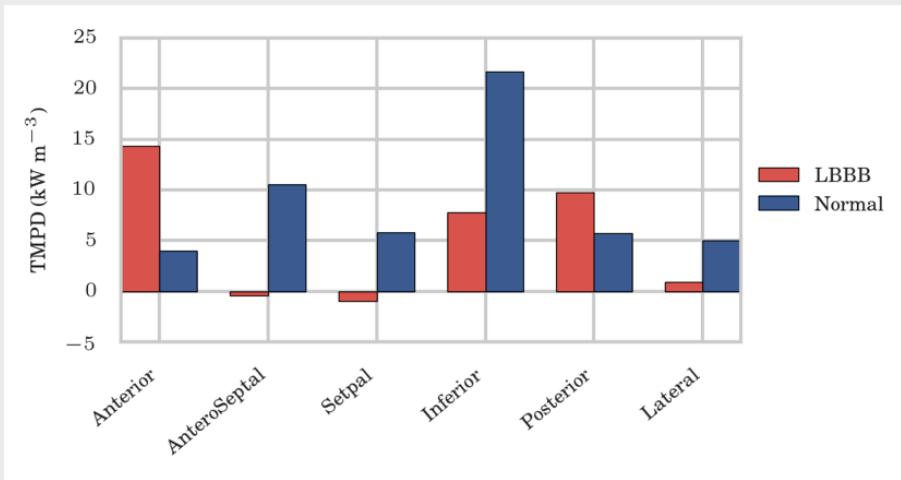


$$\begin{pmatrix} \sigma_{11} & \sigma_{12} & \sigma_{13} \\ \sigma_{21} & \sigma_{22} & \sigma_{23} \\ \sigma_{31} & \sigma_{23} & \sigma_{33} \end{pmatrix}$$

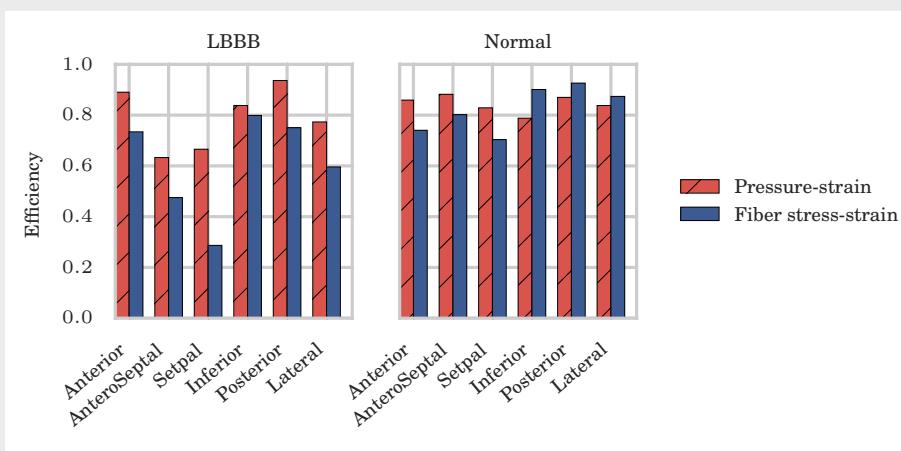
$$\begin{pmatrix} \sigma_{ff} & \cdot & \cdot \\ \cdot & \cdot & \cdot \\ \cdot & \cdot & \cdot \end{pmatrix}$$



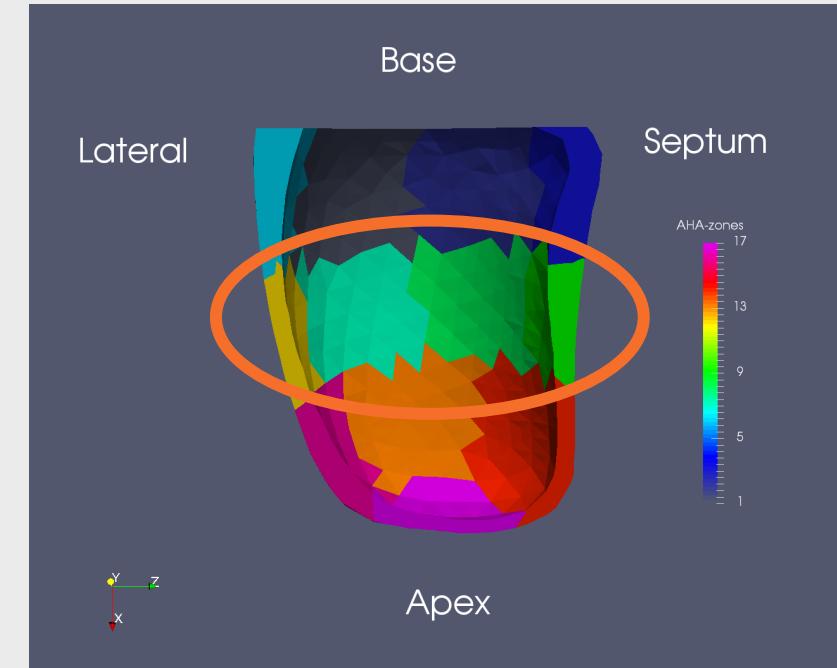
# The regional efficiency of each segment show the same trend regardless of how work is estimated



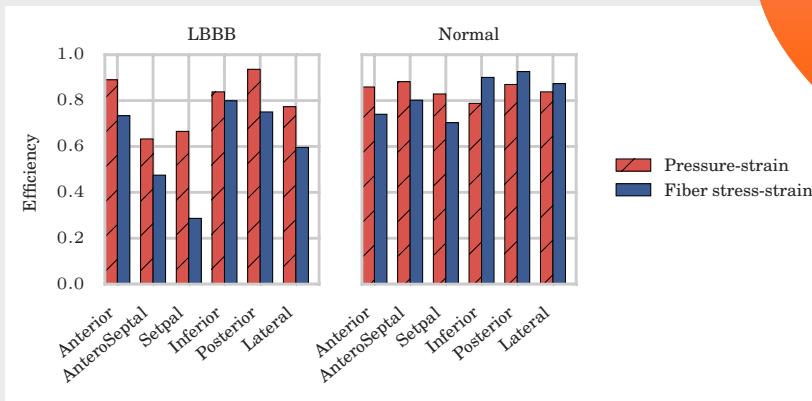
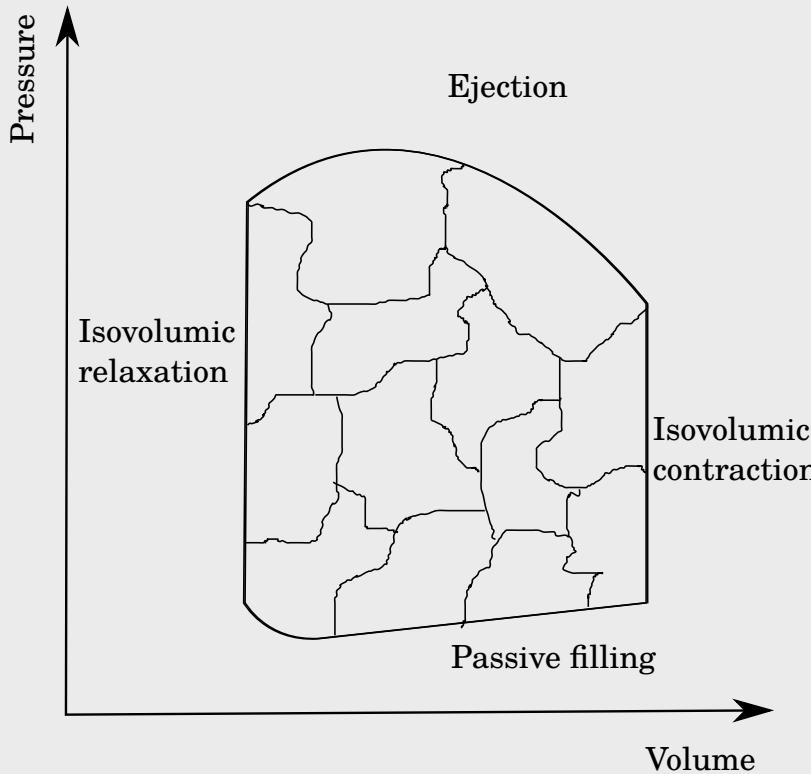
Regional total power density  
Positive values indicate generation of work  
Negative values indicate work usage



Regional efficiency  
Higher values indicate higher efficiency

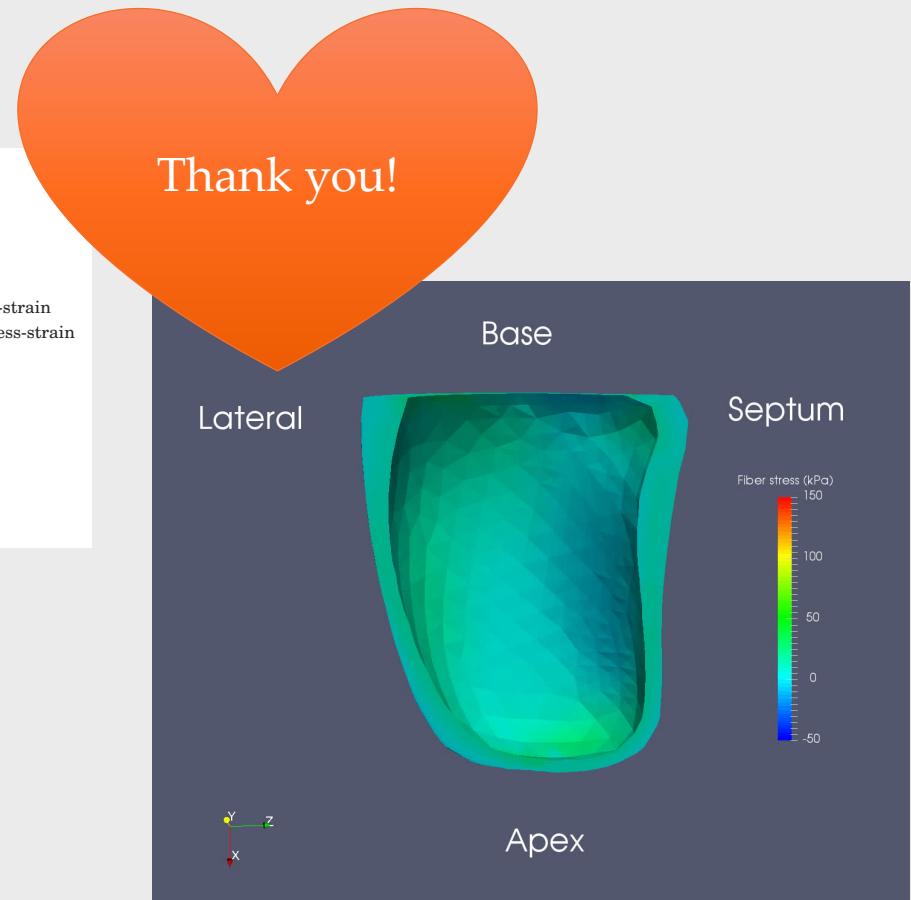


# Patient-specific modeling can be used to assess estimates regional myocardial work



## Acknowledgement

John Aalen  
Camilla K. Larsen  
Espen Remme  
Joakim Sundnes  
Otto A. Smiseth  
Samuel Wall



Thank you!



Oslo  
universitetssykehus



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