

Non-equilibrium thermodynamics of a viscoelastic solid.

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Crosslinks play an important role in determining the properties of an hydrogel. Being of different nature, such as chemical or physical, they are associated with different bonding energy. The higher the binding energy the more difficult is to reorganize the polymer network, which therefore presents a elastic behaviour. The capacity of breaking and reforming crosslinks, during which energy is dissipated, result in the macroscopic viscoelastic behaviour of gels. Consequently, the relaxation time τ_R of the hydrogel to the amount of transient crosslinks. This affect also the elastic property of the network. Softer hydrogels are characterized by lower cross-links density, which makes system deformation easier. Similarly also diffusivity of molecules into the hydrogels is affected by the crosslinks density; intuitively, the larger the density of crosslinks the smaller the mesh size of the polymers and the free volume available for the transport of solvents.

While we considering in the model the changes in the water molecules from being free to being neighbouring a polymer, we miss in the model the conformational entropy of the network. This result in internal micro-stresses which are not captured in the model.

1 Non Equilibrium Thermodynamics.

While equilibrium thermodynamics successfully apply to the description of ideal process, real processes are irreversible. In this cases, the change in entropy dS can result from the reversible exchange of energy and matter with the external environment, $d_e S$ or the internal dissipation of energy

during the process, $d_i S$ [10]:

$$dS = d_e S + d_i S, \quad d_e S = \frac{dQ}{T}, \quad (1)$$

where Q is the amount of energy added to the environment and T is the temperature. According to the second law of thermodynamics, which applies universally to any system or subsystem, $dS_i \geq 0$.

For the purpose of this study, we will focus on isothermal process, i.e. $T = \text{const}$. Under this assumption, as derived by Gurtin in [5], the second law of thermodynamics is equivalent to the following *energy imbalance inequality*:

$$\frac{d}{dt} \left\{ \int_R \psi \right\} \leq W(R) + M(R) \quad (2)$$

where R is a arbitrary control volume of the system, ψ is the Helmholtz free energy, $W(R)$ is the rate at which the environment does work on R and $M(R)$ is the inflow of mass due to transport. It is important to note that the energy inequality (2) holds for any isothermal process, independently of the specific physical system involved. Consequently, there is a constraint on the form the function ψ can assume and how this can depend on the thermodynamic variables describing the system.

The major focus of non-equilibrium thermodynamics is in defining the precise form of $d_i S$, which, unlike $d_e S$ is not a state function, but depends on the specific transformation applied to the system. This is introduced in the theory with the concepts of *thermodynamic forces* F_m (cause) and *thermodynamic fluxes* J_m (effect) has been introduced, so that $d_i S$ has the form:

$$d_i S = \sum_m F_m J_m. \quad (3)$$

Different relation between forces and fluxes have been proposed in the literature giving rise to a variety of theory, each with its specific domain of applicability [10]. In our study we will focus on “Classical Irreversible Thermodynamics” (CIT) which was pioneered by Onsager [16] and Prigogine [17] in the first half of the 20th century. This is built on three major assumptions:

1. *Local Equilibrium Hypothesis*: thermodynamic variables are locally well-defined;

2. *Linear Relation between forces F and fluxes J :*

$$J_m = \sum_k L_{mk} F_k, \quad (4)$$

where the constant L_{mk} are referred to as **phenomenological coefficients**;

3. *Microscopic Reversibility*: time reversibility of processes at the micro-scale.

Despite the wide range of applicability of such theory, this does not apply to the domain of far-from equilibrium thermodynamics, for the linear approximation breaks down. It is still under debate which range of physical phenomena lie in the domain of applicability of CIT, particularly in the novel realm of active matter, where experimental validation of theories still lacks.

2 Extracellular Matrix Composition.

Despite the tissue-specific nature of Extracellular Matrix (ECM), this is mainly composed of a network of collagen fibrils entangled with charged chains of glycosaminoglycans (GAGs). While collagen is mainly responsible for the mechanical behaviour of the tissue, GAGs can imbibe water, giving ECM the ability to swell while maintaining its structural integrity. As a result, the ECM behave as a polyelectrolyte gel [18, 19]. Besides being largely present in the natural world, synthetic polyelectrolytes are currently employed for a wide range of applications, such as drug delivery, biomedical devices, scaffolds for tissue engineering and soft robotics [ADD CITATIONS]. The increasing popularity of such material has boost the development of mathematical model of such systems, in particular focusing particularly on the their swelling and plastic behaviours [ADD CITATIONS].

There is now compelling evidence that the relaxation of stress in polymer gels, and thus in ECM is governed by the interplay of the poroelastic and viscoelastic nature of the gel. While the first determines the long range motion of solvents, visco-elastic dominates the stress relaxation dynamics at the microscopic level. Being the same level at which cells probe their environment, this suggests that the visco-elastic properties of the ECM might play a role in determining cell response [ADD ARTICLE IN NOTE AS CITATION]. Given the importance of visco-elastic properties of ECM, we will focus on

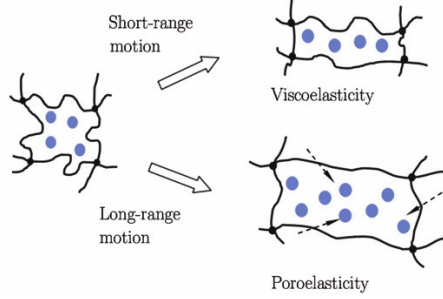


Figure 1: Illustration of the molecular processes which account for a gel deformation: viscosity is related to change in the conformation of the network which results in short-range movement of fluid relative to the polymers; poro-elasticity is instead responsible for the long-range diffusion of solvent molecules in the gel/tissue. Reproduced from [8].

how such aspect can be integrated in multiphase model of soft tissue, to better describe how this affect the macroscopic behaviour of ECM.

The theory is based on the multiplicative decomposition of the stress tensor, which have been successfully applied in the study of soft materials, such as hydrogels, rubbers and tissues [2, 4, 12, 14]. This is particularly powerful in the framework of non-equilibrium thermodynamics, which we will be using to derive our model.

We here propose two different decompositions, which will result in two different constitutive model to describe the same physical system: the extra-cellular matrix.

In the first case, following the standard Kröner decomposition [11], we decompose the deformation tensor, \mathbb{F} , into a viscous, or dissipative, component, \mathbb{F}_v , and an elastic one \mathbb{F}_e :

$$\mathbb{F} = \mathbb{F}_e \mathbb{F}_v. \quad (5)$$

As shown in Figure 2, this is equivalent to introducing a virtual configuration \mathcal{B}_v between the initial configuration \mathcal{B}_0 and the current one, \mathcal{B} . For simplicity we assume that the initial configuration corresponds to the dry stage of the hydrogel. \mathcal{B}_v is referred to as natural or relaxed configuration which correspond to the conformation the system would have if instantaneously elastically unload.

An alternative approach consists in further separating the volumetric and isochoric contribution of the deformation [3, 4, 15]. As shown in Figure 4, the first is assumed to be purely elastic, while the isochoric part of the deformation can dissipate energy due to the microscopic rearrangement of the network.

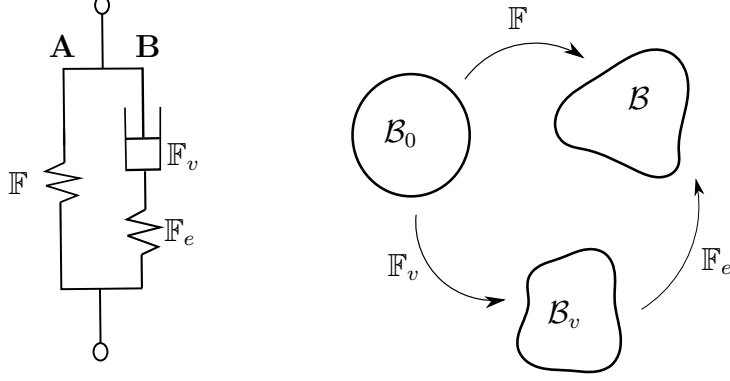


Figure 2: Rheological model 1 and corresponding deformation decomposition.

$$\mathbb{F} = \bar{\mathbb{F}}\mathbb{F}_{vol} = J^{1/3}\bar{\mathbb{F}}_e\bar{\mathbb{F}}_v, \quad (6)$$

where we have used the fact that $\mathbb{F}_{vol} = J^{1/3}\mathbb{I}$, with $J = \det \mathbb{F}$. Such decomposition introduce in the model an additional virtual configuration of the system $\bar{\mathcal{B}}$, which has the same shape as the reference configuration but different volume.

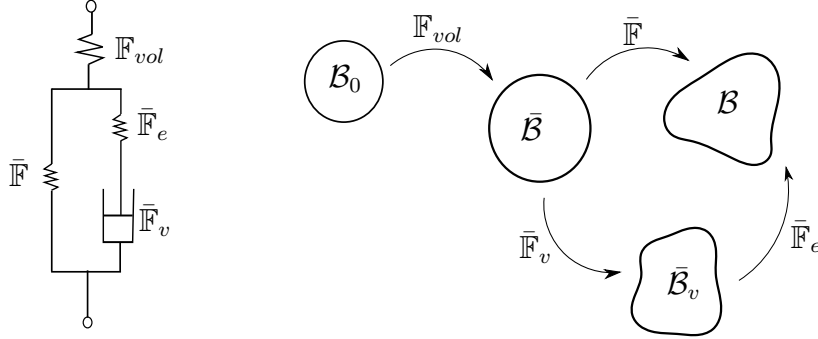


Figure 3: Rheological model 2 and corresponding deformation decomposition.

Note that both models assume that the viscous deformation \mathbb{F}_v and $\bar{\mathbb{F}}_v$ respectively preserve the volume of the body while changing its shape.

For the purpose of this study, the visco-elastic nature of collagen at the micro-scale is constitutively prescribed, supported by the result of rheological tests reported in the literature. However, there has been attempt to directly

relate this behaviour to the nano-mechanism involving single polymers chain [1]. Besides the Every configuration is characterized by a set of macro and micro variables, where the latter are responsible for changes in the atomic configuration. In the particular case considered, these are associated with the interface energy: the energy of water molecules is different when these are close to the polymer network or surrounded by other water molecules.

The system is characterised by the following primitive physical fields:

- ψ : Helmholtz free-energy,
- C : concentration of water,
- μ : chemical potential,
- \mathbb{F} : total deformation gradient,
- \mathbb{F}_e : elastic deformation gradient,
- \mathbb{F}_v : plastic deformation gradient,
- \mathbb{S} : first Piola-Kirchoff gradient,
- ξ : internal micro-stresses,
- \mathbf{j}_0 : water mass flux,
- $\mathbb{L}_v = \dot{\mathbb{F}}_v \mathbb{F}_v^{-1}$: viscous velocity gradient.

The Helmholtz free energy per unit volume of the system is given by:

$$\psi = \psi_{H_2O}(C) + \psi_{strain}(\mathbb{F}, \mathbb{F}_e) + \psi_{mix}(C) + \psi_{interface}(\mathbb{F}, \nabla_0 C). \quad (7)$$

where we assumes that the strain energy on the two branches are independent so that:

$$\psi_{strain} = \psi_A(\mathbb{F}) + \psi_B(\mathbb{F}_e). \quad (8)$$

Consequently we have that:

$$\dot{\psi}_{strain} = \frac{\partial \psi_A}{\partial \mathbb{F}} : \dot{\mathbb{F}} + \frac{\partial \psi_B}{\partial \mathbb{F}_e} : \dot{\mathbb{F}}_e \quad (9)$$

using the decomposition of the deformation tensor, we have that:

$$\dot{\mathbb{F}} = \dot{\mathbb{F}}_e \mathbb{F}_v + \mathbb{F}_e \dot{\mathbb{F}}_v \implies \dot{\mathbb{F}}_e = \dot{\mathbb{F}} \mathbb{F}_v^{-1} - \mathbb{F}_e \mathbb{L}_v, \quad (10)$$

where $\mathbb{L}_v = \dot{\mathbb{F}}_v \mathbb{F}_v^{-1}$ is the velocity gradient tensor of the dashpot element in the branch B of Figure 2. Based on this we can rewrite equation (8) as:

$$\begin{aligned}\dot{\psi}_{strain} &= \frac{\partial \psi_A}{\partial \mathbb{F}} : \dot{\mathbb{F}} + \frac{\partial \psi_B}{\partial \mathbb{F}_e} \bigg|_{\mathbb{F}_e} \mathbb{F}_v^{-T} : \dot{\mathbb{F}} - \mathbb{F}_e^T \frac{\partial \psi_B}{\partial \mathbb{F}_e} \bigg|_{\mathbb{F}_e} : \mathbb{L}_v \\ &= \frac{\partial \psi_A}{\partial \mathbb{F}} : \dot{\mathbb{F}} + \frac{\partial \psi_B}{\partial \mathbb{F}_e} \bigg|_{\mathbb{F} \mathbb{F}_v^{-1}} \mathbb{F}_v^{-T} : \dot{\mathbb{F}} - \mathbb{F}_v^{-T} \mathbb{F}^T \frac{\partial \psi_B}{\partial \mathbb{F}_e} \bigg|_{\mathbb{F} \mathbb{F}_v^{-1}} : \mathbb{L}_v.\end{aligned}\quad (11)$$

We also need to consider, the mass balance; in this case we assume that the viscous deformation is isochoric, i.e. $\det(\mathbb{F}_v) = J_v = 1$, so that, the additional condition are:

$$\begin{aligned}\dot{J} - \dot{C}v &= 0 \implies \dot{C}v - J \mathbb{F}^{-T} : \dot{\mathbb{F}}, \\ \dot{J}_v &= 0 \implies \mathbb{I} : \mathbb{L}_v = tr(\mathbb{L}_v) = 0\end{aligned}\quad (12)$$

If we now focus instead on the second rheological model, the strain energy can be further decomposed into a volumetric term and two deviatoric components, one for each branches:

$$\psi_{strain} = \psi_A(\bar{\mathbb{F}}) + \psi_B(\bar{\mathbb{F}}_e) + \psi_{vol}(J). \quad (13)$$

Consequently the full time derivative is given by:

$$\dot{\psi}_{strain} = \frac{\partial \psi_A}{\partial \bar{\mathbb{F}}} : \dot{\bar{\mathbb{F}}} + \frac{\partial \psi_B}{\partial \bar{\mathbb{F}}_e} : \dot{\bar{\mathbb{F}}}_e + \frac{\partial \psi_{vol}}{\partial J} \dot{J} \quad (14)$$

Similar to above, we exploit the decomposition of the tensor \mathbb{F} to and the definition of $\bar{\mathbb{L}}_v = \dot{\bar{\mathbb{F}}}_v \bar{\mathbb{F}}_v^{-1}$, to rewrite the above equation as:

$$\dot{\psi}_{strain} = \left(\frac{\partial \psi_A}{\partial \bar{\mathbb{F}}} + \frac{\partial \psi_B}{\partial \bar{\mathbb{F}}_e} \bigg|_{\bar{\mathbb{F}} \bar{\mathbb{F}}_v^{-1}} \bar{\mathbb{F}}_v^{-T} \right) : \dot{\bar{\mathbb{F}}} - \bar{\mathbb{F}}_v^{-T} \bar{\mathbb{F}}^T \frac{\partial \psi_B}{\partial \bar{\mathbb{F}}_e} \bigg|_{\bar{\mathbb{F}} \bar{\mathbb{F}}_v^{-1}} : \bar{\mathbb{L}}_v + \frac{\partial \psi_{vol}}{\partial J} \dot{J}. \quad (15)$$

We can now reduce the number of independent variables, by expressing $\dot{\bar{\mathbb{F}}}$ and \dot{J} in terms of the deformation tensor \mathbb{L} :

$$\dot{J} = J(\mathbb{I} : \mathbb{L}), \quad (16)$$

$$\dot{\bar{\mathbb{F}}} = J^{-1/3} \mathbb{L} \mathbb{F} - \frac{1}{3} J^{-1/3} (\mathbb{I} : \mathbb{L}) \mathbb{F} \quad (17)$$

We can thus rewrite Equation (15) as:

$$\dot{\psi}_{strain} = \left(\text{DEV} \left[J^{-1/3} \frac{\partial \psi_A}{\partial \bar{\mathbb{F}}} \bar{\mathbb{F}}^T + \frac{\partial \psi_B}{\partial \bar{\mathbb{F}}_e} \bar{\mathbb{F}}_e^T \right] + \frac{\partial \psi_{vol}}{\partial J} J \right) : \mathbb{L} - \bar{\mathbb{F}}_v^{-T} \bar{\mathbb{F}}^T \frac{\partial \psi_B}{\partial \bar{\mathbb{F}}_e} : \bar{\mathbb{L}}_v \quad (18)$$

Following the same approach as in (Sarah's article), the energy imbalance inequalities leads to:

$$\begin{aligned} & \left(\frac{\partial \psi}{\partial \nabla_0 C} - \boldsymbol{\xi} \right) \cdot \nabla_0 \dot{C} + \left(\frac{\partial \psi}{\partial C} - \mu - \nabla_0 \cdot \boldsymbol{\xi} + pv \right) \dot{C} + \nabla_0 \mu \cdot \mathbf{j}_0 \\ & + \left(\frac{\partial \psi}{\partial \mathbb{F}} \mathbb{F}^T + \frac{\partial \psi}{\partial \mathbb{F}_e} \mathbb{F}_e^T - \mathbb{S} \mathbb{F}^T - p J \mathbb{I} \right) : \mathbb{L} - \left(\mathbb{F}_v^{-T} \mathbb{F}^T \frac{\partial \psi}{\partial \mathbb{F}_e} + p_v \mathbb{I} \right) : \mathbb{L}_v \leq 0 \end{aligned} \quad (19)$$

In the second case instead, the inequalities has the following form:

$$\begin{aligned} & \left(\frac{\partial \psi}{\partial \nabla_0 C} - \boldsymbol{\xi} \right) \cdot \nabla_0 \dot{C} + \left(\frac{\partial \psi}{\partial C} - \mu - \nabla_0 \cdot \boldsymbol{\xi} + pv \right) \dot{C} + \nabla_0 \mu \cdot \mathbf{j}_0 \\ & + \left(\text{DEV} \left[J^{-1/3} \frac{\partial \psi}{\partial \bar{\mathbb{F}}} \bar{\mathbb{F}}^T + \frac{\partial \psi}{\partial \bar{\mathbb{F}}_e} \bar{\mathbb{F}}_e^T \right] - \mathbb{S} \mathbb{F}^T + J \left(\frac{\partial \psi_{vol}}{\partial J} - p \right) \mathbb{I} \right) : \mathbb{L} \\ & - \left(\bar{\mathbb{F}}_v^{-T} \bar{\mathbb{F}}^T \frac{\partial \psi}{\partial \bar{\mathbb{F}}_e} + p_v \mathbb{I} \right) : \bar{\mathbb{L}}_v \leq 0 \end{aligned} \quad (20)$$

We here consider C , $\nabla_0 C$, \mathbb{F} , \mathbb{F}_v , μ , $\nabla_0 \mu$ and \mathbf{j}_0 to be the variables defining the thermodynamic state of the system. Note that this can be split into two groups: **external** and **internal** (Which means that, in practice, these variables are measurable but not controllable, i.e., they cannot a priori be adjusted to a prescribed value through a direct action via surface or body "forces") variables. The first includes C , $\nabla_0 C$, \mathbb{F} , μ and $\nabla_0 \mu$, which are measurable and controllable quantities. In other words, this can manipulated to choose the form of their time derivative arbitrarily. Therefore, in order for (19) to be valid, we have that the terms linear in $\nabla_0 \dot{C}$, \dot{C} , \mathbb{L} of Equation (19) must be zero:

$$\xi = \frac{\partial \psi}{\partial \nabla_0 C}, \quad (21)$$

$$\mu = \frac{\partial \psi}{\partial C} - \nabla_0 \cdot \xi + pv, \quad (22)$$

$$\mathbb{S} = \begin{cases} \frac{\partial \psi}{\partial \mathbb{F}} + \frac{\partial \psi}{\partial \mathbb{F}_e} \mathbb{F}_v^{-T} - pJ\mathbb{F}^{-T} \\ \text{DEV} \left[\frac{\partial \psi}{\partial \mathbb{F}} \mathbb{F}^T + \frac{\partial \psi}{\partial \mathbb{F}_e} \mathbb{F}_e^T \right] \mathbb{F}^{-T} + \left(\frac{\partial \psi}{\partial J} - p \right) J\mathbb{F}^{-T} \end{cases} \quad (23)$$

On the other hand \mathbb{F}_v and \mathbf{j}_0 are internal variables, which describes the dissipative behaviour of the material. Since these can not be manipulated the argument used above does not apply, and (19) reduces to:

$$\mathcal{D} = \underbrace{\left(\mathbb{F}_v^{-T} \mathbb{F}^T \frac{\partial \psi}{\partial \mathbb{F}_e} + p_v \mathbb{I} \right)}_{\mathbb{M}_e^{\text{eff}}} : \mathbb{L}_v - \nabla_0 \mu \cdot \mathbf{j}_0 \geq 0, \quad (24)$$

where \mathcal{D} represents the energy dissipated in the system per unit volume of the natural configuration \mathcal{B}_v , $\mathbb{M}_e^{\text{eff}}$ is the effective Mandel stress in the natural configuration. The first term is associated with the viscous response of the dashpot in branch B; physically this is associated with the energy dissipated in the breaking and forming of crosslinks in the network, which increase the conformational entropy of the system. On the other hand, the second term is related to the relative diffusion of the water molecules, hence the dependency on $\nabla_0 \mu$.

As shown in [6], the most general form for \mathbb{L}_v and \mathbf{j}_0 would be:

$$\mathbb{L}_v = A(\mathbf{\Lambda}_0, \nabla_0 \mu, \mathbb{M}_e^{\text{eff}}) \mathbb{M}_e^{\text{eff}} + B(\mathbf{\Lambda}_0, \nabla_0 \mu, \mathbb{M}_e^{\text{eff}}) \nabla_0 \mu, \quad (25)$$

$$\mathbf{j}_0 = -K(\mathbf{\Lambda}_0, \nabla_0 \mu, \mathbb{M}_e^{\text{eff}}) \mathbb{M}_e^{\text{eff}} - D(\mathbf{\Lambda}_0, \nabla_0 \mu, \mathbb{M}_e^{\text{eff}}) \nabla_0 \mu, \quad (26)$$

where $\mathbf{\Lambda}_0 = \{\mathbb{F}, \mathbb{F}_v, C, \nabla_0 C, \mu\}$, A is a forth order, B and K third order, D a second order tensors. Assuming to be in a linear non-equilibrium regime, we have that all coefficients are independent of $\nabla_0 \mu$ and $\mathbb{M}_e^{\text{eff}}$. Having also considered isotropic materials, *Curie's law* implies that $K \equiv 0$ and $\mathbb{B} \equiv 0$, so that \mathcal{D} reduces to:

$$\mathcal{D} = A(\mathbf{\Lambda}_0)\mathbb{M}_e^{\text{eff}} : \mathbb{M}_e^{\text{eff}} + D(\mathbf{\Lambda}_0)\nabla_0\mu \cdot \nabla_0\mu \geq 0.$$

Based on Onsager reciprocal relation, which assumes microscale reversibility, the parameter $D(\mathbf{\Lambda}_0)$, the diffusion coefficient, is positive and the tensor A must be symmetric and positive semi-definite. In our example we consider it to be $A = \eta^{-1}(\mathbf{\Lambda}_0)\mathbb{I}$, where \mathbb{I} is the identity tensor and η is the viscosity. Consequently the dynamical equation for the system are:

$$\eta(\mathbf{\Lambda}_0)\mathbb{L}_v = \left(\mathbb{F}_v^{-T}\mathbb{F}^T \frac{\partial\psi}{\partial\mathbb{F}_e} + p_v\mathbb{I} \right) \quad (27)$$

$$\mathbf{j}_0 = -D(\mathbf{\Lambda}_0)\nabla_0\mu \quad (28)$$

where the diffusion coefficient $D(\mathbf{\Lambda}_0)$ is defined as:

$$D_0 = \frac{DC}{k_B T} \mathbb{F}^{-1}\mathbb{F}^{-T} \quad (29)$$

with D being the diffusion coefficient in the current configuration \mathcal{B} . To complete the model we need to specify the form of the free energy. For what concerns the strain energy, we assume both springs to behave as a neo-Hookean material, so that:

$$\begin{aligned} \psi_A(\mathbb{F}) &= \frac{G_A}{2} [(I_{\mathbb{B}} - 3) - \ln III_{\mathbb{B}}], \\ \psi_B(\mathbb{F}_e) &= \frac{G_B}{2} [(I_{\mathbb{B}_e} - 3) - \ln III_{\mathbb{B}_e}], \end{aligned} \quad (30)$$

where $\mathbb{B} = \mathbb{F}\mathbb{F}^T$, $\mathbb{B}_e = \mathbb{F}_e\mathbb{F}_e^T$ and I and III are their first and third invariants.

Consequently, we have that:

$$\begin{aligned} \frac{\partial\psi}{\partial\mathbb{F}_e} &= \frac{\partial\psi_B}{\partial\mathbb{F}_e} = G_B(\mathbb{F}_e - \mathbb{F}_e^{-T}) \\ \implies \eta(\mathbf{\Lambda}_0)\mathbb{L}_v &= G_B [(\mathbb{C}_e - \mathbb{I}) + \tilde{p}_v\mathbb{I}] \\ \implies \mathbb{L}_v &= \frac{[\mathbb{C}_e + (\tilde{p}_v - 1)\mathbb{I}]}{2\tau_R(\mathbf{\Lambda}_0)} \end{aligned} \quad (31)$$

where $\mathbb{C}_e = \mathbb{F}_e^T\mathbb{F}_e$, $\tilde{p}_v = p_v/G_B$ and τ_R is the relaxation time of the system.

Note that based on Equation (31), \mathbb{L}_v is a symmetric tensor. Consequently:

$$\begin{aligned}\mathbb{L}_v &= \underbrace{d_v}_{\text{stretching viscous tensor}} + \underbrace{W_v}_{\text{spin viscous tensor}} \\ d_v &= \frac{1}{2}(\mathbb{L}_v + \mathbb{L}_v^T) = L_v \quad W_v = \frac{1}{2}(\mathbb{L}_v - \mathbb{L}_v^T) = \mathbb{O}\end{aligned}\tag{32}$$

Given the condition on J_v , we have that:

$$(-\tilde{p}_v + 1) = \frac{1}{3}\text{tr}(\mathbb{C}_e) = \frac{1}{3}\text{tr}(\mathbb{B}_e)\tag{33}$$

where $\mathbb{B}_e = \mathbb{F}_e \mathbb{F}_e^T$; if we consider its time derivative we have that:

$$\begin{aligned}\dot{\mathbb{B}}_e &= \mathbb{L}\mathbb{B}_e + \mathbb{B}_e\mathbb{L}^T - 2\mathbb{F}_e d_v \mathbb{F}_e^T \\ &= \mathbb{L}\mathbb{B}_e + \mathbb{B}_e\mathbb{L}^T - \frac{1}{\tau_R(\mathbf{\Lambda}_0)}\mathbb{F}_e \left[\mathbb{C}_e - \frac{1}{3}\text{tr}(\mathbb{B}_e)\mathbb{I} \right] \mathbb{F}_e^T \\ &= \mathbb{L}\mathbb{B}_e + \mathbb{B}_e\mathbb{L}^T - \underbrace{\frac{1}{\tau_R(\mathbf{\Lambda}_0)}\mathbb{B}_e \left[\mathbb{B}_e - \frac{1}{3}\text{tr}(\mathbb{B}_e)\mathbb{I} \right]}_{\text{DEV}[\mathbb{B}_e]}.\end{aligned}\tag{34}$$

In the second case the argument holds as before, with a different definition of the viscous dissipation:

$$\bar{\mathbb{L}}_v = \bar{\mathbb{F}}_e^T \frac{\partial \psi_B}{\partial \bar{\mathbb{F}}_e} + p_v \mathbb{I}\tag{35}$$

where ψ_B is now defined as:

$$\psi_B = \frac{G_B}{2}(I_{\bar{\mathbb{B}}_e} - 3).\tag{36}$$

Consequently we obtain that:

$$\bar{\mathbb{L}}_v = \frac{\text{DEV}[\bar{\mathbb{C}}_e]}{2\tau_R(\mathbf{\Lambda}_0)}\tag{37}$$

Using the fact that the viscous deformation has zero spin, we can derive the following ODE for $\bar{\mathbb{B}}_e$:

$$\dot{\bar{\mathbb{B}}}_e = \bar{\mathbb{B}}_e\mathbb{L}^T + \mathbb{L}\bar{\mathbb{B}}_e - \frac{2}{3}\text{tr}(\mathbb{L})\bar{\mathbb{B}}_e - \frac{1}{\tau_R}\bar{\mathbb{B}}_e\text{DEV}[\bar{\mathbb{B}}_e]\tag{38}$$

Finally, the second approach requires to specify the strain energy related to the volumetric deformation. As discussed in [14], different formulation can be used to capture the real behaviour of the system. To be consistent with the previous model we will again use a logarithmic strain energy:

$$\psi_{vol}(J) = \frac{\kappa}{2} \ln J^2, \quad (39)$$

where κ is the bulk modulus of the system. Note that the above formulation present several limitation in the description of large deformation [14]. Despite this, it remains one of the most common form used and just recently researchers has been focusing on developing more accurate and consistent model. Given that, and the other terms in the energy, we obtain:

$$\mu = \mu_0 + pv - \gamma J \nabla^2 C + kT \left[\ln \frac{Cv}{1+Cv} + \frac{1}{1+Cv} + \frac{\chi}{(1+Cv)^2} \right], \quad (40)$$

$$\mathbb{T} = \begin{cases} -p\mathbb{I} + \mathbb{T}_A + \mathbb{T}_B + \gamma \left[\frac{1}{2} |\nabla C|^2 \mathbb{I} - \nabla C \otimes \nabla C \right], \\ \left(\frac{\kappa}{1+Cv} - p \right) \mathbb{I} + \mathbb{T}_A + \mathbb{T}_B + \gamma \left[\frac{1}{2} |\nabla C|^2 \mathbb{I} - \nabla C \otimes \nabla C \right], \end{cases} \quad (41)$$

$$\mathbb{T}_A = \begin{cases} \frac{G_1}{1+Cv} (\mathbb{B} - \mathbb{I}), \\ \frac{G_1}{1+Cv} \bar{\mathbb{B}}^D, \end{cases} \quad \mathbb{T}_B = \begin{cases} \frac{G_2}{1+Cv} (\mathbb{B}_e - \mathbb{I}), \\ \frac{G_2}{1+Cv} \bar{\mathbb{B}}_e^D \end{cases} \quad (42)$$

where the Cauchy stress is given by $\mathbb{T} = J^{-1} \mathbb{S} \mathbb{F}^T$, and the apices D is a shortening for the deviatoric part of the tensor.

3 Spinodal Decomposition

The governing equation of the system are:

$$J = \det F = 1 + Cv, \quad (43)$$

$$\dot{C} = -\nabla_0 \cdot \mathbf{j}_0 = 0, \quad (44)$$

$$\mathbf{j}_0 = JF^{-1}\mathbf{j}, \quad (45)$$

$$\mathbf{j} = -\frac{k_B T}{\zeta_0 v} (1 + Cv)^{\beta-1} \left[\frac{1 + (1 - 2\chi)Cv}{(1 + Cv)^3} \nabla C + \frac{Cv}{k_B T} \nabla p - \frac{\gamma C}{k_B T} \nabla [(1 + Cv) \nabla^2 C] \right], \quad (46)$$

$$\nabla \cdot \mathbb{T} = \mathbf{0}, \quad (47)$$

$$\mathbb{T} = -p\mathbb{I} + \mathbb{T}_A + \mathbb{T}_B + \gamma \left[\frac{1}{2} |\nabla C|^2 \mathbb{I} - \nabla C \otimes \nabla C \right], \quad (48)$$

$$\mathbb{T}_A = \frac{G_1}{1 + Cv} (\mathbb{B} - \mathbb{I}), \quad (49)$$

$$\mathbb{T}_B = \frac{G_2}{1 + Cv} (\mathbb{B}_e - \mathbb{I}), \quad (50)$$

$$\dot{\mathbb{B}}_e = L\mathbb{B}_e + \mathbb{B}_e L^T - \frac{2}{\tau_R(\mathbf{T})} \mathbb{B}_e \text{DEV}[\mathbb{B}_E]. \quad (51)$$

with the initial condition $\mathbb{B}_e(\mathbf{X}, 0) = \mathbb{B}(\mathbf{X}, 0)$. We can now non-dimensionalise the model, using the characteristic length scale L_0 , the characteristic time τ_0 to rescale the space and time variable respectively. Stresses and pressure are scaled by G_1 while the fluxes by \mathfrak{J} , the concentration by v^{-1} and the chemical

potential by $k_B T$. Consequently the set of equation turns to:

$$J = \det F = 1 + C, \quad (52)$$

$$\dot{C} = -\frac{\tau_0 \mathfrak{J} v}{L_0} \nabla_0 \cdot \mathbf{j}_0 = 0, \quad (53)$$

$$\mathbf{j}_0 = J F^{-1} \mathbf{j}, \quad (54)$$

$$\mathbf{j} = -\frac{k_B T}{\mathfrak{J} \zeta_0 v^2 L_0} (1 + C)^{\beta-1} \left[\frac{1 + (1 - 2\chi)C}{(1 + C)^3} \nabla C + \frac{C v G_1}{k_B T} \nabla p \right. \\ \left. - \frac{\gamma C}{v k_B T L_0^2} \nabla [(1 + C) \nabla^2 C] \right], \quad (55)$$

$$\nabla \cdot \mathbb{T} = \mathbf{0}, \quad (56)$$

$$\mathbb{T} = J^{-1} S F^T = -p \mathbb{I} + \frac{\mathbb{B} - \mathbb{I}}{1 + C} + \frac{G_2 (\mathbb{B}_e - \mathbb{I})}{G_1 (1 + C)} \\ + \frac{\gamma}{v^2 L_0^2 G_1} \left[\frac{1}{2} |\nabla C|^2 \mathbb{I} - \nabla C \otimes \nabla C \right], \quad (57)$$

$$\dot{\mathbb{B}}_e = L \mathbb{B}_e + \mathbb{B}_e L^T - \frac{2 \tau_0}{\tau_R(\mathbf{\Gamma})} \mathbb{B}_e \text{DEV}[\mathbb{B}_E]. \quad (58)$$

We now define $\mathfrak{J} = L_0 / (\tau_0 v)$ and $\tau_0 = \tau_D = (\zeta_0 v L_0^2) / (k_B T)$ where τ_D is the characteristic time scale of diffusion. We also define the following non-dimensional parameters:

$$\tau^* = \frac{\tau_D}{\tau_R}, \quad g_1 = \frac{G_1 v}{k_B T}, \quad g_2 = \frac{G_2 v}{k_B T}, \quad \omega = \frac{\gamma}{v k_B T L_0^2}, \quad (59)$$

where ω is a measure of the dimensionless interface energy, while g_1 and g_2 are referred to as effective elastic constant of branch A and B respectively.

We also consider the form of the chemical potential which in non-dimensional form is given by $\mu^* = -\mu_0 + \mu / (k_B T)$. By dropping the star, we have that:

$$\mu = p g_1 - \omega J \nabla^2 C + \underbrace{\left[\ln \frac{C}{1 + C} + \frac{1}{1 + C} + \frac{\chi}{(1 + C)^2} \right]}_{\Pi} \quad (60)$$

where Π is the adimensional form of the osmotic pressure. We thus obtain the following non-dimensional system:

$$J = \det F = 1 + C, \quad (61)$$

$$\dot{C} = -\nabla_0 \cdot \mathbf{j}_0 = 0, \quad (62)$$

$$\mathbf{j}_0 = JF^{-1}\mathbf{j}, \quad (63)$$

$$\mathbf{j} = -(1+C)^{\beta-1} \left[\frac{1+(1-2\chi)C}{(1+C)^3} \nabla C + g_1 C \nabla p - \omega C \nabla [(1+C) \nabla^2 C] \right], \quad (64)$$

$$\nabla \cdot \mathbb{T} = \mathbf{0}, \quad (65)$$

$$\mathbb{T} = -p\mathbb{I} + \frac{\mathbb{B} - \mathbb{I}}{1+C} + \frac{g_2}{g_1} \frac{\mathbb{B}_e - \mathbb{I}}{1+C} + \frac{\omega}{g_1} \left[\frac{1}{2} |\nabla C|^2 \mathbb{I} - \nabla C \otimes \nabla C \right], \quad (66)$$

$$\dot{\mathbb{B}}_e = L\mathbb{B}_e + \mathbb{B}_e L^T - 2\tau^* \mathbb{B}_e \text{DEV}[\mathbb{B}_E]. \quad (67)$$

Combining Equation (65)-(66), we can obtain an expression for ∇p :

$$\nabla p = \nabla \cdot \left(\frac{\mathbb{B} - \mathbb{I}}{1+C} \right) + \frac{g_2}{g_1} \nabla \cdot \left(\frac{\mathbb{B}_e - \mathbb{I}}{1+C} \right) + \frac{\omega}{g_1} \nabla \cdot \left(\frac{1}{2} |\nabla C|^2 \mathbb{I} - \nabla C \otimes \nabla C \right)$$

which can be substitute into Equation (64) to obtain:

$$\begin{aligned} \mathbf{j} = & -(1+C)^{(\beta-1)} \left[\frac{1+(1-2\chi)C}{(1+C)^3} \nabla C + g_1 C \nabla \cdot \left(\frac{\mathbb{B} - \mathbb{I}}{1+C} \right) \right. \\ & + g_2 C \nabla \cdot \left(\frac{\mathbb{B}_e - \mathbb{I}}{1+C} \right) - \omega C \nabla [(1+C) \nabla^2 C] \\ & \left. + \omega C \nabla \cdot \left(\frac{1}{2} |\nabla C|^2 \mathbb{I} - \nabla C \otimes \nabla C \right) \right]. \end{aligned} \quad (68)$$

4 Uniaxial swelling

In this section, we consider the case in which the gel undergoes a uni-axial constraint deformation:

$$\mathbb{F} = \begin{bmatrix} 1 & 0 & 0 \\ 0 & 1 & 0 \\ 0 & 0 & J(Z, t) \end{bmatrix} \quad (69)$$

so that $\mathbb{B} = \text{diag}(1, 1, J^2)$, $C = C(z, t)$. Since $\mathbb{B}_e(Z, 0) = \mathbb{B}(Z, 0)$ is a diagonal matrix, the off-diagonal term of the matrix B_e remain equal to zero. The symmetry of the problem with respect to x and y guarantees that $\mathbb{B}_{e;11} = \mathbb{B}_{e;22} = \mathbb{B}_{e,x}(Z, t)$ for any $t > 0$. We here consider the case of a forced swelling, i.e. we impose the flux at the boundary $Z = 1$. Consequently, the system governing equation in the reference configuration reduce to:

$$\partial_t C = -\partial_Z j_0, \quad (70)$$

$$\partial_t B_{e,x} = -\frac{2\tau^*}{3} B_{e,x} (B_{e,x} - B_{e,z}), \quad (71)$$

$$\partial_t B_{e,z} = -2\frac{B_{e,z}}{1+C}\partial_Z j_0 - \frac{4\tau^*}{3} B_{e,z} (B_{e,z} - B_{e,x}), \quad (72)$$

$$B_{e,x}(Z, 0) \equiv 1, \quad B_{e,z}(Z, 0) \equiv J^2(Z, 0) \quad \forall Z \in [0, 1], \quad (73)$$

$$j_0 = -(1+C)^{\beta-2} \left[\frac{1+(1-2\chi)C}{(1+C)^3} \partial_Z C + g_1 C \partial_Z \left(\frac{2C+C^2}{1+C} \right) + g_2 C \partial_Z \left(\frac{B_{e,z}-1}{1+C} \right) - \omega C \partial_Z R \right] \quad (74)$$

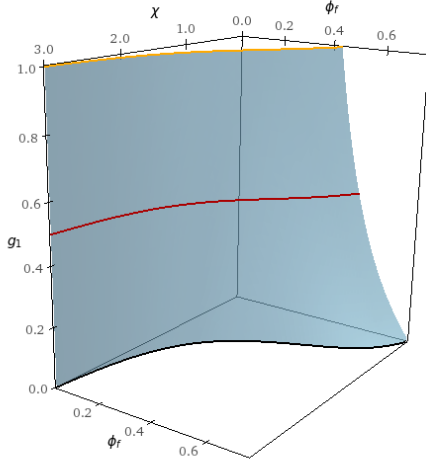
$$\partial_Z C = 0 \quad \text{at } Z \in \{0, 1\}, \quad j_0 = 0 \quad \text{at } Z = 0, \quad \forall t > 0, \quad (75)$$

$$R \equiv -\frac{1}{2} \frac{(\partial_Z C)^2}{(1+C)^2} + \frac{\partial_{ZZ} C}{1+C} \quad (76)$$

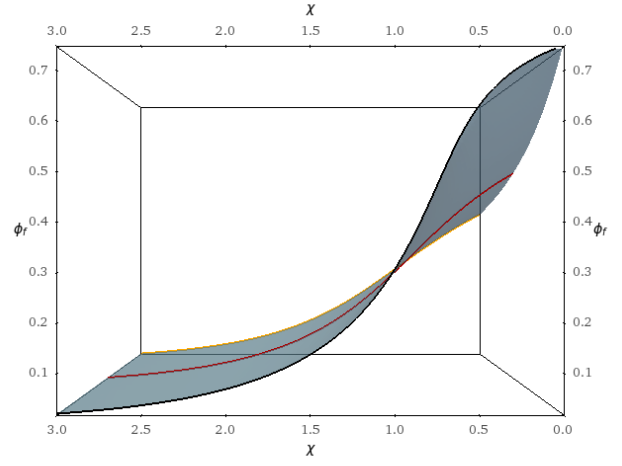
In order to have a well-defined solution to the problem, we need to introduce an additional condition at the boundary $Z = 1$. Depending on whether we want to study the free or forced swelling of the gel, we will impose respectively:

$$\mu = 0, \quad (77)$$

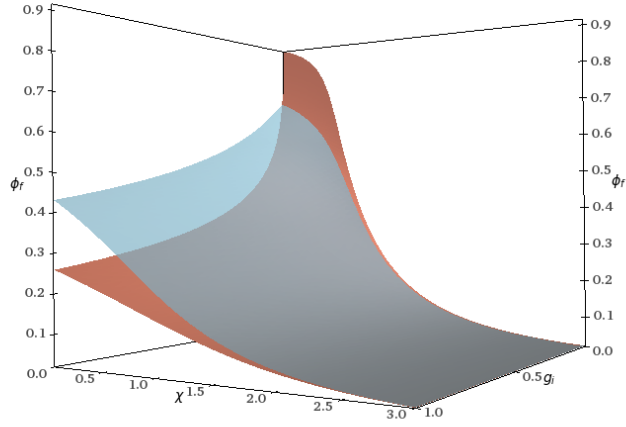
$$j_0 = -Q, \quad (78)$$



(a)



(b)



(c)

Figure 4: (a)-(b) Two different view of the manifold defined by $F(C; \chi, g_2) = 0$, for $g_1 = 0.01$. Lines represent the intersection of the manifold with the planes $g_2 = 0$ (black), $g_2 = 0.5$ (red) and $g_2 = 1$ (orange). For any given value of χ , $\phi_f^{eq}(g_2)$ is a decreasing function of g_2 . (c) Comparison between the manifold $F(C; \chi, g_2)$ (blue as above) and $F(C; \chi, g_1)$ (red) for $g_2 = 0.01$. We note that generally $\phi_f^{eq}(g_2) > \phi_f^{eq}(g_1)$ except for $g_1 \sim g_2 \rightarrow 0$.

where Q is the non dimensional flux imposed at the boundary.

The first case of free-swelling, as been largely study in the literature. After an initial phase of expansion, the gel equilibrates with the bath, i.e. $\mu = 0$ at any point. Given that $\mathbb{T} = 0$ on the boundary, we have that:

$$p = \frac{(1+C)^2 - 1}{1+C} + \frac{g_2}{g_1} \frac{B_{e,z} - 1}{1+C} - \frac{\omega}{g_1} \frac{(\partial_Z C)^2}{(1+C)^2} \quad (79)$$

$$\mu = (g_1 p + \Pi) - \omega \partial_Z \left[\frac{\partial_Z C}{1+C} \right]. \quad (80)$$

The homogeneous equilibrium, i.e. $\partial_Z C \equiv 0$ and $\partial_t B_{e,z} \equiv 0$, is thus implicitly defined by the equation $F(C_{eq})$, where we define F as:

$$F(C) = g_1 \frac{2C + C^2}{1+C} + g_2 \frac{(1+C)^{\frac{2}{3}} - 1}{1+C} + \ln \left(\frac{C}{1+C} \right) + \frac{1+C+\chi}{(1+C)^2} \quad (81)$$

4.1 Linear Stability Analysis: Normal Mode Analysis

Let us consider the equilibrium condition, with the initial constant state $C = C_0$, then we have that:

$$B_{e,x}^{eq} = B_{e,z}^{eq} = B_0 = (1+C_0)^{2/3}. \quad (82)$$

If now expand the solution around the equilibrium state, we obtain:

$$\begin{aligned} C(Z, t) &= C_0 + \delta C_1 \exp(\lambda t + iKZ), \\ B_{e,x}(Z, t) &= B_0 + B_1^x \delta C_1 \exp(\lambda t + iKZ), \\ B_{e,z}(Z, t) &= B_0 + B_1^z \delta C_1 \exp(\lambda t + iKZ). \end{aligned} \quad (83)$$

which yield to the following implicit definition of the growth rate:

$$\begin{aligned} \lambda^2 + \lambda \left(2\tau^* B_0 + (1+C_0)^{\beta-2} \mathcal{V} \right) + (1+C_0)^{\beta-2} 2\tau^* B_0 \left(\mathcal{V} - \frac{4g_2 K^2}{3} \frac{C_0 B_0}{(1+C_0)^2} \right) &= 0, \\ \mathcal{V} &= \mathcal{S} K^2 + \frac{g_2 C_0 (B_0 + 1) K^2}{(1+C_0)^2} + \omega K^4 \frac{C_0}{1+C_0}, \\ \mathcal{S} &= \frac{1 + (1-2\chi)C_0}{(1+C_0)^3} + g_1 \frac{C_0 [(1+C_0)^2 + 1]}{(1+C_0)^2}. \end{aligned}$$

In order for the homogeneous solution to be stable, both the solution of the parabolic equation in λ must be negative. Since $\tau^* > 0$, then the modes are stable when the following two conditions are satisfied:

$$2\tau^* B_0 + (1 + C_0)^{\beta-2} \mathcal{V} > 0, \quad (84)$$

$$\mathcal{V} - \frac{4g_2 K^2}{3} \frac{C_0 B_0}{(1 + C_0)^2} > 0. \quad (85)$$

Since condition (85) implies condition (84), the homogeneous solution is unstable whenever (85) is not satisfied for at least one wavenumber K . In other words phase separation occurs whenever the following condition holds:

$$\exists K \text{ s.t. } \underbrace{\left(\mathcal{S} + g_2 C_0 \frac{1 - \frac{1}{3}(1 + C_0)^{2/3}}{(1 + C_0)^2} \right)}_{\tilde{\mathcal{S}}} K^2 + \omega \frac{C_0}{1 + C_0} K^4 < 0 \quad (86)$$

which is equivalent to imposing that $\tilde{\mathcal{S}} < 0$.

While the parameter τ^* does not affect the stability of the system, this determines the dynamics of the system.

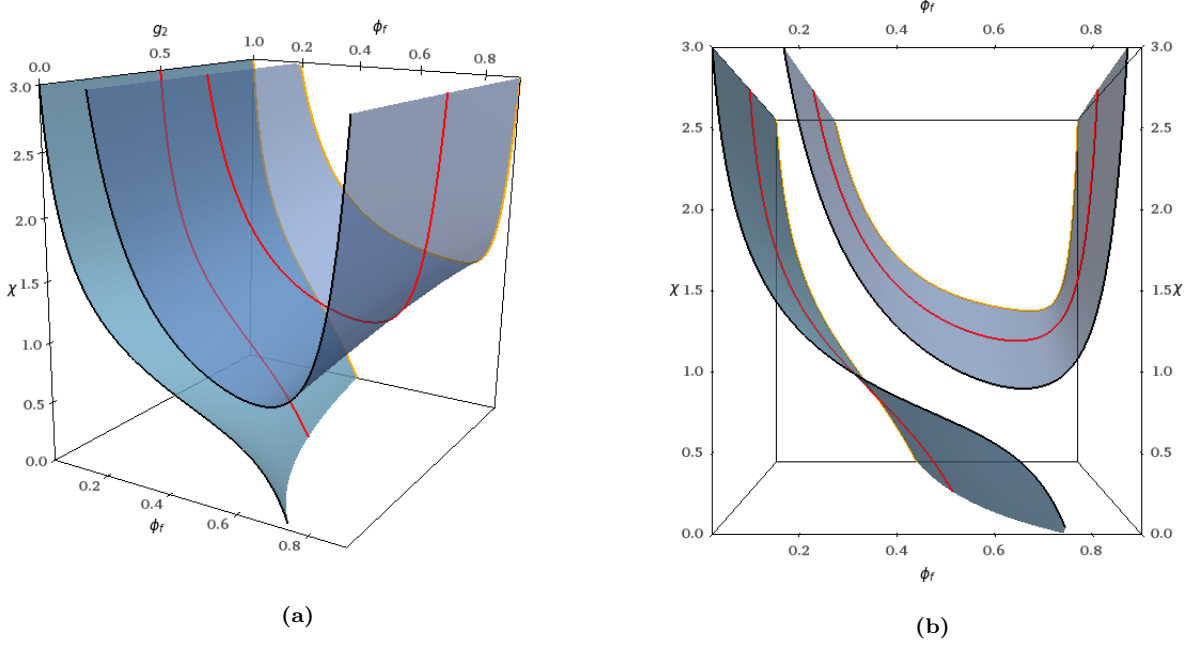


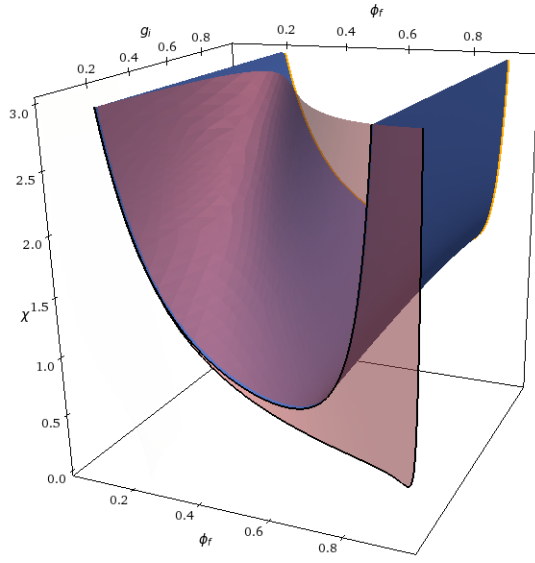
Figure 5: Comparison between the manifold defined by $F = 0$ (as in Figure 4, light blue) and $S(g_2, \chi, C) = 0$ (blue), where we have fixed $g_1 = 0$. As before the lines represent the intersection of the manifolds with the plane $g_2 = 0$ (black), $g_2 = 0.5$ (red) and $g_2 = 1$ (orange). The blue manifold delimits the region of instability (above the surface), which shrinks as the value of g_2 increase. This means that the larger g_2 the more unlikely is for the phase separation to occur.

5 Numerical Solution

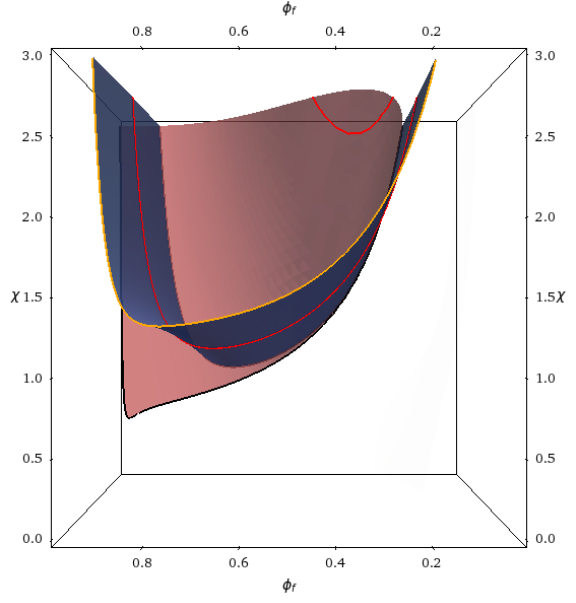
The system is solved numerically a staggered grid: while j_0 is computed on the edge of each cell, C , B_e and R are evaluated at the centre. The resulting system of ODEs is solved using a semi-implicit method, which reduces the cost of each iteration to the solution of a linear system. The Neumann condition is consider introducing ghosts point.

5.1 Dependency on τ^* .

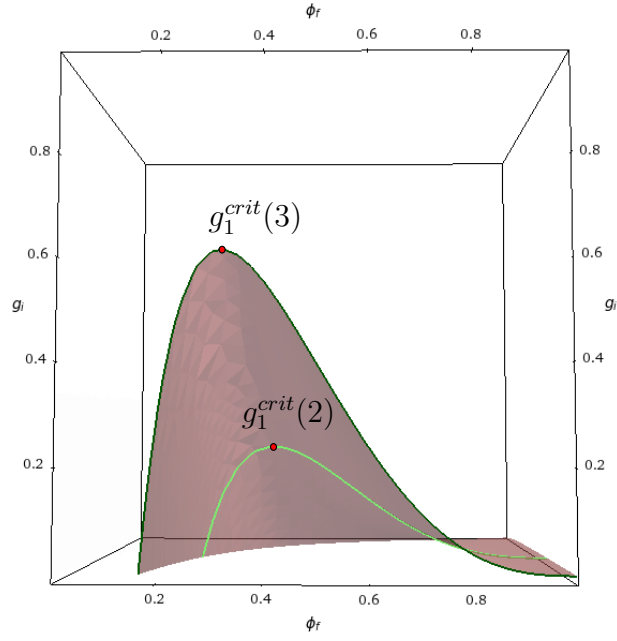
We first analyse how the phase separation process is affected by the parameter, τ^* , which represent the dimensionless time response of the system. As shown by the linear stability analysis in Section 4.1, this parameter does not affect the stability of the homogeneous solution, and thus the presence of phase separation. However, numerical simulation highlights its role in



(a)



(b)



(c)

Figure 6: Manifold implicitly defined by the equation $\tilde{S}(g_i, C, \chi) = 0$, where $i = 2$ and $g_1 = 0.01$ (blue surface), $i = 1$ and $g_2 = 0.01$ (red surface). The lines highlight the intersection of the manifolds with the plane $g_i = 0$ (black), $g_i = 0.5$ (red) and $g_i = 1$ (orange). Note that there is a critical value of $g_1^{crit}(\chi)$ beyond which there is $\tilde{S}(g_1, C, \chi) = 0$ has no solution, as illustrated in (c).

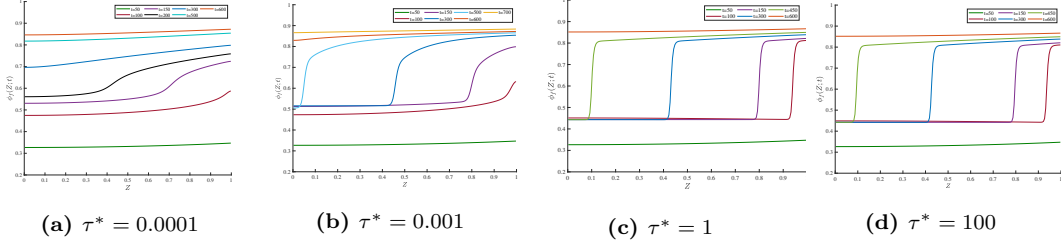


Figure 7: Numerical simulation of the full model showing the effect of the parameter τ^* on the onset, propagation and shape of the interface separating the solvent-rich and solvent-poor regions.

determining the dynamic response of the system.

As shown in Figure 7, the onset of the phase-separation is delayed and the interface between the solvent rich and solvent poor region is smoother. In order to investigate what happens, we study Equation (71)-(72) in the case of $\tau^* \ll 1$. By expanding $B_{e,x}$ and $B_{e,z}$ in terms of the small parameter τ^* , we obtain that:

$$\begin{aligned} B_{e,z} &= (1+C)^2 \left(1 - \frac{4}{3}\tau^* \int_0^t (2C + C^2) ds \right) + O((\tau^*)^2), \\ B_{e,x} &= 1 + \frac{2}{3}\tau^* \int_0^t (2C + C^2) ds + O((\tau^*)^2). \end{aligned} \quad (87)$$

In this regime the first order approximation of the flux is given by:

$$\begin{aligned} j_0 &= -(1+C)^{\beta-2} \left\{ \left[\frac{1 + (1-2\chi)C}{(1+C)^3} \right] \partial_Z C + \underbrace{(g_1 + g_2)}_{g_{eq}} C \partial_Z \frac{2C + C^2}{1+C} \right. \\ &\quad \left. - \frac{4\tau^*}{3} g_2 C \partial_Z \left[(1+C) \int_0^t 2C + C^2 ds \right] - \omega C \partial_Z R \right\} \end{aligned}$$

which is equivalent to the behaviour of a simply elastic material characterised by the parameters g_{eq} plus a perturbation in τ^* . In the case of $\tau^* = 0$, the onset of phase separation is determined by the value of g_{eq} . As previously analysed in the literature, for the set of parameter used, phase separation occurs if $g < g_{crit} = 0.019$. In the example presented in Figure 7, $g_{eq} = 0.02 > g_{crit}$. Consequently, as long as the term linear in τ is negligible, the formation of a miscibility gap can be delayed at the point that this never occur as in Figure 7(a).

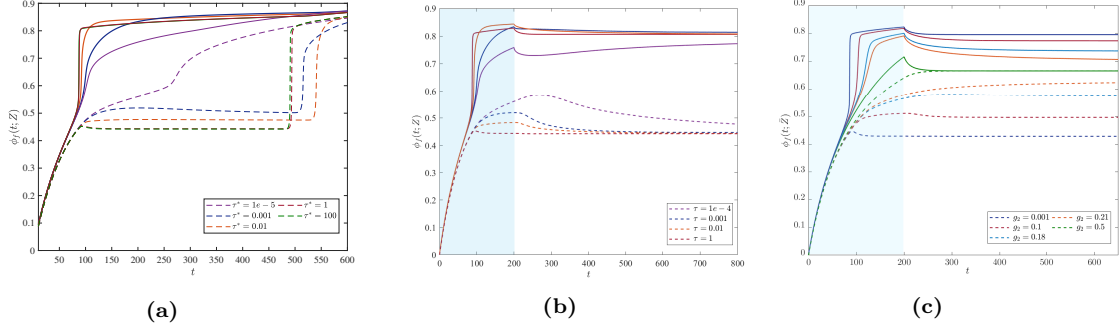


Figure 8: Evolution of the (a) solvent volume fraction at the substrate, $Z = 0$ (dotted line), and the surface $Z = 1$ (full line) and (b) the position of the interfacial $Z = \bar{S}(t)$, which is implicitly defined by $\phi_f(\bar{S}, t) = 0.6$. The other parameters values are $g_1 = g_2 = 0.01$, $\chi = 1$, $\omega = 10^{-6}$, $\beta = 1$ and $Q = 0.01$.

We also consider the case in which the flux Q is non-zero only for a finite amount of time. Under this condition, the phase separation starts later, once the unstable modes drive the system towards a non-homogeneous but stationary solution.

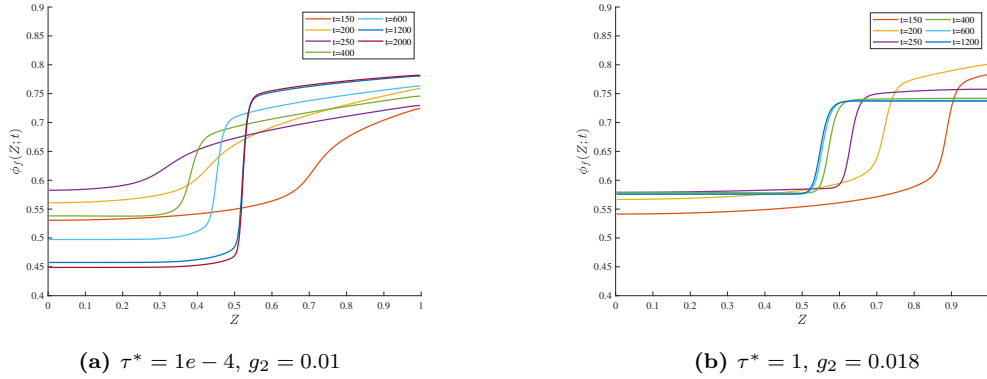


Figure 9: Solution of the full system with $Q = Q_0 H(t - 200)$, where H is the Heaviside function; other parameters in the model are $g_1 = 0.01$, $\chi = 1$.

In the case instead of fast relaxation times, the stress \mathbb{B}_e , quickly reach its steady state, i.e. $\mathbb{B}_e = (1 + C)^{2/3} \mathbb{I}$. Under this consideration the flux can be written as:

$$j_0 = -(1 + C)^{\beta-2} \left\{ \left[\frac{1 + (1 - 2\chi)C}{(1 + C)^3} \right] \partial_Z C - \omega C \partial_Z R \right. \\ \left. + C \partial_Z \left[\frac{2C + C^2}{1 + C} \left(g_1 + \frac{g_2}{1 + (1 + C)^{4/3} + (1 + C)^{2/3}} \right) \right] \right\}$$

When C is small the two constant g_1 and g_2 contribute equally, but as C increases g_1 becomes dominant. However, as shown in Figure 8(c), the magnitude of g_2 can affect the quantity of solvent that diffuses in the gel and ultimately account for the presence or not of a phase separation.

6 Polyelectrolyte gels

This section looks at the description of polyelectrolyte gels, which are characterized by the presence of ionizable functional groups alongside the network. When considering collagen fibrils at the physiological pH, these are characterised by positive group (NH_3^+) and negative group (COO^-). Since the concentration of NH_3^+ is greater, the net surface density of the fibrils is positive. Note that this can change when fibrils are chemically cross-links, as charged groups are used in order to form such bridges [13].

In extracellular matrix, GAG chains, which carry negative charges, are dispersed in the network, leading it to a net negative charge. When modelling the ECM, collagen is assumed to be responsible for the mechanical integrity of the matrix, determining its elastic properties. On the other hand GAGs are considered responsible for the swelling behaviour of the matrix as it “traps” water molecules. Consequently, the ECM behaves overall as a polyelectrolyte gel. The ECM space is filled with fluids consisting of solvent, i.e. water, and solute, i.e. ions such as Na^+ and Cl^- , in which are the prevalent mobile ions in the system.

When a solvent with free ion diffuse into the gel, this deforms (swell), while the mobile ions interact with the fixed charge on the polymer network. A standard approach to the model of polyelectrolyte gels is the use of triphasic model, according to which the gel is a continuum composed of a solid phase (network), solvent(water), solute (mobile ions). To simplify our discussion, we do not consider chemical reactions, such as self-ionization of water or dissociation of functional groups, assuming that the pH is constant.

Let us denote by C_i , $i = 1, \dots, N$, the concentration of the different mobile ions, and by C_s the concentration of the solvent. If we now assume that volume changes due to the the presence of ions can be neglected, we still have the molecular incompressibility condition:

$$J = 1 + C_s v. \quad (88)$$

Alternatively, we could also account for the ions contribution as in [7]. We

also introduced C^f , which represents the density of fixed charges. By further assuming that the solutes are in a dilute solution, so that the volume fraction of the ions can be neglected we have that:

$$\phi_s + \phi_n = 1, \quad \phi_s = \frac{C_s v}{1 + C_s v} \quad (89)$$

where ϕ_s and ϕ_n are the volume fraction of the solvent and the network respectively.

Besides the conservation of the solvent mass, we need now to consider also the conservation of the different ion species mass, so that we have the following set of equations:

$$\dot{C}_i + \nabla_0 \mathbf{J}_i = 0, \quad i = s, 1, \dots, N \quad (90)$$

The presence of charges generates an electric field, \mathbf{E} , in the reference configuration. By denoting with Φ the electrostatic potential, we have that:

$$\mathbf{E} = -\nabla_0 \Phi, \quad \mathbf{e} = -\nabla \Phi \quad (91)$$

where \mathbf{e} is the electric field in the reference configuration. The presence of the field induces an electric displacement, \mathbf{H} (in the reference configuration), which must satisfy Gauss law or electrostatics:

$$\nabla_0 \cdot \mathbf{H} = Q, \quad (92)$$

where Q is the local total charge, which includes the contribution of both fixed and moving charges:

$$Q = e \left(\sum_i z_i C_i + z_f C_f \right), \quad (93)$$

where e is the elementary charge and z_a is the valence of the corresponding species.

Finally, we need to modify the expression of the free energy in the reference configuration ψ in order to take into account the mixing of the ions with the solute, ψ_{ions} , and the electric polarization of the polymer, ψ_p , [7]. Note also that the interfacial energy between faces is only related to C_s . Considering the gel to be an ideal dielectric, the energy associated with the electric field in the reference configuration is:

$$\psi_p = \frac{1}{2\epsilon J} \mathbf{H} \cdot \mathbb{F}^T \cdot \mathbb{F} \cdot \mathbf{H} \quad (94)$$

where ϵ is the electric permittivity, which is assumed to be independent of the deformation. Considering instead the work done by the magnetic field. On the other hand, the term ψ_{ions} accounts for the entropy of mixing ions with the solvent. Considering a dilute solution, this is given by:

$$\psi_{ions} = \sum_{i=1}^N \mu_i^0 C_i + kT \sum_{i=1}^N C_i \left(\ln \frac{C_i}{\varsigma_0^i C_s} - 1 \right), \quad (95)$$

where ς_0^i is the mole fraction of the species i , for which the chemical potential μ_i is zero.

With the potential Φ , we also have the reversible work:

$$- \int_{\partial R} \Phi \dot{\mathbf{H}} \cdot \mathbf{n} = - \int_R \underbrace{\phi \nabla_0 \cdot \dot{\mathbf{H}}}_{\dot{Q}} - \int_R \underbrace{\nabla_0 \phi}_{-\mathbf{E}} \cdot \dot{\mathbf{H}} = \int_R \mathbf{E} \cdot \dot{\mathbf{H}} - \sum_{i=1}^N e \int_R \Phi z_i \dot{C}_i$$

Note that we are here considering the reference configuration as the dry state, which implies an initial net charge in the system. On the other hand, when considering as initial state a swollen and stress-free state is assumed, standard practise is to assume *electro-neutrality*, i.e. $Q \equiv 0$.

Having specified the free energy, we can now write down the energy imbalance inequality:

$$\begin{aligned} \left\{ \int_R \psi \right\} \dot{} &\leq \int_{\partial R} (\boldsymbol{\xi} \cdot \mathbf{n}) \dot{C}_s + \int_{\partial R} \mathbb{S} \mathbf{n} \cdot \dot{\mathbf{u}} - \sum_{m=s,1,\dots,N} \int_{\partial R} \mu_m \mathbf{J}_m \cdot \mathbf{n} \\ &+ \int_R \mathbf{E} \cdot \dot{\mathbf{H}} - \sum_{i=1}^N e \int_R \Phi z_i \dot{C}_i. \end{aligned} \quad (96)$$

Hence using the divergence theorem and the fact that the inequality needs to hold for any reference volume R , we obtain the local inequality:

$$\dot{\psi} + \sum_m \nabla_0 \cdot (\mu_m \mathbf{J}_m) - \nabla_0 \cdot (\boldsymbol{\xi} \dot{C}_s) - \nabla_0 \cdot (\mathbb{S}^T \dot{\mathbf{u}}) - \mathbf{E} \cdot \dot{\mathbf{H}} + \sum_i e \Phi z_i \dot{C}_i \leq 0 \quad (97)$$

We can also include the incompressibility condition considering the Lagrange multiplier p :

$$\begin{aligned}
& \left(\frac{\partial \psi}{\partial \nabla_0 C_s} - \boldsymbol{\xi} \right) \cdot \nabla_0 \dot{C}_s + \left(\frac{\partial \psi}{\partial C_s} - \mu_s - \nabla_0 \cdot \boldsymbol{\xi} + pv \right) \dot{C}_s \\
& + \sum_i \left(\frac{\partial \psi}{\partial C_i} + e\Phi z_i - \mu_i \right) \dot{C}_i + \left(\frac{\partial \psi}{\partial \mathbf{H}} - \mathbf{E} \right) \cdot \dot{\mathbf{H}} \\
& + \left(\frac{\partial \psi}{\partial \mathbb{F}} + \frac{\partial \psi}{\partial \mathbb{F}_e} \mathbb{F}_v^{-1} - \mathbb{S} - pJ\mathbb{F}^{-T} \right) : \dot{\mathbb{F}} + \sum_m \nabla_0 \mu_m \cdot \mathbf{J}_m \\
& + \left(\mathbb{F}_v^{-T} \mathbb{F}^T \frac{\partial \psi}{\partial \mathbb{F}_e} + p_v \mathbb{I} \right) : \mathbb{L}_v \leq 0.
\end{aligned} \tag{98}$$

Hence, we obtain the following set of equation:

$$\boldsymbol{\xi} = \frac{\partial \psi}{\partial \nabla_0 C_s}, \tag{99}$$

$$\begin{aligned}
\mu_s = pv + \mu_s^0 - \nabla_0 \cdot \boldsymbol{\xi} + kT \left[\ln \frac{C_s v}{1 + C_s v} + \frac{1}{1 + C_s v} \right. \\
\left. + \frac{\chi}{(1 + C_s v)^2} - \sum_i \frac{C_i}{C_s} \right],
\end{aligned} \tag{100}$$

$$\mu_i = \underbrace{\mu_i^0 + e\Phi z_i}_{\tilde{\mu}_i} + kT \ln \frac{C_i}{\varsigma_0^i C_s}, \tag{101}$$

$$\mathbf{E} = \frac{1}{\epsilon J} \mathbb{F}^T \mathbb{F} \mathbf{H}, \tag{102}$$

$$\mathbb{S} = -pJ\mathbb{F}^{-T} + \frac{\partial \psi}{\partial \mathbb{F}} + \frac{\partial \psi}{\partial \mathbb{F}_e} \mathbb{F}_v^{-1}. \tag{103}$$

where $\tilde{\mu}_i$ is the electro-chemical potential. If we want now to evaluate \mathbb{T} , the Cauchy stress, in the case of a standard neo-Hookean solid material, is of the form:

$$\begin{aligned}
\mathbb{T} = -p\mathbb{I} + \frac{G_1}{1 + C_s v} (\mathbb{B} - \mathbb{I}) + \frac{G_2}{1 + C_s v} (\mathbb{B}_e - \mathbb{I}) \\
+ \gamma \left[\frac{1}{2} |\nabla C_s|^2 \mathbb{I} - \nabla C_s \otimes \nabla C_s \right] - \frac{1}{\epsilon} \left(\frac{1}{2} \mathbf{h} \cdot \mathbf{h} \mathbb{I} - \mathbf{h} \otimes \mathbf{h} \right)
\end{aligned}$$

where \mathbf{h} is the electric displacement in the current configuration. Using equation (102), we have that $\mathbf{h} = \epsilon \mathbf{e} = -\epsilon \nabla \Phi$. Substituting in the formula

for \mathbb{T} , we have that:

$$\begin{aligned}\mathbb{T} = & -p\mathbb{I} + \frac{G}{1+C_s v}(\mathbb{B} - \mathbb{I}) + \frac{G_2}{1+C_s v}(\mathbb{B}_e - \mathbb{I}) \\ & + \gamma \left[\frac{1}{2} |\nabla C_s|^2 \mathbb{I} - \nabla C_s \otimes \nabla C_s \right] + \epsilon \left[\frac{1}{2} |\nabla \Phi|^2 \mathbb{I} - \nabla \Phi \otimes \nabla \Phi \right].\end{aligned}$$

Similarly we can rewrite Equation—(92) in terms of ϕ :

$$-\epsilon J \nabla^2 \phi = Q. \quad (104)$$

The remaining component of the inequality accounts for the dissipation of energy due to the diffusion and viscosity, which contributes to the irreversible production of entropy. Relying again on the *Curie's law*, the two process can be decoupled. So that the viscous dissipation can be treated as in the previous section, i.e. the dynamic of \mathbb{B}_e is given by:

$$\dot{\mathbb{B}}_e = \mathbb{L}\mathbb{B}_e + \mathbb{B}_e\mathbb{L}^T - \frac{2}{\tau_R} \mathbb{B}_e \text{DEV}[\mathbb{B}_e] \quad (105)$$

On the other hand, the entropy production due to diffusion in the current configuration, ς , is given by:

$$\varsigma = - \sum_m \nabla \mu_m \cdot \mathbf{j}_m \quad (106)$$

where we can rewrite the flux as $\mathbf{j}_m = c_m(\mathbf{v}_m - \mathbf{v}_n) = c_m \bar{\mathbf{v}}_m$, where \mathbf{v}_m is the velocity of the m -th component in the current configuration, \mathbf{v}_n is the velocity of the network also in the current configuration and $\bar{\mathbf{v}}_m$ is the relative velocity of the m -th component with respect to the network.

In the framework of linear non-equilibrium thermodynamics, the transport dissipation function is given by:

$$-c_j \nabla \mu_j = \sum_b L_{jb} \bar{\mathbf{v}}_j = \sum_{i \neq j} f_{ji} (\bar{\mathbf{v}}_i - \bar{\mathbf{v}}_j) + f_{js} (\bar{\mathbf{v}}_s - \bar{\mathbf{v}}_j) + f_{jn} \bar{\mathbf{v}}_j, \quad (107)$$

$$-c_s \nabla \mu_s = \sum_i f_{si} (\bar{\mathbf{v}}_i - \bar{\mathbf{v}}_s) + f_{sn} \bar{\mathbf{v}}_s, \quad (108)$$

where f_{mi} and h_{mn} are the drag coefficients related to the interaction between fluid constituents and the polymer network respectively. Based on the Onsanger's reciprocal relation we have that:

$$f_{mb} = f_{bm}. \quad (109)$$

Common assumption in the study of mixture theory is that the solute-solute drag can be neglected so that $f_{ij} = 0$ for $i, j = 1, \dots, N$ [9,18]. The remaining drag coefficient are instead defined by:

$$f_{sn} = \frac{1}{k}, \quad f_{js} = \frac{k_B T c_j}{D_j^0}, \quad f_{js} + f_{jn} = \frac{k_B T c_j}{D_j}, \quad (110)$$

where k is the hydraulic permeability of the solvent in the network, D_j^0 is the diffusion coefficient of the solute in pure solution, while D_j is the diffusion coefficient in the gel.

Using (107)-(110), the relative velocities are of the form:

$$\bar{\mathbf{v}}_s = -\tilde{k} \left(c_s \nabla \mu_s + \sum_i \frac{D_i}{D_i^0} c_i \nabla \mu_i \right), \quad (111)$$

$$\bar{\mathbf{v}}_j = -\frac{D_j}{k_B T} \nabla \mu_j + \frac{D_j}{D_j^0} \bar{\mathbf{v}}_s, \quad (112)$$

and the coefficient \tilde{k} is defined as:

$$\frac{1}{\tilde{k}} = \frac{1}{k} + \sum_i k_B T \left(1 - \frac{D_i}{D_i^0} \right) \frac{c_i}{D_i^0}. \quad (113)$$

We will now consider just two species of ions in the solution, a positive $j = +$ and a negative $-$. We also consider the case of small ions, when we can neglect the friction between the polymer chains and the fluid, i.e. $D_i = D_i^0$. Under this assumption the system of equation simplifies as $\tilde{k} = k$. Following the work of Hennesy et al., we consider the hydraulic permeability k to be:

$$k = \frac{D_0 (1 + v C_s)^\beta}{k_B T c_s}, \quad (114)$$

Combining all together the fluxes are of the form:

$$\mathbf{j}_i = -\frac{D_i}{J} \left[\frac{e z_i C_i}{k_B T} \nabla \Phi + \nabla C_i - \frac{C_i}{C_s} \nabla C_s \right] - \frac{C_i}{C_s} \mathbf{j}_s \quad i \in \{+, -\}, \quad (115)$$

$$\begin{aligned} \mathbf{j}_s = & -\frac{D_0}{J} (1 + v C_s)^\beta \left\{ \sum_i \frac{C_i}{k_B T} \nabla \mu_i + \sum_i \left(\frac{C_i}{C_s} \nabla C_s - \nabla C_i \right) \right. \\ & \left. + \frac{v C_s}{k_B T} \nabla p + \frac{1 + v(1 - 2\chi) C_s}{(1 + C_s v)^3} \nabla C_s - \frac{\gamma C_s}{k_B T} \nabla (J \nabla^2 C_s) \right\} \end{aligned} \quad (116)$$

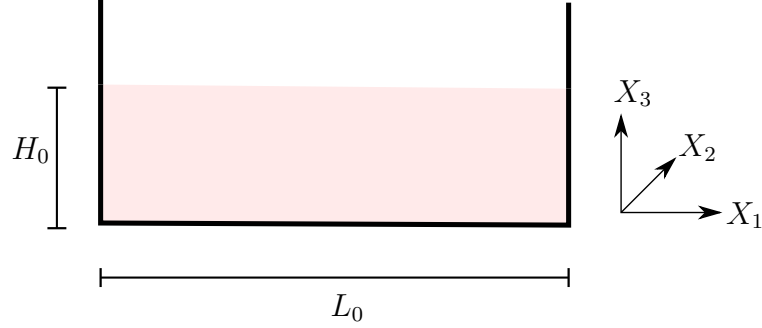


Figure 10: 2D section of the constraint swelling of a gel

and the evolution equation for the different species:

$$\partial_t C_m = -\nabla_0 \mathbf{J}_m, \quad \mathbf{J}_m = J \mathbb{F} \mathbf{j}_m \quad m = +, -, s. \quad (117)$$

6.1 Boundary Conditions.

As well known in non-equilibrium thermodynamics, the behaviour of a system is determined also by the condition imposed at the boundary. We here focus on the specific case of confined swelling, while one single face of the hydrogel is exposed to the bath.

First considering the substrate, i.e. $X_3 = 0$, we have that the hydrogel is attached to this, so that the displacement must be zero:

$$\mathbf{u} = 0. \quad (118)$$

All the fluxes needs also to vanish as the substrate is assumed to be impenetrable:

$$\mathbf{j}_m \cdot \mathbf{e}_3 = 0 \quad m = +, -, s. \quad (119)$$

As we also assumes that there is no influx of electric charges, we have that the gradient of the electric fields needs also to vanish:

$$\nabla \phi \cdot \mathbf{e}_3 = 0. \quad (120)$$

Finally, as the chemical potential of the solvent contains a second derivative of C_s , we need an additional boundary condition. In particular we prescribe the concentration gradient to vanish:

$$\nabla C \cdot \mathbf{e}_3 = 0, \quad (121)$$

which describe the case in which the energy interaction of the solvent with the network and the substrate are identical.

On the side walls, i.e. $X_1 = 0, L_0$ and $X_1 = 0, L_0$, the gel can not expand side-ways but can freely slide along the walls:

$$\mathbf{u} \cdot \mathbf{e}_k = 0, \quad \mathbf{e}_2 \mathbb{T} \mathbf{e}_k = 0 \quad (122)$$

for $k = 1, 2$. As for the substrate boundary, we also impose that:

$$\mathbf{j}_m \cdot \mathbf{e}_k = 0 \quad m = +, -, s; \quad (123)$$

$$\nabla C \cdot \mathbf{e}_k = 0 \quad \nabla \phi \cdot \mathbf{e}_k = 0. \quad (124)$$

Finally, we need to consider the bath-gel interface, which is located at $X_3 = H_0$ in the reference configuration, with H_0 being the initial thickness of the network in the dry state. If we denote by \mathbf{n} the normal to the surface in the current configuration, the continuity of the stress across the interface leads to:

$$\mathbb{T} \mathbf{n} = 0, \quad (125)$$

as we are assuming the bath to be in a stress-free state. As for the other boundary we still have that:

$$\nabla C \cdot \mathbf{n} = 0, \quad \nabla \phi \cdot \mathbf{n} = 0. \quad (126)$$

In standard constraint swelling, the chemical equilibrium of each species at the interface is imposed to be equal to the one in the bath:

$$\mu_m = \mu_m^{ext} \quad m = +, -, s. \quad (127)$$

7 Constraint Swelling in 1D.

We here consider the case of uniaxial swelling, which is characterised by the following deformation gradient:

$$\mathbb{F} = \begin{bmatrix} 1 & 0 & 0 \\ 0 & 1 & 0 \\ 0 & 0 & J(Z, t) \end{bmatrix} \quad (128)$$

so that $\mathbb{B} = \text{diag}(1, 1, J^2)$, $C_m = C_m(z, t)$. Since $\mathbb{B}_e(Z, 0) = \mathbb{B}(Z, 0)$ is a diagonal matrix, the off-diagonal term of the matrix B_e remain equal to

zero. The symmetry of the problem with respect to x and y guarantees that $\mathbb{B}_{e,11} = \mathbb{B}_{e,22} = \mathbb{B}_{e,x}(Z, t)$ for any $t > 0$. We here consider the case of a forced swelling, i.e. we impose the flux at the boundary $Z = 1$. Consequently, the system governing equation in the reference configuration reduce to:

$$\partial_t C_m = -\partial_Z J_m, \quad (129)$$

$$J_s = -D_0(1 + vC_s)^{\beta-2} \left\{ \sum_i \frac{C_i}{k_B T} \partial_Z \mu_i + \sum_i \left(\frac{C_i}{C_s} \partial_Z C_s - \partial_Z C_i \right) + \frac{vC_s}{k_B T} \partial_Z p + \frac{1 + v(1 - 2\chi)C_s}{(1 + C_s v)^3} \partial_Z C_s - \frac{\gamma C_s}{k_B T} \partial_{ZZ}((1 + vC_s) \partial_Z C_s) \right\} \quad (130)$$

$$J_i = -\frac{D_i}{(1 + vC_s)^2} \left[\frac{e z_i C_i}{k_B T} \partial_Z \Phi + \partial_Z C_i - \frac{C_i}{C_s} \partial_Z C_s \right] - \frac{C_i}{C_s} J_s \quad (131)$$

$$\partial_Z \mathbb{T}_{zz} = 0 \quad (132)$$

$$-\epsilon \partial_Z[(1 + vC) \partial_Z \phi] = Q, \quad (133)$$

$$\partial_t B_{e,z} = -\frac{2B_{e,z}}{1 + Cv} \partial_Z J_m - \frac{4}{3\tau_R} B_{e,z} (B_{e,z} - B_{e,x}) \quad (134)$$

$$\partial_t B_{e,x} = -\frac{2}{3\tau_R} B_{e,x} (B_{e,x} - B_{e,z}) \quad (135)$$

$$(136)$$

8 Steady-state solution to confined swelling.

We now analyse the steady state solution to the model in the case of confined swelling. Under this condition the hydrogel would swell until it reaches its steady state, when all chemical potential are taken to be constant and equal to the bath values [20]:

$$\mu_s^{ext} = \mu_s^0 - vkT \sum_i c_i^0, \quad (137)$$

$$\mu_i^{ext} = \mu_i^0 + kT \ln(vc_i^0), \quad (138)$$

where we have further assumed that the external pressure in the bath is zero, and c_i^0 is the concentration of the concentration of the i -th ionic species in the external solution.

Under this condition the we have that:

$$B_{e,z} = B_{e,x} = (1 + vC_s)^{2/3}, \quad (139)$$

$$\mathbb{T}_{zz} = -p + G_1 \frac{(1 + vC_s)^2 - 1}{1 + C_s v} + G_2 \frac{(1 + vC_s)^{2/3} - 1}{1 + C_s v}, \quad (140)$$

$$0 = pv + kT \left[\ln \frac{C_s v}{1 + C_s v} + \frac{1}{vC_s + 1} + \frac{\chi}{(1 + C_s v)^2} - \sum_i \left(\frac{C_i}{C_s} - v c_i^0 \right) \right], \quad (141)$$

$$C_i = \varsigma_0^i C_s v c_i^0 \exp \left[-\frac{e z_i}{kT} \phi \right], \quad (142)$$

$$z_+ C_+ + z_- C_- = -z_f C_f \quad (143)$$

Integrating Equation (132) and using the stress-free condition, we have that:

$$p = G_1 \frac{(1 + vC_s)^2 - 1}{1 + C_s v} + G_2 \frac{(1 + vC_s)^{2/3} - 1}{1 + C_s v}, \quad (144)$$

As in the work by Yu et al. [20], we here assume the solution to be ideal, i.e. $\varsigma_0^i = 1$. We further consider that both positive and negative charges have the same concentration concentration in the external bath $c_+^0 = c_-^0 = c_0$. Substituting this into Equation (142) we recover the Donnan Equilibrium solution, [18]:

$$C_+ C_- = (v C_s c_0)^2. \quad (145)$$

which needs to be coupled with the electro-neutrality condition (143), where we consider $z_+ = +1$ and $z_- = -1$:

$$C_{\pm} = \frac{1}{2} \left[\mp z_f C_f + \sqrt{(z_f C_f)^2 + (2v C_s c_0)^2} \right], \quad (146)$$

$$\phi = \frac{kT}{2e} \ln \frac{C_-}{C_+}. \quad (147)$$

Consequently the equilibrium is determined by the condition:

$$F(C_s; c_0) = 0, \quad (148)$$

where the function F is obtained equilibrating the mechanical and osmotic

pressures due to the polymer and the ions respectively:

$$F(C_s; c_0) = \ln \frac{C_s v}{1 + C_s v} + \frac{1 + C_s v + \chi}{(1 + C_s v)^2} + 2c_0 v - \sqrt{\left(\frac{z_f C_f}{C_s}\right)^2 + 4v^2 c_0^2} \\ + \frac{G_1 v}{k_B T} \frac{(1 + v C_s)^2 - 1}{1 + C_s v} + \frac{G_2 v}{k_B T} \frac{(1 + v C_s)^{2/3} - 1}{1 + C_s v} \quad (149)$$

8.1 Free-Swelling.

So far we have considered the case of constrained swelling. In this case, the two spring have a different contribution to the mechanical pressure. When instead considering the free swelling case, the stretch is equivalent in all directions. So that the deformation tensor is $\mathbb{F} = \lambda_0 \mathbb{I}$ with $\lambda_0 = (1 + C_s v)^{1/3}$. It is just trivial to recover the equilibrium condition in such case:

$$F_{free}(C_s; c_0) = \ln \frac{C_s v}{1 + C_s v} + \frac{1 + C_s v + \chi}{(1 + C_s v)^2} + 2c_0 v - \sqrt{\left(\frac{z_f C_f}{C_s}\right)^2 + 4v^2 c_0^2} \\ + \frac{(G_1 + G_2) v}{k_B T} \frac{(1 + v C_s)^{2/3} - 1}{1 + C_s v} \quad (150)$$

8.2 Static Analysis of Confined Compression.

Let us consider the case of the confined compression of a material slice with the use of a porous platen. We assume that the gels has been left freely swell so that the initial concentration is given by $C \equiv C_{eq}$ so that $F_{free}(C_{eq}; c_0) = 0$, with c_0 being fixed.

Under such condition, in a uniaxial compression the deformation gradient as a function of the strain κ is:

$$\mathbb{F} = J_{eq}^{1/3} \begin{bmatrix} 1 & 0 & 0 \\ 0 & 1 & 0 \\ 0 & 0 & (1 - \kappa) \end{bmatrix}. \quad (151)$$

We can thus easily derive the relation between strain and nominal solvent concentration: $C_s(\kappa)v = (1 + C_{eq}v)(1 - \kappa) - 1$. Using Equation (140)-(141)-

Symbol	Description	Value
C_f	Charge concentration	$3.947 \times 10^{23} \text{ m}^{-3}$
v	Volume of water molecule	$3 \times 10^{-29} \text{ m}^3$
z_f	Charge of GAG chain	-4
k_B	Boltzmann constant	$1.38 \times 10^{-23} \text{ J/K}$
T	Absolute temperature	295 K
c_0	Concentration of free ions in the bath	$9.27 \times 10^{25} \text{ m}^{-3}$

Table 1: Parameters adopted in the simulations as estimated in previous works.

(146), we have that the stress, σ , strain, κ , curved is defined by:

$$\sigma = \frac{k_B T}{v} \tilde{F}(C_s(\kappa); c_0). \quad (152)$$

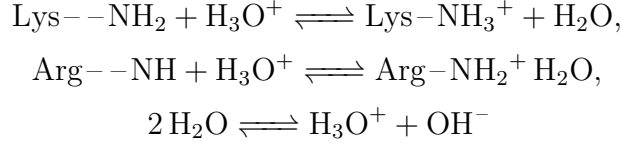
$$\begin{aligned} \tilde{F}(C_s; c_0) = & \ln \frac{C_s v}{1 + C_s v} + \frac{1 + C_s v + \chi}{(1 + C_s v)^2} + 2c_0 v - \sqrt{\left(\frac{z_f C_f}{C_s}\right)^2 + 4v^2 c_0^2} \\ & + \frac{G_1 v}{k_B T} \frac{(1 + vC_{eq})^{-4/3} (1 + vC_s)^2 - 1}{1 + C_s v} + \frac{G_2 v}{k_B T} \frac{(1 + vC_s)^{2/3} - 1}{1 + C_s v} \end{aligned}$$

In Table 1, we have listed the parameters previously estimated in the literature. Consequently, the only parameters that remain to be estimated are the two shear moduli, G_1 and G_2 , and the enthalpy of mixing, χ .

Note: there is no clear agreement on whether viscous deformation are volume preserving or not. Is there a way to discern between the two? While in the free-swelling case the two would agree even if with different values of the spring constant, the prediction would substantially differ in the case of constraint swelling.

9 Ph-dependent gels.

When considering collagen alone, this belong to the class of Ph-sensitive hydrogel. Each polymeric chain bears lysine and arginine amino-acids which are both positively charged (**basic**) at physiological pH, with a pK of 10.5 and 12.5 respectively. This requires to include in the model the protonation of the basic group and the self i:



In this case the fixed charges are not constant but depend on the concentration of H^+ ions in the solution. Consequently, we now need to consider four different types of mobile ions in the gel and external solution: Na^+ , Cl^- , OH^- and H^+ . This will be denoted by C_+ , C_- , C_{OH^-} and C_{H^+} respectively, while the positive charges coming from the basic group as C_f^+ . Note that during the reaction the number of basic group and fixed charges is conserved:

$$\begin{aligned}
C_{Lys}^+ + C_{Lys}^{\text{NH}_2} &= C_{Lys}^0, \\
C_{Arg}^+ + C_{Arg}^{\text{NH}} &= C_{Arg}^0,
\end{aligned} \tag{153}$$

where C_i^0 stands for the number of each basic group on the network per unit volume in the dry state. Note that the total concentration of fixed charges is $C_f^+ = C_{Lys}^+ + C_{Arg}^+$. Using the subscribe 1, 2 to refer to Lysine and Arginine group respectively, we can rewrite the above equation as:

$$C_f^+ = \alpha_1 C_1^0 + \alpha_2 C_2^0, \quad C_1^{\text{NH}_2} = (1 - \alpha_1) C_1^0, \quad C_2^{\text{NH}} = (1 - \alpha_2) C_2^0. \tag{154}$$

The presence of chemical reaction requires also the update of the mass balance for all the chemical species involve in the reaction, we have that the conservation law is:

$$\dot{C}_{\text{H}^+} = \Gamma_{\text{H}^+} - \nabla_0 \mathbf{J}_{\text{H}^+} \tag{155}$$

$$\dot{C}_{\text{OH}^-} = \Gamma_{\text{OH}^-} - \nabla_0 \mathbf{J}_{\text{OH}^-} \tag{156}$$

$$\dot{C}_s = \Gamma_s - \nabla_0 \mathbf{J}_s \tag{157}$$

where the Γ_i represent the net rate of production for the corresponding chemical species. Subject to the reversible chemical reaction above mentioned the Helmholtz free energy of the gel will now depend also on the number of fixed-charge. Under such assumption, we need to add an additional term in the

energy inequality (98) to account for the contribution of the reaction:

$$\begin{aligned}
& \left(\frac{\partial \psi}{\partial \nabla_0 C_s} - \boldsymbol{\xi} \right) \cdot \nabla_0 \dot{C}_s + \left(\frac{\partial \psi}{\partial C_s} - \mu_s - \nabla_0 \cdot \boldsymbol{\xi} + pv \right) \dot{C}_s + \sum_i \Gamma_i \mu_i + \frac{\partial \psi}{\partial X} \Gamma_{\text{OH}^-} \\
& + \sum_i \left(\frac{\partial \psi}{\partial C_i} + e \Phi z_i - \mu_i \right) \dot{C}_i + \left(\frac{\partial \psi}{\partial \alpha_1} + e \phi C_1^0 \right) \dot{\alpha}_1 + \left(\frac{\partial \psi}{\partial \alpha_2} + e \phi C_2^0 \right) \dot{\alpha}_2 \\
& + \left(\frac{\partial \psi}{\partial \mathbb{F}} + \frac{\partial \psi}{\partial \mathbb{F}_e} \mathbb{F}_v^{-1} - \mathbb{S} - p J \mathbb{F}^{-T} \right) : \dot{\mathbb{F}} + \sum_m \nabla_0 \mu_m \cdot \mathbf{J}_m \\
& + \left(\frac{\partial \psi}{\partial \mathbf{H}} - \mathbf{E} \right) \cdot \dot{\mathbf{H}} + \left(\mathbb{F}_v^{-T} \mathbb{F}^T \frac{\partial \psi}{\partial \mathbb{F}_e} + p_v \mathbb{I} \right) : \mathbb{L}_v \leq 0.
\end{aligned}$$

where Γ_i is considered to be zero for those species that do not participate in any reaction while X is the variable that trace the advancement of the self-ionization of water, i.e. $\dot{X} = \Gamma_{\text{OH}^-}$.

We consider the rate of self ionization of water to be Γ_0 so that the reaction rate for the different species can be rewritten as:

$$\Gamma_s = -2\Gamma_0 + \dot{\alpha}_1 C_1^0 + \dot{\alpha}_2 C_0^2, \quad (158)$$

$$\Gamma_{\text{H}^+} = \Gamma_0 - \dot{\alpha}_1 C_1^0 - \dot{\alpha}_2 C_0^2, \quad (159)$$

$$\Gamma_{\text{OH}^-} = \Gamma_0. \quad (160)$$

Substituting the above relation in the energy inequality we obtain:

$$\begin{aligned}
& \left(\frac{\partial \psi}{\partial \nabla_0 C_s} - \boldsymbol{\xi} \right) \cdot \nabla_0 \dot{C}_s + \left(\frac{\partial \psi}{\partial C_s} - \mu_s - \nabla_0 \cdot \boldsymbol{\xi} + pv \right) \dot{C}_s \\
& + \sum_i \left(\frac{\partial \psi}{\partial C_i} + e \Phi z_i - \mu_i \right) \dot{C}_i + \left(\frac{\partial \psi}{\partial \alpha_1} + e \phi C_1^0 + \mu_s C_1^0 - \mu_{\text{H}^+} C_1^0 \right) \dot{\alpha}_1 \\
& + \left(\frac{\partial \psi}{\partial \alpha_2} + e \phi C_2^0 + \mu_s C_2^0 - \mu_{\text{H}^+} C_2^0 \right) \dot{\alpha}_2 + \Gamma_0 \left(-2\mu_s + \mu_{\text{H}^+} + \mu_{\text{OH}^-} + \frac{\partial \psi}{\partial X} \right) \\
& + \left(\frac{\partial \psi}{\partial \mathbb{F}} + \frac{\partial \psi}{\partial \mathbb{F}_e} \mathbb{F}_v^{-1} - \mathbb{S} - p J \mathbb{F}^{-T} \right) : \dot{\mathbb{F}} - \sum_m \nabla_0 \mu_m \cdot \mathbf{J}_m \\
& + \left(\frac{\partial \psi}{\partial \mathbf{H}} - \mathbf{E} \right) \cdot \dot{\mathbf{H}} + \left(\mathbb{F}_v^{-T} \mathbb{F}^T \frac{\partial \psi}{\partial \mathbb{F}_e} + p_v \mathbb{I} \right) : \mathbb{L}_v \leq 0.
\end{aligned}$$

We here assume that the reaction kinetics is much faster than the diffusion so that the local equilibrium is reached instantaneously and that the energy

dissipated in the reaction is negligible. Under such assumption we have that C_f^+ , or equivalently α_1 and α_2 , and X , are an external variable and so in order for the above inequality to hold:

$$\frac{\partial \psi}{\partial \alpha_1} + e\phi C_1^0 + \mu_s C_1^0 - \mu_{H^+} C_1^0 = 0 \quad (161)$$

$$\frac{\partial \psi}{\partial \alpha_2} + e\phi C_2^0 + \mu_s C_2^0 - \mu_{H^+} C_2^0 = 0, \quad (162)$$

$$\frac{\partial \psi}{\partial X} - 2\mu_s + \mu_{H^+} + \mu_{OH^-} = 0 \quad (163)$$

We need now to specify the contribution of the different chemical reactions to the Helmholtz free energy, ψ_r . This includes the contribution due to the mixing of charged and non-charged groups, and the heat released during the protonation and self-ionization of water, enthalpy production:

$$\begin{aligned} \psi_1 = & \beta_1 C_1^0 \alpha_1 + \beta_2 C_2^0 \alpha_2 + \beta_{OH^-} X \\ & + k_B T \left(\alpha_1 C_1^0 \ln \frac{\alpha_1 C_1^0}{C_1^0 + C_2^0} + \alpha_2 C_2^0 \ln \frac{\alpha_2 C_2^0}{C_1^0 + C_2^0} \right. \\ & \left. + [(1 - \alpha_1) C_1^0 + (1 - \alpha_2) C_2^0] \ln \frac{(1 - \alpha_1) C_1^0 + (1 - \alpha_2) C_2^0}{C_1^0 + C_2^0} \right) \end{aligned} \quad (164)$$

where β_i is the increase in enthalpy associated with each reaction. Substituting Equation (164) into (161)-(163), we obtain:

$$\frac{[(1 - \alpha_1) C_1^0 + (1 - \alpha_2) C_2^0] C_{H^+}}{\alpha_1 C_1^0 C_s} = \exp \left[\frac{\beta_1 - \mu_{H^+}^0 + \mu_s}{k_B T} \right], \quad (165)$$

$$\frac{[(1 - \alpha_1) C_1^0 + (1 - \alpha_2) C_2^0] C_{H^+}}{\alpha_2 C_2^0 C_s} = \exp \left[\frac{\beta_2 - \mu_{H^+}^0 + \mu_s}{k_B T} \right] \quad (166)$$

$$\frac{C_{H^+} C_{OH^-}}{C_s^2} = \exp \left[\frac{2\mu_s - \beta_{OH^-} - \mu_{H^+}^0 - \mu_{OH^-}^0}{k_B T} \right]. \quad (167)$$

The above equation can be rewritten in terms of molar fraction by the conversion formula:

$$[H^+] = \kappa \frac{C_{H^+}}{C_s} = \kappa \frac{c_{H^+}}{c_s} \quad (168)$$

where $k = 10^3/18$ is the molarity of water. Similar relation holds for all species, so that the system of equation (167) can be written is the more

common form:

$$[H^+][OH^-] = \underbrace{\kappa^2 \exp \left[\frac{2\mu_s^0 - \beta_{OH^-} - \mu_{H^+}^0 - \mu_{OH^-}^0}{k_B T} \right]}_{K_w} \exp \left[2 \frac{\mu_s - \mu_0}{k_B T} \right], \quad (169)$$

$$\frac{[H^+][(1 - \alpha_1)C_1^0 + (1 - \alpha_2)C_2^0]}{\alpha_1 C_1^0} = \underbrace{\kappa \exp \left[\frac{\mu_s^0 + \beta_1 - \mu_{H^+}^0}{k_B T} \right]}_{K_{a,1}} \exp \left[\frac{\mu_s - \mu_0}{k_B T} \right] \quad (170)$$

$$\frac{[H^+][(1 - \alpha_1)C_1^0 + (1 - \alpha_2)C_2^0]}{\alpha_2 C_2^0} = \underbrace{\kappa \exp \left[\frac{\mu_s^0 + \beta_2 - \mu_{H^+}^0}{k_B T} \right]}_{K_{a,2}} \exp \left[\frac{\mu_s - \mu_0}{k_B T} \right] \quad (171)$$

where K_w is the equilibrium constant of water, while $K_{a,1}$ and $K_{a,2}$ acidic dissociation constant of the protonated lysine and arginine group respectively.

If we now consider the equilibrium case, we have that the potential of water in the gel is equal to the one in the bath, which is defined by equation (118):

$$[H^+][OH^-] = K_w e^{-v \sum_i c_i^0}, \quad (172)$$

$$\frac{\alpha_2 C_2^0}{\alpha_1 C_1^0} = \frac{K_{a,1}}{K_{a,2}}, \quad (173)$$

$$\frac{[H^+][(1 - \alpha_1)C_1^0 + (1 - \alpha_2)C_2^0]^2}{[OH^-]\alpha_2 C_2^0 \alpha_1 C_1^0} = \frac{K_{a,1} K_{a,2}}{K_w} \quad (174)$$

the electro-neutrality condition in the bath:

$$c_+^0 + c_{H^+}^0 = c_-^0 + c_{OH^-}^0. \quad (175)$$

Having the value of the pH in the solution bath then, since we consider the salt not to be completely dissociated:

$$\frac{c_{H^+}^0}{c_0} = \frac{1}{\kappa} 10^{-pH}, \quad \frac{c_{OH^-}^0}{c_0} = \frac{1}{\kappa} 10^{-pK_w + pH}, \quad (176)$$

and in the gel:

$$C_+ + C_{H^+} + \alpha C_0 = C_- + C_{OH^-}. \quad (177)$$

while in the solution:

$$C_i = C_s v c_i^0 \exp \left[-\frac{e z_i}{k_B T} \phi \right]. \quad (178)$$

Combining the two equation, we recover naturally the condition for the Donnan equilibrium:

$$(C_{H^+} + C_+) C_- = (C_s v c_-^0)^2 \quad (179)$$

A Korteweg stress terms.

The Korteweg stress is the part of the mechanical stress which is related to the interfacial free energy. We here report the result related to the second model. This will have a contribution from the both the derivative with respect to \bar{F} and J :

$$\mathbb{T}^{korg} = \text{DEV} \left[J^{-1} \frac{\partial \psi_{int}}{\partial \bar{F}} \bar{F}^T \right] + \frac{\partial \psi_{int}}{\partial J} \mathbb{I} \quad (180)$$

where the interface energy is given by:

$$\psi_{int}(J, \bar{F}) = \frac{\gamma}{2} J^{1/3} \bar{F}^{-1} \bar{F}^{-T} |\nabla_0 C|^2. \quad (181)$$

Using the properties of the deformation tensor \bar{F} , it can be shown that:

$$\frac{\partial}{\partial \bar{F}} (\bar{F}^{-1} \bar{F}^{-T} |\nabla_0 C|^2) \bar{F}^T = -2J^{2/3} \nabla C \otimes \nabla C, \quad (182)$$

so that the Korteweg stress is given by:

$$\mathbb{T}^{korg} = -\gamma \text{DEV} [\nabla C \otimes \nabla C] + \frac{\gamma}{6} |\nabla C|^2 \mathbb{I}. \quad (183)$$

If we now explicitly evaluate the deviatoric component we have:

$$\begin{aligned} \text{tr}(\nabla C \otimes \nabla C) &= |\nabla C|^2 \\ \text{DEV} [\nabla C \otimes \nabla C] &= \nabla C \otimes \nabla C - \frac{|\nabla C|^2}{3} \mathbb{I}. \end{aligned}$$

Substituting now the expressions back in Equation (183), we obtain:

$$\mathbb{T}^{korg} = \gamma \left[\frac{1}{2} |\nabla C|^2 \mathbb{I} - \nabla C \otimes \nabla C \right], \quad (184)$$

which is equivalent to result obtained for the first model.

References

- [1] J.S. Bergström and M.C. Boyce. Constitutive modeling of the large strain time-dependent behavior of elastomers. *Journal of the Mechanics and Physics of Solids*, 46(5):931 – 954, 1998.
- [2] D. Caccavo, S. Cascone, G. Lamberti, and A. A. Barba. Hydrogels: experimental characterization and mathematical modelling of their mechanical and diffusive behaviour. *Chem. Soc. Rev.*, 47:2357–2373, 2018.
- [3] D. Garcia-Gonzalez and A. Jerusalem. Energy based mechano-electrophysiological model of cns damage at the tissue scale. *Journal of the Mechanics and Physics of Solids*, 125:22 – 37, 2019.
- [4] Daniel Garcia-Gonzalez. Magneto-visco-hyperelasticity for hard-magnetic soft materials: theory and numerical applications. *Smart Materials and Structures*, 28(8):085020, jul 2019.
- [5] Morton E. Gurtin. Generalized ginzburg-landau and cahn-hilliard equations based on a microforce balance. *Physica D: Nonlinear Phenomena*, 92(3):178 – 192, 1996.
- [6] Morton E. Gurtin. Generalized ginzburg-landau and cahn-hilliard equations based on a microforce balance. *Physica D: Nonlinear Phenomena*, 92(3):178 – 192, 1996.
- [7] Wei Hong. *Continuum Models of Stimuli-responsive Gels*, pages 165–196. Springer Berlin Heidelberg, Berlin, Heidelberg, 2012.
- [8] Yuhang Hu and Zhigang Suo. Viscoelasticity and poroelasticity in elastomeric gels. *Acta Mechanica Solida Sinica*, 25(5):441 – 458, 2012.
- [9] A. Katzir-Katchalsky and P.F. Curran. *Nonequilibrium thermodynamics in biophysics*. Books in Biophysics. Harvard University Press, 1965.
- [10] D. Kondepudi and I. Prigogine. *Modern Thermodynamics: From Heat Engines to Dissipative Structures*. CourseSmart. John Wiley & Sons, 2014.
- [11] E. Kröner. Allgemeine Kontinuumstheorie der Versetzungen und Eigenspannungen. *Archive for Rational Mechanics and Analysis*, 4:273–334, January 1959.

- [12] Vlado A Lubarda. Constitutive theories based on the multiplicative decomposition of deformation gradient: Thermoelasticity, elastoplasticity, and biomechanics . *Applied Mechanics Reviews*, 57(2):95–108, 04 2004.
- [13] Patrick Mesquida, Dominik Kohl, Orestis Andriotis, Philipp Thurner, Melinda Duer, Sneha Bansode, and Georg Schitter. Evaluation of surface charge shift of collagen fibrils exposed to glutaraldehyde. *Scientific Reports*, 8, 12 2018.
- [14] Kevin M Moerman, Behrooz Fereidoonzezhad, and Patrick McGarry. Novel hyperelastic models for large volumetric deformations, Feb 2019.
- [15] T.A. N’Guyen, S. Lejeunes, D. Eyheramendy, and A. Boukamel. A thermodynamical framework for the thermo-chemo-mechanical couplings in soft materials at finite strain. *Mechanics of Materials*, 95:158 – 171, 2016.
- [16] Lars Onsager. Reciprocal relations in irreversible processes. i. *Phys. Rev.*, 37:405–426, Feb 1931.
- [17] I. Prigogine. *Introduction to thermodynamics of irreversible processes*. Interscience Publishers, 1968.
- [18] Shi-Lei Xue, Bo Li, Xi-Qiao Feng, and Huajian Gao. A non-equilibrium thermodynamic model for tumor extracellular matrix with enzymatic degradation. *Journal of the Mechanics and Physics of Solids*, 104:32 – 56, 2017.
- [19] Shi-Lei Xue, Shao-Zhen Lin, Bo Li, and Xi-Qiao Feng. A nonlinear poroelastic theory of solid tumors with glycosaminoglycan swelling. *Journal of Theoretical Biology*, 433:49 – 56, 2017.
- [20] Yalin Yu, Chad M. Landis, and Rui Huang. Salt-Induced Swelling and Volume Phase Transition of Polyelectrolyte Gels. *Journal of Applied Mechanics*, 84(5), 03 2017.