Numerical simulation of blood flow

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Numerical simulation of blood flow

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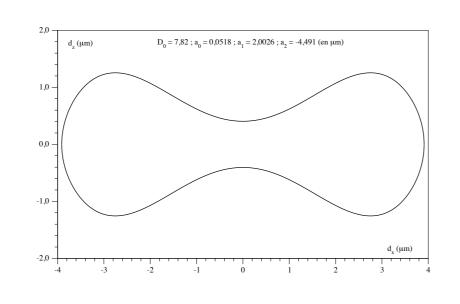


Motivation and goals

- Study of the behavior of human red blood cells
 - Physical modeling of the membrane's deformability due to its viscoelasticity
 - Mathematical modeling of the thin membrane
 - Numerical modeling of interfaces between different fluids
 - Numerical simulations
- Our approach
 - Membrane treated as a non-Newtonian viscoelastic fluid of Giesekus
 - Asymptotic modeling of the membrane as the thickness tends to 0
 - Extension of NXFEM method for interfaces to:
 - ► Nonconforming finite elements for elliptic and Stokes equations
 - ► Non-standard transmission conditions
 - Implementation in Concha library

1. Physical modeling of human red blood cells

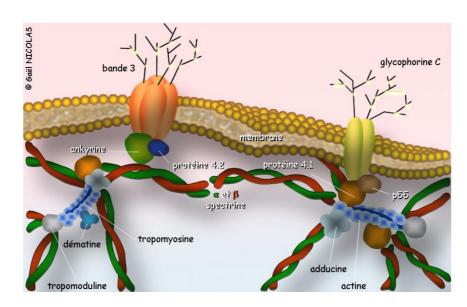
- Dimensions:
 - ullet Cell's diameter $D_0=7,\!82~\mu\mathrm{m}$
 - ullet Membrane's thickness $e_0=7,5~\mathrm{nm}$



• Equation of the surface at equilibrium (Fedosov - Evans):

$$z=\pm D_0\sqrt{1-4rac{x^2+y^2}{D_0^2}}\left(a_0+a_1rac{x^2+y^2}{D_0^2}+a_2rac{\left(x^2+y^2
ight)^2}{D_0^4}
ight)$$

- Membrane: composite material (lipid bilayer+spectrin elastic network)
 - classically, the membrane is a hyper-elastic solid



- Membrane: viscoelastic properties → in our approach, it is a viscoelastic non-Newtonian liquid
- Realistic constitutive law of Giesekus:

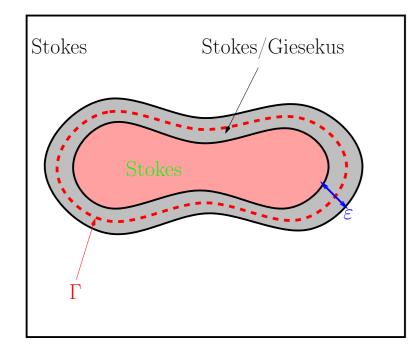
$$\lambda \left(rac{\partial}{\partial t} au + u \cdot
abla au - au (
abla u)^t -
abla u au
ight) + au + rac{\lambda}{2\eta} au \cdot au = \eta \left((
abla u)^t +
abla u
ight)$$

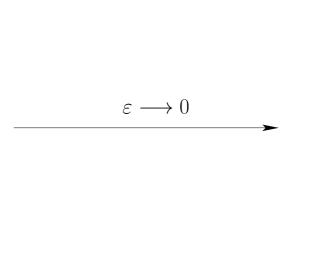
u the velocity, au the viscous stress tensor, λ the relaxation time, η the viscosity

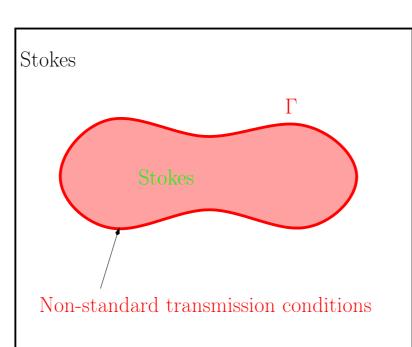
2. Mathematical modeling of the small thickness

 $ullet arepsilon := rac{e_0}{D_0} pprox 10^{-3} \leadsto ext{problem to mesh the thin membrane} \, !$

ullet We consider the limit weak problem as arepsilon tends to 0





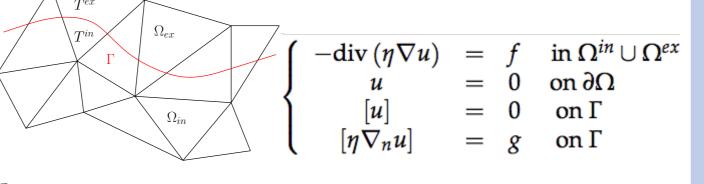


Limit model problem

- Initial model problem
- Mathematical analysis in the case of:
 Rectilinear interface
 - Stokes equations in the membrane
- Extension to smooth curved interface and to Giesekus law

3.1. Numerical modeling of interfaces: NXFEM

- Nitsche's Extended Finite Element Method (NXFEM):
 - introduced for conforming approx. of elliptic problems (Hansbo & Hansbo '02)
 - designed to take into account discontinuities on non-aligned meshes by:
 - > standard FE spaces enriched on cut cells (doubled d.o.f. : $V_h = V_h^{in} imes V_h^{ex}$)
 - interface conditions treated by Nitsche's method (additional terms in the weak form)



$$egin{aligned} A_h\left(u_h,v_h
ight) &= \sum_{T\in\mathcal{T}_h}\int_T \eta
abla u_h \cdot
abla v_h \,dx & imes ext{Classical term} \ &- \int_\Gamma \{\eta
abla_n u_h\} \left[v_h
ight] \,ds - \int_\Gamma \{\eta
abla_n v_h\} \left[u_h
ight] \,ds & imes ext{Symmetrization} \ &+ \gamma \sum_{T\in\mathcal{T}_h^\Gamma} rac{\eta_{in}\eta_{ex}|T|}{\eta_{ex}|T^{in}| + \eta_{in}|T^{ex}|} \int_{\Gamma_T} \left[u_h
ight] \left[v_h
ight] ds & imes ext{Stabilization} \end{aligned}$$

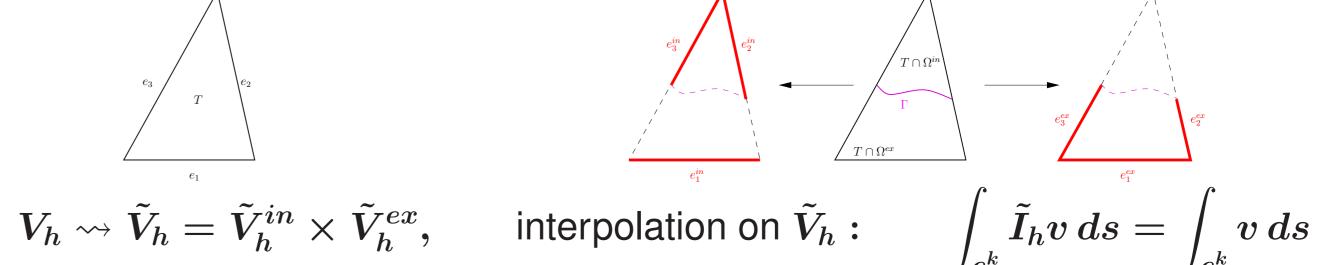
with γ a stabilization parameter

3.2. Numerical modeling of interfaces: our contributions

Development of two variants of NXFEM method for:

- Crouzeix-Raviart nonconforming finite elements
- Elliptic and Stokes equations
- Main difficulties:
 - Nonconforming approximations: estimate the consistency error on cut edges
 - Stokes equations: inf-sup condition
- Proposed solutions
- Modification of the classical basis functions on the cut triangles

$$egin{aligned} arphi_i \in P_1(T), rac{1}{|e_j|} \int_{e_j} arphi_i ds = \delta_{ij} \qquad \qquad & ilde{arphi}_i^k \in P_1(T), rac{1}{\left| rac{e_j^k}{j}
ight|} \int_{e_j^k} ilde{arphi}_i^k \, ds = \delta_{ij} \ k = in, \ ex, \quad 1 \leq i,j \leq 3 \end{aligned}$$



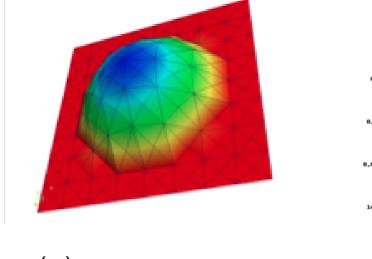
2 Addition of stabilization terms to the bilinear form $A_h(\cdot,\cdot)$

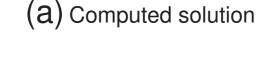
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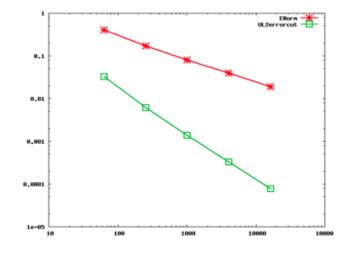
- Obtained results for elliptic and Stokes equations:
- Existence and uniqueness of the discrete solution
- Interpolation and a priori error estimates
 (optimal and robust w.r.t. geometry and coefficients)
- Convergence of the second method towards the first one when $\gamma_k \longrightarrow +\infty$

4. Implementation in Concha library and numerical tests

- Implementation of the second method for elliptic equations
- Reference test (Hansbo & Hansbo '02)
 - exact solution with highly discontinuous coefficients
 - optimal convergence rates
 - similar results to conforming f.e.







(b) L^2 and energy errors

5. Ongoing and future works

- Ongoing works:
 - Implementation in the library Concha (first method, Stokes equations ...)
- Development of NXFEM for non-standard interface conditions
- Paper on NXFEM with nonconforming f.e.
- Future works:
 - Giesekus model for a thin membrane (development and implementation)
 - Validation for realistic test-cases (two-phase flow, red blood cell...)
 - Paper on asymptotic modeling of membrane

6. Publications and conferences

- D. Capatina, R. Luce, H. El-Otmany, N.Barrau: NXFEM for solving non-standard transmission problems,
 NM2PorousMedia, Dubrovnik, September 29th October 3rd 2014
- D. Capatina, S. Delage-Santacreu, H. El-Otmany, D. Graebling: Robust NXFEM method for a nonconforming approximation on an elliptic problem, XIth World Congress on Computational Mechanics, Barcelona, 20th-25th July 2014 (mini-symposium)
- D. Capatina, S. Delage-Santacreu, H. El-Otmany, D. Graebling: Modélisation du comportement de globules rouges dans un écoulement sanguin, Journées Bordeaux-Pau-Toulouse, Anglet, 19-20 September 2013
- NXFEM with nonconforming finite elements, PhD Students Seminar, LMAP, 2012

7. Other research activities

- Participation to the ECCOMAS Conference "XFEM 2013", Lyon (France)
- Elected member in LMAP Council, 2013
- Co-organization of PhD Students Seminar, LMAP, 2013-2014
- Co-author of Guide des doctorants, Doctoral School 211, University of Pau
- Teaching (64 h/year), 2013-2014
- 8 training courses (9 ECTS)