

Exercise 04: Hodgkin-Huxley model

Theoretical Neuroscience I

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1 Analytic derivation

Start from

$$c_m \frac{dV}{dt} = -i_L - i_{Na} - i_K + i_e.$$

The different parts of the membrane current

$$i_L = g_L(V - E_L) \quad i_{Na} = g_{Na}m^3h(V - E_{Na}) \quad i_K = g_Kn^4(V - E_K)$$

can be substituted with the respective conductance times driving force:

$$c_m \frac{dV}{dt} = -g_L(V - E_L) - g_{Na}m^3h(V - E_{Na}) - g_Kn^4(V - E_K) + i_e$$

Factorize and sort according to V ...

$$= -g_LV - g_{Na}m^3hV - g_Kn^4V + g_LE_L + g_{Na}m^3hE_{Na} + g_Kn^4E_K + i_e$$

...so that we can factorize $-V$...

$$= -V(g_L + g_{Na}m^3h + g_Kn^4) + g_LE_L + g_{Na}m^3hE_{Na} + g_Kn^4E_K + i_e$$

...and factorize $(g_L + g_{Na}m^3h + g_Kn^4)$...

$$= (g_L + g_{Na}m^3h + g_Kn^4) \left(\frac{g_LE_L + g_{Na}m^3hE_{Na} + g_Kn^4E_K + i_e}{g_L + g_{Na}m^3h + g_Kn^4} - V \right)$$

...and finally divide everything by c_m .

$$\frac{dV}{dt} = \frac{g_L + g_{Na}m^3h + g_Kn^4}{c_m} \left(\frac{g_LE_L + g_{Na}m^3hE_{Na} + g_Kn^4E_K + i_e}{g_L + g_{Na}m^3h + g_Kn^4} - V \right)$$

With

$$\tau_{\text{eff}} = \frac{c_m}{g_L + g_{Na}m^3h + g_Kn^4} \quad \text{and} \quad V_{\infty}^{\text{eff}} = \frac{g_LE_L + g_{Na}m^3hE_{Na} + g_Kn^4E_K + i_e}{g_L + g_{Na}m^3h + g_Kn^4}$$

this is equal to

$$\frac{dV}{dt} = \frac{1}{\tau_{\text{eff}}} (V_{\infty}^{\text{eff}} - V)$$

2 Simulation of neurons

We start by simulating a neuron without an input current in order to observe the resting state (steady state) of the neuron. The time courses of the state variables are shown in Figure 1. The membrane voltage, as well as the n and m gating variables relax close to their steady state values within a few ms. The inactivation variable h on the other hand takes considerably longer to reach its equilibrium value (approx. 18ms to get to 90% of the final value). The steady state values are $V_{ss} = -65\text{mV}$, $n_{ss} = 0.3175$, $m_{ss} = 0.0529$ and $h_{ss} = 0.5914$.

Now we use the steady state of the neuron as the initial state for a neuron with a large constant input current of 100nA mm^{-2} (Figure 2). Within 40ms we can observe three action potentials. The first action potential has a slightly larger amplitude than the other two, who appear equal in size.

During an action potential the membrane potential rises within a few ms to $\sim 30\text{--}40\text{ mV}$ (depolarization), then falls just as quickly to around -75mV , which is 10 mV below the resting potential of -65mV (repolarization and hyperpolarization). After this the membrane potential rises slowly, almost linearly, until it reaches a threshold value (approx. -50mV) at which point another action potential is initiated. At the beginning of an action potential the sodium activation gates m open very quickly, then stay almost completely open for a few ms before closing very quickly again. The sodium inactivation gates h close more slowly than the m gates open and after the action potential is over only gradually reopen. The potassium gates n operate on a similar time scale as the h gates but open first, then gradually close again.

Next we use a different initial state for the neuron and an intermediate constant input current of 62nA mm^{-2} (Figure 3). Two action potentials are generated within 40ms. They have a slightly lower amplitude than the action potentials generated with the large input current, but otherwise the time courses do not differ much after the membrane has crossed a certain threshold.

Finally, a slightly lower constant input current of 61nA mm^{-2} is used (Figure 4). Here only a single action potential is generated. After 19.7ms the membrane voltage has returned to the initial value of -65mV , but now the gating variables are slightly different. The potassium gating variable n is slightly larger (0.374 vs. 0.37) whereas the sodium gating variables m and h are both slightly lower (0.05 and 0.49 vs. 0.08 and 0.5 respectively). These changes cause the membrane potential to rise slightly more slowly. As a result the potassium channels open enough to push the membrane potential back down, before the self-reinforcing opening of sodium channels can be triggered. This example demonstrates the high sensitivity of the Hodgkin-Huxley model to initial conditions.

We can see, that with the interaction of just four dynamic variables, the Hodgkin-Huxley model exhibits many of the properties of a real neuron:

- The characteristic time course of an action potential with depolarization, repolarization and hyperpolarization.
- Voltage-dependent firing rates.
- A refractory period, in which no additional action potentials can be elicited.
- An implicit threshold potential, above which the action potential is triggered.
- Repeated action potentials are more difficult to elicit and have a smaller amplitude.

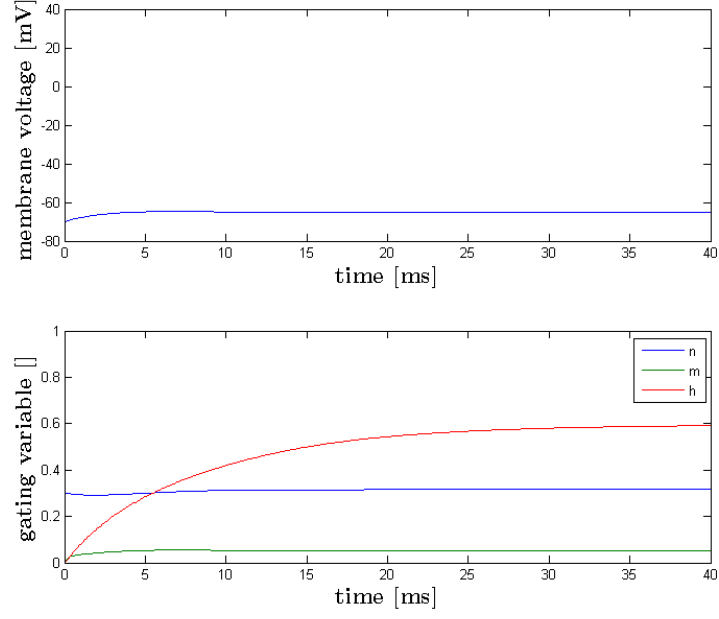


Figure 1: No input current. Initial condition: $V_0 = -70\text{mV}$, $n_0 = 0.3$, $m_0 = h_0 = 0$. Top: Membrane voltage over time. Bottom: Gating variables n, m and h over time.

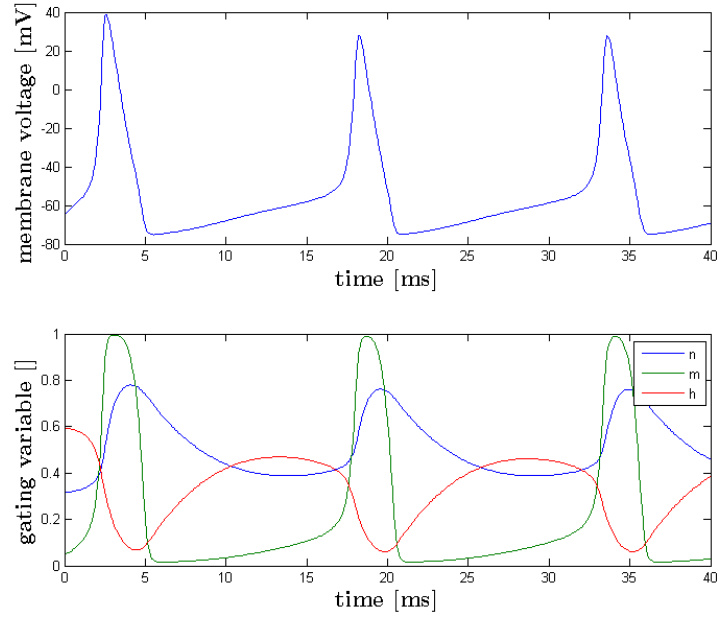


Figure 2: Constant input current of 100nA mm^{-2} . The initial condition is equal to the steady state condition of the neuron with zero input current (see Figure 1). Top: Membrane voltage over time. Bottom: Gating variables n, m and h over time.

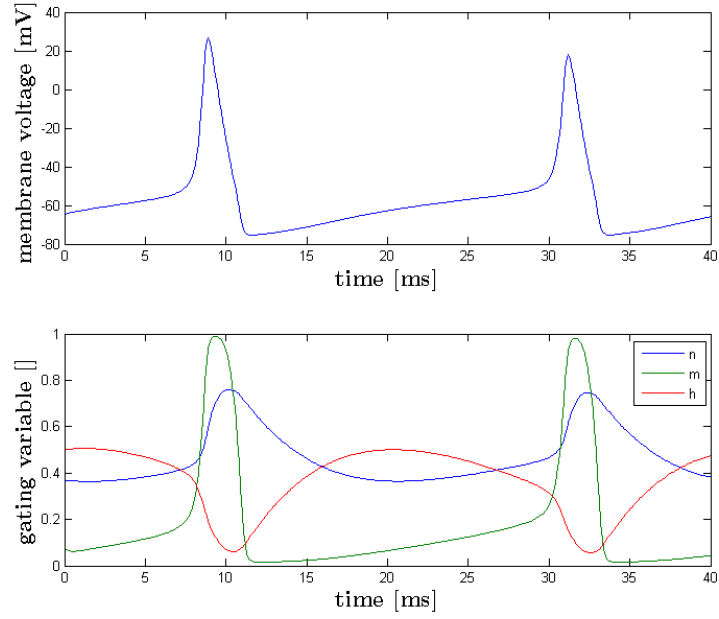


Figure 3: Constant input current of 62 nA mm^{-2} . Initial condition: $V_0 = -65 \text{ mV}$, $n_0 = 0.37$, $m_0 = 0.08$, $h_0 = 0.5$. Top: Membrane voltage over time. Bottom: Gating variables n, m and h over time.

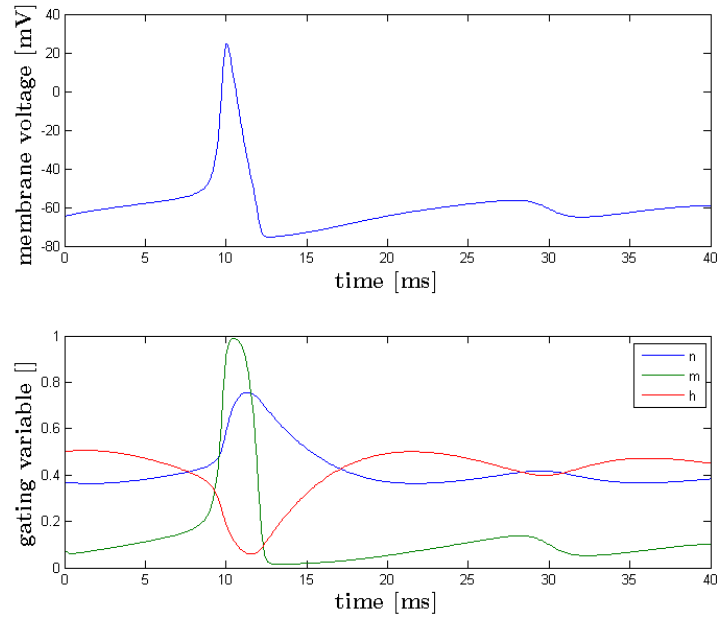


Figure 4: Constant input current of 61 nA mm^{-2} . Initial condition: $V_0 = -65 \text{ mV}$, $n_0 = 0.37$, $m_0 = 0.08$, $h_0 = 0.5$. Top: Membrane voltage over time. Bottom: Gating variables n, m and h over time.