

# Digital Image Processing in Radiography

Xiaohui Wang, PhD

David H. Foos, MS

Health Group Research Laboratory  
Eastman Kodak Company

## Outline

- **Display Processing**

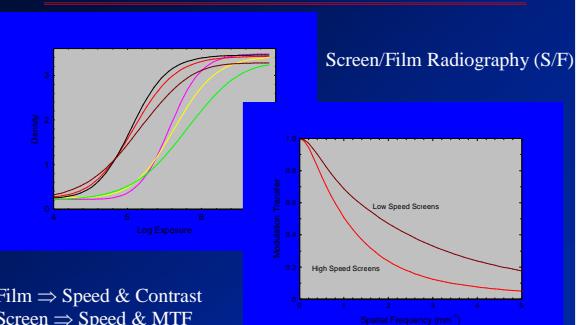
- Data preprocessing
- ROI segmentation and analysis
- Tonal rendering
- Signal equalization
- Edge restoration
- Noise suppression
- Collimation masking
- Display compensation

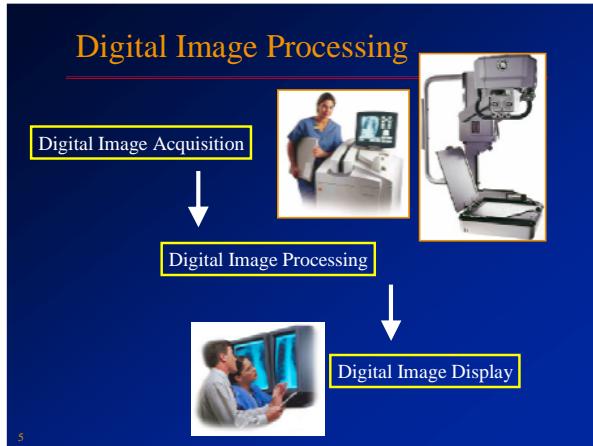
- **Image Processing Features**

- Stationary grid detection and suppression
- Long-length imaging
- Dual energy imaging
- Mammography
- Oncology processing
- Quality control testing

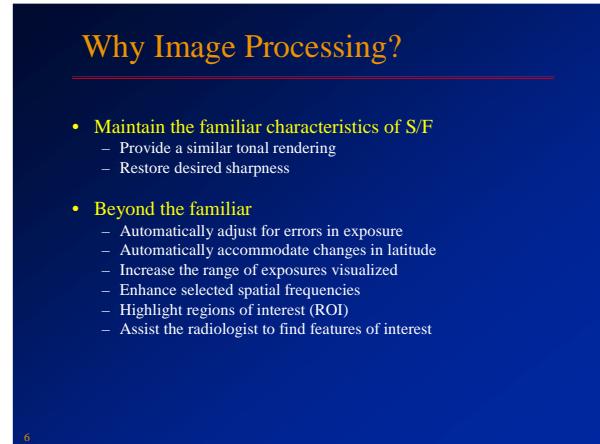
## Display Processing

## “Analog” Image Processing...

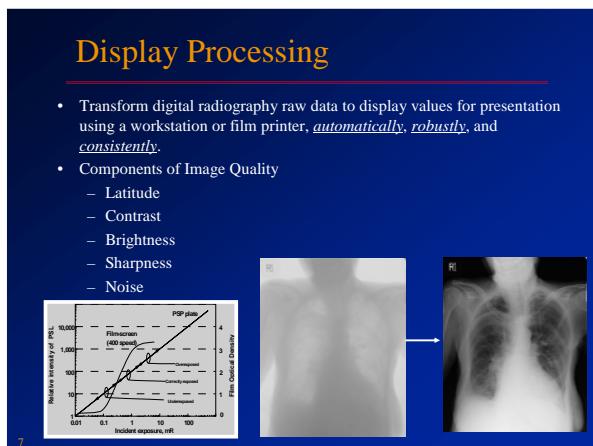




5



6



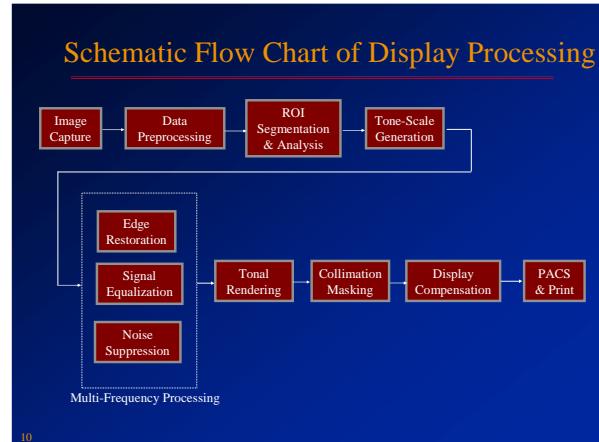
7



8



9



10

## Data Preprocessing

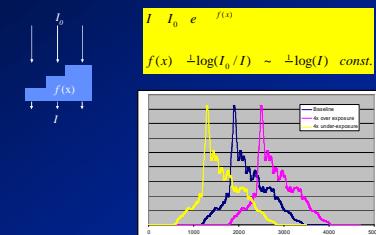
- **Image reformation**
  - Composition (dual-side CR reading)
  - Decomposition (dual energy)
  - Resize
- **Signal filtering**
  - Gain, offset, and bad pixel correction (DR)
  - Noise reduction
  - Stationary grid artifact suppression
- **Data space conversion**
  - Linear to logarithmic (const. object contrast vs. pixel value)
  - Linear to square root (const. quantum noise vs. pixel value)

11

## Data Preprocessing (cont.)

### Linear-to-log conversion

Shape of image histogram invariant to exposure



12

## ROI Segmentation & Analysis

- Extract diagnostically relevant ROIs
- Analyze ROI characteristics
- Derive the optimal display-rendering parameters
- Include four basic steps
  - Detect collimation mask
  - Detect direct exposure
  - Extract anatomy regions
  - Calculate key image descriptors



13

## Segmentation – Collimation Mask

- Confine exposure regions
- Mask applied to collimated regions to reduce viewing flare

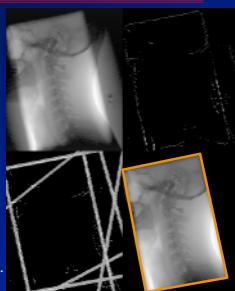


"Method for recognizing multiple radiation fields in computed radiography," X. Wang, J. Luo, R. Senn, and D. Foos, Proc SPIE 3661, 1625-36, 1999.

14

## Segmentation – Collimation Mask (cont.)

- Collimation boundary pixels
  - Edge profile analysis
  - Transition segments classification
- Candidate collimation blades
  - Edge delineation
  - FOM analysis
    - straightness
    - connectedness...
- Candidate configurations
- Select “best” configuration
  - Parallelism, convexity, orthogonality, etc.



J. Luo and R. Senn, "Collimation detection for digital radiography," Proc. SPIE 3034, 74-85 (1997).

15

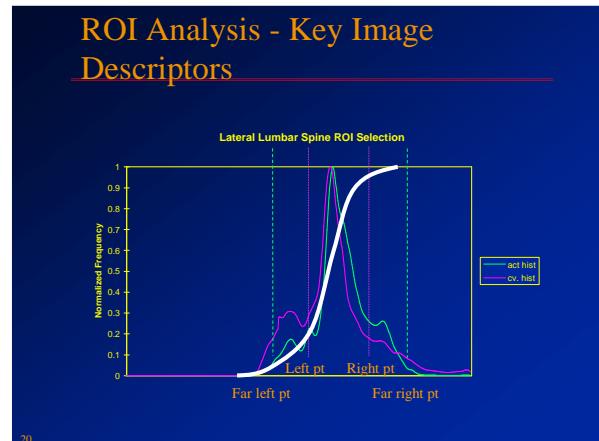
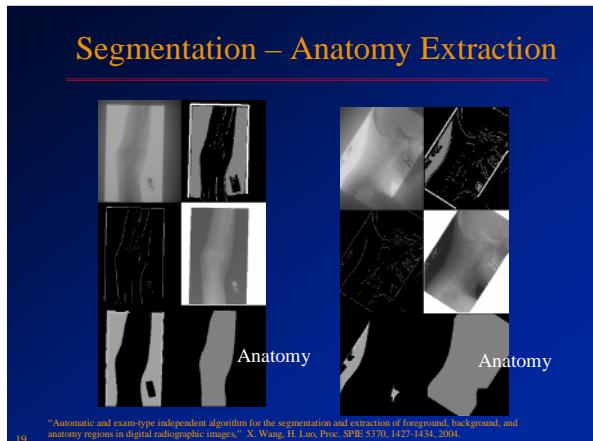
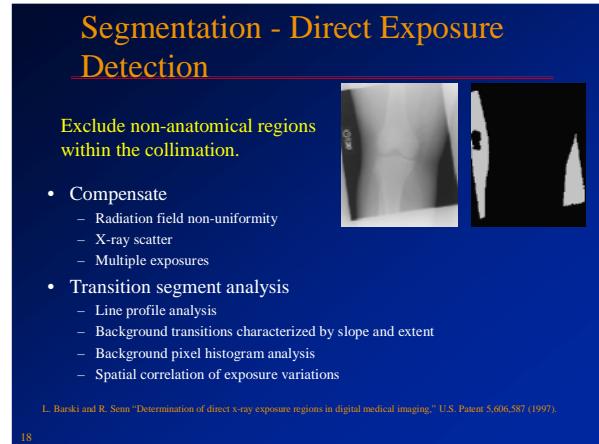
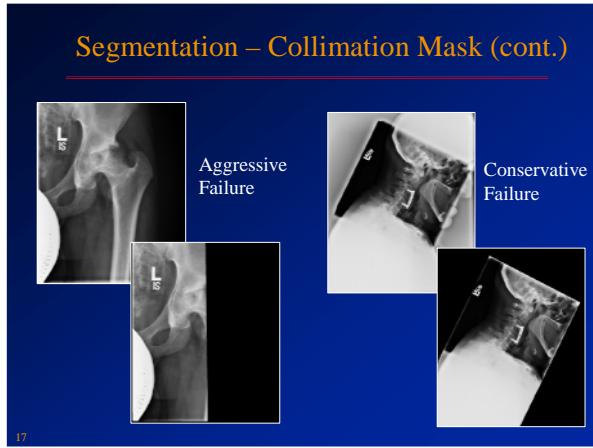
## Segmentation – Collimation Mask (cont.)

- Multiple radiation field masking
  - Optimal individual image processing
  - Exam workflow improvement



"Method for recognizing multiple radiation fields in computed radiography," X. Wang, J. Luo, R. Senn, and D. Foos, Proc. SPIE 3661, 1625-36, 1999.

16

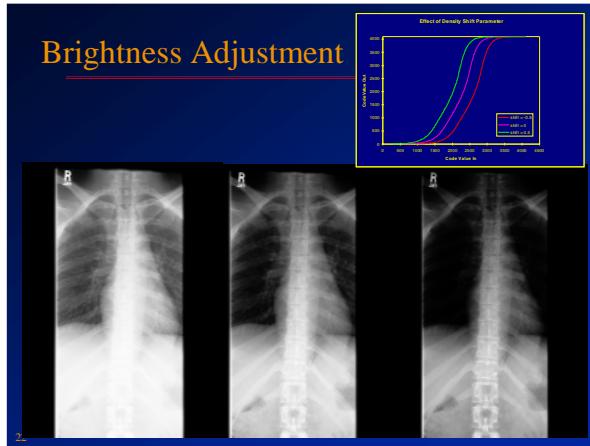


## Tone-Scale Generation

- Render image with proper brightness and contrast
  - Calculate average exposure within ROI
  - Automatically adjust for errors in exposure
- Sigmoid curve shape in general
  - Curve shift (brightness adjustment)
  - Curve rotation (contrast adjustment)
  - Toe & shoulder adjustment
- Bear different names
  - Kodak: **PTS** (Perceptual Tone Scale)
  - Fuji: **Gradation Processing**
  - ...

21

## Brightness Adjustment



## Contrast Adjustment



23

## Toe & Shoulder Adjustment



24

## Visually Optimized Tone Scale

### Perceptual Linearity -

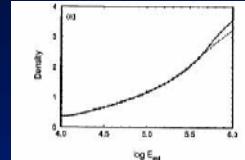
Render ROI such that... equal physical contrast being perceived as equal brightness by the observer across the full brightness range



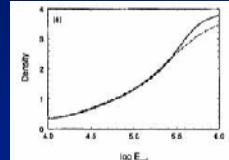
25

## Visually Optimized Tone Scale (cont.)

Radiologists prefer S/F systems with perceptually linear sensitometric response.



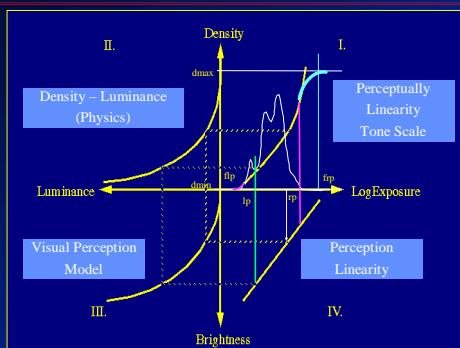
Kodak Insight Thoracic Imaging System



Kodak Insight HC Thoracic Imaging System

26

## Perceptual Tone Scale



27

## Perceptual Tone Scale (cont.)

### Equal Log (E) Equal Brightness

Daly's Global Cone Model

$$B = \frac{B_m L^n}{L^n + L_0^n}$$

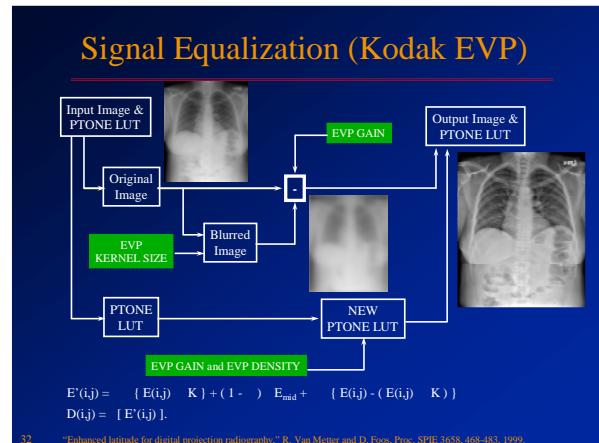
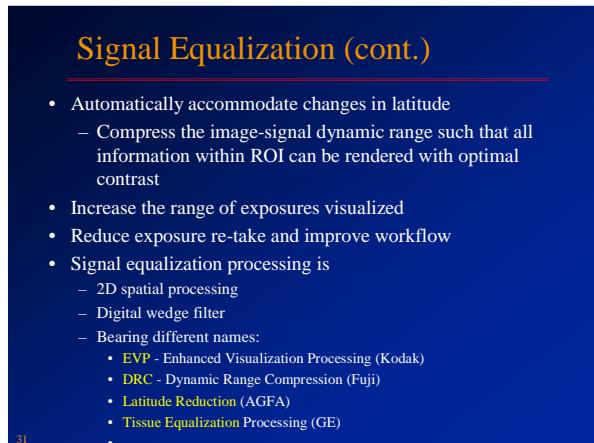
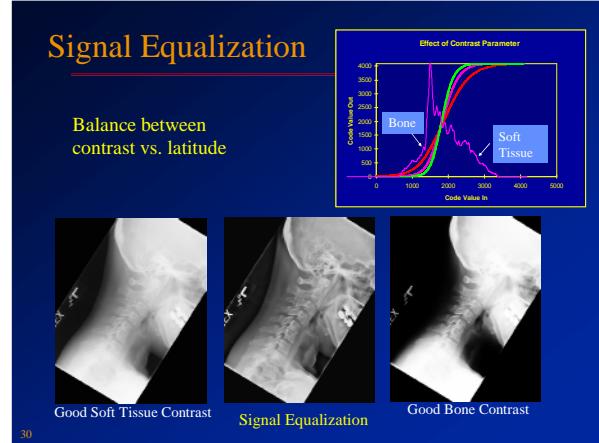
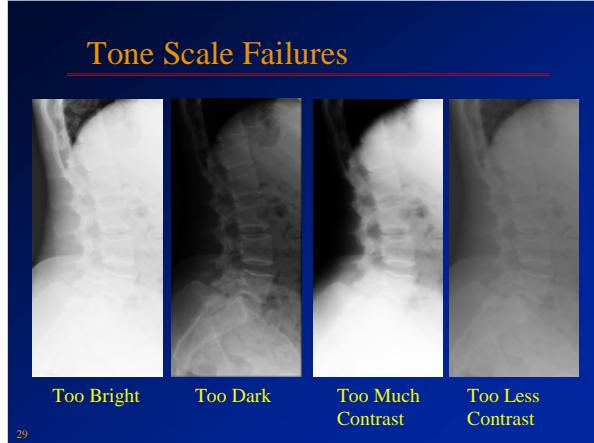
B = perceived brightness  
L = luminance of the image area  
B<sub>m</sub> = scale factor  
n = 0.7

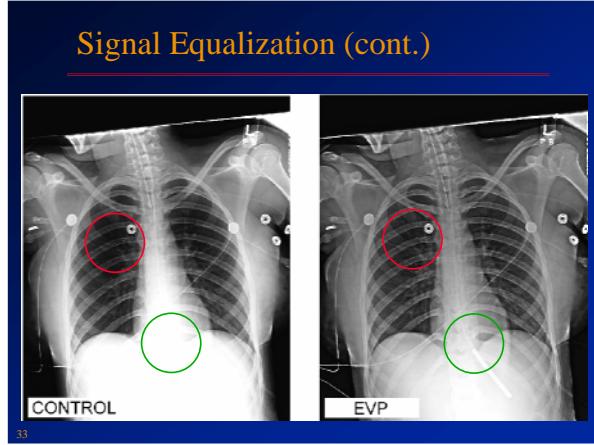
$$L_0 = 12.6 * (0.2 * L_w)^{0.63} + 1.083 * 10^{-5}$$

L<sub>w</sub> = luminance of the reference white

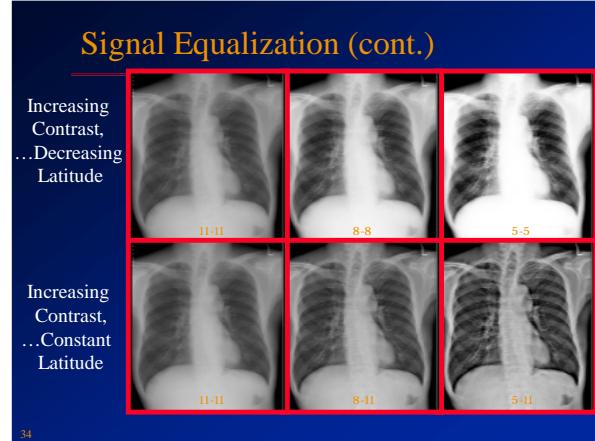
H. Lee, S. Daly, and R. Van Metter, "Visual optimization of radiographic tone scale," Proc. SPIE 3036, 118-129, 1996.

28





33



34

### RSNA 2001 Education Exhibit

1 Conference I CME  
American & Thoracic Society  
12-03 Nov to 1-03 '01

**Equalization Processing For Digital Chest Radiographs**

Henry Ford Health System  
Digital Image Research  
• Michael Flynn  
• William Eyer  
• Carl Zelcer  
Detroit, Michigan, USA

Eastman Kodak Company  
Health Science Research  
• Mary Couwenhoven  
• David Foss  
Rochester, New York, USA

Bethesda-Duke-St. Louis  
• Richard Stone  
• Bruce Whiting  
St. Louis, Missouri, USA

Duke University  
Radiology Department  
• Bruce Stone  
• Edith Morris  
• Carl Raiss  
Durham, N. Carolina, USA

A multi-center study recommending image processing parameters to be used for the display of chest radiographs

11 Subject Effect  
The optimal latitude - contrast coordinate depends on the subject  
The coordinate of optimal processing one should fall on a straight line.  
The straight line is called the Optimal Latitude-Contrast (OLC) line.  
This is due to the large variance in subjects and the small variance in the differences in subject contrast.  
Optimal contrast is found to be proportional to OLC mode which is a straight line on a log-log plot. The further one moves away from the OLC line, the greater the contrast gain or loss.

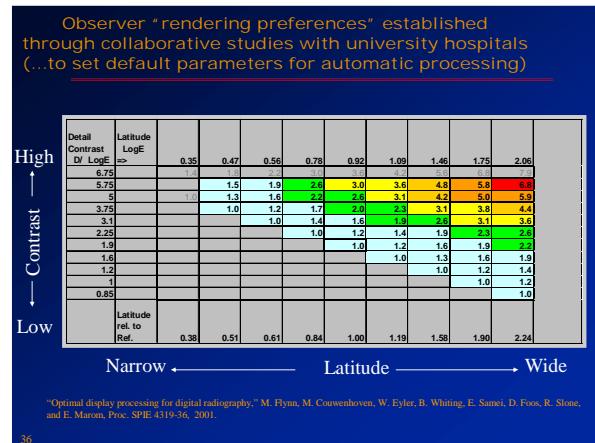
Detail Contrast Log <sub>10</sub>	Latitude	1.0	0.92	0.84	0.76	0.68	0.60	0.52	0.44	0.36
0.35	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0
0.47	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0
0.56	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0
0.78	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0
0.92	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0
1.09	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0
1.46	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0
1.75	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0
2.06	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0
5.75	1.5	1.0	2.0	3.0	3.6	4.8	5.8	6.8		
5	1.3	1.0	2.2	2.8	3.1	4.2	5.0	5.9		
3.75	1.0	1.2	1.7	2.0	2.3	3.1	3.8	4.4		
3.1	1.0	1.4	1.8	2.0	2.3	3.1	3.7	4.3		
2.25	1.0	1.2	1.4	1.9	2.1	3.1	3.7	4.3		
1.9	1.0	1.2	1.6	1.9	2.1	3.1	3.7	4.3		
1.6	1.0	1.2	1.6	1.9	2.1	3.1	3.7	4.3		
1.2	1.0	1.2	1.6	1.9	2.1	3.1	3.7	4.3		
1	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0		
0.85	1.0	1.0	1.0	1.0	1.0	1.0	1.0	1.0		

High Contrast → Low Contrast ←

Narrow ← Latitude → Wide

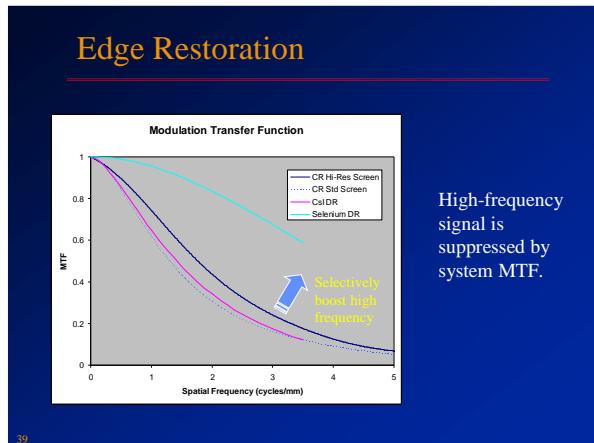
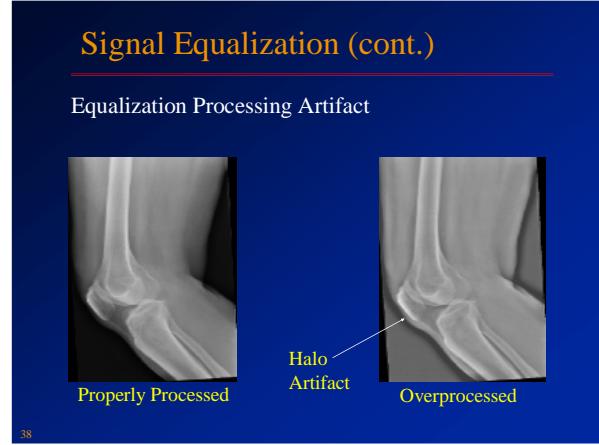
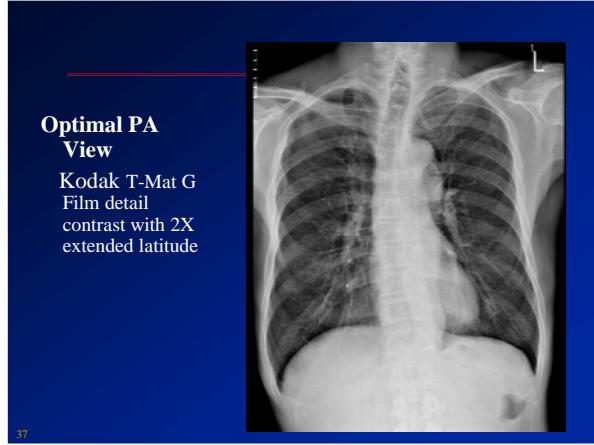
Latitude ref. to Ref.

35



"Optimal display processing for digital radiography," M. Flynn, M. Couwenhoven, W. Eyer, B. Whiting, E. Sancet, D. Foss, R. Stone, and E. Marion, Proc. SPIE 4319-36, 2001.

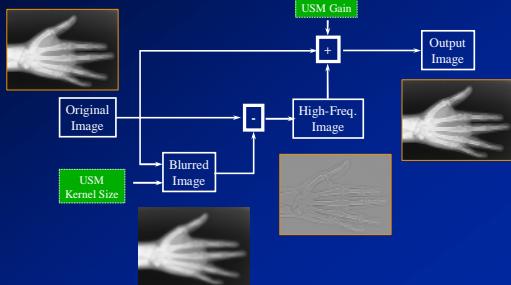
36



- ### Edge Restoration (cont.)
- Selectively boost high-frequency signals based on
    - Exam type
    - Brightness
    - Exposure
    - Diagnostic features
    - Capture device characteristics
  - Multi-frequency processing (2D spatial)
    - Kodak: **EVP & USM** (Enhanced Visualization Processing & UnSharp Mask)
    - AGFA: **MUSICA** (MUlti-Scale Image Contrast Amplification)
    - Konica: **Hybrid** (Multi-Resolution Hybrid Processing)
    - Fuji: **USM & MFP** (Multi-Objective Frequency Processing)
    - Philips: **UNIQUE** (UNified Image QUality Enhancement)
- 40

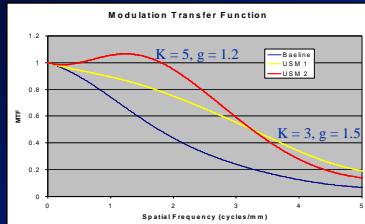
## Edge Restoration (cont.)

### Unsharp Mask Processing



41

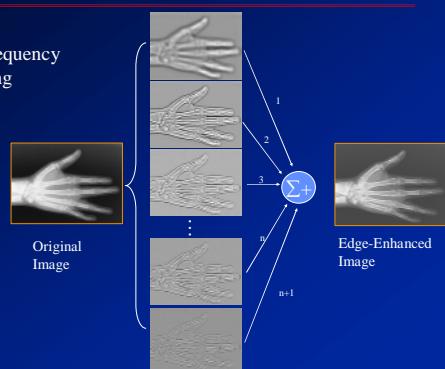
## Edge Restoration (cont.)



42

## Edge Restoration (cont.)

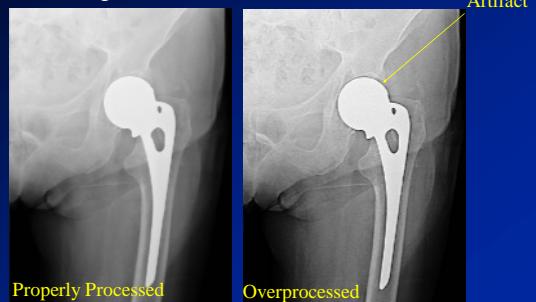
### Multi-Frequency Processing



43

## Edge Restoration (cont.)

### Processing Artifact



44

## Edge Restoration (cont.)

### Processing Artifact



45

## Noise Suppression

- It is desired to drive toward lower x-ray exposures to reduce patient dose
- The appearance of noise increases as exposure level is decreased
- A predominant source of noise in digital radiography is generally the quantum noise.
- Noise suppression should be signal dependent, it should be applied only to areas of the image that have a low SNR.
- A noise suppression algorithm needs to reduce the appearance of noise while preserving diagnostic detail.

"Observer study of a noise suppression algorithm for computed radiography images" M. Couwenhoven et al. Proc. SPIE 5749, 318-327, 2005.

46

## Noise Suppression (cont.)

Suppress the noise in low signal areas and phase out suppression in high signal areas

High Signal Areas / Less Dense Anatomy

Low Signal Areas / More Dense Anatomy

47

## Noise Suppression (cont.)

### Noise Suppression

- 2D spatial processing
- Applies to high freq. signals
- Signal dependent
- Balance between sharpness & noise



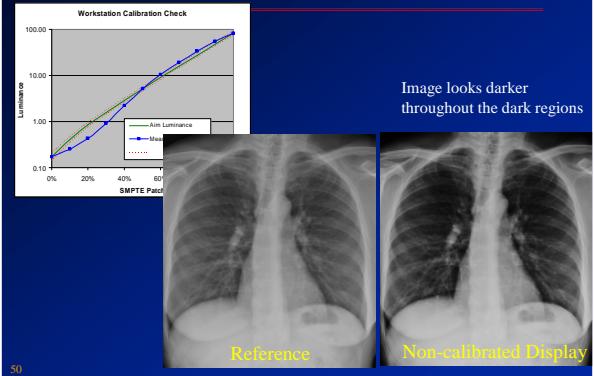
48

## Display Compensation

- Image pixel values can be mapped for different output devices
  - Film printer (monochrome 1)
  - Softcopy display (monochrome 2)
- Both capture and output devices need to be configured properly
- Output device calibration is critical to optimal image display
  - Different dynamic range and response
  - CRT vs. flat-panel
  - Images from multi-vendors viewed at same PACS workstation
  - Archived images
- DICOM Part 14 specifies grayscale display standard function (GSDF)
- AAPM TG-18 specifies display QA & QC testing

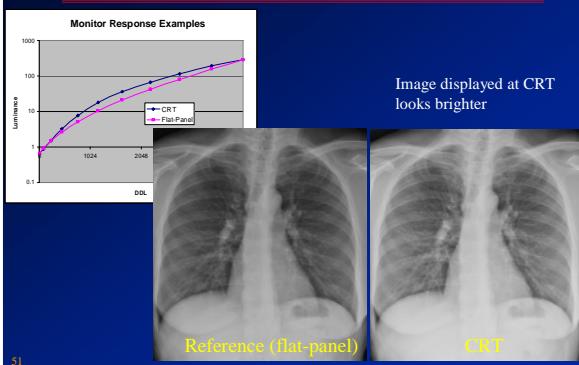
49

## Display Compensation (cont.)



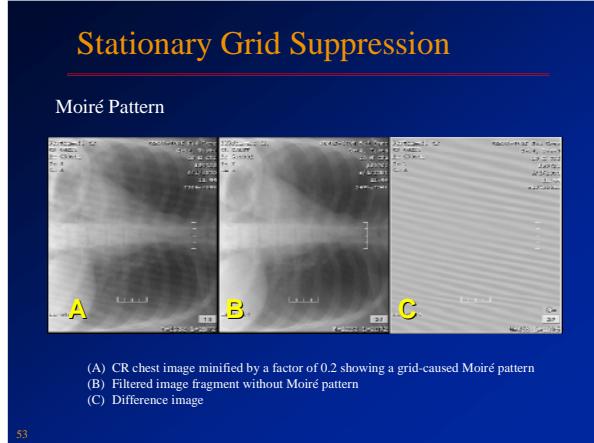
50

## Display Compensation (cont.)

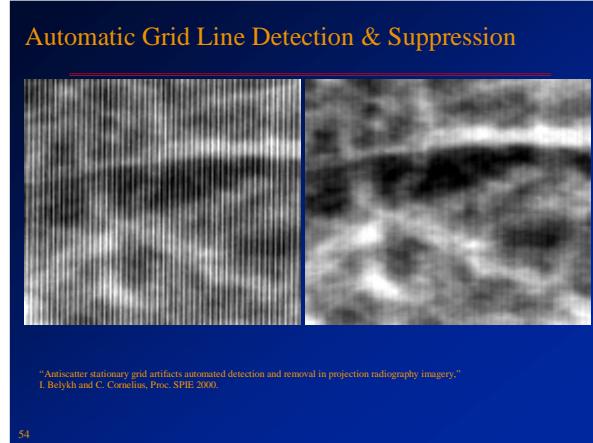


51

## Image Processing Features



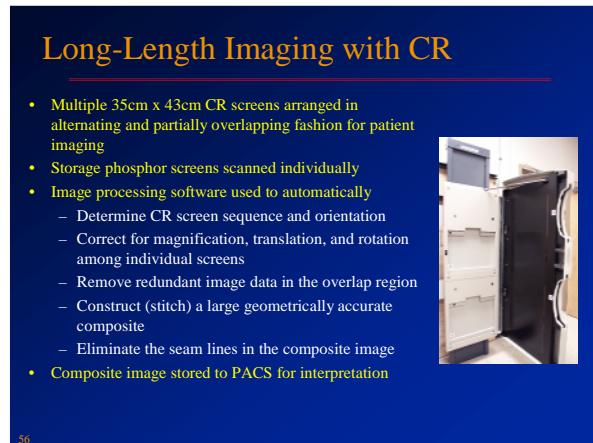
53



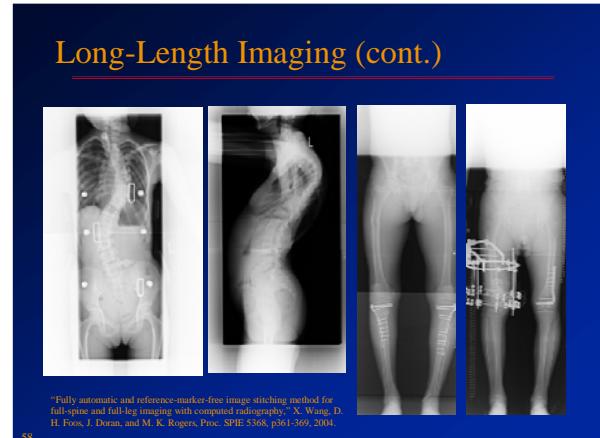
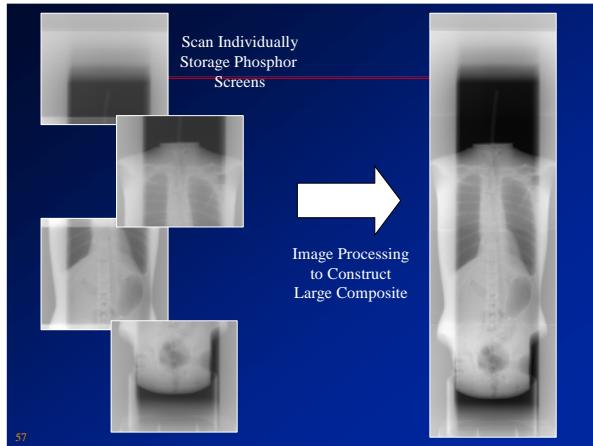
54



55



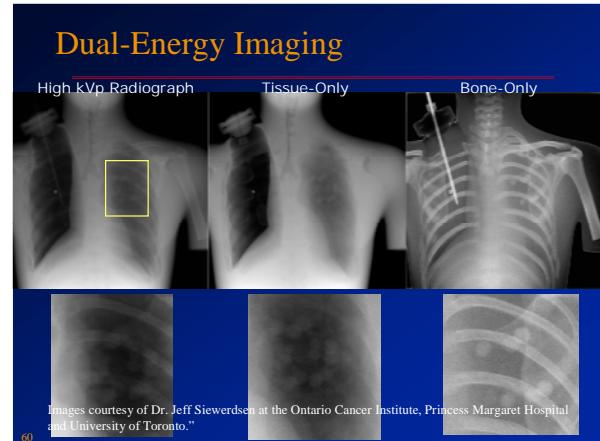
56



### Long-Length Imaging (cont.)

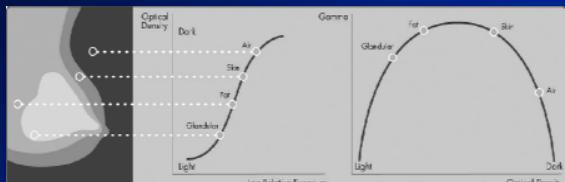
- Measurements from CR equivalent to screen-film
  - Angular
  - Absolute distance
- Visual quality of CR superior to S/F
  - Wide exposure latitude of CR
  - Equalization processing
- 35% retake rate with S/F reduced to 0% retake rate with CR
  - 43 cm width
  - Equalization processing

59



## Mammography Processing

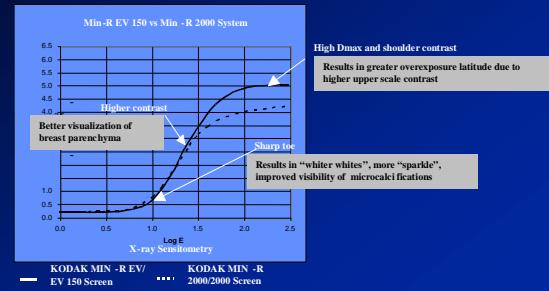
S/F: A large dynamic range is needed to detect and display all parts of the breast with good contrast



61

## Mammography Processing (cont.)

Recent advances in s/f mammography



62

## Mammography Processing

### Digital Mammography

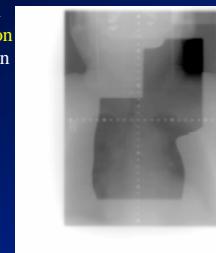
- Wide dynamic range (> 1000:1) captures all the image information
- Edge restoration enhances image details of different sizes
- Equalization processing compresses image latitude while maintaining contrast



63

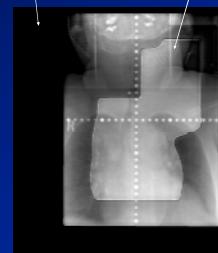
## Oncology Processing

Simulation  
Localization  
Verification

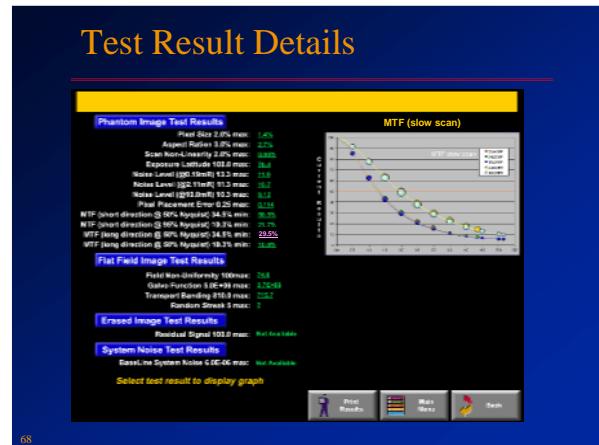
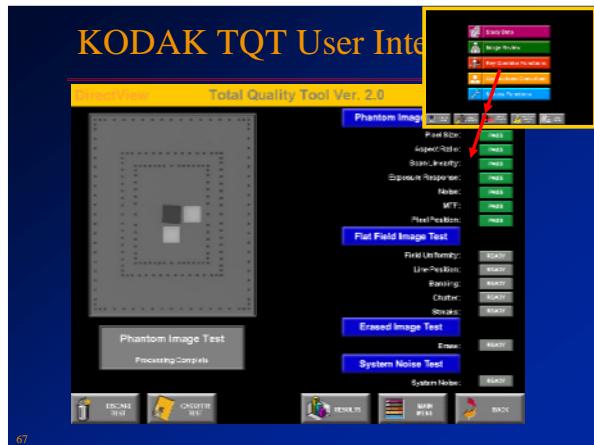
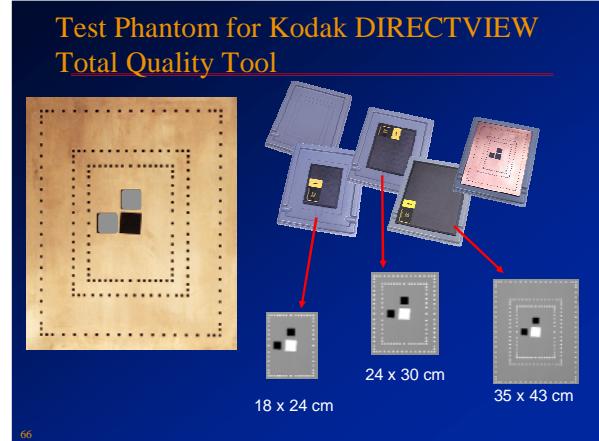


"Method for contrast-enhancement of digital portal images," S. Young, W. E. Moore, D. H. Fook, US Patent US6836570 B2

Black surround      Signal Equalization



64



## Quality Control Testing (cont.)

### Automated Image Quality Control Tool

- Precise and accurate quality control testing
- Highly reproducible quantitative results
- Detects sub-visible changes in CR image quality performance to initiate timely preventive maintenance
- Avoids hours of tedious and labor-intensive effort with a highly automated procedure
- Full data reporting in Excel format

69

## Summary

- Tone scale processing establishes the overall image brightness and global contrast
- Edge restoration enhances detail contrast
- Signal equalization extends the latitude that can be visualized while maintaining detail contrast
- Edge restoration, signal equalization, and noise suppression are 2D spatial processing
- Multi-frequency has been widely adopted, yet users should be aware of processing artifacts
- Display processing are becoming easier and more intuitive to use
- Image processing provides many new features unique to digital capture
- Image processing can provide many automations to improve work efficiency

70

## Acknowledgements

- Richard VanMetter
- Lori L. Barski
- William J. Sehnert
- Lynn M. Fletcher-Heath

71