Brain tissue temperature dynamics during functional activity and possibilities for Imaging

by

GREGGORY H. ROTHMEIER

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Dedication

 ${\bf Mama.}$

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Perera, Dhamala, Brooke, Lab Mates, Dhamala's Lab

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Brain tissue temperature dynamics during functional activity and possibilities for Imaging

A thesis presented in Partial Fulfilment of Requirements for the Degree of Master of Science in the College of Arts and Sciences Georgia State University 2012 by Greggory Rothmeier Committee:

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Chapter 1

Introduction

Chapter 2

Calculating Temperature Changes using the fMRI BOLD Response

2.1 Background

2.1.1 Generation of the Blood Oxygen Level Dependent (BOLD) Response

Since its invention in the 1950's [1] and later development in the 1970's [2], Magnetic Resonance Imaging (MRI) has allowed physicians and scientists a detailed view within the human body.

2.1.2 Previously Proposed Temperature Models

Current efforts to model temperature changes be can categorized into two classes. The first class approaches the problem by considering a single voxel deep within the brain (single-voxel approach) while the second approach considers the brain and head as an entire system (multi-voxel approach). Each of these methods has their own pros and cons which will be discussed below.

Single-Voxel Approach

A single-voxel model of temperature was first proposed by SOMEONE, but has been refined over the past HOWLONG years CITEABUNCH to include more terms. Although different approaches consider different contributions to the temperature change, they all narrow the problem down to a single voxel which is usually 2mm x 2mm. By simplifying the model, the heat equation can be simplified and the calculation is much easier to undertake. However, since the brain is not homogenous, the values used for parameters

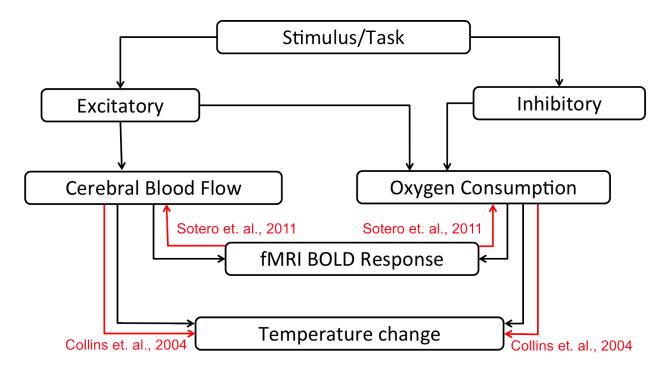


Figure 2.1: Generation of the fMRI BOLD response from changes in neuronal activity. Black arrows indicate a causal relationship while red arrows indicate existing models for the relationship. Modified from Sotero and Trujillo-Barreto [3]

such as heat production and thermal conductivity are taken from an average of the tissues. As a result, this reduces the possible accuracy of such a model when applied to a subject. The most recently published iteration of a single-voxel model was published by Sotero and Iturria-Medina [4]. The basis of this model is a modification of the Penne's Bioheat Equation [5, 4].

$$C_{t} \frac{dT(t)}{dt} = (\Delta H^{\circ} - \Delta H_{b})CMRO_{2} \mid_{0} m(t) - \rho_{b}C_{b}CBF \mid_{0} f(t)(T(t) - T_{a}) - \frac{C_{t}}{\tau}(T(t) - T_{0})$$
 (2.1)

where BLA BLA. One advantage of using eq. (2.1) is that the resting state temperature can be analytically determined by substituting $\frac{dT(t)}{dt} = 0$ [4].

$$T_{0} = T_{a} + \frac{(\Delta H \mid^{\circ} - \Delta H_{b})CMRO_{2}\mid_{0}}{\rho_{B}C_{B}CBF\mid_{0}}$$
(2.2)

If the values provided in table 2.1 are substitued into eq. (2.2), a resting temperature of 37.3057°C is found. Since the resting temperature is always greater than the arterial blood temperature, it limits the ability of the model to account for all experimental results.

While eq. (2.1) is appears complicated, conceptually the equation can be easily understood.

change in temperature = heat generated by metabolism - heat lost to convection - heat lost to conduction (2.3)

The system is a balance between heat generation (metabolism) and heat transfer (conduction and convection). The direction of heat transfer by convection is determined by the difference between the voxel temperature and the arterial blood temperature $(T(t) - T_a)$. Similarly, the direction of heat transfer by conduction is determined by the difference between the voxel temperature and the temperature of the surrounding tissue $(T(t) - T_0)$. Since T_a is less than T(0), an increase in blood flow (f(t)) will remove heat from the voxel thereby decreasing the temperature. Conversely, an increase in metabolism (m(t)) without a corresponding change in blood flow, will result in tissue warming.

$$f(t) = \frac{\alpha + \beta c}{b\beta} W(y(t)) \tag{2.4}$$

$$m(t) = af^{c+1}(t)e^{-bf(t)}$$
 (2.5)

$$y(t) = -\frac{b\beta}{\alpha + \beta c} \left[\frac{\left(A - \frac{S(t)}{S_0} - 1\right)}{Aa^{\beta}} \right]^{\left(\frac{1}{\alpha + \beta c}\right)}$$
(2.6)

Multi-Voxel Approach

Table 2.1: Parameters used to solve the single-voxel Penne's Bioheat Equation. (modified from Sotero and Iturria-Medina [4])

Parameter	Meaning	Value
$\overline{\mathrm{T}_a}$	Arterial blood temperature	37°C
C_{tissue}	Tissue Heat Capacity	$3.664 \; J/(gK)$
ΔH°	Enthalpy released by oxidation of glucose	$4.710^5 \ { m J}$
ΔH_b	Enthalpy used to release O ₂ from hemoglobin	2.810^4 J
$CMRO_2 \mid_0$	Cerebral metabolic rate of O_2 consumption at rest	$0.026310^{-6} \text{ mol/(gs)}$
$CBF _0$	Cerebral blood flow at rest	$0.0093 \text{ cm}^3/(\text{gs})$
$ ho_b$	Blood density	$1.05 \mathrm{g/cm^3}$
C_B	Blood heat capacity	3.894 J/(gK)
au	Time constant for conductive heat loss from the ROI to the surrounding tissue	190.52 s
a, b, c	Parameters of the gamma function fitted from E(f) vs. f	0.4492,0.2216,-0.9872
A	Maximum BOLD signal change	0.22
α	Steady state flow-volume relation	0.4
eta	Field-strength dependent parameter	1.5
Variable	Meaning	
m(t)	CMRO ₂ normalized to baseline	
f(t)	CBF normalized to baseline	
T(t)	Temperature	
W(t)	Lambert W Function	
$frac\Delta S(t)S_0$	Change in BOLD signal normalized to rest	

2.2 Modeling the BOLD Response

2.3 Modeling Temperature

2.3.1 The Approach

How the temperature is calculated

$$\rho c \frac{dT}{dt} = k \nabla^2 T - \rho_{blood} f(t) w c_{blood} (T - T_{blood}) + m(t) Q_m$$
(2.7)

Calculating the equilibrium temperature

Calculating Metabolism and Blood Flow Changes

Calculating the change in temperature in the active brain

2.3.2 Results

Using Theoretical BOLD Data

Using Experimental BOLD Data

Chapter 3

Detector Applications to measuring the active brain

3.1 Functional Near-Infrared fNIR Imaging

$$I = I_0 e^{-\alpha x} \tag{3.1}$$

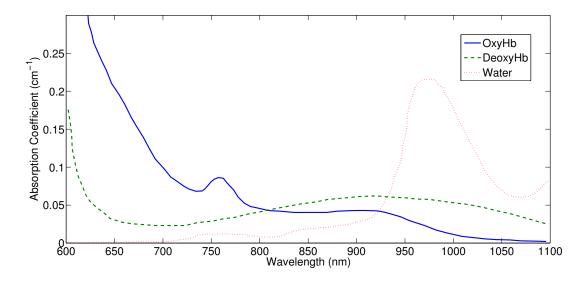


Figure 3.1: Absorption spectra of water, Hb and Dhb. From Cope [6] and HB stuff from Horecker [7]

3.2 Temperature Measurements

From the Beer-Lambert law eq. (3.1), the penetration depth, δ_p can be expressed as

$$\delta = \frac{1}{\alpha} \tag{3.2}$$

where α is the absorption coefficient. At body temperature (37°) the peak wavelength in the blackbody spectrum is approximately BLA. For water at this wavelength, α is approximately HUGE, so δ is VERY SMALL.

Chapter 4

Conclusion

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Appendix A

Code

The following sections include the code used. It was written for Matlab 2011(b) and requires SPM8 to run. Additionally, it is recommended that you have at least 4 GB of RAM in order to work with the large datasets that are produced. For information about how to visualize the data produced, see appendix B. All of the code is available through the temptools github page (https://github.com/greggroth/tempcalc)

A.1 Creating the Head Matrix

Before any calculations can be done, a matrix containing tissue-specific parameters must be created. First, a T1 contrast image should be segmented using SPM8 (http://www.fil.ion.ucl.ac.uk/spm/software/spm8/). For ease of consistency, the one provided by SPM8 in ./canonical/ is best to use. Using SPM's "New Segmentation" algorithm will segment the image into five different tissue types (gray matter, white matter, cerebral spinal fluid, soft tissue and bone). Once this is complete, run BulkImportNII() within this directory and it will return a matrix that has been populated with the tissue-specific parameters required for accurate temperature calculations. The functions fillAir() (A.1.2) and fillholes() (A.1.3) are functions required by BulkImportNII(). More information about this procedure is in section 2.3.1.

A.1.1 BulkImportNII()

```
function [ total ] = BulkImportNII(varargin)

% BulkImportNII Import NII files from a directory

% Must be run within the directory containing the files

%

% Output: head data as single with variables stored in the 4th dimension.
```

```
6
   %
7
   %
       Author: Greggory Rothmeier (greggroth@gmail.com)
8
   %
       Georgia State University
       Created: 5/31/11
9
10
   statusbar = waitbar(0,'Initializing');
11
12
   if size(varargin) == 1
13
       oldFolder = cd(varargin{1});
14
15
   end
16
17
18
   % ===========
   % = Tissue Parameters =
   % ==========
20
21
   % Each tissue type is assigned an integer index (i.e. gray matter -> 11) such that
22
   % tissue-specific parameters can be found by looking at that element within the
   % corresponding storage matrix (i.e. QmSTORE(11) -> gray matter Qm)
23
24
   % Parameters taken from Colins, 2004
25
26
   tisorder = [11 15 5 13 3]; % Using: [GM WM CSF Muscle Bone]
27
28
29
   QmSTORE = [0 0 26.1 11600 0 26.1 697 0 0 302 15575 0 697 1100 5192];
30
   cSTORE = [1006 4600 2110 3640 3800 1300 3720 3000 4200 2300 3680 3500 3720 3150
      3600];
   rhoSTORE = [1.3 1057 1080 1035.5 1007 1850 1126 1076 1009 916 1035.5 1151 1041
      1100 1027.4];
   kSTORE = [0.026 0.51 0.65 0.534 0.5 0.65 0.527 0.4 0.594 0.25 0.565 0.4975 0.4975
32
      .342 .503];
   wSTORE = [0 1000 3 45.2 0 1.35 40 0 0 2.8 67.1 3.8 3.8 12 23.7];
33
34
   % ==========
35
   % = Import the pre-segmented T1 files =
36
37
```

```
38
   % The T1 contrast image sould be segmented using SPM8.
39
       This loop needs to complete before the next one can begin
40
      Import all of the datat and store as 'cdat1', 'cdat2', etc.
   for i = 1:5
41
       eval(strcat('dat',num2str(i),' = loadNII(''rc', num2str(i), 'single_subj_T1.
42
          nii'');'))
       % Preallocate
43
       eval(strcat('out', num2str(i),' = zeros(cat(2,size(dat', num2str(i),'),7));'))
44
45
    end
46
   % ===============
47
   % = Populate the head matrix =
48
   % ===============
49
       For each data file, it fills in the data from the data storage arrays
50
       for that particular type of tissue. It picks which ever tissue is the
51
       most likely candidate for that voxel based on the segmented data
52
       PROBLEM: It returns 0 (later filled with air) if there is equal
54
   %
       probability of a voxel being two or more different types of tissue.
55
       SOLVED BY fillholes()
56
   %
57
58
   for i = 1:5
59
       % Preallocate
60
61
       holder = zeros(cat(2, size(dat1),7), 'single');
       mask = zeros(size(dat1));
62
       final = zeros(size(holder), 'single');
63
       % Create a mask that indicates whether it is the mostly likely tissue type
65
        guide = [1 2 3 4 5 1 2 3 4 5]; % This guides it through the data correctly
        eval(strcat('mask = (dat',num2str(i),'>dat',num2str(guide(i+1)),') & (dat',
67
          num2str(i), '>dat', num2str(guide(i+2)),') & (dat', num2str(i), '>dat', num2str(
          guide(i+3)),') & (dat',num2str(i),'>dat',num2str(guide(i+4)),') & (dat',
          num2str(i), '~=0);'))
```

```
68
       holder(:,:,:,1) = mask;
                                                      % move structure data to new
          matrix
        a = find(holder(:,:,:,1) == 1);
                                                      % get indicies of tissues
        [x y z t] = ind2sub(size(holder),a);
                                                     % gets coordinates from index
70
71
        \% go to each tissue point and store the info
72
        for j = 1:length(a)
73
            final(x(j),y(j),z(j),:) = [tisorder(i) 0 QmSTORE(tisorder(i)) cSTORE(
74
               tisorder(i)) rhoSTORE(tisorder(i)) kSTORE(tisorder(i)) wSTORE(tisorder(
              i))];
75
        end
76
77
       % Saves the result to a unique output variable (out1, out2, etc)
        eval(strcat('out',num2str(i),'= final;'))
79
        clearvars a x y z t holder final;
        waitbar(i/6,statusbar,sprintf(['File ',num2str(i),' Import Compete']));
82
   end
83
   \% The filleAir() function checks for any voxels which were not assigned a
84
   % tissue type and fills them in with air
85
   almostthere = fillAir(out1+out2+out3+out4+out5);
86
   % The fillholes() function corrects for a voxel having two equally-probable
87
   % tissue types
88
89
   total = single(fillholes(dat1,dat2,dat3,dat4,dat5,almostthere));
   waitbar(1,statusbar,'Saving Data')
90
91
   cd(oldFolder);
   close(statusbar);
93
94
95
   end
   A.1.2
          fillAir()
   function [ output ] = fillAir( tissue )
```

2 % fillAir() fills gaps in data with air

```
3
        Once you import all of the data using loadNII(), run it thought this to
4
        fill in the remaining spaces with air.
5
   airdata = [1 0 0 1006 1.3 0.026 0];
6
7
   % Picks out air spots
8
   a = find(tissue(:,:,:,1) == 0);
    [x y z t] = ind2sub(size(tissue),a);
10
11
   for i = 1:length(a)
12
       tissue(x(i),y(i),z(i),:) = airdata;
13
   end
14
15
   output = tissue;
17
   end
```

A.1.3 fillholes()

```
function [ out_head ] = fillholes( in1,in2,in3,in4,in5,headin)
   % fillholes() checks for misassigned voxels
2
3
   % Solves an issue where a voxel with two equally probable tissue
4
   % types resulted in being assigned as air. This checks for air
5
   % voxels that are surrounded by tissue and decides a tissue it
6
   % it would be best suited as
7
   head = squeeze(headin(:,:,:,1)); % I only need the tissue indices so this makes
      things easier down the line
10
   %% Data Storage
11
   QmSTORE = [0 0 26.1 11600 0 26.1 697 0 0 302 15575 0 697 1100 5192];
12
   cSTORE = [1006 4600 2110 3640 3800 1300 3720 3000 4200 2300 3680 3500 3720 3150
13
      3600];
14
   rhoSTORE = [1.3 1057 1080 1035.5 1007 1850 1126 1076 1009 916 1035.5 1151 1041
      1100 1027.4];
```

```
kSTORE = [0.026 0.51 0.65 0.534 0.5 0.65 0.527 0.4 0.594 0.25 0.565 0.4975 0.4975
             .342 .503];
       wSTORE = [0 1000 3 45.2 0 1.35 40 0 0 2.8 67.1 3.8 3.8 12 23.7];
16
17
              Get locations of holes
18
               Where two tissue types have the same probability
19
20
       idx1 = (in1==in2 | in1 == in3 | in1==in4 | in1==in5) & logical(in1);
21
       idx2 = (in1==in2 | in2 == in3 | in2==in4 | in2==in5) & logical(in2);
22
       idx3 = (in1==in3 | in2 == in3 | in3==in4 | in3==in5) & logical(in3);
23
       idx4 = (in1==in4 | in2 == in4 | in3==in4 | in4==in5) & logical(in4);
24
       idx5 = (in1==in5 | in2 == in5 | in3==in5 | in4==in5) & logical(in5);
25
       % This array will have a zero anywhere there were two or more common
26
       % elements between any of the five arrays.
27
       idx = idx1|idx2|idx3|idx4|idx5;
28
29
       [xmax ymax zmax] = size(in1)
30
31
       [x y z] = ind2sub(size(in1),find(idx)); % get x, y and z coordinates of the
             holes
32
       for i = 1:length(x) % go to each hole and do work
33
               34
                     &&(headin(x(i),y(i),z(i),1)==1) % keeps away from the edge and only looks
                       at voxels that were assigned air
35
                       [commonesttissue nouse secondbest] = mode([head(x(i)+1,y(i),z(i)))) head(x(i)+1,y(i),z(i))
                            (x_i)^{-1}, 
                            y(i),z(i)+1) head(x(i),y(i),z(i)-1));
                       if commonesttissue == 1 && length(secondbest{1})>=2 % if air and
36
                             something else are equally common, it'll choose air. This forces it to
                               pick the tissue if possible.
                               commonesttissue = secondbest{1}(2);
37
38
                       end
                       headin(x(i),y(i),z(i),:) = [commonesttissue 0 QmSTORE(commonesttissue)
39
                            cSTORE(commonesttissue) rhoSTORE(commonesttissue) kSTORE(
                             commonesttissue) wSTORE(commonesttissue)];
```

```
40 end
41 end
42 
43 out_head = headin;
44 
45 end
```

A.1.4 build_skin()

```
function [ head_out ] = build_skin( head_in )
   % build_skin() Creates a layer of skin around the head
2
3
   % This will check all voxels that were previously labeled
4
   % as soft tissue and checks if it has a neighbor which is air.
   % If so, then it is reassigned as skin.
   if ndims(head_in) == 4
8
       head_in = head_in(:,:,:,1);
9
   end
10
11
   % Git a list of all voxels labeled as muscle
12
   muscle_voxels = find(head_in==13);
13
14
   \% Go through each of them and check for neighboring air voxels
15
   for i=1:length(muscle_voxels)
16
      [x y z] = ind2sub(size(head_in), muscle_voxels(i));
17
      % makes sure we're not at a voxel at the boundry of the dataset
18
      if (x^{-1}) \&\& (x^{-size}(head_in,1)) \&\& (y^{-1}) \&\& (y^{-size}(head_in,2)) \&\& (z^{-1})
         && (z~=size(head_in,3))
        % Looks for neighboring voxels that are air
20
        if ((head_in(x+1,y,z)==1) | | (head_in(x-1,y,z)==1) | | (head_in(x,y+1,z)==1)
21
           head_in(x,y,z) = 14;
22
23
        end
24
      end
```

```
25   end
26
27   head_out = repair_headdata(head_in);
28
29   end
```

A.1.5 repair_headdata()

This function will go through the dataset and make sure the tissue-specific parameters are correct for the tissue type assigned for that voxel. fillAir(), fillholes() and build_skin() all correct mislabeled voxels, but they only correct the tissue assignment. After using any of these functions, the data must be passed through repair_headdata to update the stored parameters.

```
function [ head_out ] = repair_headdata( head_in )
1
   % repaid_headdata repopulates the headdata matrix
2
3
       If any changes are made to the index column in the headdata matrix, use
       this function to repopulate and correct the parameter values before running
4
   % any other functions.
5
      head_in can be either 3 or 4 dimenisions
6
7
8
     _____
   % = Parameter Storage =
10
   % ==========
11
12
   QmSTORE = [0 0 26.1 11600 0 26.1 697 0 0 302 15575 0 500 1100 5192];
13
   cSTORE = [1006 4600 2110 3640 3800 1300 3720 3000 4200 2300 3680 3500 3010 3150
14
      3600];
   rhoSTORE = [1.3 1057 1080 1035.5 1007 1850 1126 1076 1009 916 1035.5 1151 978.5
15
      1100 1027.4];
   kSTORE = [0.026 0.51 0.65 0.534 0.5 0.65 0.527 0.4 0.594 0.25 0.565 0.4975 0.3738
16
      .342 .503];
17
   wSTORE = [0 1000 3 45.2 0 1.35 40 0 0 2.8 67.1 3.8 3.3 12 23.7];
18
   if ndims(head_in) == 4
20
       head_in = head_in(:,:,:,1);
21
    end
```

A.2 Loading the fMRI Data

The following sections details the processing required to convert the BOLD data (in NIFTI format) to metabolism and blood flow time-courses that can then be used to calculate temperature.

A.2.1 Process_File_For_Temp()

The following code automates the procedure of processing and doing all the calculations on the dataset reported in Dhamala et al. [8]. It's is written for my data on my machine, but it can be used to gain a better understanding of the procedure. For a conceptual explanation, see section 2.3.1.

```
1
         How to process preprocessed BOLD data to calculate temperature
2
   3
4
   % This Matlab script was used to automate the the process of using BOLD data
5
6
   % stored in NIFTI (*.nii) format to calculate temperature changes.
7
   % particulars of the code may be specific to this case, but the procedure
   \% should be the same when doing these calculations on other datasets. All
8
   % required functions are included as an attachment to my thesis and are
9
   % available on my github (https://github.com/greggroth/tempcalc)
10
11
   cd('/Users/Greggory/Documents/Data/fmri_rhythmic_tapping01/NIFTI')
12
13
   directories = dir('*01');
14
15
      Move coregistered files to new Directory
16
   for i = 1:length(directories)
17
       dir_name = directories(i).name;
       main_path = cd( [dir_name filesep dir_name '_NIFTI_1'] );
19
       mkdir 'Coregistered'
20
       movefile('r*.nii','Coregistered')
21
       main_path = cd( [dir_name filesep dir_name '_NIFTI_2'] );
22
       mkdir 'Coregistered'
23
       movefile('r*.nii','Coregistered')
24
       cd(main_path)
25
26
   end
```

```
27
28
    %% Calculate Rest State
    disp('Calculating Rest State')
29
    for i = 1:length(directories)
30
        dir_name = directories(i).name;
31
        avg_NII_rest([dir_name filesep dir_name '_NIFTI_1' filesep 'Coregistered']);
32
        avg_NII_rest([dir_name filesep dir_name '_NIFTI_2' filesep 'Coregistered']);
33
    end
34
35
36
   %% Normalize to Rest and Mask
37
   disp('Normalize to Rest and Mask')
38
39
   for i = 1:length(directories)
        dir_name = directories(i).name;
40
        avg_NII_normalize([dir_name filesep dir_name '_NIFTI_1' filesep 'Coregistered'
41
          ], fullfile(dir_name, [dir_name '_NIFTI_1'], 'Coregistered', 'RestState', '
           RestStateAvg.nii'), 'fullBrainMask.nii');
        avg_NII_normalize([dir_name filesep dir_name '_NIFTI_2' filesep 'Coregistered'
42
           ], fullfile(dir_name, [dir_name '_NIFTI_2'], 'Coregistered', 'RestState', '
           RestStateAvg.nii'), 'fullBrainMask.nii');
    end
43
44
45
   %% Calculate metabolism and blood flow change
46
47
    disp('Calculate metabolism and blood flow change')
    for i = 1:length(directories)
48
        dir_1 = [ directories(i).name filesep directories(i).name '_NIFTI_1' filesep
49
           'Coregistered' filesep 'Normalized_to_rest'];
        dir_2 = [ directories(i).name filesep directories(i).name '_NIFTI_2' filesep
50
           'Coregistered' filesep 'Normalized_to_rest'];
        BOLDtoMF(dir_1);
51
52
        BOLDtoMF(dir_2);
53
    end
54
55
```

```
56
   \%\% Calculate the change in temperature based on metabolism and blood flow
57
   % load('equil.mat'); % equillibriumT
58
   % load('tt_headdata.mat'); % headdata
59
   mask = loadNII('fullBrainMask.nii');
60
61
   for i = 1:length(directories)
62
        disp([int2str(i) '-1 started'])
63
        tic
64
        % Part I
65
        actResult.dat = tempCalcDynMF(headdata, 37, 24, 720, 360, equillibriumT, ...
66
            fullfile(directories(i).name,[directories(i).name, _NIFTI_1,],,
67
               Coregistered', 'Normalized_to_rest', 'Output_18-Sep-2011', 'm.mat'),
            fullfile(directories(i).name,[directories(i).name,"NIFTI_1;],
68
               Coregistered', 'Normalized_to_rest', 'Output_18-Sep-2011', 'f.mat'),
69
            4, mask);
        % Store the parameters used for the calculations for reference in the future
70
        [c lmax] = max(actResult.dat(:));
71
        [likelymax x y z] = ind2sub(size(actResult.dat),lmax);
72
        actResult.likelymaxslice = round(likelymax/2);
73
        actResult.bloodT = 37;
74
        actResult.airT = 24;
75
76
        actResult.tmax = 360;
        actResult.stepf = 2;
77
        actResult.savestepf = 4;
78
79
        actResult.metabandflowdata = 'From Dataset';
80
        save(fullfile(directories(i).name,[directories(i).name '_NIFTI_1'],'
          Coregistered', 'Normalized_to_rest', 'Output_18-Sep-2011','tt_act_res.mat')
           , 'actResult');
81
        old = cd([directories(i).name,filesep,[directories(i).name '_NIFTI_1'],filesep
           , 'Coregistered', filesep, 'Normalized_to_rest', filesep, 'Output_18-Sep-2011'
          ]);
        writeT_to_nii(actResult, equillibriumT, exp_nii);
82
```

```
cd(old)
83
84
         clear actResult
85
        % Part II
        disp([int2str(i) '-2 started'])
86
         actResult.dat = tempCalcDynMF(headdata, 37, 24, 720, 360, equillibriumT, ...
87
             fullfile(directories(i).name,[directories(i).name '_NIFTI_2'],'
88
               Coregistered', 'Normalized_to_rest', 'Output_18-Sep-2011', 'm.mat'),
             fullfile(directories(i).name,[directories(i).name '_NIFTI_2'],'
89
               Coregistered', 'Normalized_to_rest', 'Output_18-Sep-2011', 'f.mat'),
               . . .
             4, mask);
90
91
         [c lmax] = max(actResult.dat(:));
         [likelymax x y z] = ind2sub(size(actResult.dat),lmax);
         actResult.likelymaxslice = round(likelymax/2);
93
         actResult.bloodT = 37;
         actResult.airT = 24;
         actResult.tmax = 360;
96
         actResult.stepf = 2;
97
        actResult.savestepf = 4;
98
        actResult.metabandflowdata = 'From Dataset';
99
        save(fullfile(directories(i).name,[directories(i).name '_NIFTI_2'],'
100
           Coregistered', 'Normalized_to_rest', 'Output_18-Sep-2011','tt_act_res.mat')
           , 'actResult');
101
        old = cd([directories(i).name,filesep,[directories(i).name '_NIFTI_2'],filesep
           ,'Coregistered', filesep,'Normalized_to_rest', filesep,'Output_18-Sep-2011'
           ]);
         writeT_to_nii(actResult, equillibriumT, exp_nii);
102
        cd(old)
103
        clear actResult
104
        disp([int2str(i) ' finished in ' num2str(toc)])
105
106
    end
```

A.2.2 avg_NII_normalize()

```
function [ ] = avg_NII_normalize( varargin )
1
   %UNTITLED6 Normalize to rest state
2
3
        Detailed explanation goes here
4
   %% Setup
5
    switch length(varargin)
6
        case 0
7
8
            fold_name = uigetdir('Directory Containing Data');
            if ~fold_name % Cancel Button
9
                return
10
            end
11
12
13
            [rest_file rest_path rest_index] = uigetfile('*.nii', 'Resting State NIFTI
               File');
            switch rest_index
                case 0
16
                     return
17
                case 1
                     rest_dat = load_nii(fullfile(rest_path,rest_file));
18
                     rest_dat = double(rest_dat.img);
19
                otherwise
20
                     error ('An error has occured loading the resting state data')
21
            end
22
23
24
            [mask_file mask_path mask_index] = uigetfile('*.nii', 'Mask');
            switch mask_index
25
                case 0
26
27
                     return
28
                case 1
                     mask_dat = load_nii(fullfile(mask_path, mask_file));
29
                     mask_dat = logical(mask_dat.img);
30
31
                     if max(size(mask_dat) ~= size(rest_dat))
                         error('The Mask and Resting State files must have the same
32
                            size')
33
                     end
```

```
34
                otherwise
35
                     error ('An error has occured loading the resting state data')
36
            end
        case 1
37
            fold_name = varargin{1};
38
            [rest_file rest_path rest_index] = uigetfile('*.nii','Resting State NIFTI
39
               File');
            switch rest_index
40
                case 0
41
42
                     return
                case 1
43
                     rest_dat = load_nii(fullfile(rest_path,rest_file));
44
                     rest_dat = double(rest_dat.img);
45
                otherwise
46
                     error ('An error has occured loading the resting state data')
            end
        case 2
50
            fold_name = varargin{1};
            rest_dat = loadNII(varargin{2});
51
            [mask_file mask_path mask_index] = uigetfile('*.nii', 'Mask');
52
            switch mask_index
53
                case 0
54
                     return
55
                case 1
56
57
                     mask_dat = load_nii(fullfile(mask_path, mask_file));
                     mask_dat = logical(mask_dat.img);
58
                     if max(size(mask_dat) ~= size(rest_dat))
59
                         error ('The Mask and Resting State files must have the same
                            size')
                     end
61
                 otherwise
62
                     error('An error has occured loading the resting state data')
63
            end
64
        case 3
65
            fold_name = varargin{1};
66
```

```
67
            rest_dat = loadNII(varargin{2});
68
            mask_dat = loadNII(varargin{3});
        otherwise
70
            return
    end
71
72
   % Go to the folder containing the files
73
    oldfold = cd(fold_name);
74
    file_list = dir('*.nii');
75
   file_count = length(file_list);
76
77
   % Make a directoy to save the normalized data to
78
79
   saveDir = 'Normalized_to_rest';
   if ~isdir(saveDir)
80
        mkdir(saveDir);
81
82
    end
    statusbar = waitbar(0, 'Initializing');
84
85
   \% for each file: load it, devide by the rest state and save it
86
   for i=1:file_count
87
88
        try
            waitbar(i/file_count, statusbar, [fold_name sprintf('%d%%', round((i/
89
               file_count) *100))]);
90
        catch err
            return
91
        end
92
        [file_path file_name file_ext] = fileparts(file_list(i).name);
        file_hold = load_nii(file_list(i).name);
94
        file_hold.img = double(file_hold.img)./rest_dat - 1;
95
        file_hold.img(~mask_dat) = 0;
                                                    % set everything outside the mask to
96
        file_hold.img(isnan(file_hold.img)) = 0;  % set all NaN's to 0
97
        file_hold.img(isinf(file_hold.img)) = 0;  % set all inf's to 0
98
```

```
99
         file_hold.img(file_hold.img == -1) = 0; % correct these for voxels that are
           giving me problems
         file_hold.hdr.dime.datatype = 16; % set the datatype to single
100
         file_hold.hdr.dime.bitpix = 16;
101
         save_nii(file_hold,fullfile(saveDir,[file_name '_rn' file_ext]))
102
103
    end
104
    close(statusbar)
105
    cd(oldfold)
106
107
108
    end
```

A.2.3 avg_NII_rest()

```
function [ ] = avg_NII_rest( varargin )
   %UNTITLED4 Summary of this function goes here
2
       Detailed explanation goes here
3
4
   %% Setup
5
   switch length(varargin)
6
        case 0
7
            fold_name = uigetdir;
8
            if ~fold_name % Cancel Button
9
                return
10
            end
11
        case 1
12
            fold_name = varargin{1};
14
        otherwise
15
    end
16
   % Go to the folder containing the files
17
   oldfold = cd(fold_name);
18
   file_list = dir('*.nii');
19
20
   % We're only interested in the rest period
21
22
   % (first and last 10 steps in this case)
```

```
file_list = file_list([1:10 170:180]);
24
   file_count = length(file_list);
25
   % Cell array to store all of the datasets in.
26
   datHolder = cell(file_count,1);
27
28
    statusbar = waitbar(0,'Initializing');
29
30
   for j=1:file_count
31
32
        try
            waitbar(j/file_count, statusbar, sprintf('%d%%', round((j/file_count)*100)));
33
        catch err
34
35
            return
36
        end
        fi = load_nii(file_list(j).name);
37
        datHolder{j} = fi.img;
39
    end
40
   %% Calculate the mean
41
   ymax = size(datHolder{1},2);
42
   zmax = size(datHolder{1},3);
43
    output = zeros(size(datHolder{1}));
44
45
   for i=1:ymax
46
47
        try
            waitbar(i/ymax,statusbar,sprintf('%d%%',round((i/ymax)*100)));
48
        catch err
49
            return
        end
51
        for k=1:zmax
52
            excStr = cell(length(datHolder),1);
53
            for l=1:length(datHolder)
54
                excStr{1} = [',datHolder{' int2str(1) '}(:,' int2str(i) ',' int2str(k)
55
                    ,),,,];
            end
56
```

```
comb = eval(['cat(1' cell2mat(excStr')')']);
57
            output(:,i,k) = mean(comb);
58
        end
    end
60
61
   close(statusbar)
62
63
   fi.img = output;
64
   mkdir('RestState')
65
    save_nii(fi,fullfile('RestState','RestStateAvg.nii'));
66
67
   cd(oldfold)
68
69
70
    end
```

A.2.4 BOLDtoMF()

```
function [ ] = BOLDtoMF( varargin)
   \%BOLDtoMF Calculate metabolism and blood from from BOLD reponse
2
3
   %
        Input: Directory containing a series of *.nii files of the BOLD
4
        response.
   %
5
6
   %
7
   %
        Output: Two new files will be created in a new subdirectory with a
   %
        variable for each time step.
8
9
   %
10
   %
        Usage:
11
   %
            BOLDtoMF
            BOLDtoMF(directory)
12
13
   %
        If a directory is not provided, one will be requested.
14
   %
15
       Method from Sotero, et. al. 2010
16
17
18
   % =======
19
   % = Setup =
```

```
% ======
21
   % if a folder isn't an argument, it'll prompt for one
22
    switch length(varargin)
23
        case 0
24
            fold_name = uigetdir;
25
            if ~fold_name % Cancel Button pressed
26
                return
27
            end
28
        case 1
29
            fold_name = varargin{1};
30
        otherwise
31
32
            error('Input is not understood')
33
    end
34
35
   % Go to the folder containing the files
   oldfold = cd(fold_name);
36
   file_list = dir('*.nii');
37
   file_count = length(file_list);
38
39
   % Set up a directory for the outputs
40
   newFolder = ['Output_', datestr(clock,1)];
41
42
   mkdir(newFolder)
43
44
   % Make *.mat files to append the data to
   m0001 = 0; f0001 = 0;
45
    save(['./' newFolder '/m.mat'],'m0001');
46
    save(['./' newFolder '/f.mat'],'f0001');
47
48
   s = loadNII(file_list(1).name);
49
   norm = ones(size(s));
50
51
   % =======
52
   % = Do Work =
53
54
   % ========
```

```
55
   \% This will calculate the metabolism and blood flow. The output is
56
   % appended to 'm.mat' and 'f.mat' within a new folder created
57
   % within the directory containing the data.
58
   statusbar = waitbar(0, 'Initializing');
59
60
   maxBOLD = 0.22;
61
62
   % Required Parameters
63
                        b c A
   % [alpha beta a
64
   p = [0.4 1.5 0.1870 0.1572 -0.6041 maxBOLD];
65
66
67
   % Calc flow and metabolism for when BOLD = 1
   s = 0;
68
   y = -((p(4)*p(2))/(p(1)+p(2)*p(5)))*((p(6)-s)/(p(6)*p(3)^p(2)))^(1/(p(1)+p(2)*p(5)))
      ));
   fNOACT = -((p(1)+p(2)*p(5))/(p(4)*p(2)))*lambertw(y);
   mNOACT = p(3)*fNOACT^(p(5)+1)*exp(-p(4)*fNOACT);
71
72
73
   %% Calc flow and metabolism
74
   disp(fold_name)
75
   for j=1:file_count
76
77
        try
78
          waitbar(j/file_count, statusbar, sprintf('%d%%', round((j/file_count)*100)))
        catch err
79
            return
81
        end
        s = loadNII(file_list(j).name); % Load up the file
82
        s(isnan(s)) = 1;
83
        s(isinf(s)) = 1;
84
        y = -((p(4)*p(2))/(p(1)+p(2)*p(5))).*((p(6)-s)./(p(6)*p(3)^p(2))).^(1/(p(1)+p(2)*p(3))).
85
          (2)*p(5));
        if (size(y,1)==91) &&(size(y,2)==109) &&(size(y,3)==91)
86
```

```
87
             f = -((p(1)+p(2)*p(5))/(p(4)*p(2))).*lambw_mex(real(y));
88
         else
             f = -((p(1)+p(2)*p(5))/(p(4)*p(2))).*lambw(y);
89
90
         end
         m = p(3)*f.^(p(5)+1).*exp(-p(4)*f);
91
         % Clean up NaNs that may have popped up
92
         m(isnan(m))=1;
93
         f(isnan(f))=1;
94
         % Normalize to resting m and f
95
         m = m./mNOACT;
96
         f = f./fNOACT;
97
98
99
         % Rename and save the data
         eval(['m' sprintf('%04d',j) ' = m;']);
100
         eval(['f' sprintf('%04d',j) ' = f;']);
101
         eval(['save(''./' newFolder '/m.mat'', ''m' sprintf('%04d',j) ''',''-append'')
102
         eval(['save(''./' newFolder '/f.mat'', ''f' sprintf('%04d',j) ''',''-append'')
103
            ; ']);
         clear m0* f0*
104
105
     end
106
107
     close(statusbar)
108
     cd(oldfold)
109
110
    end
```

A.2.5 lambw() and lambw_mex()

The lambw() function is a wrapper for the wapr() function available on Matlab FileExchange (http://www.mathworks.com/matlabcentral/fileexchange/3644-real-values-of-the-lambert-w-function/content/Lambert/wapr.m). A compiled version of this function (lambw_mex()) runs much faster and is recommended. This function is used over Matlab's built-in Lambert-W function for the sake of performance.

```
1 function [ array_out ] = lambw( array_in )
2 % lambw Wrapper for wapr()
```

```
% Available: http://www.mathworks.com/matlabcentral/fileexchange/3644-real-values
      -of-the-lambert-w-function/content/Lambert/wapr.m
        Dwapr() doesn't work any arrays over Nx1, so this steps through the
       full matrix and gives the rows to wapr. Works pretty fast.
5
6
7
   %#codegen
8
   if ndims(array_in) ~= 3
9
        error('This only works (for now) with a three dimensional array.')
10
    end
11
12
   xmax = size(array_in,1);
13
14
   ymax = size(array_in,2);
15
   array_out = zeros(size(array_in));
16
17
   for ix=1:xmax
18
        for iy=1:ymax
            array_out(ix,iy,:) = wapr(array_in(ix,iy,:));
19
20
        end
   end
21
22
23
    end
```

A.3 Calculating the Equilibrium Temperature

In order to determine the temperature fluctuations due to changes in activity, the baseline temperature must first be established for each voxel. The function tempCalcEquilibrium() will update the temperature using the Penne's bioheat equation (eq. (2.7)) until the change in temperature for each voxel falls below a certain threshold. Details about this procedure are available in section 2.3.1.

A.3.1 tempCalcEquilibrium()

```
function temperature_Out = tempCalcEquillibrium(tissue,bloodT,airT,nt,tmax,
      pastCalc,printprogress)
2
   % tempCalcEquillibrium Find the equillibrium values
        tissue: holds all of the strucual information
3
   %
        bloodT: Temperature of the blood
4
   %
        airT:
                Temperature of the surrounding ait
5
                Max number of time steps
6
   %
        nt:
7
                Total amount of time the simulation should run over
8
   %
   %
        This is based off of tempCalc() but loops until the rate of change of
9
        a each voxel is sufficiently small then outputs what's
10
   %
11
        calculated. If if takes too long to do all at once, split it up into
        smaller time chunks and use the last step from the previous dataset as
12
   %
        pastCalc in order to resume.
   %
13
   %
14
   %
        Note: This does not save the time corse because it can take a lot of step to
15
        find the equillibrium. It outputs the last time step.
   %
16
   %
17
18
   %
        Writen by Greggory Rothmeier (greggroth@gmail.com)
        Georgia State University Dept. Physics and Astronomy
19
   %
        May, 2011
20
   %
   tic
21
         Default Values
22
   if nargin<2, bloodT = 37;</pre>
                                      end
   if nargin<3, airT = 24;</pre>
24
                                      end
   if nargin<4, nt = 100;</pre>
25
                                      end
   if nargin<5, tmax = 50;</pre>
26
                                      end
```

```
if nargin<6, pastCalc = 0;</pre>
   if nargin<7, printprogress = 1; end</pre>
28
29
   % These rescue the data if the calculation is interrupted.
30
   global temperature
31
    global dirty
32
33
   c = onCleanup(@InterCatch);
34
   dirty = 1;
35
36
   dx = 2*10^-3;
                         % Voxel size (m)
37
38
39
   if nt<(2*tmax),</pre>
       warning ('Time step size is not large enough. Results will be unreliable.
          Consider increasing the number of steps or reducing tmax.')
    end
42
43
   \% Constants used that aren't already stored in tissue
44
    [xmax ymax zmax t] = size(tissue);
45
   clear t;
46
   dt = tmax/(nt-1);
47
   % rhoBlood = 1057;
48
   % wBlood = 1000;
49
50
   % cBlood = 3600;
51
   % =======
52
   % = Setup =
   % =======
54
      Starts all tissue voxels at bloodT (default 37) and maintains air at airT (
55
      default 24)
        The condition squeeze(tissue(:,:,:,)~=airIndex picks out the elements that are
56
        tissue
   %
57
58
59
   temperature = ones(3,xmax,ymax,zmax,'single')*airT;
```

```
if pastCalc == 0
61
        temperature(1, squeeze(tissue(:,:,:,1))~=1) = bloodT;
62
    else
        temperature(1,:,:,:) = pastCalc;
63
64
   end
   numElements = numel(temperature(1,:,:,:));
65
66
   % ========
67
   % = Do Work =
68
69
       This is a vectorized version of the next section. For the love of god
70
       don't make any changes to this without first looking below to make sure
71
   %
72
       you know what you're changing. This is [nearly] impossible to
   %
        understand, so take your time and don't break it.
73
   %
        data is stored in 'tissue' as such :
74
        [tissuetype 0 Qm c rho k w]; <-- second element is blank for all.
75
76
            1
                    2 3 4 5 6 7
77
      This makes an array that has smoothed out variations in k by averaging all
78
      of the k's around each voxel (including itself). This is a hap-hazard
79
      solution to the problem that if you only take the value of k for the voxel
80
      without considering what surrounds it, it doesn't matter whether the head
81
      is surrounded by air, water or anything else. Since water is a better
82
      thermal conductor than air, we need a way of accounting for this. This is
83
84
      one way:
   averagedk = (circshift(tissue(:,:,:,6),[1 0 0])+circshift(tissue(:,:,:,6),[-1 0
85
      0])+circshift(tissue(:,:,:,6),[0 1 0])+circshift(tissue(:,:,:,6),[0 -1 0])+
      circshift(tissue(:,:,:,6),[0 0 1])+circshift(tissue(:,:,:,6),[0 0 -1])+tissue
      (:,:,:,6))/7;
   rhoblood = 1057;
86
    cblood = 3600;
87
88
   %% Specify Percision Goal
89
                     % fraction of voxels have a slope less than 'zeropoint'
90
   tolerence = 1;
```

```
91
    zeropoint = 2.5e-7; % point at which the slope between two *steps* is considered
       essentially zero
92
93
    goal = numElements - tolerence*numElements;
94
    goon = numElements; % Forces the while loop to run the first time
95
    format shortG;
96
    % temperature(1,:,:,:) = Current Temperature
97
    % temperature(2,:,:) = Next Temperature
98
    % Resets after each update
99
    if printprogress
100
        disp(['Goal: ', num2str(goal),' remaining voxels'])
101
102
    end
103
    t2 = 1;
    while goon(1)>goal && t2<=nt % runs until either 'goal' elements have a slope
104
       greater than 'zeropoint' or it exceeds nt
105
       if printprogress
        disp([t2 goon(1) ((numElements-goon(1))/numElements)*100]) % progress
106
107
       end
       temperature(2,:,:) = squeeze(temperature(1,:,:,:)) + ...
108
             dt/(tissue(:,:,:,5).*tissue(:,:,:,4)).* ...
109
             ((averagedk/dx^2).*...
110
111
             (circshift(squeeze(temperature(1,:,:,:)),[1 0 0])-2*squeeze(temperature
                (1,:,:,:))+circshift(squeeze(temperature(1,:,:,:)),[-1 0 0])+... %
               shift along x
112
              circshift(squeeze(temperature(1,:,:,:)),[0 1 0])-2*squeeze(temperature
                 (1,:,:,:))+circshift(squeeze(temperature(1,:,:,:)),[0 -1 0])+... %
                shift along y
              circshift(squeeze(temperature(1,:,:,:)),[0 0 1])-2*squeeze(temperature
113
                 (1,:,:,:))+circshift(squeeze(temperature(1,:,:,:)),[0 0 -1]))... %
                shift along z
114
                 -(1/6000)*rhoblood*tissue(:,:,:,7)*cblood.*(squeeze(temperature
                    (1,:,:,:))-bloodT)+tissue(:,:,:,3));
115
             resets the air temperature back since it's also modified above, but
        %
        %
             it needs to be kept constant throughout the calculations
116
```

```
temperature(2, squeeze(tissue(:,:,:,1))==1) = airT;
117
118
             checks how quickly the temperature is changing and if it is close
             enough to zero to be considered stopped ('zeropoint')
119
         goon = size(temperature(abs(squeeze(temperature(2,:,:,:)-temperature(1,:,:,:))
120
           )>zeropoint));
         temperature(1,:,:,:) = temperature(2,:,:,:); % moves 2 back to 1
121
122
        t2 = t2 + 1;
123
     end
124
    temperature_Out = temperature(2,:,:,:);  % Only outputs the last time step
125
    dirty = 0;
126
127
128
    % equilTemperature = temperature_Out;
    % save('equil.mat','equilTemperature');
129
130
131
    %% To Combine Datasets
132
    % = 10^{-6} use this technique if there are seperate datasets that need combining
          vertcat(squeeze(res1(:,:,:,:)),squeeze(res2(2:end,:,:,:)))
133
       Where for all by the first dataset, you need to do the time from 2:end
134
       so that there are no repeats (remember that the last timestep from the
135
    % previous dataset serves as the first for the new one)
136
137
138
139
    time = toc;
140
    end
141
    function InterCatch
142
    global dirty
143
    if dirty
144
         disp('Interupt Intercepted. Inprepretating Interworkspace Data.')
145
         global temperature
146
147
        % equillibriumT = zeros([1 size(temperature(1,:,:,:))]);
         % equillibriumT(1,:,:,:) = temperature(1,:,:,:); %might be better to swtich
148
            equilT to be 3d rather than 4d
149
         equillibriumT = temperature;
```

A.4 Calculating the Temperature Change

The following function inputs the head data matrix (appendix A.1), the metabolism and blood flow time courses (crefsec:fmriprocessing) and the equilibrium temperatures (appendix A.3) and calculates the temperature time-course. More details about this algorithm can be found in section 2.3.1.

A.4.1 tempCalcDynMF

```
function temperatureOut = tempCalcDynMF(tissue,bloodT,airT,nt,tmax,pastCalc,metab,
       flow, savesteps, region)
   % tempCalcChaning Metabolism How does changin metabolism
2
   % affect things?
3
4
        tissue: holds all of the strucual information
5
   %
    %
        bloodT: Temperature of the blood
6
7
   %
        airT:
                 Temperature of the surrounding ait
                 Number of time steps
8
   %
        nt:
                 Total amount of time the simulation should run over
9
   %
        tmax:
10
   %
   %
        region: logical matrix same size as head
11
12
   %
        Writen by Greggory Rothmeier (greggroth@gmail.com)
13
   %
   %
        Georgia State University Dept. Physics and Astronomy
14
        May, 2011
    statusbar = waitbar(0,'Initializing');
17
18
   %%
         Default Values
19
    if nargin<2, bloodT = 37;</pre>
                                           end
20
    if nargin<3, airT = 24;</pre>
                                           end
21
   if nargin<4, nt = 3;</pre>
                                           end
22
23
    if nargin<5, tmax = 1;</pre>
                                           end
    if nargin<6, pastCalc = 0;</pre>
24
                                           end
25
26
   % Length of one side of a voxel (m)
```

```
dx = 2*10^-3;
   if nt < (2*tmax),
30
       warning ('Time step size is not large enough. Results will be unreliable.
31
          Consider increasing the number of steps or reducing tmax.')
    end
32
33
34
   % Constants used that aren't already stored in tissue
35
   [xmax ymax zmax t] = size(tissue);
36
37
   clear t;
   dt = ones([xmax ymax zmax])*(tmax/(nt-1));
38
39
   % rhoBlood = 1057;
   % wBlood = 1000;
   % cBlood = 3600;
41
42
43
   %% Determine Metab/Flow Data Storage System
   if ischar(metab)&&ischar(flow)
44
      % if file locations are given rather than data
45
        option = 1;
46
   else
47
      \% Preallocate matrices for holding metabolism and blood flow data
48
        metabMulti = ones([xmax ymax zmax],'single');
49
        flowMulti = ones([xmax ymax zmax],'single');
50
51
        option = 0;
   end
52
53
54
   %% Maps
   % Creates a map that identifies where there is tissue
   % the condition squeeze(tissue(:,:,:,)~=airIndex picks out the
56
   % elements that are tissue
57
58
   tmax = ceil((nt-1)/savesteps);
59
   temperatureOut = ones(tmax,xmax,ymax,zmax,'single');
60
   temperature = ones(2,xmax,ymax,zmax,'single')*airT;
61
```

```
if pastCalc == 0
63
       temperature(1, squeeze(tissue(:,:,:,1))~=1) = bloodT;
64
   else
     % Starts everything off at the pre-determined equilibium temperatures
65
       temperature(1,:,:,:) = pastCalc(end,:,:,:);
66
   end
67
   temperatureOut(1,:,:,:) = temperature(1,:,:,:);
68
69
70
   % ========
71
   % = Do Work =
72
   % ========
73
74
       This is a vectorized version of the next section. For the love of
       god don't make any changes to this without first looking below to
75
   %
       make sure you know what you're changing. This is [nearly]
76
       impossible to understand, so take your time and don't break it.
77
       data is stored in 'tissue' as such :
      [tissuetype 0 Qm c rho k w] <-- second element is blank for all.
79
          1
                  2 3 4 5 6 7]
80
81
   % This makes an array that has smoothed out variations in k by
82
   83
   \% is a hap-hazard solution to the problem that if you only take the
84
   % value of k for the voxel without considering what surrounds it, it
85
86
   % doesn't matter whether the head is surrounded by air, water or
   % anything else. Since water is a better thermal conductor than air, we
87
   % need a way of accounting for this. This is one way:
88
89
   averagedk = (circshift(tissue(:,:,:,6),[1 0 0])+circshift(tissue(:,:,:,6),[-1 0
90
      0])+circshift(tissue(:,:,:,6),[0 1 0])+circshift(tissue(:,:,:,6),[0 -1 0])+
      circshift(tissue(:,:,:,6),[0 0 1])+circshift(tissue(:,:,:,6),[0 0 -1])+tissue
      (:,:,:,6))/7;
   rhoblood = 1057;
91
   cblood = 3600;
92
93
```

```
Only saves every 4 steps to reduce the final matrix size
95
    for t2 = 1:nt-1
96
        waitbar (t2/(nt-1), statusbar, sprintf(', d, d, d, round(t2/(nt-1)*100)));
97
    % = 10^{10} if a variable needs to be used multiple times for the same time step.
98
       t3 = floor((t2-1)/4)+1; % 1 1 1 1 2 2 2 2 3 3 . . .
99
100
       \% if a file is specified, pulls the data from the file for each step
101
102
        if option
            eval(strcat('load(fullfile(metab),''-mat'',''m',sprintf('%04d',t3),'''));'))
103
            eval(strcat('load(fullfile(flow),''-mat'',''f',sprintf('%04d',t3),''');'));
104
105
            eval(strcat('metabMulti = m', sprintf('%04d',t3),';'));
106
            eval(strcat('flowMulti = f', sprintf('%04d', t3), ';'));
            eval(strcat('clear f', sprintf('%04d',t3),' m',sprintf('%04d',t3)))
107
108
        else
109
            metabMulti(region) = metab(t2);
                                               % region is hardcoded here
            flowMulti(region) = flow(t2);
110
        end
111
112
        temperature(2,:,:) = squeeze(temperature(1,:,:,:)) + ...
113
             dt./(tissue(:,:,:,5).*tissue(:,:,:,4)).* ...
114
115
             ((averagedk/dx^2).*...
             (circshift(squeeze(temperature(1,:,:,:)),[1 0 0])-2*squeeze(temperature
116
                (1,:,:,:))+circshift(squeeze(temperature(1,:,:,:)),[-1 0 0])+... %
                shift along x
117
              circshift(squeeze(temperature(1,:,:,:)),[0 1 0])-2*squeeze(temperature
                 (1,:,:,:))+circshift(squeeze(temperature(1,:,:,:)),[0 -1 0])+... %
                 shift along y
              circshift(squeeze(temperature(1,:,:,:)),[0 0 1])-2*squeeze(temperature
118
                 (1,:,:,:))+circshift(squeeze(temperature(1,:,:,:)),[0 0 -1]))... %
                 shift along z
                 -(1/6000)*rhoblood*flowMulti.*tissue(:,:,:,7)*cblood.*(squeeze(
119
                    temperature(1,:,:,:))-bloodT)+metabMulti.*tissue(:,:,:,3));
         \% resets the air temperature back since it's also modified above,
120
```

```
121
         % but it needs to be kept constant throughout the calculations
122
         temperature(2, squeeze(tissue(:,:,:,1)) == 1) = airT;
         temperatureOut(ceil(t2/savesteps),:,:,:) = temperature(2,:,:,:);
123
         temperature (1,:,:,:) = temperature (2,:,:,:); % moves 2 back to 1
124
         clear metabMulti flowMulti
125
126
    end
127
     close(statusbar);
128
    % ========
129
    % = Old Code =
130
    % ========
131
    % This is what used to be used. It's much slower (~60 times slower),
132
133
    % but it's much easier to understand compared to the above code. If any
134
    % changes need to be made above, first look through this code to ensure
    % you understand what's happening before making changes. It's really
135
136
    % easy to mess up the code above and nearly impossible to figure out
    % where.
137
138
    %
139
       good luck.
140
    % for t2 = 1:nt-1
141
           for x2 = 2:xmax-1
    %
142
143
    %
               for y2 = 2:ymax-1
144
                   for z2 = 2:zmax-1
    %
145
    %
                       if tissue(x2,y2,z2,1) ~= 1,
                            temperature(t2+1,x2,y2,z2) = temperature(t2,x2,y2,z2) + (dt
146
       /(tissue(x2,y2,z2,5)*tissue(x2,y2,z2,4)))*((tissue(x2,y2,z2,6)/dx^2)*...
    %
147
                              (temperature(t2,x2+1,y2,z2)-2*temperature(t2,x2,y2,z2)+
       temperature (t2,x2-1,y2,z2)+...
    %
                              temperature (t2, x2, y2+1, z2) -2* temperature (t2, x2, y2, z2) +
148
       temperature (t2, x2, y2-1, z2)+...
149
                              temperature(t2,x2,y2,z2+1)-2*temperature(t2,x2,y2,z2)+
       temperature(t2,x2,y2,z2-1))...
    %
                              -(1/6000)*rhoBlood*wBlood*cBlood*(temperature(t2,x2,y2,z2)
150
       -bloodT)+tissue(x2,y2,z2,3));
```

Appendix B

Visualization Tools

The temperature data is a four dimensional dataset (time, x, y and z), so good visualizations tools are necessary to analyzing the results. The primary tool I use is a modification of SliceBrowser (http://www.mathworks.com/matlabcentral/fileexchange/20604) and is provided as part of temptools (https://github.com/greggroth/tempcalc/tree/master/tt/supportfcts/SliceBrowser). In working with this, I also created a function (TempPlot()) to act as a wrapper and handle possible plotting situations depending on the number of inputs.

B.0.2 TempPlot()

```
function [ ] = TempPlot( head, tempdata, highlightRegion, slice, equil, threshold,
      point)
   %TempPlot Plot data from tempCalc() or BulkImportNII()
2
        INPUT TempPlot(structuredata)
3
              TempPlot(structuredata, temperaturedata)
4
   %
              TempPlot(structuredata,temperaturedata,highlightRegion)
5
   %
              TempPlot(structuredata,temperaturedata,highlightRegion,slice)
6
   %
7
              TempPlot(structuredata, temperaturedata, highlightRegion, slice,
      EquillibriumData)
   %
8
   %
        This function with determine which type of data it is and then plot it
9
   %
        appropiately.
10
   %
11
        equil - Equillibrium state data
12
   %
```

```
13
        threshold - threshold value for being displayed as an overlay
        REQUIRES: SliceBrowser (http://www.mathworks.com/matlabcentral/fileexchange
      /20604)
   %% Error checking and data restructuring where necessary
15
   if ndims(head) == 4
16
        head = head(:,:,:,1);
17
    elseif ndims(head) ~= 3
18
        error('Input ''head'' must have either 3 or 4 dimensions');
19
20
    end
21
   if nargin > 1
22
        if ndims(tempdata) == 3 % should only happen when comparing two equilibrium
23
           datasets
        temp = tempdata;
        tempdata = zeros([1 size(temp)]);
25
26
        tempdata(1,:,:,:) = temp;
27
        elseif ndims(tempdata) ~= 4
        error('Input ''tempdata'' must have either 3 or 4 dimensions');
28
        end
29
        tempdataShort = squeeze(tempdata(end,:,:,:));
30
    end
31
32
   if nargin > 2
33
        if ndims(highlightRegion) ~= 3
34
35
        error('Input ''highlightRegion'' must have 3 dimensions');
        end
36
        if size(highlightRegion) ~= size(head)
37
        error('Input ''highlightRegion'' must be of the same size as ''head'');
        end
39
        tempdataShort = squeeze(tempdata(end,:,:,:));
40
    end
41
42
43
   if nargin > 3
        if slice > size(tempdata,1)
44
```

```
45
        error('Input ''slice'' must be less or equal to the length of the first
           dimension of ''tempdata'');
46
        end
        tempdataShort = squeeze(tempdata(slice,:,:,:));
47
48
    end
49
    if nargin > 4
50
        if ndims(equil) == 3
51
            eq = equil;
52
        elseif ndims(equil) == 4
53
            eq = squeeze(equil(1,:,:,:));
54
        else
55
            error('Input ''equil'' must have either 3 or 4 dimensions');
56
        end
57
        clear 'equil';
58
    end
       Pick how to format the call of SliceBrowser()
61
    switch nargin
62
        case 1
63
        SliceBrowser(head,1,head);
64
        colormap(gray);
65
        case 2
66
        %SliceBrowser(squeeze(tempdata(size(tempdata,1),:,:,:)),tempdata,head);
67
68
        SliceBrowser(tempdataShort,tempdata,head);
        case 3
69
        SliceBrowser (tempdataShort, tempdata, head, highlightRegion);
        case 4
        SliceBrowser(tempdataShort,tempdata,head,highlightRegion);
72
        case 5
73
        SliceBrowser(tempdataShort-eq,tempdata,head,highlightRegion);
74
75
        {\tt SliceBrowserOverlay(tempdataShort-eq,tempdata,head,highlightRegion,threshold);}
76
        case 7
77
        imgoverlay(head,tempdataShort-eq,point,threshold)
78
```

```
79 end
80 81 end
```

B.0.3 tsliceplot

This is a visualization tool I wrote that allows you to view the change in temperature versus time for a line passing through the head. Screenshots of the tool can be seen in figs. B.1 and B.2.

Usage:

```
tsliceplot(temperature_data, equilibrium_temperature_data)
```

The script is available as part of temptools (https://github.com/greggroth/tempcalc/tree/master/t/supportfcts/tsliceplot).

Figure B.1: Experimental data for activity in the motor cortex visualized with tsliceplot.

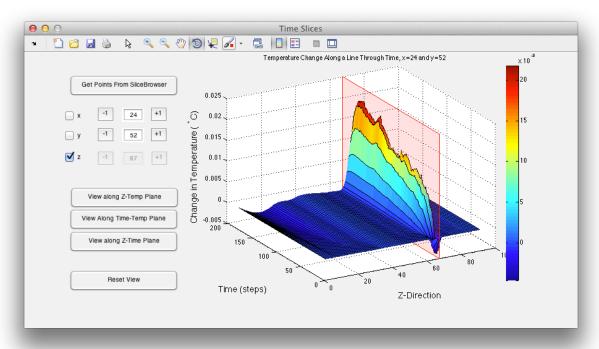


Figure B.2: The same data as is presented in fig. B.1, but viewed flat-on along the z vs. time plane.

