

## 11 M11 – Chen et al 2008 – Insulin secretion, model of the $\beta$ -cell

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### Model Name

Short name: Chen2008

Long name: Chen-Wang-Sherman's model of Insulin Secretion by Kinetic Modeling of Granule Exocytosis

### General information

#### References:

1. Chen Y, Wang S, Sherman A. Identifying the Targets of the Amplifying Pathway for Insulin Secretion in Pancreatic  $\beta$ -Cells by Kinetic Modeling of Granule Exocytosis. *Biophysical Journal*. 2008 Set 1;95(5):2226–41. 10.1529/biophysj.107.124990 <http://www.ncbi.nlm.nih.gov/pmc/articles/PMC2517041/>
2. Supplementary material for the above (online) “Beta Cell Exocytosis Model”, <http://mrbl.niddk.nih.gov/sherman/gallery/beta/Vesicle/henquin-pools.ode>

#### Abstract (from Ref 1)

A kinetic model for insulin secretion in pancreatic  $\beta$ -cells is adapted from a model for fast exocytosis in chromaffin cells. The fusion of primed granules with the plasma membrane is assumed to occur only in the “microdomain” near voltage-sensitive L-type  $\text{Ca}^{2+}$ -channels, where  $[\text{Ca}^{2+}]$  can reach micromolar levels. In contrast, resupply and priming of granules are assumed to depend on the cytosolic  $[\text{Ca}^{2+}]$ . Adding a two-compartment model to handle the temporal distribution of  $\text{Ca}^{2+}$  between the microdomain and the cytosol, we obtain a unified model that can generate both the fast granule fusion and the slow insulin secretion found experimentally in response to a step of membrane potential. The model can simulate the potentiation induced in islets by preincubation with glucose and the reduction in second-phase insulin secretion induced by blocking R-type  $\text{Ca}^{2+}$ -channels ( $\text{CaV}2.3$ ). The model indicates that increased second-phase insulin secretion induced by the amplifying signal is controlled by the “resupply” step of the exocytosis cascade. In contrast, enhancement of priming is a good candidate for amplification of first-phase secretion by glucose, cyclic adenosine 3':5'-cyclic monophosphate, and protein kinase C. Finally, insulin secretion is enhanced when the amplifying signal oscillates in phase with the triggering  $\text{Ca}^{2+}$ -signal.

#### Short summary:

The model includes: a membrane; two types of inward  $\text{Ca}^{++}$  voltage-gated channels (L- and R-type); two corresponding compartments for calcium (microdomain and cytosol, respectively, Figure a below); insulin-carrying vesicles, arranged as a chain of states (from resupply to releasing, Figure b).

- Membrane depolarization is modeled as an input function  $V(t)$ ;
- $V$  influences the fraction of open L- and R- channels through the sigmoid function  $\text{minf}(V)$ ;
- Ions flow through L-type channels into  $C_{md}$  and through R-type channels into  $C_i$  (Ref. 1, Figure 1 and Figure a, left);
- $C_i$  leaks through the currents SERCA, PMCA, NCX and leak (eq. (6) and Figure a, right);
- $C_i$  gates priming ( $r_2$ ) and resupply ( $r_3$ ) rates for pre-docked granules;
- $C_{md}$  gates binding and fusion.

The equations for  $C_{md}$ ,  $C_i$  are a nonlinear 2-ODE system coupled to the membrane depolarization (glucose) input. Granule compartments  $N_{<...>}$  are a linear 10-ODE system with time-varying coefficients. Secretion is a simple integral; ISR is the secretion in the

last 2 min (per min). The original paper used a least-squares approach to fit the following parameters:  $g_L, B, k_1, k_{-1}, r_1, r_{-1}, r_2^0, r_{-2}, r_3^0, r_{-3}, u_1, u_2, u_3, K_p$ , plus the steady state (used as initial values).

#### Model and data source

The model and data have been derived from publications and the XPP implementation provided as supplementary material (Refs. 1-2).

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#### Structural model

Variables [symbol: description (units, ref values)]:

Symbol (eqns.)	Variable (code)	Description	Ref. v.	Units
$t$	t	time	0 – 60	min
$r_2$	r2	calcium-gated resupply rate	$0 - r_2^0$	$s^{-1}$
$r_3$	r3	calcium-gated priming rate	$0 - r_3^0$	$s^{-1}$
$N_1$	N1	no. of granules in primed microdomain pool	14.71 (*)	granules
$N_2$	N2	no. of granules in bound microdomain pool	0.612 (*)	granules
$N_3$	N3	no. of granules in triggered microdomain pool	0.008 (*)	granules
$N_4$	N4	no. of granules in fused microdomain pool	0 (*)	granules
$N_5$	N5	no. of granules in primed cytosol pool	24.54 (*)	granules
$N_6$	N6	no. of granules in docked cytosol pool	218.02 (*)	granules
$N_F$	NF	number of granules in fused pool	0.003 (*)	granules
$N_R$	NR	number of granules in releasing pool	0.51 (*)	granules
$SE$	SE	total secretion	0 – 250	granules
$ISR$	ISR	average secretion over the last 2 min	0 – 200	pg/islet/ min
$V$	V	Current membrane depolarization	-70 – -20	mV
$J_{SERCA}$	Jserca	Leak through SERCA	$0 - J_{SERCA}^{max}$	$\mu M/s$
$J_{PMCA}$	Jpmca	Leak through PMCA	$0 - J_{PMCA}^{max}$	$\mu M/s$
$J_{NCX}$	Jncx	Leak through NCX	-4 – 2	$\mu M/s$
$L$	L	Instantaneous total leak		$\mu M/s$
$I_L$	IL	Current through L-type channel	~ -1	fA
$I_R$	IR	Current through R-type channel	~ -0.3	fA
$J_L$	JL	Molar flux through L-type channel	~ -1.3	$\mu M/ms$
$J_R$	JR	Molar flux through R-type channel	~ -0.001	$\mu M/ms$
$C_{md}$	Cmd	Microdomain calcium concentration	0 – 40	$\mu M$
$C_i$	Ci	Cytosol calcium concentration	0 – 0.3	$\mu M$

(\*) Steady-state value

Parameters [symbol: description (units, ref values)]:

Symbol (eqns.)	Variable (code)	Description	Values	Units
$- (*)$	GlucFact	factor amplifying resupply in presence of glucose (1.2 at 3 mM glucose)	0 or 1.2	–
$k_1$	k1	Binding rate in microdomain (maximum)	20	$\mu\text{M}^{-1} \text{s}^{-1}$
$k_{-1}$	km1	Unbinding rate in microdomain	100	$\text{s}^{-1}$
$r_1$	r1	Cytosol to microdomain migration rate	0.6	$\text{s}^{-1}$
$r_{-1}$	rm1	Microdomain to cytosol migration rate	1	$\text{s}^{-1}$
$r_2^0$	r20	Priming rate in cytosol (maximum)	0.006	$\text{s}^{-1}$
$r_{-2}$	rm2	Cytosol un-priming rate	0.001	$\text{s}^{-1}$
$r_3^0$	r30	Resupply rate (maximum)	1.205	$\text{s}^{-1}$
$r_{-3}$	rm3	Un-resupply rate	0.0001	$\text{s}^{-1}$
$u_1$	u1	Fusion rate	2000	$\text{s}^{-1}$
$u_2$	u2	Fused-to-relasing rate	3	$\text{s}^{-1}$
$u_3$	u3	Release rate	0.02	$\text{s}^{-1}$
$K_p$	Kp	[Ca $^{++}$ ] for half-maximal effect on priming	2.3	$\mu\text{M}$
$K_p (*)$	Kp2	[Ca $^{++}$ ] for half-maximal effect on resupply	2.3	$\mu\text{M}$
$g_L$	gL	L-type channel conductivity	250	pS
$B$	B	Transport rate from microdomain to cytosol	200	$\text{s}^{-1}$
$V_m$	Vm	L-type channel switching voltage	-20	mV
$s_m$	sm	L-type channel switching range	5	mV
$V_{Ca}$	Vca	Calcium membrane reversal potential (?)	25	mV
$v_{cell}$	vcell	Volume of cell	1.15e-12	L
$v_{md}$	vmd	Volume of microdomain	4.2e-15	L
$f_V$	fv	$v_{md}/v_{cell}$	0.00365	-
$f_i$	fi	Free to bound Ca $^{++}$ ratio in cytosol	0.01	-
$f_{md}$	fmd	Free to bound Ca $^{++}$ ratio in microdomain	0.01	-
$J_{SERCA}^{max}$	Jsercamax	SERCA maximum leak flux	41	$\mu\text{M/s}$
$K_{SERCA}$	Kserca	SERCA Ca $^{++}$ half-switching concentration	0.27	$\mu\text{M}$
$J_{PMCA}^{max}$	Jpmcamax	PMCA maximum leak flux	21	$\mu\text{M/s}$
$K_{PMCA}$	Kpmca	PMCA Ca $^{++}$ half-switching concentration	0.5	$\mu\text{M}$
$J_{NCX}^0$	Jncx0	NCX leak rate constant	18.67	$\mu\text{M/s}$
$J_{leak}$	Jleak	Time-independent Ca $^{++}$ leak	-0.94	$\mu\text{M/s}$

(\*) notation used in the paper's equations is slightly different from the code. See "implementation notes"

Constants [symbol: description (units, values)]:

Symbol (eqns.)	Variable (code)	Description	Values	Units
$\alpha$	alpha	(1/2) Faraday $^{-1}$	5.18e-16	$\mu\text{M/ms/fA}$

## Equations

Chain of granules (see Figure b for interpretation of the subscripts to N):

$$\begin{aligned}
 dN_1/dt &= -[3k_1C_{\text{md}}(t) + r_{-1}]N_1 + k_{-1}N_2 + r_1N_5 \\
 dN_2/dt &= 3k_1C_{\text{md}}(t)N_1 - [2k_1C_{\text{md}}(t) + k_{-1}]N_2 + 2k_{-1}N_3 \\
 dN_3/dt &= 2k_1C_{\text{md}}N_2 - [k_1C_{\text{md}}(t) + 2k_{-1}]N_3 + 3k_{-1}N_4 \\
 dN_4/dt &= k_1C_{\text{md}}(t)N_3 - [3k_{-1} + u_1]N_4 \\
 dN_5/dt &= r_{-1}N_1 - [r_1 + r_{-2}]N_5 + r_2N_6 \\
 dN_6/dt &= r_3 + r_{-2}N_5 - [r_{-3} + r_2]N_6 \\
 dN_F/dt &= u_1N_4 - u_2N_F \\
 dN_R/dt &= u_2N_F - u_3N_R,
 \end{aligned}$$

Calcium dynamics:

$$\begin{aligned}
 dC_{\text{md}}(t)/dt &= f_{\text{md}}J_L(t) - f_{\text{md}}B[C_{\text{md}}(t) - C_i(t)] \\
 dC_i(t)/dt &= f_iJ_R(t) + f_vf_iB[C_{\text{md}}(t) - C_i(t)] - f_iL(C_i(t)),
 \end{aligned}$$

Ca++ inward currents:

$$\begin{aligned}
 J_L(t) &= -\alpha I_L(t)/v_{\text{md}}, \\
 J_R(t) &= -\alpha I_R(t)/v_{\text{cell}}, \\
 I_L(t) &= g_L m_{\infty}(V(t))[V(t) - V_{\text{Ca}}], \\
 I_R(t) &= 0.25g_L m_{\infty}(V(t))[V(t) - V_{\text{Ca}}],
 \end{aligned}$$

Ca++ leak currents:

$$\begin{aligned}
 L(C_i) &= J_{\text{SERCA}} + J_{\text{PMCA}} + J_{\text{NCX}} + J_{\text{leak}}, \\
 J_{\text{SERCA}} &= J_{\text{SERCA}}^{\text{max}}/[1 + (K_{\text{SERCA}}/C_i)^2], \\
 J_{\text{PMCA}} &= J_{\text{PMCA}}^{\text{max}}/[1 + K_{\text{PMCA}}/C_i], \\
 J_{\text{NCX}} &= J_{\text{NCX}}^0[C_i - 0.25], \\
 J_{\text{leak}} &= -0.94\mu\text{M}/s.
 \end{aligned}$$

Effect of Ca++ on granule dynamics:

$$\begin{aligned}
 r_2 &= r_2^0 C_i(t)/[C_i(t) + K_p] \\
 r_3 &= r_3^0 C_i(t)/[C_i(t) + K_p],
 \end{aligned}$$

### Input data

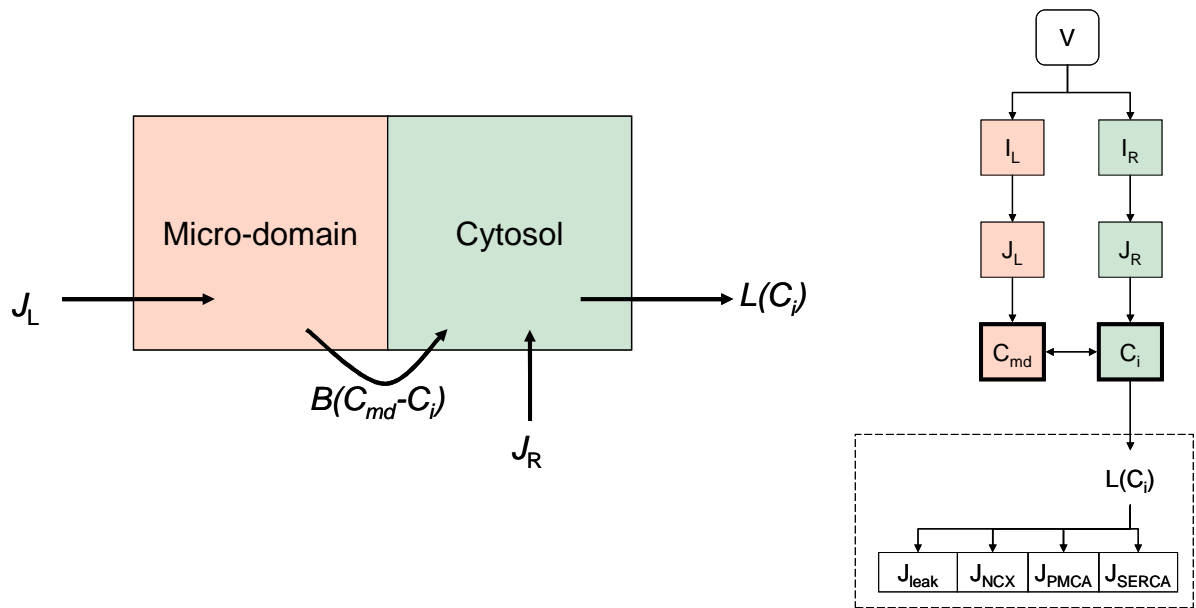
$V(t)$ : membrane depolarization. Square wave between -70 and -20 mV with 6 min down and 6 min up to reproduce Figure 4, left; steady high for Figure 4, right. Other protocols are also used.

### Predicted values

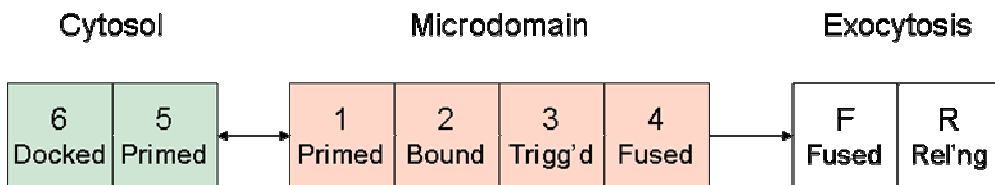
ISR: “instantaneous” insulin secretion in the last 2 min (per minute). The model predicts (and parameters were fitted to reproduce) this quantity.

### Graphical representation

The graphical representations below are adapted from Ref. 1.



**Figure a:** Calcium compartments (left) and block diagram of the effect of  $V$  on calcium concentrations  $C$  through the currents  $I$  and ion fluxes  $J$  (right). Cytosol calcium leaks through the currents shown in the dashed box.



**Figure b:** Chain of granules. One-character labels refer to the subscripts in the ODEs.

## Statistical model

This model has no stochastic components.

## Simulation/Estimation

### *Equation solver*

Used ode15s in Matlab/Simulink; other solvers may work. Where allowed by the language, discontinuities in the square-wave  $V$  input are implemented as events. Otherwise, the integration timestep becomes important.

### *Estimated parameters*

No parameters are estimated.

## Implementation remarks

Each of the implementations is a refactoring of the original XPP code (found in Ref. 2 above). Modular language constructs have been used where possible to split the model into separate calcium and vesicle components for readability.

Variables, parameters and units have been kept the same as the original code. Resupply rates  $r_1$  and  $r_2$  are affected by two different parameters, called  $K_p$  and  $K_{p2}$  in the code, with the same value; the equations use a single symbol  $K_p$ . Intervals given for variables and parameters reflect the ones used to reproduce paper's Figure 4.

## Data description

The model in the original paper fits data provided in Henquin J-C, Ishiyama N, Nenquin M, Ravier MA, Jonas J-C. Signals and Pools Underlying Biphasic Insulin Secretion. Diabetes. 2002 Feb 1;51(90001):60S–67.

## Model encoding

### *Languages*

The model has been implemented in several languages in order to benchmark the expressivity of the different approaches to modularity and language features.

### *Code*

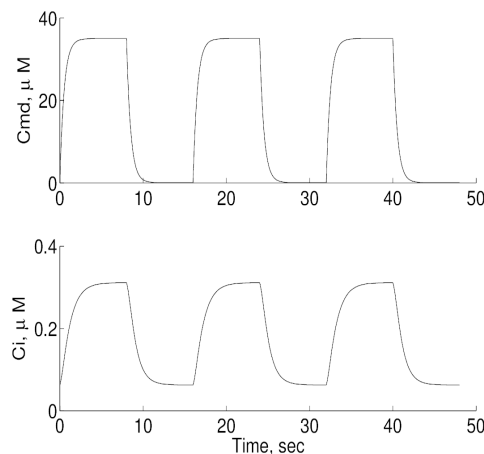
File “Readme\_Chen2008.txt” provides a technical description of the different implementations. The code for each can be found in its own directory, as follows:

- XPP (original code available at <http://lbn.niddk.nih.gov/sherman/gallery/beta/Vesicle/> )
- Matlab (tested in R2012a) and Octave (tested in 3.6.2)
- Simulink (tested in R2012a)
- Modelica (tested in OpenModelica)
- Berkeley Madonna (tested with Madonna v. 9.0.74, JEngine 1.8, JRE 1.6.0)
- Antimony, from which these are automatically generated (tested with QTAntimony 2.3 beta):
  - Flat SBML (tested in COPASI 4.8, [www.copasi.org](http://www.copasi.org), and RoadRunner/SBW Simulation Tool v1.4.4424.32048, [sbw.sourceforge.net](http://sbw.sourceforge.net)). See enclosed *NOTES.txt* file for details.
  - Modular SBML, according to the *sbml-comp* extension.

## Consistency with published results

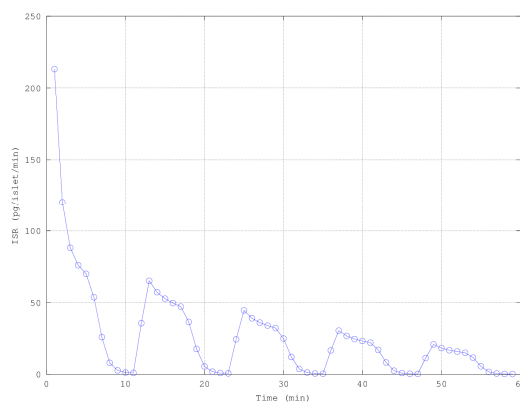
### *Reproduction of artworks*

The model correctly reproduces the simulated  $[Ca^{++}]$  in the microdomain and cytosol when a square wave of 16 sec period is applied as the membrane potential. Figure c below closely corresponds to Figure 2 of the original paper, Ref. [1]; it was obtained using the Matlab implementation with the ode15s solver.

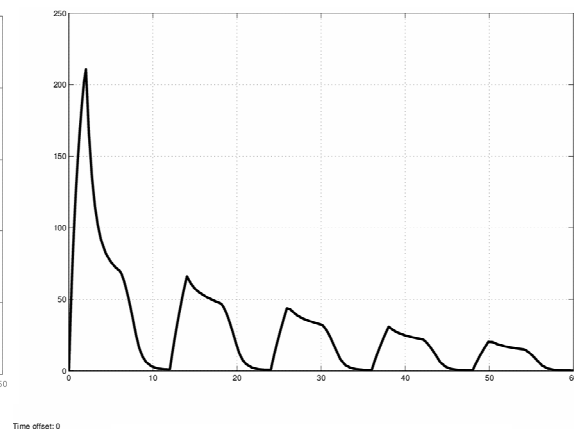


**Figure c:  $C_i$  and  $C_{md}$  as output by the Matlab implementation. Compare with Figure 2 of Ref. [1].**

The model also correctly reproduces the simulated ISR, provided as in Chen's paper (compare with open squares of Figure 4 in [1]). Outputs from Octave/Isode (Figure d1) and Simulink/ode15s solvers (Figure d2) are shown below.



**Figure d1: ISR output of the provided Octave implementation**



**Figure d2: ISR output of the provided Simulink implementation**

### *Inconsistent results*

No inconsistent results found.

### *Suggested additional outputs*

No relevant additional outputs.