Numerical Instabilities in Analytical Pipelines Lead to Large and Meaningful Variability in Brain Networks

Gregory Kiar¹, Yohan Chatelain², Pablo de Oliveira Castro³, Eric Petit⁴, Ariel Rokem⁵, Gaël Varoquaux⁶, Bratislav Misic¹, Alan C. Evans^{1†}, Tristan Glatard^{2†}

The analysis of brain-imaging data requires complex and often non-linear transformations to support findings on brain function or pathologies. And yet, recent work has shown that variability in the choices that one makes when analyzing data can lead to quantitatively and qualitatively different results, endangering the trust in conclusions¹⁻³. Even within a given method or analytical technique, numerical instabilities could compromise findings^{4–7}. We instrumented a structural-connectome estimation pipeline with Monte Carlo Arithmetic^{8,9}, a technique to introduce random noise in floating-point computations, and evaluated the stability of the derived connectomes, their features^{10,11}, and the impact on a downstream analysis^{12,13}. The stability of results was found to be highly dependent upon which features of the connectomes were evaluated, and ranged from perfectly stable (i.e. no observed variability across executions) to highly unstable (i.e. the results contained no trustworthy significant information). While the extreme range and variability in results presented here could severely hamper our understanding of brain organization in brain-imaging studies, it also leads to an increase in the reliability of datasets. This paper highlights the potential of leveraging the induced variance in estimates of brain connectivity to reduce the bias in networks alongside increasing the robustness of their applications in the detection or classification of individual differences. This paper demonstrates that stability evaluations are necessary for understanding error and bias inherent to scientific computing, and that they should be a component of typical analytical workflows.

Keywords

Stability — Reproducibility — Network Neuroscience — Neuroimaging

¹Montréal Neurological Institute, McGill University, Montréal, QC, Canada; ²Department of Computer Science and Software Engineering, Concordia University, Montréal, QC, Canada; ³ Department of Computer Science, Université of Versailles, Versailles, France; ⁴ Exascale Computing Lab, Intel, Paris, France; 5 Department of Psychology and eScience Institute, University of Washington, Seattle, WA, USA; ⁶ Parietal project-team, INRIA Saclay-ile de France, France; †Authors contributed equally.

- 2 has shaped our understanding of the structure and function 8 topathies", such as Alzhiemer's Disease and Schizophrenia, 3 of the brain across a variety of organisms and scales over 9 but potentially pave the way for therapeutics 19-23. 4 the last decade 11,14–18. In humans, these wiring diagrams are 5 obtained in vivo through Magnetic Resonance Imaging (MRI), 11 plex computational methods and software. Tools are trusted to
- The modelling of brain networks, called connectomics, 7 This can not only improve understanding of so-called "connec-
- However, the analysis of brain imaging data relies on com-6 and show promise towards identifying biomarkers of disease. 12 perform everything from pre-processing tasks to downstream

¹⁴ rigorous evaluation on bespoke datasets, in the absence of ⁵⁰ either the inputs or throughout the pipelines^{4,9}. The pipelines 15 ground-truth this is often evaluated through measures of re- 51 were sampled 20 times per collection and once without per-16 liability^{24–27}, proxy outcome statistics, or agreement with 52 turbations, resulting in a total of 4,200 connectomes. 17 existing theory. Importantly, this means that tools are not 18 necessarily of known or consistent quality, and it is not un-19 common that equivalent experiments may lead to diverging 20 conclusions^{1,5–7}. While many scientific disciplines suffer 21 from a lack of reproducibility²⁸, this was recently explored 22 in brain imaging by a 70 team consortium which performed 23 equivalent analyses and found widely inconsistent results¹, 24 and it is likely that software instabilities played a role.

The present study approached evaluating reproducibility 26 from a computational perspective in which a series of brain 27 imaging studies were numerically perturbed such that the 28 plausibility of results was not affected, and the biological 29 implications of the observed instabilities were quantified. We 30 accomplished this through the use of Monte Carlo Arithmetic 31 (MCA)⁸, a technique which enables characterization of the 32 sensitivity of a system to small perturbations. We explored 33 the impact of perturbations through the direct comparision 34 of structural connectomes, the consistency of their features, 35 and their eventual application in a neuroscience study. Finally 36 we conclude on the consequences and opportunities afforded 37 by the observed instabilities and make recommendations for 38 the roles stability analyses may play towards increasing the 39 reliability of brain imaging research.

40 Graphs Vary Widely With Perturbations

41 Prior to exploring the analytic impact of instabilities, a direct 78 average of 3 significant digits across all groups, demonstrat-42 understanding of the induced variability was required. A sub- 79 ing a significant limitation in the reliability independent edge 44 dataset²⁹ was randomly selected to contain 25 individuals with 81 single digit per edge in any case, indicating that only the 45 two sessions of imaging data, each of which was subsampled 82 magnitude of edges in naively computed groupwise average 46 into two components, resulting in four collections per individ- 83 connectomes can be trusted. The combination of these results 47 ual. Structural connectomes were generated with canonical 84 with those presented in Figure 1A suggests that while specific

18 statistical evaluation. While these tools undoubtedly undergo 49 strumented with MCA, replicating computational noise at

The stability of connectomes was evaluated through the 54 deviation from reference and the number of significant digits 55 (Figure 1). The comparisons were grouped according to dif-56 ferences across simulations, subsampling of data, sessions of 57 acquisition, or subjects. While the similarity of connectomes 58 decreases as the collections become more distinct, connec-59 tomes generated with input perturbations show considerable 60 variability, often reaching deviations equal to or greater than 61 those observed across individuals or sessions (Figure 1A; 62 right). This finding suggests that instabilities inherent to 63 these pipelines may mask session or individual differences, 64 limiting the trustworthiness of derived connectomes. While 65 both pipelines show similar performance, the probabilistic 66 pipeline was more stable in the face of pipeline perturbations 67 whereas the deterministic was more stable to input perturbations (p < 0.0001 for all; exploratory). The stability of 69 correlations can be found in Supplemental Section S1.

The number of significant digits per edge across connec-71 tomes (Figure 1B) similarly decreases across groups. While 72 the cross-MCA comparison of connectomes generated with 73 pipeline perturbations show nearly perfect precision for many 74 edges (approaching the maximum of 15.7 digits for 64-bit 75 data), this evaluation uniquely shows considerable drop off $_{76}$ in performance across data subsampling (average of < 4 dig-77 its). In addition, input perturbations show no more than an 45 set of the Nathan Kline Institute Rockland Sample (NKIRS) 80 weights. Significance across individuals did not exceed a 48 deterministic and probabilistic pipelines^{30,31} which were in- 85 edge weights are largely affected by instabilities, macro-scale

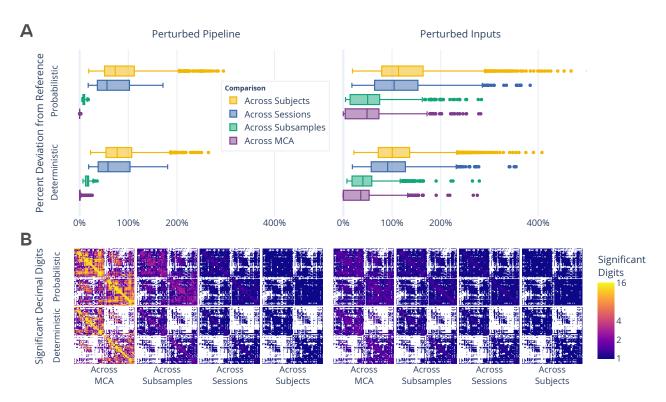


Figure 1. Exploration of perturbation-induced deviations from reference connectomes. (A) The absolute deviations, in the form of normalized percent deviation from reference, shown as the across MCA series relative to Across Subsample, Across Session, and Aross Subject variations. (B) The number of significant decimal digits in each set of connectomes as obtained after evaluating the effect of perturbations. In the case of 16, values can be fully relied upon, whereas in the case of 1 only the first digit of a value can be trusted. Pipeline- and input-perturbations are shown on the left and right, respectively.

86 network topology is stable.

Biases Are Reduced

89 We assessed the reproducibility of the dataset through mimick-90 ing and extending a typical test-retest experiment²⁶ in which 91 the similarity of samples across multiple measurements were 92 compared to distinct samples in the dataset (Table 1, with 93 additional experiments and explanation in Supplemental Sec- 108 94 tion S2). The ability to separate connectomes across subjects 109 identification of brain networks, it is similarly reliant on net-95 (Hypothesis 1) is an essential prerequisite for the applica- 110 work similarity across equivalent acquisitions (Hypothesis 2). 96 tion of brain imaging towards identifying individual differ- 111 In this case, connectomes were grouped based upon session, ₉₇ ences¹⁸. In testing hypothesis 1, we observe that the dataset ₁₁₂ rather than subject, and the ability to distinguish one session ₉₈ is separable with a score of 0.64 and 0.65 (p < 0.001; opti- ₁₁₃ from another was computed within-individual and aggregated.

100 However, we can see that inducing instabilities through MCA 101 improves the reliability of the dataset to over 0.75 in each 87 Subject-Specific Signal is Amplified While Off-Target 102 case (p < 0.001 for all), significantly higher than without instrumentation (p < 0.005 for all). This result impactfully 104 suggests the utility of perturbation methods for synthesizing 105 robust and reliable individual estimates of connectivity, serv-106 ing as a cost effective and context-agnostic method for dataset 107 augmentation.

While the separability of individuals is essential for the 99 mal score: 1.0; chance: 0.04) without any instrumentation. 114 Both the unperturbed and pipeline perturbation settings per-

Table 1. The impact of instabilities as evaluated through the separability of the dataset based on individual (or subject) differences, session, and subsample. The performance is reported as mean Discriminability. While a perfectly separable dataset would be represented by a score of 1.0, the chance performance, indicating minimal separability, is 1/the number of classes. H_3 could not be tested using the reference executions due to too few possible comparisons. The alternative hypothesis, indicating significant separation, was accepted for all experiments, with p < 0.005.

			Reference Execution		Perturbed Pipeline		Perturbed Inputs	
Comparison	Chance	Target	Det.	Prob.	Det.	Prob.	Det.	Prob.
H ₁ : Across Subjects	0.04	1.0	0.64	0.65	0.82	0.82	0.77	0.75
H_2 : Across Sessions	0.5	0.5	1.00	1.00	1.00	1.00	0.88	0.85
<i>H</i> ₃ : Across Subsamples	0.5	0.5			0.99	1.00	0.71	0.61

with a score of 1.0 (p < 0.005; optimal score: 0.5; chance: 142 of individual connectivity. 117 0.5), indicating a dominant session-dependent signal for all 143 118 individuals despite no intended biological differences. How- 144 amplification of meaningful biological signal alongside a re-119 ever, while still significant relative to chance (score: 0.85 145 duction of off-target signal. This result appears strikingly like and 0.88; p < 0.005 for both), input perturbations lead to 146 a manifestation of the well-known bias-variance tradeoff³² significantly lower separability of the dataset (p < 0.005 for 147 in machine learning, a concept which observes a decrease in 122 all). This reduction of the difference between sessions of data 148 bias as variance is favoured by a model. In particular, this 123 within individuals suggests that increased variance caused 149 highlights that numerical perturbations can be used to not by input perturbations reduces the impact of non-biological 150 only evaluate the stability of pipelines, but that the induced acquisition-dependent bias inherent in the brain graphs.

127 uate the interaction between the dataset and tool, the use of 128 subsampling allowed for characterizing the separability of 153 Distributions of Graph Statistics Are Reliable, But 129 networks sampled from within a single acquisition (Hypoth- 154 Individual Statistics Are Not 130 esis 3). While this experiment could not be evaluated using 155 Exploring the stability of topological features of connectomes 131 reference executions, the executions performed with pipeline 156 is relevant for typical analyses, as low dimensional features are 132 perturbations showed near perfect separation between sub- 157 often more suitable than full connectomes for many analytical samples, with scores of 0.99 and 1.0 (p < 0.005; optimal: 158 methods in practice 11. A separate subset of the NKIRS dataset 134 0.5; chance: 0.5). Given that there is no variability in data 159 was randomly selected to contain a single non-subsampled 185 acquisition or preprocessing that contributes to this reliable 160 session for 100 individuals, and connectomes were generated 136 identification of scans, the separability observed in this exper- 161 as above. 137 iment may only be due to instability or bias inherent to the 162 198 pipelines. The high variability introduced through input per- 163 features 10 was explored in Figure 2. The cumulative den-199 turbations considerably lowered the reliability towards chance 164 sity of the features was computed within individuals and the

115 fectly preserved differences between cross-sectional sessions 141 this as an effective method for obtaining lower-bias estimates

Across all cases, the induced perturbations showed an 151 variance may be leveraged for the interpretation as a robust Though the previous sets of experiments inextricably eval- 152 distributions of possible results.

The stability of several commonly-used multivariate graph 140 (score: 0.71 and 0.61; p < 0.005 for all), further supporting 165 mean density and associated standard error were computed

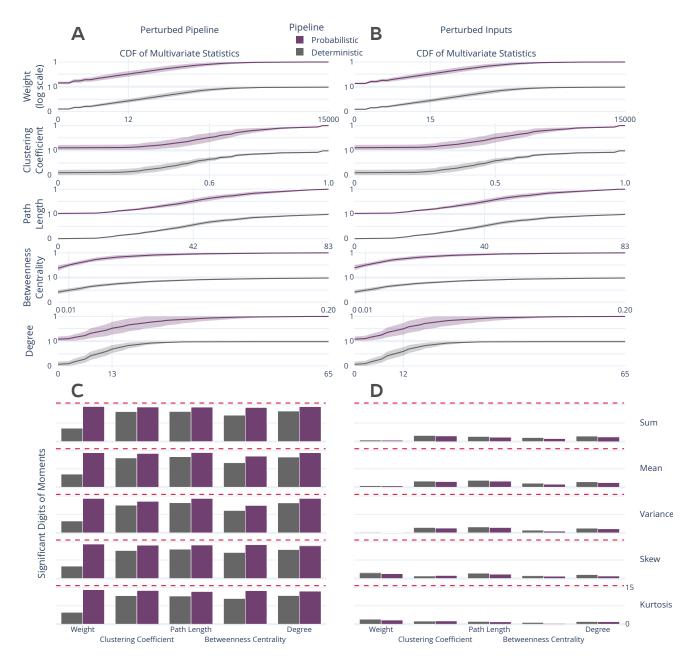


Figure 2. Distribution and stability assessment of multivariate graph statistics. (**A**, **B**) The cumulative distribution functions of multivariate statistics across all subjects and perturbation settings. There was no significant difference between the distributions in A and B. (**C**, **D**) The number of significant digits in the first 5 five moments of each statistic across perturbations. The dashed red line refers to the maximum possible number of significant digits.

In addition to the comparison of distributions, the stabil167 nificant difference beetween the distributions for each feature 172 ity of the first 5 moments of these features was evaluated 168 across the two perturbation settings, suggesting that the topo- 173 (Figures 2C and 2D). In the face of pipeline perturbations, 169 logical features summarized by these multivariate features are 174 the feature-moments were stable with more than 10 signifi170 robust across both perturbation modes. 175 cant digits with the exception of edge weight when using the

more stable for all comparisons (p < 0.0001; exploratory). 213 elling brain-phenotype relationships is not possible, but rather 178 In stark contrast, input perturbations led to highly unstable 214 it sheds light on impactful uncertainty that must be accounted 179 feature-moments (Figure 2D), such that none contained more 215 for in this process, and supports the use of ensemble modeling 180 than 5 significant digits of information and several contained 216 techniques. 181 less than a single significant digit, indicating a complete lack 182 of reliability. This dramatic degradation in stability for in- 217 Discussion dividual measures strongly suggests that these features may 218 The perturbation of structural connectome estimation pipelines 184 be unreliable as individual biomarkers when derived from a 219 with small amounts of noise, on the order of machine error, single pipeline evaluation, though their reliability may be in- 220 led to considerable variability in derived brain graphs. Across 186 creased when studying their distributions across perturbations. 221 all analyses the stability of results ranged from nearly per-187 A similar analysis was performed for univariate statistics and 222 fectly trustworthy (i.e. no variation) to completely unreliable 188 can be found in Supplemental Section S3.

189 Uncertainty in Brain-Phenotype Relationships

190 While the variability of connectomes and their features was 191 summarized above, networks are commonly-used as inputs to machine learning models tasked with learning brain-phenotype 193 relationships 18. To explore the stability of these analyses, we 194 modelled the relationship between high- or low- Body Mass 195 Index (BMI) groups and brain connectivity 12,13, using stan-196 dard dimensionality reduction and classification tools, and 197 compared this to reference and random performance (Fig-198 ure 3).

The analysis was perturbed through distinct samplings of 200 the dataset across both pipelines and perturbation methods. 201 The accuracy and F1 score for the perturbed models varied 202 from 0.520 - 0.716 and 0.510 - 0.725, respectively, rang-203 ing from at or below random performance to outperforming 209 **Underestimated False Positive Rates** While the instabil-204 performance on the reference dataset. This large variability 240 ity of brain networks was used here to demonstrate the lim-205 illustrates a previously uncharacterized margin of uncertainty 241 itations of modelling brain-phenotype relationships in the 206 in the modelling of this relationship, and limits confidence in 242 context of machine learning, this limitation extends to classi-208 portion of explained variance in these samples ranged from 244 comparisons in a hypothesis testing framework will be accom-200 88.6% — 97.8%, similar to the reference, suggesting that the 245 panied by reported false positive rates, the accuracy of these 210 range in performance was not due to a gain or loss of mean- 246 rates is critically dependent upon the reliability of the samples

176 deterministic pipeline, though the probabilistic pipeline was 212 outcome. Importantly, this finding does not suggest that mod-

223 (i.e. containing no trustworthy information). Given that the 224 magnitude of introduced numerical noise is to be expected 225 in typical settings, this finding has potentially significant im-226 plications for inferences in brain imaging as it is currently 227 performed. In particular, this bounds the success of studying ²²⁸ individual differences, a central objective in brain imaging ¹⁸, 229 given that the quality of relationships between phenotypic 230 data and brain networks will be limited by the stability of the 231 connectomes themselves. This issue was accentuated through 232 the crucial finding that individually derived network features ²³³ were unreliable despite there being no significant difference 234 in their aggregated distributions. This finding is not damn-235 ing for the study of brain networks as a whole, but rather is 236 strong support for the aggregation of networks, either across 237 perturbations for an individual or across groups, over the use 238 of individual estimates.

reported accuracy scores on singly processed datasets. The 243 cal hypothesis testing, as well. Though performing individual 211 ingful signal, but rather the reduction of bias towards specific 247 used. In reality, the true false positive rate for a test would be

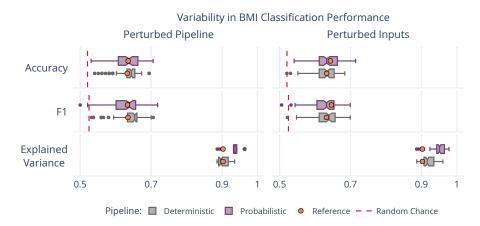


Figure 3. Variability in BMI classification across the sampling of an MCA-perturbed dataset. The dashed red lines indicate random-chance performance, and the orange dots show the performance using the reference executions.

248 a combination of the reported confidence and the underlying 272 pensive collection of repeated measurements choreographed ₂₇₃ by massive cross-institutional consortia^{34,35}. The finding that 249 variability in the results, a typically unknown quantity. When performing these experiments outside of a repeated- 274 perturbing experiments using MCA both increased the relia-250 251 measure context, such as that afforded here through MCA, it 275 bility of the dataset and decreased off-target differences across 252 is impossible to empirically estimate the reliability of samples. 276 acquisitions opens the door for a promising paradigm shift. 253 This means that the reliability of accepted hypotheses is also 277 Given that MCA is data-agnostic, this technique could be used 254 unknown, regardless of the reported false positive rate. In 278 effectively in conjunction with, or in lieu of, realistic noise 255 fact, it is a virtual certainty that the true false positive rate 279 models to augment existing datasets. While this of course 256 for a given hypothesis exceeds the reported value simply as 280 would not replace the need for repeated measurements when 257 a result of numerical instabilities. This uncertainty inherent 281 exploring the effect of data collection paradigm or study lon-258 to derived data is compounded with traditional arguments 282 gitudinal progressions of development or disease, it could be 259 limiting the trustworthiness of claims³³, and hampers the 283 used in conjunction with these efforts to increase the reliabil-260 ability of researchers to evaluate the quality of results. The 284 ity of each distinct sample within a dataset. In contexts where accompaniment of brain imaging experiments with direct 285 repeated measurements are collected to increase the fidelity of 262 evaluations of their stability, as was done here, would allow 286 the dataset, MCA could potentially be employed to increase 263 researchers to simultaneously improve the numerical stability 287 the reliability of the dataset and save millions of dollars on of their analyses and accurately gauge confidence in them. 288 data collection. This technique also opens the door for the 265 The induced variability in derived brain networks may be 289 characterization of reliability across axes which have been 266 leveraged to estimate aggregate connectomes with lower bias 290 traditionally inaccessible. For instance, in the absence of a 267 than any single independent observation, leading to learned 291 realistic noise model or simulation technique similar to MCA, 268 relationships that are more generalizable and ultimately more 292 the evaluation of network stability across data subsampling 293 would not have been possible. 269 useful.

270 **Cost-Effective Data Augmentation** The evaluation of reli- 294 **Shortcomings and Future Questions** Given the complex-271 ability in brain imaging has historically relied upon the ex- 295 ity of recompiling complex software libraries, pre-processing was not perturbed in these experiments. Other work has shown that linear registration, a core piece of many elements of prethat linear registration, a core piece of many elements of preprocessing such as motion correction and alignment, is sensitive to minor perturbations. It is likely that the instabilities
tive to minor perturbations, it is likely that the instabilities
that the instabilities with one another, resulting in even greater variability. While
the analyses performed in this paper evaluated a single dataset
and set of pipelines, extending this work to other modalities
and analyses is of interest for future projects.

This paper does not explore methodological flexibility or 344 compare this to numerical instability. Recently, the nearly 345 someone in brain imaging has been clearly demonstrated. The 348 approach taken in these studies complement one another and 349 explore instability at the opposite ends of the spectrum, with 350 some one end and the unavoidable error implicit in the digital 351 representation of data on the other. It is of extreme interest 354 to combine these approaches and explore the interaction of 355 these scientific degrees of freedom with effects from software 356 implementations, libraries, and parametric choices.

Finally, it is important to state explicitly that the work presented here does not invalidate analytical pipelines used in 360 [9] brain imaging, but merely sheds light on the fact that many 361 studies are accompanied by an unknown degree of uncertainty due to machine-introduced errors. The presence of unknown 363 [10] error-bars associated with experimental findings limits the 365 impact of results due to increased uncertainty. The desired 366 [11] outcome of this paper is to motivate a shift in scientific com-367 puting – particularly in neuroimaging – towards a paradigm 368 which favours the explicit evaluation of the trustworthiness of 369 [12] claims alongside the claims themselves.

328 References

R. Botvinik-Nezer, F. Holzmeister, C. F. Camerer, A. Dreber, J. Huber, 374
M. Johannesson, M. Kirchler, R. Iwanir, J. A. Mumford, R. A. Adcock 375

et al., "Variability in the analysis of a single neuroimaging dataset by 376
many teams," *Nature*, pp. 1–7, 2020.

- [2] C. M. Bennett, M. B. Miller, and G. L. Wolford, "Neural correlates of interspecies perspective taking in the post-mortem Atlantic salmon: An argument for multiple comparisons correction," *Neuroimage*, vol. 47, no. Suppl 1, p. S125, 2009.
- ^[3] A. Eklund, T. E. Nichols, and H. Knutsson, "Cluster failure: Why fMRI inferences for spatial extent have inflated false-positive rates," *Proceedings of the national academy of sciences*, vol. 113, no. 28, pp. 7900–7905, 2016.
- G. Kiar, P. de Oliveira Castro, P. Rioux, E. Petit, S. T. Brown, A. C.
 Evans, and T. Glatard, "Comparing perturbation models for evaluating
 stability of neuroimaging pipelines," *The International Journal of High Performance Computing Applications*, 2020.
 - [5] A. Salari, G. Kiar, L. Lewis, A. C. Evans, and T. Glatard, "File-based localization of numerical perturbations in data analysis pipelines," arXiv preprint arXiv:2006.04684, 2020.
 - E. B. Lewis, C. Y. Lepage, N. Khalili-Mahani, M. Omidyeganeh, S. Jeon, P. Bermudez, A. Zijdenbos, R. Vincent, R. Adalat, and A. C. Evans, "Robustness and reliability of cortical surface reconstruction in CIVET and FreeSurfer," *Annual Meeting of the Organization for Human Brain Mapping*, 2017.
 - T. Glatard, L. B. Lewis, R. Ferreira da Silva, R. Adalat, N. Beck, C. Lepage, P. Rioux, M.-E. Rousseau, T. Sherif, E. Deelman, N. Khalili-Mahani, and A. C. Evans, "Reproducibility of neuroimaging analyses across operating systems," *Front. Neuroinform.*, vol. 9, p. 12, Apr. 2015.
 - [8] D. S. Parker, Monte Carlo Arithmetic: exploiting randomness in floating-point arithmetic. University of California (Los Angeles). Computer Science Department, 1997.
 - [9] C. Denis, P. de Oliveira Castro, and E. Petit, "Verificarlo: Checking floating point accuracy through monte carlo arithmetic," 2016 IEEE 23nd Symposium on Computer Arithmetic (ARITH), 2016.
 - R. F. Betzel, A. Griffa, P. Hagmann, and B. Mišić, "Distance-dependent consensus thresholds for generating group-representative structural brain networks," *Network neuroscience*, vol. 3, no. 2, pp. 475–496, 2019.
 - M. Rubinov and O. Sporns, "Complex network measures of brain connectivity: uses and interpretations," *Neuroimage*, vol. 52, no. 3, pp. 1059–1069, Sep. 2010.
 - B.-Y. Park, J. Seo, J. Yi, and H. Park, "Structural and functional brain connectivity of people with obesity and prediction of body mass index using connectivity," *PLoS One*, vol. 10, no. 11, p. e0141376, Nov. 2015.
- A. Gupta, E. A. Mayer, C. P. Sanmiguel, J. D. Van Horn, D. Woodworth,
 B. M. Ellingson, C. Fling, A. Love, K. Tillisch, and J. S. Labus, "Patterns of brain structural connectivity differentiate normal weight from overweight subjects," *Neuroimage Clin*, vol. 7, pp. 506–517, Jan. 2015.
- et al., "Variability in the analysis of a single neuroimaging dataset by 376 [14] T. E. Behrens and O. Sporns, "Human connectomics," *Current opinion* many teams," *Nature*, pp. 1–7, 2020. 377 in neurobiology, vol. 22, no. 1, pp. 144–153, 2012.

- M. Xia, Q. Lin, Y. Bi, and Y. He, "Connectomic insights into topologi- 422 [31]
 cally centralized network edges and relevant motifs in the human brain," 423

 Frontiers in human neuroscience, vol. 10, p. 158, 2016.
- J. L. Morgan and J. W. Lichtman, "Why not connectomics?" *Nature methods*, vol. 10, no. 6, p. 494, 2013.
- M. P. Van den Heuvel, E. T. Bullmore, and O. Sporns, "Comparative connectomics," *Trends in cognitive sciences*, vol. 20, no. 5, pp. 345–361, 2016.
- J. Dubois and R. Adolphs, "Building a science of individual differences from fMRI," *Trends Cogn. Sci.*, vol. 20, no. 6, pp. 425–443, Jun. 2016.
- A. Fornito and E. T. Bullmore, "Connectomics: a new paradigm for understanding brain disease," *European Neuropsychopharmacology*, vol. 25, no. 5, pp. 733–748, 2015.
- G. Deco and M. L. Kringelbach, "Great expectations: using wholebrain computational connectomics for understanding neuropsychiatric disorders," *Neuron*, vol. 84, no. 5, pp. 892–905, 2014.
- T. Xie and Y. He, "Mapping the alzheimer's brain with connectomics," *Frontiers in psychiatry*, vol. 2, p. 77, 2012.
- M. Filippi, M. P. van den Heuvel, A. Fornito, Y. He, H. E. H. Pol, 441 [37]
 F. Agosta, G. Comi, and M. A. Rocca, "Assessment of system dys- 442
 function in the brain through mri-based connectomics," *The Lancet* 443
 Neurology, vol. 12, no. 12, pp. 1189–1199, 2013.
- M. P. Van Den Heuvel and A. Fornito, "Brain networks in schizophrenia," 445 [38]
 Neuropsychology review, vol. 24, no. 1, pp. 32–48, 2014.
- J. J. Bartko, "The intraclass correlation coefficient as a measure of reliability," *Psychol. Rep.*, vol. 19, no. 1, pp. 3–11, Aug. 1966.
- A. M. Brandmaier, E. Wenger, N. C. Bodammer, S. Kühn, N. Raz, and U. Lindenberger, "Assessing reliability in neuroimaging research through intra-class effect decomposition (ICED)," *Elife*, vol. 7, Jul. 2018.
- E. W. Bridgeford, S. Wang, Z. Yang, Z. Wang, T. Xu, C. Craddock,
 J. Dey, G. Kiar, W. Gray-Roncal, C. Coulantoni *et al.*, "Eliminating
 accidental deviations to minimize generalization error: applications in
 connectomics and genomics," *bioRxiv*, p. 802629, 2020.
- G. Kiar, E. Bridgeford, W. G. Roncal, V. Chandrashekhar, and others, "A High-Throughput pipeline identifies robust connectomes but troublesome variability," *bioRxiv*, 2018.
- 414 [28] M. Baker, "1,500 scientists lift the lid on reproducibility," *Nature*, 2016.
- K. B. Nooner, S. J. Colcombe, R. H. Tobe, M. Mennes *et al.*, "The 461 NKI-Rockland sample: A model for accelerating the pace of discovery 462 science in psychiatry," *Front. Neurosci.*, vol. 6, p. 152, Oct. 2012.
- E. Garyfallidis, M. Brett, B. Amirbekian, A. Rokem, S. van der Walt, 464
 M. Descoteaux, I. Nimmo-Smith, and Dipy Contributors, "Dipy, a library 465 [43]
 for the analysis of diffusion MRI data," *Front. Neuroinform.*, vol. 8, p. 8, 466
 Feb. 2014.

- [31] E. Garyfallidis, M. Brett, M. M. Correia, G. B. Williams, and I. Nimmo-Smith, "QuickBundles, a method for tractography simplification," *Front. Neurosci.*, vol. 6, p. 175, Dec. 2012.
- S. Geman, E. Bienenstock, and R. Doursat, "Neural networks and the bias/variance dilemma," *Neural computation*, vol. 4, no. 1, pp. 1–58, 1992.
- J. P. Ioannidis, "Why most published research findings are false," *PLoS medicine*, vol. 2, no. 8, p. e124, 2005.
- D. C. Van Essen, S. M. Smith, D. M. Barch, T. E. Behrens, E. Yacoub,
 K. Ugurbil, W.-M. H. Consortium *et al.*, "The WU-Minn human connectome project: an overview," *Neuroimage*, vol. 80, pp. 62–79, 2013.
- J. Blautzik, J. C. Breitner, R. L. Buckner, V. D. Calhoun, F. X. Castellanos *et al.*, "An open science resource for establishing reliability and reproducibility in functional connectomics," *Scientific data*, vol. 1, no. 1, pp. 1–13, 2014.
- M. Jenkinson, C. F. Beckmann, T. E. J. Behrens, M. W. Woolrich, and
 S. M. Smith, "FSL," *Neuroimage*, vol. 62, no. 2, pp. 782–790, Aug.
 2012.
 - [37] J. L. Lancaster, D. Tordesillas-Gutiérrez, M. Martinez, F. Salinas, A. Evans, K. Zilles, J. C. Mazziotta, and P. T. Fox, "Bias between mni and talairach coordinates analyzed using the icbm-152 brain template," *Human brain mapping*, vol. 28, no. 11, pp. 1194–1205, 2007.
 - [38] A. Klein and J. Tourville, "101 labeled brain images and a consistent human cortical labeling protocol," *Front. Neurosci.*, vol. 6, p. 171, Dec. 2012.
 - D. Sohier, P. De Oliveira Castro, F. Févotte, B. Lathuilière, E. Petit, and O. Jamond, "Confidence intervals for stochastic arithmetic," Jul. 2018.
- J. Benesty, J. Chen, Y. Huang, and I. Cohen, "Pearson correlation coefficient," in *Noise Reduction in Speech Processing*, I. Cohen, Y. Huang,
 J. Chen, and J. Benesty, Eds. Berlin, Heidelberg: Springer Berlin
 Heidelberg, 2009, pp. 1–4.
- 454 [41] C. A. Raji, A. J. Ho, N. N. Parikshak, J. T. Becker, O. L. Lopez, L. H.
 455 Kuller, X. Hua, A. D. Leow, A. W. Toga, and P. M. Thompson, "Brain
 456 structure and obesity," *Hum. Brain Mapp.*, vol. 31, no. 3, pp. 353–364,
 457 Mar. 2010.
- T. Glatard, G. Kiar, T. Aumentado-Armstrong, N. Beck, P. Bellec,
 R. Bernard, A. Bonnet, S. T. Brown, S. Camarasu-Pop, F. Cervenansky,
 S. Das, R. Ferreira da Silva, G. Flandin, P. Girard, K. J. Gorgolewski,
 C. R. G. Guttmann, V. Hayot-Sasson, P.-O. Quirion, P. Rioux, M.-É.
 Rousseau, and A. C. Evans, "Boutiques: a flexible framework to integrate command-line applications in computing platforms," *Gigascience*,
 vol. 7, no. 5, May 2018.
 - [43] G. Kiar, S. T. Brown, T. Glatard, and A. C. Evans, "A serverless tool for platform agnostic computational experiment management," *Front. Neuroinform.*, vol. 13, p. 12, Mar. 2019.

$Numerical\ Instabilities\ in\ Analytical\ Pipelines\ Lead\ to\ Large\ and\ Meaningful\ Variability\ in\ Brain\ Networks\ --\ 10/18$

```
_{\rm 468} ^{\rm [44]}~ H. Huang and M. Ding, "Linking functional connectivity and structural
```

ity, vol. 6, no. 2, pp. 99–108, 2016.

connectivity quantitatively: a comparison of methods," Brain connectiv-

Methods

472 Dataset

473 The Nathan Kline Institute Rockland Sample (NKI-RS)²⁹ 474 dataset contains high-fidelity imaging and phenotypic data 475 from over 1,000 individuals spread across the lifespan. A 476 subset of this dataset was chosen for each experiment to both 477 match sample sizes presented in the original analyses and to 478 minimize the computational burden of performing MCA. The 479 selected subset comprises 100 individuals ranging in age from $_{480}$ 6 – 79 with a mean of 36.8 (original: 6 – 81, mean 37.8), 481 60% female (original: 60%), with 52% having a BMI over 25 482 (original: 54%).

Each selected individual had at least a single session 484 of both structural T1-weighted (MPRAGE) and diffusion-485 weighted (DWI) MR imaging data. DWI data was acquired 486 with 137 diffusion directions; more information regarding the acquisition of this dataset can be found in the NKI-RS data 488 release²⁹.

In addition to the 100 sessions mentioned above, 25 indi-490 viduals had a second session to be used in a test-retest analysis. ⁴⁹¹ Two additional copies of the data for these individuals were 492 generated, including only the odd or even diffusion directions $_{493}$ (64 + 9 B0 volumes = 73 in either case). This allowed for an 495 levels of MCA and session-level variation.

 $_{499}$ 100 sessions of full-resolution data from 100 individuals for $_{535}$ rounding is performed on a value x at precision t by: 500 subsequent analyses.

501 Processing

507 ing was performed on full-resolution sessions, ensuring that 508 an additional confound was not introduced in this process 509 when comparing between downsampled sessions. The pre-510 processing described here was performed once without MCA, and thus is not being evaluated.

Structural connectomes were generated from preprocessed data using two canonical pipelines from Dipy³⁰: deterministic 514 and probabilistic. In the deterministic pipeline, a constant 515 solid angle model was used to estimate tensors at each voxel and streamlines were then generated using the EuDX algo-517 rithm³¹. In the probabilistic pipeline, a constrained spherical 518 deconvolution model was fit at each voxel and streamlines 519 were generated by iteratively sampling the resulting fiber ori-520 entation distributions. In both cases tracking occurred with 8 seeds per 3D voxel and edges were added to the graph based 522 on the location of terminal nodes with weight determined by 523 fiber count.

The random state of the probabilistic pipeline was fixed 525 for all analyses. Fixing this random seed allowed for explicit 526 attribution of observed variability to Monte Carlo simulations rather than internal state of the algorithm.

528 Perturbations

529 All connectomes were generated with one reference execu-494 extra level of stability evaluation to be performed between the 530 tion where no perturbation was introduced in the processing. 531 For all other executions, all floating point operations were In total, the dataset is composed of 100 downsampled 532 instrumented with Monte Carlo Arithmetic (MCA)⁸ through sessions of data originating from 50 acquisitions and 25 in- 533 Verificarlo 9. MCA simulates the distribution of errors im-498 dividuals for in depth stability analysis, and an additional 534 plicit to all instrumented floating point operations (flop). This

$$inexact(x) = x + 2^{e_x - t}\xi \tag{1}$$

 $_{502}$ The dataset was preprocessed using a standard FSL 36 work- $_{536}$ where e_x is the exponent value of x and ξ is a uniform ranflow consisting of eddy-current correction and alignment. The 537 dom variable in the range $(-\frac{1}{2},\frac{1}{2})$. MCA can be introduced in MNI152 atlas³⁷ was aligned to each session of data, and the re- 538 two places for each flop: before or after evaluation. Performsulting transformation was applied to the DKT parcellation³⁸. 539 ing MCA on the inputs of an operation limits its precision, 506 Downsampling the diffusion data took place after preprocess- 540 while performing MCA on the output of an operation high542 referred to as Precision Bounding (PB) and the latter is called 578 ture and severity of instabilities through each of these lenses. 543 Random Rounding (RR).

Using MCA, the execution of a pipeline may be performed 580 Wilcoxon signed-rank tests. 545 many times to produce a distribution of results. Studying the 546 distribution of these results can then lead to insights on the 547 stability of the instrumented tools or functions. To this end, 548 a complete software stack was instrumented with MCA and is made available on GitHub at https://github.com/ 550 gkiar/fuzzy.

Both the RR and PB variants of MCA were used indepen-552 dently for all experiments. As was presented in⁴, both the 553 degree of instrumentation (i.e. number of affected libraries) and the perturbation mode have an effect on the distribution 555 of observed results. For this work, the RR-MCA was ap-556 plied across the bulk of the relevant libraries and is referred 557 to as Pipeline Perturbation. In this case the bulk of numerical 558 operations were affected by MCA.

Conversely, the case in which PB-MCA was applied across 560 the operations in a small subset of libraries is here referred 561 to as Input Perturbation. In this case, the inputs to operations within the instrumented libraries (namely, Python and Cython) ses were perturbed, resulting in less frequent, data-centric pertur-564 bations. Alongside the stated theoretical differences, Input 565 Perturbation is considerably less computationally expensive 566 than Pipeline Perturbation.

All perturbations were targeted the least-significant-bit for all data (t = 24 and t = 53 in float32 and float64, re-569 spectively⁹). Simulations were performed 20 times for each 602 standard deviation across graphs, respectively. The upper pipeline execution. A detailed motivation for the number of 603 bound on significant digits is 15.7 for 64-bit floating point simulations can be found in³⁹.

572 Evaluation

573 The magnitude and importance of instabilities in pipelines 607 thereby removing any subject- and session-effects and provid-574 can be considered at a number of analytical levels, namely: 608 ing a direct measure of the tool-introduced variability across 575 the induced variability of derivatives directly, the resulting 609 perturbations. A distribution was formed by aggregating these 576 downstream impact on summary statistics or features, or the 610 individual results.

541 lights round-off errors that may be introduced. The former is 577 ultimate change in analyses or findings. We explore the na-579 Unless otherwise stated, all p-values were computed using

581 Direct Evaluation of the Graphs

582 The differences between simulated graphs was measured di-583 rectly through both a direct variance quantification and a 584 comparison to other sources of variance such as individual-585 and session-level differences.

586 Quantification of Variability Graphs, in the form of adja-587 cency matrices, were compared to one another using three 588 metrics: normalized percent deviation, Pearson correlation, 589 and edgewise significant digits. The normalized percent devi-⁵⁹⁰ ation measure, defined in⁴, scales the norm of the difference between a simulated graph and the reference execution (that 592 without intentional perturbation) with respect to the norm of 593 the reference graph. The purpose of this comparison is to 594 provide insight on the scale of differences in observed graphs relative to the original signal intensity. A Pearson correlation 596 coefficient⁴⁰ was computed in complement to normalized per-597 cent deviation to identify the consistency of structure and not 598 just intensity between observed graphs.

Finally, the estimated number of significant digits, s', for 600 each edge in the graph is calculated as:

$$s' = -\log_{10} \frac{\sigma}{|\mu|} \tag{2}$$

where μ and σ are the mean and unbiased estimator of 604 data.

The percent deviation, correlation, and number of signifi-606 cant digits were each calculated within a single session of data, 611 Class-based Variability Evaluation To gain a concrete un- 644 H_{A2} : Sessions within an individual are distinct 612 derstanding of the significance of observed variations we ex- 645 613 plore the separability of our results with respect to understood 646 614 sources of variability, such as subject-, session-, and pipeline-615 level effects. This can be probed through Discriminability²⁶. 616 a technique similar to ICC²⁴ which relies on the mean of a 617 ranked distribution of distances between observations belong-618 ing to a defined set of classes. The discriminability statistic is 619 formalized as follows:

$$Disc. = Pr(\|g_{ij} - g_{ij'}\| \le \|g_{ij} - g_{i'j'}\|)$$
(3)

at observation j, where $i \neq i'$ and $j \neq j'$.

observation belonging to a given class will be more similar to 658 explored the stability of several commonly-used univariate 624 other observations within that class than observations of a dif- 659 (graphwise) and multivariate (nodewise or edgewise) features. 625 ferent class. It is a measure of reproducibility, and is discussed 660 The features computed and subsequent methods for compari-626 in detail in 26. This definition allows for the exploration of 661 son in this section were selected to closely match those comdeviations across arbitrarily defined classes which in practice 662 puted in 10. 628 can be any of those listed above. We combine this statistic 929 with permutation testing to test hypotheses on whether differ-630 ences between classes are statistically significant in each of 631 these settings.

With this in mind, three hypotheses were defined. For 633 each setting, we state the alternate hypotheses, the variable(s) 634 which were used to determine class membership, and the 635 remaining variables which may be sampled when obtaining 636 multiple observations. Each hypothesis was tested indepen-637 dently for each pipeline and perturbation mode, and in every 638 case where it was possible the hypotheses were tested using 639 the reference executions alongside using MCA.

640 H_{A1} : Individuals are distinct from one another

Class definition: Subject ID 641 642 session), MCA (1 subsample, 1 session) Class definition: Session ID | Subject ID Comparisons: Subsample, MCA (1 subsample)

647 H_{A3} : Subsamples are distinct

Class definition: Subsample | Subject ID, Session ID

Comparisons: MCA

As a result, we tested 3 hypotheses across 6 MCA ex-651 periments and 3 reference experiments on 2 pipelines and 2 652 perturbation modes, resulting in a total of 30 distinct tests.

(3) 653 Evaluating Graph-Theoretical Metrics

654 While connectomes may be used directly for some analyses, where g_{ij} is a graph belonging to class i that was measured 655 it is common practice to summarize them with structural mea-656 sures, which can then be used as lower-dimensional proxies Discriminability can then be read as the probability that an 657 of connectivity in so-called graph-theoretical studies 11. We

> 663 Univariate Differences For each univariate statistic (edge 664 count, mean clustering coefficient, global efficiency, modu-665 larity of the largest connected component, assortativity, and 666 mean path length) a distribution of values across all perturba-667 tions within subjects was observed. A Z-score was computed 668 for each sample with respect to the distribution of feature 669 values within an individual, and the proportion of "classically significant" Z-scores, i.e. corresponding to p < 0.05, was 671 reported and aggregated across all subjects. The number of 672 significant digits contained within an estimate derived from a 673 single subject were calculated and aggregated.

674 Multivariate Differences In the case of both nodewise (de-675 gree distribution, clustering coefficient, betweenness central-676 ity) and edgewise (weight distribution, connection length) fea-Comparisons: Session (1 subsample), Subsample (1 677 tures, the cumulative density functions of their distributions 678 were evaluated over a fixed range and subsequently aggre682 a sample and aggregated.

683 Evaluating A Brain-Phenotype Analysis

Though each of the above approaches explores the instabil- 720 Code Availability 685 ity of derived connectomes and their features, many modern 686 studies employ modeling or machine-learning approaches, for 687 instance to learn brain-phenotype relationships or identify dif-688 ferences across groups. We carried out one such study and ex-689 plored the instability of its results with respect to the upstream 691 tions. We performed the modeling task with a single sampled 692 connectome per individual and repeated this sampling and $_{693}$ modelling 20 times. We report the model performance for $_{728}$ Author Contributions 694 each sampling of the dataset and summarize its variance.

695 **BMI Classification** Structural changes have been linked to 696 obesity in adolescents and adults⁴¹. We classified normal-697 weight and overweight individuals from their structural net-698 works (using for overweight a cutoff of BMI $> 25^{13}$). We 699 reduced the dimensionality of the connectomes through prin-700 cipal component analysis (PCA), and provided the first N-701 components to a logistic regression classifier for predicting 702 BMI class membership, similar to methods shown in 12,13. 703 The number of components was selected as the minimum set 738 Acknowledgments 704 which explained > 90% of the variance when averaged across 739 This research was financially supported by the Natural Sci-705 the training set for each fold within the cross validation of 740 ences and Engineering Research Council of Canada (NSERC) 706 the original graphs; this resulted in a feature of 20 compo-741 (award no. CGSD3-519497-2018). This work was also sup-707 nents. We trained the model using k-fold cross validation, 742 ported in part by funding provided by Brain Canada, in partner-

709 Data Availability

710 The unprocessed dataset is available through The Consortium 745 Additional Information 711 of Reliability and Reproducibility (http://fcon_1000.746 Supplementary Information is available for this paper. Corre-712 projects.nitrc.org/indi/enhanced/), including 747 spondence and requests for materials should be addressed to 713 both the imaging data as well as phenotypic data which may 748 Tristan Glatard at tristan. qlatard@concordia.ca. 714 be obtained upon submission and compliance with a Data Us-

679 gated across individuals. The number of significant digits 715 age Agreement. The connectomes generated through simula-680 for each moment of these distributions (sum, mean, variance, 716 tions have been bundled and stored permanently (https:// 681 skew, and kurtosis) were calculated across observations within 717 doi.org/10.5281/zenodo.4041549), and are made 718 available through The Canadian Open Neuroscience Platform 719 (https://portal.conp.ca/search, search term "Kiar").

721 All software developed for processing or evaluation is publicly 722 available on GitHub at https://github.com/gkpapers/ 723 2020 ImpactOfInstability. Experiments were launched ⁷²⁴ using Boutiques⁴² and Clowdr⁴³ in Compute Canada's HPC 725 cluster environment. A set of MCA instrumented software $_{690}$ variability of connectomes characterized in the previous sec- $_{726}$ containers is available on Github at https://github. 727 com/gkiar/fuzzy.

729 GK was responsible for the experimental design, data pro-730 cessing, analysis, interpretation, and the majority of writing. All authors contributed to the revision of the manuscript. YC, POC, and EP were responsible for MCA tool development and 333 software testing. AR, GV, and BM contributed to experimen-734 tal design and interpretation. TG contributed to experimental 735 design, analysis, and interpretation. TG and ACE were responr36 sible for supervising and supporting all contributions made by 737 GK. The authors declare no competing interests for this work.

 $_{708}$ with k = 2, 5, 10, and N (equivalent to leave-one-out; LOO). $_{743}$ ship with Health Canada, for the Canadian Open Neuroscience 744 Platform initiative.

S1. Graph Correlation

The correlations between observed graphs (Figure S1) across each grouping follow the same trend to as percent deviation, as shown in Figure 1. However, notably different from percent deviation, there is no significant difference in the correlations between pipeline or input instrumentations. By this measure, the probabilistic pipeline is more stable in all cross-MCA and cross-directions except for the combination of input perturbation and cross-MCA (p < 0.0001 for all; exploratory).

The marked lack in drop-off of performance across these settings, inconsistent with the measures show in Figure 1 is due to the nature of the measure and the graphs. Given that structural graphs are sparse and contain considerable numbers of zero-weighted edges, the presence or absense of an edge dominated the correlation measure where it was less impactful for the others. For this reason and others⁴⁴, correlation is not a commonly used measure in the context of structural connectivity.

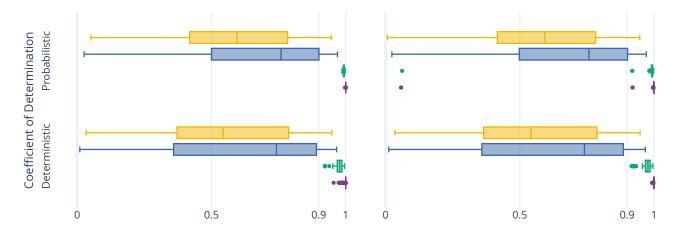


Figure S1. The correlation between perturbed connectomes and their reference.

S2. Complete Discriminability Analysis

Table S1. The complete results from the Discriminability analysis, with results reported as mean \pm standard deviation Discriminability. As was the case in the condensed table, the alternative hypothesis, indicating significant separation across groups, was accepted for all experiments, with p < 0.005.

				Reference Execution		Perturbed P	ipeline	Perturbed Inputs		
Exp.	Subj.	Sess.	Samp.	Det.	Prob.	Det.	Prob.	Det.	Prob.	
1.1	All	All	1	0.64 ± 0.00	0.65 ± 0.00	0.82 ± 0.00	0.82 ± 0.00	0.77 ± 0.00	0.75 ± 0.00	
1.2	All	1	All	1.00 ± 0.00	1.00 ± 0.00	1.00 ± 0.00	1.00 ± 0.00	0.93 ± 0.02	0.90 ± 0.02	
1.3	All	1	1			1.00 ± 0.00	1.00 ± 0.00	0.94 ± 0.02	0.90 ± 0.02	
2.4	1	All	All	1.00 ± 0.00	1.00 ± 0.00	1.00 ± 0.00	1.00 ± 0.00	0.88 ± 0.12	0.85 ± 0.12	
2.5	1	All	1			1.00 ± 0.00	1.00 ± 0.00	0.89 ± 0.11	0.84 ± 0.12	
3.6	1	1	All			0.99 ± 0.03	1.00 ± 0.00	0.71 ± 0.07	0.61 ± 0.05	

The complete discriminability analysis includes comparisons across more axes of variability than the condensed version.

The reduction in the main body was such that only axes which would be relevant for a typical analysis were presented. Here,
each of Hypothesis 1, testing the difference across subjects, and 2, testing the difference across sessions, were accompanied
with additional comparisons to those shown in the main body.

Subject Variation Alongside experiment 1.1, that which mimicked a typical test-retest scenario, experiments 1.2 and 1.3 rould be considered a test-retest with a handicap, given a single acquisition per individual was compared either across subsamples or simulations, respectively. For this reason, it is unsurprising that the dataset achieved considerably higher discriminability scores.

767 **Session Variation** Similar to subject variation, the session variation was also modelled across either both or a single subsample. In both of these cases the performance was similar, and the finding that input perturbation reduced the off-target signal was consistent.

S3. Univariate Graph Statistics

Figure S2 explores the stability of univariate graph-theoretical metrics computed from the perturbed graphs, including modularity, global efficiency, assortativity, average path length, and edge count. When aggregated across individuals and perturbations, the distributions of these statistics (Figures S2A and S22B) showed no significant differences between perturbation methods for either deterministic or probabilistic pipelines.

However, when quantifying the stability of these measures across connectomes derived from a single session of data, the two perturbation methods show considerable differences. The number of significant digits in univariate statistics for Pipeline Perturbation instrumented connectome generation exceeded 11 digits for all measures except modularity, which contained more than 4 significant digits of information (Figure S2C). When detecting outliers from the distributions of observed statistics for a given session, the false positive rate (using a threshold of p = 0.05) was approximately 2% for all statistics with the exception of modularity which again was less stable with an approximately 10% false positive rate. The probabilistic pipeline is significantly more stable than the deterministic pipeline (p < 0.0001; exploratory) for all features except modularity. When more than 3 significant digits or a false positive rate lower than nearly 6% (Figure S2D). The deterministic pipeline was more more than 4 significant digits or a false positive rate lower than nearly 6% (Figure S2D). The deterministic pipeline was more than 5 significant digits or a false positive rate lower than nearly 6% (Figure S2D).

Two notable differences between the two perturbation methods are, first, the uniformity in the stability of the statistics, and second, the dramatic decline in stability of individual statistics in the input perturbation setting despite the consistency in the overall distribution of values. It is unclear at present if the discrepancy between the stability of modularity in the pipeline perturbation context versus the other statistics suggests the implementation of this measure is the source of instability or if it is implicit to the measure itself. The dramatic decline in the stability of features derived from input perturbed graphs despite no difference in their overall distribution both shows that while individual estimates may be unstable the comparison between aggregates or groups may be considered much more reliable; this finding is consistent with that presented for multivariate statistics.

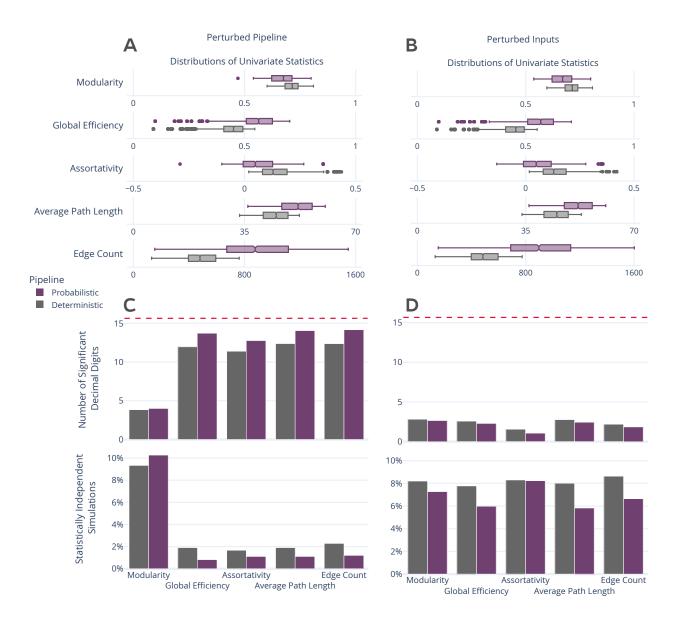


Figure S2. Distribution and stability assessment of univariate graph statistics. (**A**, **B**) The distributions of each computed univariate statistic across all subjects and perturbations for Pipeline and Input settings, respectively. There was no significant difference between the distributions in A and B. (**C**, **D**; top) The number of significant decimal digits in each statistic across perturbations, averaged across individuals. The dashed red line refers to the maximum possible number of significant digits. (**C**, **D**; bottom) The percentage of connectomes which were deemed significantly different (p < 0.05) from the others obtained for an individual.