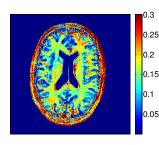
Dictionary-Free MRI Parameter Estimation via Kernel Ridge Regression

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Quantitative MRI (QMRI) Parameter Estimation

Given: MR image sequence informative about a physical process

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- diffusion
- multi-compartmental relaxation
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Task: estimate MR tissue properties characterizing the process

- flow velocity
- diffusivity
- compartmental relaxivity
- . . .

QMRI Problem Statement

Given: at each voxel, image sequence $\mathbf{y} \in \mathbb{C}^D$ modeled as

$$y = s(x, \nu) + \epsilon \tag{1}$$

- $\mathbf{x} \in \mathbb{R}^L$
- $\nu \in \mathbb{R}^K$
- $\mathbf{s}: \mathbb{R}^{L+K} \mapsto \mathbb{C}^D$
- $oldsymbol{\epsilon} \in \mathbb{C}^D$

latent free parameters

known parameters

signal model

noise $\sim \mathbb{C}\mathcal{N}(\mathbf{0}_D, \mathbf{\Sigma})$

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- grid search e.g., for MR fingerprinting [Ma et al., 2013]

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- design nonlinear functions $\widehat{x}_l(\cdot) := \widehat{h}_l(\cdot) + \widehat{b}_l$ for $l \in \{1, \dots, L\}$ that map each $\mathbf{q}_n := [\operatorname{Re}(\mathbf{y}_n)^\mathsf{T}, \operatorname{Im}(\mathbf{y}_n)^\mathsf{T}, \boldsymbol{\nu}_n^\mathsf{T}]^\mathsf{T} \in \mathcal{Q}$ to $x_{l,n} \in \mathbb{R}$

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$$(\widehat{h}_l, \widehat{b}_l) \in \left\{ \arg \min_{\substack{h_l \\ b_l \in \mathbb{R}}} \frac{1}{N} \sum_{n=1}^{N} (h_l(\mathbf{q}_n) + b_l - x_{l,n})^2 \right\}$$

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Solution: solve a kernel ridge regression (KRR) problem

- restrict function space over which we optimize
- include function regularization

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Hilbert space: complete inner product function space

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Reproducing kernel Hilbert space (RKHS)

Hilbert space $\mathbb H$ over input space $\mathcal Q$ with *reproducing property*

$$\langle h, \mathbf{k}(\cdot, \mathbf{q}) \rangle_{\mathbb{H}} = h(\mathbf{q}), \qquad \forall h \in \mathbb{H}, \mathbf{q} \in \mathcal{Q}$$

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Relevant facts

- Bijection between RKHS \mathbb{H} and RK k [Aronszajn, 1950]
- Function $k(\cdot, \mathbf{q}) \in \mathbb{H}$ called a *feature mapping*

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- Nonlinear kernel corresponds to nonlinear estimation
- ullet We use $k(\mathbf{q},\mathbf{q}') \leftarrow \exp\left(-rac{1}{2}ig\|\mathbf{\Lambda}^{-1}(\mathbf{q}-\mathbf{q}')ig\|_2^2
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Solve: for each desired latent parameter $l \in \{1, ..., L\}$,

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• Optimal \hat{h}_l over \mathbb{H} takes form [Schölkopf et al., 2001]

$$\widehat{h}_{l}(\cdot) \equiv \sum_{n=1}^{N} \widehat{a}_{l,n} \mathbf{k}(\cdot, \mathbf{q}_{n})$$
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• Plug (4) into (3); solve now instead for $(\widehat{a}_l, \widehat{b}_l)$; construct:

$$\widehat{x}_{l}(\cdot) = \sum_{n=1}^{N} \widehat{a}_{l,n} \mathbf{k}(\cdot, \mathbf{q}_{n}) + \widehat{b}_{l}$$
 (5)

Non-iterative closed-form solution, for $l \in \{1, ..., L\}$:

$$\widehat{\mathbf{x}}_{l}(\cdot) = \mathbf{x}_{l}^{\mathsf{T}} \left(\frac{1}{N} \mathbf{1}_{N} + \mathsf{M}(\mathsf{KM} + N\rho_{l} \mathbf{I}_{N})^{-1} \left(\mathbf{k}(\cdot) - \frac{1}{N} \mathsf{K} \mathbf{1}_{N} \right) \right)$$
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• $\mathbf{x}_l := [x_{l,1}, \dots, x_{l,N}]^\mathsf{T}$ training pt regressands

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$$\bullet \ \mathbf{x}_l := [x_{l,1}, \dots, x_{l,N}]^\mathsf{T} \qquad \text{training pt regressands}$$

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 Gram matrix

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Can we scale computation with *L* more gracefully?

- Yes, in fact (6) separable in $l \in \{1, ..., L\}$ by construction
- However, explicitly computing **K** may be undesirable...

Suppose there exists "approximate feature mapping" $\tilde{\mathbf{z}}: \mathcal{Q} \mapsto \mathbb{R}^Z$ such that $\tilde{\mathbf{Z}}:=[\tilde{\mathbf{z}}(\mathbf{q}_1),\dots,\tilde{\mathbf{z}}(\mathbf{q}_N)]$ has for $\dim(\mathcal{Q}) \ll Z \ll N$ $\mathbf{K} \approx \tilde{\mathbf{Z}}^T \tilde{\mathbf{Z}}. \tag{7}$

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which is regularized ("ridge") Z-dimensional affine regression!

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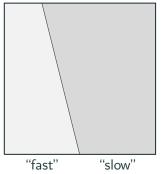
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Does such a $\tilde{\mathbf{z}}$ exist and work well in practice?

- Yes, e.g. for "shift invariant" kernels (like our Gaussian) of form $k(\mathbf{q}, \mathbf{q}') \equiv k(\mathbf{q} \mathbf{q}')$ [Rahimi and Recht, 2007]
- ullet In such cases, can reduce from $\sim\!N^2$ to $\sim\!NZ$ computations

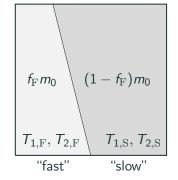
Application: Myelin Water Fraction (MWF) Imaging





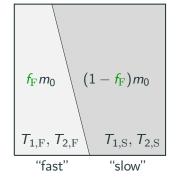
Application: Myelin Water Fraction (MWF) Imaging

simple two-compartment model



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Goal: rapidly estimate f_F (proxy for MWF) in white matter (WM)

Application: MWF Imaging

Problem dimensions (per voxel)

- $\mathbf{x} \leftarrow [f_{\mathrm{F}}, T_{1,\mathrm{F}}, T_{2,\mathrm{F}}, T_{1,\mathrm{S}}, T_{2,\mathrm{S}}, m_0]^{\mathsf{T}}$
- u \leftarrow flip angle variation
- y ← voxel values from 10 datasets

[Nataraj et al., 2017]

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Use KRR to estimate just $f_{\rm F}$

- Separable prior on \mathbf{x} : f_{F}, m_0 uniform; others log-uniform
- $N \leftarrow 10^6$ training points
- $Z \leftarrow 10^3$ kernel approximation order

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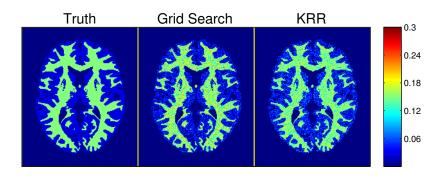
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Compare against grid search

- ullet unconstrained search would require $\sim \! 100^5$ dictionary atoms
- we artificially constrain search here to limit computation

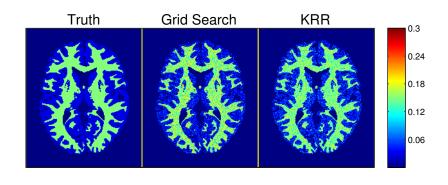
MWF Imaging: Simulation Result

Fast-fraction $f_{\rm F}$ estimates, in simulation:



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 \sim 4h 40s training, 2s testing

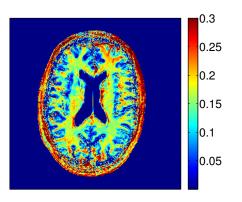
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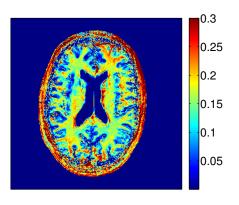
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- KRR estimates in single slice took about 70s
- KRR MWF estimates in WM comparable to literature



Contributions

• Fast KRR method for nonlin MRI multiparameter estimation

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 - Key insight: even with complicated MR signal models, can simulate training points "for free"

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 - Key insight: even with complicated MR signal models, can simulate training points "for free"
 - Convert *nonlinear estimation* problem into *nonlinear regression* problem that we solve in closed-form with kernels

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- Conceptual: model selection, performance analysis
- Experimental: validation studies

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Backup: An Overview of Model Selection

Some model parameters require manual selection...

• Kernel shape
$$k(\mathbf{q}, \mathbf{q}') \leftarrow \exp\left(-\frac{1}{2} \left\| \mathbf{\Lambda}^{-1} (\mathbf{q} - \mathbf{q}') \right\|_2^2\right)$$

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- Prior on **x** from tissue properties
- *N*, *Z* empirical methods

...but others tuned automatically

- Kernel smoothing length-scale $\Lambda \leftarrow \mathsf{diag}\Bigl(\sum_{n=1}^{N} \mathbf{q}_n\Bigr)$
- Regularization parameters $\rho_l \leftarrow \frac{1}{N^2} \mathbf{x}_l^\mathsf{T} \mathbf{M} \mathbf{x}_l$
- ullet Prior on known u density estimation