DEGENERATE EVOLUTION SYSTEMS MODELING THE CARDIAC ELECTRIC FIELD AT MICRO AND MACROSCOPIC LEVEL

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Dedicated to the memory of Brunello Terreni.

ABSTRACT. We study the reaction-diffusion systems of FitzHugh-Nagumo type related to the behaviour of the electrical conduction of cardiac muscle at micro-and macroscopic level. We introduce a variational formulation for both models and we identify a unifying structure. In this framework, adapting the tools of (degenerate) abstract evolution equations in Hilbert spaces, we derive existence, uniqueness and some regularity results. Finally we also deduce convergence and error estimates of a semidiscrete approximation scheme.

1. Introduction

The aim of this paper is to study the reaction-diffusion systems arising from the mathematical models of the cardiac electric activity at the micro- and macroscopic level.

Recent theoretical and computational advanced studies in electrocardiology investigating the electrical behavior of the anisotropic cardiac tissue are based on the so called "bidomain" model as a representation of the macroscopic tissue properties [41, 16, 23]. This approach conceives the cardiac muscle, despite its discrete structure, as the coupling of two anisotropic continuous superimposed domains. We refer to [24] for an extensive review on the use of the bidomain approach for simulating the electrical behavior of the cardiac tissue. Recently in [37, 30] it was presented a first formal derivation of the bidomain continuous representation of the cardiac tissue from a discrete model consisting of a periodic network of interconnected cells.

A distinctive feature of the mathematical description of both models, i.e. the macroscopic bidomain and the microscopic cellular models, lies in the structure of the coupling between the intra- and extra-cellular media. Both models are reaction-diffusion systems (see e.g. [50, 12]) but of degenerate parabolic type.

The microscopic model of the cardiac tissue. At a microscopic level the cardiac cellular structure of the tissue can be viewed as composed by two volumes: the intra-cellular space (inside the cells) and the extra-cellular space (outside) separated by the active membrane.

More specifically at the microscopic level the cardiac structure is composed of a collection of elongated cardiac cells, connected end–to–end and/or side–to–side by

Key words and phrases. Degenerate evolution equations, reaction-diffusion systems of FitzHugh-Nagumo type, cardiac electric field, bidomain model.

This work was partially supported by grants of M.U.R.S.T. (cofin1999–9901107579, cofin2000-MM01151559) and of the Institute of Numerical Analysis of the C.N.R., Pavia, Italy.

 (μ_1)

junctions, surrounded by the extra-cellular fluid. The end-to-end contacts forms the long fibers structure of the cardiac muscle whereas the presence of lateral junctions establishes a connection between the elongated fibers. Since the interconnection between cells has junction resistance comparable to that of the intra-cellular volume, we can consider the cardiac tissue as a single isotropic intramural connected domain Ω_i separated from the extra-cellular fluid Ω_e by a membrane surface Γ_m .

The geometry and the main physical quantities. Therefore

$$\Omega := \Omega_i \cup \Omega_e \cup \Gamma_m \subset \mathbb{R}^3$$
 is the physical region occupied by the heart, $\Omega_{i,e}$ are the disjoint intra- and extra-cellular domains,

their interface $\overline{\Gamma}_m = \partial \Omega_i \cap \partial \Omega_e$ is the active membrane.

We denote by u_i , u_e

the intra- and extra-cellular electric potentials $u_{i,e}: \overline{\Omega_{i,e}} \to \mathbb{R}$, whose difference is the transmembrane potential $v := u_i - u_e : \Gamma_m \to \mathbb{R}$, and by σ_i , σ_e

$$(\mu_3)$$
 the intra- and extra-cellular conductivities $\sigma_{i,e}: \overline{\Omega_{i,e}} \to \mathbb{R}, \quad \inf_{\Omega_{i,e}} \sigma^{i,e} > 0.$

Basic equations. Due to the current conservation law, the normal current flux through the membrane is continuous: if ν_i, ν_e denote the unit exterior normals to the boundary of Ω_i and Ω_e respectively, satisfying $\nu_i = -\nu_e$ on Γ_m , we have

$$\sigma_i \nabla u_i \cdot \nu_i + \sigma_e \nabla u_e \cdot \nu_e = 0$$
, on Γ_m .

On the other hand, since the only active source elements lie on the membrane Γ_m , each flux equals the membrane current per unit area I_m , which consists of a capacitive and a ionic term (see [27]):

$$(\mu_4) \quad \sigma_i \nabla u_i \cdot \nu_i + I_m = -\sigma_e \nabla u_e \cdot \nu_e + I_m = 0, \quad I_m := \mathsf{C}_m \partial_t v + I_{ion}, \quad \text{on } \Gamma_m,$$

where C_m is the surface capacitance of the membrane; in particular, Γ_m is a discontinuity surface for the potential.

Moreover, denoting by I_i^s, I_e^s the (given) stimulation currents applied to the intra- and extra-cellular space, we have

$$(\mu_5) -\operatorname{div}(\sigma_i \nabla u_i) = I_i^s, \quad \text{in } \Omega_i, \quad -\operatorname{div}(\sigma_e \nabla u_e) = I_e^s, \quad \text{in } \Omega_e.$$

If suitable (lateral and initial) boundary conditions are provided, to complete the system (μ_4 - μ_5) a further constitutive description of the ionic current I_{ion} is needed.

The ionic current: Hodgkin-Huxley model. Dynamics structure of the ionic models have been developed extending the Hodgkin-Huxley formalism [25] to the ionic current source density of the cardiac membrane (see e.g. [20, 34, 18]) and are of the type

(1.1)
$$I_{ion} = I_{ion}(v, w_1, \dots, w_k) = \sum_{n} I_n(v, w_1, \dots, w_k),$$

where w_1, \ldots, w_k are additional gating variables taking their values between 0 and 1 and each I_n is a polynomial function of the form

$$I_n(v, w_1, \dots, w_k) := \mathsf{G}_n \, \Pi_{j=1}^k \, w_j^{p_{j,n}} \, (v - \mathsf{v}_n).$$

Here $p_{k,n}$ are integers (some of which may be zero), G_n is the conductance and the equilibrium potential v_n depends on the intra- and extra-cellular concentration of the ionic species n.

Relation (1.1) should be coupled with the system of first order differential equations linking each gating variable to the transmembrane potential v: it has the form

$$(1.2) \partial_t w_j = r_j(v, w_j) := \alpha_j(v) (1 - w_j) - \beta_j(v) w_j, \quad j = 1, \dots, k,$$

where α_i and β_i are in general positive rational functions of exponentials in v.

The FitzHugh-Nagumo simplification and the recovery variable. Simplified models are often used for simulating the propagation of excitation wavefronts in large myocardial domains. In this work we first focus on a excitable model of the FitzHugh-Nagumo type, which was first introduced as a simplified membrane kinetic of the Hodgkin-Huxley equations in the description of the transmission of nervous electric impulses (see e.g. [14, 36]). It requires only one additional

$$(\mu_6)$$
 recovery variable $w: \Gamma_m \to \mathbb{R}$,

and (1.1), (1.2) reduce to

$$\begin{cases} I_{ion} = I_{ion}(v,w) := F(v) + \Theta w, \\ \partial_t w = r(v,w) := \eta v - \gamma w, \end{cases} \text{ on } \Gamma_m,$$

$$(\mu_7) \qquad \text{where } \Theta, \eta, \gamma \geq 0 \text{ are given constants and}$$

$$F \in C^1(\mathbb{R}) \text{ is a cubic-like function with } \inf_{\mathbb{D}} F' > -\infty.$$

We refer to (μ_1, \ldots, μ_7) as the *microscopic model*, together with Neumann boundary conditions imposed on u_i, u_e on the remaining part of the boundaries $\Gamma_{i,e} := \partial \Omega_{i,e} \setminus \Gamma_m$ respectively

$$(\mu_8) \qquad \qquad \sigma_i \nabla u_i \cdot \nu_i = G_i \quad \text{on } \Gamma_i, \quad \sigma_e \nabla u_e \cdot \nu_e = G_e \quad \text{on } \Gamma_e,$$

and with the (degenerate) initial Cauchy condition

$$(\mu_9)$$
 $v(x,0) = v^0(x), \quad w(x,0) = w^0(x), \quad \text{on } \Gamma_m.$

Thus our problem consists of two adjoining open domains with their boundaries partly intersecting, of a Poisson equation in each of them, and, on the common boundary, of two conditions connecting the fluxes and the potentials. In contrast to classical problems for the Poisson equation with a jump discontinuity across some surface, here the boundary conditions for the potentials is a dynamic boundary condition involving the assistant variable w.

The macroscopic "bidomain" model. At a macroscopic level, in spite of the discrete cellular structure, the cardiac tissue can be represented by a continuous model, called bidomain model (see e.g. [24, 17, 41] and also [30]), which attempts to describe the averaged electric potentials and current flows inside (intra-) and outside (extra-cellular space) the cardiac cells. The equations should result from an homogenization process as shown formally in [37] working on a scaled version of the cellular model on a periodic cardiac structure. For completeness we will present another formal derivation of the average model by using the standard two-scaled method in the Appendix A and we defer to a forthcoming paper the rigorous mathematical justification of the model by the tools of Γ -convergence theory.

In this homogenized representation the heart domain coincides with the intra-(i) and extra-cellular (e) ones, which are two interpenetrating and superimposed continua connected at each point by the cardiac cellular membrane, i.e.

$$(M_1)$$
 $\Omega \equiv \Omega_i \equiv \Omega_e \subset \mathbb{R}^3$ is the physical region occupied by the heart

$$(M_2) \quad \begin{array}{c} u_i, u_e: \Omega \to \mathbb{R} \quad \text{are the intra- (i) and extra-cellular (e) electric potentials} \\ v:= u_i - u_e: \Omega \to \mathbb{R} \quad \text{is the transmembrane potential.} \end{array}$$

The anisotropy of the (i)–(e) media depends on the fiber structure of the myocardium. At the macroscopic level the fibers are regular curves, whose unit tangent vector at the point x is denoted by $\vec{a} = \vec{a}(x)$. Denoting by $\sigma_{i,e}^l(x)$, $\sigma_{i,e}^t(x)$ the conductivity coefficients along and across the fiber direction at a point x and always assuming axial simmetry for $\sigma_{i,e}^t$, the conductivity tensors $M_{i,e}$ in the media (i), (e), can be expressed by

$$M_{i,e}(x) = \sigma_{i,e}^t I + (\sigma_{i,e}^l - \sigma_{i,e}^t) \vec{a} \otimes \vec{a},$$

and they are

$$(M_3)$$
 symmetric, positive definite, continuous tensors $M_{i,e}: \overline{\Omega} \to \mathbb{M}^{3\times 3}$.

To the potentials u_i , u_e are associated the current densities $\vec{I}_{i,e} := -M_{i,e} \nabla u_{i,e}$; since induction effects are negligible, the current field can be considered quasi–static and they are related to the membrane current per unit volume i_m and to the injected stimulating currents $i_{i,e}^s$ by the conservation laws

$$(M_4) -\operatorname{div}(M_i \nabla u_i) = -i_m + i_i^s, -\operatorname{div}(M_e \nabla u_e) = i_m + i_e^s, \operatorname{in} \Omega.$$

On the other hand the membrane current per unit volume i_m is the sum of a capacitance and a ionic term

$$(M_5) i_m = \mathsf{c}_m \partial_t v + i_{ion} \quad \text{in } \Omega.$$

Again the FitzHugh-Nagumo model supply the form of the ionic current i_{ion} by means of a

$$(M_6)$$
 recovery variable $w: \Omega \to \mathbb{R}$,

and of

$$\begin{cases} i_{ion} = i_{ion}(v, w) = f(v) + \theta w, \\ \partial_t w = r(v, w) = \eta v - \gamma w \end{cases}$$
 on Ω
where $\theta, \eta, \gamma \geq 0$ are given constants and $f \in C^1(\mathbb{R})$ is a cubic-like function with $\inf_{\mathbb{R}} f' > -\infty$.

In fact, c_m and the forms of f, i_{ion} are related to the corresponding microscopic quantities by the relation

$$c_m = \beta C_m$$
, $f(v) = \beta F(v)$, $\theta = \beta \Theta$, $i_{ion}(v, w) = \beta I_{ion}(v, w)$,

where β is the ratio of membrane area per unit of tissue volume.

We complete the Reaction-Diffusion system (M_1, \ldots, M_7) by imposing Neumann boundary conditions on u_i, u_e on $\partial\Omega$ respectively

$$(M_8) M_i \nabla u_i \cdot \nu = g_i, \quad M_e \nabla u_e \cdot \nu = g_e,$$

and by assigning the (degenerate) initial Cauchy condition

$$(M_9)$$
 $v(x,0) = v^0(x), \quad w(x,0) = w^0(x), \quad \text{on } \Omega.$

When $M_i = \lambda M_e$, with λ constant, the macroscopic system $(M_1 - M_9)$ in the variables (u_i, u_e, w) is equivalent to a parabolic reaction-diffusion equation in $v = u_i - u_e$ coupled with the dynamics of the recovery variable w. This case is called in literature equal anisotropic ratio and this assumption is often used in modeling cardiac tissue. Experimental evidence indicates that this simplifying hypothesis is definitely not applicable to cardiac muscle. The degenerate structure of the mathematical model is primarily the result of differences in the intra- and extracellular anisotropy of the cardiac tissue. Morover unequal anisotropic ratio makes possible more complex phenomena [52, 51] and can play an important role for the re-entrant excitation [53, 42].

Plan of the paper. In the two following sections we will propose a variational formulation of both the microscopic problem (μ_1, \ldots, μ_9) and the macroscopic one (M_1, \ldots, M_9) . We will show that they have a common structure which fits into the abstract framework of (degenerate) evolution variational inequalities in Hilbert spaces; therefore, we will focus on the basic structural features of both the models, and we will state our main results about existence, uniqueness, and regularity of their solutions.

In \S 4, we will present the abstract version of the evolution problems shared by the micro- and macroscopic models, we will discuss the links with the results available in the literature, and we will introduce an approach which allows us to eliminate the time degeneration; in this way it is possible to apply finer results which give a better insight into the properties of the solutions: in particular, general stability and approximation results could also be applied for the time discretization of both the systems.

The effort to enucleate a similar variational structure in the problems not only allows to reduce the length and the difficulty of the proofs, but also suggests a possible way to deduce the macroscopic setting from the microscopic one. However, the classical theory for convex evolution problems (see e.g. [1]) cannot be directly applied, due to the degeneracy and to the different kind of domains where the microscopic (Γ_m) and the macroscopic (Ω) quantities live. Nevertheless, we will show in a forthcoming work a possible way to overcome this difficulty; in the Appendix of the present paper, by developing formal asymptotic expansions using the two–scales method and neglecting the presence of stimulation currents, we will show how to convert the microscopic model of the cellular media into the averaged continuum "bidomain" representation of the cardiac tissue.

2. Variational formulation of the microscopic problem

In this section we will deal with the system (μ_1, \ldots, μ_9) presented in the Introduction and we will rewrite it in a suitable variational form.

Fixing technical assumptions and notation. Besides (μ_1, \ldots, μ_9) , we are also assuming that

$$(\mu_1')$$
 Ω_i, Ω_e are Lipschitz domains and at least one of them is connected, Γ_m is a (non empty) Lipschitz hypersurface.

From the mathematical point of view, it is not always necessary to restrict the dimension of the ambient space, which we will denote by d. The regularity assumptions on F could be relaxed: so $F: \mathbb{R} \to \mathbb{R}$ could be a continuous function such that

$$(\mu_7')$$
 $F(0) = 0;$ $\exists \lambda_F \ge 0:$ $\frac{F(x) - F(y)}{x - y} \ge -\lambda_F, \quad \forall x, y \in \mathbb{R}, \text{ with } x \ne y.$

More general existence results in dimension d=3 (see Proposition 2.4) will also require that F has a cubic growth at infinity, i.e.

$$(\mu_7'') \qquad \qquad 0 < \liminf_{|s| \to +\infty} \frac{F(s)}{s^3} \leq \limsup_{|s| \to +\infty} \frac{F(s)}{s^3} < +\infty.$$

]0, T[is the evolution time interval, and we define the associated space-time domains following the usual notation of [32]

(2.1)
$$Q_{i,e} := \Omega_{i,e} \times]0, T[, \qquad \Sigma_{i,e,m} := \Gamma_{i,e,m} \times]0, T[.$$

The formal statement of $(\mu_1 - \mu_9)$ is then:

Problem (μ) . Given

(2.2)
$$I_{i,e}^s: Q_{i,e} \to \mathbb{R}, \quad G_{i,e}: \Sigma_{i,e} \to \mathbb{R}, \quad \text{and} \quad v^0, w^0: \Gamma_m \to \mathbb{R},$$

we seek

$$u_{i,e}: Q_{i,e} \to \mathbb{R}, \quad w: \Sigma_m \to \mathbb{R}, \quad v:=u_i-u_e: \Sigma_m \to \mathbb{R},$$

satisfying the equations on $Q_{i,e}$ and $\Sigma_{i,e}$

(2.3)
$$\begin{cases} -\operatorname{div}\left(\sigma_{i,e}\nabla u_{i,e}\right) = I_{i,e}^{s}, & \text{in } Q_{i,e}, \\ \sigma_{i,e}\nabla u_{i,e} \cdot \nu_{i,e} = G_{i,e} & \text{on } \Sigma_{i,e}, \end{cases}$$

the evolution system on the surface Σ_m

(2.4)
$$\begin{cases} \mathsf{C}_m \partial_t v + F(v) + \Theta w = -\sigma_i \nabla u_i \cdot \nu_i = \sigma_e \nabla u_e \cdot \nu_e & \text{on } \Sigma_m, \\ \partial_t w + \gamma w - \eta v = 0 & \text{on } \Sigma_m, \\ v(x,0) = v^0(x), \quad w(x,0) = w^0(x) & \text{on } \Gamma_m. \end{cases}$$

Variational formulation. In order to write the variational formulation of Problem (μ) , let us assume at first that for a.e. $t \in]0,T[$

(2.5)
$$I_{i,e}^{s}(\cdot,t) \in L^{2}(\Omega_{i,e}), \quad G_{i,e}(\cdot,t) \in H^{-1/2}(\Gamma_{i,e}),$$

$$(2.6) u_{i,e}(\cdot,t), \ \partial_t u_{i,e}(\cdot,t) \in H^1(\Omega_{i,e}), \quad w(\cdot,t), \ \partial_t w(\cdot,t) \in L^2(\Gamma_m),$$

so that the trace operator $u_{i,e} \mapsto u_{i,e}|_{\Gamma_m}$ is well defined and maps continuously $H^1(\Omega_{i,e})$ onto $H^{1/2}(\Gamma_m)$ (cf. [32]). By using the simplified notation $v := u_i - u_e$ instead of $u_i|_{\Gamma_m} - u_e|_{\Gamma_m}$, we also suppose that

$$(2.7) F(v(\cdot,t)) \in L^1(\Gamma_m) \cap H^{-1/2}(\Gamma_m).$$

We choose the test functions

(2.8)
$$\hat{u}_{i,e} \in H^1(\Omega_{i,e}), \quad \hat{w} \in L^2(\Gamma_m), \quad \text{with} \quad \hat{v} := \hat{u}_i - \hat{u}_e \in H^{1/2}(\Gamma_m),$$

and we multiply the two equations of the first row of (2.4) by the trace of \hat{u}_i and $-\hat{u}_e$ respectively, and the next equation by $\rho\hat{w}$, ρ being the ratio Θ/η . Summing up

them after an integration on Γ_m (we denote by \mathscr{H}^{d-1} the usual (d-1)-dimensional Hausdorff measure) we get

(2.9)
$$\int_{\Gamma_{m}} \left(\mathsf{C}_{m} \, \partial_{t} v \, \hat{v} + \rho \, \partial_{t} w \, \hat{w} \right) d\mathcal{H}^{d-1} \\
+ {}_{H^{-1/2}(\Gamma_{m})} \langle F(v), \hat{v} \rangle_{H^{1/2}(\Gamma_{m})} + \rho \gamma \int_{\Gamma_{m}} w \, \hat{w} \, d\mathcal{H}^{d-1} \\
+ \sum_{i,e} \int_{\Omega_{i,e}} \sigma_{i,e} \nabla u_{i,e} \cdot \nabla \hat{u}_{i,e} \, dx + \Theta \int_{\Gamma_{m}} \left(w \hat{v} - v \hat{w} \right) d\mathcal{H}^{d-1} = \\
= \sum_{i,e} \int_{\Omega_{i,e}} I_{i,e}^{s} \, \hat{u}_{i,e} \, dx + \sum_{i,e} {}_{H^{-1/2}(\Gamma_{i,e})} \langle G_{i,e}, \hat{u}_{i,e} \rangle_{H^{1/2}(\Gamma_{i,e})},$$

where we used (2.3) and the Green formulae

$$\begin{split} &_{H^{-1/2}(\Gamma_m)} \langle \sigma_{i,e} \nabla u_{i,e} \cdot \nu_{i,e} \, \hat{u}_{i,e} \rangle_{H^{1/2}(\Gamma_m)} = \\ &= \int_{\Omega_{i,e}} \left(\sigma_{i,e} \nabla u_{i,e} \cdot \nabla \hat{u}_{i,e} + \operatorname{div}(\sigma_{i,e} \nabla u_{i,e}) \, \hat{u}_{i,e} \right) dx \\ &- {}_{H^{-1/2}(\Gamma_{i,e})} \langle \sigma_{i,e} \nabla u_{i,e} \cdot \nu_{i,e}, \hat{u}_{i,e} \rangle_{H^{1/2}(\Gamma_{i,e})} = \\ &= \int_{\Omega_{i,e}} \sigma_{i,e} \nabla u_{i,e} \cdot \nabla \hat{u}_{i,e} \, dx - \int_{\Omega_{i,e}} I^s_{i,e} \, \hat{u}_{i,e} \, dx - {}_{H^{-1/2}(\Gamma_{i,e})} \langle G_{i,e}, \hat{u}_{i,e} \rangle_{H^{1/2}(\Gamma_{i,e})}. \end{split}$$

which are justified by the usual arguments of [32]. Let us point out the particular structure of (2.9), which is common to more general situations.

"Vector" functional spaces. Denoting by boldface letters u, \hat{u}, \ldots the triple of functions $(u_i, u_e, w), (\hat{u}_i, \hat{u}_e, \hat{w}), \ldots$, we introduce the product space

(2.10)
$$\mathbf{X} := H^1(\Omega_i) \times H^1(\Omega_e) \times L^2(\Gamma_m),$$

and the bilinear forms

(2.11)
$$b(\boldsymbol{u}, \hat{\boldsymbol{u}}) := \int_{\Gamma_m} \left[\mathsf{C}_m(u_i - u_e)(\hat{u}_i - \hat{u}_e) + \rho \, w \hat{w} \right] d\mathcal{H}^{d-1},$$

(2.12)
$$a(\boldsymbol{u}, \hat{\boldsymbol{u}}) := \sum_{i,e} \int_{\Omega_{i,e}} \sigma_{i,e} \nabla u_{i,e} \cdot \nabla \hat{u}_{i,e} \, dx + \rho \gamma \int_{\Gamma_m} w \, \hat{w} \, d\mathcal{H}^{d-1} + \Theta \int_{\Gamma_m} \left[w(\hat{u}_i - \hat{u}_e) - (u_i - u_e) \hat{w} \right] d\mathcal{H}^{d-1},$$

which are defined for every $u, \hat{u} \in X$.

If (2.5) holds and v^0, w^0 belong to $L^2(\Gamma_m)$, then we can also associate to the right hand member of (2.9) and to the initial data the time-depending family of linear functionals $\boldsymbol{L}(t) \in \boldsymbol{X}'$ and the linear functional $\boldsymbol{\ell}^0 \in \boldsymbol{X}'$ respectively, which act on a generic elements $\hat{\boldsymbol{u}} \in X$ in the following way

(2.13)
$$\begin{cases} \langle \boldsymbol{L}(t), \hat{\boldsymbol{u}} \rangle := \sum_{i,e} \int_{\Omega_{i,e}} I_{i,e}^{s} \, \hat{u}_{i,e} \, dx + \sum_{i,e} {}_{H^{-1/2}(\Gamma_{i,e})} \langle G_{i,e}, \hat{u}_{i,e} \rangle_{H^{1/2}(\Gamma_{i,e})}, \\ \langle \boldsymbol{\ell}^{0}, \hat{\boldsymbol{u}} \rangle := \int_{\Gamma_{m}} \left(\mathsf{C}_{m} \, v^{0} \, (\hat{u}_{i} - \hat{u}_{e}) + \rho \, w^{0} \, \hat{w} \right) dx. \end{cases}$$

The remaining (non-linear term) $\mathfrak{F}:D(\mathfrak{F})\subset X\to X'$ is defined by

(2.14)
$$\langle \mathfrak{F}\boldsymbol{u}, \hat{\boldsymbol{u}} \rangle := {}_{H^{-1/2}(\Gamma_m)} \langle F(u_i - u_e), \hat{u}_i - \hat{u}_e \rangle_{H^{1/2}(\Gamma_m)},$$

for every $\boldsymbol{u} \in D(\mathfrak{F}), \, \hat{\boldsymbol{u}} \in \boldsymbol{X}$, with

(2.15)
$$D(\mathfrak{F}) := \{ \boldsymbol{u} \in \boldsymbol{X} : F(u_i - u_e) \in L^1(\Gamma_m) \cap H^{-1/2}(\Gamma_m) \}.$$

We collect all these calculations in the following standard lemma.

Lemma 2.1. Let $X, b(\cdot, \cdot), a(\cdot, \cdot), L, \mathfrak{F}$ be defined by $(2.10), \ldots, (2.15)$ respectively, and let us suppose that

$$(2.16) I_{i,e}^s \in L^2(Q) = L^2(0,T;L^2(\Omega_{i,e})), G_{i,e} \in L^2(0,T;H^{-1/2}(\Gamma_{i,e})).$$

Then u_i, u_e, w satisfy (2.6), (2.7) and solve Problem (μ) if and only if the function

(2.17)
$$\boldsymbol{u}(t) := (u_i(\cdot, t), u_e(\cdot, t), w(\cdot, t)), \quad belongs \ to \ W^{1,1}(0, T; \boldsymbol{X}),$$

and solves the abstract evolution equation

$$(2.18) \quad \begin{cases} b(\boldsymbol{u}', \hat{\boldsymbol{u}}) + a(\boldsymbol{u}, \hat{\boldsymbol{u}}) + \langle \mathfrak{F}\boldsymbol{u}, \hat{\boldsymbol{u}} \rangle = \langle \boldsymbol{L}(t), \hat{\boldsymbol{u}} \rangle, & \forall \, \hat{\boldsymbol{u}} \in \boldsymbol{X}, \quad a.e. \ in \]0, T[\,, \\ b(\boldsymbol{u}(0), \hat{\boldsymbol{u}}) = \langle \boldsymbol{\ell}^0, \hat{\boldsymbol{u}} \rangle, & \forall \, \hat{\boldsymbol{u}} \in X. \end{cases}$$

Remark 2.2. Different types of (variational) boundary conditions could also be considered in Problem (μ) , by simply modifying X and L. E.g., if we want to impose the homogeneous Dirichlet condition

$$(2.19) u_e = 0, on \Gamma_e,$$

instead of the corresponding Neumann one, we can replace $H^1(\Omega_e)$ by its closed subspace

$$H^1_{\Gamma_e}(\Omega_e) := \left\{ u \in H^1(\Omega_e) : u_{|\Gamma_e} = 0, \text{ in the sense of traces} \right\}$$

in the definition (2.10) of X.

Remark 2.3. We point out that (2.11), (2.12), and (2.14) are not modified by adding to u, \hat{u} a constant vector \mathbf{c} of the type

(2.20)
$$\mathbf{c} := (c, c, 0), \quad \forall c \in \mathbb{R}.$$

Analogously, the solutions u_i, u_e, w of Problem (μ) can be determined at every time t up to this kind of additive constants. Therefore, it is natural to replace X by its quotient

(2.21)
$$\mathbf{V} := \left(H^1(\Omega_i) \times H^1(\Omega_e) \times L^2(\Gamma_m)\right) / \left\{ (c, c, 0) : c \in \mathbb{R} \right\}$$

and to look for u with values in V; to simplify our notation, we still denote by (u_i, u_e, w) the corresponding equivalence class and take for granted to check the independence of the particular representative.

As usual, we can identify the dual V' of V with the closed subspace of X' whose elements L verify

(2.22)
$$\langle \mathbf{L}, \mathbf{c} \rangle = 0$$
, for every \mathbf{c} given by (2.20).

It follows that we have to impose the compatibility condition

(2.23)
$$\sum_{i,e} \int_{\Omega_{i,e}} I_{i,e}^{s} dx + \sum_{i,e} {}_{H^{-1/2}(\Gamma_{i,e})} \langle G_{i,e}, 1 \rangle_{H^{1/2}(\Gamma_{i,e})} = 0, \text{ a.e. in }]0, T[,$$

in order to have $L(t) \in V'$ in the case of (2.13). Finally, we note that \mathfrak{F} maps $D(\mathfrak{F})$ into V' without any further restriction.

Where to choose initial data. In order to avoid extra regularity assumptions on the solution and to understand how to choose the correct functional framework for the initial data, we introduce the linear continuous operators $A, B: V \to V'$ associated to a, b respectively, i.e.

(2.24)
$$\langle A\boldsymbol{u}, \hat{\boldsymbol{u}} \rangle := a(\boldsymbol{u}, \hat{\boldsymbol{u}}), \quad \langle B\boldsymbol{u}, \hat{\boldsymbol{u}} \rangle := b(\boldsymbol{u}, \hat{\boldsymbol{u}}), \quad \forall \, \boldsymbol{u}, \hat{\boldsymbol{u}} \in \boldsymbol{V}.$$

Then we can rewrite (2.18) in the operator form

$$(2.25) \qquad (B\mathbf{u}(t))' + A\mathbf{u}(t) + \mathfrak{F}\mathbf{u}(t) = \mathbf{L}(t) \quad \text{in } \mathbf{V}', \quad \text{for a.e. } t \in]0, T[,$$

which suggests that (2.17) can be weakened by asking

(2.26)
$$u \in L^2(0,T; \mathbf{V}), \quad Bu \in W^{1,1}_{loc}(0,T; \mathbf{V}') \cap C^0([0,T]; \mathbf{V}'),$$

so that we can give a meaning in V' to the initial value of Bu. Let us introduce the distribution spaces $\tilde{V}_b \subset \tilde{V}'_b$ on Γ_m

$$\tilde{V}_b := H^{1/2}(\Gamma_m) \times L^2(\Gamma_m), \quad \tilde{V}'_b := H^{-1/2}(\Gamma_m) \times L^2(\Gamma_m),$$

and let us observe that the operator $B: V \to V'$ admits the decomposition

$$(2.27) B = \tilde{B}^* J_b \tilde{B}, \quad b(\boldsymbol{u}, \hat{\boldsymbol{u}}) = {}_{\boldsymbol{V}'} \langle B \boldsymbol{u}, \hat{\boldsymbol{u}} \rangle_{\boldsymbol{V}} = {}_{\tilde{V}'_b} \langle J_b \tilde{B} \boldsymbol{u}, \tilde{B} \hat{\boldsymbol{u}} \rangle_{\tilde{V}_b}$$

where $J_b: \tilde{V}_b \to \tilde{V}_b'$ is the inclusion map, \tilde{B} is the linear surjection

(2.28)
$$\tilde{B}: \mathbf{V} \to \tilde{V}_b, \quad \tilde{B}\mathbf{u} := \left(\sqrt{\mathsf{C}_m} (u_i - u_e), \sqrt{\rho} w\right)$$

and $\tilde{B}^*: \tilde{V}'_h \to V'$ is the transposed linear isomorphism

(2.29)
$$\langle \tilde{B}^*(v,w), \hat{\boldsymbol{u}} \rangle :=_{H^{-1/2}(\Gamma_m)} \langle \sqrt{\mathsf{C}_m} \, v, \hat{v} \rangle_{H^{1/2}(\Gamma_m)} + \int_{\Gamma_m} \sqrt{\rho} \, w \, \hat{w} \, d\mathcal{H}^{d-1}, \quad \forall \, \hat{\boldsymbol{u}} \in \boldsymbol{V}.$$

We observe that (2.26) entails

$$(u_i - u_e, w) \in C^0([0, T]; \tilde{V}_b')$$

so that we have to require $(v^0, w^0) \in \tilde{V}'_b$ at least.

On the other hand, if \mathfrak{F} would be linear, we could read from the equation that $\tilde{B}\boldsymbol{u}$ belongs also to $H^1(0,T;\tilde{V}_b')\cap L^2(0,T;\tilde{V}_b)$, and we could deduce by standard interpolation results (cf. [32]), the mapping

(2.30)
$$t \mapsto (v(t), w(t))$$
 is uniformly continuous in $\tilde{H}_b := L^2(\Gamma_m) \times L^2(\Gamma_m)$.

Even if $B\mathbf{u}$ does not belong to $H^1(0,T;\mathbf{V}')$ in the general nonlinear case, however (2.30) still holds, and we shall require

$$(2.31) (v^0, w^0) \in L^2(\Gamma_m) \times L^2(\Gamma_m), \quad \ell^0 \in H_b := \tilde{B}^*(\tilde{H}_b)$$

writing the initial condition as

$$(2.32) (B\mathbf{u})(0) = \ell^0 \in H_b.$$

Main result. We have now all the elements to reformulate Problem (μ) in an abstract variational form and to state our main result about it.

Problem $(A\mu)$. Let us assume that (2.16), (2.23), and (2.31) hold. Then, if V, b, a, L, \mathfrak{F} are defined by (2.21), (2.11),...,(2.14) respectively, we look for

(2.33)
$$u \in L^2(0,T; \mathbf{V}), \text{ with } Bu \in W^{1,1}_{loc}(0,T; \mathbf{V}') \cap C^0([0,T]; \mathbf{V}')$$

satisfying the abstract Cauchy problem (2.25), (2.32).

Theorem 1. In the framework of (μ_1, \ldots, μ_9) , (μ'_1, μ'_7) , let us assume that

(2.34)
$$I_{i,e}^s \in W^{1,1}(0,T;L^2(\Omega_{i,e})), \quad G_{i,e} \in W^{1,1}(0,T;H^{-1/2}(\Gamma_{i,e})),$$

and (2.23), (2.31) are satisfied. Then there exists a unique solution u of Problem $(A\mu)$; in particular there exist a couple

$$u_i, u_e \in L^2(0, T; H^1(\Omega_{i,e})) \cap C^0([0, T]; H^1(\Omega_{i,e}))$$

uniquely determined up to a family of additive constants c(t) and a unique couple (v, w) with (2.35)

$$v \in C^0([0,T]; L^2(\Gamma_m)) \cap L^2(0,T; H^{1/2}(\Gamma_m)), \quad \partial_t v \in L^1_{loc}(0,T; H^{-1/2}(\Gamma_m)),$$

$$(2.36) w, \partial_t w \in C^0([0,T]; L^2(\Gamma_m)) \cap L^2(0,T; H^{1/2}(\Gamma_m)),$$

which solve the microscopic model (μ_1, \ldots, μ_9) , as formulated by Problem (μ) , in the standard distribution sense. Moreover, if

(2.37)
$$v^0 \in H^{1/2}(\Gamma_m), \quad v^0 F(v^0) \in L^1(\Gamma_m),$$

then

$$(2.38) \quad u_{i,e} \in C^0([0,T]; H^1(\Omega_{i,e})), \quad \partial_t v \in L^2(\Sigma_m), \quad w \in C^0([0,T]; H^{1/2}(\Gamma_m)).$$

Structural properties. The proof of this theorem follows from a direct application of Theorem 4 of $\S 4$; now we limit ourselves to point out some distinctive properties of $a,b,\mathfrak{F},\boldsymbol{L}$ which will guide us in the choice and the application of the abstract framework and which are common to different situations, as the macroscopic model. These properties will conclude the proof of theorem 1.

P1. b is symmetric and the associated quadratic form (which we will denote by b again) is nonnegative but its kernel has infinite dimension, so that (2.18) is a degenerate evolution equation. However, by (μ_3) and Poincaré inequality, the sum of the quadratic forms associated to a and b is coercive on V, i.e.

$$(2.39) \exists \alpha > 0: \quad a(\boldsymbol{u}, \boldsymbol{u}) + b(\boldsymbol{u}, \boldsymbol{u}) \ge \alpha \|\boldsymbol{u}\|_{\boldsymbol{V}}^{2}, \quad \forall \boldsymbol{u} \in \boldsymbol{V},$$

and a verifies

$$|a(\boldsymbol{u}, \hat{\boldsymbol{u}}) - a(\hat{\boldsymbol{u}}, \boldsymbol{u})|^{2} = 4\Theta^{2} \left| \int_{\Gamma_{m}} \left(v \hat{\boldsymbol{w}} - \hat{\boldsymbol{v}} \, \boldsymbol{w} \right) d\mathcal{H}^{d-1} \right|^{2}$$

$$\leq \frac{4\Theta^{2}}{\rho \mathsf{C}_{m}} \int_{\Gamma_{m}} \left(\mathsf{C}_{m} v^{2} + \rho w^{2} \right) d\mathcal{H}^{d-1} \int_{\Gamma_{m}} \left(\mathsf{C}_{m} \hat{\boldsymbol{v}}^{2} + \rho \hat{\boldsymbol{w}}^{2} \right) d\mathcal{H}^{d-1}$$

$$\leq \frac{4\Theta^{2}}{\rho \mathsf{C}_{m}} b(\boldsymbol{u}, \boldsymbol{u}) \ b(\hat{\boldsymbol{u}}, \hat{\boldsymbol{u}}).$$

P2. The nonlinear operator $\mathfrak{F}:D(\mathfrak{F})\subset V\to V'$ is a linear perturbation of a subdifferential one; in order to show this fact, let us set for $\lambda\in\mathbb{R}$

(2.41)
$$F_{\lambda}(v) := F(v) + \lambda v, \quad \phi_{\lambda}(v) := \int_{0}^{v} F_{\lambda}(s) \, ds = \frac{\lambda C_{m}}{2} v^{2} + \int_{0}^{v} F(s) \, ds.$$

In this way, if $\lambda \geq \lambda_F/C_m$, F_{λ} is an increasing function whose primitive ϕ_{λ} is convex. We introduce the convex l.s.c. functional on V

(2.42)
$$\Phi(\boldsymbol{u}) := \begin{cases} \int_{\Gamma_m} \left(\phi_{\lambda}(u_i - u_e) + \frac{\lambda}{2} \rho w^2 \right) d\mathcal{H}^{d-1}, & \text{if } \phi(u_i - u_e) \in L^1(\Gamma_m) \\ +\infty & \text{otherwise,} \end{cases}$$

and, adapting the results of [9], we know that a functional $\ell \in V'$ belongs to the subdifferential $\partial \Phi(u)$ if and only if

$$(2.43) \quad \begin{cases} F_{\lambda}(u_i - u_e) \in L^1(\Gamma_m) \cap H^{-1/2}(\Gamma_m), & \text{i.e. } \boldsymbol{u} \in D(\mathfrak{F}), \text{ and} \\ \langle \boldsymbol{\ell}, \hat{\boldsymbol{u}} \rangle = {}_{H^{-1/2}(\Gamma_m)} \langle F_{\lambda}(u_i - u_e), \hat{u}_i - \hat{u}_e \rangle_{H^{1/2}(\Gamma_m)} + \lambda \rho \int_{\Gamma_m} w \hat{w} \, d\mathcal{H}^{d-1}. \end{cases}$$

This formula shows that $\ell \in \partial \Phi(u)$ is equivalent to

$$\langle \boldsymbol{\ell}, \hat{\boldsymbol{u}} \rangle = \langle \mathcal{F} \boldsymbol{u}, \hat{\boldsymbol{u}} \rangle + \lambda \int_{\Gamma_m} \left(\mathsf{C}_m(u_i - u_e) \left(\hat{u}_i - \hat{u}_e \right) + \rho w \hat{w} \right) d\mathcal{H}^{d-1} =$$
$$= \langle \mathfrak{F} \boldsymbol{u}, \boldsymbol{u} \rangle + \lambda b(\boldsymbol{u}, \hat{\boldsymbol{u}}),$$

i.e.

$$\mathfrak{F} = \partial \Phi - \lambda B.$$

Let us remark that if $v \in L^2(\Gamma_m)$, the property $\phi(v) \in L^1(\Gamma_m)$ is equivalent to ask $vF(v) \in L^1(\Gamma_m)$, by the monotonicity of F_{λ} and (2.41).

P3. Let us denote by $K_b \subset V$ the kernel of B and $b(\cdot, \cdot)$, i.e.

(2.45)
$$K_b := \{ \boldsymbol{u} \in \boldsymbol{V} : u_i|_{\Gamma_m} \equiv u_e|_{\Gamma_m}, \ w \equiv 0 \} = \{ \boldsymbol{u} \in \boldsymbol{V} : b(\boldsymbol{u}, \boldsymbol{u}) = 0 \}.$$

The functional Φ is invariant with respect to the translation of K_b , or equivalently, it admits the obvious decomposition

(2.46)
$$\Phi := \tilde{\phi}_b \circ \tilde{B}, \quad \text{where} \quad \tilde{\phi}_b : \tilde{V}_b \to [0, +\infty]$$

can be formally obtained from (2.42) by replacing $u_i - u_e$ with v. Analogously, $\mathfrak F$ can be written as

(2.47)
$$\mathfrak{F} = \tilde{B}^* \circ \tilde{\phi}_b \circ \tilde{B}, \quad \text{with} \quad \tilde{\phi}_b : D(\tilde{\phi}_b) \subset \tilde{V}_b \to \tilde{V}_b'.$$

We observe that, with respect to the duality between \tilde{V}_b and \tilde{V}_b' , $\tilde{\Phi}$ and $\tilde{\mathfrak{F}}$ have the same properties of Φ , \mathcal{F} with respect to $\boldsymbol{V}, \boldsymbol{V}'$.

P4. We can characterize the image $V'_b := \tilde{B}^*(\tilde{V}'_b)$ as the closed subspace of V'

$$(2.48) V_b' := \{ \boldsymbol{\ell} \in \boldsymbol{V}' : \langle \boldsymbol{\ell}, \boldsymbol{u} \rangle = 0, \quad \forall \, \boldsymbol{u} \in \boldsymbol{K}_b \}$$

Setting $V_b := \tilde{B}^*J_b(\tilde{V}_b) = B(\boldsymbol{V}) \subset V_b'$, endowed with the induced norm, \tilde{B}^* establishes an isomorphism between the Hilbert triple $V_b, \tilde{H}_b, \tilde{V}_b'$ and V_b, H_b, V_b' , where H_b is the intermediate interpolation space $H_b := (V_b, V_b')_{1/2,2}$. It is easy to translate all the properties holding in one of these triples (as in the next Theorem 4) into the corresponding ones in the other setting.

Extra regularity. In the case of a single parabolic equation of second order, further regularity properties can often be deduced by the usual maximum principle arguments (see [50]); since we are dealing with a parabolic system, this technique can not be applied.

In any case, we are mostly interested to point out the abstract variational structure of the micro- and macroscopic problems, which is preserved by the asymptotic (formal) limit and which will play a crucial role in a rigorous asymptotic analysis. Postponing to a forthcoming paper this study, here we do not exploit further regularity properties, which are also influenced by the particular choice of F and by the singular character of the boundary conditions at the junction points of Γ_i , Γ_e , and Γ_m . Let us only mention another existence result under slightly weaker assumptions, which is important for the specific cardiac model we are referring to, and which is an immediate consequence of the abstract theory.

Proposition 2.4. Suppose that (the space dimension) d = 3, Γ_m has a finite measure, and F has a cubic growth at infinity as in (μ_7'') . Then (2.35) and (2.36) hold even if we assume (2.16) instead of the stronger (2.34).

Proof. By the Sobolev Imbedding Theorem, we know that $H^{1/2}(\Gamma_m)$ is continuously imbedded into $L^4(\Gamma_m)$, and consequently

$$L^2(\Gamma_m) \subset L^{4/3}(\Gamma_m) \subset H^{-1/2}(\Gamma_m).$$

We deduce that, for $\lambda \geq \lambda_F$ and suitable constants C_i dependent only on Γ_m

(2.49)
$$||F(v)||_{H^{-1/2}(\Gamma_m)}^{4/3} \le C_1 ||F(v)||_{L^{4/3}(\Gamma_m)}^{4/3} \le C_2 \left(1 + \int_{\Gamma_m} v^4 d\mathcal{H}^2\right)$$

$$\le C_3 \left(1 + \int_{\Gamma_m} \phi_{\lambda}(v) d\mathcal{H}^2\right) \le C_3 \left(1 + \Phi(\boldsymbol{u})\right);$$

thus we can apply the next Proposition 4.3.

3. Variational formulation of the macroscopic problem.

We now consider the variational formulation of the macroscopic bidomain model (M_1, \ldots, M_9) . Because of the analogy with the procedure of the previous section, we will proceed on more quickly.

Preliminaries. As we did before, we slightly reinforce (M_1, M_3, M_7) by requiring that

 (M_1') Ω is a Lipschitz domain of \mathbb{R}^d , $\Gamma = \partial \Omega$, $\nu :=$ unitary exterior normal to Γ , As usual we set $Q := \Omega \times]0, T[$, $\Sigma := \Gamma \times]0, T[$.

We also suppose that $M_i(x), M_e(x)$, are measurable and satisfy the uniform ellipticity condition

$$(M_3')$$
 $\exists \alpha, m > 0 : \alpha |\xi|^2 \le M_{i,e}(x) \xi \cdot \xi \le m |\xi|^2, \quad \forall \xi \in \mathbb{R}^d, \ x \in \Omega.$ Finally, f is a continuous function with

$$(M_7')$$
 $f(0) = 0;$ $\exists \lambda_f \ge 0:$ $\frac{f(x) - f(y)}{x - y} \ge -\lambda_f, \quad \forall x, y \in \mathbb{R}, \text{ with } x \ne y;$

sometimes we will also require that f has a cubic growth at infinity, i.e.

$$(M_7'') \qquad \qquad 0 < \liminf_{|s| \to +\infty} \frac{f(s)}{s^3} \leq \limsup_{|s| \to +\infty} \frac{f(s)}{s^3} < +\infty.$$

The following problem collects the discussion presented in the Introduction:

Problem (M). Given

(3.1)
$$i_{i,e}^s: Q \to \mathbb{R}, \quad g_{i,e}: \Sigma \to \mathbb{R}, \quad \text{and} \quad v^0, w^0: \Omega \to \mathbb{R},$$

we seek

$$u_i, u_e, w: Q \to \mathbb{R}$$
, with $v:=u_i-u_e$,

which solve

(3.2)
$$\begin{cases} \mathsf{c}_{m}\partial_{t}v + f(v) + \theta w = \operatorname{div}\left(M_{i}\nabla u_{i}\right) + i_{i}^{s} & \text{in } Q, \\ \mathsf{c}_{m}\partial_{t}v + f(v) + \theta w = -\operatorname{div}\left(M_{e}\nabla u_{e}\right) - i_{e}^{s} & \text{in } Q, \\ \partial_{t}w + \gamma w - \eta v = 0 & \text{in } Q, \\ v(x, 0) = v^{0}(x), \quad w(x, 0) = w^{0}(x) & \text{in } \Omega, \\ M_{i,e}\nabla u_{i,e} \cdot \nu = g_{i,e} & \text{on } \Sigma. \end{cases}$$

Arguing as in the previous section, we introduce the Hilbert spaces

(3.3)
$$X := H^1(\Omega) \times H^1(\Omega) \times L^2(\Omega), \quad V := X/\{(c, c, 0) : c \in \mathbb{R}\},$$

(whose generic elements (u_i, u_e, w) we denote by \boldsymbol{u} again), the bilinear forms on $\boldsymbol{V} \times \boldsymbol{V}$ (here $\rho := \theta/\eta$)

(3.4)
$$b(\boldsymbol{u}, \hat{\boldsymbol{u}}) := \int_{\Omega} \left[c_m (u_i - u_e)(\hat{u}_i - \hat{u}_e) + \rho \, w \hat{w} \right] dx,$$

$$(3.5) \quad a(\boldsymbol{u}, \hat{\boldsymbol{u}}) := \sum_{i,e} \int_{\Omega} M_{i,e} \nabla u_{i,e} \cdot \nabla \hat{u}_{i,e} \, dx + \theta \int_{\Omega} \left[w(\hat{u}_i - \hat{u}_e) - (u_i - u_e) \hat{w} \right] dx,$$

the functionals on X

(3.6)
$$\begin{cases} \langle \boldsymbol{L}(t), \hat{\boldsymbol{u}} \rangle := \sum_{i,e} \int_{\Omega} i_{i,e}^{s} \, \hat{u}_{i,e} \, dx + \sum_{i,e} {}_{H^{-1/2}(\Gamma)} \langle g_{i,e}, \hat{u}_{i,e} \rangle_{H^{1/2}(\Gamma)}, \\ \langle \boldsymbol{\ell}^{0}, \hat{\boldsymbol{u}} \rangle := \int_{\Omega} \left(\mathsf{C}_{m} \, v^{0} \, \hat{v} + \rho \, w^{0} \, \hat{w} \right) dx, \end{cases}$$

and the operator $\mathfrak{F}:D(\mathfrak{F})\subset \mathbf{V}\to \mathbf{V}'$

(3.7)
$$\langle \mathfrak{F}\boldsymbol{u}, \hat{\boldsymbol{u}} \rangle := \int_{\Omega} \left[f(u_i - u_e)(\hat{u}_i - \hat{u}_e) \right] dx,$$

with domain

$$(3.8) D(\mathfrak{F}) := \{ \boldsymbol{u} \in \boldsymbol{V} : f(u_i - u_e) \in L^1(\Omega) \cap (H^1(\Omega))' \};$$

this means that for every $u \in D(\mathfrak{F})$ there exists a constant C > 0 such that

(3.9)
$$\int_{\Omega} f(u_i - u_e) \zeta \, dx \le C \|\zeta\|_{H^1(\Omega)}, \quad \forall \zeta \in H^1(\Omega) \cap L^{\infty}(\Omega).$$

Again we observe that all these definitions are compatible with the quotient space V, provided that

(3.10)
$$\int_{\Omega} \left(i_i^s + i_e^s \right) dx + {}_{H^{-1/2}(\Gamma)} \langle g_i + g_e, 1 \rangle_{H^{1/2}(\Gamma)} = 0, \quad \text{for a.e. } t \in]0, T[.$$

Here is the precise statement of Problem (M) in a variational abstract form.

Problem (AM). Let us assume that

(3.11)
$$i_{i,e}^s \in L^2(Q), \quad g_{i,e} \in L^2(0,T;H^{-1/2}(\Gamma)), \quad v^0, w^0 \in L^2(\Omega),$$

and (3.10) is satisfied. Then, if $V, b, a, L, \ell^0, \mathfrak{F}$ are defined by (3.3),...,(3.7) respectively, and A, B are defined as in (2.24), we seek $\boldsymbol{u}(t) := (u_i(\cdot, t), u_e(\cdot, t), w(\cdot, t))$, with

(3.12)
$$\mathbf{u} \in L^2(0,T;\mathbf{V}), \quad B\mathbf{u} \in W^{1,1}_{loc}(0,T;\mathbf{V}') \cap C^0([0,T];\mathbf{V}'),$$

satisfying for

(3.13)
$$(B\mathbf{u})' + A\mathbf{u} + \mathfrak{F}\mathbf{u} = \mathbf{L}, \text{ in } \mathbf{V}', \text{ a.e. in }]0, T[,$$

together to the initial condition

$$(3.14) \qquad (B\mathbf{u})(0) = \ell^0.$$

Also for this problem we could repeat the same structural remarks $\mathbf{P1}, \ldots, \mathbf{4}$ of the previous section, the basic properties of V, b, a, \mathfrak{F}, L being the same. We deduce the following statement.

Theorem 2. In the framework of the macroscopic model (M_1, \ldots, M_9) , (M'_1, M'_3, M'_7) , let us assume that (3.11) and (3.10) are satisfied, together with

$$(3.15) i_i^s + i_e^s \in W^{1,1}(0,T;L^2(\Omega)), g_{i,e} \in W^{1,1}(0,T;H^{-1/2}(\Gamma)).$$

Then Problem (AM) admits a unique solution u. In particular there exist a couple

$$u_i, u_e \in L^2(0, T; H^1(\Omega)),$$

uniquely determined up to a family of additive constants c(t), and a unique couple (v,w) with

(3.16)
$$v \in C^0([0,T]; L^2(\Omega)) \cap L^2(0,T; H^1(\Omega)), \quad \partial_t v \in L^2_{loc}(0,T; L^2(\Omega)),$$

 $w, \partial_t w \in C^0([0,T]; L^2(\Omega)),$

which solve the macroscopic model (M_1, \ldots, M_9) in the sense of Problem (M). Moreover, if

(3.17)
$$v^0 \in H^1(\Omega), \quad v^0 f(v^0) \in L^1(\Omega),$$

then

$$(3.18) u_{i,e} \in C^0([0,T]; H^1(\Omega)), \quad \partial_t v \in L^2(Q), \quad w \in C^0([0,T]; H^1(\Omega)).$$

Proof. We argue as before by invoking Theorem 4 of the next session; in this case we can establish an isomorphism of the "abstract Hilbert triple" V_b, H_b, V_b' introduced there with the "concrete"

$$\tilde{V}_b := H^1(\Omega) \times L^2(\Omega), \quad \tilde{H}_b := L^2(\Omega) \times L^2(\Omega), \quad \tilde{V}_b' := \left(H^1(\Omega)\right)' \times L^2(\Omega)$$

via the transpose of the operator $\tilde{B}\boldsymbol{u} := (u_i - u_e, w)$. The first condition of (3.15) follows from the simple splitting

$$\int_{\Omega} (i_i^s u_i + i_e^s u_e) dx = \frac{1}{2} \int_{\Omega} (i_i^s - i_e^s) (u_i - u_e) dx + \frac{1}{2} \int_{\Omega} (i_i^s + i_e^s) (u_i + u_e) dx$$

Further results. We conclude this section by extending Theorem 2 in two different directions.

Proposition 3.1. Suppose that d = 3, and (M_7'') holds; then, if (3.11) holds, Problem (\mathbf{M}) admits a unique strong solution \mathbf{u} . Moreover, if (3.15) and (3.17) hold, then

$$(3.19) -\operatorname{div}\left(M_{i,e}\nabla u_{i,e}\right) \in L^2(Q).$$

Proof. It follows from Propositions 4.3 and 4.4 by the same arguments of Proposition 2.4. $\hfill\Box$

Remark 3.2. If

(3.20)
$$\Omega$$
 is of class $C^{1,1}$, $M_{i,e}$ are Lipschitz in Ω ,

and

(3.21)
$$g_{i,e} \in L^2(0,T;H^{1/2}(\Gamma)),$$

then (3.19) and standard regularity estimates for elliptic problems yield

$$(3.22) u_{i,e} \in L^2(0,T;H^2(\Omega)).$$

Proposition 3.3. Suppose that (3.20) holds and $M_i\nu$ and $M_e\nu$ have the same direction on Γ . If

(3.23)
$$\partial_t i_{i,e}^s \in L^2(Q), \quad \partial_t g_{i,e} \in L^2(0,T;H^{-1/2}(\Gamma))$$

and

(3.24)
$$v^0 \in H^2(\Omega), \quad f(v^0) \in L^2(\Omega), \quad g_{i,e}(0) \in H^{1/2}(\Gamma)$$

then, for every $\varepsilon > 0$,

$$(3.25) \quad v \in W^{1,\infty}(0,T;L^2(\Omega)) \cap H^{3/2-\varepsilon}(0,T;L^2(\Omega)), \quad u_{i,e} \in H^1(0,T;H^1(\Omega)).$$

Proof. It follows from the third implication of Theorem 4.

4. The abstract theory.

Let V be a (separable) Hilbert space with dual V', $\langle \cdot, \cdot \rangle$ denoting the duality pairing between them,

$$(A_1)$$
 let $a(\cdot,\cdot)$, $b(\cdot,\cdot)$: $\mathbf{V} \times \mathbf{V} \to \mathbb{R}$ be continuous bilinear forms,

with the associated linear continuous operators

$$(A_2)$$
 $A, B : \mathbf{V} \to \mathbf{V}'; \quad \langle A\mathbf{u}, \mathbf{w} \rangle = a(\mathbf{u}, \mathbf{w}), \quad \langle B\mathbf{u}, \mathbf{w} \rangle = b(\mathbf{u}, \mathbf{w}), \quad \forall \mathbf{u}, \mathbf{w} \in \mathbf{V},$

$$(A_3)$$
 let $\mathfrak{F}: D(\mathfrak{F}) \subset V \to V'$ be a (nonlinear) operator.

We are interested to the following abstract Cauchy problem.

Problem (A). Given
$$L \in L^2(0,T; V')$$
 and $\ell^0 \in V'$, find

$$\boldsymbol{u} \in L^2(0,T;\boldsymbol{V}), \quad \text{with} \quad B\boldsymbol{u} \in W^{1,1}_{loc}(0,T;\boldsymbol{V}') \cap C^0([0,T];\boldsymbol{V}')$$

such that

(4.1)
$$\begin{cases} (B\boldsymbol{u})' + A\boldsymbol{u} + \mathfrak{F}\boldsymbol{u} = \boldsymbol{L}, & \text{a.e. in }]0, T[, \\ (B\boldsymbol{u})(0) = \boldsymbol{\ell}^0. \end{cases}$$

Degenerate parabolic equations of this kind have been studied by many authors (see [11, 8, 19, 15], and [13, 49, 21] for an extensive bibliography) in a very general context: e.g. V could be a reflexive Banach space and A a (pseudo)monotone bounded operator; under suitable compatibility assumptions [19] also B could be nonlinear. In particular, adapting a result of [13] via the techniques developed in [7], an existence and uniqueness result could be given for a weak formulation of (4.1). Another possible way is to use a regularizing method as in [19], replacing the (possibly) degenerate bilinear form b with a coercive one b_{ε} and proving uniform estimates with respect to $\varepsilon \to 0^+$ in an appropriate functional setting. A natural choice in this approach is

$$b_{\varepsilon}(u, w) := b(u, w) + \varepsilon(u, w)_{\mathbf{V}}.$$

Main assumptions. In this paper, inspired by the structural properties **P1-4** we detailed in § 2, we follow a more direct way, exploiting the particular compatibility of the nonlinear operator \mathfrak{F} with respect to the degeneration of b.

More precisely, we assume that b is symmetric and positive, but possibly degenerate on the closed subspace K_b :

 (A_4) $b(\boldsymbol{u}, \boldsymbol{w}) = b(\boldsymbol{w}, \boldsymbol{u}),$ $b(\boldsymbol{u}, \boldsymbol{u}) \geq 0;$ $b(\boldsymbol{u}, \boldsymbol{u}) = 0 \Leftrightarrow \boldsymbol{u} \in \boldsymbol{K}_b \quad \forall \boldsymbol{u}, \boldsymbol{w} \in \boldsymbol{V},$ a is weakly coercive on \boldsymbol{V} and "almost" symmetric:

$$(A_5) \quad \exists \alpha, c > 0: \quad \begin{cases} a(\boldsymbol{u}, \boldsymbol{u}) + b(\boldsymbol{u}, \boldsymbol{u}) \ge \alpha \|\boldsymbol{u}\|_{\boldsymbol{V}}^2, \\ |a(\boldsymbol{u}, \boldsymbol{w}) - a(\boldsymbol{w}, \boldsymbol{u})|^2 \le c b(\boldsymbol{u}, \boldsymbol{u}) b(\boldsymbol{w}, \boldsymbol{w}), \end{cases} \quad \forall \boldsymbol{u}, \boldsymbol{w} \in \boldsymbol{V}.$$

We will suppose that $\mathfrak{F} = \partial \Phi - \lambda B$, $\lambda \geq 0$, is a linear perturbation of the subdifferential of

$$(A_6) \qquad \Phi: \mathbf{V} \to [0, +\infty] \quad \text{proper, convex, l.s.c. function,}$$

$$\ell = \mathfrak{F} \mathbf{u} \quad \Leftrightarrow \quad \langle \ell, \mathbf{w} - \mathbf{u} \rangle + \lambda b(\mathbf{u}, \mathbf{w} - \mathbf{u}) + \Phi(\mathbf{w}) < \Phi(\mathbf{u}), \quad \forall \mathbf{w} \in \mathbf{V}.$$

Finally, we shall assume that Φ is invariant with respect to the translation of K_b :

$$(A_7) \qquad \Phi(\boldsymbol{u} + \boldsymbol{k}) = \Phi(\boldsymbol{u}) \quad \forall \, \boldsymbol{u} \in \boldsymbol{V}, \, \, \boldsymbol{k} \in \boldsymbol{K}_b, \quad \text{or, equivalently,}$$

$$\langle \mathfrak{F}\boldsymbol{u}, \boldsymbol{k} \rangle = 0, \quad \mathfrak{F}(\boldsymbol{u} + \boldsymbol{k}) = \mathfrak{F}(\boldsymbol{u}), \quad \forall \, \boldsymbol{u} \in D(\mathfrak{F}), \, \forall \, \boldsymbol{k} \in \boldsymbol{K}_b.$$

A reduction technique. We shall show that Problem (A) can be reduced, by the "change of variable v := Bu", to a usual (non degenerate) evolution variational inequality of the type

(4.2)
$$v(0) = \ell^0$$
, $(v' + (A_b - \lambda)v - L_b, v - w)_b + \Phi_b(v) \leq \Phi_b(w)$, $\forall w \in V_b$ in a suitable Hilbert triple $V_b \subset H_b \subset V_b'$, with A_b, L_b, Φ_b related in a explicit way to A, L, Φ .

In this formulation, regularity and approximation results are easier and deeply studied (see [33, 10, 7, 31, 22, 2, 48]) and they give corresponding information about the original problem A. In particular the study of the time discretization by the backward Euler method and of some further regularity properties of (4.1) are developed by [2, 43, 47, 48, 38]. In order to state our results, we introduce the Hilbert spaces

(4.3)
$$V_b = B(\mathbf{V})$$
, with the norm $||v||_b = \inf \{ ||\mathbf{u}||_{\mathbf{V}} : \mathbf{u} \in \mathbf{V}, B\mathbf{u} = v \}$, and

$$(4.4) V_b' = \left\{ L \in \mathbf{V}' : \langle L, \mathbf{k} \rangle = 0, \quad \forall \mathbf{k} \in \mathbf{K}_b \right\}.$$

It is easy to see that V_b is included in V'_b and it is isomorphic to the quotient space V/K_b , whereas V'_b is isomorphic to its dual, so that our notation is correct. We denote by $J: V_b \to V$ a right inverse of B, defined by

(4.5)
$$Jv = u \Leftrightarrow Bu = v$$
, and $a(u, k) = 0$, $\forall k \in K_b$.

By (A_5) $a(\cdot,\cdot)$ is coercive on K_b ; Lax-Milgram lemma ensures that J is a linear isomorphism. Observe that, when a is symmetric, (4.5) is equivalent to the minimization problem

$$(4.6) B\mathbf{u} = v, \quad a(\mathbf{u}, \mathbf{u}) = \min \{a(\mathbf{w}, \mathbf{w}) : B\mathbf{w} = v\}.$$

Each element $u \in V$ admits the linear decomposition

$$(4.7) u = Jv + k: v = Bu, k = u - JBu \in K_b.$$

We define the duality pairing between V'_b and V_b as

$$(4.8) \qquad (\ell, v)_b := _{\mathbf{V}'} \langle \ell, \mathbf{J} v \rangle_{\mathbf{V}} = _{\mathbf{V}'} \langle \ell, \mathbf{u} \rangle_{\mathbf{V}}, \quad \forall \ell \in V_b', \ v \in V_b, \ \mathbf{u} \in B^{-1}v.$$

It is easy to see that $(\cdot, \cdot)_b$ restricted to $V_b \times V_b$ is a scalar product, associated to the intermediate norm

$$(4.9) |v|_b^2 := (v, v)_b = b(\mathbf{J}v, \mathbf{J}v).$$

By the standard duality theory, we can identify the completion H_b of V_b with respect to this norm with the space

$$(4.10) H_b' = \Big\{ \ell \in V_b' : \sup_{w \in \mathbf{V} \setminus \mathbf{K}_b} \frac{\langle \ell, w \rangle}{\sqrt{b(w, w)}} = \sup_{v \in V_b \setminus \{0\}} \frac{(\ell, v)_b}{|v|_b} < +\infty \Big\}.$$

In this way V_b , $H_b \equiv H_b'$, V_b' becomes a standard Hilbert triple and defining

(4.11)
$$\Phi_b(v) := \Phi(\boldsymbol{J}v), \qquad a_b(v, w) := a(\boldsymbol{J}v, \boldsymbol{J}w),$$

we can consider the following evolution variational inequality:

Problem
$$(A_b)$$
. Given $L_b \in L^2(0,T;V_b')$ and $\ell^0 \in V_b'$, find

$$v \in L^2(0,T;V_b) \cap W^{1,1}_{loc}(0,T;V_b') \cap C^0([0,T];V_b')$$

such that:

(4.12)
$$(v' + (A_b - \lambda)v - L_b, v - w)_b + \Phi_b(v) \le \Phi_b(w), \quad \forall w \in V_b, \text{ a.e. in }]0, T[, v(0) = \ell^0.$$

The link with problem (A) is given by the following result.

Theorem 3. The function u is a strong solution of problem (A) if and only if it admits the decomposition

$$(4.13) u = u_L + Jv,$$

where u_{L} solves

$$(4.14) u_{\mathbf{L}}(t) \in \mathbf{K}_b, \quad a(u_{\mathbf{L}}(t), \mathbf{k}) = \langle \mathbf{L}(t), \mathbf{k} \rangle, \quad \forall \mathbf{k} \in \mathbf{K}_b, \text{ a.e. in }]0, T[,$$

and v is a solution of problem (A_b) with respect to

$$(4.15) L_b(t) := \mathbf{L}(t) - Au_{\mathbf{L}}(t).$$

Proof. Observe that $L_b(t) \in V_b'$ for a.e. $t \in]0, T[$ so that (4.12) makes sense. Let \boldsymbol{u} be a strong solution of Problem (\boldsymbol{A}) and $v := B\boldsymbol{u}$; by (A_7) we have $\mathfrak{F}\boldsymbol{u} \in V_b'$ so that, taking the duality of each member of equation (4.1) by a generic element $\boldsymbol{k} \in \boldsymbol{K}_b$ we get

$$(4.16) a(\mathbf{u}(t), \mathbf{k}) = \langle \mathbf{L}(t), \mathbf{k} \rangle, \quad \forall \mathbf{k} \in \mathbf{K}_b, \text{ for a.e. } t \in]0, T[.$$

This implies that

$$a(\boldsymbol{u}(t) - u_{\boldsymbol{L}}(t), \boldsymbol{k}) = 0$$
, $B(\boldsymbol{u}(t) - u_{\boldsymbol{L}}(t)) = v(t)$, $\forall \boldsymbol{k} \in \boldsymbol{K}_b$, for a.e. $t \in]0, T[$, i.e. $\boldsymbol{u} - u_{\boldsymbol{L}} = \boldsymbol{J}v$ by definition (4.5).

Coming back to equation (4.1), since $\mathfrak F$ is invariant by $\pmb K_b$ -translations, we read that

(4.17)
$$v' + A(Jv) + \mathfrak{F}(Jv) = (Bu)' + A(u - u_L) + \mathfrak{F}(u - u_L) = L - Au_L = L_b.$$

Taking the duality of (4.17) with J(v-w), $w \in V_b$, and recalling (4.11), we get

$$(v', v - w)_b + a_b(v, v - w) - (L_b, v - w)_b = \langle \mathcal{F}(\boldsymbol{J}v), w - v \rangle \le$$

$$\le \Phi(\boldsymbol{J}w) - \Phi(\boldsymbol{J}v) - \lambda b(\boldsymbol{J}v, \boldsymbol{J}(w - v)) = \Phi_b(w) - \Phi_b(v) - \lambda(v, w - v)_b$$

by (A_6) , (4.5), (4.8), and (4.11); therefore, v solves (4.12).

Let now v be a solution of (4.12), u_L be given by (4.14), and $u := u_L + Jv$. By (4.11) and (4.15) we deduce

$$\langle B(\boldsymbol{J}v)' + A(\boldsymbol{J}v) - L_b, \boldsymbol{J}(v-w) \rangle \leq \Phi(\boldsymbol{J}w) - \Phi(\boldsymbol{J}v) - \lambda \langle B\boldsymbol{J}v, \boldsymbol{J}(w-v) \rangle, \quad \forall w \in V_b.$$

By (4.14), (4.5), and (A_7) we have

$$\langle B\boldsymbol{J}v' + A(\boldsymbol{J}v) - (\boldsymbol{L} - Au_{\boldsymbol{L}}), \boldsymbol{J}v + u_{\boldsymbol{L}} - (\boldsymbol{J}w + \boldsymbol{k}) \rangle \leq \Phi(\boldsymbol{J}w + \boldsymbol{k}) - \Phi(\boldsymbol{J}v + u_{\boldsymbol{L}}) - \lambda \langle B\boldsymbol{J}v, \boldsymbol{J}w + \boldsymbol{k} - (\boldsymbol{J}v + u_{\boldsymbol{L}}) \rangle, \quad \forall w \in V_b, \ \forall \boldsymbol{k} \in \boldsymbol{K}_b.$$

Since $Bu_{\boldsymbol{L}} \equiv 0$, (4.15) yields

$$\langle (B\boldsymbol{u})' + A\boldsymbol{u} - \boldsymbol{L}, \boldsymbol{u} - (\boldsymbol{J}w + \boldsymbol{k}) \rangle \leq \Phi(\boldsymbol{J}w + \boldsymbol{k}) - \Phi(\boldsymbol{u}) - \lambda \langle B\boldsymbol{u}, \boldsymbol{J}w + \boldsymbol{k} - \boldsymbol{u} \rangle,$$

for every choice of $w \in V_b$, $\mathbf{k} \in \mathbf{K}_b$. Since $\mathbf{V} = \mathbf{J}(V_b) + \mathbf{K}_b$ thanks to (4.7), by (A_6) we deduce that

$$(B\mathbf{u})' + A\mathbf{u} - \mathbf{L} = -\mathfrak{F}\mathbf{u}$$

i.e. (4.1).

Main result. We have now all the elements to state our main result.

Theorem 4. Let us assume that

(4.18)
$$\ell^0 \in \overline{D(\Phi_b)}^{H_b}, \quad L \in W^{1,1}(0,T; V') + L^2(0,T; H'_b).$$

Then there exists a unique strong solution u of problem (A) with

(4.19)
$$v := B\mathbf{u} \in H^1_{loc}(0, T; H_b) \cap C^0([0, T]; H_b), \quad \mathbf{u} \in C^0([0, T]; V).$$
If

(4.20)
$$\ell^0 \in V_b, \quad and \quad \exists \, \boldsymbol{u}^0 \in D(\Phi) : \, B\boldsymbol{u}^0 = \ell^0,$$

then

$$(4.21) v := B\mathbf{u} \in H^1(0, T; H_b), \quad \mathbf{u} \in C^0([0, T]; V).$$

Finally, if

$$(4.22) L \in H^1(0,T; \mathbf{V}'), \ell^0 \in V_b, J\ell^0 \in D(\mathfrak{F}), A(J\ell^0) + \mathfrak{F}(J\ell^0) \in H_b'$$

then

(4.23) $\mathbf{u} \in H^1(0,T; \mathbf{V})$ and $v = B\mathbf{u} \in W^{1,\infty}(0,T; H_b) \cap H^{3/2-\varepsilon}(0,T; H_b),$ for every $\varepsilon > 0$.

Proof. Let us observe that (A_4, \ldots, A_7) imply that

(4.24) $a_b(\cdot,\cdot) - \lambda(\cdot,\cdot)_b$ is weakly coercive on V_b , Φ_b is l.s.c. and convex on V_b .

By the general theory of evolution variational inequalities (see e.g. [6], prop. II.2 and [48], thm. 3), if (4.22) holds then problem (A_b) admits a unique strong solution

$$(4.25) v \in H^1(0,T;V_b) \cap W^{1,\infty}(0,T;H_b) \cap H^{3/2-\varepsilon}(0,T;H_b),$$

and Theorem 3 gives (4.23). Moreover, the mapping $(L_b, \ell^0) \mapsto v$ is Lipschitz with respect to the norm (cf. [48, 4.12]) of

$$\left(L^2(0,T;V_b') + L^1(0,T;H_b')\right) \times H_b$$

with values in $L^{\infty}(0,T;H_b) \cap L^2(0,T;V_b)$. This regular dependence of the solution from the data and a standard density argument allow us to prove the other two results (which are already known, in a slightly different form, when $a(\cdot,\cdot)$ is symmetric; cf. [6, cor. II.2] by simply showing the corresponding a priori estimates. To get (4.21), we write (4.12) as a differential equation governed by the subdifferential of Φ_b in H_b and multiply it by v', obtaining

$$|v'|_b^2 + \frac{d}{dt} \left[\frac{1}{2} a_b(v, v) + \Phi_b(v) \right] = (L_b, v')_b - \frac{1}{2} \left[a_b(v, v') - a_b(v', v) \right] + \lambda(v, v')_b$$

$$\leq (L_b, v')_b + (c + \lambda)|v|_b |v'|_b,$$

thanks to (A_5) . By integrating in time and applying Gronwall lemma, we get the estimate

$$\int_0^T |v'|_b^2 dt + \sup_{t \in [0,T]} \left[a_b(v,v) + \Phi_b(v) \right]$$

$$\leq C \left[\|\boldsymbol{\ell}^0\|_{V_b}^2 + \Phi_b(\boldsymbol{\ell}^0) + \|L_b\|_{W^{1,1}(0,T;V_b') + L^2(0,T;H_b)} \right]$$

with C independent of the data. Since $\Phi_b(\ell^0) = \Phi(u^0)$, (4.21) follows by (4.20).

The first implication follows by the same technique, multiplying the equation by tv' (cf. [6]).

Remark 4.1. Analogous results hold if \mathfrak{F} is a multivalued (subdifferential) operator; we considered the single-valued case, in order to simplify our exposition.

Remark 4.2. We could give an existence and uniqueness result for a suitable weak formulation of problems (\mathbf{A}) , (\mathbf{A}_b) (see [6, rem. II.5], and [48, rem. 1.1]), which requires

(4.26)
$$L \in L^2(0,T; V') + L^1(0,T; H_b), \quad \ell^0 \in \overline{D(\Phi_b)}^{H_b}$$

and gives $\boldsymbol{u} \in L^2(0,T;\boldsymbol{V})$ with $B\boldsymbol{u} \in C^0([0,T];H_b) \cap H^{1/2-\varepsilon}(0,T;H_b)$, for every $\varepsilon > 0$, together to the a priori estimate (cf. [48, 3.1 and thm. 3])

$$(4.27) \sup_{[0,T]} b(\boldsymbol{u},\boldsymbol{u}) + \int_0^T \left[\|\boldsymbol{u}\|_{\boldsymbol{V}}^2 + \Phi(\boldsymbol{u}) \right] dt \leq C \left[\|L_b\|_{L^2(0,T;\boldsymbol{V}') + L^1(0,T;\boldsymbol{H}_b)}^2 + |\boldsymbol{\ell}^0|_b^2 \right].$$

We give two other simple regularity results, under some additional assumptions on \mathfrak{F} .

Proposition 4.3. Assume that $D(\mathfrak{F}) \equiv D(\Phi)$ and that there exists C > 0, $p \in]1,2]$ such that

If (4.26) holds (instead of the stronger (4.18)), then Problem (\mathbf{A}) admits a unique strong solution.

Proof. Starting from the strongest result of Theorem 4 and the a priori estimate (4.27), we deduce

$$(4.29) \quad \|v'\|_{L^{p}(0,T;\mathbf{V}')}^{p} + \|\mathfrak{F}\boldsymbol{u}\|_{L^{p}(0,T;\mathbf{V}')}^{p} \le C \left[T + \int_{0}^{T} \left(\|\boldsymbol{u}\|_{\mathbf{V}}^{2} + \Phi(\boldsymbol{u})\right) dt\right]$$

$$\le C \left[1 + \|\boldsymbol{L}\|_{L^{2}(0,T;\mathbf{V}') + L^{1}(0,T;H_{b})}^{2} + |\boldsymbol{\ell}^{0}|_{b}^{2}\right]$$

with C independent of the data. By the usual density arguments, this is sufficient to obtain a strong solution of the problems $(\mathbf{A}), (\mathbf{A}_b)$ under (4.26).

Proposition 4.4. Assume that $D(\mathfrak{F}) \equiv V$, $\mathfrak{F}(V) \subset H_b$ and there exists C > 0, $p \ge 1$ such that

If (4.20) holds, we get

$$(4.31) A\boldsymbol{u} - \boldsymbol{L} \in L^2(0, T; H_b)$$

Proof. It is an immediate consequence of (4.21) and the equation (4.1).

Approximation results. We conclude this section with an example of the possible approximation results, which follow by applying the theory developed in [48, 38] to the abstract formulation (A_b) : other a priori and a posteriori estimates are available and it should not be difficult to translate them in the framework of the micro- and macroscopic problems (μ, M) ; this is also the starting point for a complete space-time discretization, as studied in [46] (for other approximation results in the context of reaction-diffusion problems, see e.g. [26, 28, 35]; a different abstract approach has been developed in [4].)

We choose a partition \mathcal{P} of the time interval [0,T] into N subintervals

$$(4.32) \mathcal{P} := \{ 0 = t_0 < t_1 < \dots < t_{N-1} < t_N = T \},$$

with variable step $\tau_n := t_n - t_{n-1}$, and we consider the sequence $\{U_n\}_{n=0}^N$ whose first term is given and satisfies $BU^0 = \ell^0$ and the other ones are recursively defined for $1 \le n \le N$ by

$$\frac{1}{\tau_n}B(U^n - U^{n-1}) + A(U^n) + \mathfrak{F}U^n = L^n, \text{ for } n = 1, \dots, N,$$

where L^n is a suitable approximation of \boldsymbol{L} in the time interval $(t_{n-1}, t_n]$, e.g. $L^n := \boldsymbol{L}(t_n)$.

Hereafter, U is the piecewise linear interpolant of the values $\{U_n\}_{n=0}^N$ on the grid \mathcal{P} and $|\tau| := \max_{1 \leq n \leq N} \tau_n$ denotes the maximum of the time-step sizes. Combining Theorems 8 and 9 of [38] (see also [48, Thm. 3] in the case of a uniform mesh) we get

Theorem 5. Assume that (4.22) holds. Then we have the estimate

(4.33)
$$\|\boldsymbol{u} - \boldsymbol{U}\|_{L^{2}(0,T;\boldsymbol{V})} + \max_{t \in [0,T]} b(\boldsymbol{u} - \boldsymbol{U}, \boldsymbol{u} - \boldsymbol{U}) \le C|\tau|,$$

with C independent of the partition \mathcal{P} .

APPENDIX A. THE DERIVATION OF THE "BIDOMAIN" MODEL

For completeness in this appendix, using the two–scales method, we develop formal asymptotic expansions and we convert a microscopic model of the cellular media into an averaged continuum representation of the cardiac tissue, when the presence of stimulation currents are neglected and $\sigma_{i,e}$ do not depend on the position x. With respect to the procedure followed in [37], based on current balances expressed by means of integral identities, the formal derivation here presented is shorter and more standard. For the electric potentials u_i , u_e we can consider two characteristic length scales, the microscopic one related to a typical dimension d_c of the cells (e.g. the cell diameter is of order $10^{-3}cm$) and the other macroscopic one determined by a suitable length constant of the tissue. Following [37] we consider the dimensionless parameter

$$\varepsilon^2 = \mathsf{d}_c/(\mathsf{R}_m \sigma_i)$$
 with $\mathsf{R}_m^{-1} = \partial_v I_{ion}(0,0)$

assuming that v = 0, w = 0 is the equilibrium point for the problem (μ) .

We convert the cellular problem into a non-dimensional form, by scaling space and time with the macroscopic units of length $\mathsf{L}=\mathsf{d}_c/\varepsilon$ and with respect to the membrane constant $\mathsf{T}=\mathsf{R}_m\ \mathsf{C}_m$ i.e.

$$\hat{x} = x/L, \quad \hat{t} = t/T$$

the microscopic space variable measured in unit cell is defined by

$$\xi := \widehat{x}/\varepsilon = x/\mathsf{d}_c$$
.

Disregarding the presence of applied current terms, rescaling the equations (μ_4) , (μ_5) in the intra- and extra-cellular potentials we obtain:

(A.1)
$$\begin{cases} -\Delta u_{i,e} = 0 & \text{in } \Omega_{i,e}^{\varepsilon}, \\ \varepsilon \left(\partial_{t} v + I(v, w) = -\nabla u_{i} \cdot \nu_{i} = \alpha \ \nabla u_{e} \cdot \nu_{e} & \text{on } \Gamma_{m}^{\varepsilon}, \\ \partial_{t} w = r(v, w) & \text{on } \Gamma_{m}^{\varepsilon}, \end{cases}$$

where $\alpha := \sigma_e/\sigma_i$, $I = R_m I_{ion}$, and for convenience, the superscripts $\hat{}$ of the dimensionless variables are omitted.

In order to establish a formal relationship between a cellular model and the macroscopic bidomain structure we consider an ideal geometry and interconnection model of the cardiac cells assuming a periodic organization of the cellular tissue i.e. a periodic network of interconnected cells similar to a regular lattice of interconnected cylinders.

More precisely Ω_i^{ε} and Ω_e^{ε} are two open, disjoint, connected, periodic domains covering the entire space i.e. $\overline{\Omega}_i^{\varepsilon} \cup \overline{\Omega}_i^{\varepsilon} = \mathbb{R}^3$ with their common boundary $\partial \Omega_i^{\varepsilon} \cap \partial \Omega_e^{\varepsilon} = \Gamma_m^{\varepsilon}$ locally Lipschitz.

For $\alpha > 0$, we set

$$Y^{\varepsilon} = [0, \varepsilon]^2 \times [0, \alpha \varepsilon], \quad Y^{\varepsilon}_{i, e} = \Omega^{\varepsilon}_{i, e} \cap Y^{\varepsilon}, \quad \partial Y^{\varepsilon}_{i} \cap \partial Y^{\varepsilon}_{e} = S^{\varepsilon}$$

which defines the elementary unit ε -sized box with its intra- and extra-cellular parts, whose periodic repetition cover the whole space \mathbb{R}^3 , while

$$Y, Y_i, Y_e, S$$

denote the corresponding transformed sets expressed in the microscopic variable $\xi = x/\varepsilon$. When the reference parallelepiped Y^{ε} represents a volume box including a cardiac cell unit, then α can be interpreted as the ratio between the length and the diameter of the elongated cardiac cells.

To investigate solutions of (A.1) we use the two-scales method (see [3, 5, 45, 44, 29, 40, 29]) and we seek a solution u_i and u_e having the following asymptotic form in powers of ε of the type (the indexes i and e are omitted):

(A.2)
$$u = u_0(x, \xi, t) + \varepsilon u_1(x, \xi, t) + \varepsilon^2 u_2(x, \xi, t) + \varepsilon^2 u_2$$

where x denotes the slow macroscopic variable and $\xi = x/\varepsilon$ the fast microscopic one. The slow and fast variables correspond respectively to the global and local structure of the field and the coefficients u_k are 1-periodic function of ξ .

Considering the full derivative operators,

$$\nabla u = \varepsilon^{-1} \nabla_{\xi} u + \nabla_{x} u,$$

$$\Delta u = \varepsilon^{-2} \Delta_{\xi\xi} u + \varepsilon^{-1} \operatorname{div}_{\xi} \nabla_{x} u + \varepsilon^{-1} \operatorname{div}_{x} \nabla_{\xi} u + \Delta_{xx} u,$$

substituting the asymptotic form for $u = u_i$ into the original equation (A.1) and equating the coefficients of the powers -1, 0, 1, of ε to zero, we obtain the following equations for the functions $u_k(x, \xi, t)$, k = 0, 1, 2:

(A.3)
$$\begin{cases} \Delta_{\xi\xi}u_0 = 0 & \text{in } Y_i, \\ \nabla_{\xi} \cdot \nu_{\xi}u_0 = 0 & \text{on } S, \end{cases}$$

(A.4)
$$\begin{cases} \Delta_{\xi\xi}u_1 = -2\mathrm{div}_x \nabla_{\xi} u_0 & \text{in } Y_i, \\ \nabla_{\xi} u_1 \cdot \nu_{\xi} + \nabla_x u_0 \cdot \nu_{\xi} = 0 & \text{on } S, \end{cases}$$

(A.5)
$$\begin{cases} \Delta_{\xi\xi}u_{2} = -\operatorname{div}_{x}\nabla_{\xi}u_{1} - \operatorname{div}_{\xi}\nabla_{x}u_{1} - \Delta_{xx}u_{0} & \text{in } Y_{i}, \\ \nabla_{\xi}u_{2} \cdot \nu_{\xi} + \nabla_{x}u_{1} \cdot \nu_{\xi} = -(\partial_{t}v_{0} + I(v_{0}, w_{0})) & \text{on } S, \\ v_{0} = u_{i,0} - u_{e,0}, & \partial_{t}w_{0} = r(v_{0}, w_{0}). \end{cases}$$

In the previous problems x appears as a parameter and we seek 1-periodic solutions in ξ on the reference cell Y_i . We recall the following well known result [39, 3].

Lemma A.1. Let Ω be a bounded domain with Lipschitz boundary and S be a subset of $\partial\Omega$. If $f_k(\xi)$, k=0,1,2,3 e $g(\xi)$ are 1-periodic bounded, measurable functions in ξ then the problem

$$\begin{cases} Find \ u \in H^1(\Omega) \ periodic \ such \ that: \\ -\Delta u = f_0 - \operatorname{div} \mathbf{f} & in \ \Omega, \\ \nabla u \cdot \nu = \nu_{\xi} \cdot \mathbf{f} + g & on \ S, \end{cases}$$

admits a unique solution apart from an additive constant if and only if

$$\int_{\Omega} f_0 - \int_{S} g = 0.$$

Applying this lemma to problem (A.3) we obtain that the 1-periodic solution u_0 is independent of ξ ; since u_0 depends only on the macroscopic variable x then it represents a potential average over Y_i .

Problem (A.4) becomes:

(A.6)
$$\Delta_{\xi\xi}u_1 = 0 \text{ in } Y_i, \quad \nabla_{\xi}u_1 \cdot \nu_{\xi} = -\nabla_x u_0 \cdot \nu_{\xi} \text{ on } S,$$

and lemma A.1 guarantees its solvability. An easy check shows that the solution of (A.4) can be represented as:

(A.7)
$$u_1(x,\xi,t) = -\boldsymbol{w}(\xi) \cdot \nabla_x u_0 + \tilde{u}_1(x,t),$$

where $\boldsymbol{w} = (w^1(\xi), w^2(\xi), w^3(\xi))^T$ satisfies:

(A.8)
$$\Delta_{\xi\xi}w^k = 0, \quad \text{in } Y_i, \qquad \nabla_{\xi}w^k \cdot \nu_{\xi} = n_{\xi_k} \quad \text{on } S, \quad k = 1, 2, 3.$$

These problems are solvable by lemma A.1 apart an additive constant, which can be fixed e.g. by the condition $\int_S w^k = 0$.

Problem (A.5) becomes:

(A.9)
$$\begin{cases} \Delta_{\xi\xi}u_2 = \operatorname{div}_{\xi} \nabla_x (\nabla_x u_0 \cdot \boldsymbol{w}) + \operatorname{div}_x \nabla_{\xi} (\nabla_x u_0 \cdot \boldsymbol{w}) - \Delta_{xx} u_0 & \text{in } Y_i, \\ \nabla_{\xi} u_2 \cdot \nu = \nabla_{\xi} (\nabla_x u_0 \cdot \boldsymbol{w}) \cdot \nu - (\partial_t v_0 + I(v_0, w_0)) & \text{on } S. \end{cases}$$

Applying always lemma A.1 for the solvability of problem (A.9) for the class of 1–periodic functions we obtain:

$$-\int_{Y_i} \operatorname{div}_x \nabla_{\xi} (\nabla_x u_0 \cdot \boldsymbol{w}) d\xi - \int_{Y_i} \Delta_{xx} u_0 d\xi + \int_{S} (v_{0,t} + I(v_0, w_0)) d\sigma_{\xi} = 0.$$

Considering that u_0 is independent of ξ and substituting in (A.7) it follows:

(A.10)
$$\operatorname{div}_{x} \left[\int_{Y_{i}} \nabla_{\xi} \boldsymbol{w} \, d\xi - |Y_{i}| I \right] \cdot \nabla_{x} u_{0} + |S| (\partial_{t} v_{0} + I(v_{0}, w_{0})) = 0,$$

where $\nabla_{\xi} \mathbf{w} = [\nabla_{\xi} w^1, \nabla_{\xi} w^2, \nabla_{\xi} w^3]$ and $|Y_i|$, |S| denote the volume and the area of Y_i and S respectively.

Let $\widehat{\beta} = |S|/|Y|$ be the ratio between the surface membrane and the volume of the unit cell; then we have:

$$\operatorname{div}_{x}\left[\frac{1}{|Y|}\left(\int_{Y_{i}}\nabla_{\xi}\boldsymbol{w}\,d\xi-|Y_{i}|I\right)\nabla_{x}u_{0}\right]+\widehat{\beta}(\partial_{t}v_{0}+I(v_{0},w_{0}))=0,$$

with reference to medium (i) $w_i = w$ and we set

(A.11)
$$D_i = \frac{1}{|Y|} \left\{ |Y_i|I - \int_{Y_i} \nabla_{\xi} \boldsymbol{w}_i \ d\xi \right\}.$$

Applying the Green formula and taking into account the periodicity of w_i we have the following expression for the macroscopic tensor of intra-cellular conductivity:

$$D_i = \frac{1}{|Y|} \left\{ |Y_i|I - \int_S \nu_i \otimes \boldsymbol{w}_i \, d\sigma_{\xi} \right\}.$$

Hence we obtain the following "averaged equation" for the intra-cellular potential:

$$\operatorname{div} D_i \nabla_{x} u_{i,0} = \widehat{\beta} \left(\partial_t v_0 + I(v_0, w_0) \right)$$

Proceeding similarly for $u=u_e$ we obtain the following averaged equation for the extra-cellular potential:

$$\operatorname{div} D_e \nabla_{x} u_{e,0} = -\widehat{\beta} \left(\partial_t v_0 + I(v_0, w_0) \right),\,$$

where

$$(A.12) D_e = \frac{\alpha_e}{|Y|} \left\{ |Y_e|I - \int_{Y_e} \nabla_{\xi} \mathbf{w}_e d\xi \right\} \\ = \frac{\alpha_e}{|Y|} \left\{ |Y_e|I - \int_{S} \nu_e \otimes \mathbf{w}_e d\sigma_{\xi}, \right\}, \qquad \alpha_e = \sigma_e/\sigma_i,$$

and w_e^k , k = 1, 2, 3, are solutions of:

$$\Delta_{\xi\xi} w_e^k = 0$$
, in Y_e , $\nabla_{\xi} w_e^k \cdot \nu_e = \nu_e^k$ on S , $k = 1, 2, 3$.

Finally we rescale the previous dimensionless equations using $x = \hat{x} \cdot \mathsf{L}$ and $t = \hat{t} \cdot \mathsf{T}$, and we denote by Y^d , Y_i^d , Y_e^d , S^d the dimensional sets in the variable $x = \xi \cdot \mathsf{d}_c$ corresponding to Y, Y_i , Y_e , S, respectively; moreover we set $\beta = |S^d|/|Y^d| = \hat{\beta}/\mathsf{d}_c$.

Summarizing, for a periodic network of interconnected cells the governing dimensional equations, at the zero order in ε , of the macroscopic intra- and extra-cellular potentials are given by:

(A.13)
$$\begin{cases} \operatorname{div} M_i \nabla_x u_i = \beta \left(\partial_t v + I_{ion}(v, w) \right), \\ \operatorname{div} M_e \nabla_x u_e = -\beta \left(\partial_t v + I_{ion}(v, w) \right), \\ v = u_i - u_e, \quad \partial_t w = r(v, w), \end{cases}$$

where the effective conductivity tensors are given by:

$$M_{i,e} = rac{\sigma_{i,e}}{|Y^d|} \left\{ |Y_{i,e}^d| I - \int_{S^d} \nu_{i,e} \otimes \boldsymbol{w}_{i,e} \, d\sigma_{\xi} \right\},$$

with $\nu_{i,e}$ unit normal to S^d pointing outside $Y_{i,e}^d$ and w_i^k and w_e^k solutions of the cellular problems:

$$\Delta \boldsymbol{w}_i = 0 \quad \text{in } Y_i^d, \qquad \nabla_{\xi} \boldsymbol{w}_i \cdot \nu_i = \nu_i \quad \text{on } S^d,$$

$$\Delta \boldsymbol{w}_e = 0 \quad \text{in } Y_e^d, \qquad \nabla_{\xi} \boldsymbol{w}_e \cdot \nu_e = \nu_e \quad \text{on } S^d.$$

Remark A.2. Following [5], it is easy to verify that the macroscopic conductivity tensors of the intra-cellular M_i and extra-cellular M_e spaces are symmetric and positive definite.

REFERENCES

- [1] H. Attouch, Variational convergence for functions and operators, Pitman (Advanced Publishing Program), Boston, MA, 1984.
- [2] C. Baiocchi, Discretization f evolution variational inequalities, Partial differential equations and the calculus of variations, Vol. I (F. Colombini, A. Marino, L. Modica, and S. Spagnolo, eds.), Birkhäuser Boston, Boston, MA, 1989, pp. 59–92.
- [3] N. Bakhvalov and G. Panasenko, Homogenisation: averaging processes in periodic media, Kluwer Academic Publishers Group, Dordrecht, 1989, Mathematical problems in the mechanics of composite materials, Translated from the Russian by D. Leĭtes.
- [4] F. Bassetti, Variable time-step discretization of degenerate evolution equations in Banach spaces, Tech. report, IAN-CNR, Pavia, 2001.
- [5] A. Bensoussan, J.-L. Lions, and G. Papanicolaou, Asymptotic analysis for periodic structures, North-Holland Publishing Co., Amsterdam, 1978.
- [6] H. Brézis, Monotonicity methods in Hilbert spaces and some applications to nonlinear partial differential equations, Contribution to Nonlinear Functional Analysis, Proc. Sympos. Math. Res. Center, Univ. Wisconsin, Madison, 1971, Academic Press, New York, 1971, pp. 101–156.
- [7] H. Brézis, Opérateurs maximaux monotones et semi-groupes de contractions dans les espaces de Hilbert, North-Holland Publishing Co., Amsterdam, 1973, North-Holland Mathematics Studies, No. 5. Notas de Matemática (50).

- [8] H. Brezis, On some degenerate nonlinear parabolic equations, Nonlinear Functional Analysis (Proc. Sympos. Pure Math., Vol. XVIII, Part 1, Chicago, Ill., 1968), Amer. Math. Soc., Providence, R.I., 1970, pp. 28–38.
- [9] H. Brézis, *Intégrales convexes dans les espaces de Sobolev*, Proceedings of the International Symposium on Partial Differential Equations and the Geometry of Normed Linear Spaces (Jerusalem, 1972), vol. 13, 1972, pp. 9–23 (1973).
- [10] H. Brézis, Problèmes unilatéraux, J. Math. Pures Appl. (9) 51 (1972), 1–168.
- [11] H. Brézis C. Bardos, Sur une classe de problèmes d'evolution non linéaires, J. Differential Equations 6 (1969), 345–394.
- [12] N. F. Britton, Reaction-diffusion equations and their applications to biology, Academic Press Inc. [Harcourt Brace Jovanovich Publishers], London, 1986.
- [13] R. W. Carroll and R. E. Showalter, Singular and degenerate Cauchy problems, Academic Press [Harcourt Brace Jovanovich Publishers], New York, 1976, Mathematics in Science and Engineering, Vol. 127.
- [14] R. G. Casten, H. Cohen, and P. A. Lagerstrom, Perturbation analysis of an approximation to the Hodgkin-Huxley theory, Quart. Appl. Math. 32 (1974/75), 365–402.
- [15] P. Colli and A. Visintin, On a class of doubly nonlinear evolution equations, Comm. Partial Differential Equations 15 (1990), no. 5, 737–756.
- [16] P. Colli Franzone and L. Guerri, Spreading of excitation in 3-d models of the anisotropic cardiac tissue, Math. Biosc. 113 (1993), 145–209.
- [17] P. Colli Franzone, L. Guerri, and S. Rovida, Wavefront propagation in an activation model of the anisotropic cardiac tissue: asymptotic analysis and numerical simulations, J. Math. Biol. 28 (1990), no. 2, 121–176.
- [18] J. Cronin, Mathematics of cell electrophysiology, Marcel Dekker Inc., New York, 1981.
- [19] E. DiBenedetto and R. E. Showalter, Implicit degenerate evolution equations and applications, SIAM J. Math. Anal. 12 (1981), no. 5, 731–751.
- [20] L. Ebihara and E. A. Johnson, Fast sodium current in cardia muscle, Biophys. J. 32 (1980), 779–790.
- [21] A. Favini and A. Yagi, Degenerate differential equations in Banach spaces, Marcel Dekker Inc., New York, 1999.
- [22] R. Glowinski, J.-L. Lions, and R. Trémolières, Numerical analysis of variational inequalities, North-Holland Publishing Co., Amsterdam, 1981, Translated from the French.
- [23] C. S. Henriquez, A. L. Muzikant, and C. K. Smoak, Anisotropy, fiber curvature, and bath loading effects on activation in thin and thick cardiac tissue preparations: simulations in a three dimensional bidomain model, J. Cardiovasc. Electrophysiol. 7 (1996), 424–444.
- [24] C. S. Henriquez, Simulating the electrical behavior of cardiac tissue using the bidomain model, Crit. Rev. Biomed. Engr. 21 (1993), 1–77.
- [25] A. L. Hodkin and A. F. Huxley, A quantitative description of membrane current and its application to conduction and excitation in nerve, J. Physiol. 117 (1952), 500–544.
- [26] D. Hoff, Stability and convergence of finite difference methods for systems of nonlinear reaction-diffusion equations, SIAM J. Numer. Anal. 15 (1978), no. 6, 1161–1177.
- [27] J. J. B. Jack, D. Noble, and R. W. Tsien, Electric current flow in excitable cells, Clarendon Press, Oxford, 1983.
- [28] J. W. Jerome, Convergence of successive iterative semidiscretizations for FitzHugh-Nagumo reaction diffusion systems, SIAM J. Numer. Anal. 17 (1980), no. 2, 192–206.
- [29] V. V. Jikov, S. M. Kozlov, and O. A. Oleĭnik, Homogenization of differential operators and integral functionals, Springer-Verlag, Berlin, 1994, Translated from the Russian by G. A. Yosifian [G. A. Iosif'yan].
- [30] J. Keener and J. Sneyd, Mathematical physiology, Springer-Verlag, New York, 1998.
- [31] J.-L. Lions, Quelques méthodes de résolution des problèmes aux limites non linéaires, Dunod, Gauthier-Villars, Paris, 1969.
- [32] J.-L. Lions and E. Magenes, *Non-homogeneous boundary value problems and applications*. *Vol. I-II*, Springer-Verlag, New York, 1972, Translated from the French by P. Kenneth, Die Grundlehren der mathematischen Wissenschaften, Band 182.
- [33] J.-L. Lions and G. Stampacchia, Variational inequalities, Comm. Pure Appl. Math. 20 (1967), 493–519.
- [34] C. H. Luo and Y. Rudy, A dynamic model of the cardiac ventricular action potential. i. simulations of ionic currents and concentration changes, Circ. Res. 74 (1994), 1071–1096.

- [35] M. Mascagni, The backward Euler method for numerical solution of the Hodgkin-Huxley equations of nerve conduction, SIAM J. Numer. Anal. 27 (1990), no. 4, 941–962.
- [36] R. M. Miura, Accurate computation of the stable solitary wave for the FitzHugh-Nagumo equations, J. Math. Biol. 13 (1981/82), no. 3, 247–269.
- [37] J. S. Neu and W. Krassowska, *Homogenization of syncitial tissues*, Crit. Rev. Biom. Engr. **21** (1993), 137–199.
- [38] R. H. Nochetto, G. Savaré, and C. Verdi, A posteriori error estimates for variable time-step discretizations of nonlinear evolution equations, Comm. Pure Appl. Math. 53 (2000), no. 5, 525–589.
- [39] O. A. Oleïnik, A. S. Shamaev, and G. A. Yosifian, Mathematical problems in elasticity and homogenization, North-Holland Publishing Co., Amsterdam, 1992.
- [40] O. A. Oleĭnik and T. Shaposhnikova, On homogenization problems for the Laplace operator in partially perforated domains with Neumann's condition on the boundary of cavities, Atti Accad. Naz. Lincei Cl. Sci. Fis. Mat. Natur. Rend. Lincei (9) Mat. Appl. 6 (1995), no. 3, 133–142.
- [41] B. J. Roth, How the anisotropy of the intracellular and extracellular conductivities influence stimulation of cardiac muscle, J. Math. Biol. 30 (1992), 633–646.
- [42] B. J. Roth and W. Krassowska, The induction of reentry in cardiac tissue. The missing link: how electric fields alter transmembrane potential, Chaos 8 (1998), 204–219.
- [43] J. Rulla, Error analysis for implicit approximations to solutions to Cauchy problems, SIAM J. Numer. Anal. 33 (1996), 68–87.
- [44] E. Sánchez-Palencia and A. Zaoui (eds.), Homogenization techniques for composite media, Springer-Verlag, Berlin, 1987, Papers from the course held in Udine, July 1–5, 1985.
- [45] E. Sánchez-Palencia, Nonhomogeneous media and vibration theory, Springer-Verlag, Berlin, 1980.
- [46] S. Sanfelici, Convergence of the galerkin approximation of a degenerate evolution problem in electrocardiology, to appear on Numer. Methods Partial Differential Equations.
- [47] G. Savaré, Approximation and regularity of evolution variational inequalities, Rend. Acc. Naz. Sci. XL Mem. Mat. XVII (1993), 83–111.
- [48] G. Savaré, Weak solutions and maximal regularity for abstract evolution inequalities, Adv. Math. Sci. Appl. 6 (1996), 377–418.
- [49] R. E. Showalter, Monotone operators in Banach space and nonlinear partial differential equations, American Mathematical Society, Providence, RI, 1997.
- [50] J. Smoller, Shock waves and reaction-diffusion equations, second ed., Springer-Verlag, New York, 1994.
- [51] N. Trayanova, K. Skouibine, F. Aguel, The role of cardiac tissue structure in defibrillation, Chaos 8 (1998), 221–253.
- [52] J. P. Wikswo, Tissue anisotropy, the cardiac bidomain, and the virtual cathod effect, Cardiac Electrophysiology: From Cell to Beside (D. P. Zipes and J. Jalife, eds.), W. B. Saunders Co., Philadelphia, 1994, pp. 348–361.
- [53] A. L. Wit, S. M. Dillon, and J. Coromilas, Anisotropy reentry as a cause of ventricular tachyarhythmias, Cardiac Electrophysiology: From Cell to Beside (D. P. Zipes and J. Jalife, eds.), W. B. Saunders Co., Philadelphia, 1994, pp. 511–526.

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