

# TV-Based Deconvolution for Medical Imaging

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Here we discuss the extension of the semi-implicit method for TV denoising to TV deconvolution using Rician and Poisson noise models.

**Notations** Let  $\mathcal{N}_{i,j,k}$  denote the six axial neighbors of voxel  $(i, j, k)$  in three dimensions, and define

$$g_{i,j,k}^\ell = \left[ \epsilon + \sum_{n \in \mathcal{N}_{i,j,k}} (u_n^\ell - u_{i,j,k}^\ell)^2 \right]^{-1/2}$$

where superscript  $\ell$  denotes iteration. In the following,  $\lambda$  is the weight on the fidelity term,  $\sigma$  is a parameter of the Rician distribution related to the standard deviation, and  $\gamma = \lambda/\sigma^2$ .

**Rician** We use a semi-implicit scheme. For Rician noise, it is

$$u_{i,j,k}^{\ell+1} = \frac{u_{i,j,k}^\ell + dt \left( \sum_{n \in \mathcal{N}_{i,j,k}} g_n^\ell u_n^\ell + \gamma K^* \left[ -K u^\ell + \frac{I_1(f K u^\ell / \sigma^2)}{I_0(f K u^\ell / \sigma^2)} f \right]_{i,j,k} \right)}{1 + dt \left( \sum_{n \in \mathcal{N}_{i,j,k}} g_n^\ell \right)}. \quad (1)$$

Unfortunately, the scheme must have  $dt$  sufficiently small for stability. It is not clear how choose  $dt$  a priori so that the scheme is guaranteed to be stable. The largest possible  $dt$  depends on the image, on  $K$ , and on the parameters. It seems that smaller  $dt$  is necessary for larger values of  $\lambda$  and for blurs  $K$  with greater support.

Rician deconvolution is implemented as a C/MEX function in `riciandeconv3mx.c`, which is called from MATLAB as

```
u = riciandeconv3mx(f,K,sigma,lambda,NumIter,dt)
```

For simplicity, the routine is limited to isotropic Gaussian blurs. The parameters are

<code>f</code>	input volumetric image (3D double array)
<code>K</code>	standard deviation of the Gaussian blur in voxels
<code>sigma</code>	parameter $\sigma$ of the Rician noise
<code>lambda</code>	regularization parameter
<code>NumIter</code>	number of method iterations
<code>dt</code>	timestep parameter

Parameter `lambda` balances the accuracy of deconvolution vs. denoising strength: smaller `lambda` implies stronger denoising but at the cost of deconvolution accuracy.

A substantial amount of computation time is spent evaluating convolutions (about 50% for the example in Figure 1), which is one motivation for restricting to only Gaussian blurs. Gaussian convolution is implemented using the recursive filtering algorithm of Alvarez and Mazorra [1] in `gaussianblur.c`.

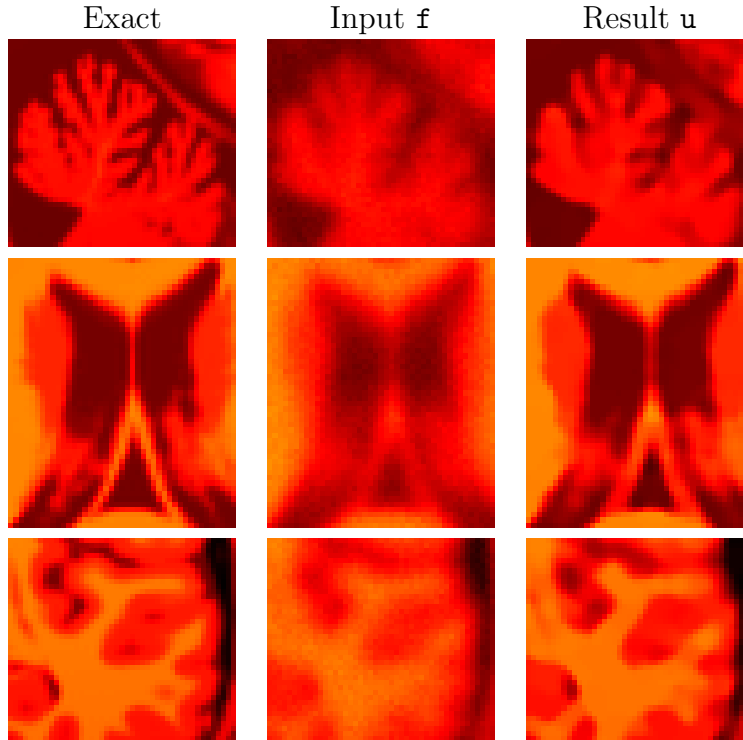


Figure 1: Experiment with TV-based Rician deconvolution. *Left column:* a simulated MRI brain volume of size  $217 \times 181 \times 181$  was taken as the exact data. *Middle column:* the exact data was blurred ( $K = 1.8$ ) and corrupted with Rician noise ( $\sigma = 0.008$ ) to produce the input data. *Right column:* the restored result was computed using `riciandeconv3mx` (`lambda` = 0.085, `NumIter` = 100, `dt` = 0.001) with a computation time of 179 s.

For correct results, it is critical that `dt` is chosen small enough for stability. Unfortunately, how small `dt` must be depends on the image and the other parameters, so experimentation is required to set `dt` appropriately.

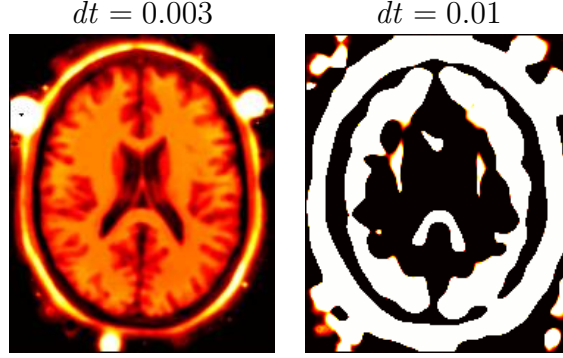


Figure 2: Examples of instability where  $dt$  is too large, computed with `NumIter` = 5. The maximum stable  $dt$  depends on the image and parameters.

**Poisson** Following [2], we can derive a similar semi-implicit scheme for Poisson noise as

$$\begin{aligned} \min_u \int |\nabla u| \, dx + \lambda \int (Ku - f \log Ku) \, dx \\ \partial_t u = \operatorname{div} \left( \frac{\nabla u}{|\nabla u|} \right) + \lambda K^* \left( \frac{f}{Ku} - 1 \right) \\ \frac{u_{i,j,k}^{\ell+1} - u_{i,j,k}^{\ell}}{dt} = \sum_{n \in \mathcal{N}_{i,j,k}} g_{i,j,k}^{\ell} (u_n^{\ell} - u_{i,j,k}^{\ell+1}) + \lambda K^* \left( \frac{f}{Ku^{\ell}} - 1 \right) \\ u_{i,j,k}^{\ell+1} = \frac{u_{i,j,k}^{\ell} + dt \left( \sum_{n \in \mathcal{N}_{i,j,k}} g_n^{\ell} u_n^{\ell} + \lambda K^* \left( \frac{f}{Ku^{\ell}} - 1 \right) \right)}{1 + dt \left( \sum_{n \in \mathcal{N}_{i,j,k}} g_n^{\ell} \right)}. \end{aligned}$$

Poisson deconvolution is implemented as a C/MEX function in `poissondeconv3mx.c`, and is called from MATLAB as

```
u = poissondeconv3mx(f,K,lambda,NumIter,dt)
```

The parameters are the same as `riciandeconv3mx`, except there is no `sigma` parameter for the Poisson model. As with `riciandeconv3mx`, it is important to choose `dt` sufficiently small for stability, and the maximum stable `dt` depends on the image and the parameters.

## References

- [1] L. ALVAREZ AND L. MAZORRA. “Signal and image restoration using shock filters and anisotropic diffusion” *SIAM Journal on Numerical Analysis*, 1994.
- [2] T. LE, R. CHARTRAND AND T. ASAKI. “A Variational Approach to Constructing Images Corrupted by Poisson Noise,” *JMIV*, vol. 27(3), pp. 257–263, 2007.

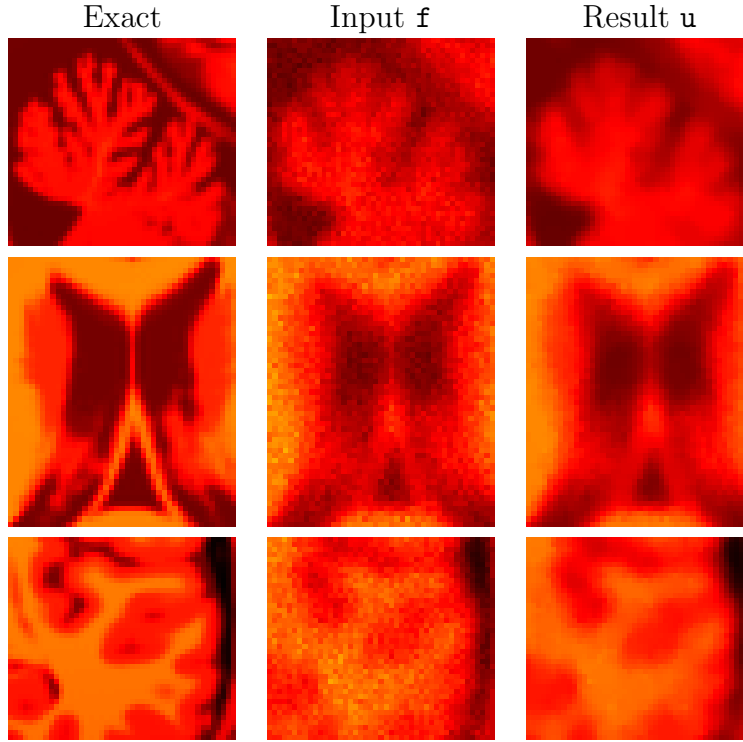


Figure 3: Experiment with TV-based Poisson deconvolution. *Left column:* a simulated MRI brain volume of size  $217 \times 181 \times 181$  was taken as the exact data. *Middle column:* the exact data was blurred ( $K = 1.8$ ) and corrupted with Poisson noise to produce the input data. *Right column:* the restored result was computed using `poissondeconv3mx` (`lambda = 15`, `NumIter = 200`, `dt =  $8 \times 10^{-5}$` ) with a computation time of 340 s.