Data Augmentation Through Monte Carlo Arithmetic Leads to More Generalizable Classification in Connectomics

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Abstract

Machine learning models are commonly applied to human brain imaging datasets in an effort to associate function or structure with behaviour, health, or other individual phenotypes. Such models often rely on low-dimensional maps generated by complex processing pipelines. However, the numerical instabilities inherent to pipelines limit the fidelity of these maps and introduce computational bias. Monte Carlo Arithmetic, a technique for introducing controlled amounts of numerical noise, was used to perturb a structural connectome estimation pipeline, ultimately producing a range of plausible networks for each sample. The variability in the perturbed networks was captured in an augmented dataset, which was then used for an age classification task. We found that resampling brain networks across a series of such numerically perturbed outcomes led to improved performance in all tested classifiers, preprocessing strategies, and dimensionality reduction techniques. Importantly, we find that this benefit does not hinge on a large number of perturbations, suggesting that even minimally perturbing a dataset adds meaningful variance which can be captured in the subsequently designed models.

Keywords

Stability — Network Neuroscience — Neuroimaging — Machine Learning — Generalizability

Introduction

3 The application of machine learning has become common-4 place for the identification and characterization of individual ⁵ biomarkers in neuroimaging¹. Models have been applied to 6 discriminate between measures of brain structure or function ⁷ based upon phenotypic variables related to disease^{2–4}, devel- ₂₂ 8 opment⁵, or other axes of potential consequence^{6,7}.

16 to learn generalizable relationships among data, and leads 31 widely accepted noise models in connectomics, the necessity

17 to biased predictors. Traditionally, this bias has been re-18 duced through the collection and application of repeated-19 measurement datasets^{15,16}, though this requires considerable 20 resources and is not feasible in the context of all clinical 21 populations.

Dataset augmentation has been broadly demonstrated as 23 an effective technique for improving the generalizability of These models often build representations upon processed 24 learned models, especially in deep learning¹⁷. In neuroimag-10 imaging data, in which 3D or 4D images have been trans- 25 ing, augmentation is often performed throughout the process formed into estimates of structure⁸, function⁹, or connective 26 of tool validation and requires either realistic data simula-12 ity¹⁰. However, there is a lack of reliability in these esti- 27 tors or phantom datasets¹⁸, which significantly limits their 18 mates, including variation across analysis team¹¹, software 28 applicability to real data. Recent advances in deep learning 14 library 12, operating system 13, and instability in the face of nu- 29 have made dataset augmentation far more accessible 19, inmerical noise¹⁴. This uncertainty limits the ability of models 30 cluding in medical imaging^{20,21}. However, due to the lack of

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32 of compute-intensive training, and the associated infrastruc-34 network neuroscience remains largely uncharted territory (see 74 //github.com/gkpapers/2021AggregateMCA. 35 Appendix 1 for details).

Perturbation methods which inject small amounts of noise 75 Dataset 37 through the execution of a pipeline, such as Monte Carlo 76 An existing dataset containing Monte Carlo Arithmetic (MCA) 41 sible results, where no single observation is more or less valid 80 of the data and processing follows here. 42 than the others – including those which were left unperturbed. 81 48 specific augmentation models.

56 ability of their performance across the two. We demonstrate 95 of 3,403 unique weighted connections. 57 the efficacy of using MCA as a method for dataset augmenta- 96 59 brain-phenotype relationships.

Materials & Methods

62 The objective of this study was to evaluate the impact of aggre-101 turbed with a zero-centered random variable 1-bit beyond the 63 gating collections of unstable brain networks towards learning 102 precision of the system^{22,23}. In practice, this resulted in per-64 robust brain-phenotype relationships. We sampled and aggre- 103 turbations that were analogous to an inexact trailing decimal 65 gated simulated networks within individuals to learn relation- 104 value of, say, 0.6 being rounded up to 1.0 in 60% of evalu-66 ships between brain connectivity and individual phenotypes, 105 ations and down to 0.0 for the remaining 40%. The pertur-67 in this case age, and compared this to baseline performance on 106 bations were randomly sampled for each operation, and thus 68 this task. We compared aggregation strategies with respect to 107 the unique combinations of error accumulation over multiple 69 baseline validation performance, performance out-of-sample, 108 executions of a pipeline lead to potentially distinct terminal 70 and generalizability. The experimental workflow is visualized 109 results. The MCA approach is pipeline- and data-agnostic, 71 in Figure 1.

All developed software and analysis resources for this 33 tural requirements, the application of dataset augmentation to 73 project have been made available through GitHub at https:

38 Arithmetic (MCA)^{22,23}, have recently been used to induce 77 perturbed structural human brain networks was used for these 39 instabilities in structural connectome estimation software²⁴. 78 experiments²⁵. While further information on the processing 40 Importantly, this technique produces a range of equally plau- 79 and curation of this dataset ca be found in 14, a brief description

The networks were derived from diffusion MRI data from ⁴³ While sampling from a set of perturbed connectomes may ⁸² the Nathan Kline Institute Rockland Sample dataset¹⁶. The 44 have an impact on learning brain-phenotype relationships 14, 83 data were denoised and aligned prior to undergoing modelling 45 there remains potential for leveraging the distribution of per- 84 via a probabilistic tractography pipeline built using Dipy²⁶ 46 turbed results to augment datasets in lieu of increasing sample 85 with a fixed random state. The streamlines were ultimately ⁴⁷ sizes, performing repeated measurements, or developing data- ⁸⁶ mapped to regional network connections using the Desikan-87 Killiany-Tourville parcellation²⁷. The raw input data to this Using an existing collection of MCA-perturbed structural 88 pipeline consisted of 4-dimensional images (with the fourth 50 connectomes²⁵, we trained classifiers on networks sampled 89 dimension corresponding to unique diffusion directions) con-₅₁ from the distribution of results and evaluated their perfor-₉₀ taining O(10⁸) voxels, and the derived connectomes were ₅₂ mance relative to using only the unperturbed networks. We ₉₁ matrices with dimensions 83×83 , where each value at loca- $_{53}$ evaluate several techniques for resampling the networks, and $_{92}$ tion (i, j) corresponds to the strength of connection between 54 compare classifiers through their validation performance, the 93 region i and region j. As connections are undirected (i.e. the 55 performance on an out-of-sample test set, and the generaliz- 94 edge (i, j) is equal to the edge (j, i)), the matrices each consist

Perturbations were introduced for the diffusion modelling 58 tion which leads to more robust and generalizable models of 97 of this dataset using sparsely-introduced Monte Carlo Arith-98 metic at the level of machine-precision, simulating expected 99 error over a typical pipeline execution. The MCA workflow 100 was such that each inexact floating-point operation was per-110 making it widely applicable to a variety of pipelines or do-

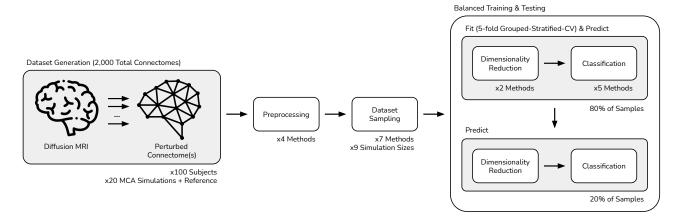


Figure 1. Experiment workflow. MCA-simulated connectomes were previously generated for 100 subjects, 20 times each. The resulting dataset of 2,000 connectomes were independently preprocessed using one of 4 techniques. The dataset was then sampled according to one of 7 dataset sampling strategies and using one of 9 possible number of MCA simulations per subject. The dataset was split into balanced training and testing sets, and fed into the models. The models consisted of one of 2 dimensionality reduction techniques prior to classification using one of 5 classifier types. The models were fit and made predictions on the training set prior to making predictions on the test set.

mains which may suffer a lack of context-specific perturbation 132 Preprocessing 112 or dataset augmentation strategies.

113 119 gation methods in a typical learning context for neuroimag- 140 standard techniques: 120 ing^{29,30}. Exploring the relationship between the number of 121 simulations and performance further allows for the cost of 122 MCA-enabled resampling to be evaluated in the context of 123 dataset augmentation.

125 data strongly implicated in brain connectivity was desired. 126 Participant age, which has consistently been shown to have a 127 considerable impact on brain connectivity 31-34, was selected and turned into a binary target by dividing participants into adult (> 18) and non-adult groups (68% adult). For subse-130 quent validation of findings, body mass index was chosen as 149 **Z-Score** The edge weights were z-scored to have a mean 131 a second target (50% overweight).

133 Prior to being used for this task, the brain networks were rep-This dataset contains a single session of data from 100 ₁₃₄ resented as symmetric 83 × 83 adjacency matrices, sampled individuals ($100 \times 1 \times 1$). The number of subjects included is upon the Desikan-Killiany-Tourville²⁷ anatomical parcella-115 consistent for the types of analyses performed below, and con-136 tion. To reduce redundancy in the data, all edges belonging 116 sidered large in general for neuroimaging²⁸. Each sample was 137 to the upper-triangle of these matrices were preserved and simulated 20 times, resulting in 2,000 unique graphs. This 138 vectorized, resulting in a feature vector of 3,403 edges per 118 collection enabled the exploration of subsampling and aggre- 139 sample. All samples were preprocessed using one of four

> 141 **Raw** The raw streamline count edge-weight intensities were 142 used as originally calculated.

143 **Log Transform** The log10 of edge weights was taken, and As the target for classification, individual-level phenotypic 144 edges with 0 weight prior to the transform were reset to 0.

> 145 **Rank Transform** The edges were ranked based on their in-146 tensity, with the largest edge having the maximum value. Ties 147 were settled by averaging the rank, and all ranks were finally 148 min-max scaled between 0 and 1.

150 intensity of 0 and unit variance.

151 Machine Learning Pipelines

 $_{152}$ The preprocessed connectomes were fed into pipelines consist- $_{188}$ samples, consistent with $_{37}$. 153 ing of two steps: dimensionality reduction and classification. 189 158 applied using one of two methods:

159 **Principal Component Analysis** The connectomes were pro-160 jected into the 20 dimensions of highest variance. The number 161 of components was chosen to capture approximately 90% of 162 the variance present within the dataset.

163 Feature Agglomeration The number of features in each 164 connectome were reduced by combining edges according to 165 maximum similarity/minimum variance using agglomerative 166 clustering³⁵. The number of resulting features was 20, to be 167 consistent with the number of dimensions present after PCA, 168 above.

After dimensionality reduction, samples were fed into 170 one of five distinct classifiers as implemented through scikit 171 learn³⁶:

172 **Support Vector Machine** The model was fit using a radial 209 to the following procedures: basis function (RBF) kernel, L2 penalty, and a balanced regu-174 larization parameter to account for uneven class membership.

175 Logistic Regression A linear solver was used due to the 176 relatively small dataset size. L2 regularization and balanced 213 **Truncate** The number of significant digits²² per-edge was 177 class weights were used, as above.

178 K-Nearest Neighbour Class membership was determined using an L2 distance and the nearest 10% of samples, scaling 180 with the number of samples used for training.

181 Random Forest 100 decision trees were fit using balanced 182 class weights, each splitting the dataset according to a maximum of 4 features per node (corresponding to the rounded 184 square root of 20 total features).

186 tially such that sample weights were iteratively adjusted to 224 lapping sampling of the datasets.

187 prioritize performance on previously incorrectly-classified

The hyperparameters for all models were refined from 154 Given the high dimensionality (3,403 features) of the net-190 their default values to be appropriate for a small and imworks, the relatively small number of samples, and standard balanced dataset. The performance for all pipeline combinapractice in the field^{3,7,9}, no experiments were considered with- 192 tions of preprocessing methods, dimensionality reduction techout dimensionality reduction. Dimensionality reduction was 193 niques, and models using the reference (i.e. unperturbed) exe-194 cutions in the dataset ranged from an F1 score of 0.64–0.875 195 with a mean of 0.806; this evaluation was performed on a 196 consistent held-out test set which was used for all experiments, as described in a following section. This set of models 198 was chosen as it includes i) well understood standard tech-199 niques, ii) both parametric and non-parametric methods, iii) 200 both ensemble and non-ensemble methods, and iv) models 201 which have been commonly deployed for the classification of 202 neuroimaging datasets^{2–4,6,7,31,38,39}

203 Dataset Sampling

204 A chief purpose of this manuscript involves the comparison 205 of various forms of aggregation across equivalently-simulated 206 pipeline outputs. Accordingly, the dataset was resampled 207 after preprocessing but prior to dimensionality reduction and 208 classifiers were trained, evaluated, and combined according

210 **Reference** Networks generated without any MCA pertur-211 bations were selected for input to the models, serving as a 212 benchmark.

214 calculated using all simulated networks, and the edge weights 215 in the reference graph were truncated to the specified number 216 of digits. Importantly, this is the only method used which de-217 liberately squashes the variance observed across simulations.

218 **Jackknife** The datasets were repeatedly sampled such that 219 a single randomly chosen observation of each unique network 220 was selected (i.e. derived from the same input datum). This 221 resampling was performed 100 times, resulting in the total 222 number of resamplings being 5× larger than the number of 185 **AdaBoost** A maximum of 50 decision trees were fit sequen- 223 unique observations per network, ensuring a broad and over226 same network were used as the samples for training and eval- 264 tions from the same individual, relevant for the mega-analysis 227 uation.

Similar to the above, the edgewise mean of all obser-229 vations for each network were computed and used as input 230 data to the classifiers in both collections.

231 **Consensus** A distance-dependent average network⁴⁰ was computed across all observations of each network. This data-233 aware aggregation method, developed for structural brain 234 network analysis, preserves network properties often distorted 235 when computing mean or median networks.

237 simultaneously for classification, increasing the effective sam-238 ple size. Samples were organized such that all observations 239 of the same network only appeared within a single fold for 240 training and evaluation, ensuring double-dipping was avoided. 276

241 **Meta-analysis** Individual classifiers trained across jackknife dataset resamplings, above, were treated as independent mod-243 els and aggregated into an ensemble classifier. The ensemble 244 was fit using a logistic regression classifier across the outputs 245 of the jackknifed classifiers to learn a relationship between 246 the predicted and true class labels.

The robustness and possible benefit of each subsampling 248 approach was measured by evaluation on a subset of all MCA 249 simulations, including 9 distinct numbers of simulations, rang-250 ing from 2 to 20 simulations per sample. Combining the 251 dataset sampling methods, the set of simulations, preprocess-252 ing strategies, dimensionality reduction techniques, and clas-253 sifier models, there were 2,520 perturbed models trained and 254 evaluated next to 40 reference models.

255 Training & Evaluation

²⁵⁶ Prior to training models on the brain networks, 20% of sub- ²⁹³ data to that on unseen data"¹⁹. 257 jects were excluded from each dataset for use as an out-of- 294 258 sample test dataset for all experiments. With the remaining 295 experiments with respect to their reference were used to mea-259 80% of subjects, cross validation was performed following a 296 sure the change in performance for each dataset sampling stratified grouped k-fold approach (k = 5). In this approach, ²⁹⁷ technique, and statistical comparisons were made through samples were divided into training and validation sets such 298 Wilcoxon Signed-Rank tests. 262 that the target variable was proportionally represented on

The edgewise median of all observations of the 263 each side of the fold (stratified), conditional upon all observa-265 dataset sampling method, falling upon the same side of the 266 fold (grouped). This resulted in 5 fold-trained classifiers per 267 configuration, each trained on 64% of the samples and val-268 idated on 16%, prior to each being tested on the remaining 269 20% of held-out samples. All random processes used in deter-270 mining the splits used the same seed to remove the effect of 271 random sampling.

Classifiers were primarily evaluated on both the valida-273 tion and test (out-of-sample) sets using F1 score, a standard 274 measure for evaluating classification performance. The gener-236 **Mega-analysis** All observations of each network were used 275 alizability of predictions was defined as:

$$G = 1 - |F1_{test} - F1_{validation}| \tag{1}$$

where a score of 1 (maximum) indicates the equivalent per-277 formance across both the validation and test sets, and a lower 278 score (minimum of 0) indicates inconsistent performance. The 279 absolute change in performance was used in Eq. 1, resulting 280 in a score which penalizes spurious over-performance simi-281 larly to under-performance. This is a desired attribute of the 282 measure as all inconsistency, whether due to chance or model 283 fit, is undesirable when applying a classifier out-of-sample. ²⁸⁴ Importantly, this measure does not use training performance as the reference, as is common in deep learning, but instead 286 considers the validation performance. This is because training performance is prone to unrealistic inflation due to dataset 288 memorization which may arise in some classifiers; K-Nearest Neighbours is a good example of this. Given that the valida-290 tion performance is typically reported on classic models, this 291 can be considered a practical definition of generalizability, 292 and is still in the spirit of "evaluating performance on seen

Differences in F1 score and generalizability for perturbed

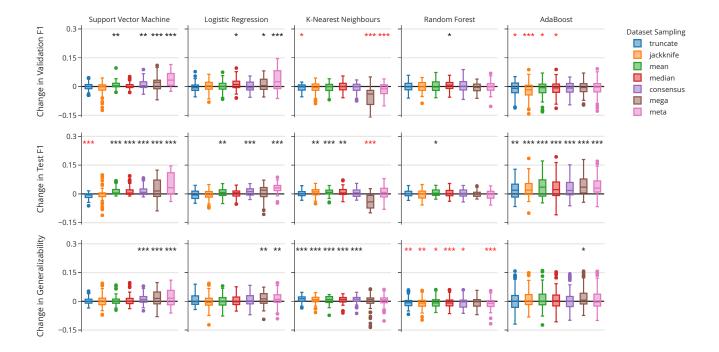


Figure 2. Relative change in classifier performance with respect to classifier type and dataset sampling strategies as measured by change in F1 score on the validation set (top) or test set (middle), as well as the generalizability of performance (bottom). Each star annotation indicates an order of magnitude of statistically significant change, beginning at 0.05 for one star and decreasing from there, with those in black or red indicating an increase or decrease due to resampling, respectively.

300 Results

The figures and findings presented in this section represent a summary of the complete experiment table which consists of performance measures and metadata for all 2,560 models tested. The complete performance table alongside the table of significant differences, are made available through the GitHub repository.

307 Data Resampling Improves Classification

The overall performance of each subsampling method is summarized in Table 1. The change in performance was measured in both cases as a change in F1 score on the validation set, the change in F1 score on the test set, and the change in overall generalizability, a measure which summarizes the similarity between validation and test performance for a given model (Eq. 1).

Across all classifier types it was found that consensus,

mega-, and meta-analytic approaches outperformed other dataset resampling methods. The dataset sampling methods led to improved testing performance and generalizability on

Table 1. Statistically significant change in performance. Red values indicate significant decline in performance, black values indicate improvement, and empty cells indicate no change. A single star represents p < 0.05, and each additional star is an additional order of magnitude of significance.

Dataset Sampling	Validation	Test	Generalizability
Truncate	**		
Jackknife	**	**	
Mean		***	
Median		***	
Consensus		***	*
Mega-Analysis	*	*	***
Meta-Analysis	**	***	*

320 spectively. These results were similar to those found in the 360 ter of the model. At present this parameter was scaled linearly prediction of body mass index, which noted 0.033 and 0.017 361 with the number of MCA simulations used, however, it is both 322 improvements in F1 and generalizability on average, respec- 362 possible that an improved scaling function exists or that the 323 tively. Further detail on the results associated with body mass 363 model performance degrades with large sample sizes making 324 index prediction can be found in Appendix 2. The noted 364 it a poor model choice given this resampling technique. 325 improvement for both tasks is consistent with other dataset 365 augmentation approaches mentioned in the following sec- 366 icant change in validation or testing performance across the 327 tion, which typically report improvements from 0.01–0.1¹⁹. 367 majority of resampling techniques. However, these classifiers 328 In some cases, such as several configurations of AdaBoost 368 did experience a significant decrease in the generalizability 329 classifiers, improvements of up to 0.170 in F1 and 0.150 in 369 of their performance, meaning that there was a larger discrep-330 generalizability were simultaneously observed, with model 370 ancy between training and testing performance in many cases. generalizability peaking at 0.994.

339 networks contains biologically meaningful signal.

342 machine and logistic regression models improve across each 382 the added variability in samples. of the three measures for a variety of dataset sampling tech- 383 344 niques, suggesting that the addition of the MCA-perturbed 384 ality reduction, and classifiers performed more harmoniously 345 samples improves the training, testing, and overall generaliz- 385 than others, there was no significant relationship between the 346 ability of these classifiers.

348 classifiers experienced minimal change in validation and of- 388 above results show that dataset augmentation through MCA-349 ten saw their performance decline. However, the improvement 389 perturbed pipeline outputs may be an effective way to improve 350 of these classifiers on the test set suggests that resampling re- 390 the performance and generalizability of non-ensemble clasduced overfitting in these classifiers. In the case of KNN, this 391 sifiers tasked with modelling brain-phenotype relationships, 352 translates to improved generalizability, while in the case of 392 both within and out of sample, especially when variance is 353 AdaBoost generalizability was largely unchanged, suggesting 393 captured rather than removed. 354 that the model went from underperforming to overperforming after dataset resampling. The unique decline in performance 394 Resampling Leads to Consistent Performance 356 when using the mega-analytic resampling technique on KNN 395 To better characterize the benefit of resampling, the relation-357 classifier is suggestive of poor hyper-parameterization, as 396 ship between the magnitude of improvement and the baseline

are average from 0.773 to 0.812 and from 0.960 to 0.965, re- 359 ratio of the number of samples in the dataset to the k parame-

The random forest classifiers uniquely did not see a signif-This distinction from the other models is possibly due to the The only method which did not improve performance at 372 fact that random forest is a simple ensemble technique which 333 all was the truncation resampling approach. This method 373 takes advantage of training many independent classifiers and 334 was distinct from the others in that the variance observed 374 samples them to assign final class predictions, allowing this across simulations was used to estimate and squash variance 375 approach to form more generalizable predictions, and thus the 336 in the reference network, whether other approaches captured 376 addition of more data does not significantly improve perfor-337 the variance. The finding that truncation hurts performance 377 mance further. While AdaBoost is also an ensemble method, 338 importantly suggests that the variability across the observed 378 the iterative training of models with increasing emphasis on 379 difficult samples allows for the added variance in those sam-The change in performance for each model and dataset 380 ples to play an increasingly central role in the construction of sampling technique is shown in Figure 2. The support vector 381 class relationships, and thus more directly takes advantage of

While certain combinations of preprocessing, dimension-386 performance of any single resampling method and prepro-Distinctly, k-nearest neighbours (KNN) and AdaBoost 387 cessing or dimensionality reduction technique. Overall, the

358 there is a strong relationship between the performance and the 397 performance of the classifier were further explored (Figure 3).

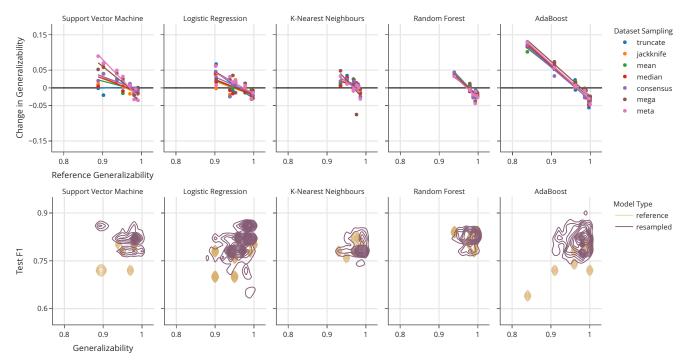


Figure 3. Relationship between generalizability and resampling. Top: change in the generalizability of classifiers with respect to the reference generalizability. Each data point represents the mean change in generalizability for all models using the same preprocessing and dimensionality reduction techniques for a given classifier and dataset sampling strategy. Bottom: contour density distributions of generalizability and F1 scores across all models for both reference and resampled training.

398 We found that the increase in the generalizability of a classifier 416 in the top-right of the shown plots, the dataset resampling 399 was inversely related to the baseline generalizability (Figure 3; 417 techniques consistently shift the distributions in this direction 400 top). In other words, the less generalizable a classifier was 418 and often improve classifiers along one or both of these axes. 401 originally, the more its generalizability improved (significant 419 Importantly, the variance in performance across both mea- $_{402}$ at p < 0.05 for all dataset sampling strategies and classifier $_{420}$ sures is significantly decreased, suggesting that resampling 403 other than KNN). There were several situations in which the 421 leads to more reliable and reproducible classifiers. 404 generalizability of models were noted to decrease, however, 405 though this only occurred for models with high generalizabil- 422 Number of Simulations is Largely Unimpactful 406 ity scores (all > 0.935). Importantly, the relative change in 423 While we previously noted an increase in classifier perfor-407 generalizability shifts scores towards a single "mode", sug- 424 mance due to perturbation-enabled dataset resampling, it was 408 gesting a less biased estimate of the true generalizability of 425 important to explore the relationship between the number of 409 performance on the task, and mitigating both under- and over- 426 simulated samples and performance (Figure 4). There was no 410 performance due to chance.

412 alizability (Figure 3; bottom), it becomes apparent that even 430 In the case of the mega-analytic approach, however, there was 413 for the majority of models which may not have improved 431 a significant positive relationship between the number of sam-414 performance along both axes, either their generalizability or 432 ples used and the generalizability of performance, though

427 relationship between the number of independent simulations and performance, as measured by either F1 or generalizability, When exploring the relationship between F1 and gener- 429 for all dataset resampling techniques other than mega-analysis. 415 F1 score is improved. While an ideal classifier would reside 433 there remained no increase in F1 score. The mega-analysis

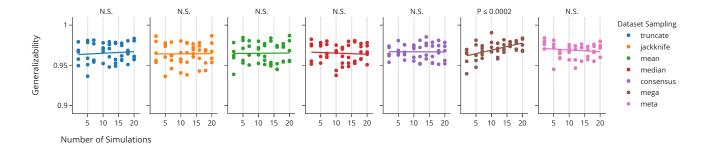


Figure 4. The generalizability of classifiers using each dataset sampling technique with respect to the number of MCA simulations. Each number of simulations was sampled a single time, to avoid artificial skewing of the dataset due to the inclusion of "higher" or "lower" quality samples; a single drawing of each split mimics a true perturbation experiment context.

495 samples being provided directly to the classifiers, thus mimics 462 results obtained through MCA is valuable and signal-rich it-496 an increase in sample size for traditional experiments. While 463 self, and an important determination of performance is the 437 outlying samples may play a small role in many of the pro- 464 inclusion of this variability. Recent work has demonstrated 438 posed forms of resampling, or non-existent in the median case, 465 another impactful source of variability in machine learning 499 the mega analytic approach treats all simulations with equal 466 benchmark performance, namely the initialization and pa-440 importance as unique samples in the dataset. In this case, the 467 rameterization of models⁴¹. Our studies reached a common 441 relationship we observe is consistent to what one might expect 468 conclusion, which is that model performance can be improved 442 when increasing the number of samples.

Discussion

445 The numerical perturbation of analytic pipelines provides a 447 for dataset augmentation. Using a technique such as MCA, 448 samples can be simulated across an array of controlled exe-449 cutions and used to enrich datasets with a range of plausible 450 results per sample. We demonstrate that this method of dataset augmentation can be used to improve the training, testing, and 452 generalizability of classifiers.

Through the training and evaluation of 2,560 models com-454 bining varying strategies for preprocessing, dimensionality 455 reduction, classifier, and resampling, we found consistent im-456 provement across all measured axes. Interestingly, while there 483

494 approach is the only approach which changes the number of 461 result importantly demonstrates that the added variability in 469 by considering a variety of individually-biased estimators. 470 These results are both elegant realizations of the bias-variance 471 trade-off⁴².

While the non-ensemble methods benefited most obviunique, data-agnostic, and computationally unintrusive method 473 ously from the dataset resampling strategies, where both F1 474 and generalizability were often improved, the results pre-475 sented in Figure 3 demonstrate that variability in performance 476 across both of these axes was reduced across all classifier 477 configurations. While a reduction in the variability of per-478 formance is desirable in itself, this figure also illustrates that 479 the performance of resulting models converges around the 480 more performant models in the case of all classifiers. The ⁴⁸¹ reduction in variability also results in models which differed 482 less significantly when looking across classifier types.

Although performance was improved by the integration of 457 was a statistically significant improvement when using many 484 MCA simulated samples, performance was not significantly 458 dataset resampling techniques, there was no significant im- 485 related to the number of simulations used in any case other 459 provement in the performance, and in fact a reduction, using 466 than the mega-analytic resampling strategy. The independence 460 the truncation resampling method as is shown in Table 1. This 487 of performance and number of simulations is encouraging, as

⁴⁸⁸ a key limitation for using Monte Carlo methods is the often ⁵²⁸ be poorly described in the resulting dataset ⁴⁶. 489 extreme computational overhead. The ability to use a small 529 490 number of simulations and achieve equivalent performance 530 in favour of dataset augmentation through numerical pertur-491 through the majority of resampling techniques allows for sig-531 bations, the improvement from these methods has not been 492 nificantly better performance without added data collection 532 directly compared to additional data acquisitions in this exper-493 and only a theoretical doubling the sample processing time. 593 iment due to the limited sample size of the available perturbed ⁴⁹⁴ The benefit of increasing the number of simulations in the ⁵⁵⁴ dataset²⁵. Previous studies exploring the effect of sample size 495 mega-analytic case could be considered an analog to increas- 595 on neuroimaging classification tasks have shown that vari-496 ing the sample size of an experiment. While the range of 596 ability in performance decreases with sample size 47, where 497 simulations used here demonstrated a consistent improvement 597 a doubling of sample size from 100 to 200 approximately 498 in generalizability, there will be a plateau in performance, 598 corresponded to halving the uncertainty in performance 43. 499 either at a perfect score or, more likely, before this is reached. 539 However, this decrease in variability is often accompanied 500 Further work is required for characterizing the relationship 540 by a decrease in out of sample performance in practice⁴⁸. A 501 between the performance of mega-analytic resampling and the 541 meta-analysis across 69 studies showed that increasing sample soz number of simulations, though it is likely that this relationship staz size was negatively related to out-of-sample performance⁴⁹, 503 will be domain-specific and dependent on other experimental 543 where accuracy was noted to decline by approximately 5% in 504 design variables such as the number of features per sample. 544 a similar doubling from 100 to 200 samples, suggesting that

511 performance near chance or near perfect. Characterizing the 551 from increased data collection. 512 behaviour of this technique across a range of classification 552 513 contexts and performances would shed light on whether this 553 the unbalanced nature of datasets. When using a nearest-514 technique could be applied globally or if it is limited to mak- 554 neighbour classifier, for instance, a dramatic difference in the 515 ing "good" models better.

₅₁₇ lead to uncertainty in modelling⁴³. This is generally planned ₅₅₇ balanced sampling is not possible, such as when considering 518 for in one of two ways: the collection of vast datasets, as is 558 a rare clinical population, perturbation-augmented datasets 519 the case in the UK-BioBank which strives to collect samples 559 could be applied for realistic upsampling of data. In this case, 520 from half a million individuals¹⁵, or the collection of repeated 550 a mega-analytic aggregation strategy could be used in which 521 measurements from the selected samples, as is the case in the 561 more simulations would be performed for members of the 522 Consortium of Reliability and Reproducibility which orches- 562 under-represented class, similar to the balancing of weights 523 trates multiple centres and scanners, each collecting multiple 563 applicable to some models. This application is particularly ₅₂₄ acquisitions¹⁶. In either case, the additional data collection by ₅₆₄ important, as upsampling is often challenging in biological 525 these initiatives is both financially and temporally expensive 565 contexts where realistic simulation models are sparse. 526 and leads to unintended confounding effects associated with 566

While the results presented here provide strong evidence While our study shows that classifiers with poorer baseline 545 a major contribution of increasing sample size in neuroimag-506 performance benefit more from augmentation, an important 546 ing is a reduction in overfitting which must occur prior to a 507 limitation of this is the operating point to which that claim 547 possible boost in performance. Our finding that MCA-based 508 remains true. For example, it is unlikely that the trend ob- 548 dataset augmentation reduced overfitting and improved upon 509 served here for a task with a mean reference performance 549 baseline performance is encouraging, and suggests that mod-510 of 0.81 would hold across models operating with reference 550 els trained using such perturbed datasets may benefit more

A common issue in many machine learning contexts is 555 membership of each group could have significant impact on It is a well understood problem that small sample sizes 556 model hyper-parameters and performance. In contexts where

The presented dataset augmentation technique was not 527 time of day⁴⁴, weather⁴⁵, or other off-target variables that may 567 compared directly to other strategies due to a lack of readily

570 lished which performed dataset augmentation on structural 609 All software developed for processing or evaluation is publicly ple sclerosis patients on binarized connectivity graphs²¹. This 611 2021AggregateMCA. Experiments were launched on Com-573 work adapted a generative adversarial network (GAN) archi- 612 pute Canada's HPC cluster environment. 574 tecture, a structure that is commonly used in other domains $_{575}$ of data augmentation. Published applications using $_{GANs}$ $_{613}$ Author Contributions 576 or other deep learning approaches for image data augmenta- 614 GK was responsible for the experimental design, data process-577 tion have reported increases in classification accuracy from $578 \ 0.01 - 0.1^{19}$. Given the average improvement in performance of 0.04 presented here, MCA-based augmentation can be considered consistent with the other types of data augmentation 581 when used for classification. The data-agnostic and training-582 free nature of the MCA approach also enables this technique 583 to be combined with other forms of dataset enhancement, such 584 as directly in GANS or through the addition of realistic noise, 585 when available. MCA has not been tested for other common 586 applications of data augmentation, such as object detection or 587 segmentation.

Conclusion

590 This work demonstrates the benefit of augmenting datasets 591 through numerical perturbations. We present an approach 592 which leverages the numerical instability inherent to pipelines 629 **References** 593 for creating more accurate and generalizable classifiers. While 630 594 the approach and results demonstrated here were specifically 595 relevant in the context of brain imaging, the data-agnostic 596 method for inducing perturbations and off-the-shelf machine 597 learning techniques used suggest that this approach may be 635 598 widely applicable across domains. This work uniquely shows 599 that numerical uncertainty is an asset which can be harnessed 600 to increase the signal captured from datasets and lead to more 601 robust learned relationships.

602 Data & Code Availability

603 The perturbed connectomes were publicly available in a data 604 resource previously produced and made available by the authors 25 . They can be found persistently at https://doi. $_{646}$ $^{[5]}$ M. Zhang, C. Desrosiers, Y. Guo, B. Khundrakpam, N. Al-Sharif, 606 org/10.5281/zenodo.4041549, and are made avail- 647

568 available alternatives. Through a literature search, shown in 607 able through The Canadian Open Neuroscience Platform 569 Appendix 1, it was found that only a single paper was pub- 608 (https://portal.conp.ca/search, search term "Kiar"). 571 connectomics data, specifically for the classification of multi- 610 available on GitHub at https://github.com/gkpapers/

615 ing, analysis, interpretation, and the majority of writing. All 616 authors contributed to the revision of the manuscript. TG and 617 ACE contributed to experimental design, analysis, interpre-618 tation. The authors declare no competing interests for this 619 work. Correspondence and requests for materials should be ad-620 dressed to Gregory Kiar at gregory.kiar@childmind.

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641

- [1] C.-W. Woo, L. J. Chang, M. A. Lindquist, and T. D. Wager, "Building better biomarkers: brain models in translational neuroimaging," Nature neuroscience, vol. 20, no. 3, p. 365, 2017.
- N. A. Crossley, A. Mechelli, J. Scott, F. Carletti, P. T. Fox, P. McGuire, and E. T. Bullmore, "The hubs of the human connectome are generally implicated in the anatomy of brain disorders," Brain, vol. 137, no. Pt 8, pp. 2382-2395, Aug. 2014.
- S. Payabvash, E. M. Palacios, J. P. Owen, M. B. Wang, T. Tavassoli, M. Gerdes, A. Brandes-Aitken, D. Cuneo, E. J. Marco, and P. Mukherjee, "White matter connectome edge density in children with autism spectrum disorders: Potential imaging biomarkers using Machine-Learning models," Brain Connect., vol. 9, no. 2, pp. 209-220, Mar. 2019.
- E. Tolan and Z. Isik, "Graph theory based classification of brain connectivity network for autism spectrum disorder," in Bioinformatics and Biomedical Engineering. Springer International Publishing, 2018, pp. 520-530.
- G. Kiar, P. Valdes-Sosa, J.-B. Poline, and A. Evans, "Brain status mod-

- eling with non-negative projective dictionary learning," Neuroimage, p. 695 116226, Oct. 2019.
- K. Zhu, X. Du, M. Kerich, F. W. Lohoff, and R. Momenan, "Random forest based classification of alcohol dependence patients and healthy controls using resting state MRI," Neurosci. Lett., vol. 676, pp. 27–33,
 May 2018.

648

649

- B.-Y. Park, J. Seo, J. Yi, and H. Park, "Structural and functional brain
 connectivity of people with obesity and prediction of body mass index
 using connectivity," <u>PLoS One</u>, vol. 10, no. 11, p. e0141376, Nov. 2015.
- B. S. Wade, S. H. Joshi, B. A. Gutman, and P. M. Thompson, "Machine learning on high dimensional shape data from subcortical brain surfaces:
 A comparison of feature selection and classification methods," <u>Pattern</u>
 <u>Recognition</u>, vol. 63, pp. 731–739, 2017.
- S. Weis, K. R. Patil, F. Hoffstaedter, A. Nostro, B. T. Yeo, and S. B. Eickhoff, "Sex classification by resting state brain connectivity," <u>Cerebral</u> cortex, vol. 30, no. 2, pp. 824–835, 2020.
- B. C. Munsell, C.-Y. Wee, S. S. Keller, B. Weber, C. Elger, L. A. T. 712
 da Silva, T. Nesland, M. Styner, D. Shen, and L. Bonilha, "Evaluation of 713
 machine learning algorithms for treatment outcome prediction in patients 714 [24]
 with epilepsy based on structural connectome data," Neuroimage, vol. 715
 118, pp. 219–230, 2015.
- R. Botvinik-Nezer, F. Holzmeister, C. F. Camerer, A. Dreber, J. Huber, 717
 M. Johannesson, M. Kirchler, R. Iwanir, J. A. Mumford, R. A. Adcock 718 [25]
 et al., "Variability in the analysis of a single neuroimaging dataset by 719
 many teams," Nature, pp. 1–7, 2020.
- A. Bowring, C. Maumet, and T. E. Nichols, "Exploring the impact of 721 analysis software on task fMRI results," <u>Human brain mapping</u>, vol. 40, 722 no. 11, pp. 3362–3384, 2019.
- A. Salari, G. Kiar, L. Lewis, A. C. Evans, and T. Glatard, "File-based localization of numerical perturbations in data analysis pipelines,"

 GigaScience, vol. 9, no. 12, 12 2020, giaa106.
- G. Kiar, Y. Chatelain, P. de Oliveira Castro, E. Petit, and others, "Numerical instabilities in analytical pipelines lead to large and meaningful variability in brain networks," bioRxiv, 2020.
- C. Sudlow, J. Gallacher, N. Allen, V. Beral, P. Burton, J. Danesh, 731
 P. Downey, P. Elliott, J. Green, M. Landray et al., "UK biobank: an open 732
 access resource for identifying the causes of a wide range of complex 733
 diseases of middle and old age," Plos med, vol. 12, no. 3, p. e1001779, 734
 2015.
- X.-N. Zuo, J. S. Anderson, P. Bellec, R. M. Birn, B. B. Biswal, 736 [30]
 J. Blautzik, J. C. Breitner, R. L. Buckner, V. D. Calhoun, F. X. Castel-737
 lanos et al., "An open science resource for establishing reliability and 738
 reproducibility in functional connectomics," Scientific data, vol. 1, no. 1, 739 [31]
 pp. 1–13, 2014.
- J. Nalepa, M. Marcinkiewicz, and M. Kawulok, "Data augmentation 741 for brain-tumor segmentation: a review," Frontiers in computational 742 neuroscience, vol. 13, p. 83, 2019.

- M. S. Graham, I. Drobnjak, and H. Zhang, "Realistic simulation of artefacts in diffusion MRI for validating post-processing correction techniques," <u>NeuroImage</u>, vol. 125, pp. 1079–1094, 2016.
- [19] C. Shorten and T. M. Khoshgoftaar, "A survey on image data augmentation for deep learning," <u>Journal of Big Data</u>, vol. 6, no. 1, pp. 1–48, 2019.
- [20] X. Yi, E. Walia, and P. Babyn, "Generative adversarial network in medical imaging: A review," <u>Medical image analysis</u>, vol. 58, p. 101552, 2019.
- [21] B. Barile, A. Marzullo, C. Stamile, F. Durand-Dubief, and D. Sappey-Marinier, "Data augmentation using generative adversarial neural networks on brain structural connectivity in multiple sclerosis," <u>Computer</u> Methods and Programs in Biomedicine, vol. 206, p. 106113, 2021.
- 708 [22] D. S. Parker, Monte Carlo Arithmetic: exploiting randomness in
 709 floating-point arithmetic. University of California (Los Angeles). Com710 puter Science Department, 1997.
 - [23] C. Denis, P. de Oliveira Castro, and E. Petit, "Verificarlo: Checking floating point accuracy through Monte Carlo Arithmetic," <u>2016 IEEE</u> <u>23nd Symposium on Computer Arithmetic (ARITH)</u>, 2016.
- [24] G. Kiar, P. de Oliveira Castro, P. Rioux, E. Petit, S. T. Brown, A. C.
 Evans, and T. Glatard, "Comparing perturbation models for evaluating stability of neuroimaging pipelines," <u>The International Journal of High</u>
 Performance Computing Applications, 2020.
- [25] G. Kiar, "Numerically perturbed structural connectomes from 100 individuals in the NKI Rockland dataset," Apr. 2020.
- [26] E. Garyfallidis, M. Brett, B. Amirbekian, A. Rokem, S. van der Walt, M. Descoteaux, I. Nimmo-Smith, and Dipy Contributors, "Dipy, a library for the analysis of diffusion MRI data," <u>Front. Neuroinform.</u>, vol. 8, p. 8, Feb. 2014.
- [27] A. Klein and J. Tourville, "101 labeled brain images and a consistent human cortical labeling protocol," <u>Front. Neurosci.</u>, vol. 6, p. 171, Dec. 2012.
- D. Szucs and J. P. Ioannidis, "Sample size evolution in neuroimaging research: An evaluation of highly-cited studies (1990–2012) and of latest practices (2017–2018) in high-impact journals,"

 NeuroImage, vol. 221, p. 117164, 2020. [Online]. Available: https:
 //www.sciencedirect.com/science/article/pii/S1053811920306509
 - [29] S. I. Dimitriadis, M. Drakesmith, S. Bells, G. D. Parker, D. E. Linden, and D. K. Jones, "Improving the reliability of network metrics in structural brain networks by integrating different network weighting strategies into a single graph," 2017.
 - [30] C. R. Buchanan, C. R. Pernet, K. J. Gorgolewski, A. J. Storkey, and M. E. Bastin, "Test–retest reliability of structural brain networks from diffusion MRI," Neuroimage, vol. 86, pp. 231–243, Feb. 2014.
 - T. B. Meier, A. S. Desphande, S. Vergun, V. A. Nair, J. Song, B. B. Biswal, M. E. Meyerand, R. M. Birn, and V. Prabhakaran, "Support vector machine classification and characterization of age-related reorganization of functional brain networks," <u>Neuroimage</u>, vol. 60, no. 1, pp. 601–613, Mar. 2012.

- K. Wu, Y. Taki, K. Sato, S. Kinomura, R. Goto, K. Okada, R. Kawashima, 792
 Y. He, A. C. Evans, and H. Fukuda, "Age-related changes in topolog- 793
 ical organization of structural brain networks in healthy individuals," 794
 Hum. Brain Mapp., vol. 33, no. 3, pp. 552–568, Mar. 2012. 795
- [33] S. Y. Bookheimer, D. H. Salat, M. Terpstra, B. M. Ances, D. M. Barch, 796
 R. L. Buckner, G. C. Burgess, S. W. Curtiss, M. Diaz-Santos, J. S. 797 [46]
 Elam, B. Fischl, D. N. Greve, H. A. Hagy, M. P. Harms, O. M. Hatch, 798
 T. Hedden, C. Hodge, K. C. Japardi, T. P. Kuhn, T. K. Ly, S. M. Smith, 799
 L. H. Somerville, K. Uğurbil, A. van der Kouwe, D. Van Essen, R. P. 800
 Woods, and E. Yacoub, "The lifespan Human Connectome Project in 801
 aging: An overview," Neuroimage, vol. 185, pp. 335–348, Jan. 2019.
- T. Zhao, M. Cao, H. Niu, X.-N. Zuo, A. Evans, Y. He, Q. Dong, and 803
 N. Shu, "Age-related changes in the topological organization of the 804
 white matter structural connectome across the human lifespan," Hum. 805
 Brain Mapp., vol. 36, no. 10, pp. 3777–3792, 2015.
- J. H. Ward, "Hierarchical grouping to optimize an objective function," 807 [48]
 Journal of the American Statistical Association, vol. 58, no. 301, pp. 808
 236–244, 1963. 809
- F. Pedregosa, G. Varoquaux, A. Gramfort, V. Michel, B. Thirion, 810 [49]
 O. Grisel, M. Blondel, P. Prettenhofer, R. Weiss, V. Dubourg, and Oth-811
 ers, "Scikit-learn: Machine learning in Python," the Journal of machine
 Learning research, vol. 12, pp. 2825–2830, 2011.
- Y. Freund and R. E. Schapire, "A Decision-Theoretic generalization of 814
 On-Line learning and an application to boosting," <u>J. Comput. System</u>
 <u>Sci.</u>, vol. 55, no. 1, pp. 119–139, Aug. 1997.
- B. Tunç, B. Solmaz, D. Parker, T. D. Satterthwaite, M. A. Elliott, M. E.
 Calkins, K. Ruparel, R. E. Gur, R. C. Gur, and R. Verma, "Establishing
 a link between sex-related differences in the structural connectome
 and behaviour," Philos. Trans. R. Soc. Lond. B Biol. Sci., vol. 371, no.
 1688, p. 20150111, Feb. 2016.
- D. R. Nayak, R. Dash, and B. Majhi, "Brain MR image classification using two-dimensional discrete wavelet transform and AdaBoost with
 Random Forests," Neurocomputing, vol. 177, pp. 188–197, Feb. 2016.
- R. F. Betzel, A. Griffa, P. Hagmann, and B. Misic, "Distance-dependent consistency thresholds for generating group-representative structural brain networks," bioRxiv, 2018.
- X. Bouthillier, P. Delaunay, M. Bronzi, A. Trofimov, B. Nichyporuk,
 J. Szeto, N. Mohammadi Sepahvand, E. Raff, K. Madan, V. Voleti et al.,
 "Accounting for variance in machine learning benchmarks," <u>Proceedings</u>
 of Machine Learning and Systems, vol. 3, 2021.
- 784 ^[42] S. Geman, E. Bienenstock, and R. Doursat, "Neural networks and the bias/variance dilemma," <u>Neural computation</u>, vol. 4, no. 1, pp. 1–58, 1992.
- G. Varoquaux, "Cross-validation failure: small sample sizes lead to large error bars," Neuroimage, vol. 180, pp. 68–77, 2018.
- G. Vandewalle, S. N. Archer, C. Wuillaume, E. Balteau, C. Degueldre,
 A. Luxen, P. Maquet, and D.-J. Dijk, "Functional magnetic resonance
 imaging-assessed brain responses during an executive task depend on

- interaction of sleep homeostasis, circadian phase, and per3 genotype," Journal of Neuroscience, vol. 29, no. 25, pp. 7948–7956, 2009.
- X. Di, M. Wolfer, S. Kühn, Z. Zhang, and B. B. Biswal, "Estimations of the weather effects on brain functions using functional mri–a cautionary tale," bioRxiv, p. 646695, 2019.
- L. Chaddock, K. I. Erickson, R. S. Prakash, J. S. Kim, M. W. Voss, M. VanPatter, M. B. Pontifex, L. B. Raine, A. Konkel, C. H. Hillman et al., "A neuroimaging investigation of the association between aerobic fitness, hippocampal volume, and memory performance in preadolescent children," <u>Brain research</u>, vol. 1358, pp. 172–183, 2010.
- O. C. Chu, A.-L. Hsu, K.-H. Chou, P. Bandettini, C. Lin, A. D. N. Initiative et al., "Does feature selection improve classification accuracy? impact of sample size and feature selection on classification using anatomical magnetic resonance images," <u>Neuroimage</u>, vol. 60, no. 1, pp. 59–70, 2012.
- [48] H. G. Schnack and R. S. Kahn, "Detecting neuroimaging biomarkers for psychiatric disorders: sample size matters," <u>Frontiers in psychiatry</u>, vol. 7, p. 50, 2016.
- A. A. Pulini, W. T. Kerr, S. K. Loo, and A. Lenartowicz, "Classification accuracy of neuroimaging biomarkers in attention-deficit/hyperactivity disorder: Effects of sample size and circular analysis," <u>Biological Psychiatry</u>: Cognitive Neuroscience and Neuroimaging, vol. 4, no. 2, pp. 108–120, 2019.

Appendix 1: Dataset Augmentation in Diffusion MRI Connectomics

817 To demonstrate the sparsity of existing applications and techniques which have been developed for dataset augmentation in network neuroscience, a PubMed query (Figure 5) was run and the results were explored. The query was performed on May 819 28th, 2021, and the results are discussed below with the complete results file published in this project's GitHub repository. The 820 results of this query indicated:

• 13 total papers which were flagged as relevant.

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- 5 of which were related to dataset augmentation, with the other 8 having been incorrectly flagged as relevant and were either focused on clinical practice, non-human data, or analyzed relationships between structural and functional networks.
 - 4 of which were related to some modality of MRI, the other 1 focusing on high resolution CT imaging.
- 1 of which was focused on improving classification performance through dataset augmentation, with the remaining 3 either centered on applications in transfer learning across datasets of different quality, leveraging T1w MRI data for age prediction, or improving segmentation of MR perfusion images of stroke patients.

The sole paper²¹ which closely mirrored the focal application and demonstrates how a novel generative adversarial network was used to improve the classification of multiple sclerosis patients from healthy controls. This paper demonstrated an improvement in F1 score from 0.66 to 0.81. This technique used binary structural connectivity networks for disease prediction using a dataset containing 48 patients.

((diffusion MRI) OR (diffusion weighted imaging) OR (dwi) OR (dMRI) OR (d-MRI) OR (diffusion Imaging))

AND (brain)

AND ((network) OR (connectome) OR (structural connectome))

AND ((data augmentation) OR (dataset augmentation))

Figure 5. Demonstrative PubMed query to identify papers which apply dataset augmentation in network neuroscience.

Appendix 2: Augmentation Improvement in a BMI Classification Task

To validate that the observed benefit of using Monte Carlo Arithmetic-derived networks wasn't only found in the specific age classification task tested, we reproduced a body mass index (BMI) classification task⁷. The experimental configuration shown here was identical to the above, with the class labels assigned via a threshold of BMI > 25, which is consistent with examples from the literature⁷.

One key distinction from the age classification task was that the majority of models in the BMI classification task did not perform statistically better than chance using the reference networks. While 36/40 combinations of network preprocessing, dimensionality reduction, and classifier type produced a model which was meaningfully better than chance for the age classification task without dataset augmentation, only 10/40 reference models were significant for the BMI task. The performance for all models was still included in the following analysis in the interest of consistency.

Table 2. Statistically significant change in performance for body mass index classification. Red values indicate significant decline in performance, black values indicate improvement, and empty cells indicate no change. A single star represents p < 0.05, and each additional star is an additional order of magnitude of significance.

Dataset Sampling	Validation	Test	Generalizability
Truncate		*	***
Jackknife		***	***
Mean		*	*
Median		*	**
Consensus		***	**
Mega-Analysis	***	***	*
Meta-Analysis	***	***	**

Table 2 shows statistically significant change for each dataset augmentation technique aggregated across all models used for body mass index classification. Similarly to the results presented in the main body of this article, the mega- and meta-analytic techniques were superior to the others, and resulted in improvements in model performance both within and out of sample, alongside improving the generalizability in performance. For these two techniques, the performance improved from 0.590 to 0.623 on average, with an improvement in generalizability from 0.921 to 0.939. In the case of the other dataset sampling strategies, it was noted that the performance decreased while the generalizability increased for each configuration. This suggests that models were "over-performing" prior to the data augmentation, and resampling networks served as a regularization. When considering these summaries alongside Figure 6, we can see that the noted decrease in test performance was likely driven by the significant reduction in performance of the AdaBoost models while noting an improvement of generalizability suggests a previous over-performance of models built using this classifier type. Figure 7 also shows consistent results to those presented above, in which the generalizability trends towards a "central" score, and that the dataset sampling approaches tend to shift the model performance either towards increased F1, generalizability, or both.

The classifiers and more generally model combinations which performed the best given dataset augmentation via MCA varied across the two experiments, and it is important to note that this was expected and does not change the significance of the presented findings. The purpose of this work was not to design an ideal experimental configuration that was uniformly out-performing another, but demonstrate the efficacy of MCA as a dataset augmentation technique, in particular for domains in which alternatives may not exist more generally.

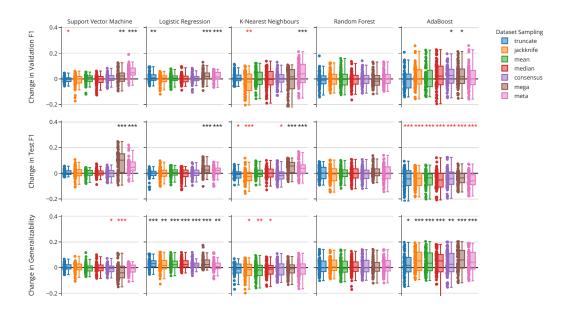


Figure 6. Relative change in classifier performance with respect to classifier type and dataset sampling strategies as measured by change in F1 score on the validation set (top) or test set (middle), as well as the generalizability of performance (bottom) for the body mass index classification task. Each star annotation indicates an order of magnitude of statistically significant change, beginning at 0.05 for one star and decreasing from there, with those in black or red indicating an increase or decrease due to resampling, respectively.

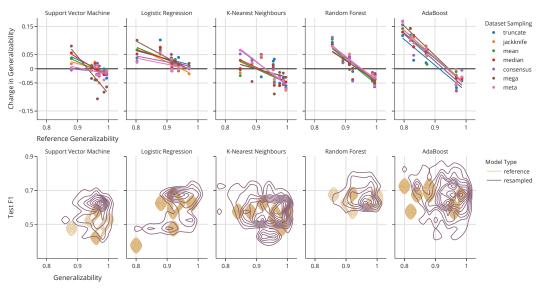


Figure 7. Relationship between generalizability and resampling. Top: change in the generalizability of classifiers with respect to the reference generalizability. Each data point represents the mean change in generalizability for all models using the same preprocessing and dimensionality reduction techniques for a given classifier and dataset sampling strategy. Bottom: contour density distributions of generalizability and F1 scores across all models for both reference and resampled training.