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February 3, 2017

Nicholas Ayache Co-editor in Chief Medical Image Analysis

Subject: MEDIA-D-16-00507 - Response to reviewers

## Dear Sir or Madam,

We would like to thank the reviewers for their pertinent remarks that have increased the quality of the manuscript. Whenever possible, the comments of the reviewers have been addressed and highlighted in the article.

Please, find below a point-by-point response to each of the issues raised by the reviewers.

## Reviewer #1:

- 1. In a typical DCE based analysis, the contrast enhanced images are rigidly registered to T1w images for intensity normalization. Typically for multiparametric MRI based CAD system for prostate cancer detection T1w images are present. This is useful in differentiating cancers from blood hemorrhage following prostate biopsy. Please discuss why a pre or a post contrast T1w image is missing from the clinical trial that will be using DCE images.
  - Maybe it was not entirely clear from the text but the DCE sequence used in this work is based on T1w. In other words, the pre-contrast acquisition corresponds to the first volumes in the sequence before the contrast injection. To avoid confusion, this has been clarified in the Material section (p. 15/l. 275). Additionally, the risk of blood hemorrhage is discarded since the biopsies are carried out after the MRI acquisition.
- 2. The other advantage of normalizing to T1w images are patient specific information will be preserved. Different patients may have different cancer lesions of different grades (having different kinetic expression in DCE) and normalizing all patients to the same space may result in loss of information. Please comment.
  - Our normalization is designed to align the *mean kinetic expression*. The mean kinetic expression contains cancer and non-cancer kinetic information. Assuming that the amount of cancer information (voxels) is much lower than the normal tissue, the use of this normalization allows to minimize undersired patient-specific (overall-intensity, mean contrast, uptake, ...) without affecting the lesion information.
- 3. T1w normalization will be probably be more robust to change in mag-

net, machine, reconstruction software and acquisition parameters across different institutions as the objective is normalization to be patient and institution specific. Please comment how the presented model may be affected in a multi-institutional study.

In line with the previous comment on the use of T1w, we want to clarify that DCE is based on T1w sequence. Moreover, our method does not rely on any manufacturer/machine-specific settings. Subsequently, our approach should work on any type of devices, enabling multi-institutional studies. We included these remarks in our future work section in p. 23/l. 396.

- 4. Please discuss how the improvement in prostate cancer detection in DCE-MRI impacts the current clinical CAD pipeline. According to PIRADS v2 guidelines more emphasis is laid upon T1w, T2w and DWI compared to DCE images. Experienced radiologists can detect prostate cancers in peripheral zone with a high degree of accuracy (higher than 0.6 AUC). The transition zone lesions are more difficult to distinguish. Please comment how the model performs in detection of transition zone lesions. Further please comment how this model adds value to already established clinical pipeline of detecting prostate cancer (PIRADS).
  - We have included a new stratified analysis, separating PZ and CG, which showed an increase of the classification performance in CG after applying our normalization method as depicted in Fig. 8 p. 22. The PIRADS v2 emphasizes that DCE-MRI has to be included in mp-MRI acquisition to detect small lesions. However, it also warns that the benefit is modest. Therefore, the impact of an improvement of detection in DCE-MRI can only be evaluated in a fully mp-MRI CAD system which is beyond the scope of this paper. Indeed, we recently showed, Lemaitre, Guillaume. Computer-Aided Diagnosis for Prostate Cancer using Multi-Parametric Magnetic Resonance Imaging. Diss. Université de Bourgogne; Universitat de Girona, 2016; Chapt. 6/p. 150/Table 6.10 —, that DCE-MRI features are considered important and the combination with other modalities will lead to better classification results. However, in our humble opinion, including those additional results will clutter the paper.
- 5. Comparing the results of semi-automatic approach and the presented approach of curve fitting using the entire curve the results are not significantly different (0.65 AUC vs 0.66 AUC). The presented model is however automatic which would reduce inter-rater variance in a semi-automatic method. Please present a discussion comparing these two results.
  - It is important to notice that for both approaches, semi-quantitative and entire enhanced signal —, the results are obtained using our normalization approach, showing the importance of this step. We added a discussion in p. 23/l. 388 regarding the semi-quantitative approach and entire enhanced signal classification. The semi-quantitative approach reduces the number of features to analyze, speeding up the classification. However, it relies on the curve fitting which is also time consuming and might fail.
- 6. Use of single feature for a random forest classifier (Table 2) may be detrimental for the classifier as random sub-sampling of the features are not possible. Please present the comparison with some linear classifiers like linear SVM.

A classification using a linear SVM has been added in additional material. Unlike a

linear SVM, RF allows to find multiple thresholds, leading to a much complex decision boundary for this feature. Bootstrapping the samples for each tree allows to cope with the over-fitting of each decision trees. Results with SVM show no particular improvement in comparison with RF. Therefore, we do not think that including a linear SVM will be beneficial for the paper as are the results provided in the additional material showing.

## Reviewer #4:

1. The title is misleading and not very scientific and I would recommend to remove the second part and reword the first part to cover the contents of the paper.

We are not against changing the title but we would like to take advantage of this revision to get the opinion of all reviewers regarding this matter.

- 2. The use of the English language needs some attention: get it all proof read. As suggested, the manuscript has been corrected by an English editing service to ensure a good quality writing. A certificate of the service can be provided upon request.
- 3. What guided biopsy was used: US?

  The guided biopsy was performed with a TRUS. We added this statement in p. 15/l. 275.
- 4. The number of cases seems low. This is mentioned as possibly affecting the results and that the limitations might be based on the sample size. At the end of section 5 one could draw the conclusion that they should do a more extensive study.

The reviewer is right with the comment, unfortunately due to the difficulty on acquiring and annotating this kind of data, we cannot provide a larger database at this time. However, a statement has been added in the discussions p. 23/l. 396, describing this limitation of the study.

- 5. How would this translate to other types of MRI systems: it would be good to see experimental results on this or at least some discussion.

  Refer to reviewer #1 / comment 3 since this is a shared remark.
- 6. The disappointing performance and large standard deviation of the PUN model should be investigated and explained.

A discussion is added in p. 17/l. 320. The original published model lacks of degrees of freedom. Two additional parameters will allow for a better fit. However, we used the original formulation in our experiments.

7. There should be a detailed discussion on the results to indicate which differences are statistically significant. "Significant" is mentioned in the conclusions, but there is no evidence for this.

We added a Wilcoxon significance test - see Fig. 7. Now, the term significant is only used for p < 0.05.

8. The overall results seem poor and this could be further discussed.

It is difficult to compare with the state-of-the-art methods since the dataset used are different and the reported results in those studies are usually linked to a mp-MRI CAD instead of only DCE. Nevertheless, our results are in the same range than Litjens, Geert, et al. "Computer-aided detection of prostate cancer in MRI." IEEE transactions on medical imaging 33.5 (2014): 1083-1092 regarding the classification

- performance of the Tofts parameters.
- 9. Sections 5 and 6 are both disappointingly short. After including the remarks from the reviewers, this section has become much longer.
- 10. Some journals references incomplete. Gliozzi et al. is not a single page. Check: Schabel, Shanbhag, Zhu.

The references have been corrected.

## Reviewer #5:

1. There are however several issues with the paper In the current state. Using quantitative parameters obtained from pharmacokinetic models as an endpoint comparison indeed may be important as the models provide physiological information related to capillary permeability, blood fraction and interstitial space volume, etc.. However I am not really convinced by the detailed results presented in Table 2, as no statistical test was performed when the classification performances are higher with normalized data, and for some of the models the results are worst. For me, the benefits of the method are not fully demonstrated in terms of classification performance using the models. How these parameters are modified with the normalization?

This is important to emphasize that our goal was to propose a normalization method to allow classification of the entire enhanced signal which should perform as good as the current models. For the sake of completeness, we apply the same normalization on the different pharmacokinetic models and, as mentioned by the reviewer — the results are not significantly better as the model parameters might have a different interpretation after the normalization is applied. Indeed, these experiments were carried out to investigate the benefit or not of the normalization with the current models.

- 2. Some of the benefits or improvements may be demonstrated before any further classification step. The method could be useful when performing population analysis with the raw data, previous to defining a model. We do not really see which analysis can be performed to evaluate the benefits of our methods before the classification step. A study of the variances with and without normalization could be carried out but an evaluation after classification seems equivalent and a good manner to evaluate the benefit of the normalization. In fact, these are the results reported in Fig. 6(c).
- 3. Figure 1 is not pertinent for the goal of this paper. It is not clear how is represented the interindividual variation in figure 2? In Fig 2a the PDFs are concatenated in time to obtain a heatmap representation, but in 2 b-c the differences across individuals does not appear.

  Figure 1 is used to illustrate inter-patients variation in T2w-MRI and to highlight the need of a different normalization approach than the one needed in T2w. We have clarified in the caption that Fig. 1 is related to T2w, and if requested by the reviewers, Figure 1 could be removed. We improve the Fig. 2. Figure 2(a) presents only the process to build the heatmap. In Fig. 2(b)-2(c), we added parameters which highlight more clearly the variations and added their corresponding values in caption.
- 4. It is not clear the rational of equation 1, as the parameters are rather

empirical. There are no other ways to smooth the heatmap, for example through a diffusion process, solving a PDE equation? Or by registering through the series?

There is probably a confusion. We do not try to smooth the heatmap but we search a smooth estimate. Equation 1 represents the weight of the graph and is a standard way to formalize graph-based problem in image processing which often includes a data driven term and a smoothing term.

5. The theoretical foundations of equation 3 are not clear. Other registration methods for time signas may have been included.

While other registrations could have been used, using a rigid registration directly affect the variations  $\alpha_i$  and  $\Delta_t$ . Non rigid registration is deemed not necessary as the main parameters that we propose to recover are translations and scaling. Moreover, this kind of registration might induce deformation artifacts which could impact on the overall contrast enhancement over time.

6. Other question that may be raised is the influence of the equation parameters (tau, alfa..) in the pharmacokinetic models. Do they change with f(t)?

We think that this question is related to the results presented in Sect. 4.1

7. A thorough review of the structure and in general an improvement of the paper in terms of writing may be helpful to fully understand the message, the rational and the proposed methodology.

As suggested, the manuscript has been corrected by an English editing service to ensure a good quality writing.

Thank you for your time and consideration.

I look forward to your reply.

Sincerely,

Guillaume Lemaître