

Estimating fMRI Timescale Maps

UC San Diego
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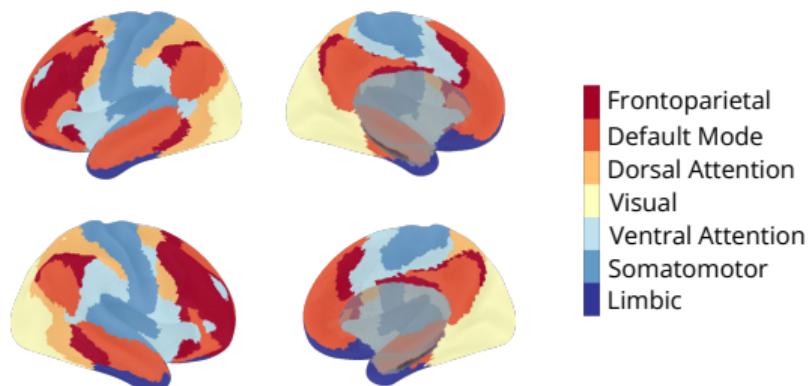
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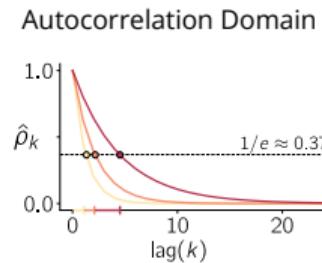
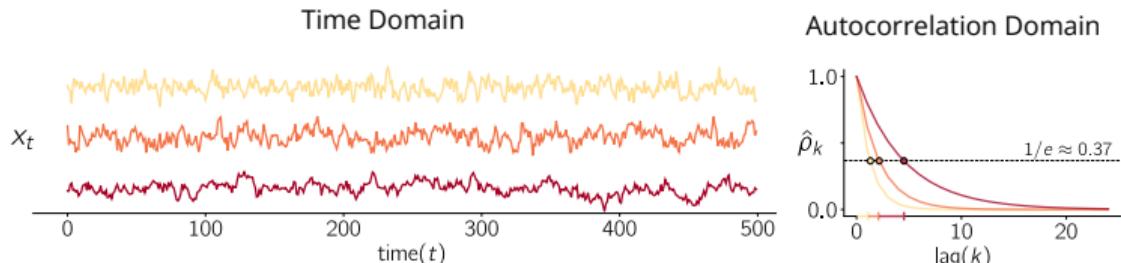
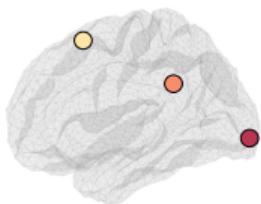
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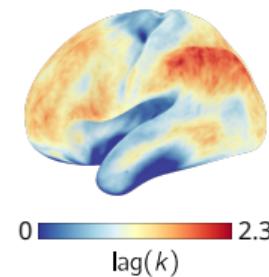


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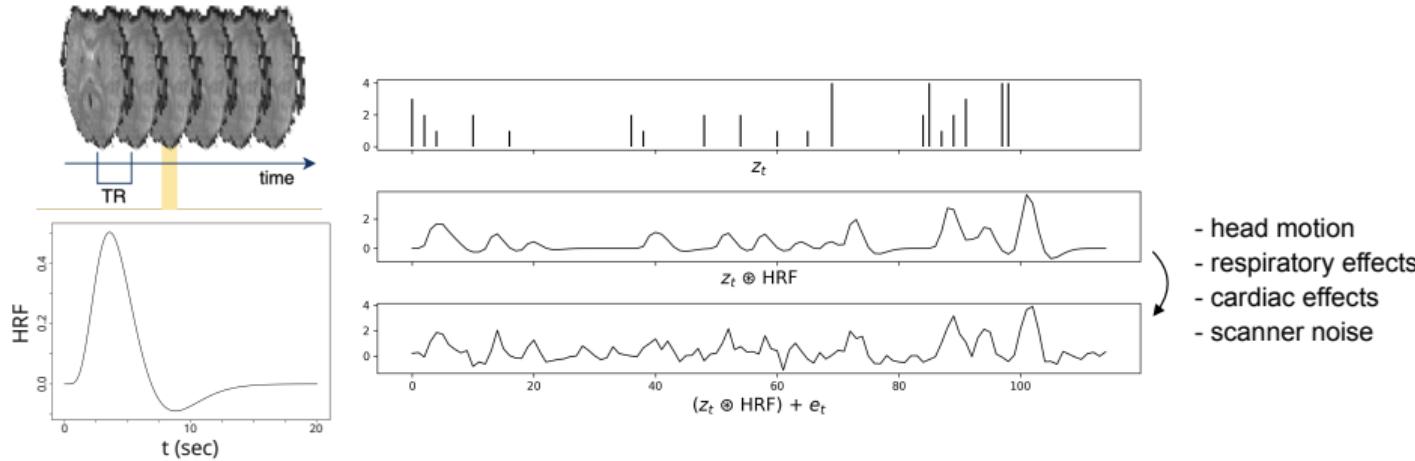
- Neural time series exhibit time-lagged correlations that decay, reflecting how brain regions integrate information over time.
- The timescale parameter quantifies the rate of decay.
- Timescale maps follow a hierarchical organization across the cortex: fast autocorrelation decay in sensory areas, slow in associative areas.



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- Resting-state functional magnetic resonance imaging (fMRI) provides whole-brain noninvasive recording of spontaneous brain activity.
- An fMRI time series reflects hemodynamic changes of the underlying electrical activity of neurons.

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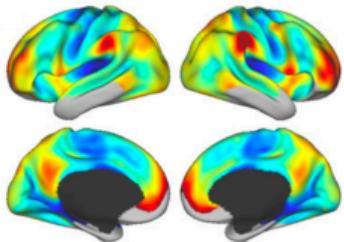
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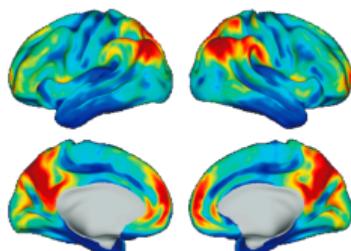
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A. Cortical fMRI Timescale Maps



Raut et al., 2020



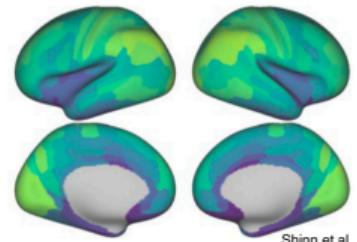
Mitra et al., 2014



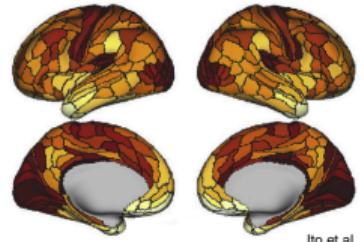
Lurie et al., 2024



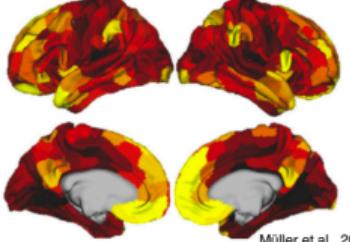
Shafeei et al., 2020



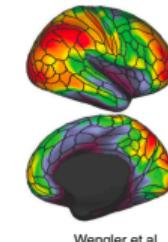
Shinn et al., 2023



Ito et al., 2020

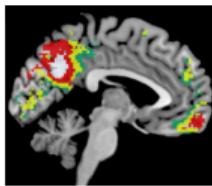


Müller et al., 2020

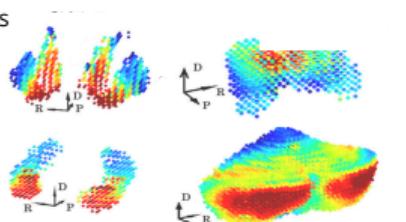


Wengler et al., 2020

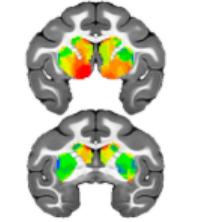
B. Subcortical fMRI Timescale Maps



Kaneoke et al., 2012



Raut et al., 2020



Manea et al., 2022

Existing Methods

- Time-Domain Linear Model [6/25 papers]
- Autocorrelation-Domain Nonlinear Model [18/25 papers]
- (Frequency-Domain Nonlinear Model [3/25 papers])

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Limitations of Existing Methods

- Assume exponentially decaying autocorrelation, which may not hold.
- Provide only point estimates without standard errors, limiting statistical inference.

Contributions

- Generalize assumptions to include all stationary and mixing processes.
- Introduce standard errors that account for misspecified autocorrelation decay.
- Establish statistical properties: consistency and asymptotic normality.
- Demonstrate parameter recovery in realistic simulations.
- Apply methods to fMRI data from the Human Connectome Project (HCP).

Assumptions

Let $\{X_t, t \in \mathbb{Z}\}$ be a discrete-time stochastic process that is **stationary** and **strong mixing**, and $x_t = \{x_1, x_2, \dots, x_T\}$ be an observed sample of X_t . Assume X_t and x_t are demeaned.

Stationarity Implies

$$\gamma_k = \text{cov}[X_t, X_{t-k}] = \mathbb{E}[X_t X_{t-k}], \quad (1)$$

$$\rho_k = \text{corr}[X_t, X_{t-k}] = \gamma_0^{-1} \gamma_k. \quad (2)$$

Mixing Implies

- Ergodicity, ensuring consistent estimation by the ergodic theorem.
- Autocorrelations (2) decay sufficiently fast to apply a central limit theorem for correlated observations.

Hansen [2022], White and Domowitz [1984], Newey and West [1987]

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Autoregressive Model (AR1) Projection

$$X_t = \phi X_{t-1} + e_t \quad (3)$$

Squared Error Minimization

$$S(\phi) = \mathbb{E}[(X_t - \phi X_{t-1})^2], \quad \phi^* = \operatorname{argmin}_{\phi} S(\phi) \quad (4)$$

Timescale Definition

$$\phi^* = (\mathbb{E}[X_{t-1}^2])^{-1} (\mathbb{E}[X_t X_{t-1}]) \quad (5)$$

$$\tau^* = g(\phi^*) = -\frac{1}{\log(|\phi^*|)} \quad (6)$$

Linear Least Squares (LLS) Estimation

$$\hat{\phi}_{LLS}^* = \left(\sum_{t=2}^T X_{t-1}^2 \right)^{-1} \left(\sum_{t=2}^T X_t X_{t-1} \right) \quad (7)$$

$$\hat{\tau}_{LLS}^* = g(\hat{\phi}_{LLS}) = -\frac{1}{\log(|\hat{\phi}_{LLS}|)} \quad (8)$$

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Exponential Decay Model Projection

$$\rho_k = \phi^k + e_k, \text{ for } k \in \{0, 1, \dots, K\} \quad (9)$$

Squared Error Minimization

$$S(\phi) = \mathbb{E}[(\rho_k - \phi^k)^2], \quad \phi^* = \operatorname{argmin}_{\phi} S(\phi) \quad (10)$$

Timescale Definition

$$\tau^* = g(\phi^*) = -\frac{1}{\log(|\phi^*|)} \quad (11)$$

Nonlinear Least Squares (NLS) Estimation

$$\hat{\phi}_{\text{NLS}}^* = \operatorname{argmin}_{\phi} \hat{S}(\phi) \quad (12)$$

$$\hat{\tau}_{\text{NLS}}^* = g(\hat{\phi}_{\text{NLS}}^*) = -\frac{1}{\log(|\hat{\phi}_{\text{NLS}}^*|)} \quad (13)$$

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Standard Error Estimation

1. Time-Domain Method

$$\widehat{se}_{NW}(\hat{\phi}_{LLS}^*) = \sqrt{\hat{q}^{-1} \hat{\omega} \hat{q}^{-1}}, \quad \widehat{se}_{NW}(\hat{\tau}_{LLS}^*) \approx \widehat{se}_{NW}(\hat{\phi}_{LLS}^*) \cdot \frac{d}{d\phi} g(\hat{\phi}_{LLS}^*) \quad (14)$$

$$\hat{q} = \frac{1}{T} \sum_{t=2}^T x_{t-1}^2, \quad \hat{\omega} = \sum_{\ell=-M}^M \left(1 - \frac{|\ell|}{M+1}\right) \frac{1}{T} \sum_{1 \leq t-\ell \leq T} (x_{t-1} \cdot \hat{e}_t)(x_{t-1-\ell} \cdot \hat{e}_{t-\ell}) \quad (15)$$

2. Autocorrelation-Domain Method

$$\widehat{se}_{NW}(\hat{\phi}_{NLS}^*) = \sqrt{\hat{q}^{-1} \hat{\omega} \hat{q}^{-1}}, \quad \widehat{se}_{NW}(\hat{\tau}_{NLS}^*) \approx \widehat{se}_{NW}(\hat{\phi}_{NLS}^*) \cdot \frac{d}{d\phi} g(\hat{\phi}_{NLS}^*) \quad (16)$$

$$\hat{m}_{\phi,k} = k \hat{\phi}_{NLS}^{*k-1}, \quad \hat{q} = \frac{1}{K} \sum_{k=0}^K (\hat{m}_{\phi,k})^2, \quad \hat{\omega} = \sum_{\ell=-M}^M \left(1 - \frac{|\ell|}{M+1}\right) \frac{1}{K} \sum_{1 \leq k-\ell \leq K} (\hat{m}_{\phi,k} \cdot \hat{e}_k)(\hat{m}_{\phi,k-\ell} \cdot \hat{e}_{k-\ell}) \quad (17)$$

3. Autocorrelation/Time-Domain Method, equation (14) except for:

$$\hat{e}_t = x_t - \hat{\phi}_{NLS}^* \cdot x_{t-1} \quad (18)$$

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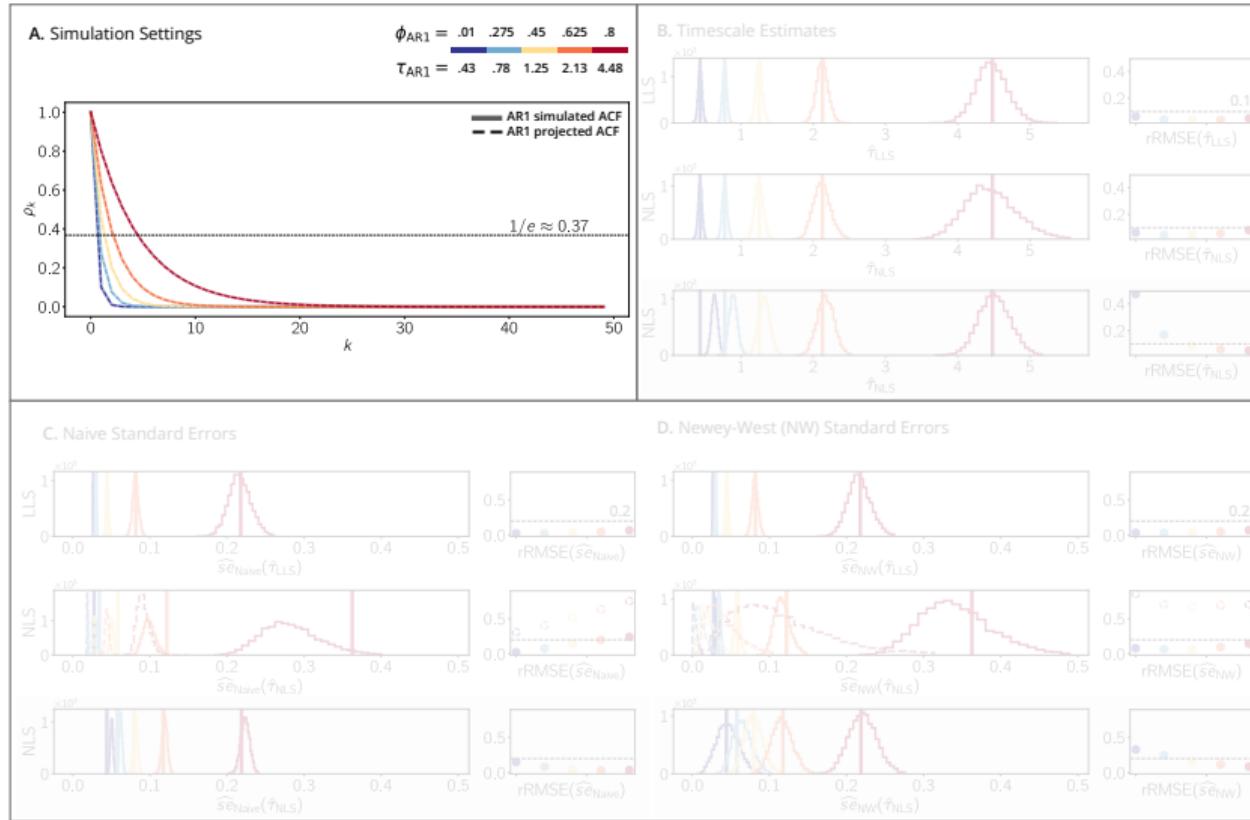
References

AR1 Simulations

$N = 10,000$ repeats, $T = 4,800$ timepoints

$$x_t = \phi x_{t-1} + e_t, \quad e_t \sim \mathcal{N}(0, 1) \quad \rho_k = \phi^k + e_k, \quad e_k \sim \mathcal{N}(0, 1)$$

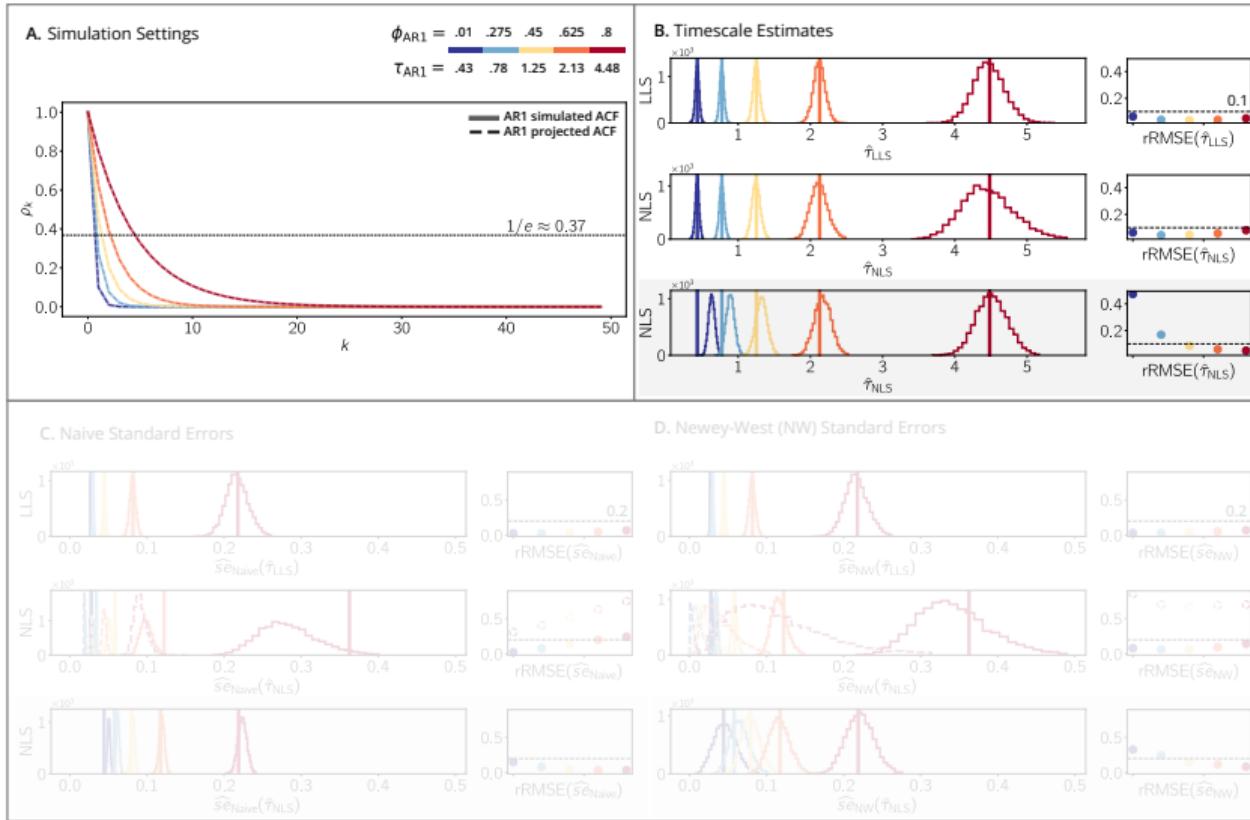
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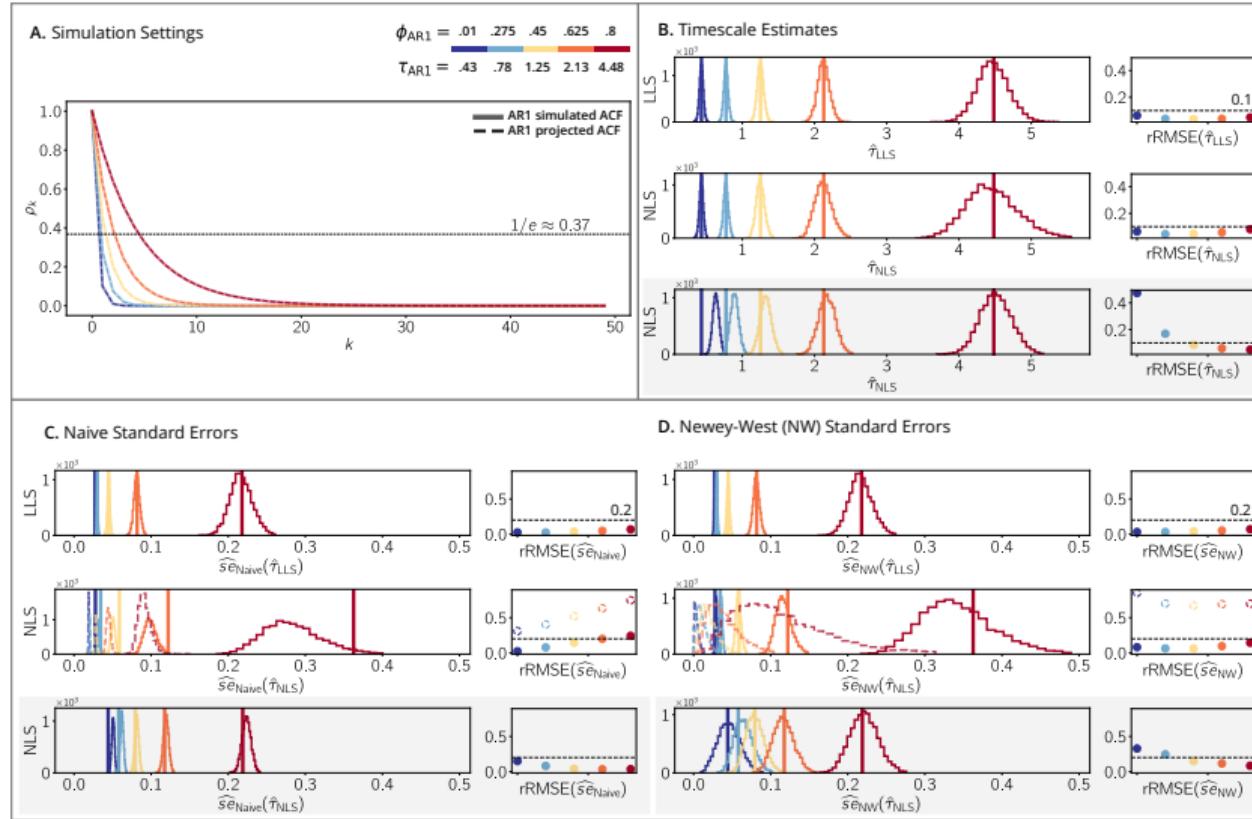
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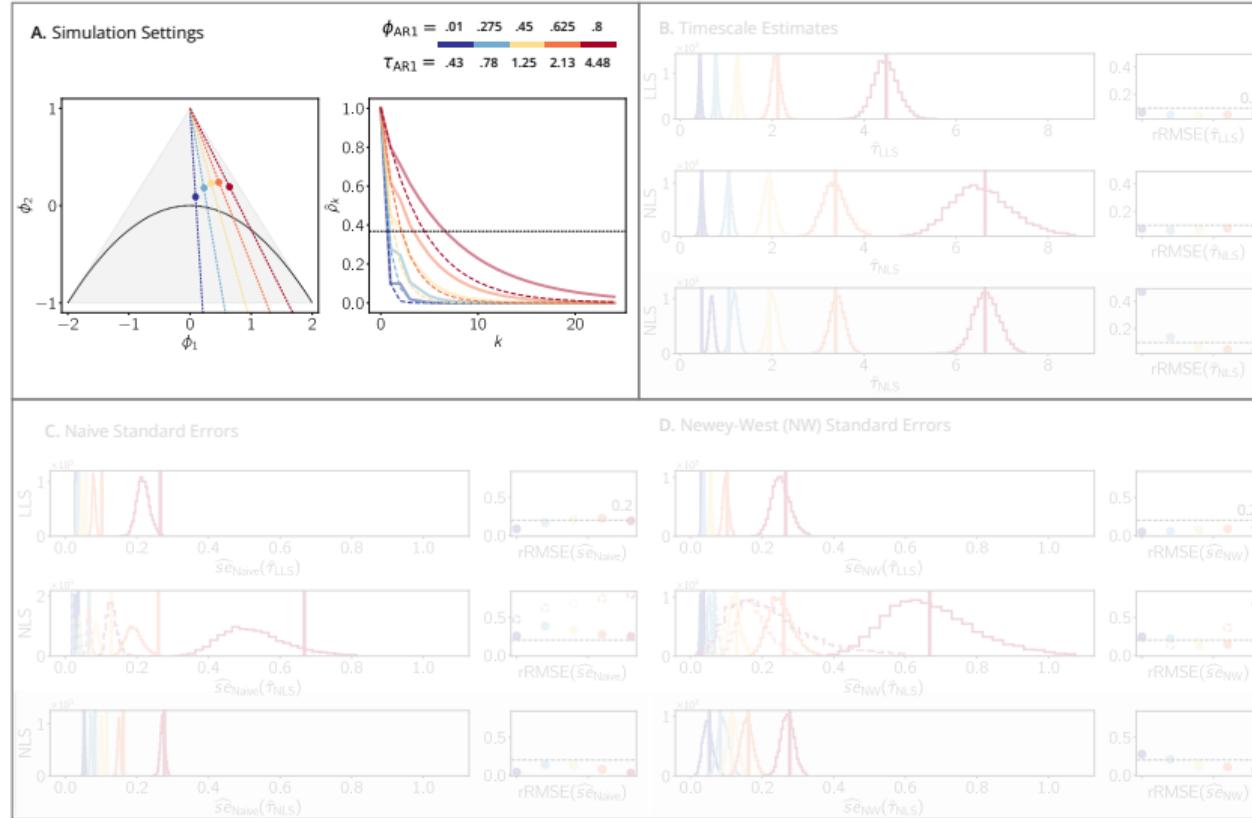
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AR2 Simulations $N = 10,000$ repeats, $T = 4,800$ timepoints

$$x_t = \phi_1 x_{t-1} + \phi_2 x_{t-2} + e_t, \quad e_t \sim \mathcal{N}(0, 1) \quad \rho_k = \phi_1 \rho_{k-1} + \phi_2 \rho_{k-2} + e_k, \quad e_k \sim \mathcal{N}(0, 1)$$



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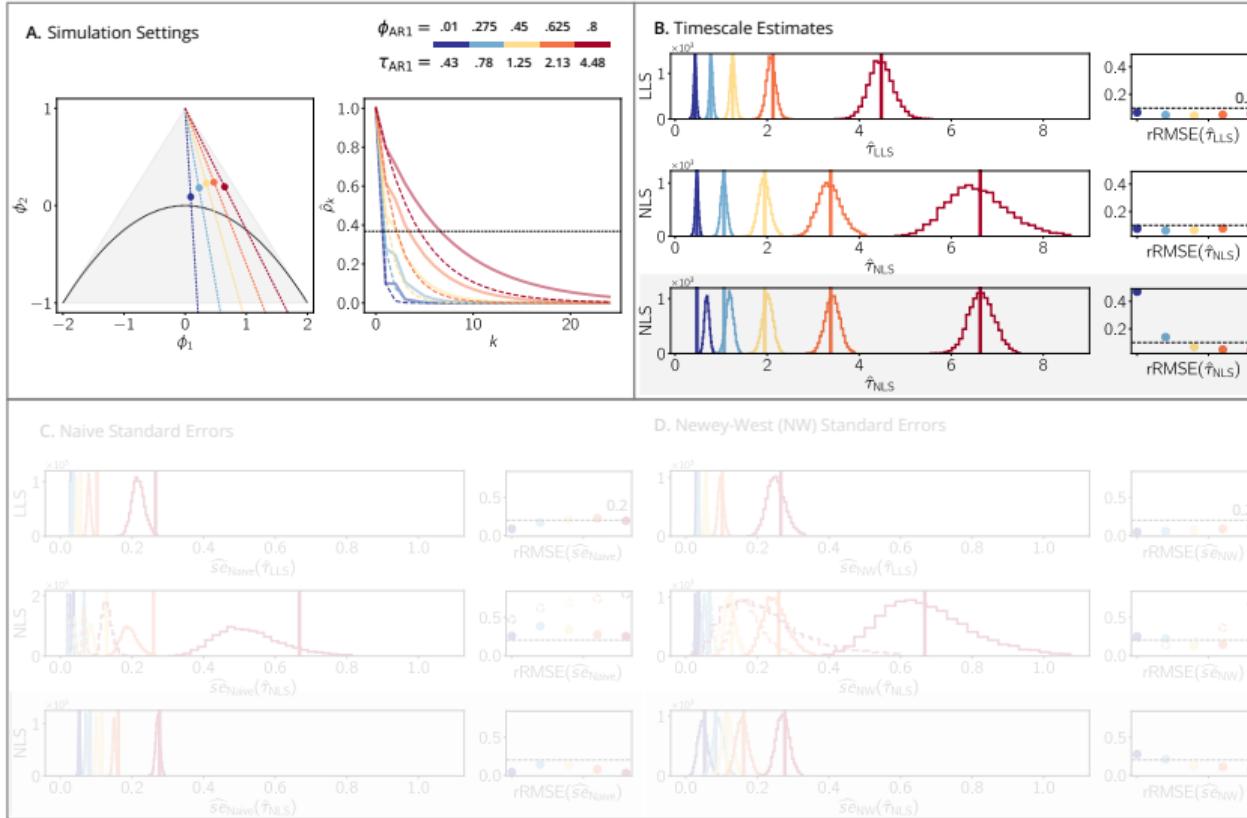
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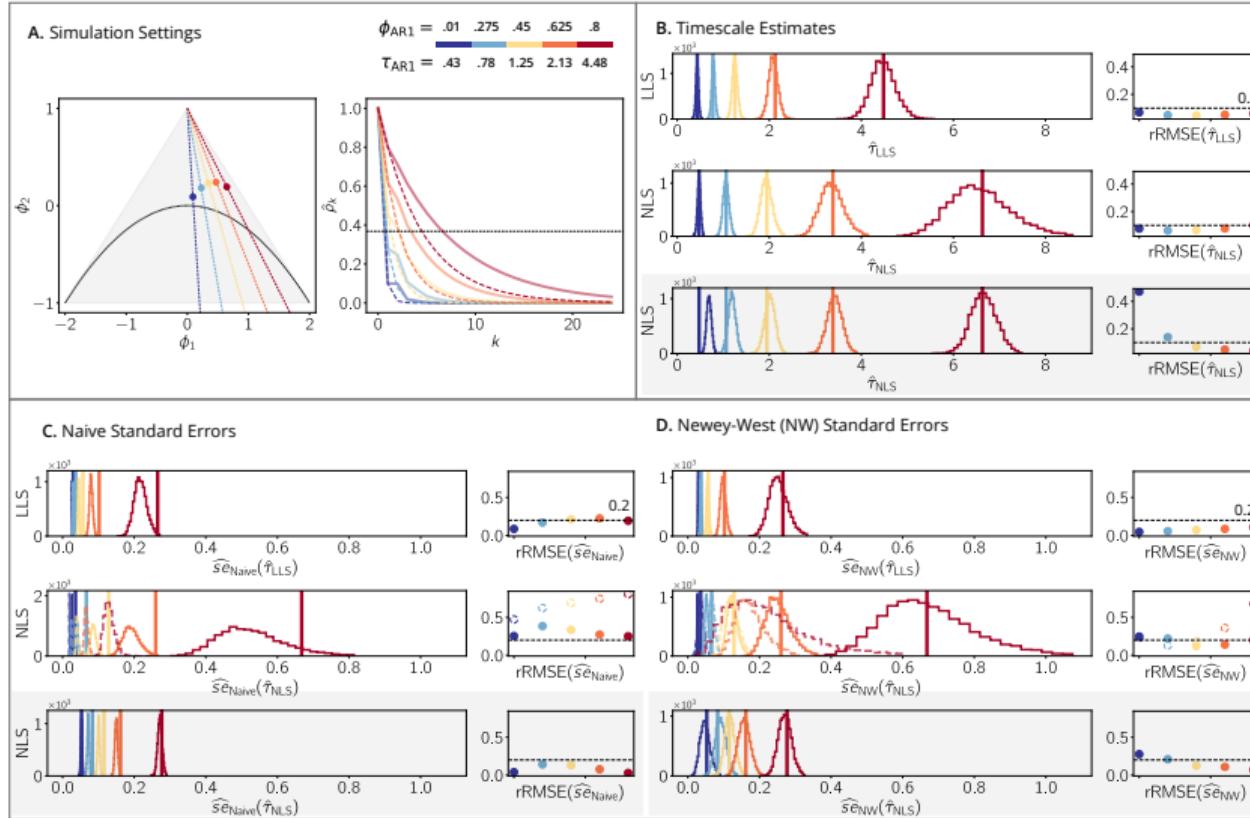
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Realistic rfMRI Simulations

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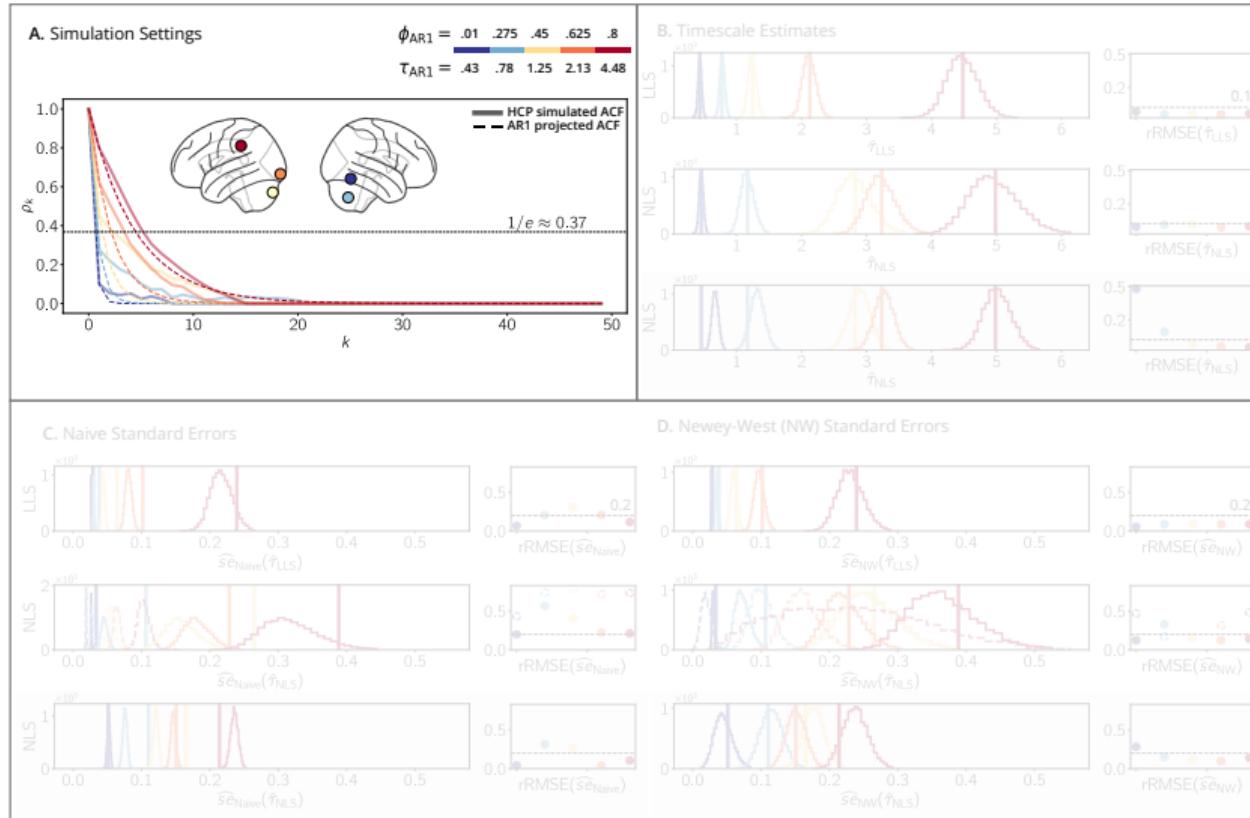
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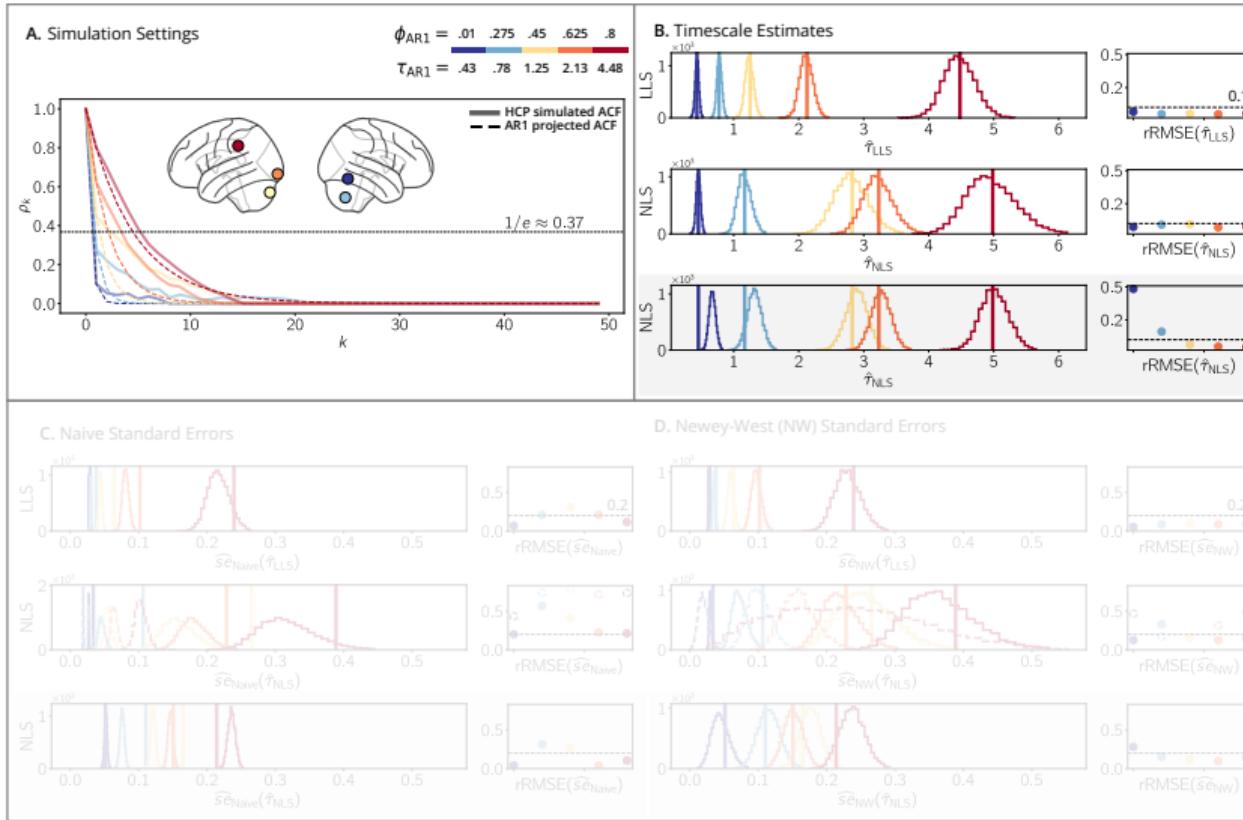
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$$x_t \sim \mathcal{N}(0, \hat{\Sigma}) \quad \rho_k = \hat{\rho}_k + e_k, \quad e_k \sim \mathcal{N}(0, 1)$$

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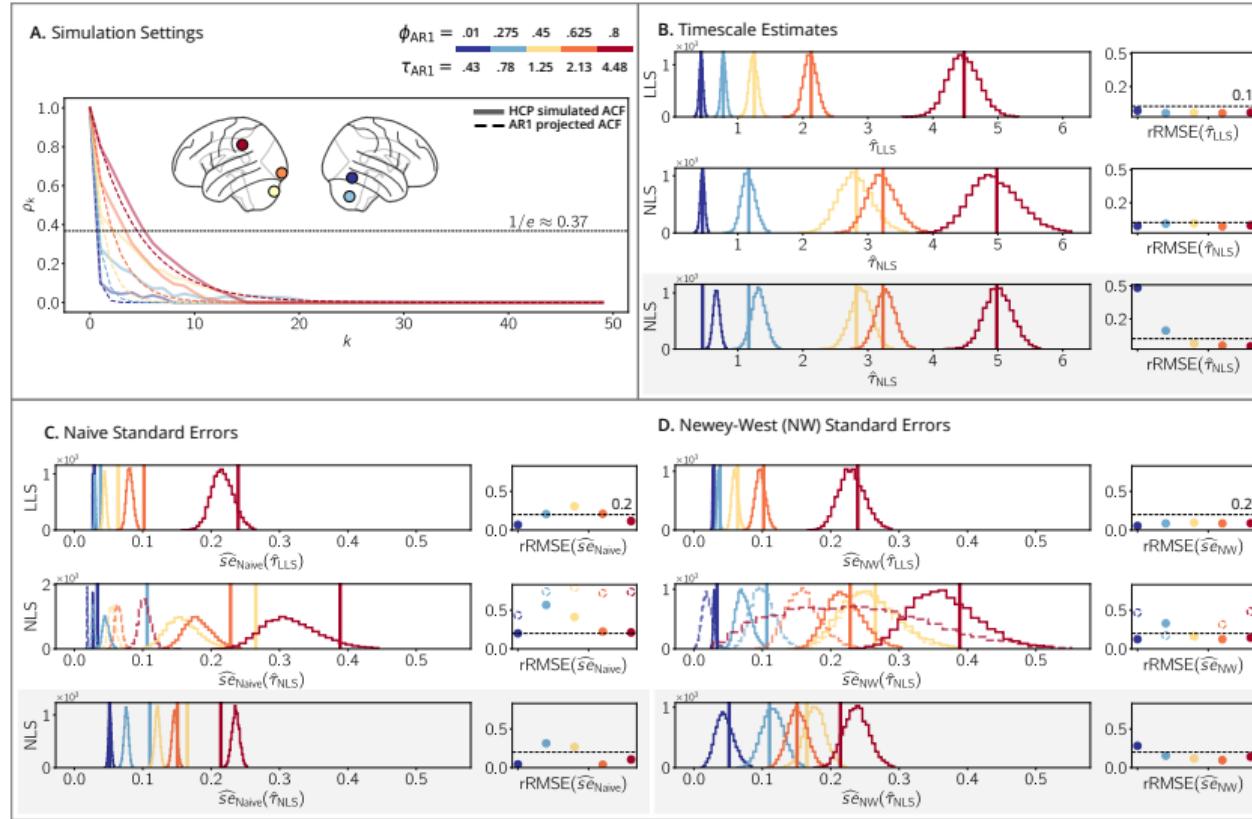
2. Methods

3. Simulations

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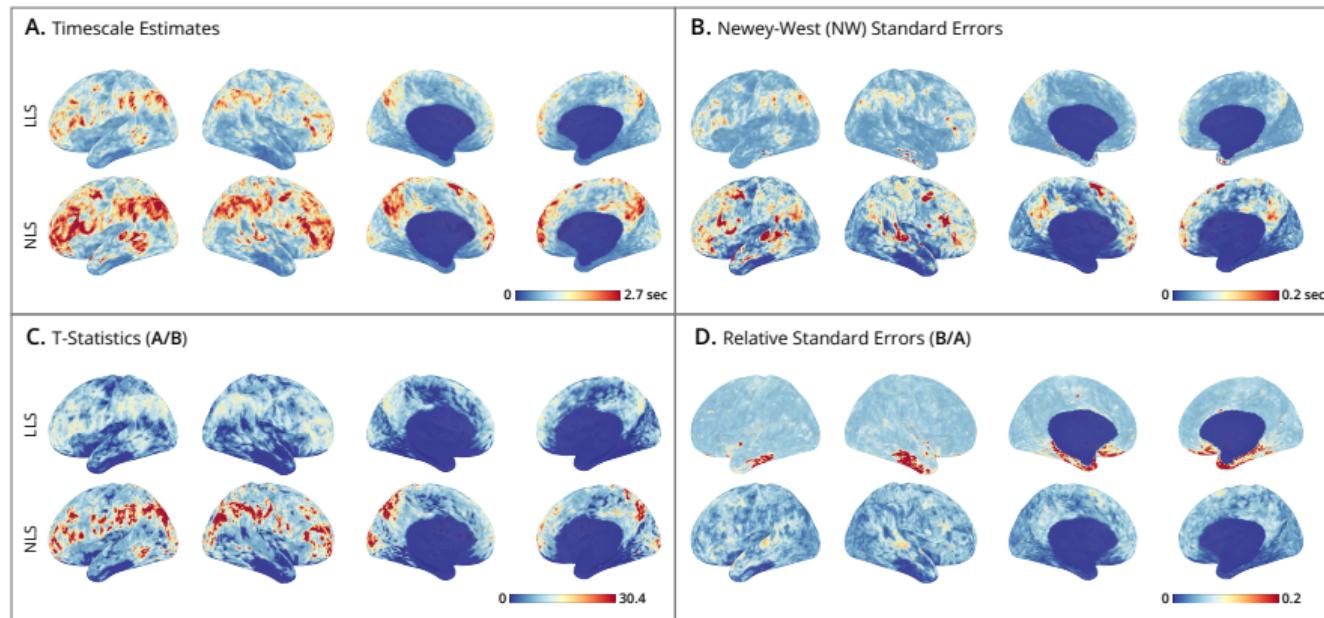
References



Subject-Level Results

$N = 1$ subject, $T = 4,800$ timepoints, $V = 64,984$ vertices

Human Connectome Project (HCP)



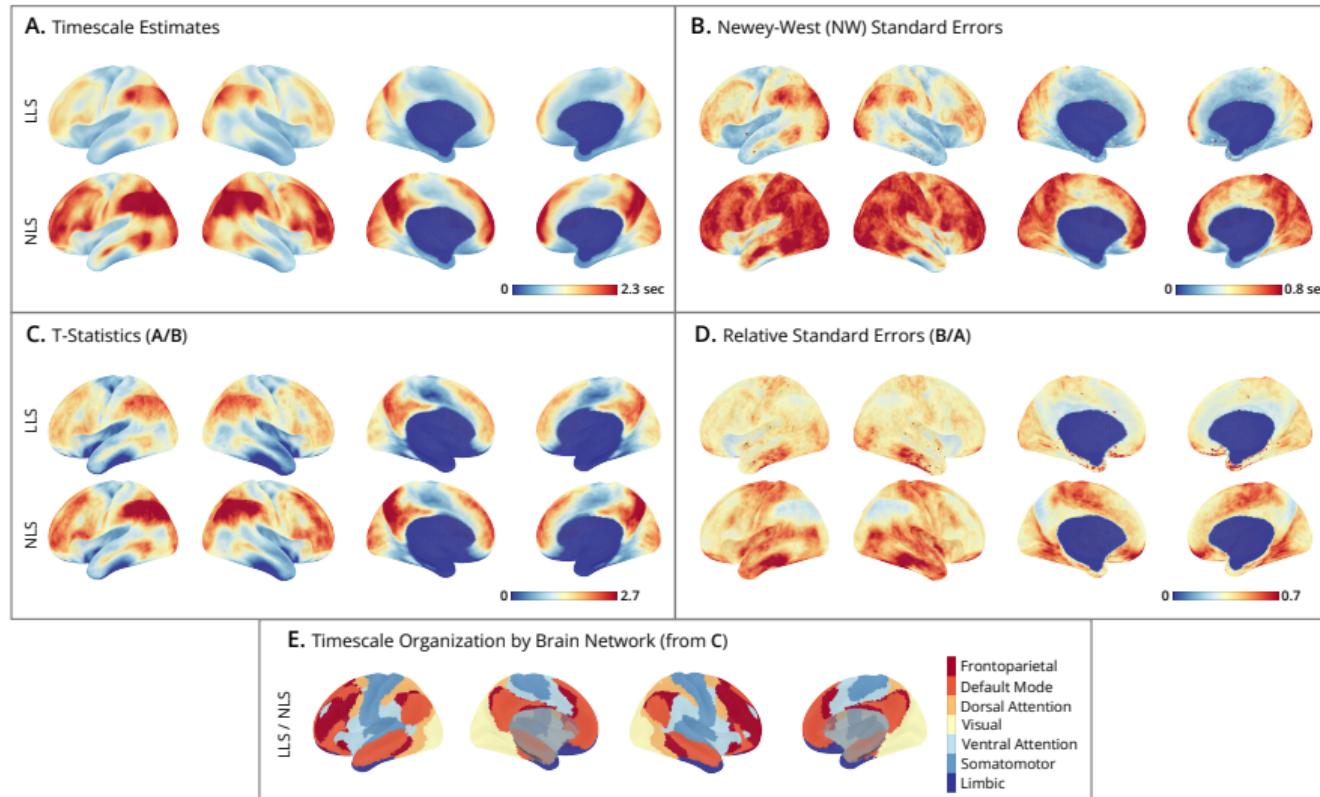
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Group-Level Results

$N = 180$ subjects, $T = 4,800$ timepoints, $V = 64,984$ vertices Human Connectome Project (HCP)

$$\bar{\tau} = \frac{1}{N} \sum_{n=1}^N \hat{\tau}_n,$$

$$\widehat{se}(\bar{\tau}) = \sqrt{\frac{1}{N} \sum_{n=1}^N \widehat{se}(\hat{\tau}_n)^2 + \frac{1}{N} \sum_{n=1}^N (\hat{\tau}_n - \bar{\tau})^2}$$



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1. We formalized and compared time- and autocorrelation-domain methods for fMRI timescale mapping.
2. Both methods are consistent under broad conditions (stationary, mixing), though they estimate distinct timescale values.
3. We introduced robust standard errors to enable valid statistical inference, addressing a key limitation of prior work.
4. Comparatively, the time-domain method is more accurate under model misspecification and is more computationally efficient for high-dimensional fMRI data.
5. Both methods produce timescale maps that align with known functional brain organization.
6. Our work provides a foundation for future research on the role of timescales in brain structure and function.

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References

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Thank you!

paper:



<https://doi.org/10.1101/2025.04.23.650300>

code:



<https://github.com/griegner/fmri-timescales>